SAPIENZA UNIVERSITÀ DI ROMA

INFN

CENTRO RICERCHE ENRICO FERMI

24 th iWoRiD International Workshop on Radiation Imaging Detectors

Test beam results of a fluorescence-based monitor for ultra-high dose rates

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FLASH Radiotherapy with hIgh
Dose-rate particle beAms

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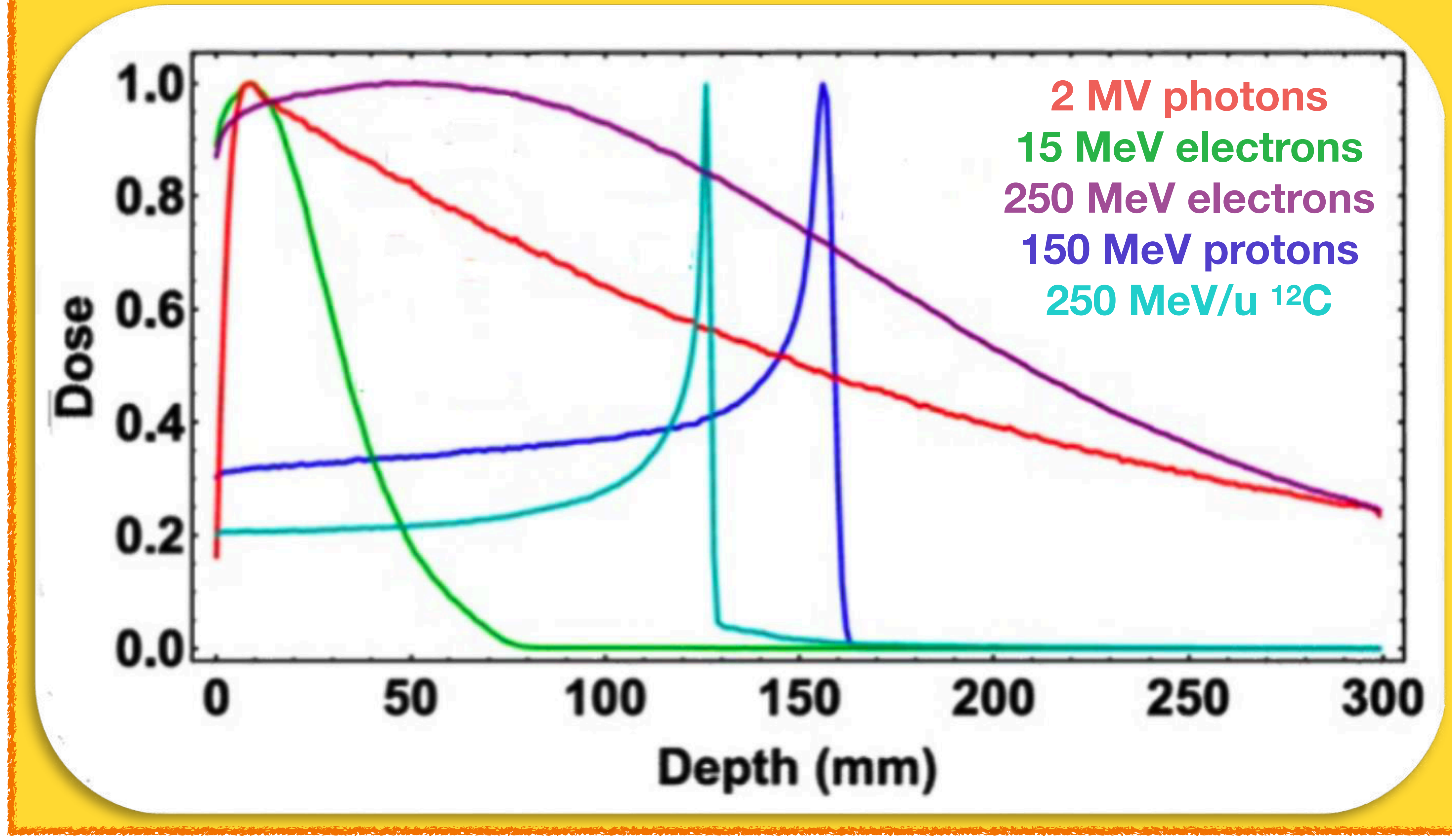
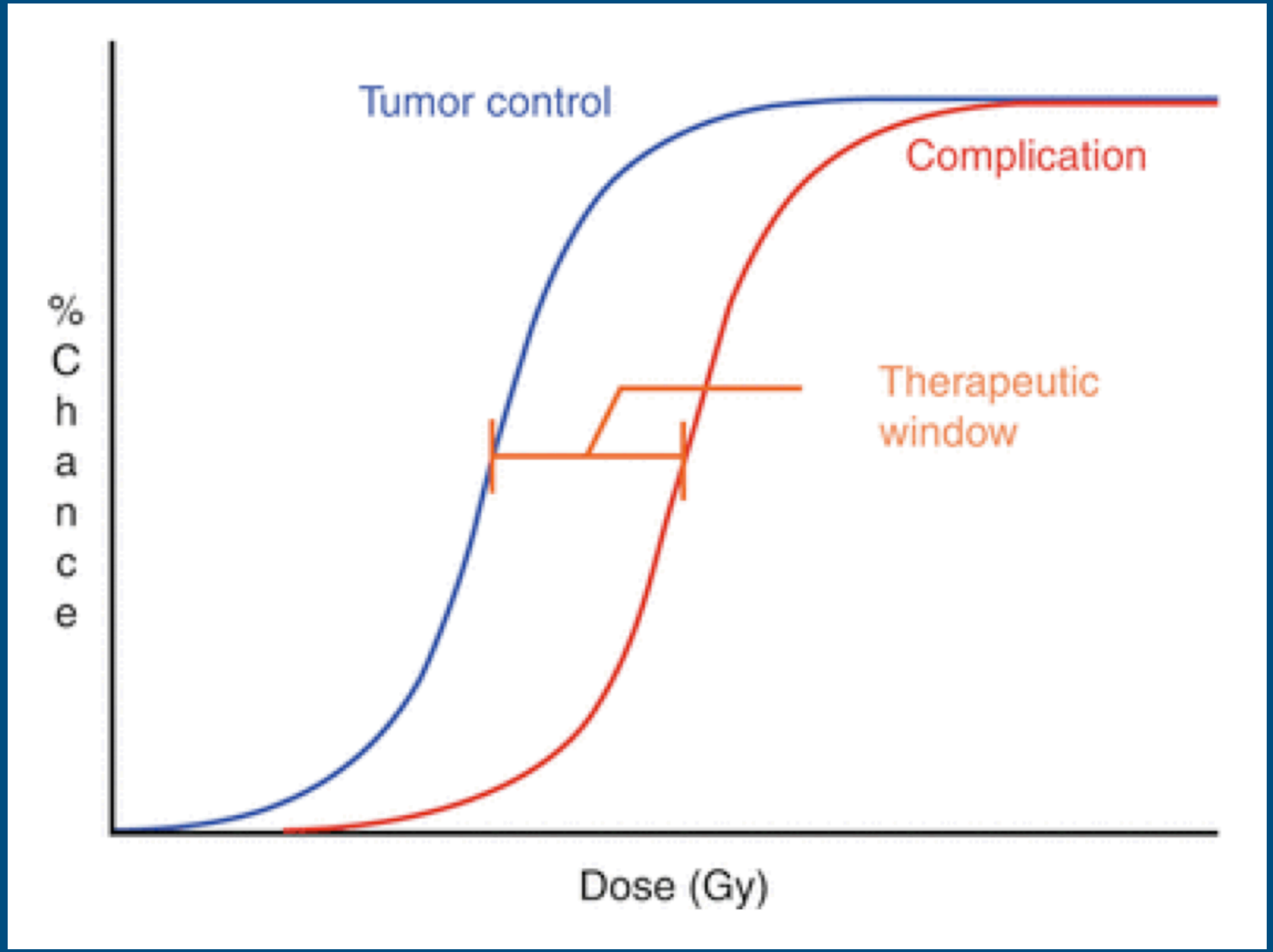
Radiotherapy

Goal: destroy tumors while saving the healthy tissue

- **Therapeutical beam** (electrons, photons, light ions) release energy inside the human tissues — **dose** — following an optimized **treatment plan**.





$$D = \frac{dE}{dm}\,[\mathrm{Gy}]$$

$$LET = \frac{dE_L}{dx}\,[\mathrm{MeV/cm}]$$

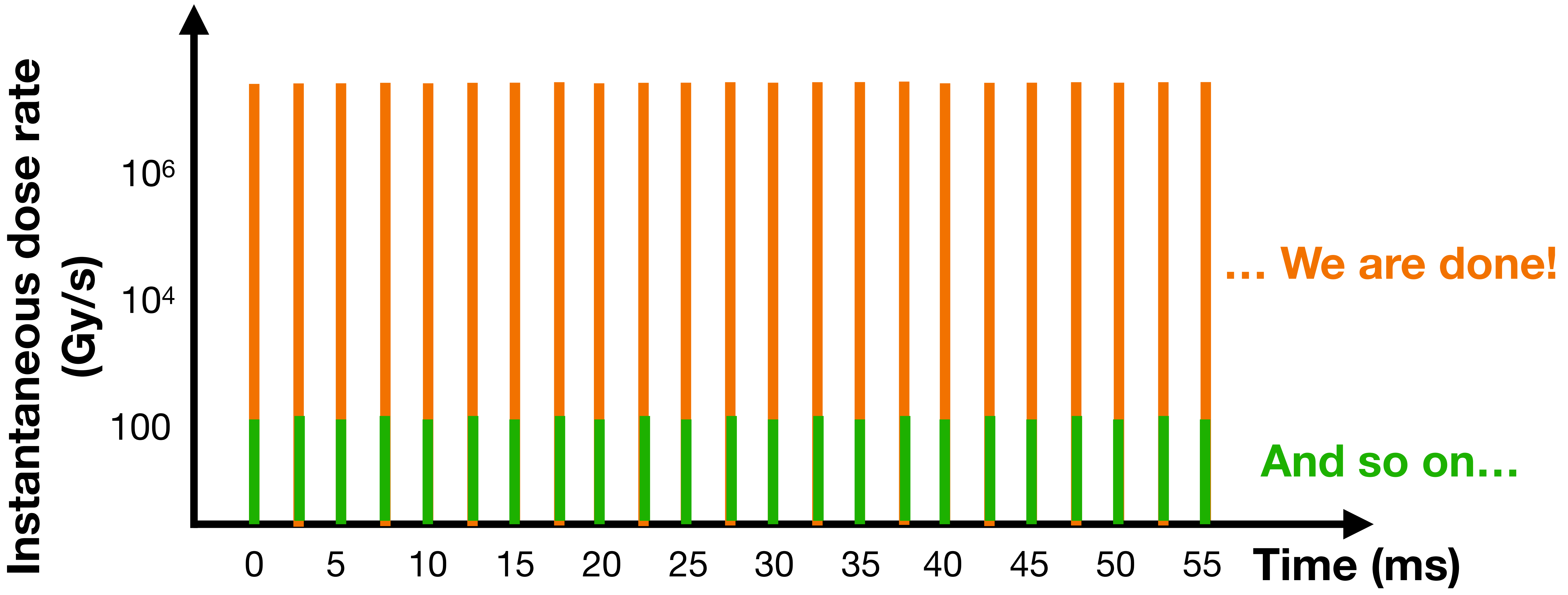
Dose: the amount of radiation we need to deliver during treatment (also as function of time).

