

# Application to society: Imaging in particle therapy

Aafke Kraan

National Institute of Nuclear Physics, Section of Pisa, Italy



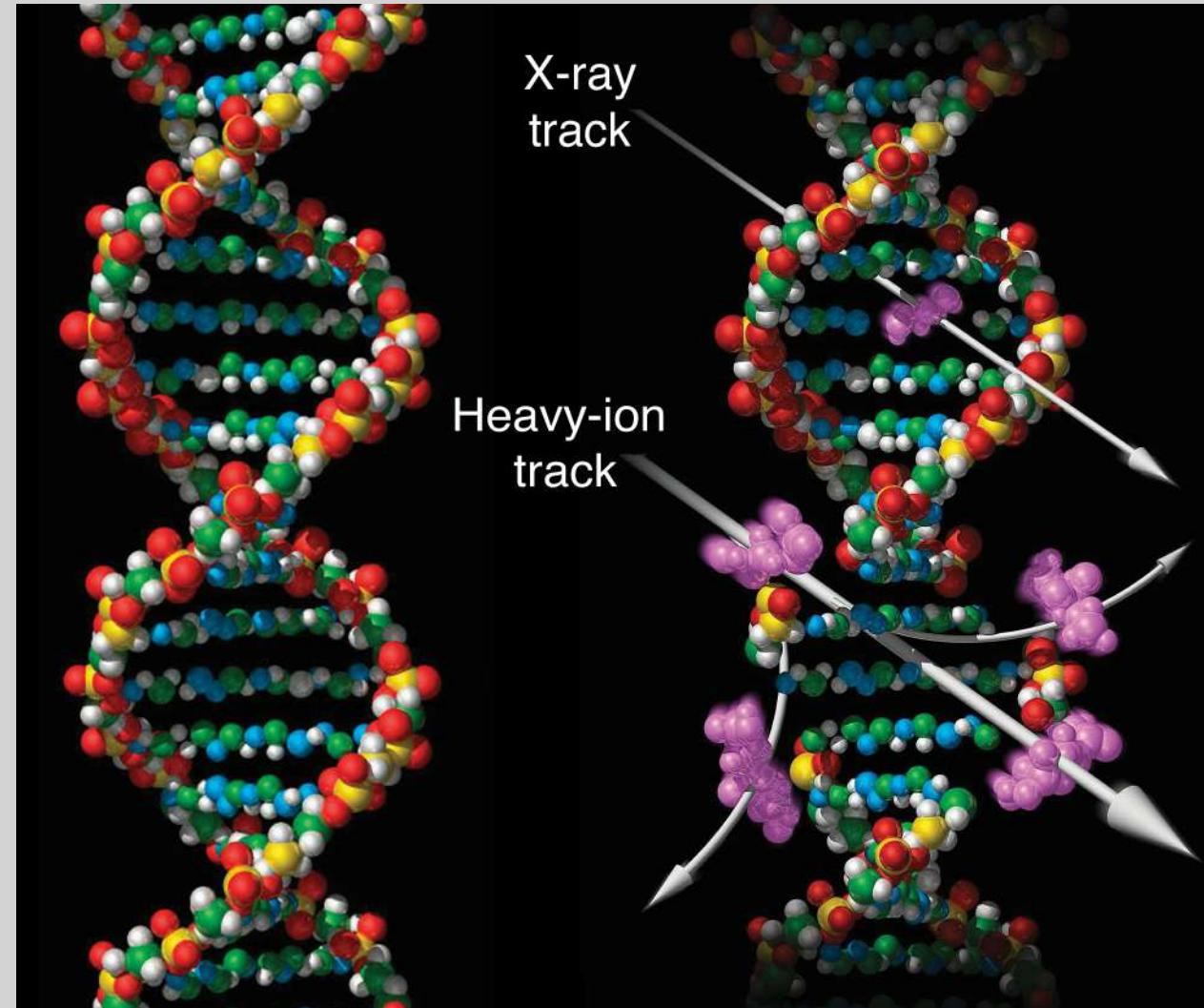
# Outline

- Introduction to particle therapy
- Imaging in particle therapy
- Imaging methods taking advantage of nuclear interactions
- Proton radiography and proton tomography
- Conclusions

# Particle therapy

- Radiotherapy=usage of radiation to kill tumorous cells
- Conventional radiotherapy: mostly photons (x-ray)
- Particle therapy=special kind of radiotherapy
- What particles?
  - Protons : up to 250 MeV
  - Carbon : up to 400 MeV/u
  - Others: Helium, Oxygen, ...
- Particle beams can deliver energy to small volume, penetrate in depth (different from lasers), interact with cells, molecules, and atoms (electrons and nuclei)

→ destroy cancerous cells



# Particle therapy

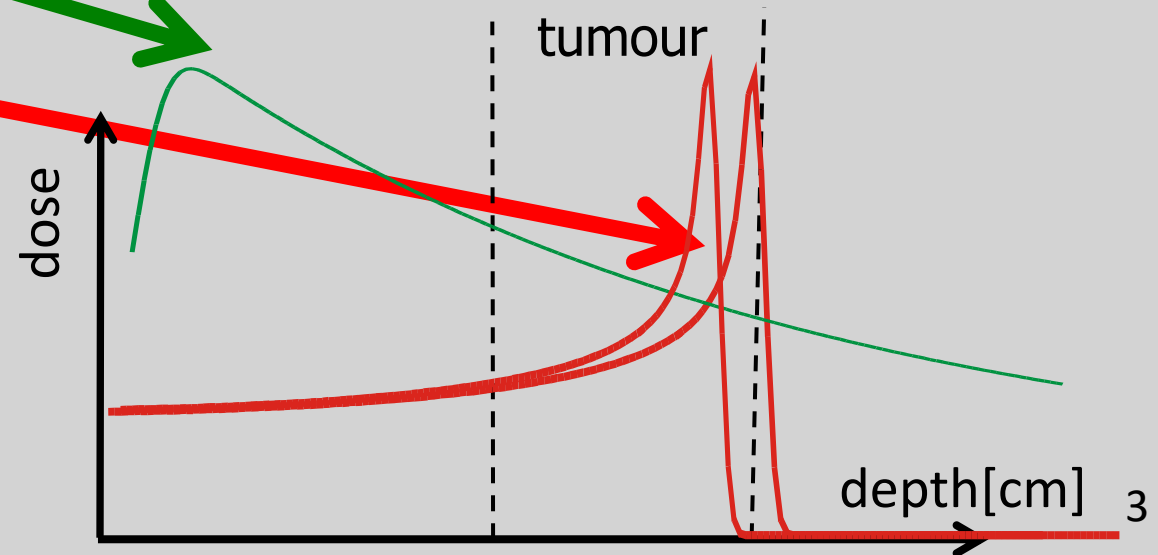
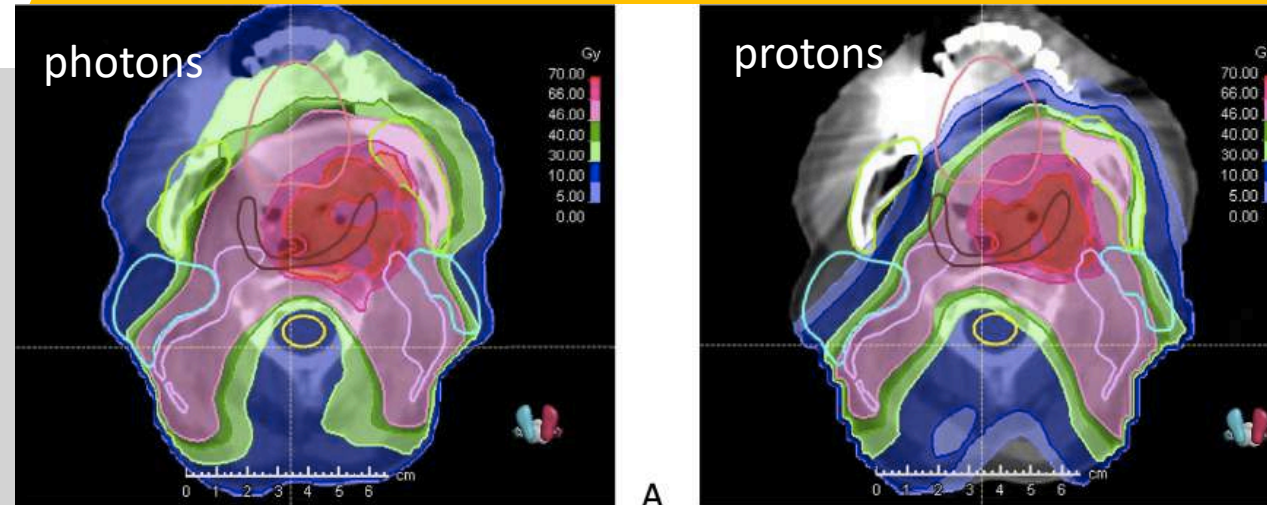
From: A. Beddok et. al., Radiotherapy and Oncology 147 (2020) 30–39

- Compared to photons, charge particles have a more selective energy deposition
  - Photons: high dose delivered in front and behind tumor
  - Charged particles: Bragg Peak: Dose spot
    - Energy  $\sim$  depth
    - Nr. particles  $\sim$  height

$$-\frac{dE}{dx} = \frac{4\pi}{m_e c^2} \cdot \frac{nz^2}{\beta^2} \cdot \left(\frac{e^2}{4\pi\epsilon_0}\right)^2 \cdot \left[ \ln\left(\frac{2m_e c^2 \beta^2}{I \cdot (1-\beta^2)}\right) - \beta^2 \right]$$

Bethe-bloch

Reminder: dose [Gy]=Energy [J]/mass [kg]



# Particle therapy

End of 2020, more than 290'000 patients have been treated worldwide with Particle Therapy

- about 250'000 with protons
- about 40'000 with C-ions
- 3'500 with He, pions and with other ions.

India:

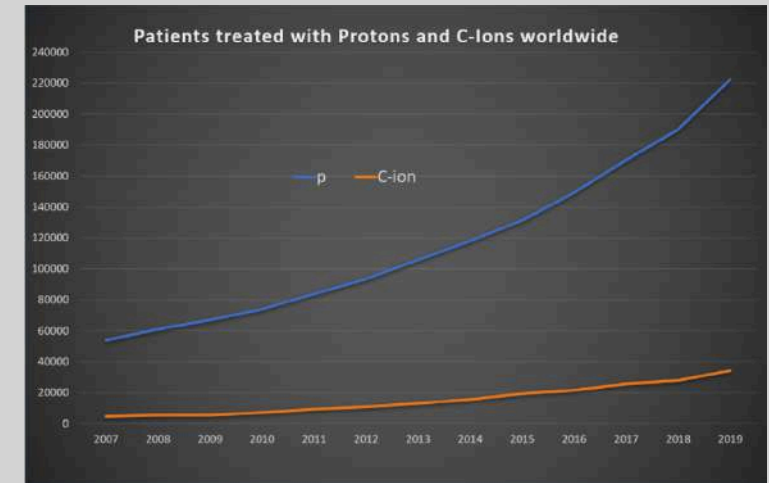


The Apollo Proton Cancer Centre was inaugurated on **January 25, 2019** in Chennai

South East Asia's first Proton Therapy Centre

From: <https://www.ptcog.ch/index.php/ptcog-patient-statistics>

Idea by Robert Wilson, 1946

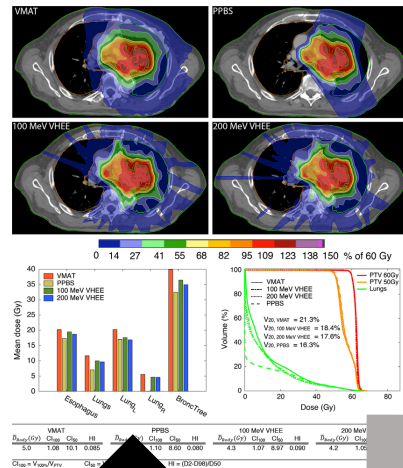


# Particle therapy

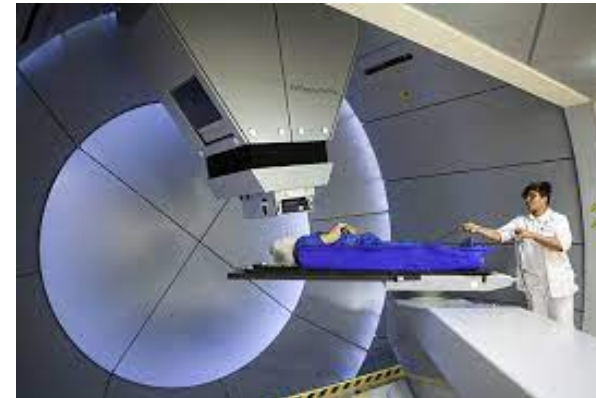
Consultation



Treatment planning



Treatment delivery (few weeks)



Follow-up



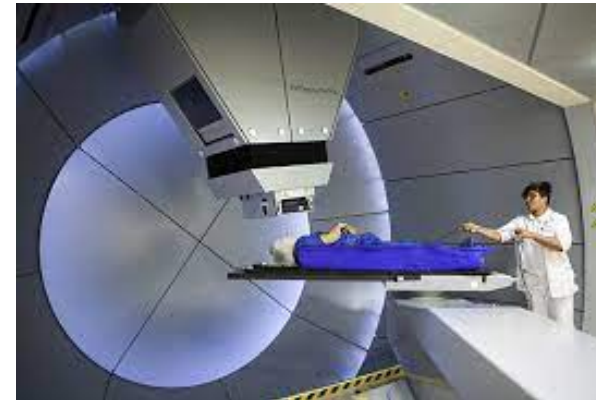
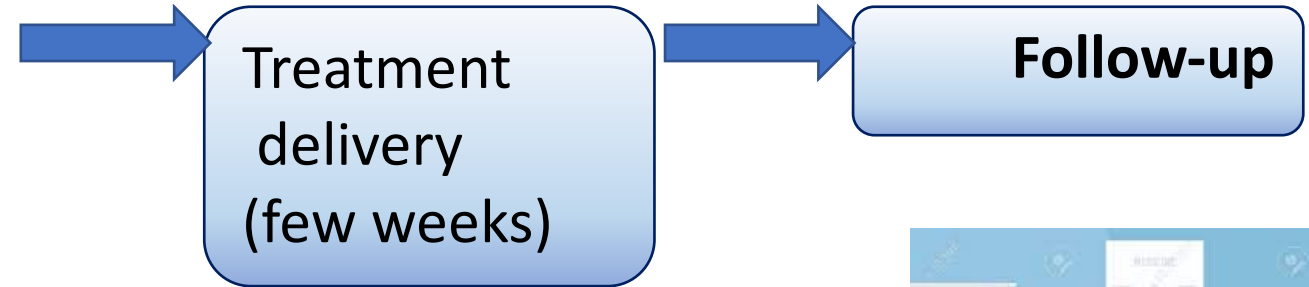
CT scan  
Structures  
Dose prescription

Usually after N weeks:  
CT scan with structures

# Imaging in particle therapy

**Pre-treatment:** for diagnosis, contouring and treatment planning

- Computed Tomography
  - Single Energy CT
  - Dual Energy CT
- MRI: Magnetic Resonance Imaging
- SPECT: Single-photon emission computed tomography
- PET: Positron-Emission-Tomography

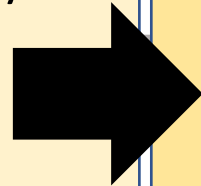


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**Treatment:** for patient daily positioning, dose delivery and evaluation of anatomical changes

- In-room image guidance
  - X-ray
  - Cone –beam CT
  - Future: proton CT (pCT) or proton radiography
- During treatment:
  - PET;
  - prompt gamma;
  - charged fragments
  - Implantable dosimeters for direct Bragg peak evaluation.

**Follow-up**

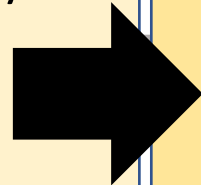


S

# Imaging in particle therapy

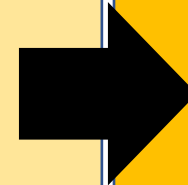
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**Post-treatment:** patient follow-up and post-treatment assessment

- MRI
- CT

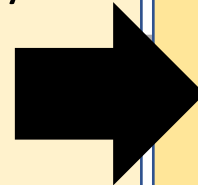
# Imaging in particle therapy

See also J. Seco, M.F. Spadea, Imaging in particle therapy: State of the art and future perspective, Acta Oncologica 54, 9, 1254-1258, 2015

See also A. Del Guerra, Ionizing Radiation Detectors for Medical Imaging

**Pre-treatment:** for diagnosis, contouring and treatment planning

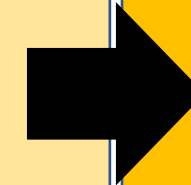
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- **During treatment:**
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  - **prompt gamma;**
  - **charged fragments**
  - Implantable dosimeters for direct Bragg peak evaluation.

