

TRINITY COLLEGE DUBLIN



CENTER FOR PHYSICAL SCIENCES AND TECHNOLOGY





Marius Jakulis Jason foundation

Comparison of Electrochemical Systems for Sensing Redox Active Molecules

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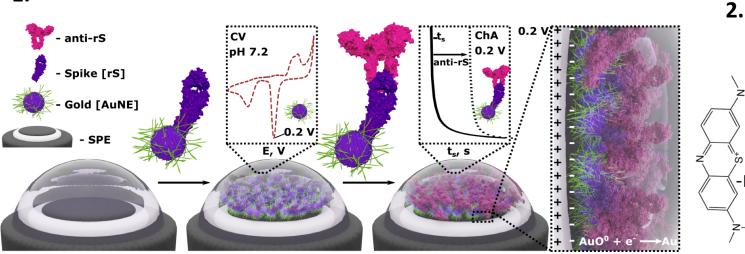
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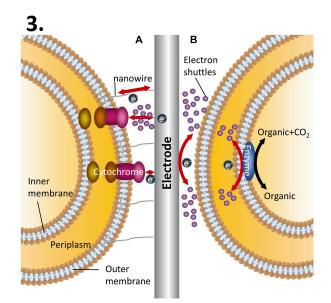
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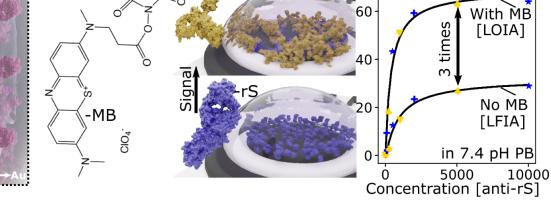
Research Field

- 1. Electrochemical detection of antibodies against SARS-CoV-2 Spike protein based on miniaturised platforms
- 2. Electrochemical investigation of potential drugs against SARS-CoV-2 Spike protein
- 3. Microbial Electrochemistry for investigation of electron transfer for application to microbial electrochemical cells anodes





Signal



^{H₂N-}∕‱-anti-rS

Work will be performed in collaboration of previous international research groups and LtD Delta Biosciences

What are biomarkers and why are they important?

Indicators in disease process

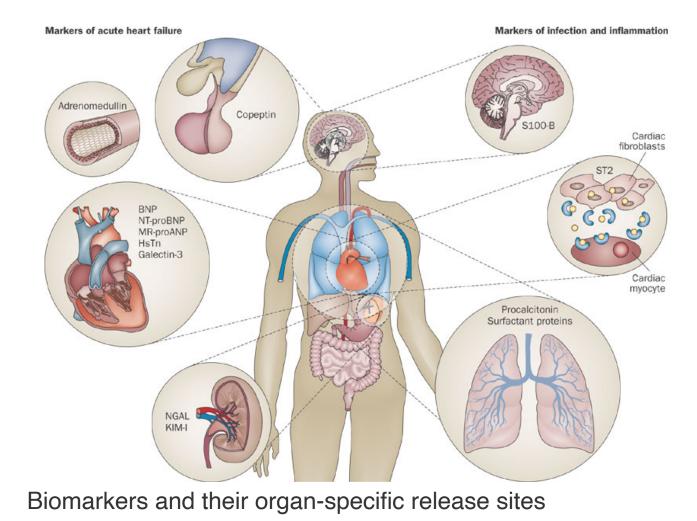
- Nucleic acids
- Proteins
- Small molecules