Linear Energy Transfer: energy as a function of distance travelled inside the tissue… we can play with this.

FLASH effect

- The usual way a radiotherapy treatment is delivered is through a **pulsed** structure. The total dose is delivered in tens of **fractions** (~2 Gy, ~minutes or hours), each made of a sequence of pulses (~1 μs) carrying a small amount of dose.
- Recently, a new approach has gained great attention, to the point of being considered the next paradigm in the future of RT.
- An increased radio-resistance — **reduced toxicity** — is observed **in normal tissues** when delivering a single irradiation at ***ULTRAHIGH*** dose rates in a very short time (keeping anti-tumor efficacy).
- This has been named **FLASH** effect. Its biological mechanisms are not yet understood, and there is a lot of investigation going on.
- New accelerators are entering commissioning and operation, new theories are emerging awaiting validation…

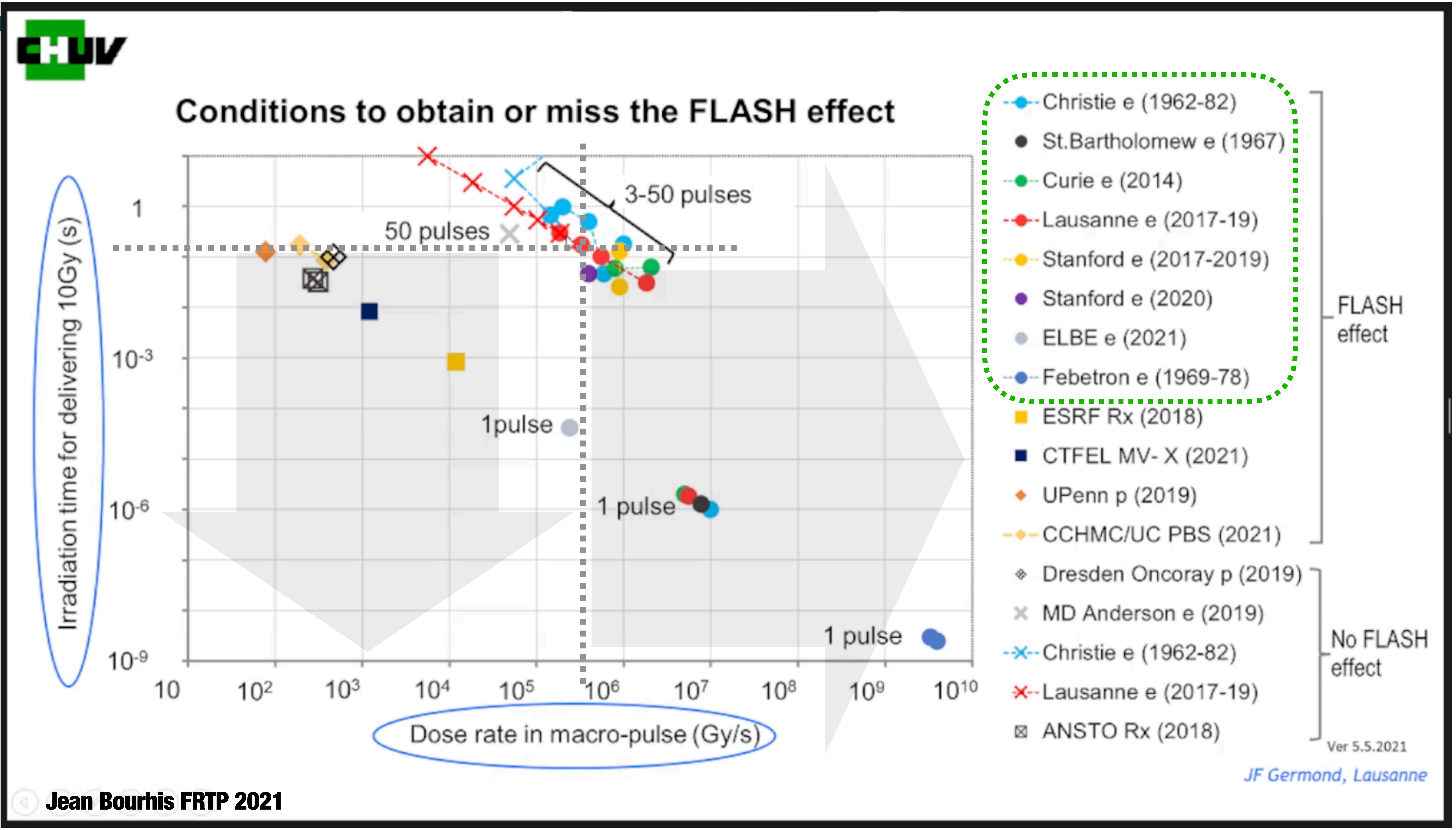
J. Wilson, et al., Ultra-high dose rate (FLASH) radiotherapy: Silver bullet or fool's gold?, Front. Oncol. 9:1563 (2020). doi:10.3389/fonc.2019.01563



Beam characteristics	CONV	FLASH
Dose per pulse	~ 0.4 mGy	> 1 Gy
Inst. dose rate (single pulse)	~ 100 Gy/s	> 10^6 Gy/s
Mean dose rate (single fraction)	~ 0.1 Gy/s	> 100 Gy/s
Total treatment time	~ days	< 100 ms

FLASH effect

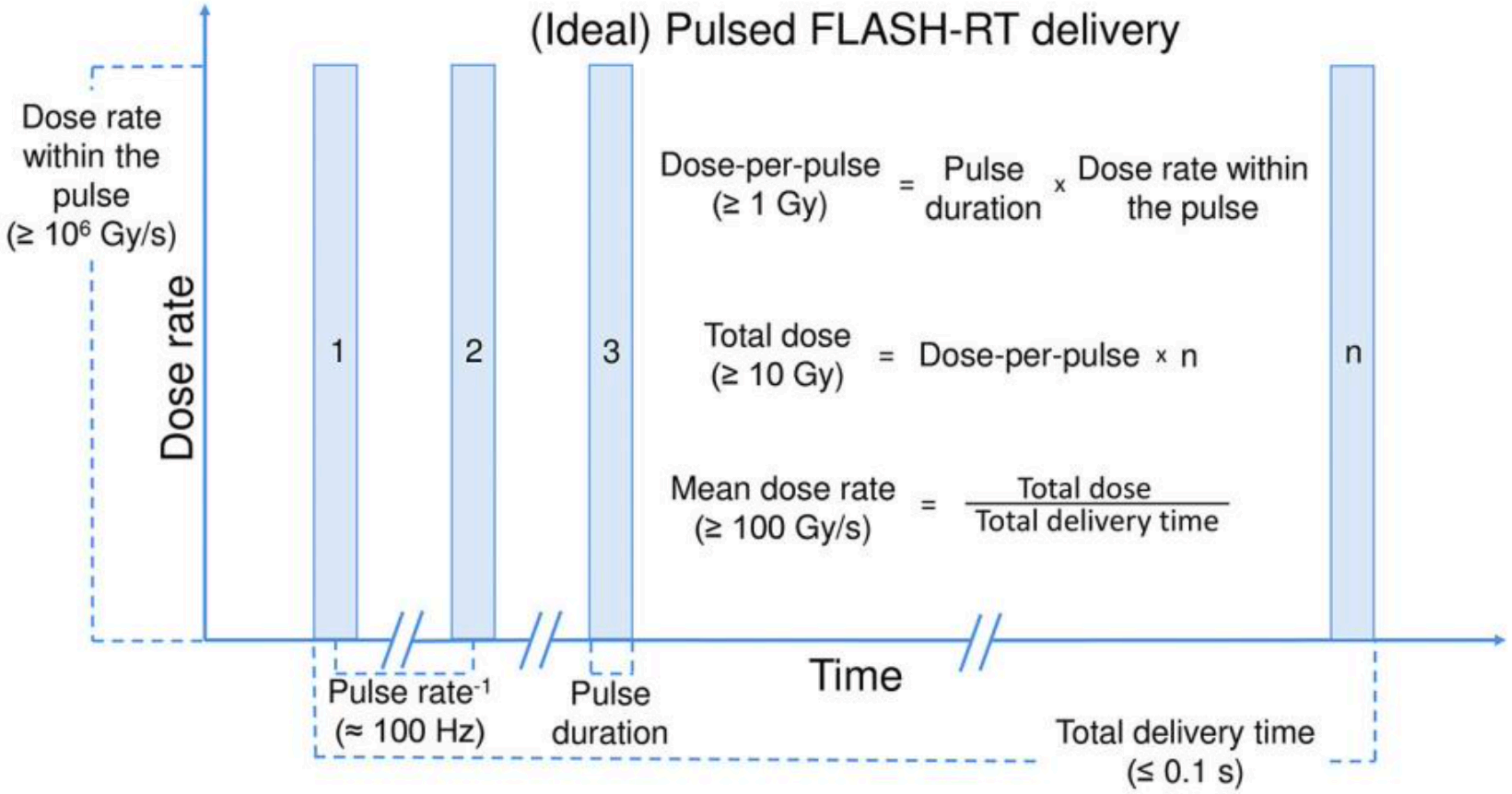
- Currently the experimental evidence points to the description of FLASH as a **threshold** effect. However, its characterization is complicated by many uncertainties:
  - **In measurement strategies**: it is difficult to evaluate quantitatively the sparing effect during *in vivo* evaluations;
  - **In dose measurements:** it is difficult to de-convolute the role played by the **dose within each pulse** and the **time of irradiation**.