**TODAY**



**Post-treatment:** patient follow-up and post-treatment assessment

- MRI
- CT

# Imaging in particle therapy: uncertainties

## Patient related

- daily positioning on the couch
- internal organ motion
- changes in air cavities
- tumour regression
- weight loss

## Physics related

- CT HU (e.g. calibration apparatus)
- conversion to proton stopping power
- dose calculation uncertainties

## Other sources

- RBE values
- Tumor heterogeneity
- Contouring uncertainties
- Reconstruction artifacts in CT
- Machine related

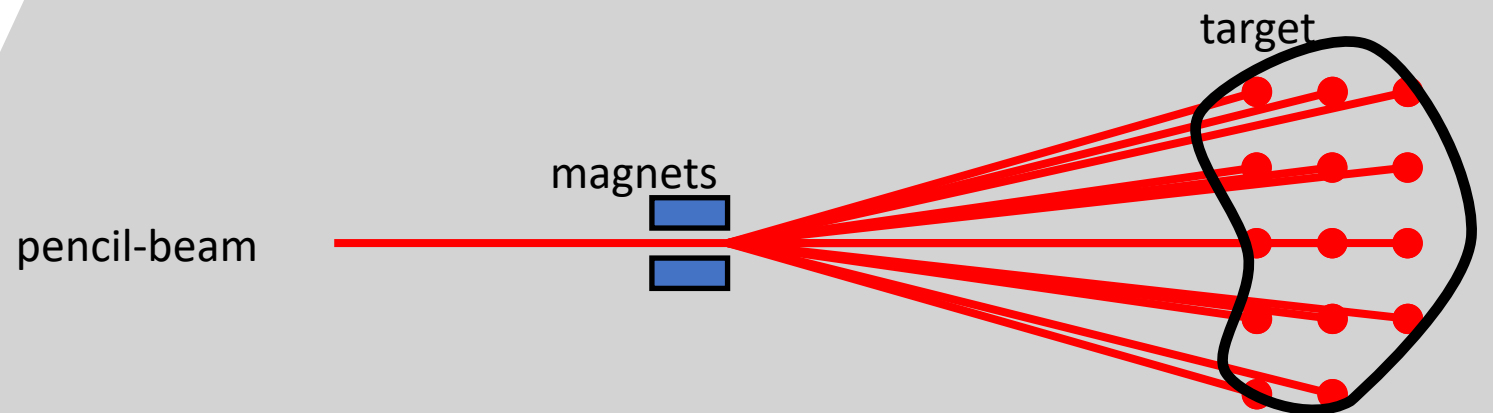
Dose/Bragg Peak  
Monitoring is advisable!

# Particle therapy

One of **the most** impactful developments since the advent of proton therapy has been **pencil beam scanning (PBS)**

(applied widely worldwide, also at Apollo Proton Cancer Centre )

Small currents: 10 nA for a typical dose of 1 Gy to 1 liter in 1 minute.



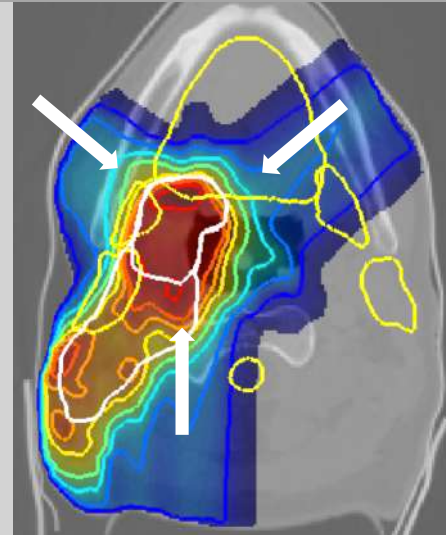
# Dose impact of uncertainties

- Very precise...
- But different uncertainties can lead to dose distortions...

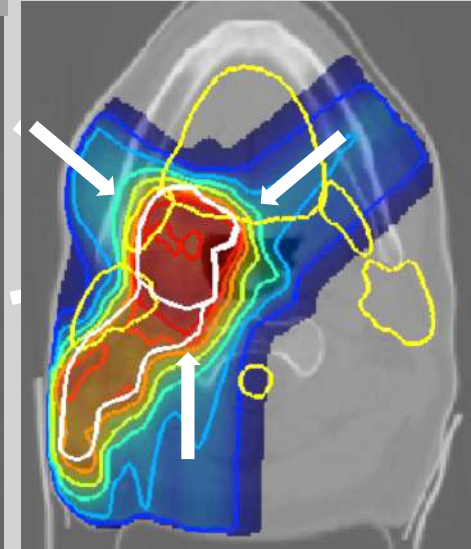
From: Kraan, Int J Radiat Oncol Biol Phys 2013;87(5):888-96.



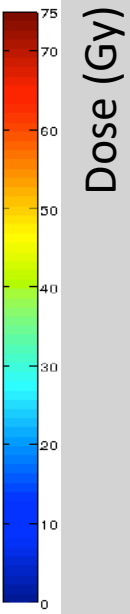
Planned dose



Delivered dose when  
Anatomy changed



Delivered dose when  
patient misaligned



Dose/Bragg Peak  
Monitoring is advisable!

# Treatment monitoring

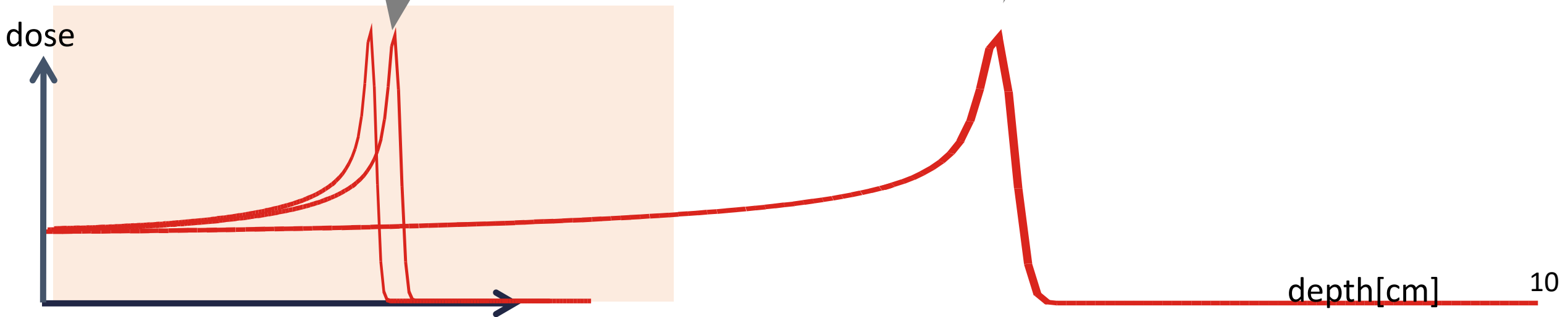
Based on Nuclear Reactions of Hadrons in Tissue

- Off-line & On-line PET
- Prompt gamma's and neutrons
- Prompt charged particles (only for Ions)

Beam stopping inside patient

Based on X-ray CT- analogous: pCT (only for Protons)

Beam going through



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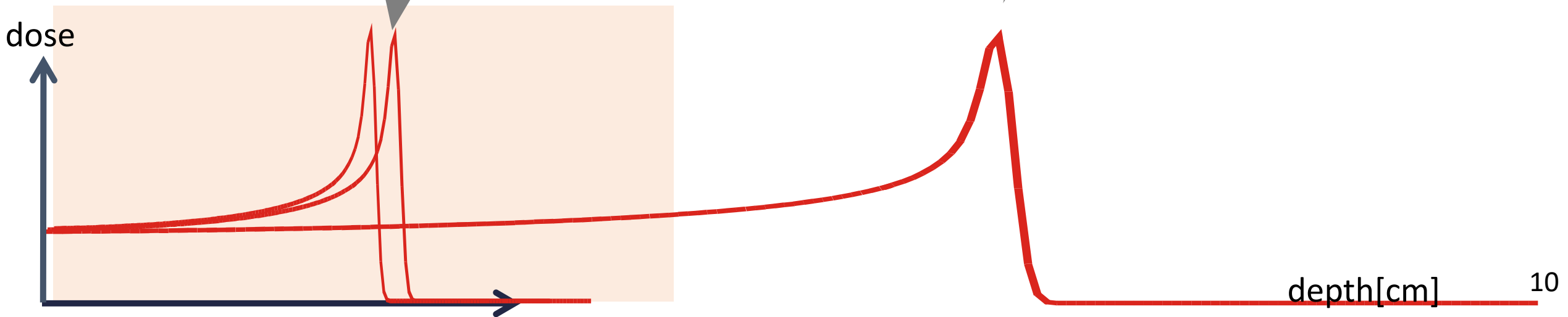
Beam stopping inside patient

Slides 11-35

Based on X-ray CT- analogous: pCT (only for Protons)

Beam going through

Slides 36-39



# Nuclear interactions in particle therapy



1940-2009

*“Physical Measurements with High-Energy Radioactive Beams”*

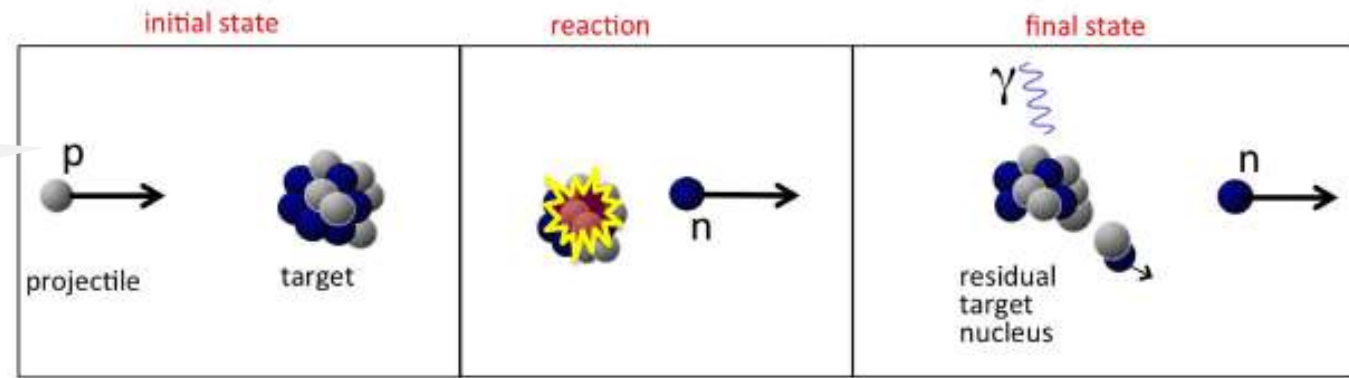
A. Chatterjee, W. Saunders, E. L. Alpen, J. Alonso, J. Scherer and J. Llacer Radiation Research, Vol. 92, No. 2 (Nov 1982), pp. 230-244

## **Abstract**

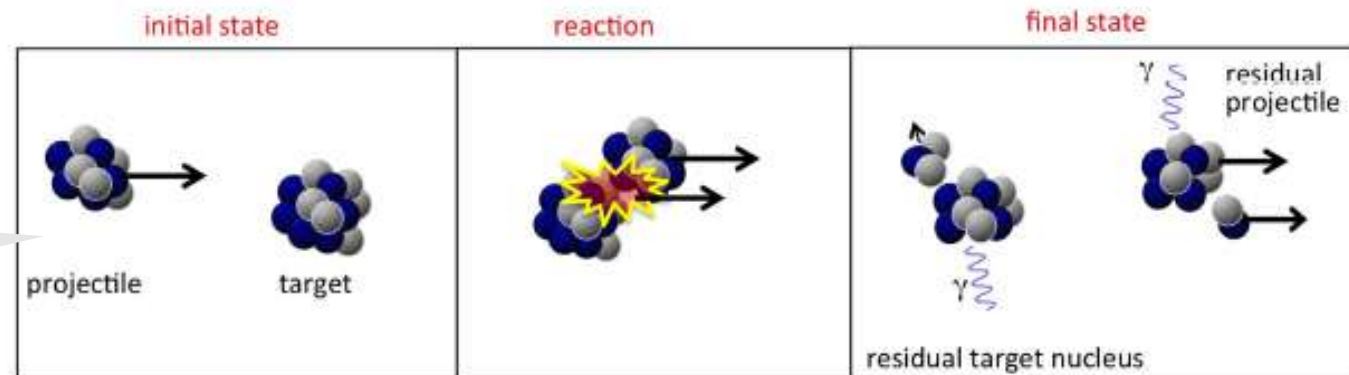
“Physical measurements were made with **high-energy radioactive beams (positron emitters) produced as secondary particles from a heavy-particle accelerator**. Data are presented for water-equivalent thickness of a silicon diode, a comparison of Bragg peak ionization depth vs stopping depth, and differential stopping depths when a beam is intercepted by heterogeneous materials in the orthogonal direction. A special positron-emitting beam analyzing (PEBA) system was used to form images of the stopped radioactive beam. **These measurements will have direct impact on charged-particle radiotherapy, since the precise range of beams of charged particles to targets within patients can be measured and used for treatment planning. Also, during the treatments the stopping point of the beam can be monitored to verify that the treatment is being delivered as planned.**

# Nuclear interactions in particle therapy

Proton therapy:  
Example of  
proton nucleus  
interaction



Carbon therapy:  
Example of  
nucleus nucleus  
interaction

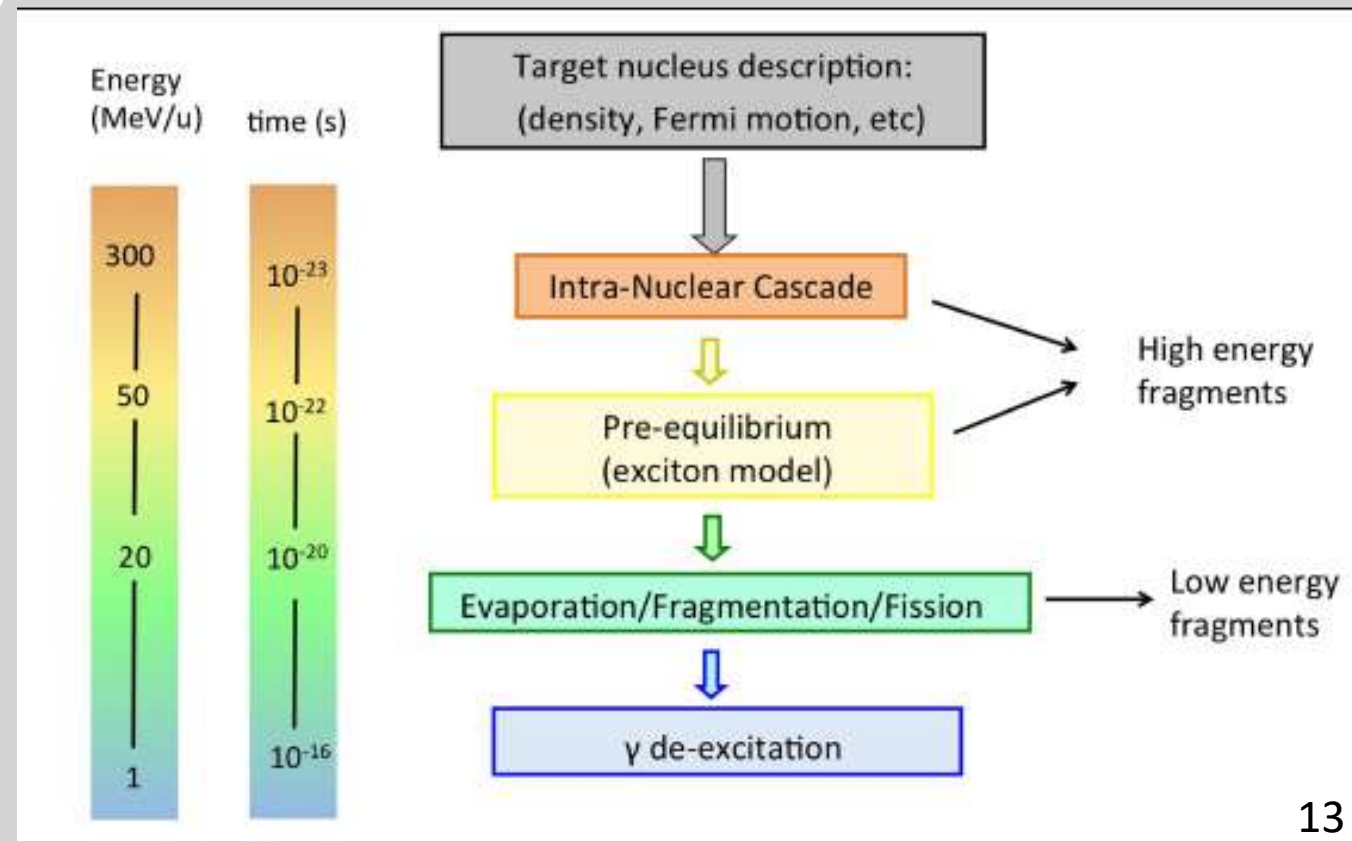


# Nuclear interactions in particle therapy

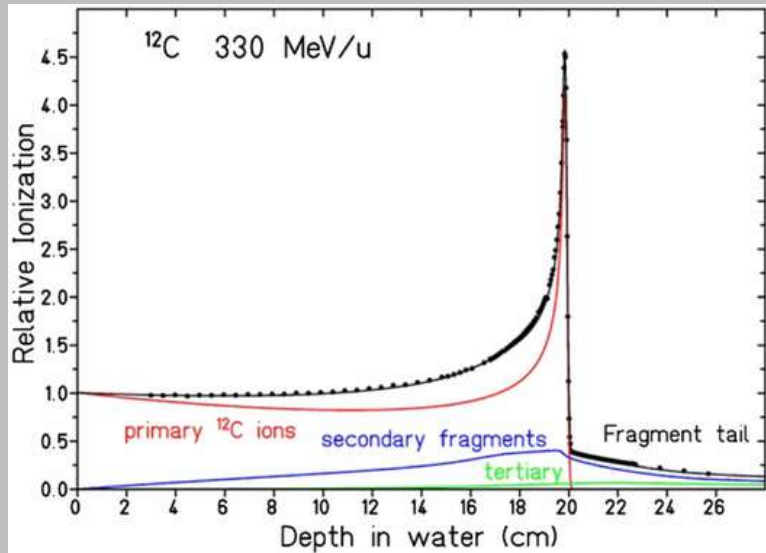
- Many stages in nuclear reaction...

