

Multiscale phase contrast imaging in biomedical research: the experience at Elettra

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CompactLight Complementary Use and Opportunities

Synchrotron Radiation for Mammography (SYRMA) project: first clinical trial of clinical mammography

- X-ray Mammography (generally with 2 views) is the main examination used for detecting early breast cancer, widely adopted in screening programs
- It is **not enough effective** for dense breasts as lesions have similar X-ray properties of fibrous tissue

Aim : explore the potentials of phase contrast imaging on selected clinical cases

Recruitment criteria: patients whose conventional diagnosis (Rx and US) gave uncertain results.

Modality: Propagation based phase contrast planar imaging (2 projections)

Energy range: 17- 22 keV monochromatic, selected according to the breast thickness and glandularity

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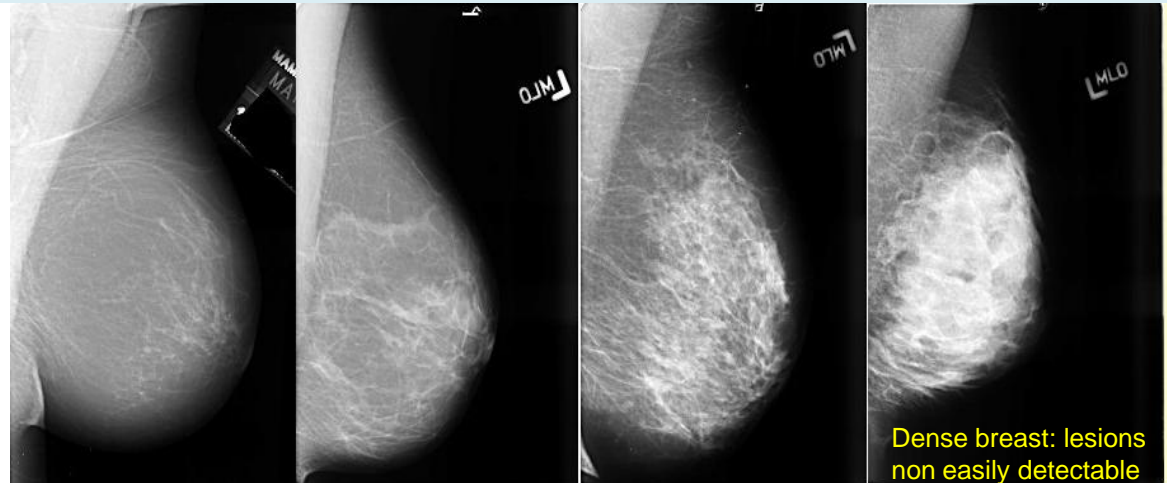


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Radiographs of breasts with increasing density: mainly adipose breast (left) up to high fibro-glandularity breast (right)

C.Dullin, G.Tromba

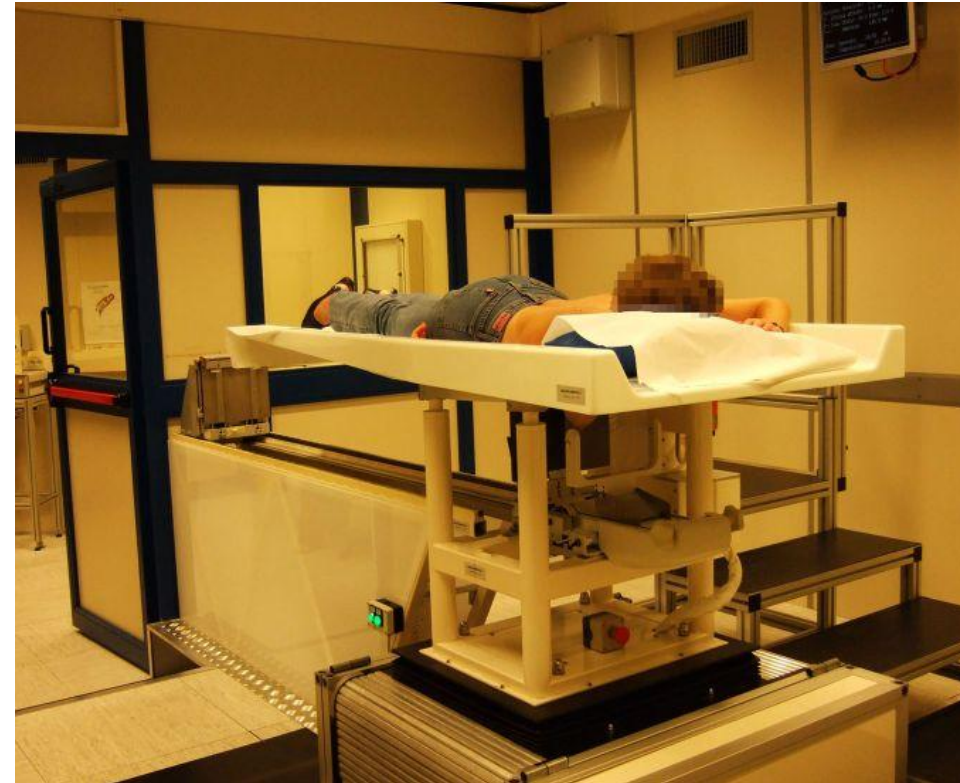
Outcomes of the first protocol

Expert radiologists compared the visibility of different features (such as lesions, calcifications, architectural distortions, focal asymmetries, etc.) in the conventional and SR images.

Exams with SR have:

- higher specificity,
- better agreement with the golden standard (biopsy),
- improved image quality,
- strong reduction of delivered doses.