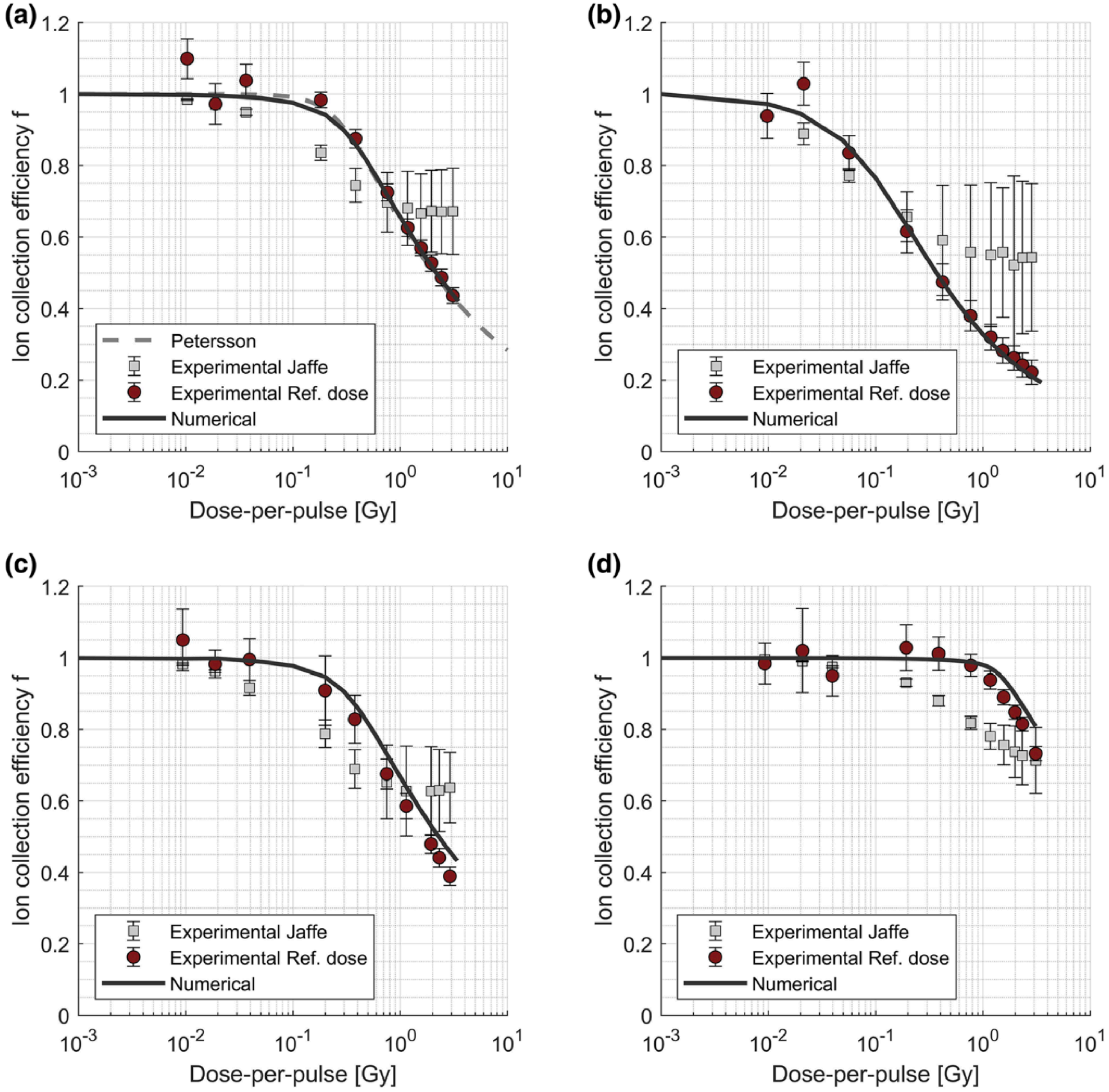


Jean Bourhis FRTP 2021

FLASH effect

- Beam monitoring is a cornerstone of this research, that must provide the reliable assessment of the (sometimes extreme) beam parameters.
- Problem is, BM can be hardly operated in FLASH environment. ICs undergo substantial energy dependencies due to **volume recombination**.
- (There are attempts to characterize this saturation effect by introducing correction factors.)

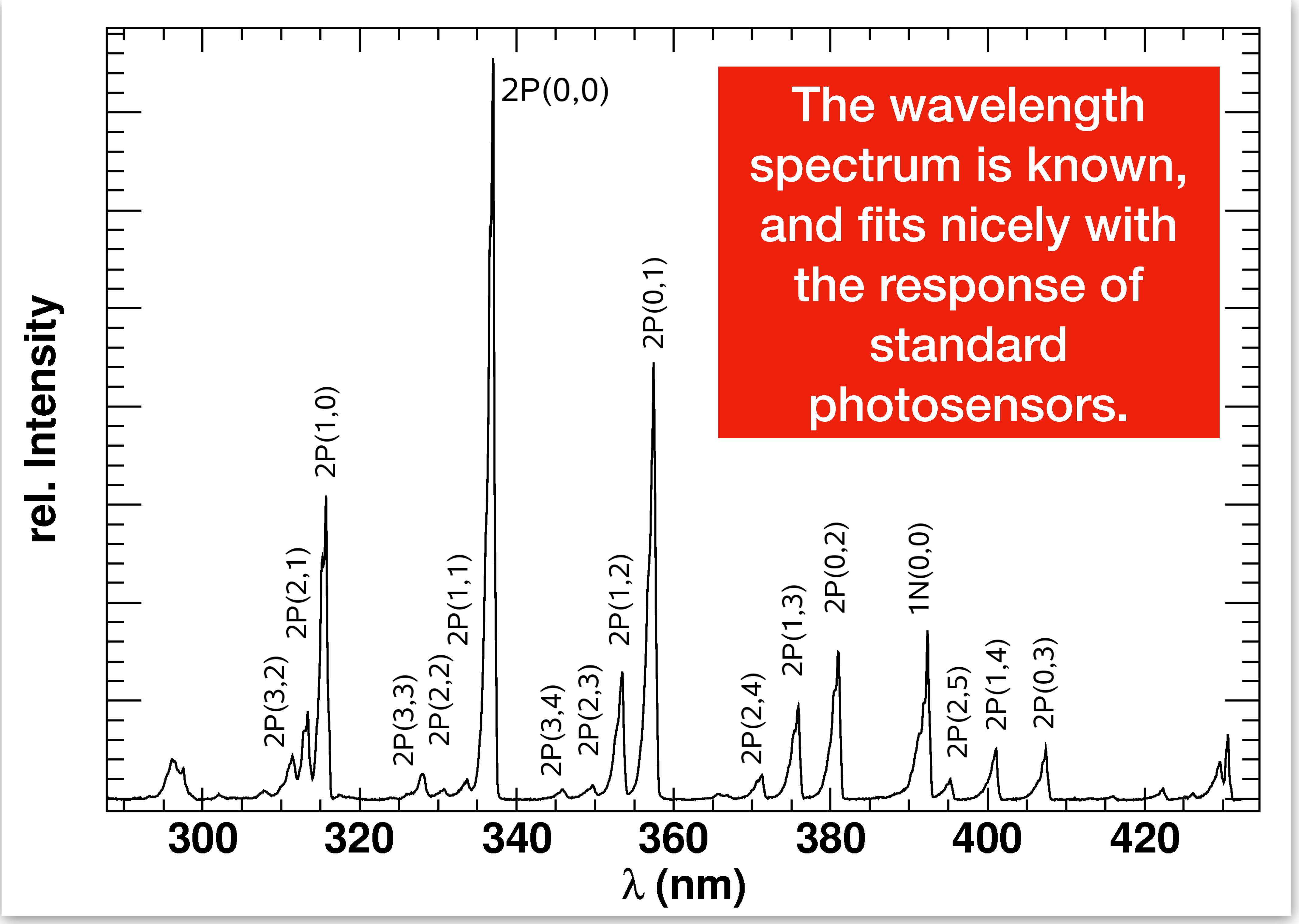




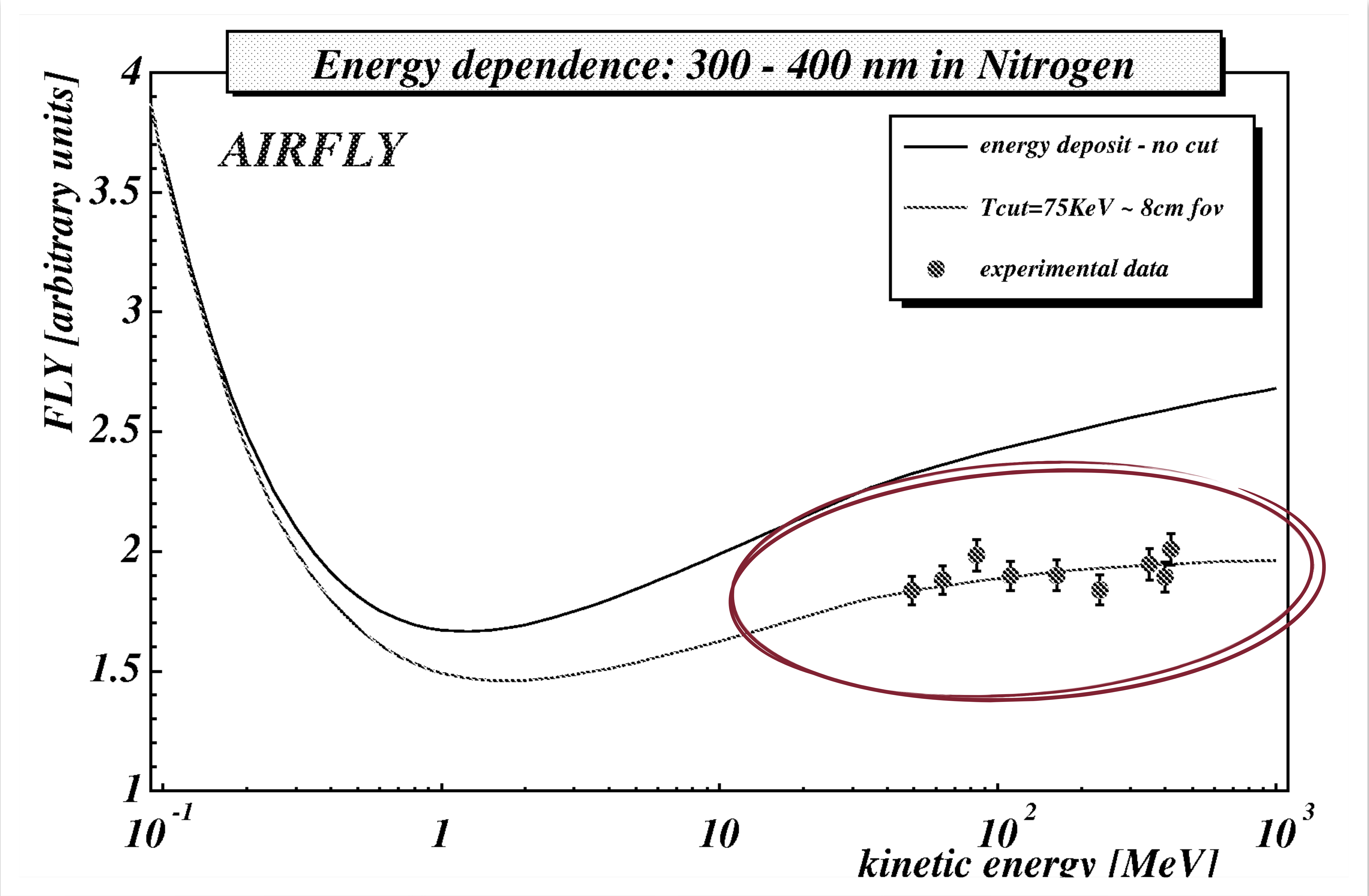
Ion collection efficiency for the ionization chambers with a polarizing voltage of 300 V. **(a)** Advanced Markus, **(b)** EWC2, **(c)** EWC1, **(d)** EWC05. doi: 10.1002/mp.14620