Battistoni G, Bauer J, Böhlen T, Cerutti F, Chin M, et al. The FLUKA code: an accurate simulation tool for particle therapy. *Fron Oncol.* (2016). 6:116. doi:10.3389/fonc.2016.00116

Ref.: AK, *Frontiers in Oncology*, 07 July 2015 doi: 10.3389, adapted from A. Ferrari's presentations



# Nuclear interactions in particle therapy



## Consequences

Loss of beam fluence. For 290 MeV/u carbons: 50% of ions have nuclear reaction

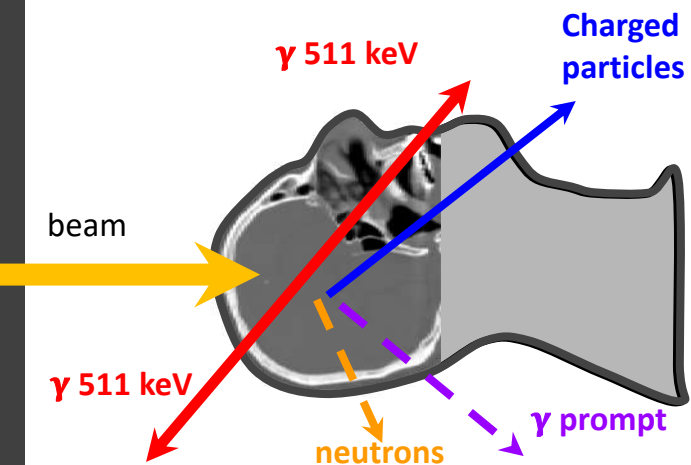
The dose distributions are modified:

Build-up region of Bragg curve

Height of the Bragg peak.

Carbon therapy: dose beyond the Bragg peak.

Low energetic secondary particles --> "low dose envelope"



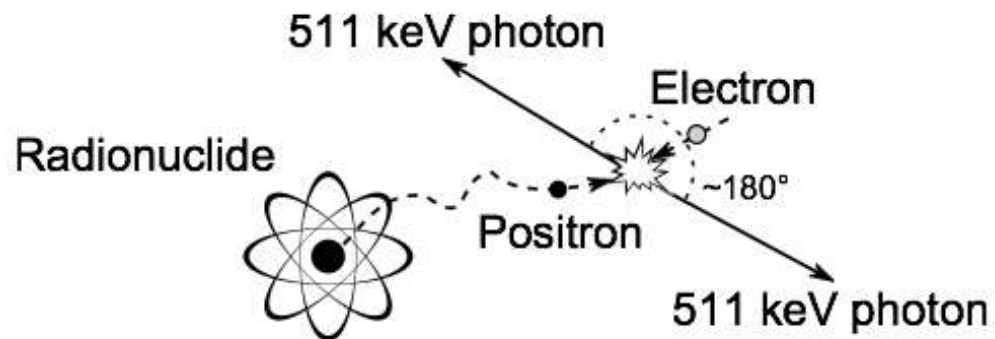
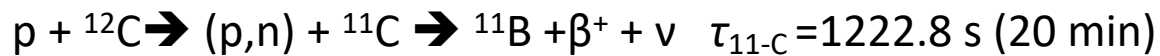
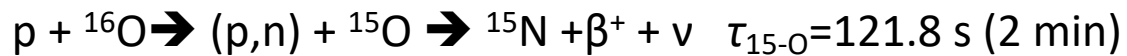
+ Various types of secondary particles are produced.  
Kinematics depend on stage during nuclear reaction

- +  $\beta^+$  emitting isotopes  $\rightarrow$  PET
- + Prompt gammas
- + Charged fragments are produced

# Nuclear interactions in particle therapy

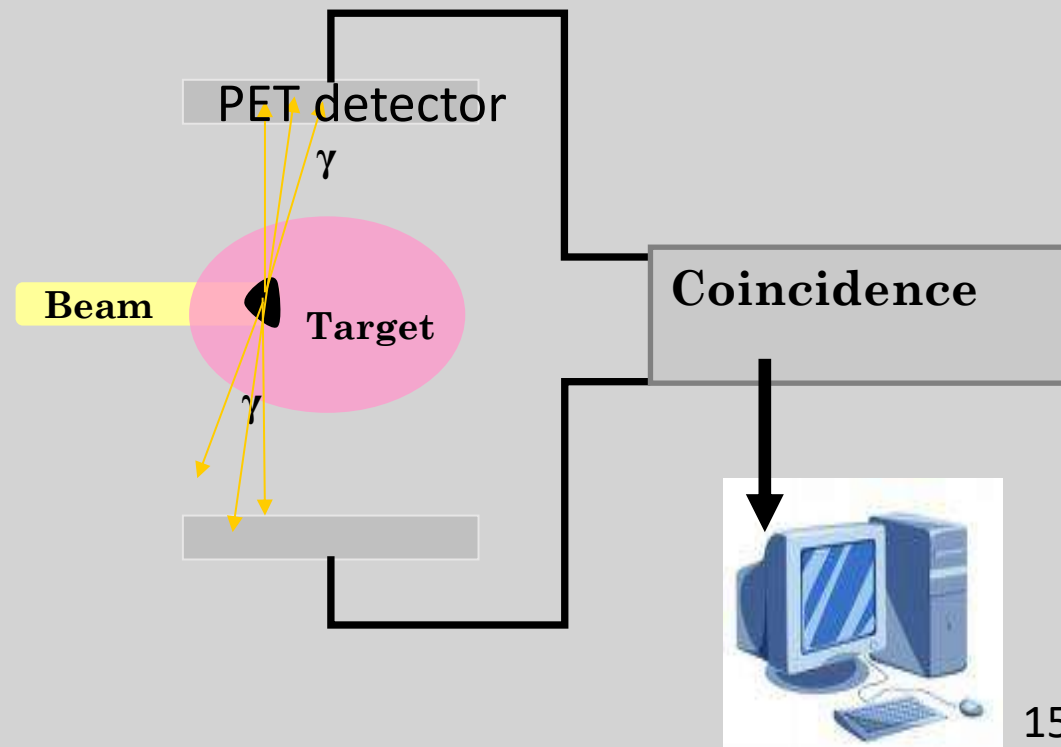
- One of the ways to verify the delivered dose is by means of PET (Positron-Emission-Tomography)
- Therapeutic hadron beams produce  $\beta^+$  emitters in the body

E.g. proton beam:



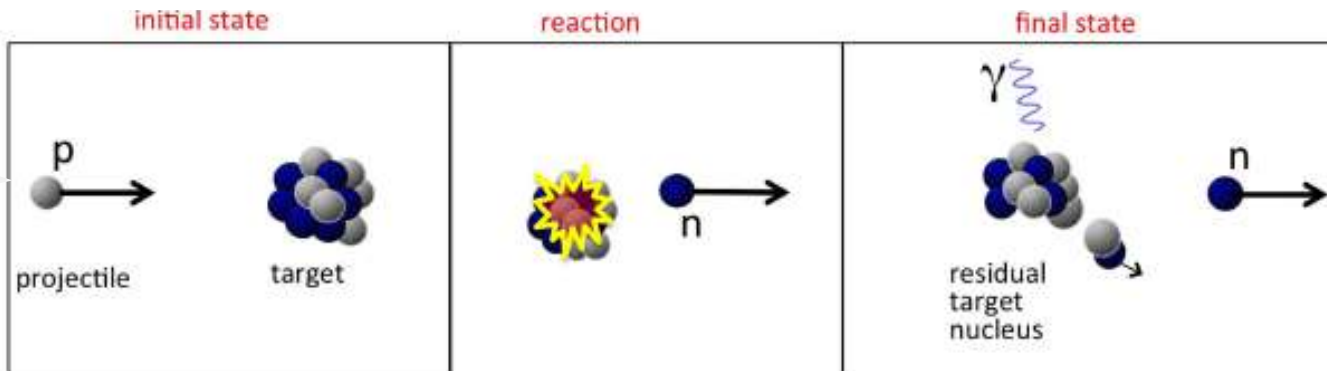
**PET activity=**

nr of radioactive decays per time-interval

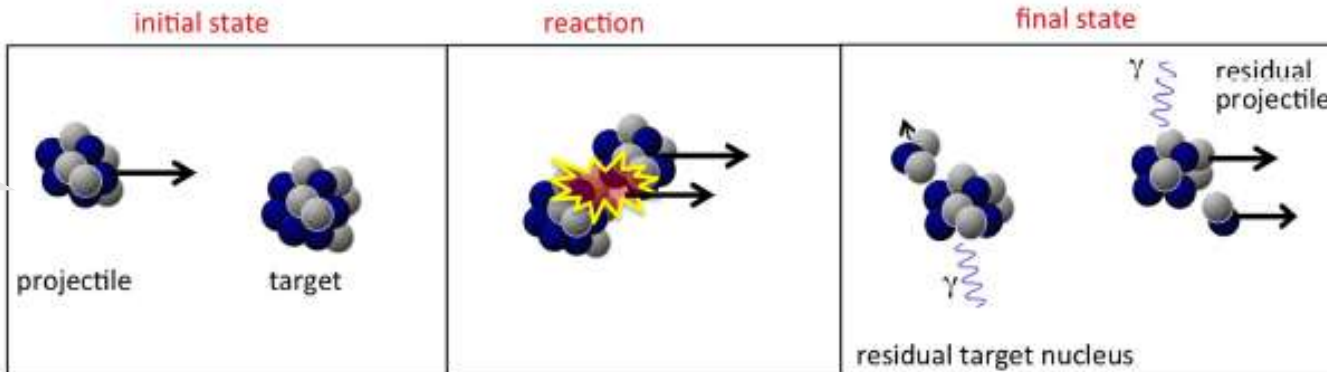


# Nuclear interactions in particle therapy

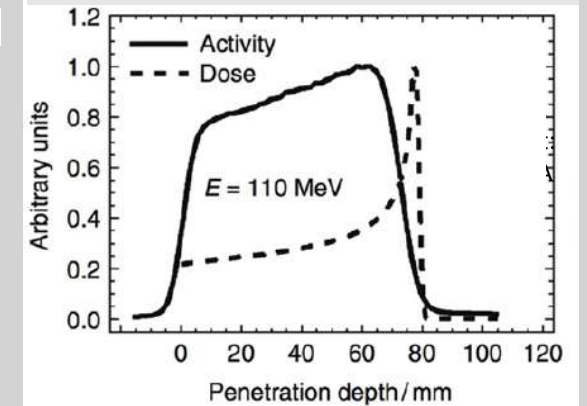
Proton therapy:  
Example of proton nucleus interaction



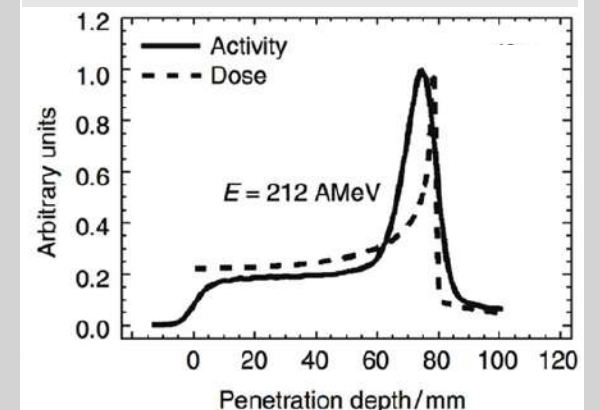
Carbon therapy:  
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Beam: proton Target: PMMA



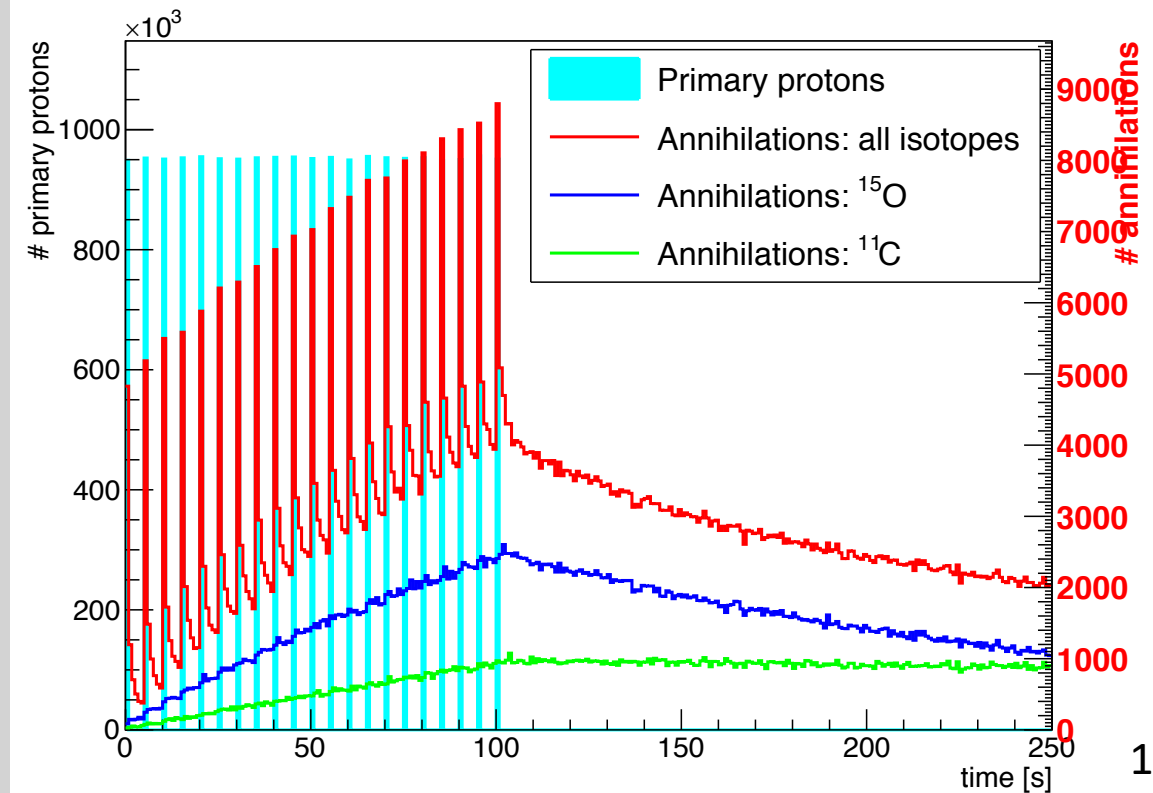
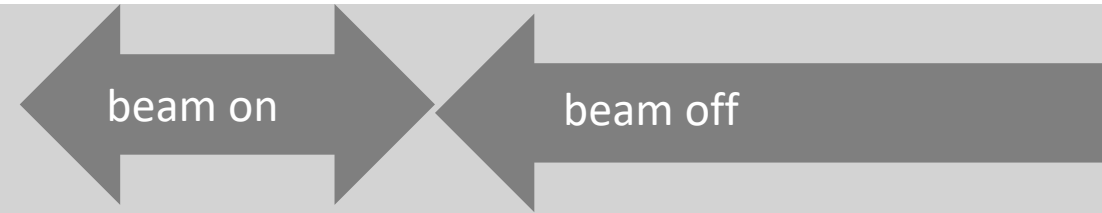
Beam:  $^{12}\text{C}$  Target: PMMA



Beta+ activity indirectly related with Bragg peak position!

# Nuclear interactions in particle therapy

FLUKA simulation of beta+ annihilation in phantom for a proton beam



# PET monitoring in particle therapy

K. Parodi and J. Polf. "In vivo range verification in particle therapy", Medical Physics 45, 2018

A.C. Knopf and A Lomax. "In vivo proton range verification: a review". In: Phys Med. Biol. 58.15 (2013), R131–160.