The patient facility at Elettra



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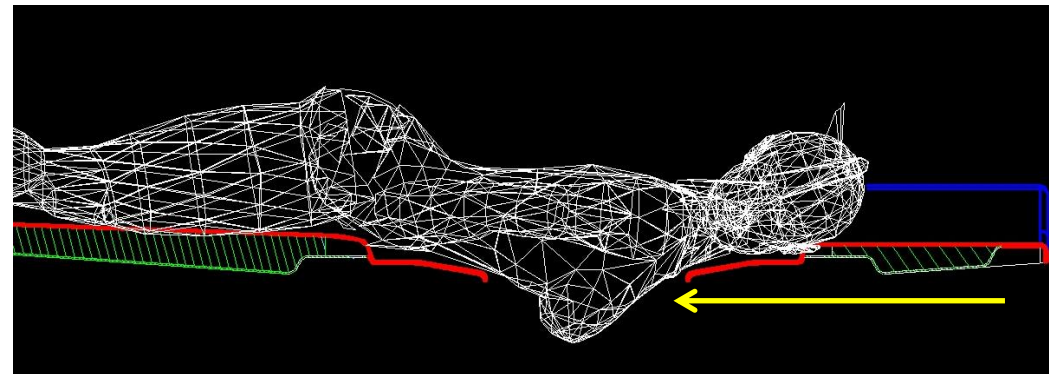
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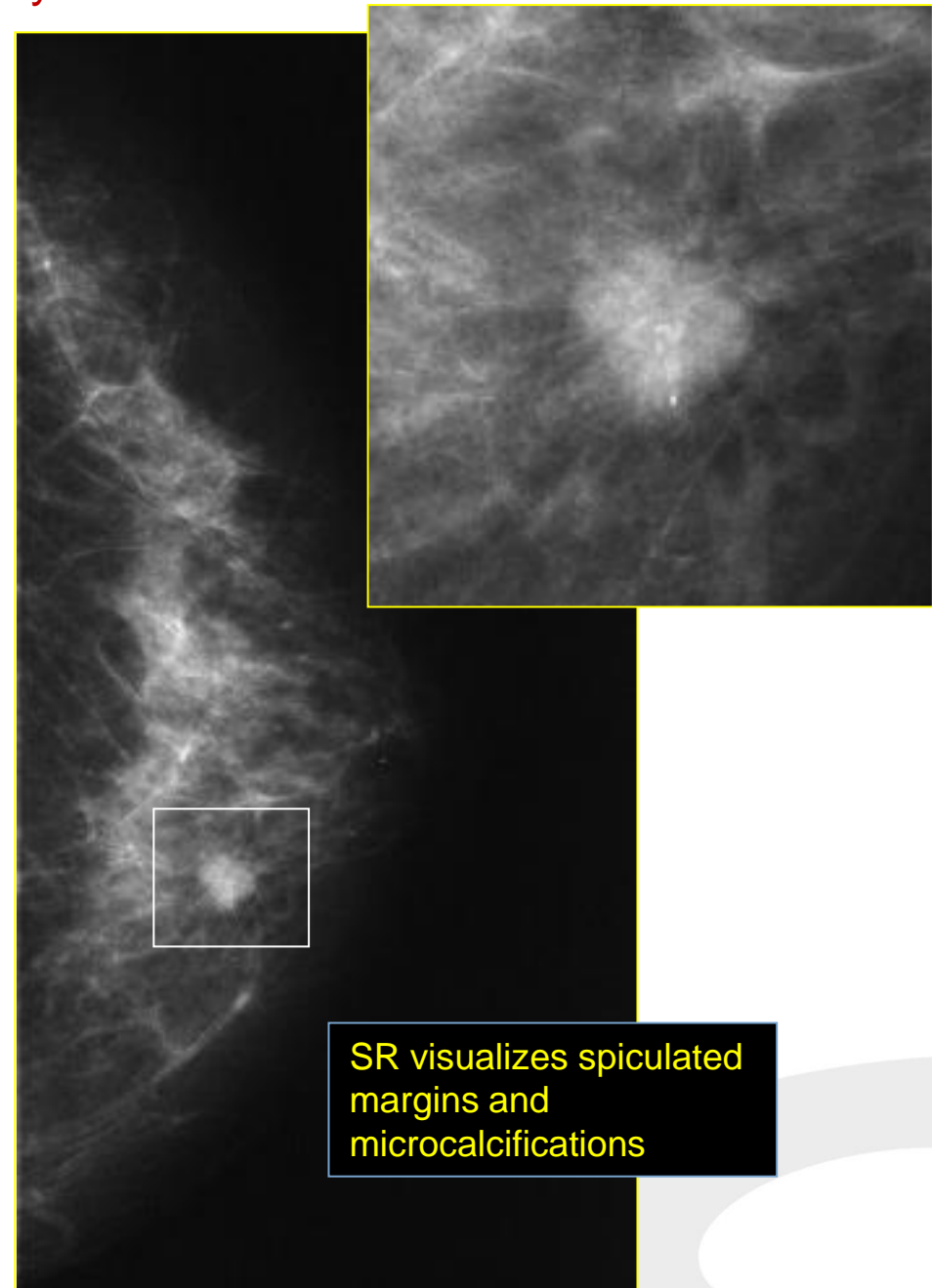
*E.Castelli et al.: Radiology, vol 259 (2011),
R.Longo et al., Phil. Trans. R. Soc. A 372 (2014)*