Fluorescence for FLASH BM

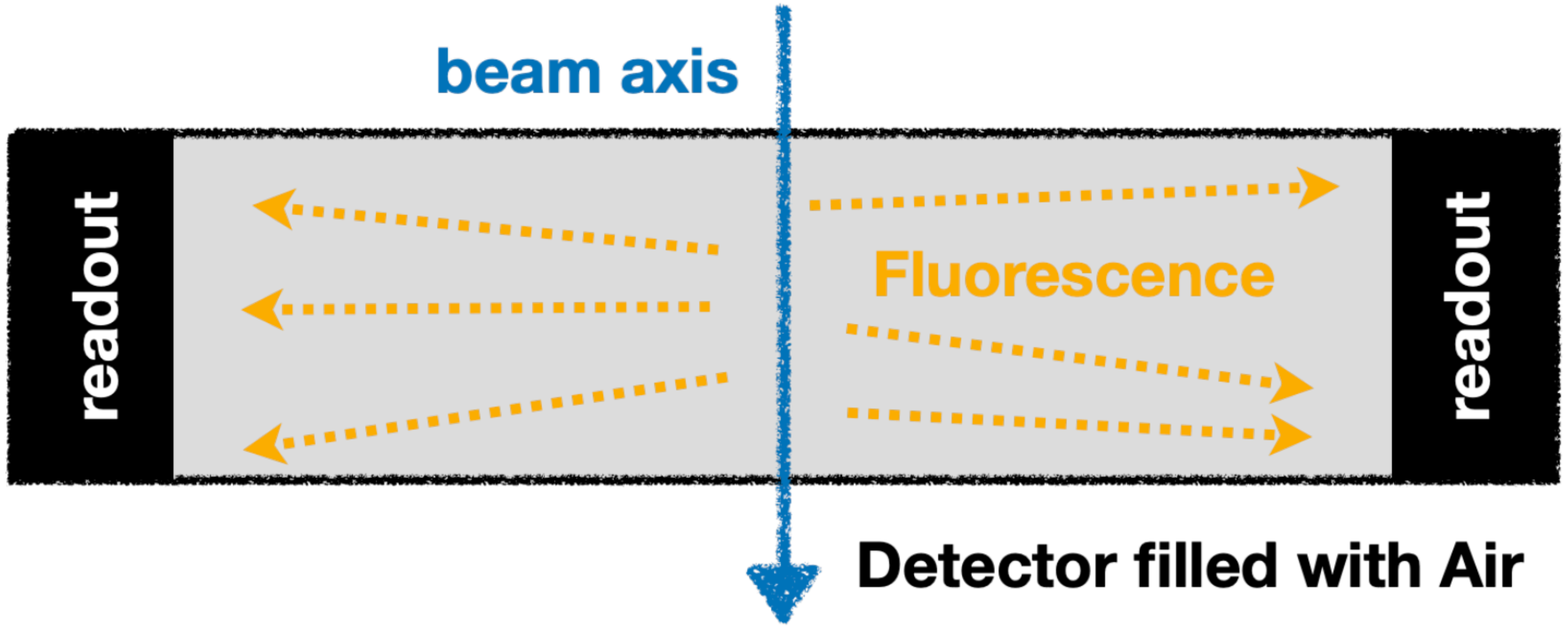
- According to data in literature, air fluorescence can do the job for us.
- In general, fluorescence is a form of luminescence. It is the emission of light from an excited atom or molecule, with a lifetime of the excited state around 10^{-8} s.
- In air, fluorescence occurs on the nitrogen molecule and it is excited via electron impact.



The wavelength spectrum is known, and fits nicely with the response of standard photosensors.



Fluorescence for FLASH BM



- Pressure and temperature dependencies, as well as the impact of different percentages of quenching elements, are present in literature, and can be accounted for with detector calibration.

- Above all else, the philosophy of using air as the active volume is to be as "invisible" to the beam as possible. The system should have minimal impact (the **empty box** approach).

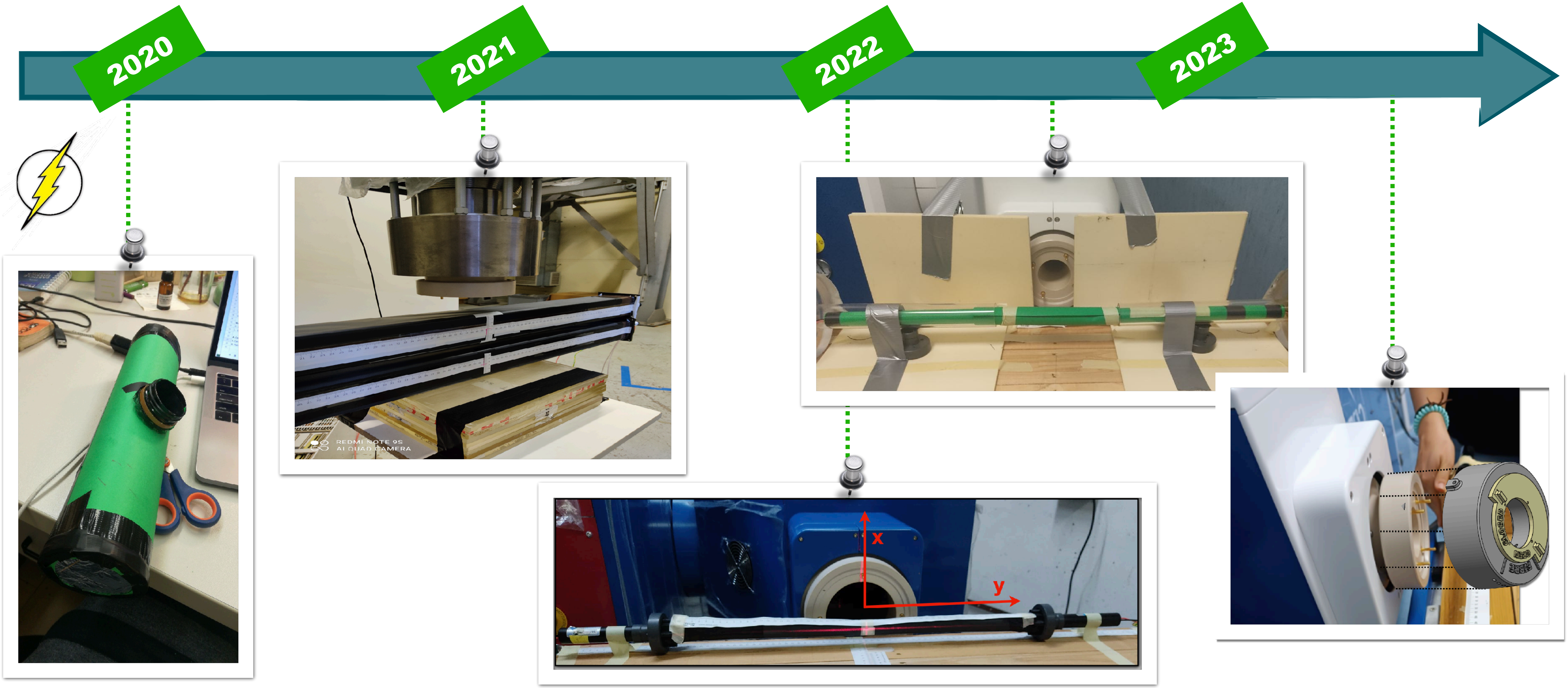
- Conceptually, it would fit nicely with the ultra-high dose rate regime of FLASH-RT.

- Fluorescence is already used to detect extensive air showers in atmosphere. However, it has been rarely, if ever, exploited for medical BM purposes; it is thus a rather open field for research.

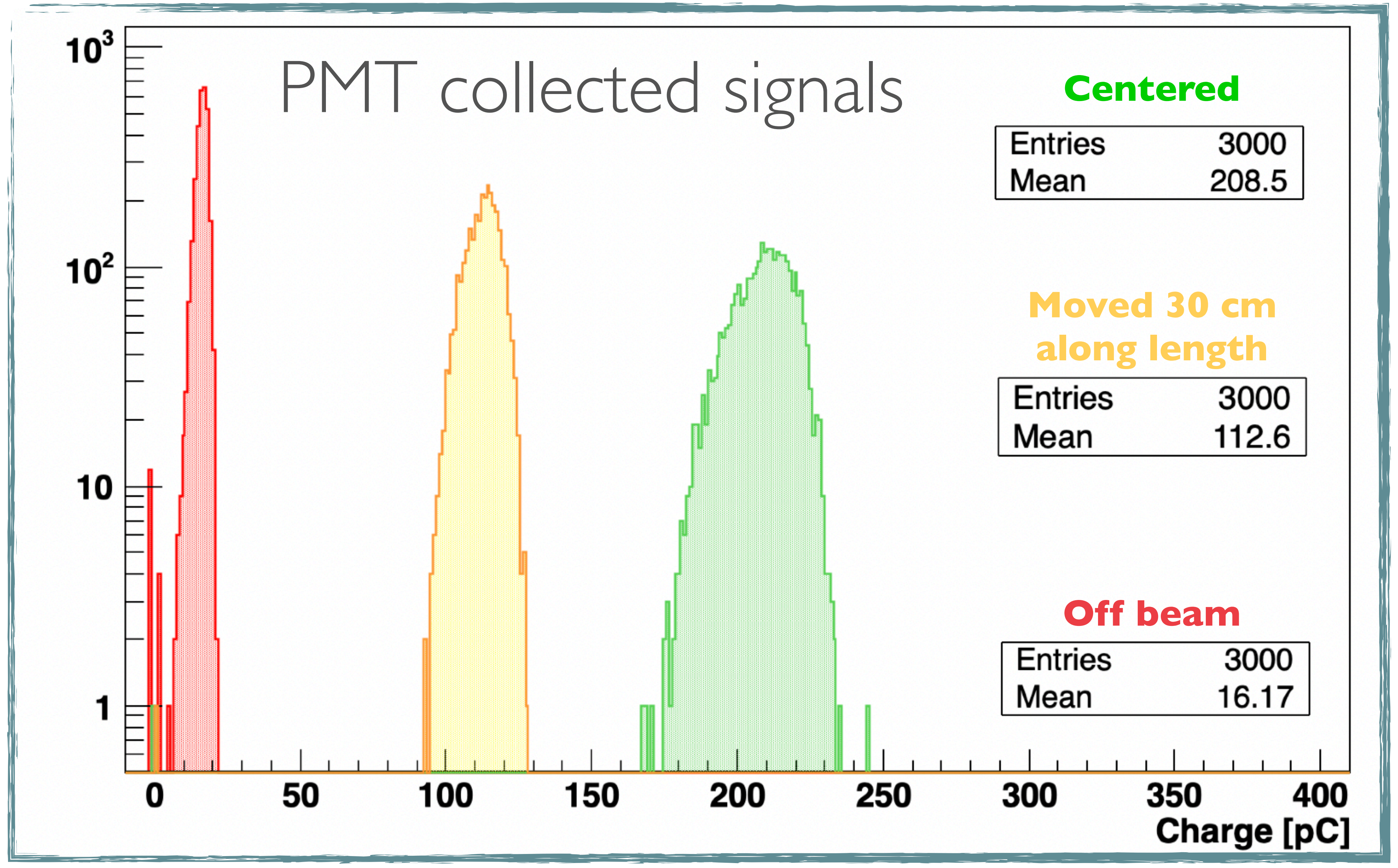
Photon emission	Isotropic
Excited state lifetime	10 ns
Wavelength spectrum	290-430 nm
Fluorescence yield	$\propto dE/dx$ (~ 4 ph./m)
Signal-to-#e⁻ relation	**LINEAR**