First pioneer work by W. Enghardt et al. in the '90 with Carbon Ions (*GSI/Bastei tomograph*)

**Off-line PET** = dose delivery and PET in different locations  
(*MGH/Heidelberg/CHIBA*)

- Advantages
  - Commercial PET scanner 360 degrees (no image artefacts)
- Disadvantages:
  - Patient re-positioning
  - Data loss of very short living isotopes (e.g.  $^{15}\text{O}$ )
  - Radio-isotope wash-out



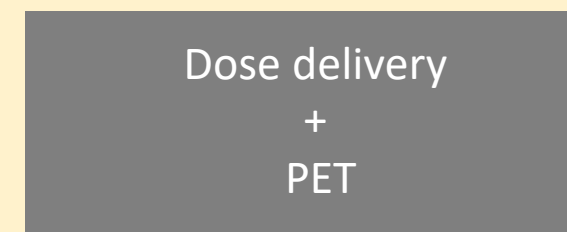
**On-line PET** = dose delivery and PET in same room

→ In Room-PET: data when beam is off  
(*GSI/PISA-CNAO/CHIBA/MGH/HEIDELBERG*)



→ In-beam-PET: data when beam on (*PISA-Torino-CNAO/CHIBA-openPET*)

- Disadvantages:
  - Image artefacts
  - Small statistics (not much  $^{11}\text{C}$ )



# PET monitoring in particle therapy

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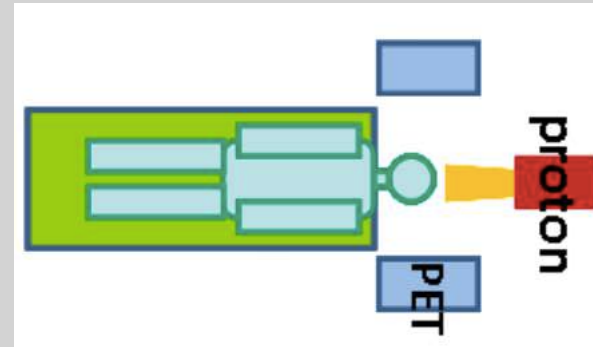
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**COVERED TODAY**

Dose delivery  
+  
PET

# PET monitoring in particle therapy

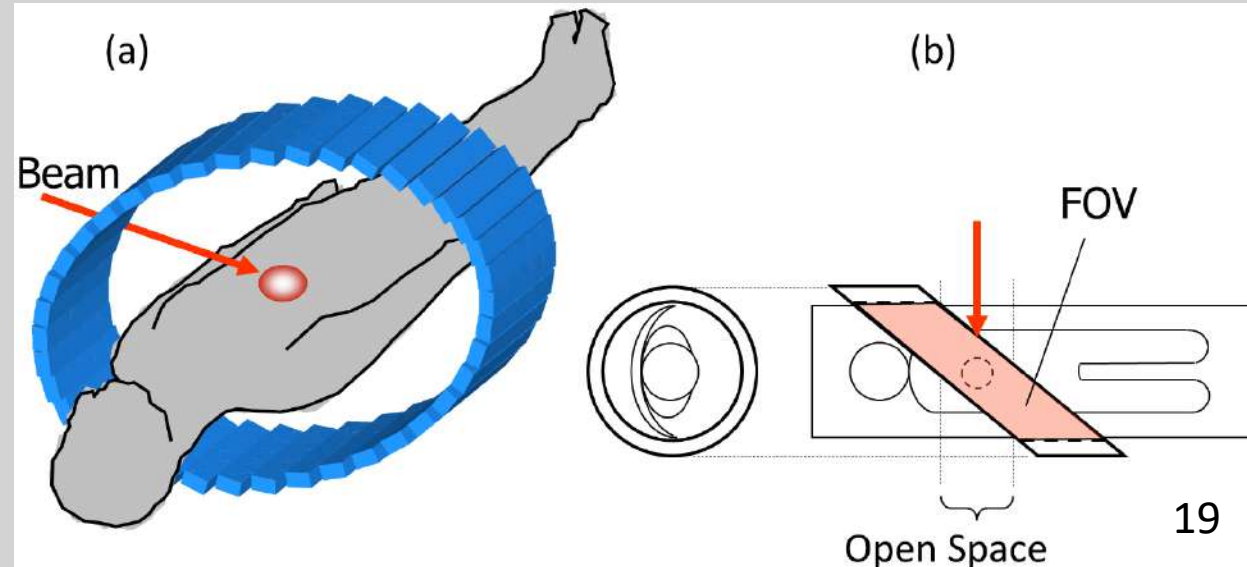
- Main problem in in-beam PET: difficult to integrate with dose delivery system, position systems, etc ...
- Solutions
  - Two planes (see next)
  - Particular geometries
    - Example: Open PET system @ CHIBA, Japan



V. Rosso et al, DoPET: an in-treatment monitoring system for particle therapy, *Radiotherapy and Oncology* 118:S92

G.M. Bisogni et al.: *Journal of Medical Imaging* 4 (Dec. 2016), p. 011005

Tashima et al 2016 *Phys. Med. Biol.* 61 1795



# PET monitoring in particle therapy

## INnovative Solutions for In-beam DosimEtry in Hadrontherapy

Pisa, Torino, Roma "La Sapienza", Bari, INFN

**INSIDE coordinator: M. G. Bisogni (Pisa)**



This project has been supported by Italian MIUR under the program PRIN 2010-2011 project nr. 2010P98A75 and by EU FP7 for research, technological development and demonstration under grant agreement no 317446 (INFIERI)



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P. Sala

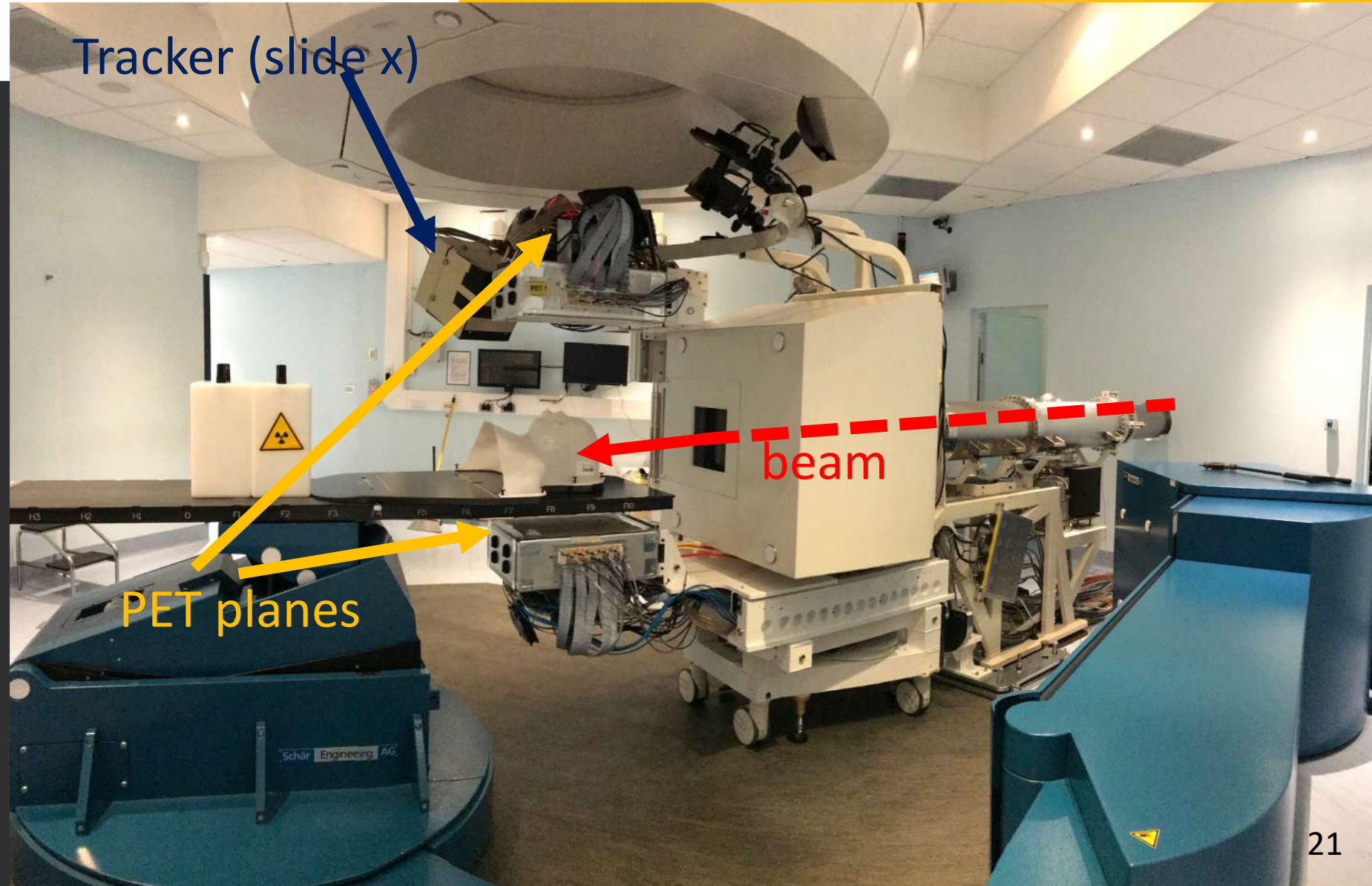
# INSIDE

INSIDE detector :

- Designed in 2010-2013
- Constructed 2014-2016
- Installed at CNAO since 2016
  - Close to nozzle
  - Operated during beam delivery and up to about 30 seconds after

*InSide*

CNAO

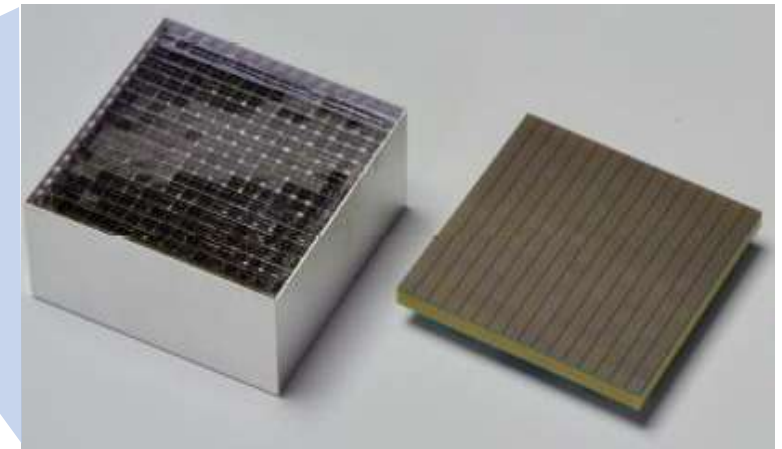
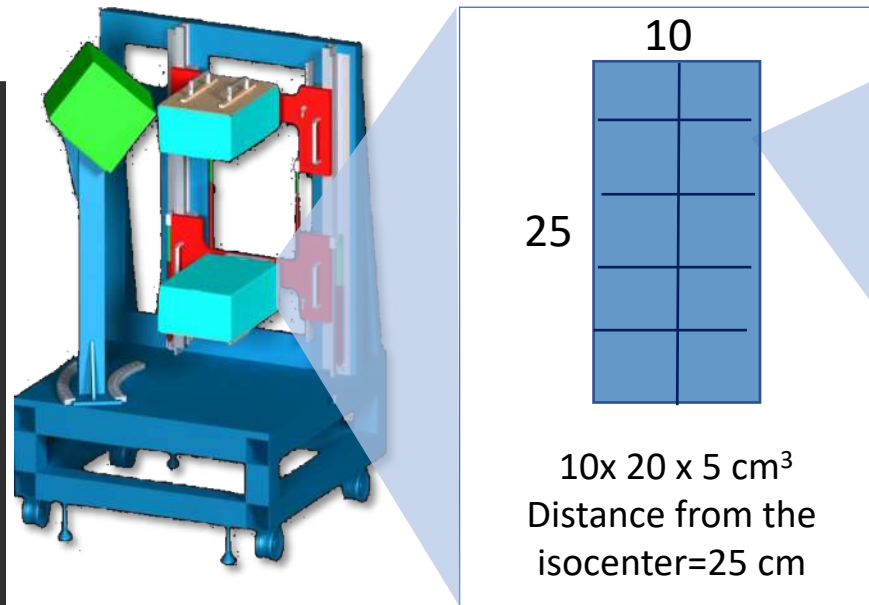


# INSIDE: in-beam PET

Courtesy of A. Del Guerra. Krakow 2015

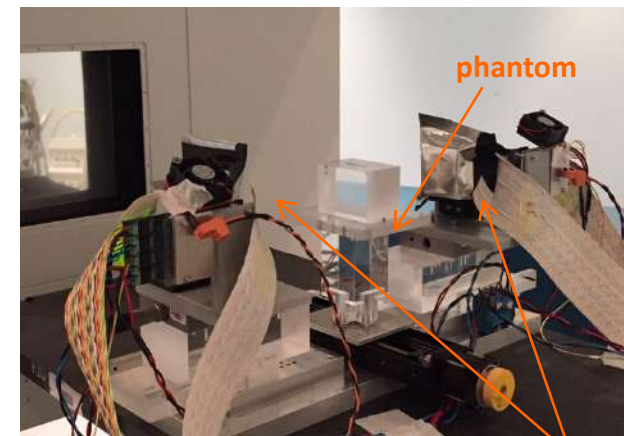
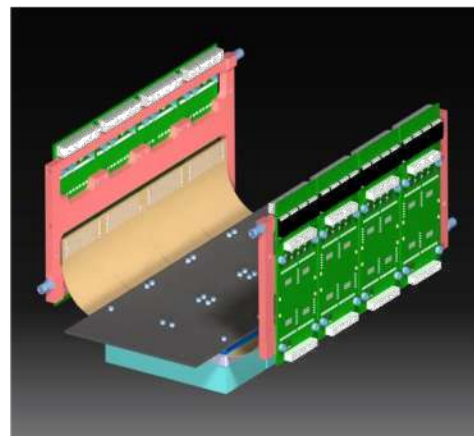
## Main features

- coincidence window = 2 ns
- CTR (Ge68) = 1.2 ns FWHM
- Avg energy resolution = 13 MeV
- image reconstruction method: MLEM



256 LFS pixel crystals (3x3x20mm<sup>3</sup>) coupled one to one to MPPCs (Multi Pixel Photon Counters, SiPMs).

Solid model  
Of the PET  
head



Demonstrator  
1 vs 1 module

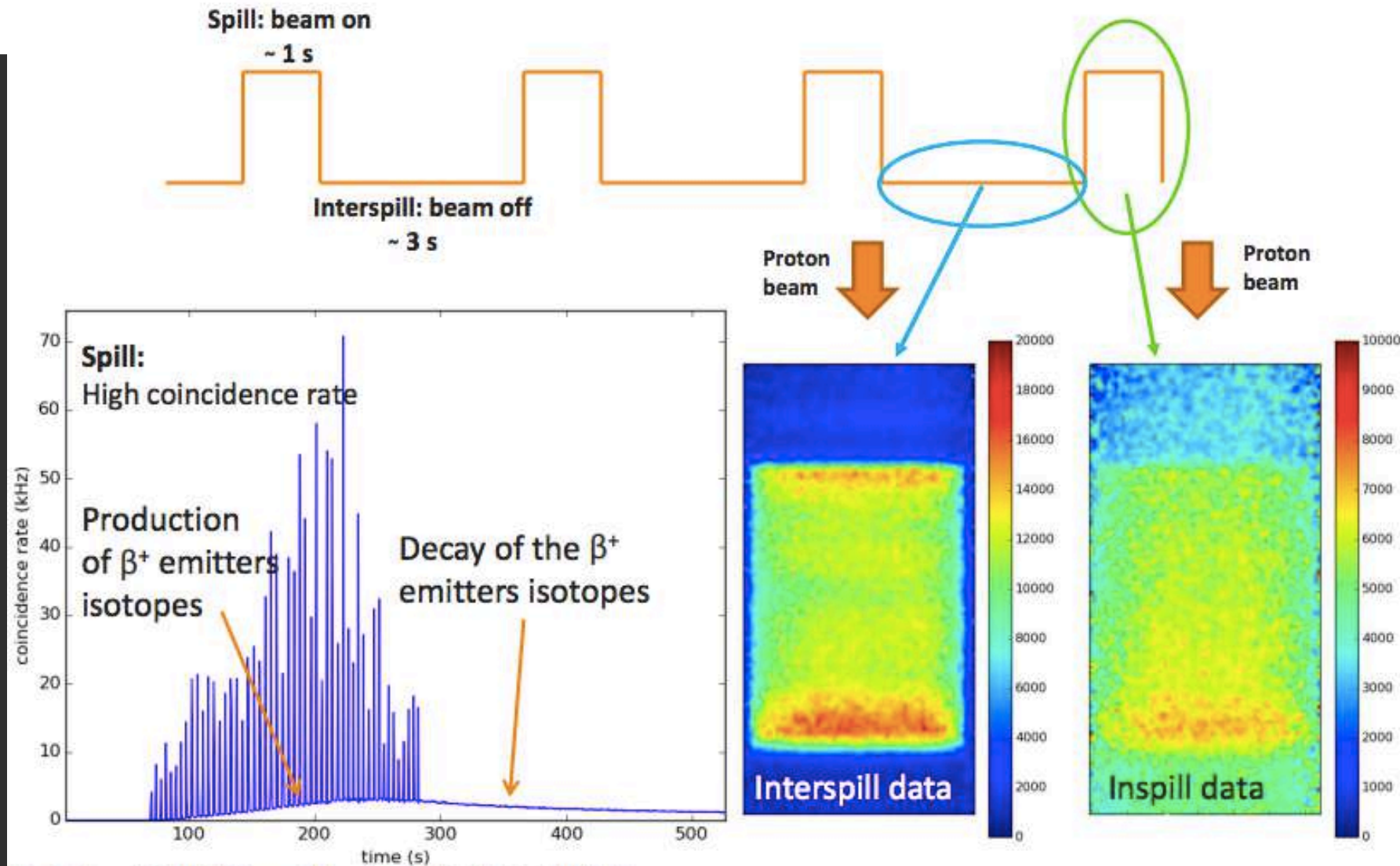
G.M. Bisogni et al.:Journal of Medical Imaging4 (Dec. 2016), p. 011005.

Work partly supported by European Union: EndoTOFPET-US project and Marie Curie Early Initial Training Network Fellowship (PITN-GA-2011-289355-PicoSEC-MCNet).