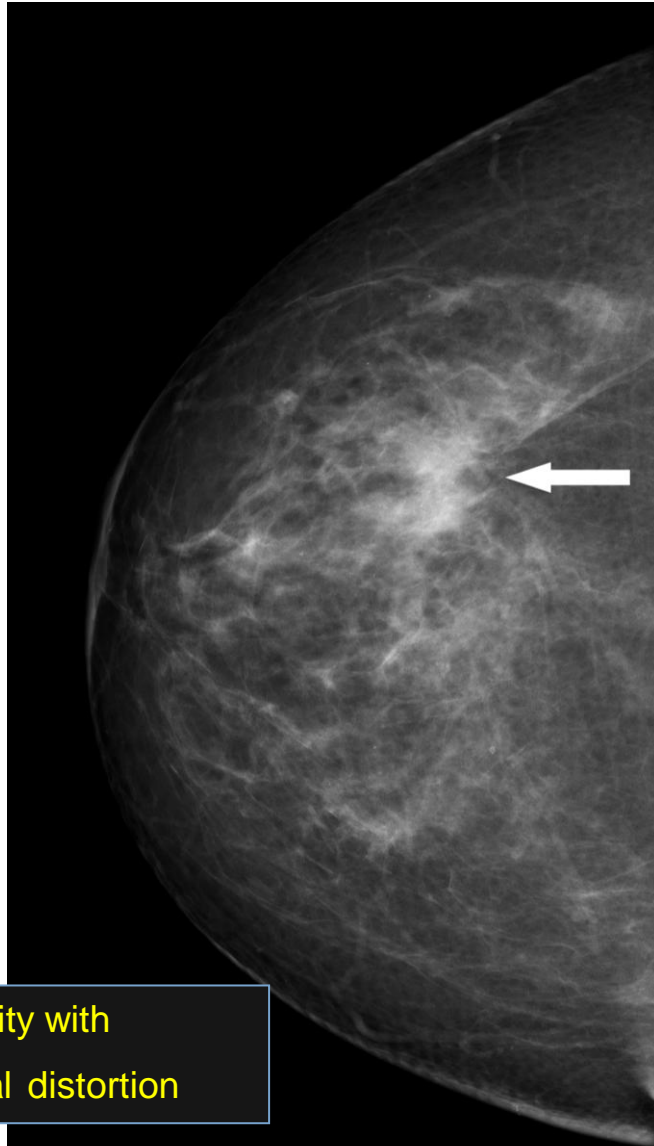
Conventional mammography



Synchrotron Radiation



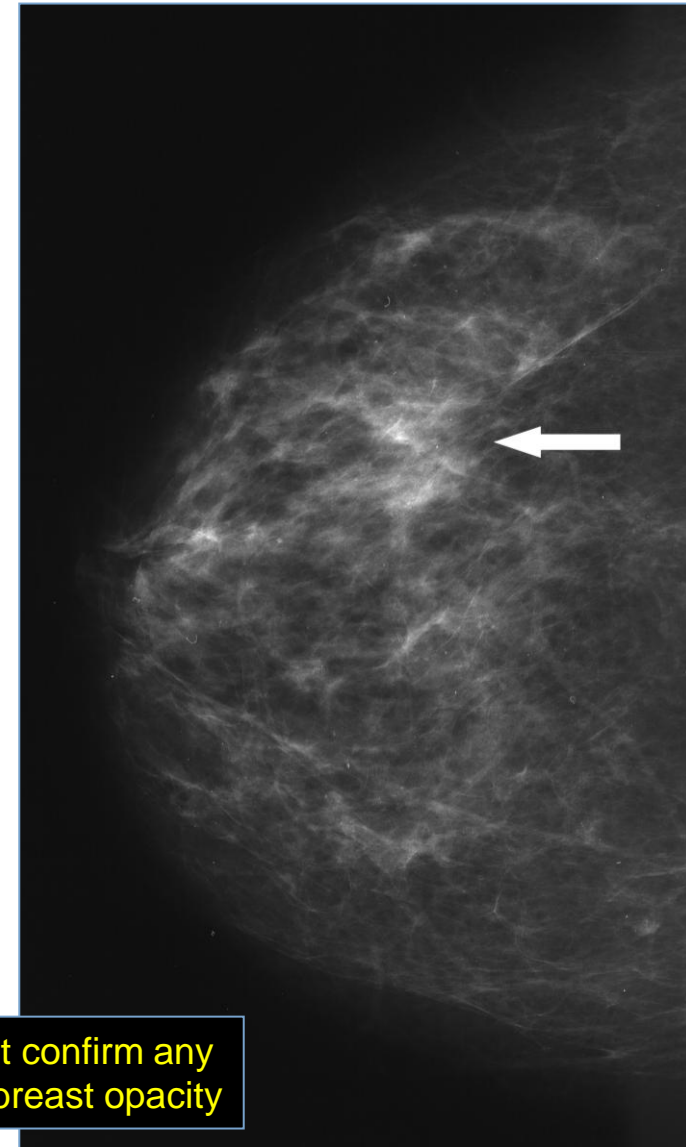
Conventional mammography



Conv: opacity with
architectural distortion

5.9 cm compressed breast
29 kVp Rh/Rh
MGD 1.3 mGy

Synchrotron Radiation



SR does not confirm any
suspicious breast opacity

5.4 cm compressed breast
19.5 keV
MGD 0.8 mGy

Motivations

- Projection X-ray mammography has important limitations in breast cancer detection, particularly in the dense breasts.
- 3D imaging approach implemented in additional breast imaging modalities: breast tomosynthesis, breast ultrasound, breast MRI, all used in combination.
- First dedicated breast CT systems are obtaining promising results.
- Our previous experience: SR phase contrast mammography outperforms conventional mammography

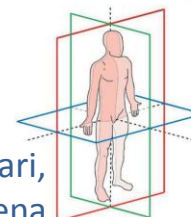
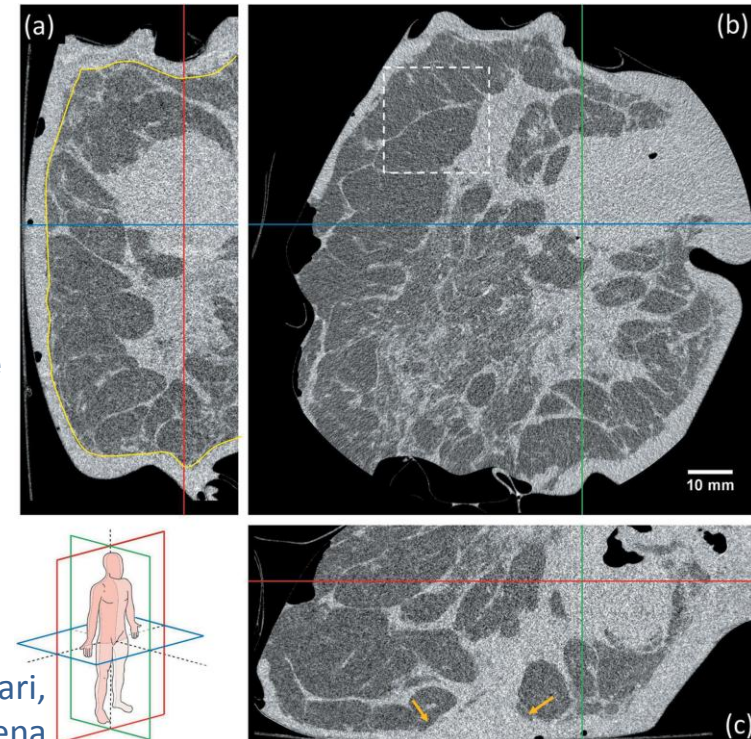