FlashDC

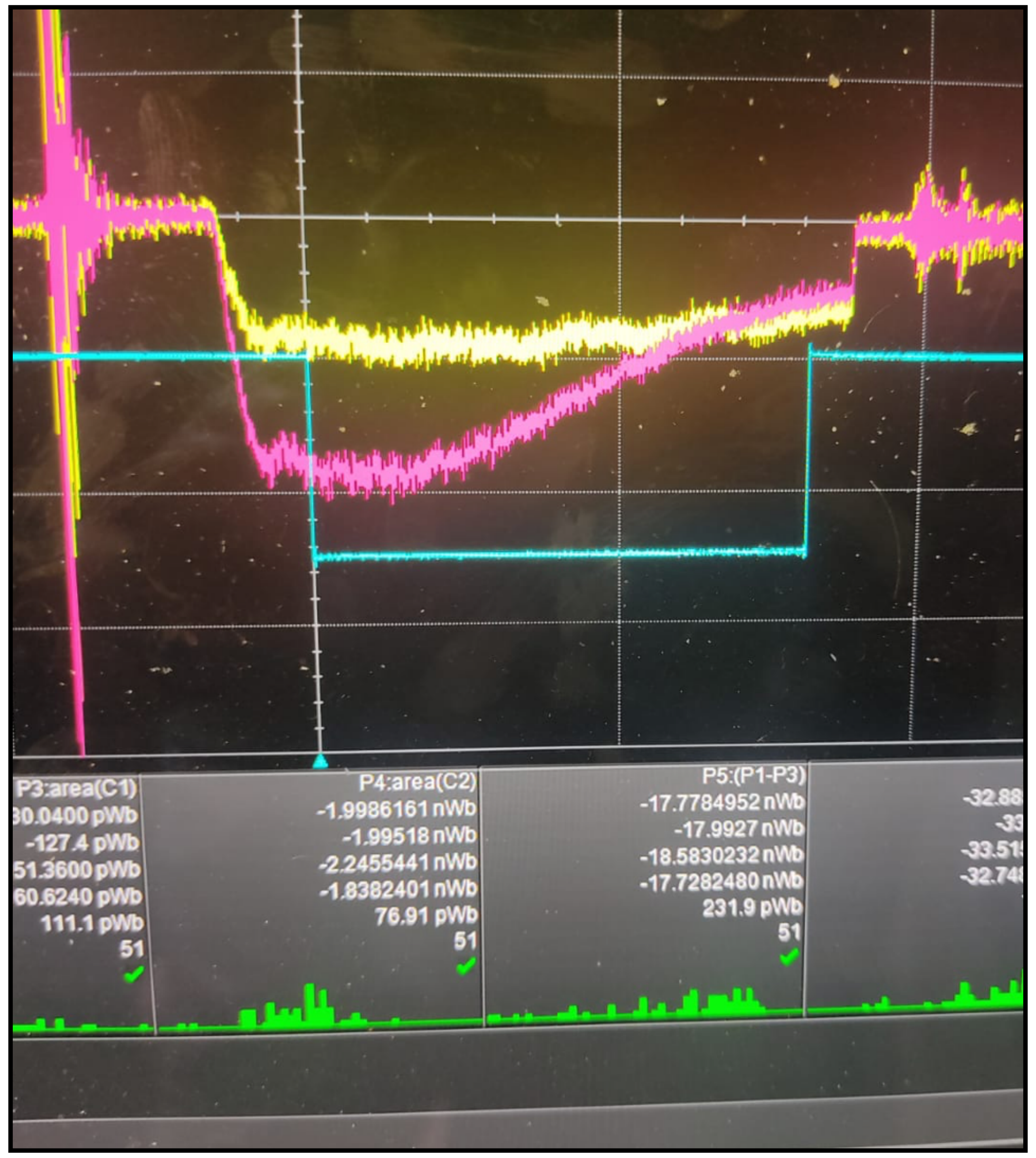
The first mandatory step is the validation of detection technique (linearity with the dose rate per pulse) with dedicated test beam at FLASH facilities.

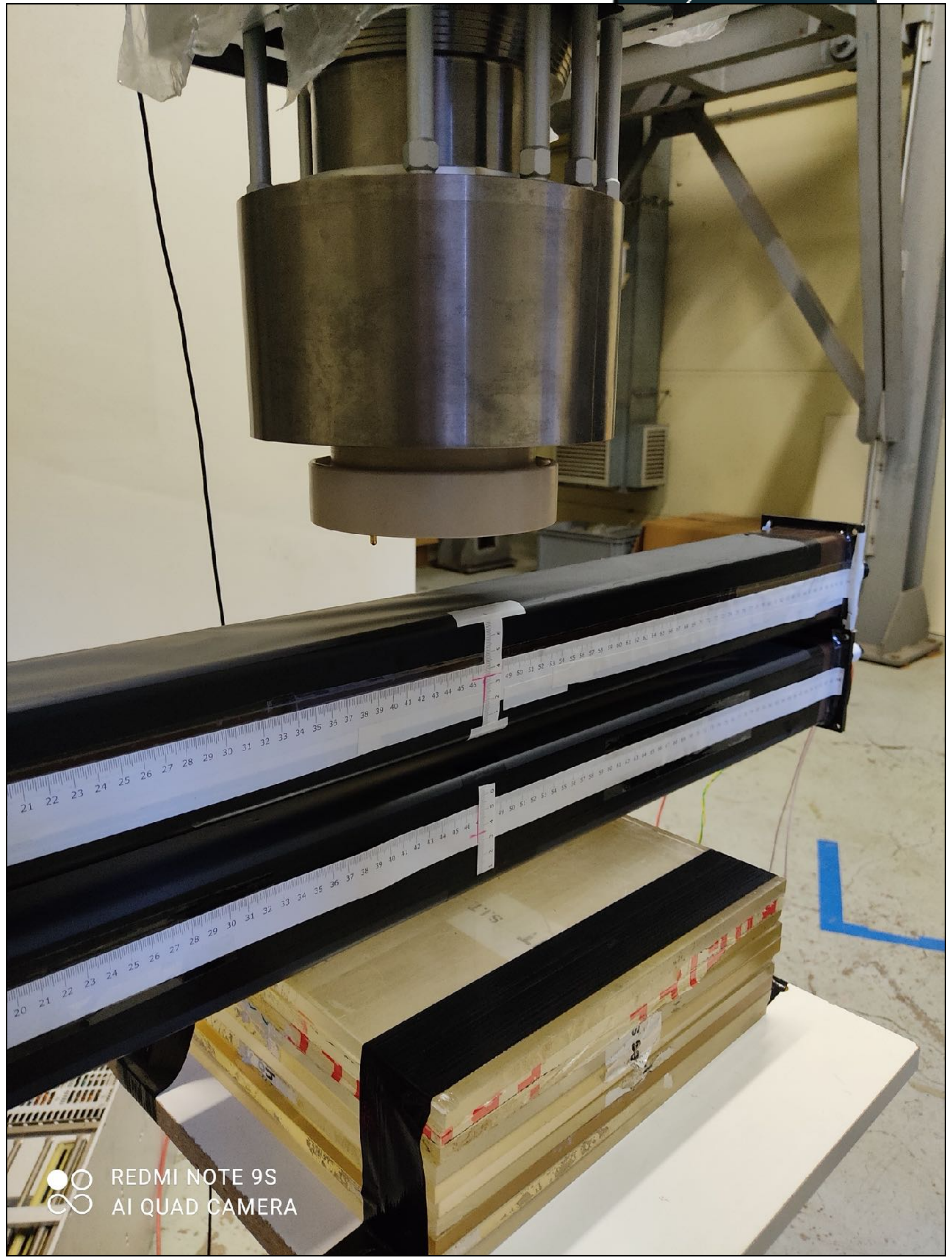


FLASH beam monitoring



- The first test is always the IN-OFF beam validation.