PET modules

**Inside**

# INSIDE: in-beam PET



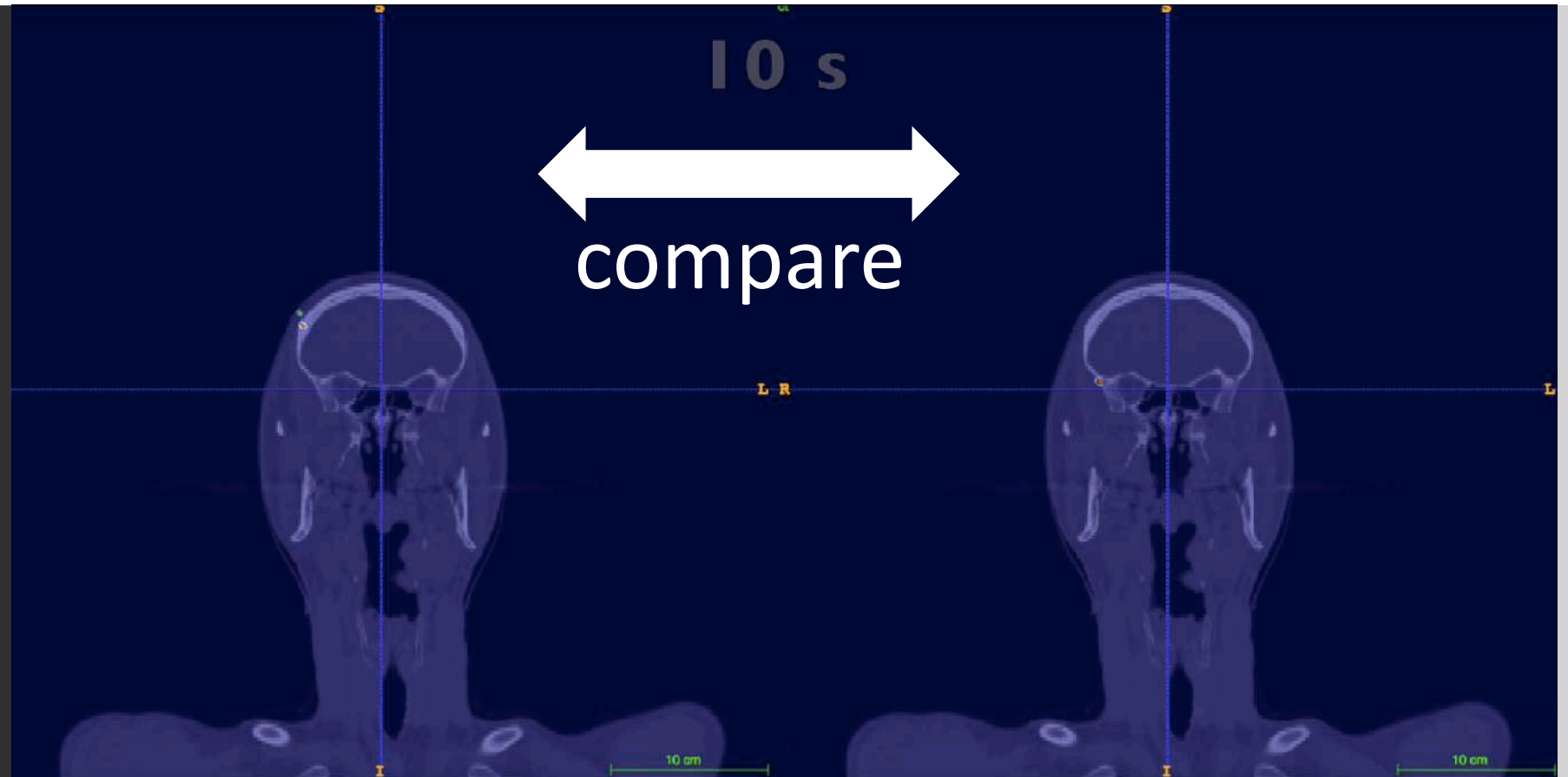
Courtesy of M.G. Bisogni,  
SIF, Italy, 2019

# INSIDE: in-beam PET

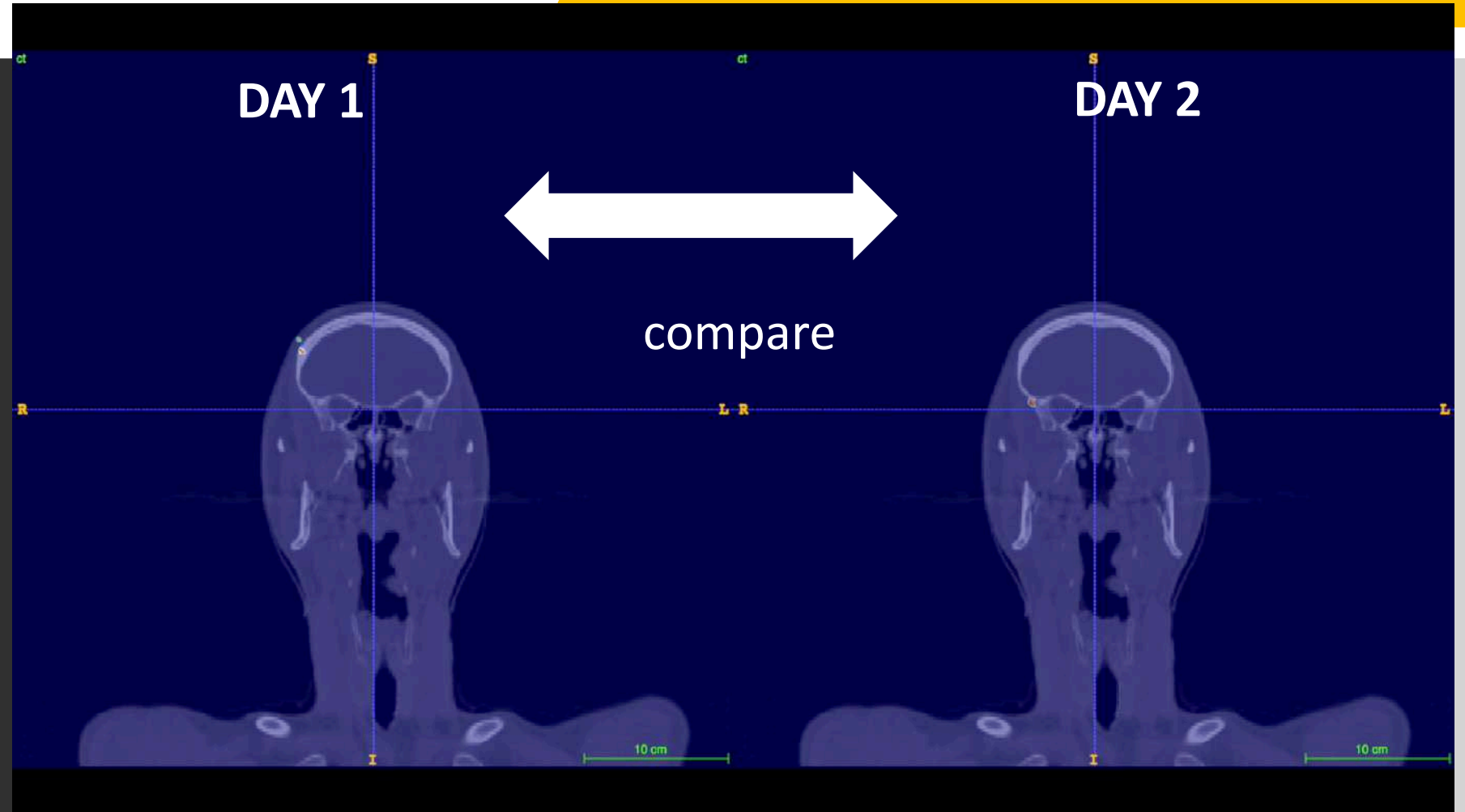
V. Ferrero et al., "Online proton therapy monitoring: clinical test of a Silicon-photodetector-based in-beam PET"  
Scientific Reports, (2018) 8:4100

E. Fiorina et al,  
Front. Phys. 2021

F. Pennazio et al. :Phys.Med.  
Biol.63 2018



# INSIDE: in-beam PET



V. Ferrero et al., "Online proton therapy monitoring: clinical test of a Silicon-photodetector-based in-beam PET"  
Scientific Reports, (2018) 8:4100

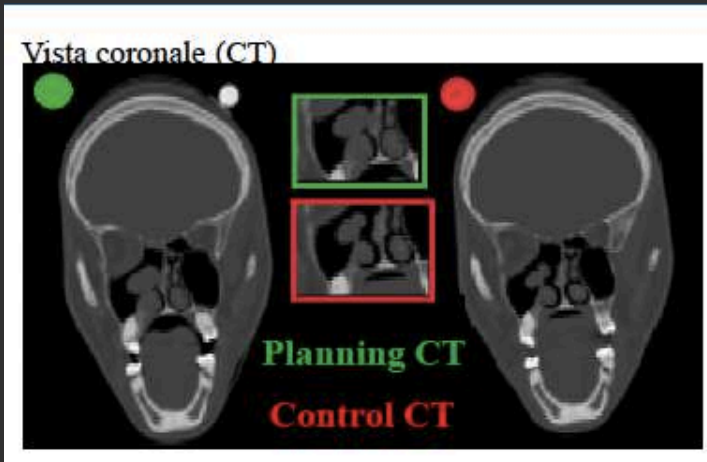
E. Fiorina et al,  
Front. Phys. 2021

F. Pennazio et al. :Phys.Med.  
Biol.63 2018

# INSIDE: in-beam PET

Work in progress...

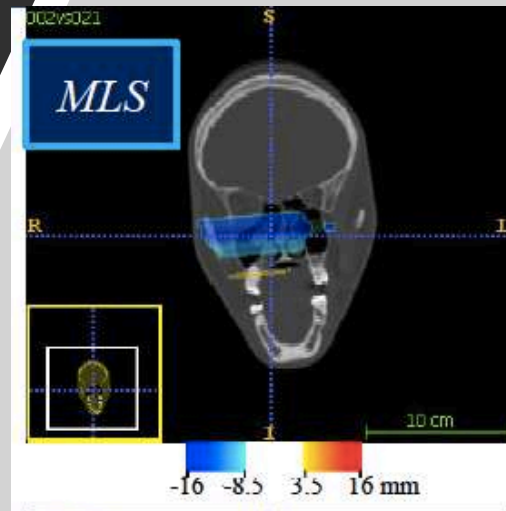
- ACC (adrenocortical carcinoma) patient part of clinical trial
- Thesis work (M. Mogliorni)
- In-beam PET data for various fractions



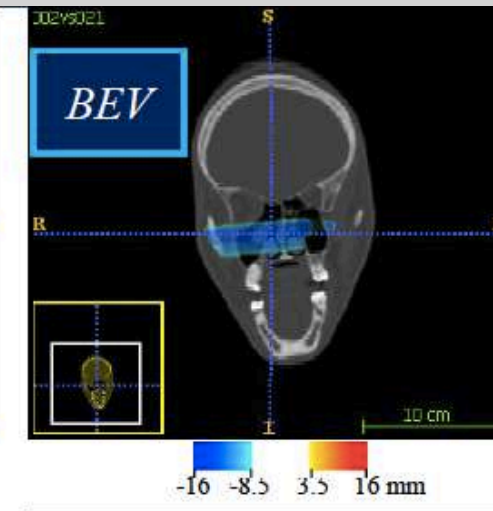
Different range identification methods compared for patient subject to small anatomical changes