Aims

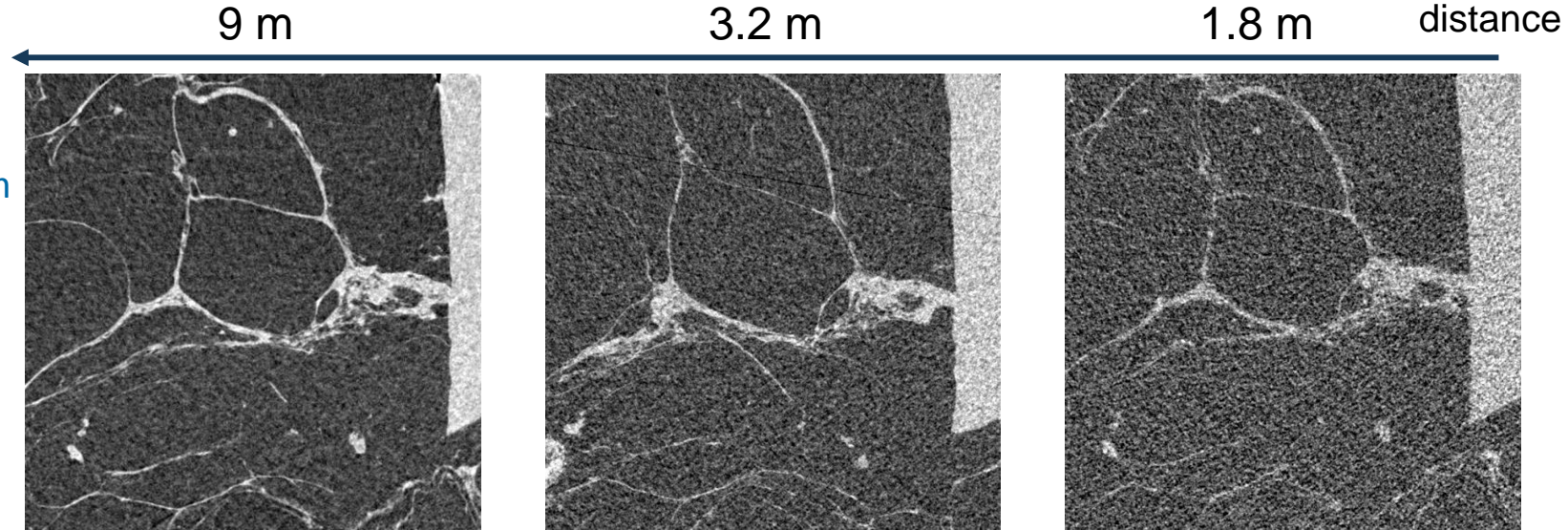
- Evaluate the effectiveness of **low dose phase contrast breast CT** on selected patients
- Reduction of Mean Glandular Dose (MGD) up to 5 or 2 mGy

Methods

- Use of sensitive Single photon counting detector (Pixirad)
- Optimization of X-ray Energy: 26-38 keV
- Application of propagation based phase contrast imaging and phase retrieval algorithms
- Optimization of reconstruction algorithms



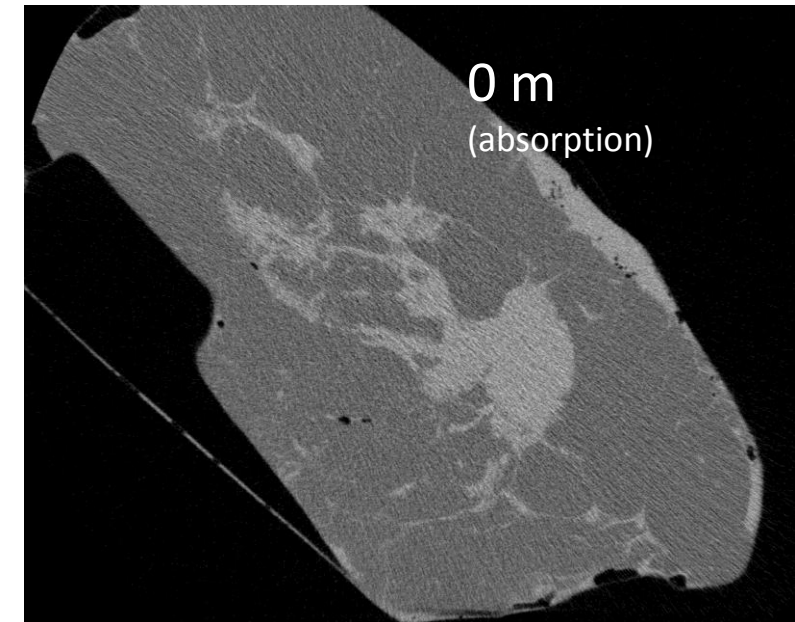
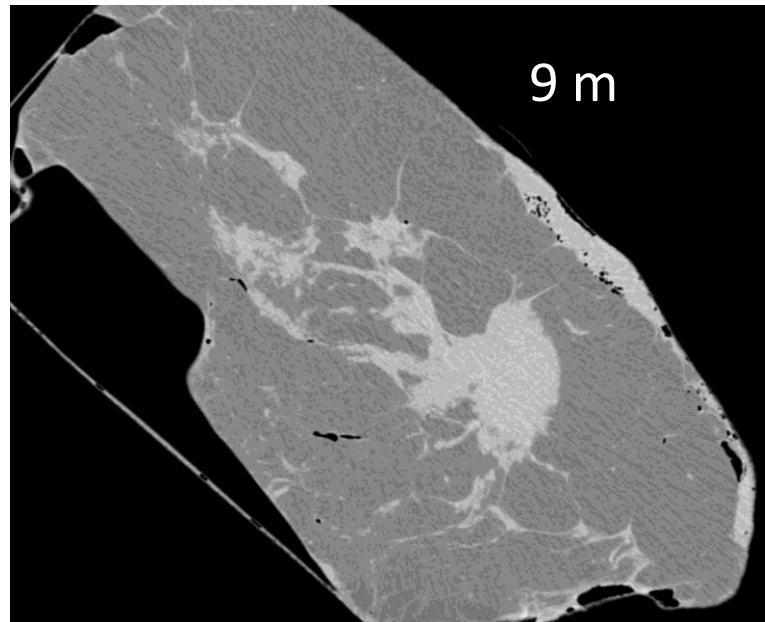
Mastectomy detail
approx. size: 1.5 x 1.5 cm
E = 32 keV
Pixirad detector
MGD ~ 5 mGy



*L.Brombal et al.; Phys.
Med. Biol.63, 2018*

Reconstruction of low dose CT slice with application of phase retrieval algorithm (Paganin 2002)