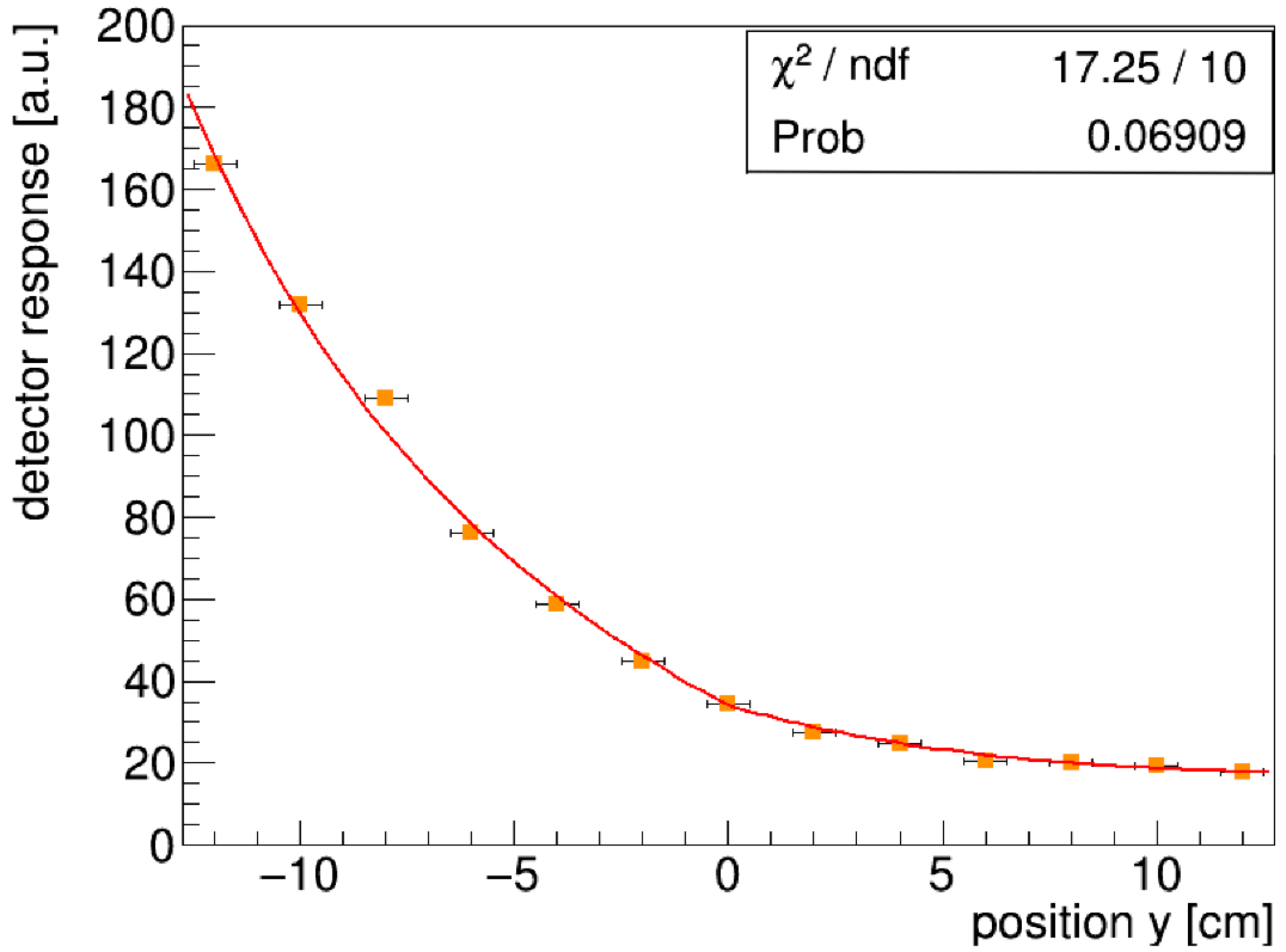




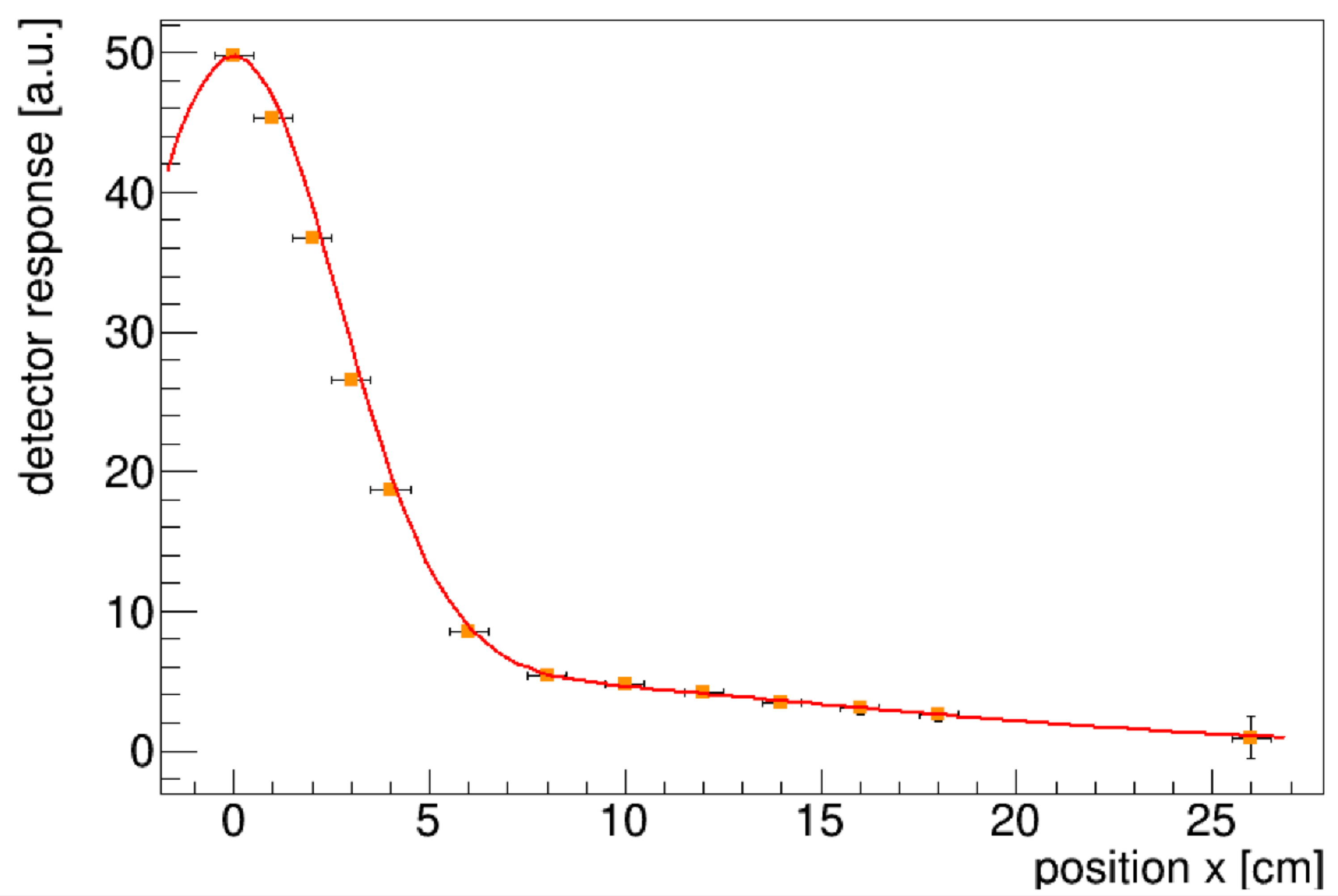
- Beside the detector geometry we have to be able to prove that the signal that we see is really the fluorescence… not trivial at all!
- Various test beams performing systematic analysis of **signal-to-dose linearity**, **background reduction**, **geometry optimization**…

FLASH beam monitoring

The signal is sensitive to the position with respect to the beam (shift, in/off beam)

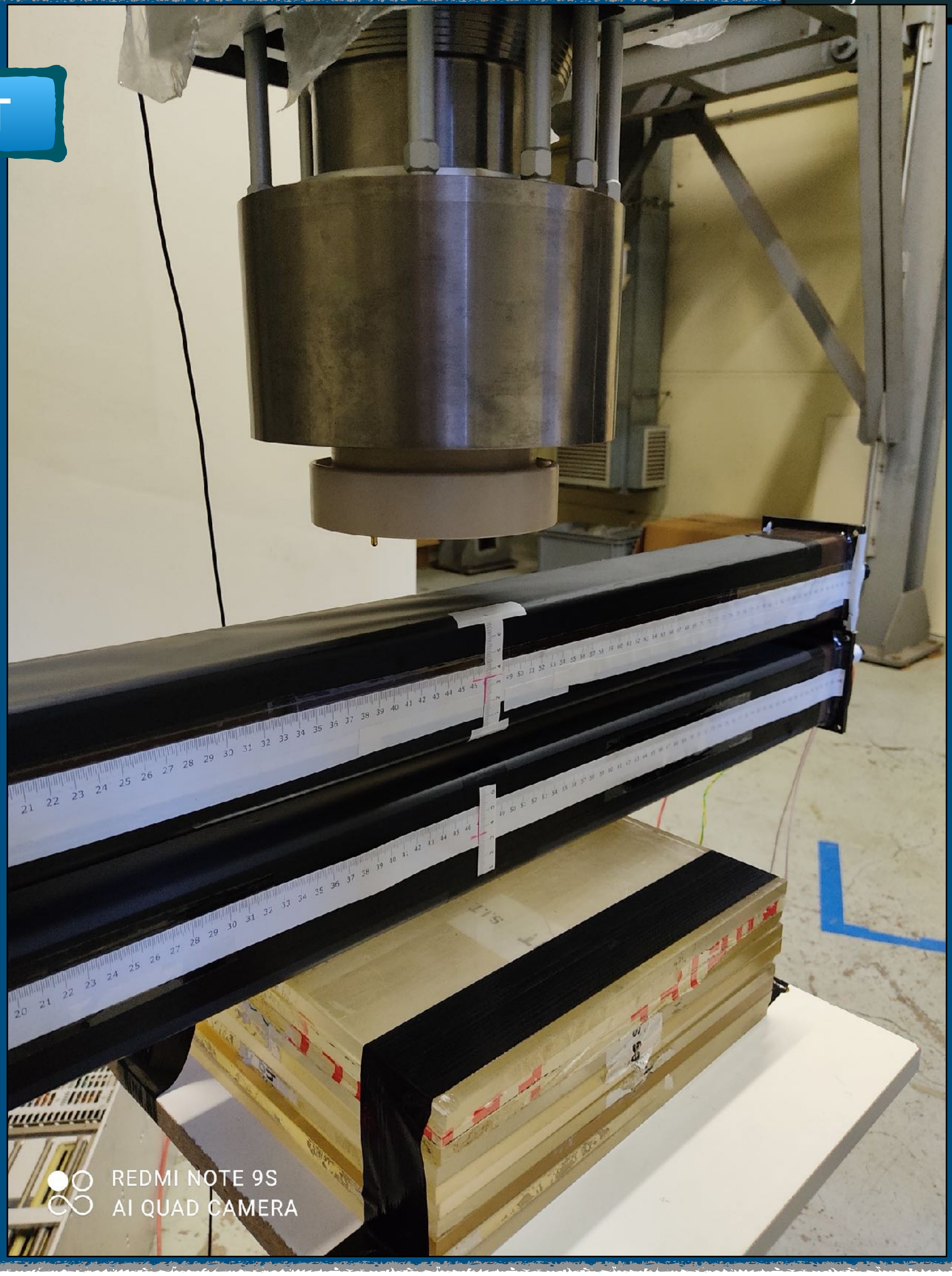


- We verified the expected geometry dependencies of the detector response in different positions.
- Further indication that the signal is indeed due to the production of optical photons **inside** the active volume.



- Plot obtained gradually moving the detector off the beam to reconstruct the transverse shape.
- The in-beam/off-beam difference is observed.