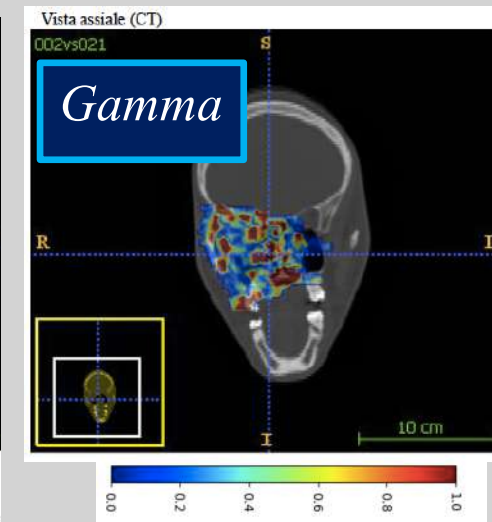
Fraction 2 versus 21



Fraction 2 versus 21



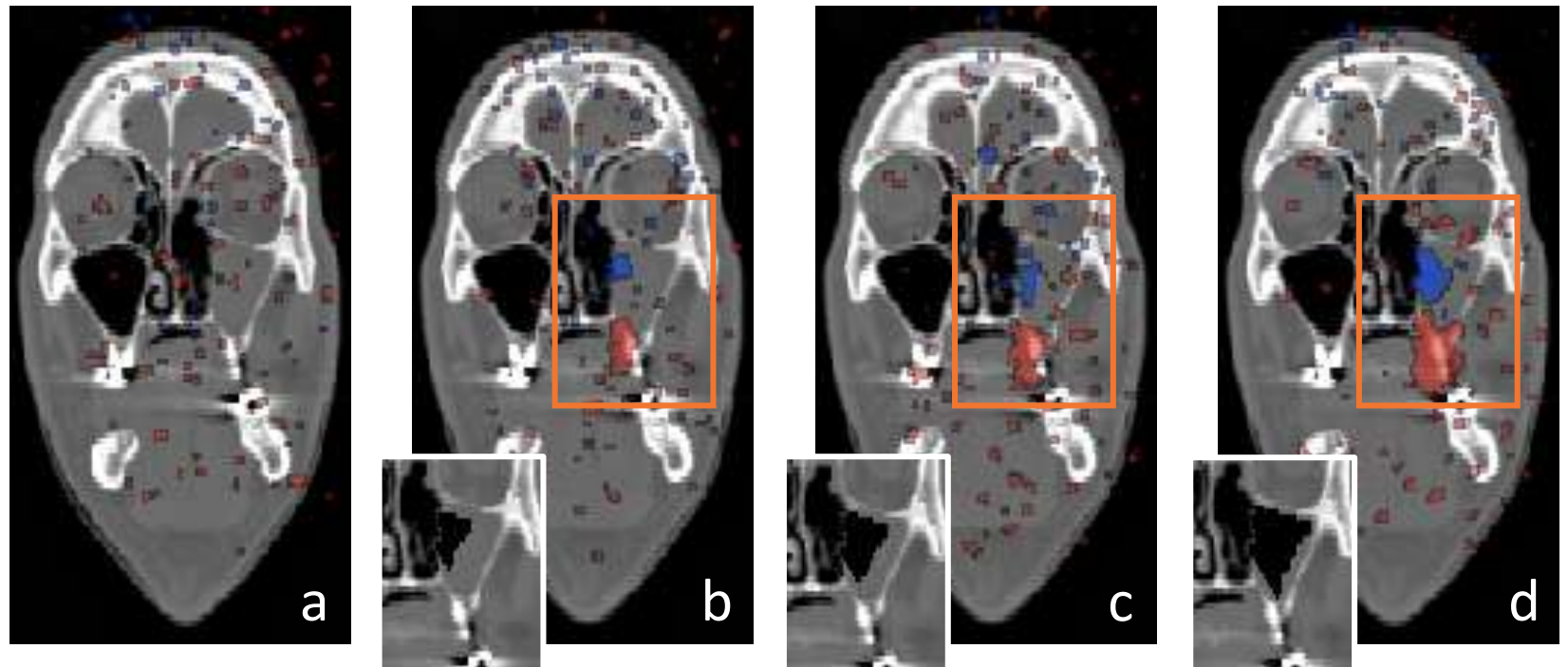
Fraction 2 versus 21



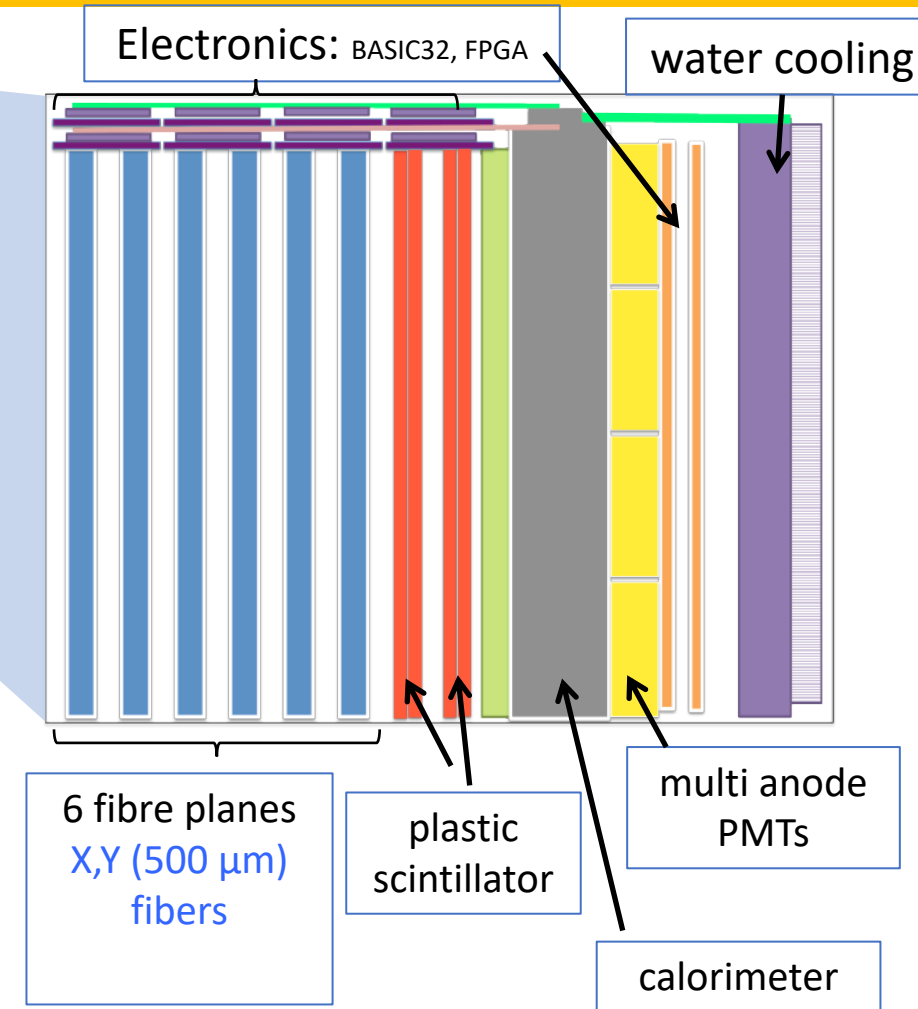
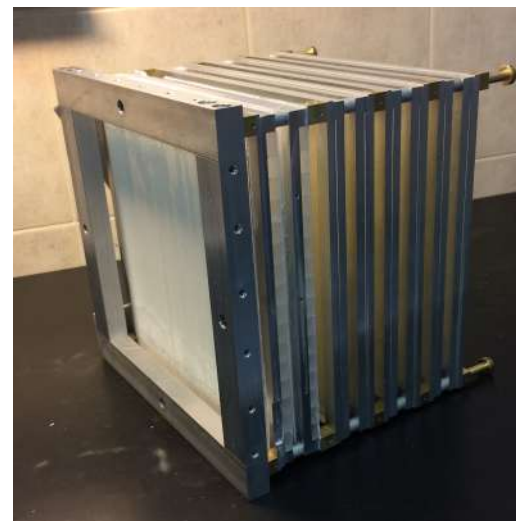
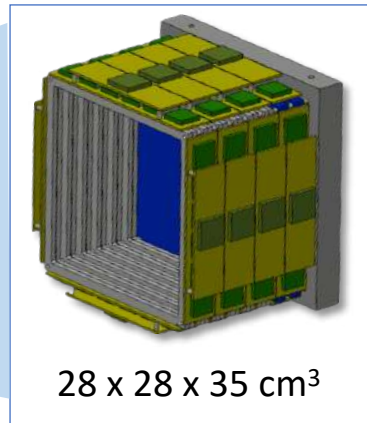
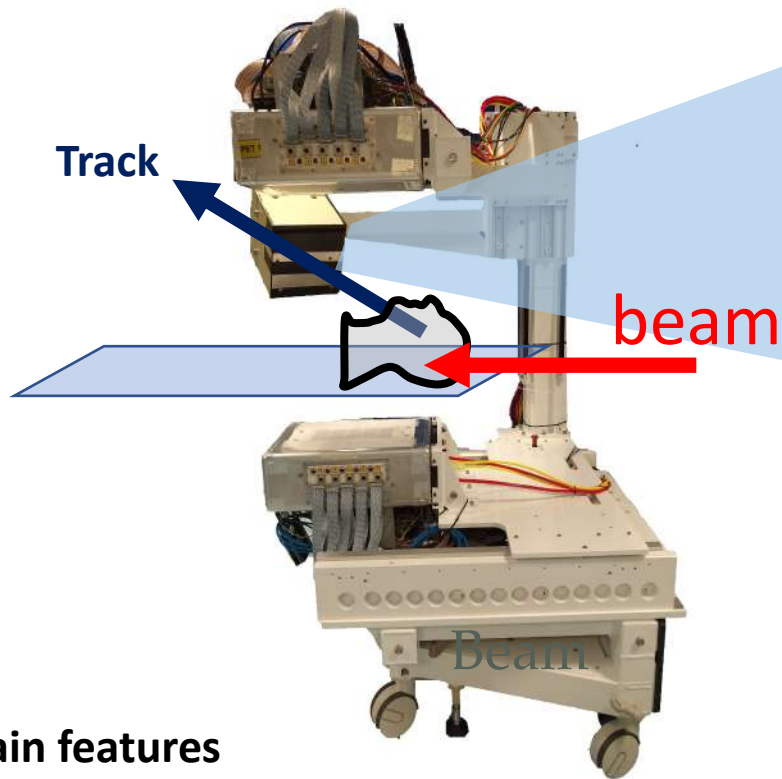
# INSIDE: in-beam PET

- New analysis methods are being developed...
- Voxel-Based Morphometry approach
- Monte Carlo study: voxel-wise two-tailed statistical tests of the simulated PET images
- Can locate changes with respect to expectations

A.C.Kraan, A.Berti, A. Retico, et al, accepted in Medical Physics



# INSIDE: particle tracker

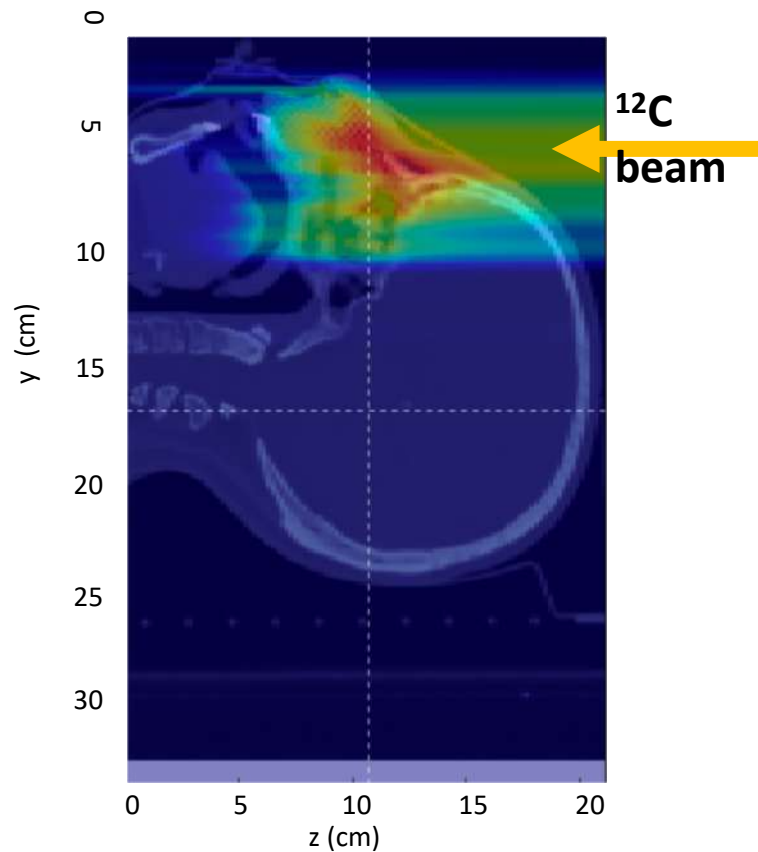


## Main features

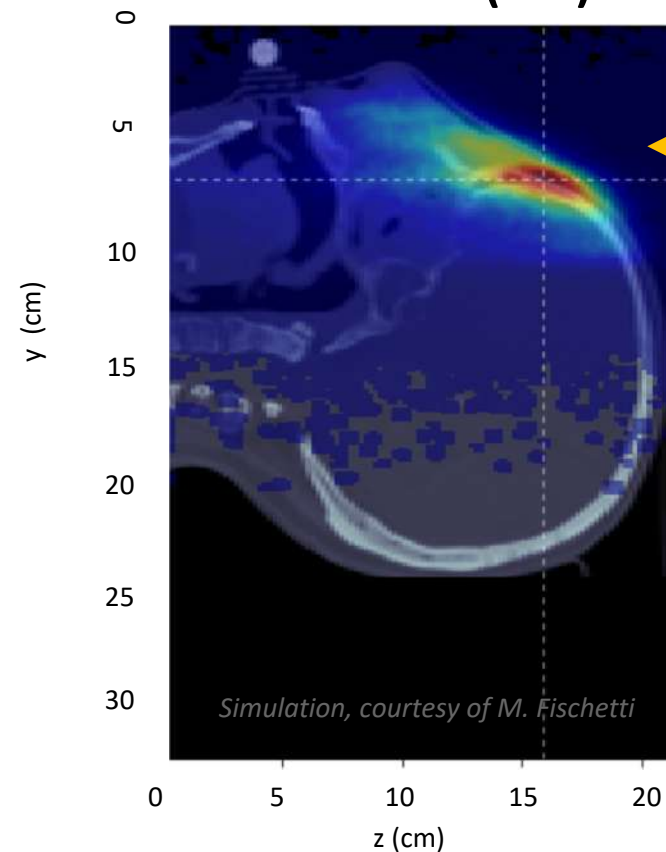
- Synchronization with Dose Delivery System signal (carbon only!)
- Image reconstruction method: backtracking with Point Of Closest Approach

# INSIDE: particle tracker

**Dose**



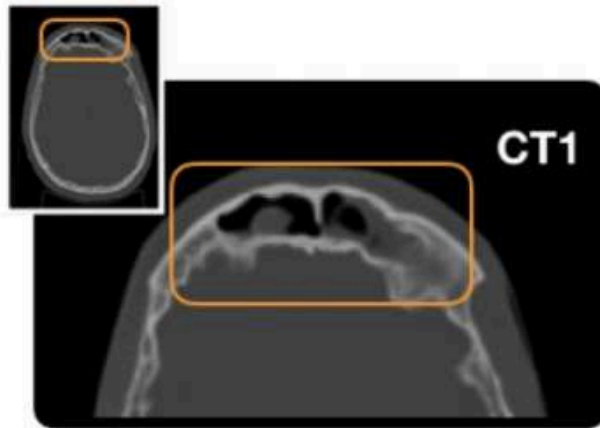
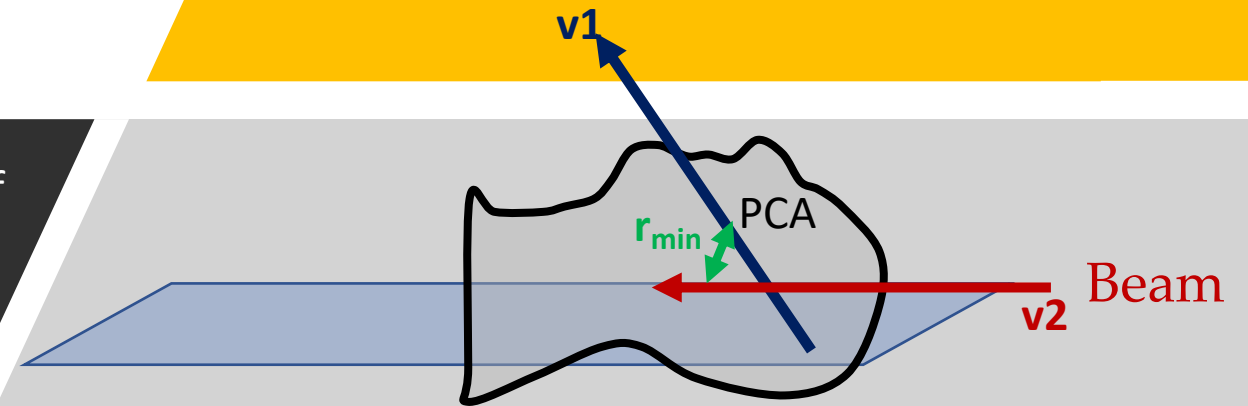
**Fragment emission distribution (MC)**



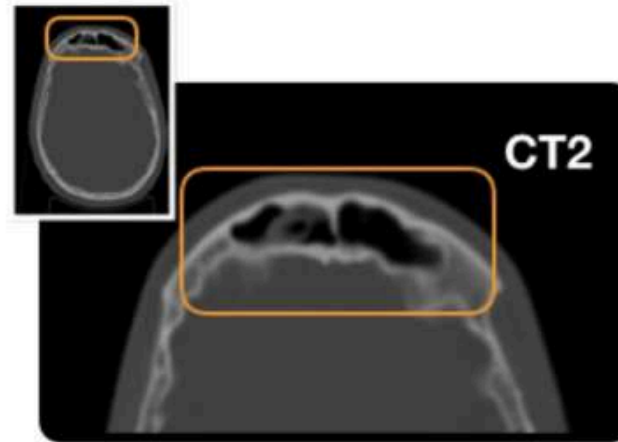
M. Fischietti et. a., Inter-fractional monitoring of  $^{12}\text{C}$  ions treatments: results from a clinical trial at the CNAO facility, Scientific Reports 10, 20735 (2020)

# INSIDE: particle tracker

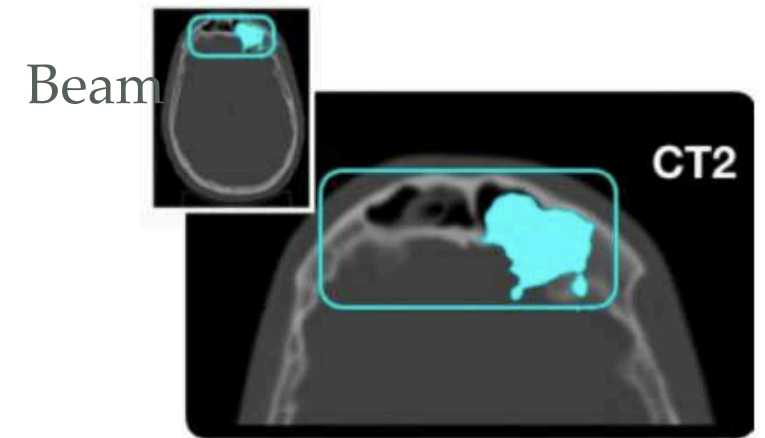
Production points of the fragments obtained as Points of Closest Approach (PCA) of the reconstructed track with the nominal incoming beam direction



(a)



(b)



(c)

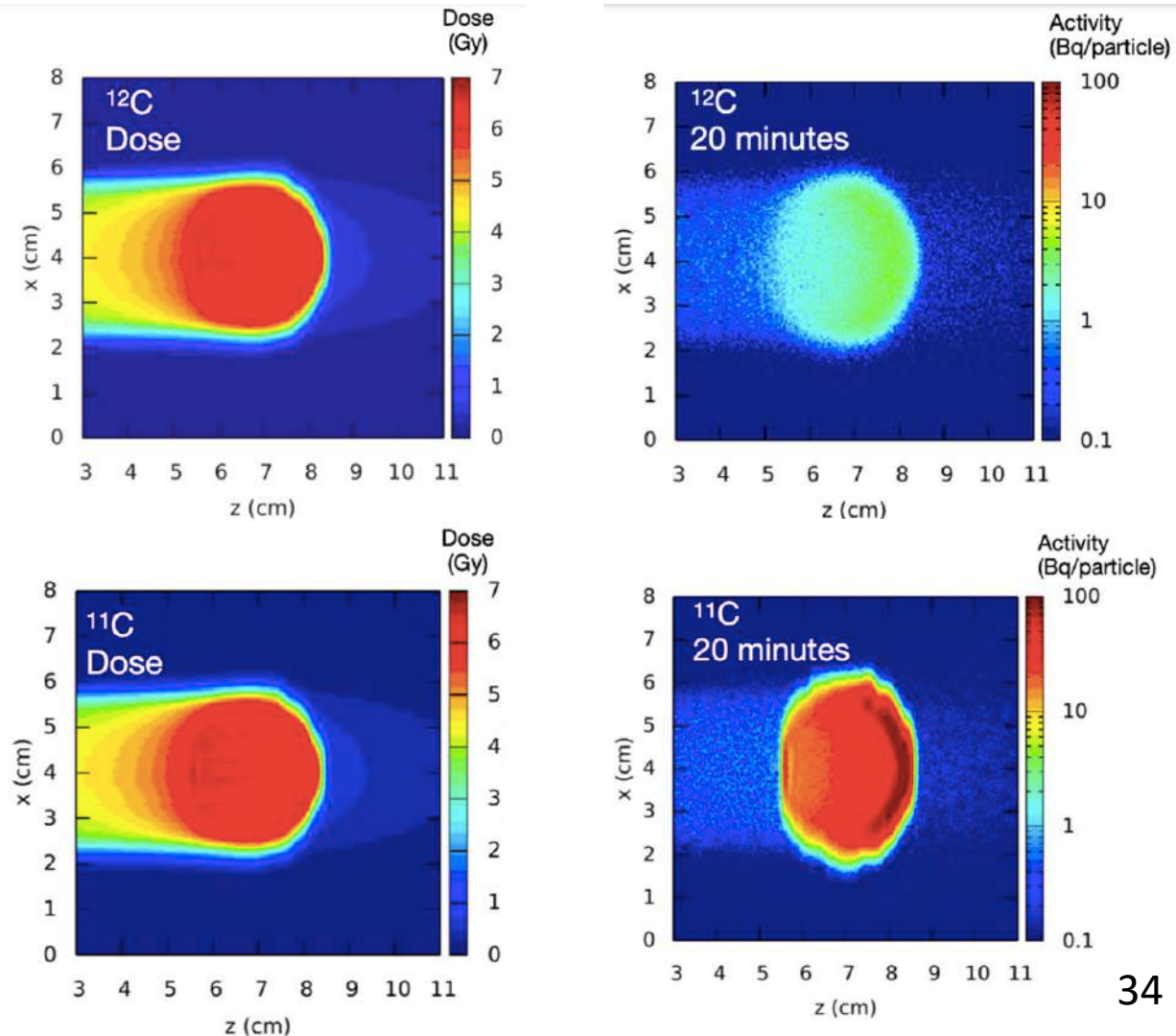
M. Fischietti et. a., Inter-fractional monitoring of  $^{12}\text{C}$  ions treatments: results from a clinical trial at the CNAO facility, Scientific Reports 10, 20735 (2020)

(a) of CT1 , (b) CT2 (c) CT2 with superimposed the distribution of the PCAs belonging to the SPBs that have a **p-value below 0.02** when testing the consistency between the first monitored fraction and the last one.