Mastectomy slice
Size: 7 x 3 cm
E = 32 keV
XCounter detector
MGD ~ 5 mGy

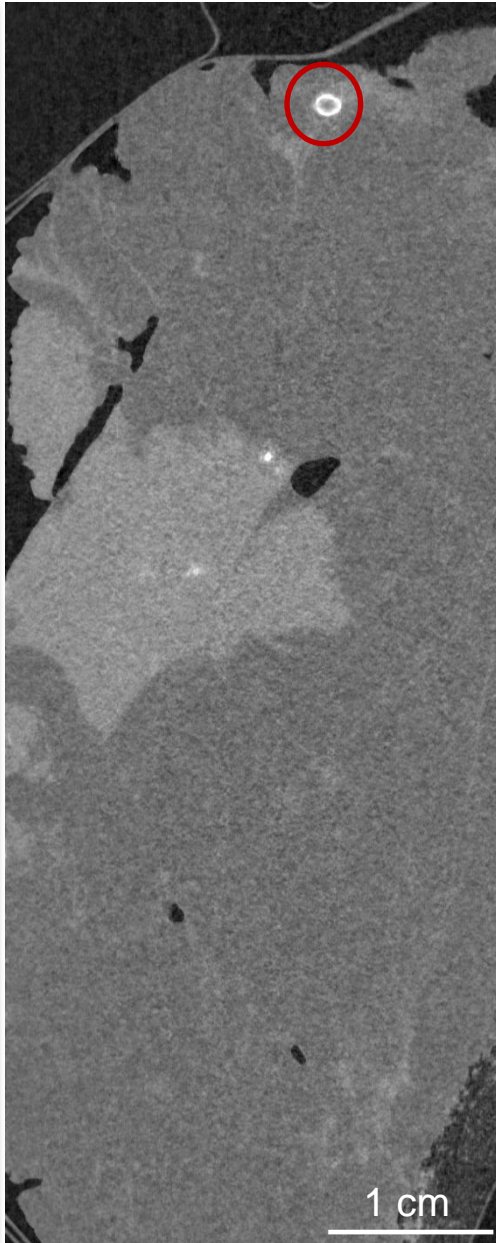


*Baran et al.: Phys. Med.
Biol. 62, 2017*

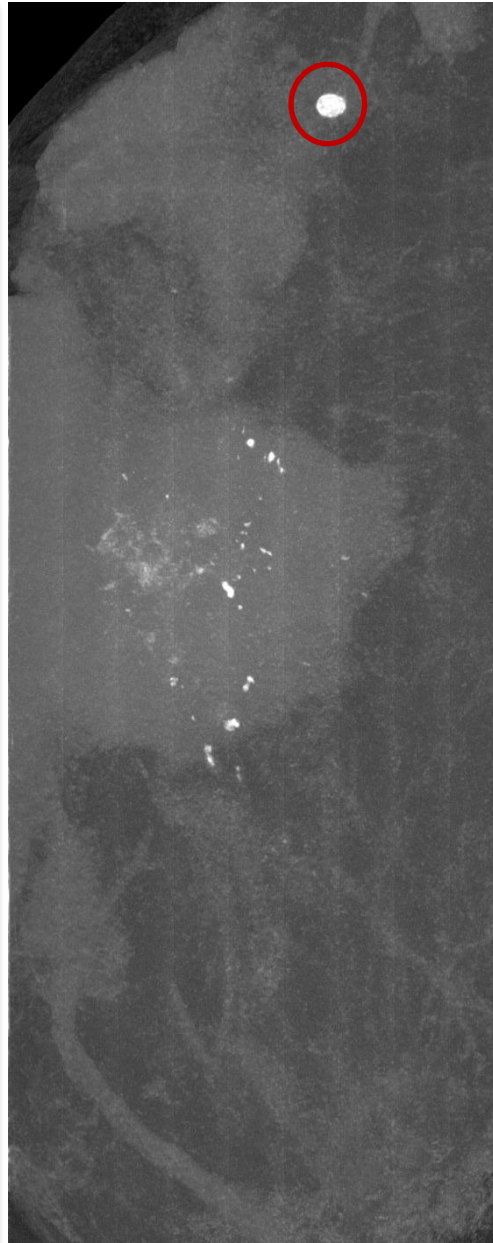
Low dose Breast CT – accurate 3D localization of microcalcifications

Tissue showing a moderate-grade infiltrating ductal carcinoma with a maximum diameter of 2.4 cm

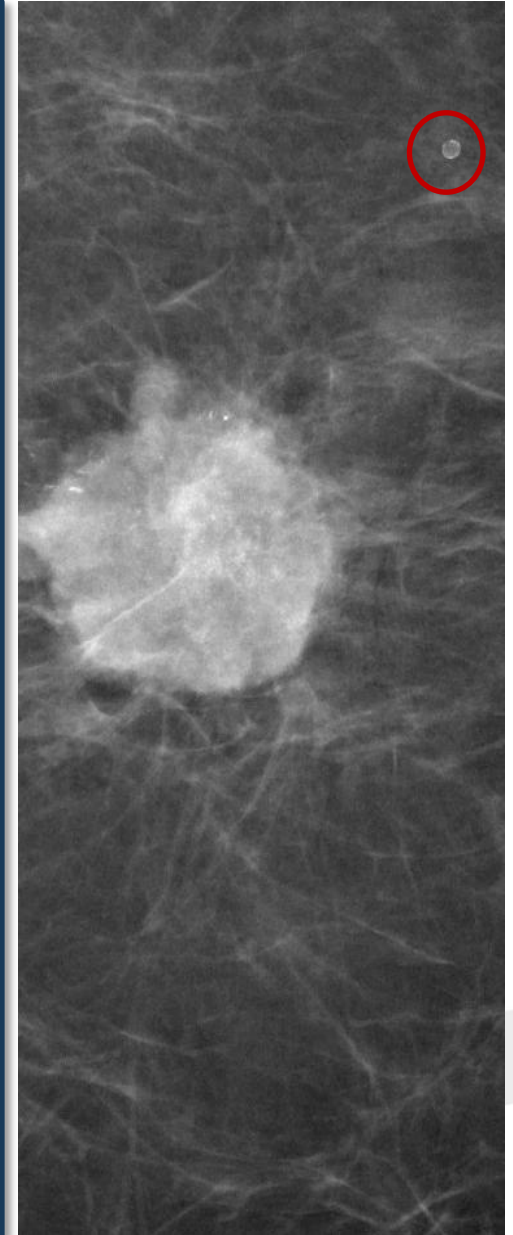
PHASE RETRIEVED BREAST-CT



MAX. INTENSITY PROJECTION



IN-VIVO CLINICAL MAMMOGRAPHY



Comparison between Propagation Based-CT (PB-CT) and Dedicated Breast Cone Beam-CT (CB-CT)

Aim: to compare the diagnostic performance of two techniques for breast 3D imaging.