2020: SIT



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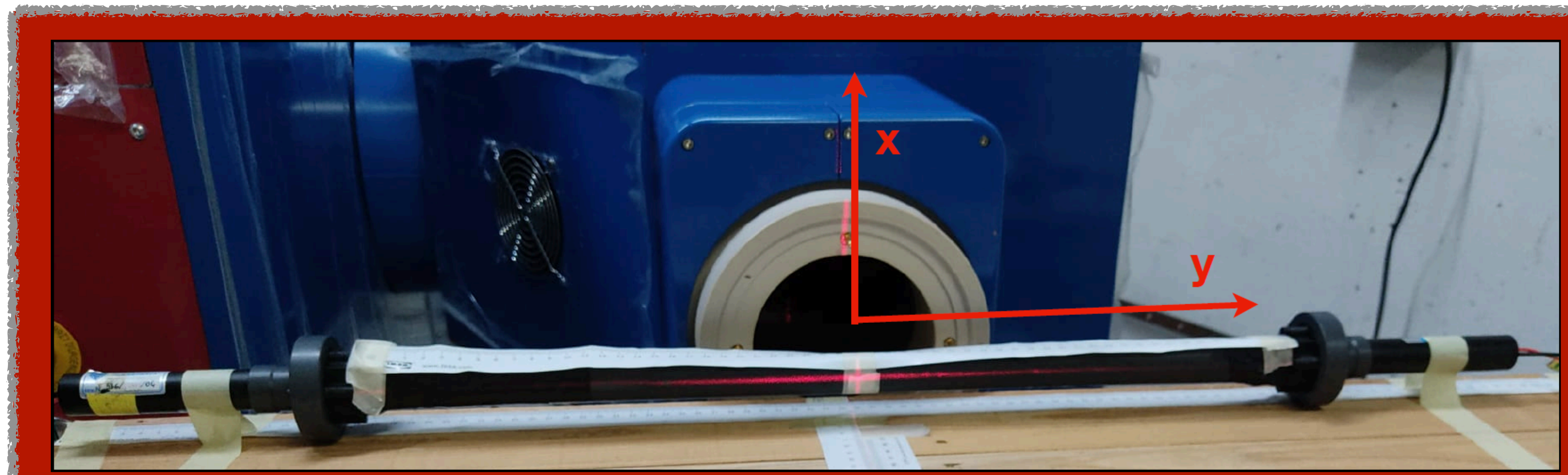
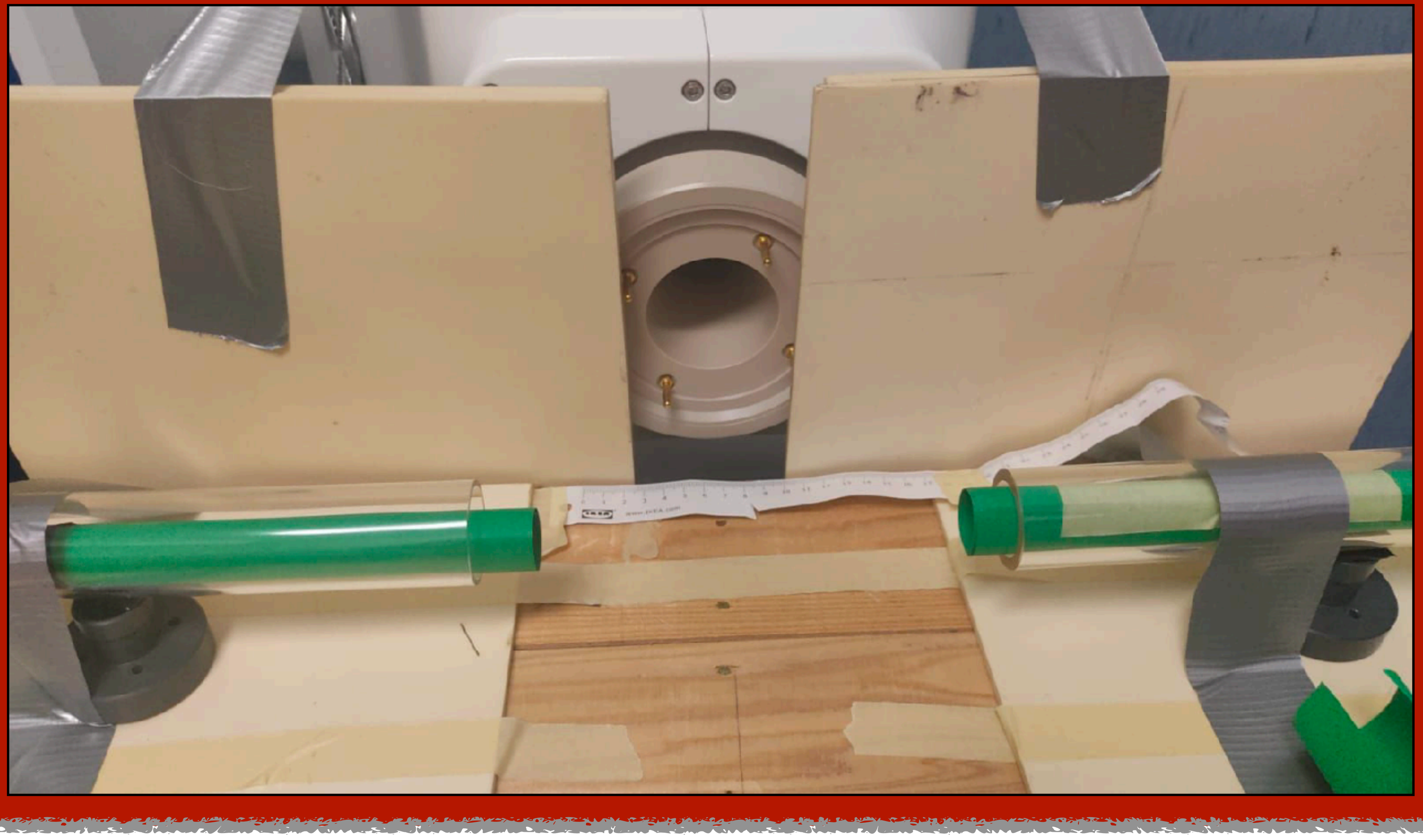
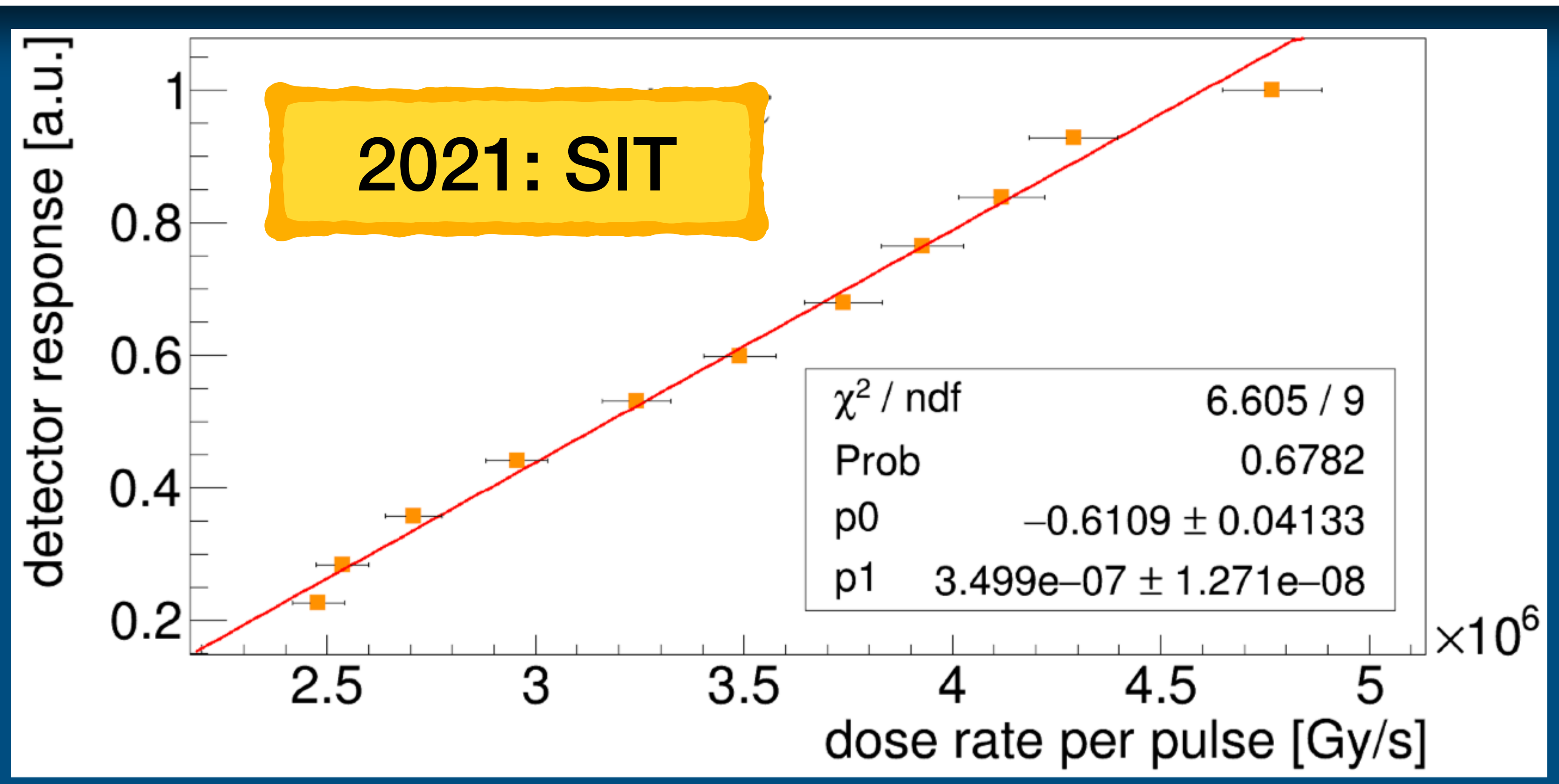
FLASH beam monitoring

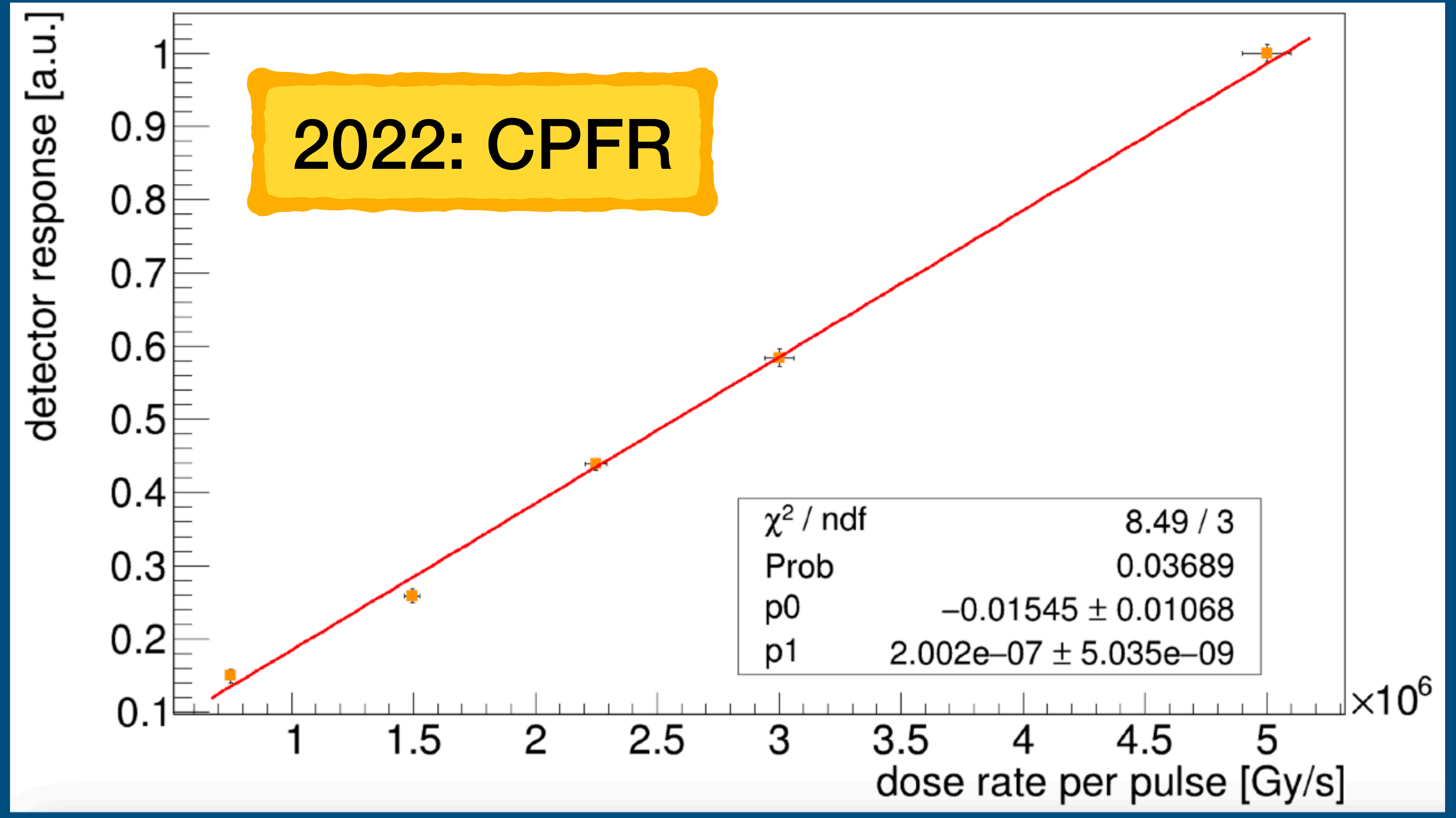


- The machine available at Pisa is the first electron beam accelerator that can provide different beam currents => it is the best place to verify the detector linearity!
- However the background induced by the PVC box forced us to remove the material from the beam line.