# BARB project

(Biomedical Applications of Radioactive ion Beams)

- FAIR project Darmstadt
- Carbon beams: not much beta+ activity generated...
- But higher intensity for the PET signal can be obtained using beta+ -radioactive beams directly for treatment
- Difficult (low intensity)
- Intensity upgrade of the SIS-18 synchrotron and improved isotopic separation at FAIR (Facility for Antiproton and Ion Research at GSI) → now possible to reach radioactive ion beams with sufficient intensity to treat a tumor in small animals
- $^{11}\text{C}$  and  $^{15}\text{O}$  beams

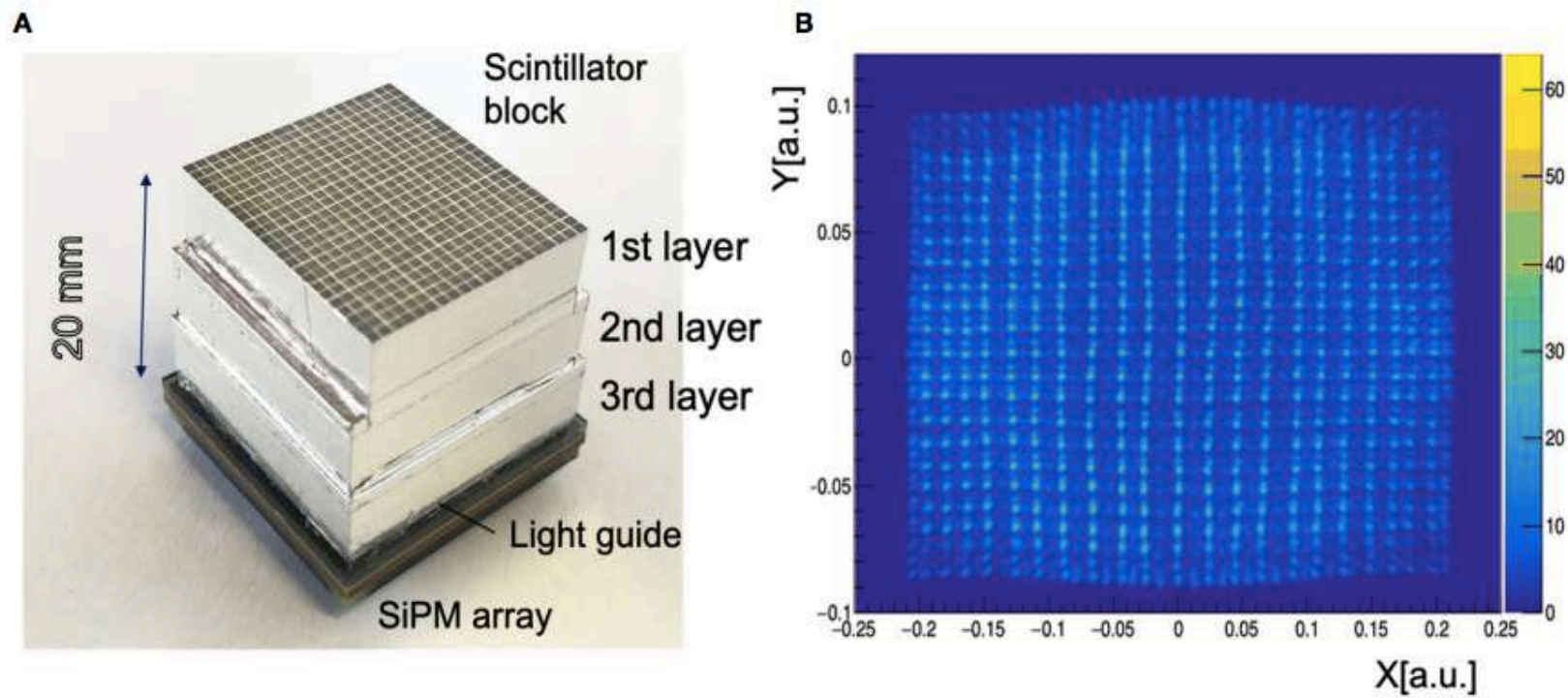


# BARB project

(Biomedical Applications of Radioactive ion Beams)

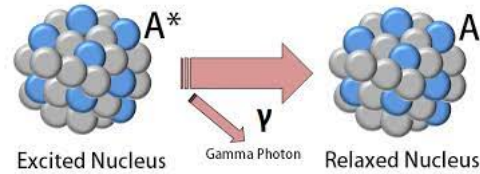
- Small-animal PET scanner in development

Daria Boscolo et al., Front Oncol 2021. eCollection Radioactive Beams for Image-Guided Particle Therapy: The BARB Experiment at GSI



**FIGURE 6** | LMU hybrid  $\gamma$ -PET detector **(A)** A 3-layer PET detector developed at LMU Munich in collaboration with NIRS-QST. The PET detector consists of a 3-layer scintillator block, a light guide and an  $8 \times 8$  SiPM array. **(B)** A flood map of the 3-layer PET detector exposed to a  $^{22}\text{Na}$  radioactive point source.

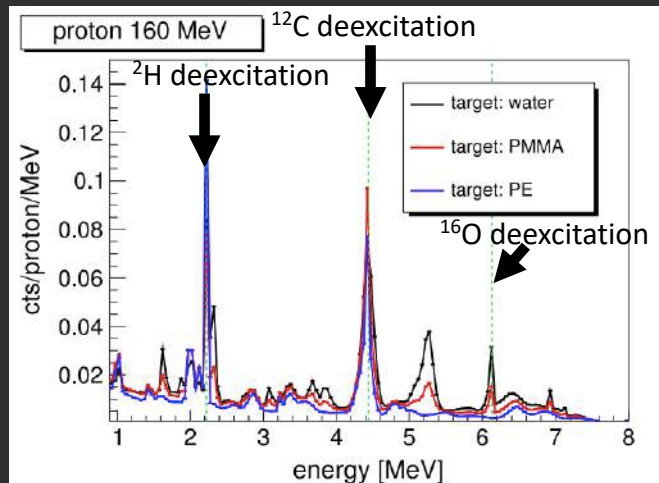
# Prompt gamma



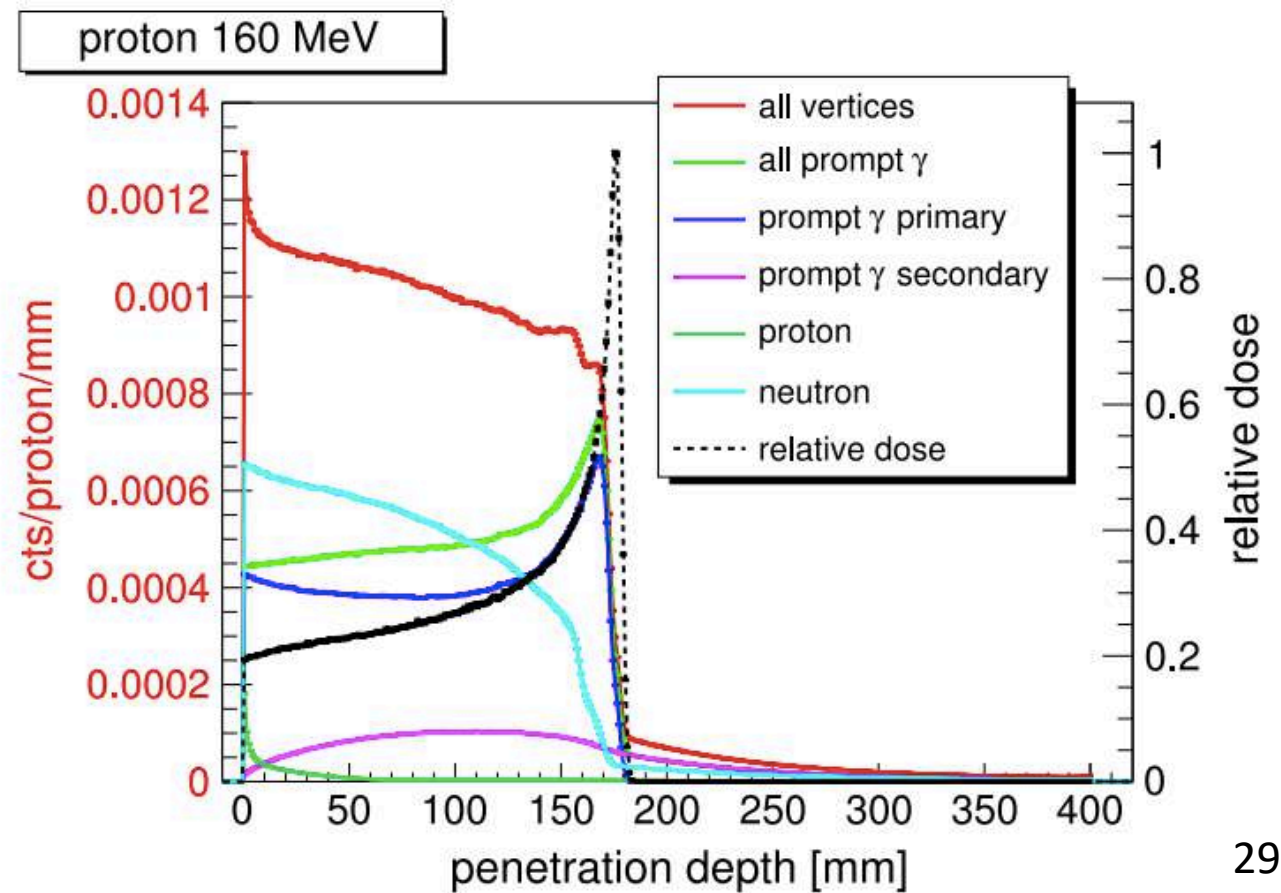
First proposed in 2003 by Stichelbaut and Jongen, first prototype by Min in 2006

Difficulties with detecting prompt gamma's:

- Broad energy spectrum (up to 10 MeV!!)
- Large background (neutrons)
- High instantaneous count rates
- Compatibility constraints with patient irradiation.



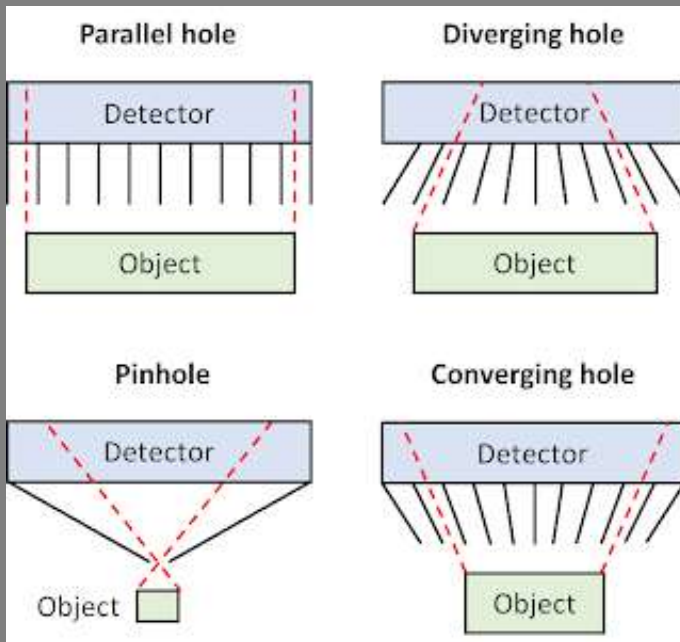
J.Krimmer, D.Dauvergne, J.M.Létang, É.Testa, Prompt-gamma monitoring in hadrontherapy: A review, NIM A 878, 2018, pp 58-73



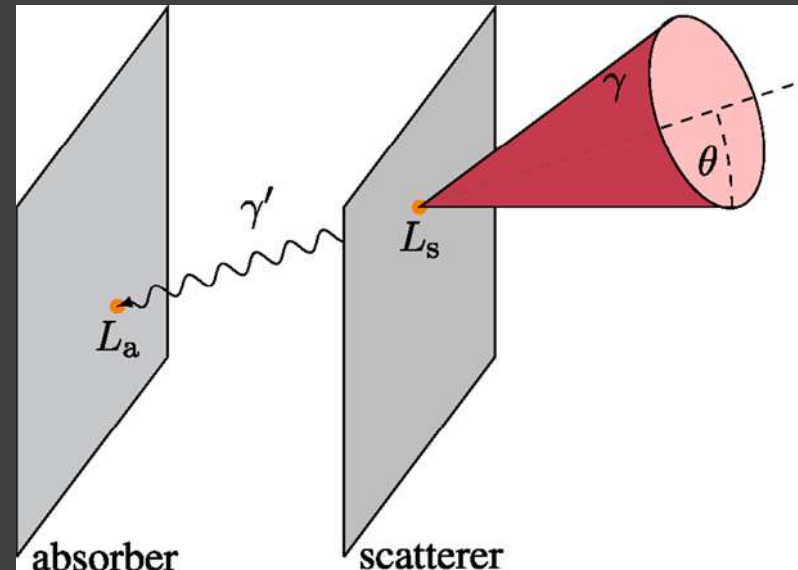
# Prompt gamma

See for information and references: J.Krimmer, D.Dauvergne, J.M.Létang, É.Testa, Prompt-gamma monitoring in hadrontherapy: A review, NIM A 878, 2018, pp 58-73

## Collimated gamma cameras

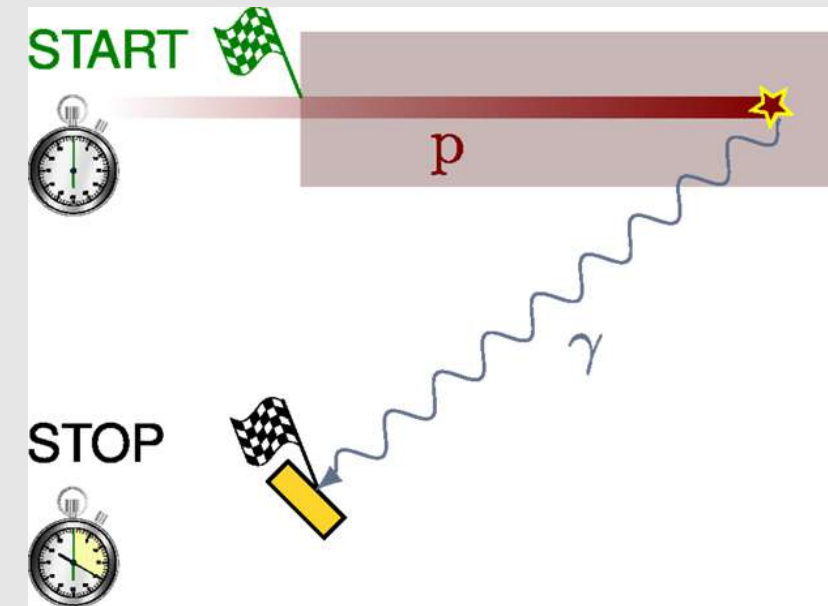


## Compton cameras



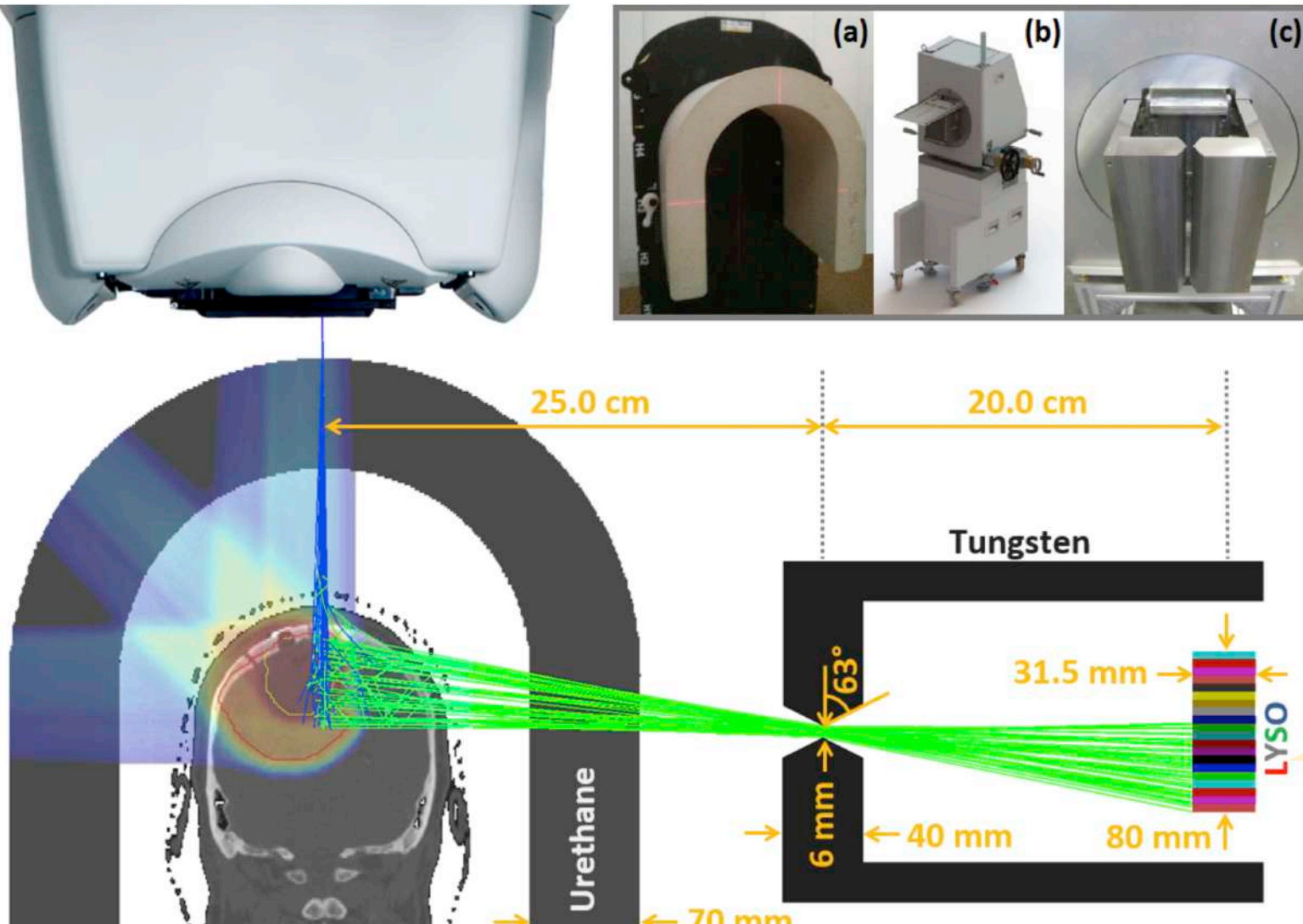
From F. Hueso-González, Front. Oncol., 2016