✓ PB-CT parameters at SYRMEP:

$E = 32\text{--}40\text{ keV}$, prop. distance = 9.3 m, 1800 projections over 180°

Detector used = XCounter photon counting detector (XC-FLITE FX2) with a pixel size of $100\text{ }\mu\text{m}$

Data processing: phase retrieval (Paganin et al., 2002) and CT FBP reconstruction.

Mean Glandular Dose = 5 mGy

✓ CB-CT parameters:

Koning Breast-CT system (x-ray tube with a 0.3 mm focal spot size).

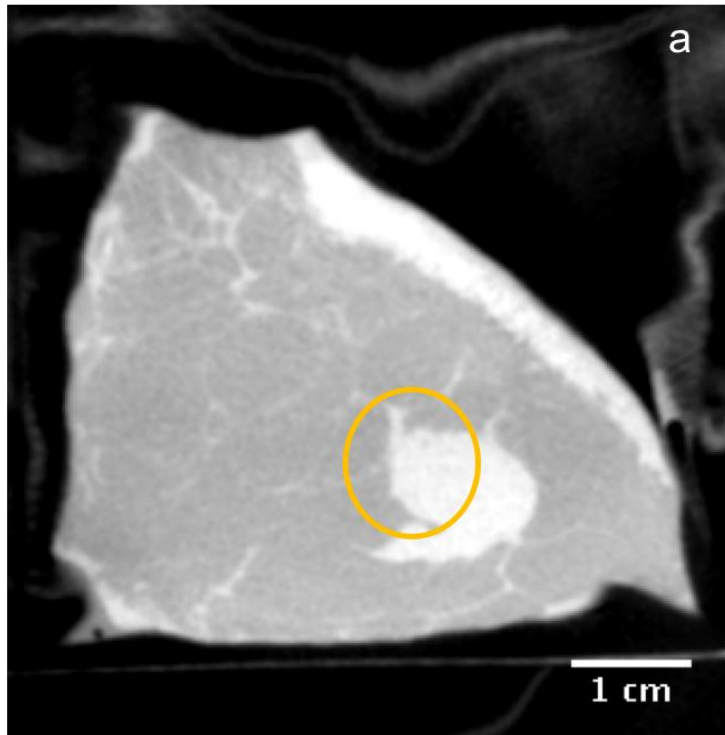
Operation parameters: 49 kVp, 120 mAs, 360° rotation

Detector used: flat panel with a pixel size of $273\text{ }\mu\text{m}$

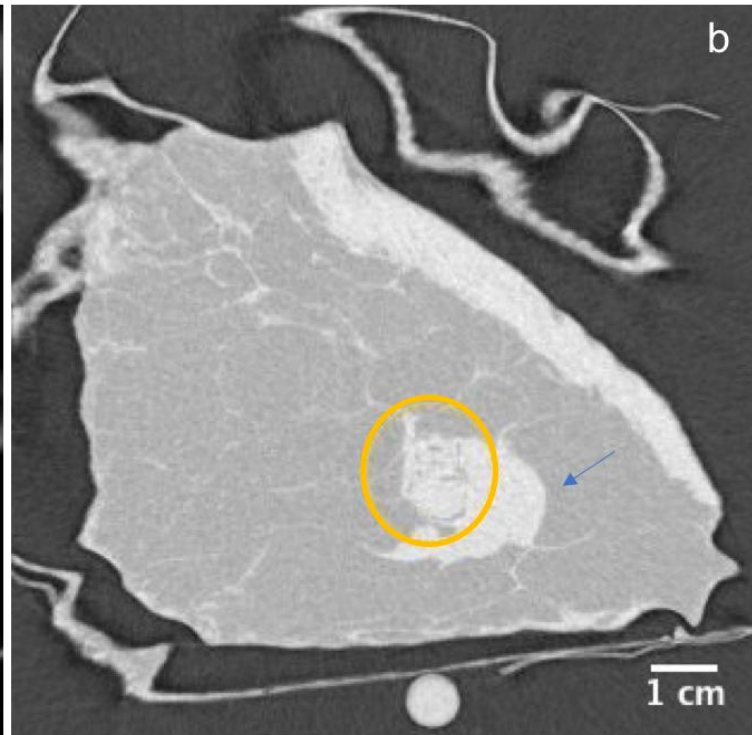
Mean Glandular dose = 5.8 mGy



Conventional



Synchrotron

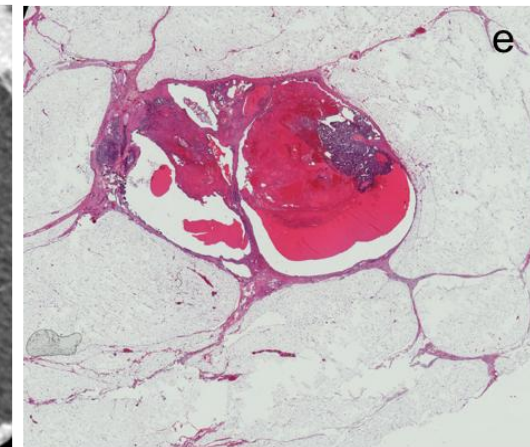
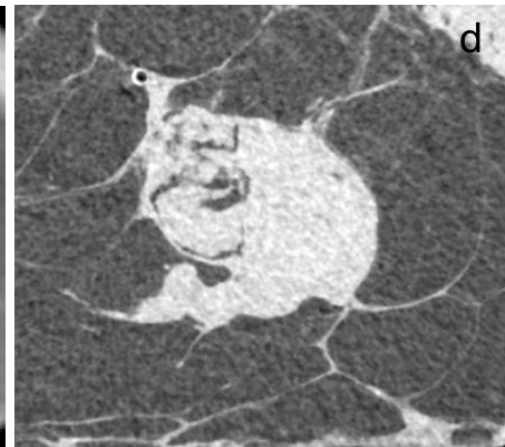
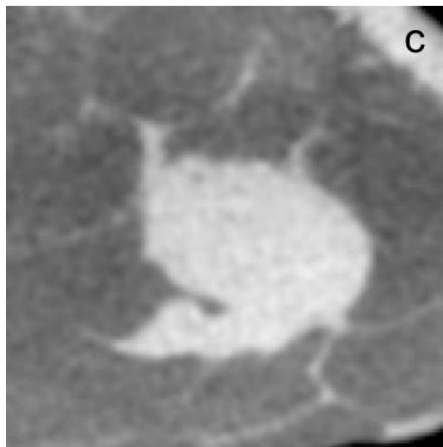


Excised breast sample including an *in situ* intraductal papillary carcinoma.

a) image obtained with the dedicated CB-CT system (Konig).

b) image obtained with PB-CT technique.