Improving the quality of life by

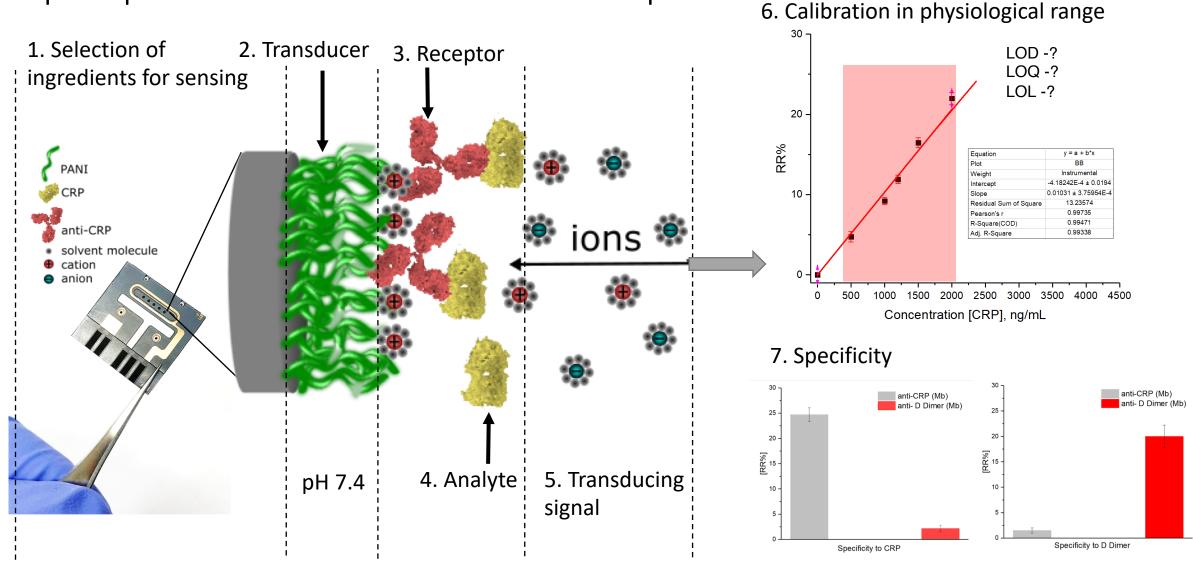
- Identification of disease
- Monitoring of disease-preventing organ (liver, kidney, heart and lung) injury into organ failure
- Effective disease treatment in advance

How to improve biosensing?

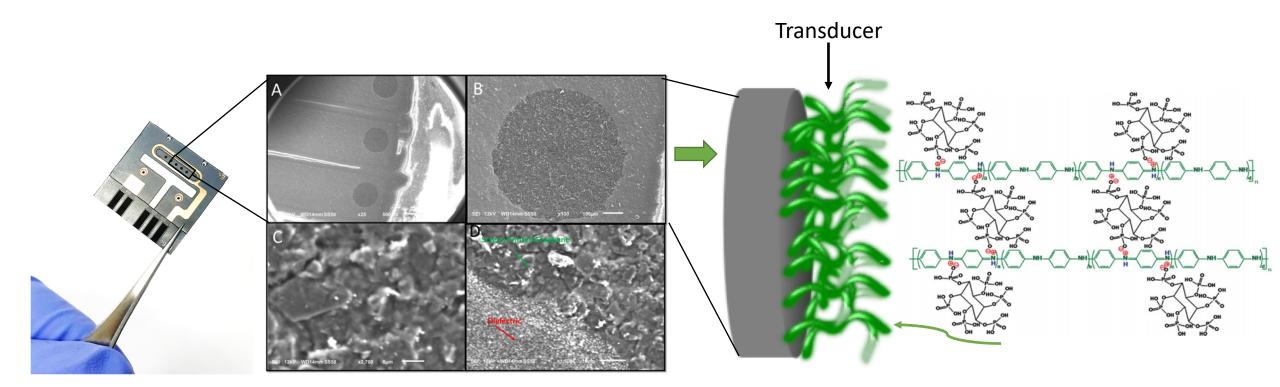
 using a panel of biomarkers, provides greater sensitivity and specificity



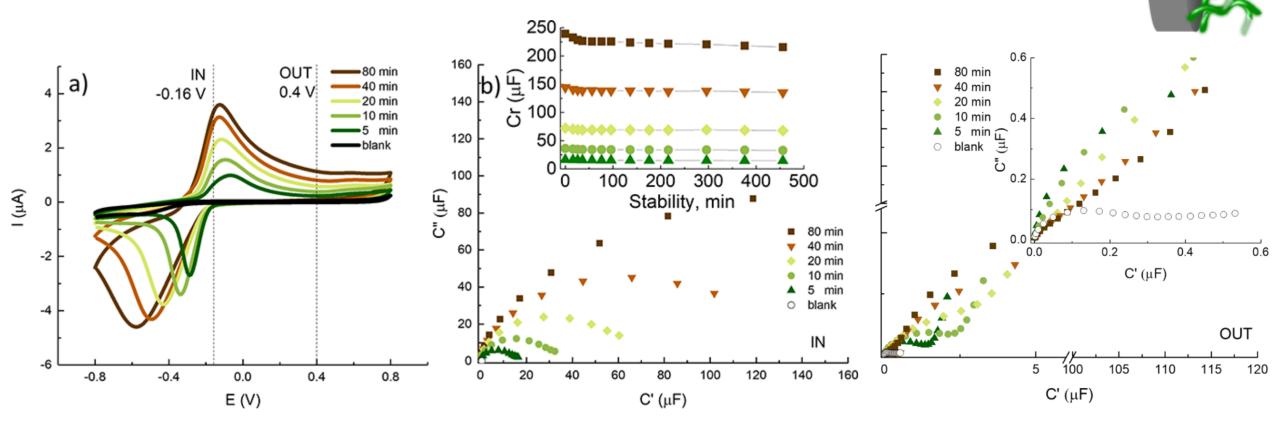
http://www.nature.com/nrcardio/journal/v9/n8/fig_tab/nrcardio.2012.60_F1.html