## Others, for instance timing



From F. Hueso-González, Front. Oncol., 2016

# Prompt gamma



Example of clinical applications of **collimated gamma** imaging systems:

IBA-USA collaboration: report 2 mm precision to detect shift

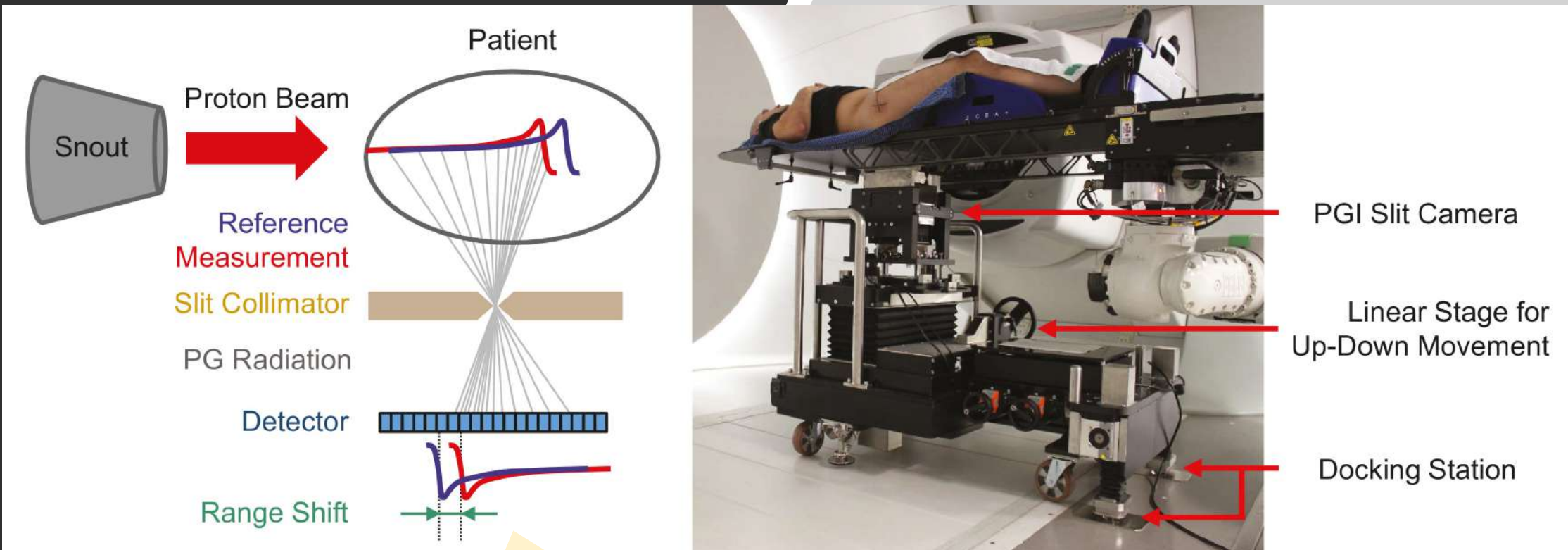
Yunhe Xie et al , Prompt Gamma Imaging for In Vivo Range Verification of Pencil Beam Scanning Proton Therapy Int. J. Rad. Onc. Bio. Phys. 99, 1, 2017, pp 210-218

Reversed projection of the prompt gamma depth emission profile is produced on the crystals

# Prompt gamma

Other example of clinical applications of **collimated gamma** imaging systems:

J. Berthold et al, Int. J. Rad. Onc. Bio. Phys. 111, 4, **15 November 2021**, Pages 1033-1043



Reversed projection

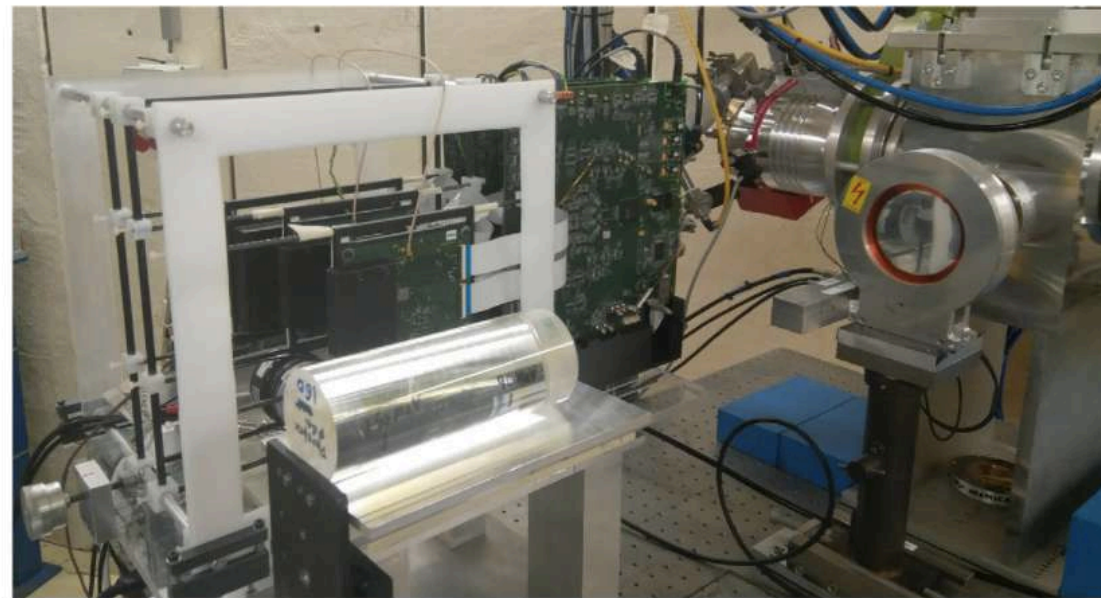
validation uncertainty of this second-generation PGI slit camera is about 1 mm ( $2\sigma$ )

# Prompt gamma

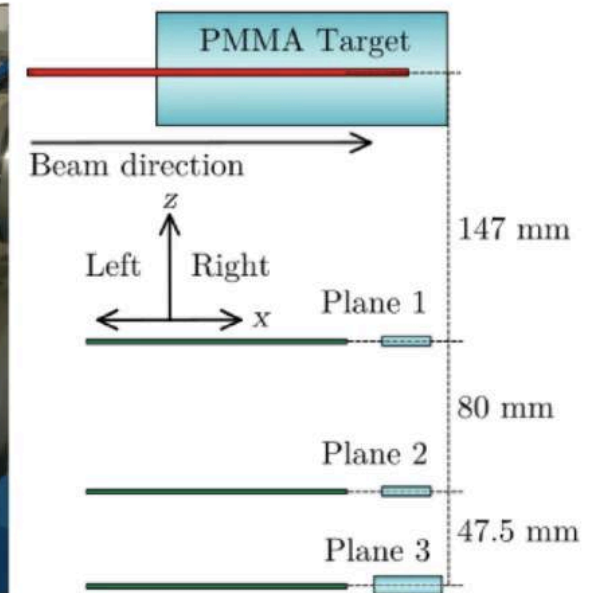
MACACO II Compton camera multi-layer Compton camera based on LaBr<sub>3</sub> scintillator crystals and SiPMs

E. Muñoz et al, Nature Scientific Reports 2021

- Allows calculation of the distal fall-off and identification of target displacements of 3 mm.



(a)



(b)

(a) Picture of the experimental set-up showing beam exit, PMMA target and Compton camera. (b) Diagram of relative distances in the experimental set-up.

# Particle therapy

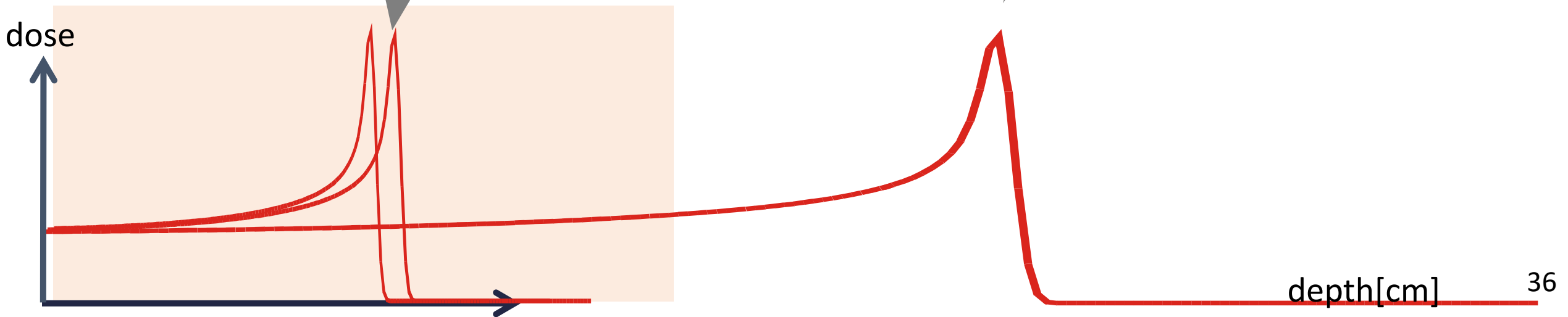
Based on Nuclear Reactions of Hadrons in Tissue

- Off-line & On-line PET
- Prompt gamma's and neutrons
- Prompt charged particles (only for Ions)

Beam stopping inside patient

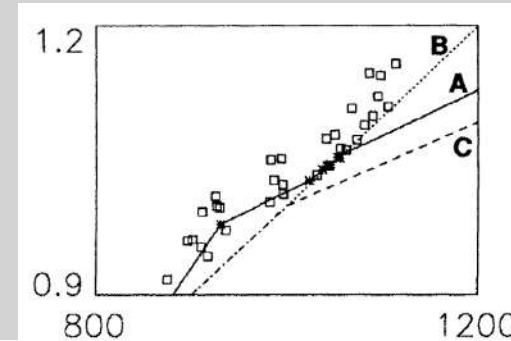
Based on X-ray CT- analogous: pCT (only for Protons)

Beam going through

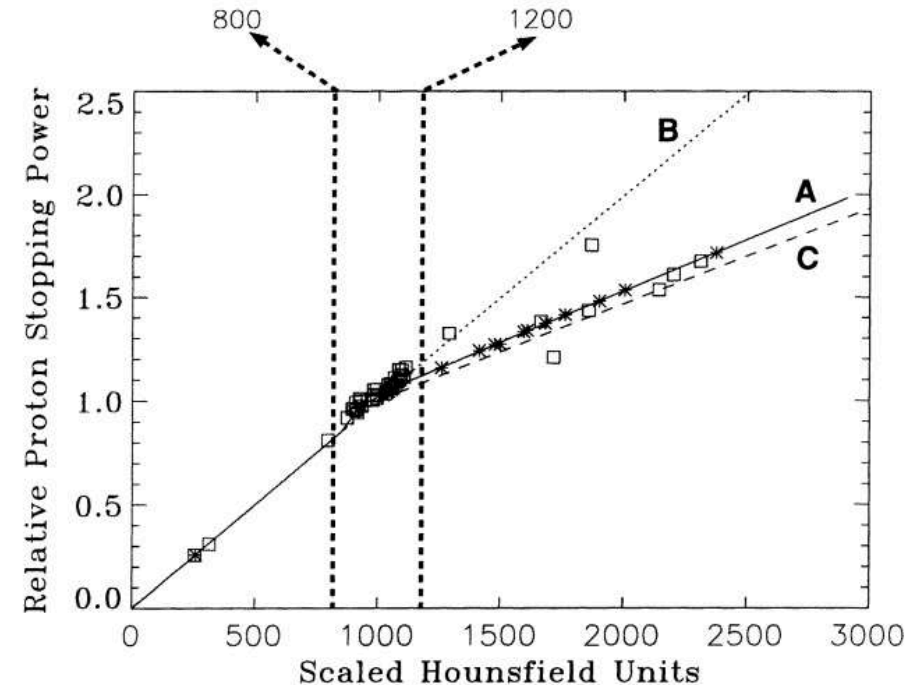


# Proton CT: motivation

- Proton range depends on stopping power along the proton path.
  - Currently stopping power determined by CT scan (x-Ray based)
  - CT Hounsfield units have to be converted to particle stopping power... based on calibration curves → uncertainties!
- 
- Can be improved...
    - Dual energy CT
    - Proton CT (see next)
    - ...



Schneider. Pedroni 1996  
41(1):111-24.

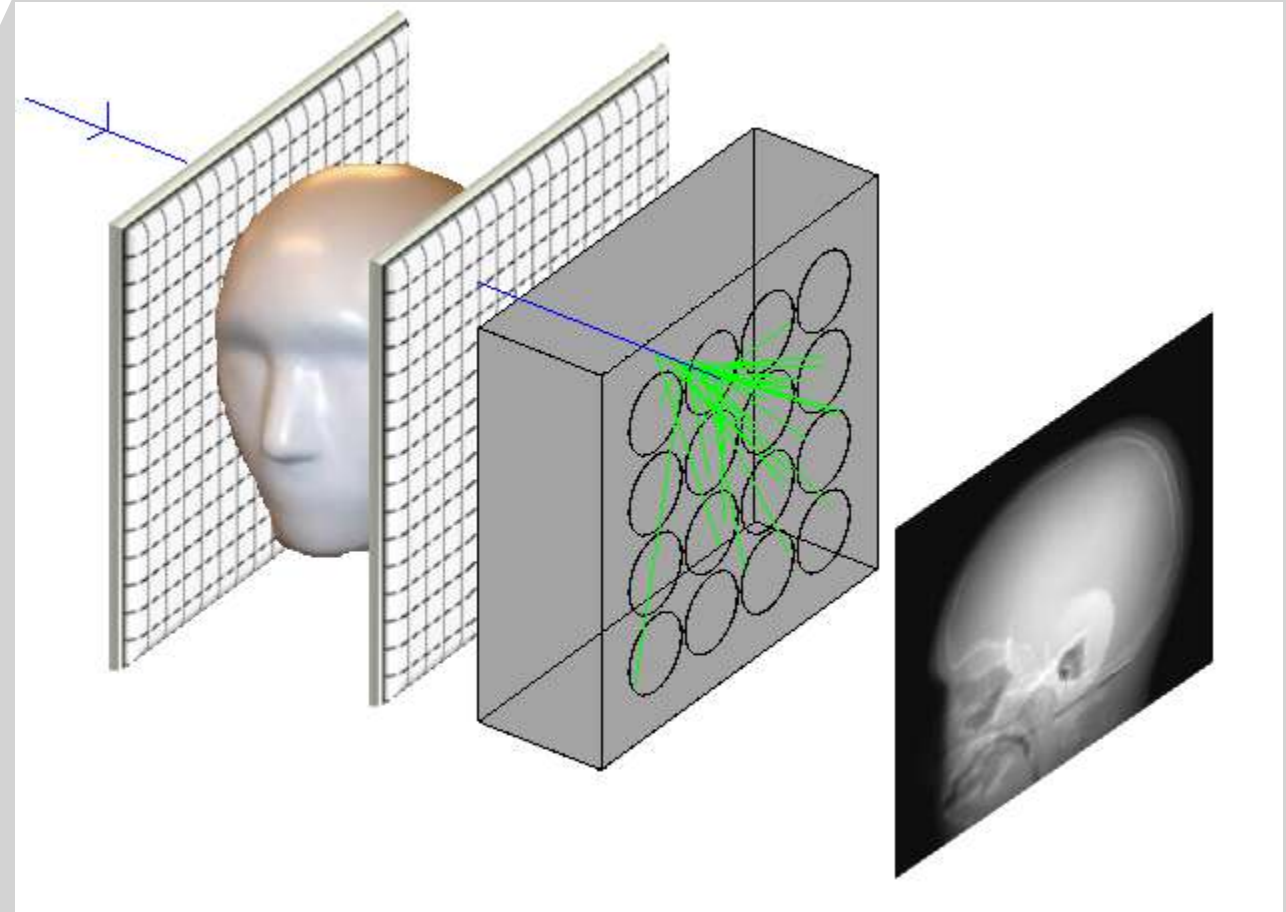


# Proton CT

Using same particles (i.e. protons) but with higher energy, so that they pass through the target:

- Measure the position with a tracker before and after the target
- Measure the residual energy with an energy detector (calorimeter) downstream
- Make one planar view to obtain a proton-radiography (pR)
  - Source of image contrast is the energy loss of the transmitted protons (the integrated stopping powers of protons in the patient).
- Make many projections to obtain a proton-CT (pCT)
- Idea was originally proposed by Allan Cormack in 1963  
( J.Appl. Phys.1963,34, p.2722)

<https://www.niu.edu/crcd/prospective-user/projects/proton-medical-imaging.shtml>



# Proton CT

Many initiatives...and much literature

Robert P Johnson,  
Review of medical radiography and tomography with proton beams  
Rep. Prog. Phys. 81 (2018) 016701 (21pp)

# Conclusions

- Many applications of detectors and instrumentation in particle therapy
- Imaging is used during all stages of particle therapy
- Today discussed a few of the techniques, focusing on techniques used for treatment monitoring

**Many thanks to the organizers of this workshop for the opportunity to give this lecture today!**