The blue arrow indicates the part of the lesion with regular borders, the yellow circle highlights the infiltrating part.



c) Close-up CB-CT

d) Close-up PB-CT

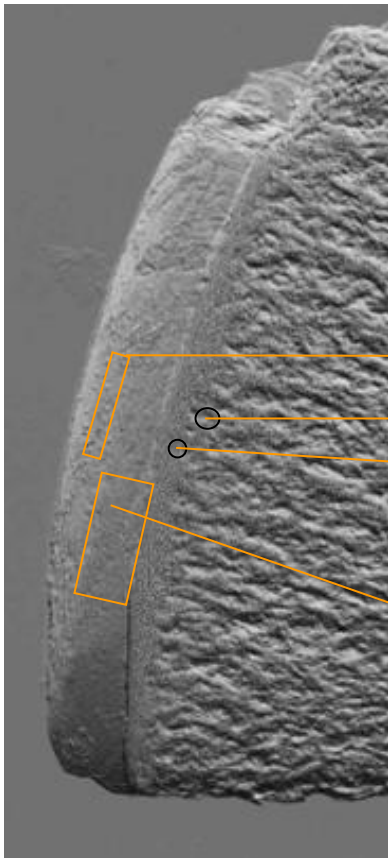
e) Histological Image

Osteoarthritis (OA) is a disease characterized by the progressive degeneration of articular cartilage. It has a high incidence in the adult population. Affecting mainly the elderly population, it is one of the main causes of disability worldwide. Conventional radiography detects only **important osseous changes**, at advanced stages of disease, when therapeutic strategies are less effective. **Early changes** in the **cartilage** and other **articular tissues** are **not** directly visible. MRI imaging works better but the maximum achievable spatial resolution is not always adequate.

Need to study:

- cartilage
- cartilage-bone interfaces
- changes in the bone structure

Aim: detect the architectural arrangement of collagen within cartilage and evaluate how the cartilage degeneration affects the underlying subchondral and trabecular bone.



Superficial Layer (Zone of horizontal collagen fibers with flat cells)

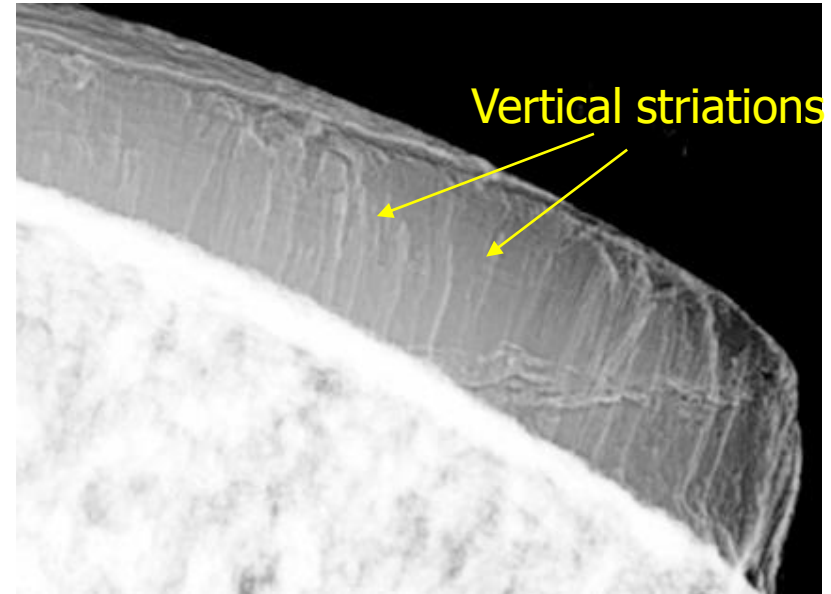
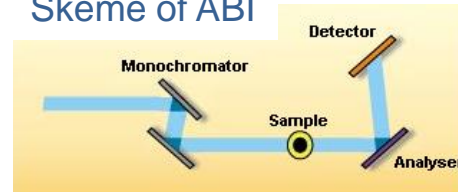
Subchondral Bone Plate (**Important for diagnostic purposes in OA**)

Tidemark (Border between normal and mineralized cartilage)

Transitional and Deep Layer (round cells, collagen fiber switches from horizontal to vertical orientation, increasing stiffness and material density)

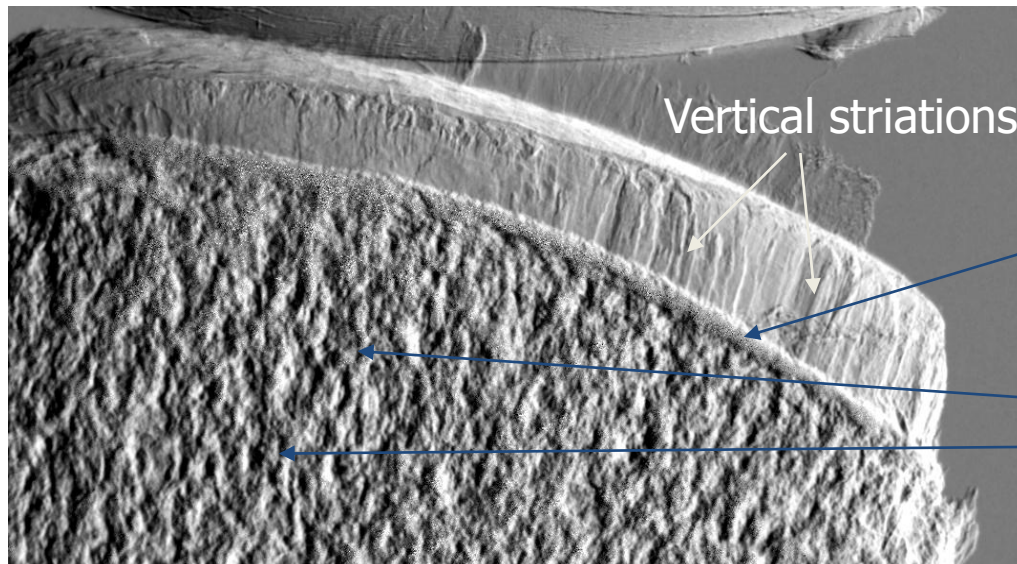
- The Analyzer Based Imaging (ABI) technique allows to visualize the discontinuities in the sample and the inner structures invisibles by means of conventional imaging.
- The transition bone-cartilage is emphasized.
- The articular cartilage striations are well visible due to X-ray diffraction at edges of fibers