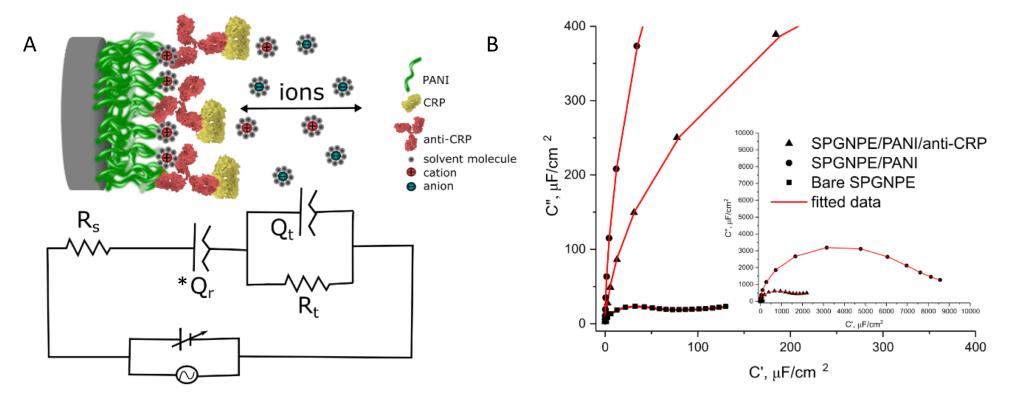
A. Baradoke, R. Hein, X. Li, J.J. Davis, Reagentless Redox Capacitive Assaying of C-Reactive Protein at a Polyaniline Interface, Anal. Chem. 92 (2020) 3508–3511. doi:10.1021/acs.analchem.9b05633.



SEM micrographs of SPGNPE chip - A, single working electrode -B, zoom in screen printed graphene - C, edge of electrode and dielectric (screen printed on top of graphene) used for sealing -D. showing structure of graphene ink and dielectric used for sealing of the electrode. Structure of PANI-PA demonstrating protonation zone between PO₃H₂ and NH₂ groups during electropolymerisation forming homogeneous structure.



Electrochemical characterization of PANI-PA films after different polymerization times (5–80 min) in 0.1 M PB, pH 7.4. (a) CVs at scan rate of 100 mV s⁻¹. (b) Capacitive Nyquist plots at redox IN potential (-0.16 V), where Cr can be resolved as the diameter of the semicircular region. The inset shows the temporal stability of Cr; after an initial signal decrease, the baseline is stable within $\leq 2\%$. (c) Measurements at redox out potencial.



A- Scheme of sensor layers and developed equivalent circuit for quantification of capacitive signal (calculated from Qr).
 B- Capacitive Nyquist plots demonstrating increase of capacitive signal after redox active polymer and decrease after antibody loading;

*Qr- Constant phase element used for non-ideal redox capacitance (Cr).