Scheme of ABI



Apparent absorption image

Refraction image

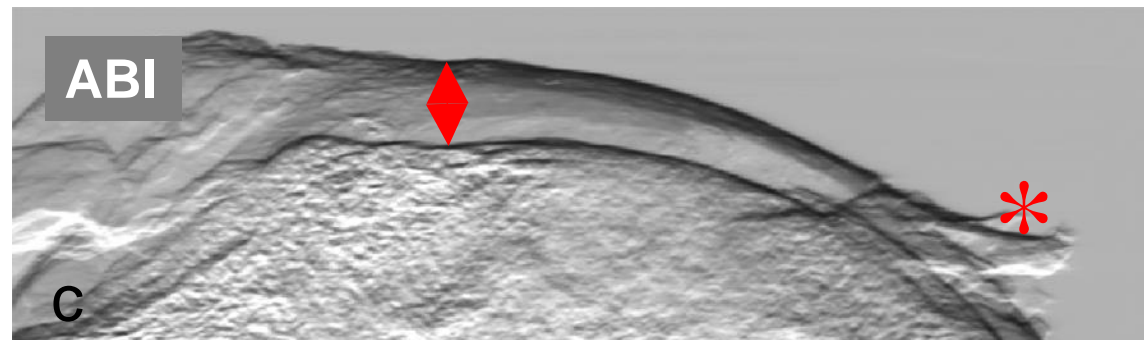
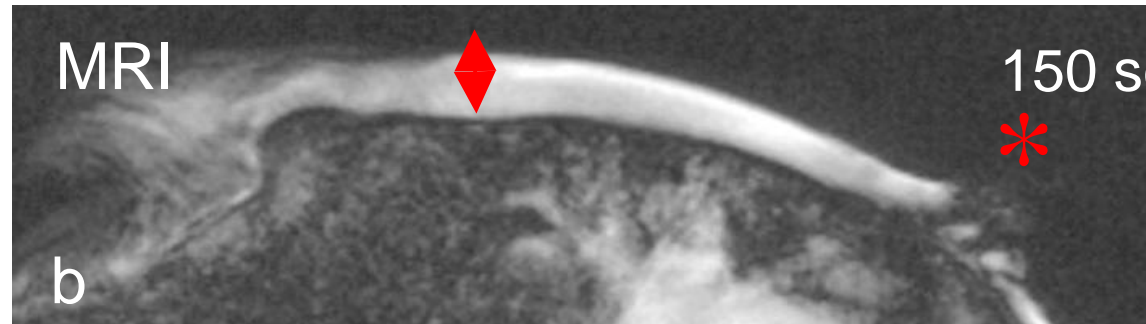
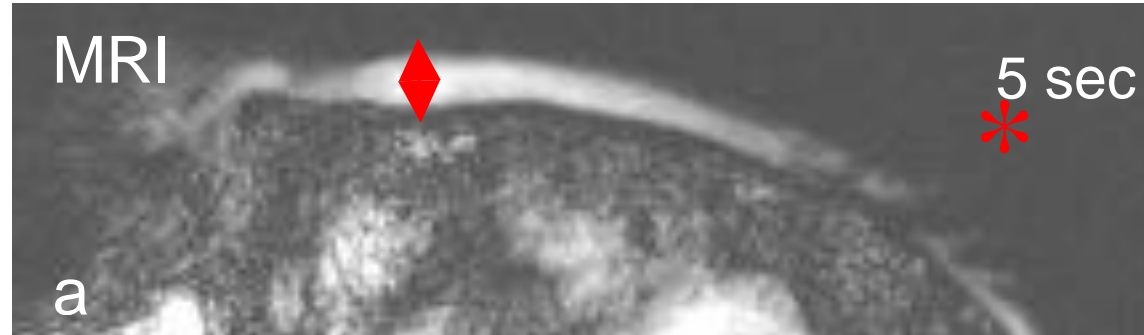


Subchondral
bone

Elettra
25 keV

Trabecular bone

Femur head core cuts: comparison with MRI



	High resolution (virtual histology)	Tissues imaging/small animals	Clinical Breast imaging	Clinical Lung CT	Clinical Cartilages
Sample horiz size	1 - 20 mm	10 – 50 mm	6 - 15 cm	> 30 cm (Local Area)	8 - 15 cm
Sample thickness	1 - 10 mm	10 - 150 mm	6 - 15 cm	> 25 cm	6 - 10 cm
Pixel size (μm)	0.3 - 4	9 - 50 (in-vivo)	50 – 60	100	30-50
Energy range (keV)	8 – 40	17 – 30	17 -22 (2D imaging) 30 - 40 (CT)	40 – 60	22 - 30
Energy resolution	large bandwidth acceptable	low $\Delta E/E$ required with contrast agents	large bandwidth acceptable	large bandwidth acceptable	low $\Delta E/E$ required with ABI technique
Flux (min req)	10^{10} - 10^{12} ph/mm ² /s	$5 \cdot 10^7$ - 10^8 ph/mm ² /s	10^8 ph/mm ² /s	10^8 ph/mm ² /s	$5 \cdot 10^7$ - 10^8 ph/mm ² /s
Typical time for each CT scan	some sec to some mins (according to the available flux)	some sec to some mins (for in-vitro), 10 s or more for CT, according to acquisition mode	1-2 s for planar scan, 10 - 20 s for CT	1-2 s for planar scan, 10 s for CT (breath hold)	1-2 s for planar scan, 10 - 60 s for CT
Acquisition modality for CT	free running	Free running (breath hold) or retrospective gating or perspective gating	free running	Free running (breath hold) or perspective gating	free running

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Thanks for your attention!
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