^{1.0}[a)

0.8

6.0 C, (μE)

0.2

0.0 0.0

0.5

1.0

1.5

C' (µF)

2.0

2.5

3.0

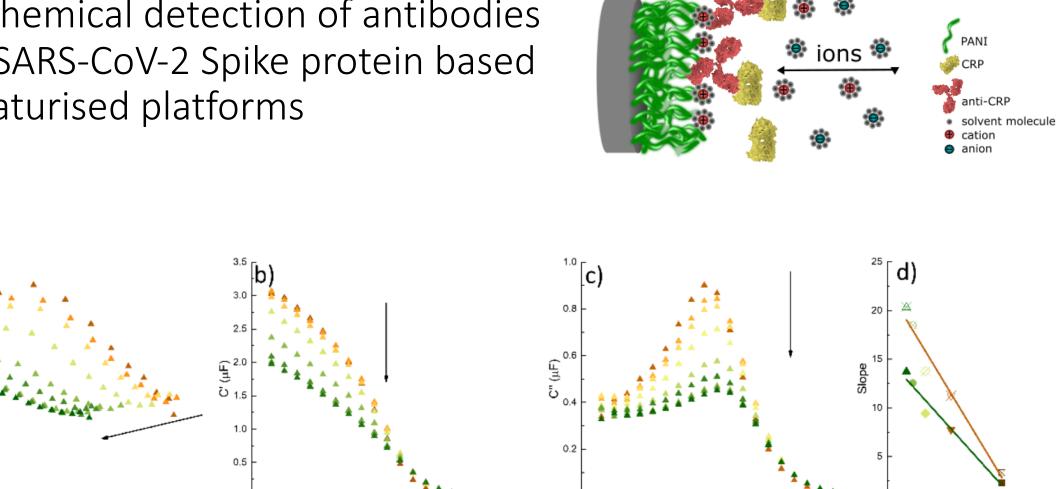
3.5

0.1

10

f (Hz)

100



Redox capacitive data for anti-CRP/PANI-10min after exposure to increasing concentrations of CRP in 1% FBS. a) Capacitive Cole-Cole plots. b) and c) Bode plots of the real and imaginary capacitance, respectively. d) Slope of the linear region of the calibration curve (sensitivity) as a function of polymerization time.

1000

10000

0.1

10

f (Hz)

100

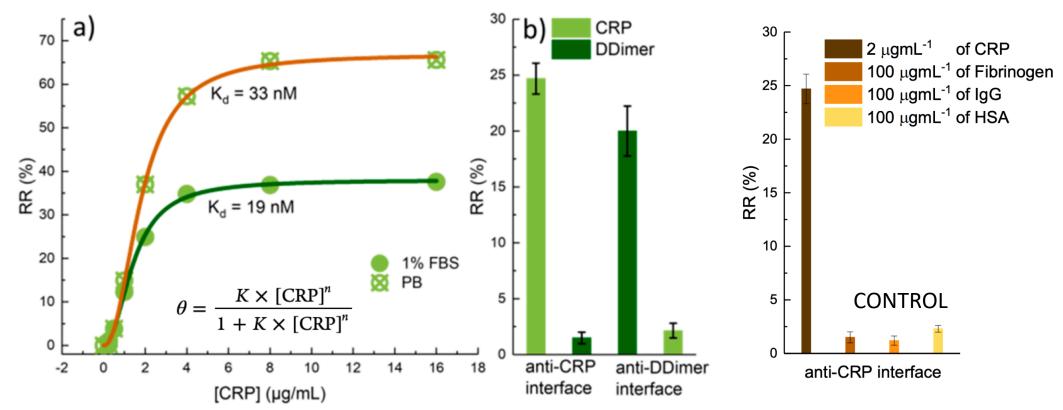
1000

10000

20 40 60

Polymerisation time (min)

0



(a) Relative response of PANI-10 min/anti-CRP toward CRP in PB and in 1% of FBS in clinically relevant range. The data was fitted to a Langmuir–Freundlich isotherm. (b) Relative response of anti-CRP or anti-D-dimer-modified PANI-10 min after exposure to 2 μg/mL of CRP or D-dimer in 1% FBS. Error bars represent one standard deviation from independent measurements on different electrodes.

Publications

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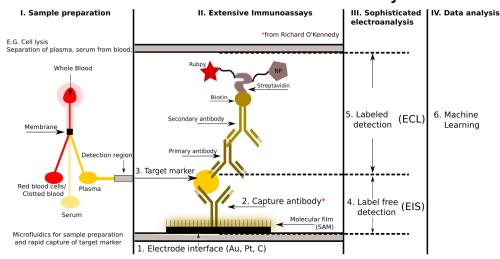
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BAC Marius Jakulis **Jason foundation** Alexandra Elsakova Viktorija Liustrovaite 000000000000 0000000000000 Flexible screen printed electro 000 0000 00 0 hanks to Dr. Emmanuel Kada