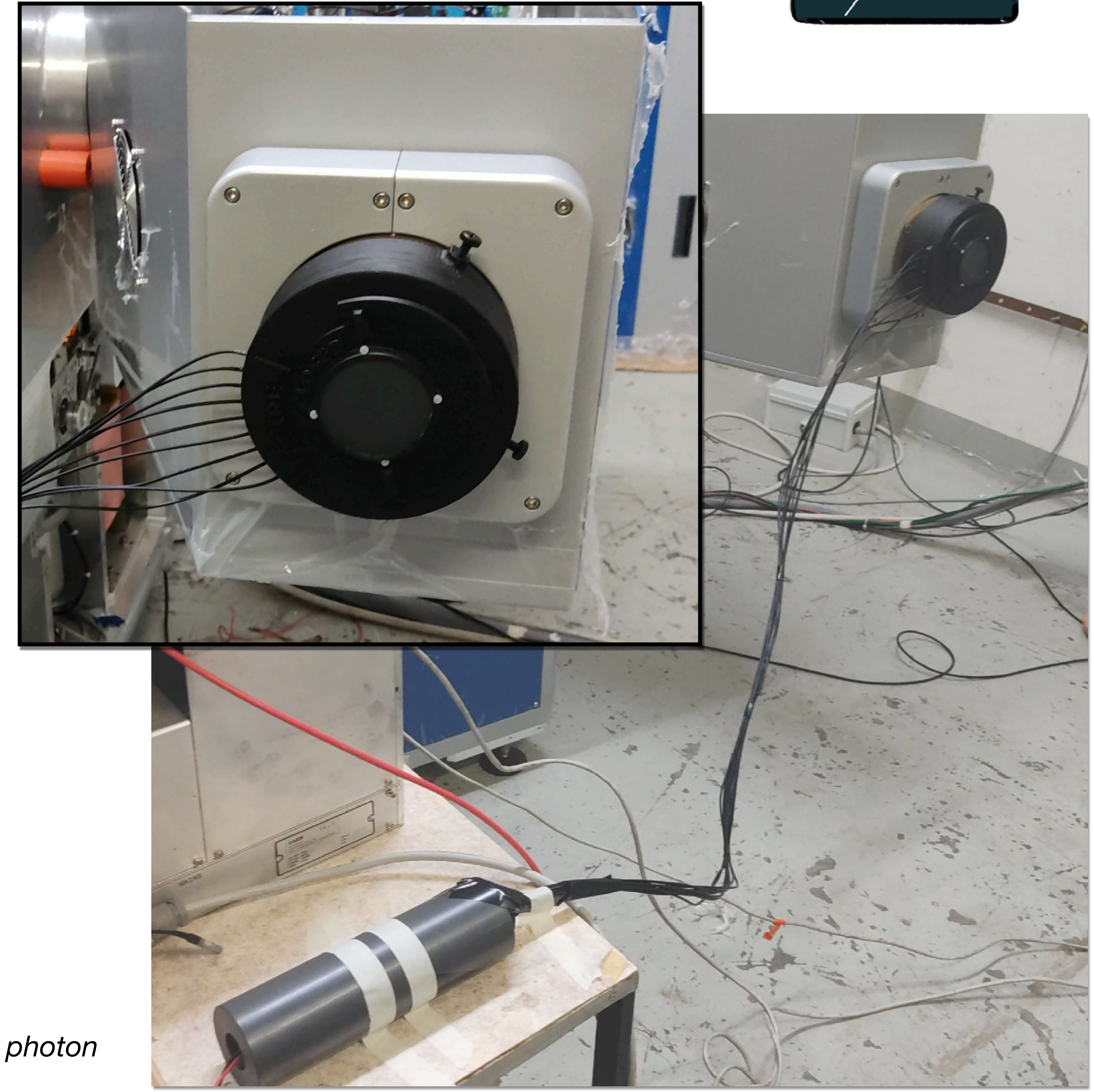
A linear response is observed over the full range of intensities explored.





FLASH beam monitoring

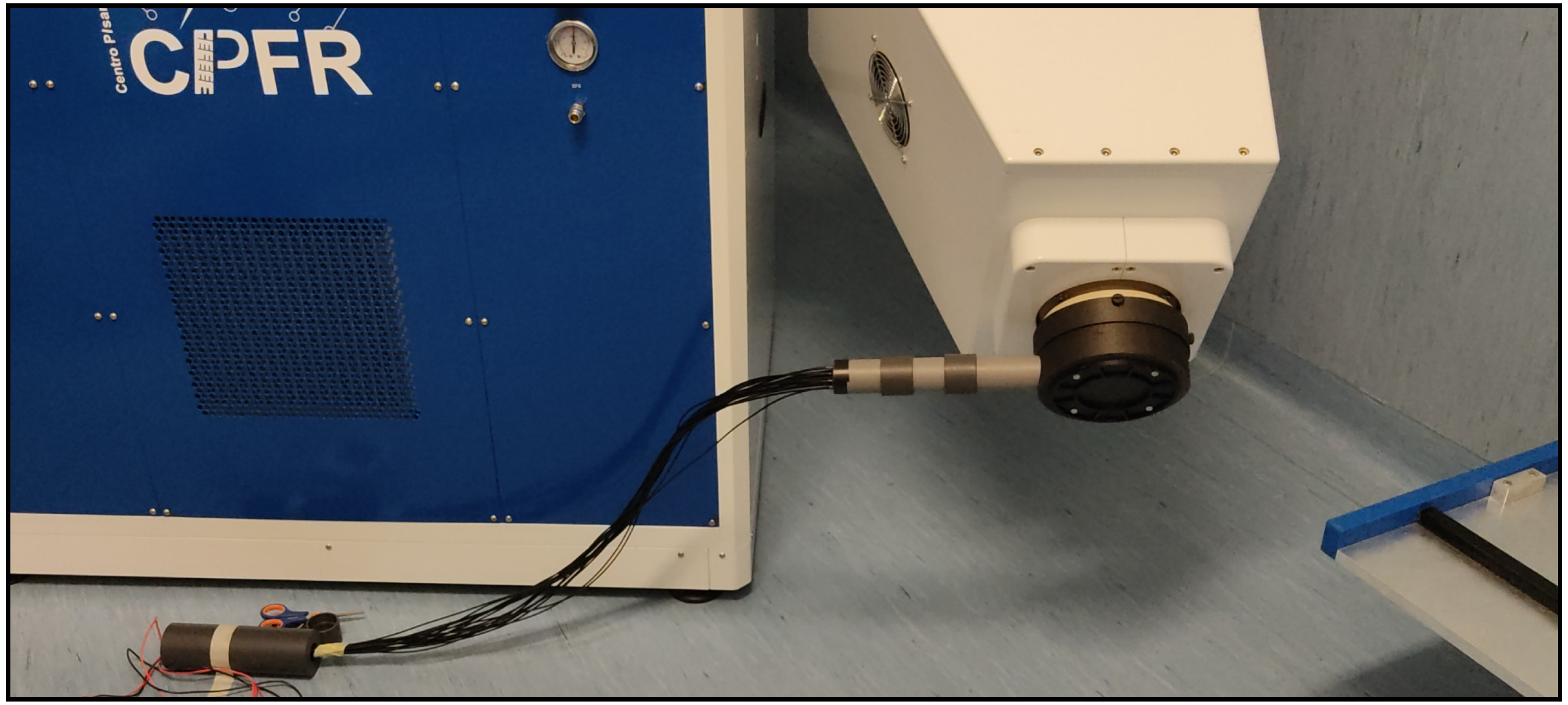
- Optimized detectors are under development in order to reduce both the background correlated with the beam and the impact on the beam line
- A new detector based on optical fibers could allow to drive and collect the fluorescence light far from the beam line.



- A preliminary measurement at SIT demonstrated that, even if we distance the light collection system from the beam, we are still not able to “switch off” the signal.
- **Cherenkov light** is produced inside the fibers [1]. The background is still too important.
- We need to further distance the system from the beam, carrying the light outside the room.

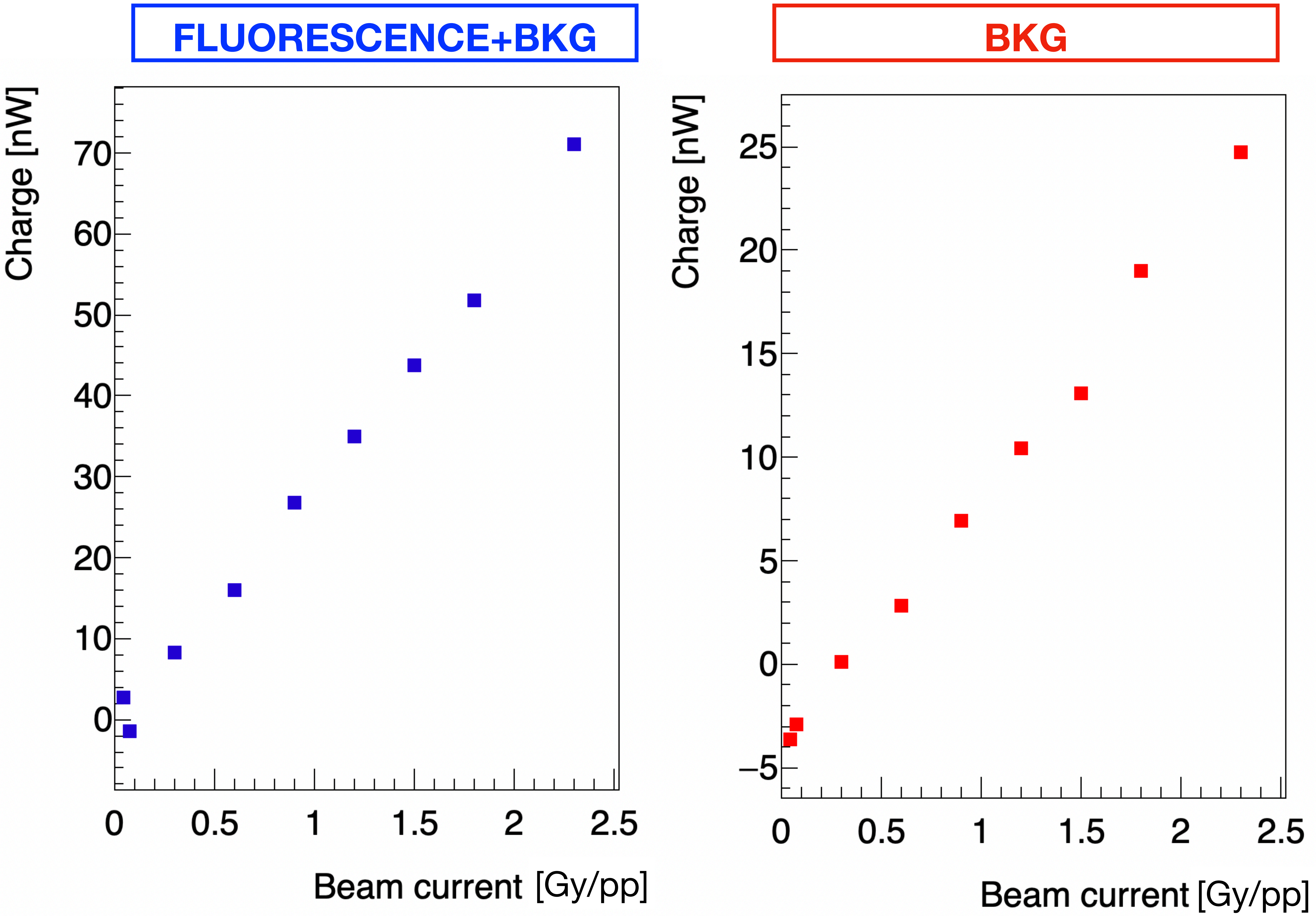
[1] Journal of Biomedical Optics, Vol. 18, Issue 2, 027001 (2013).
Kyoung Won Jang et al. *Application of Cerenkov radiation generated in plastic optical fibers for therapeutic photon beam dosimetry.* https://doi.org/10.1117/1.JBO.18.2.027001

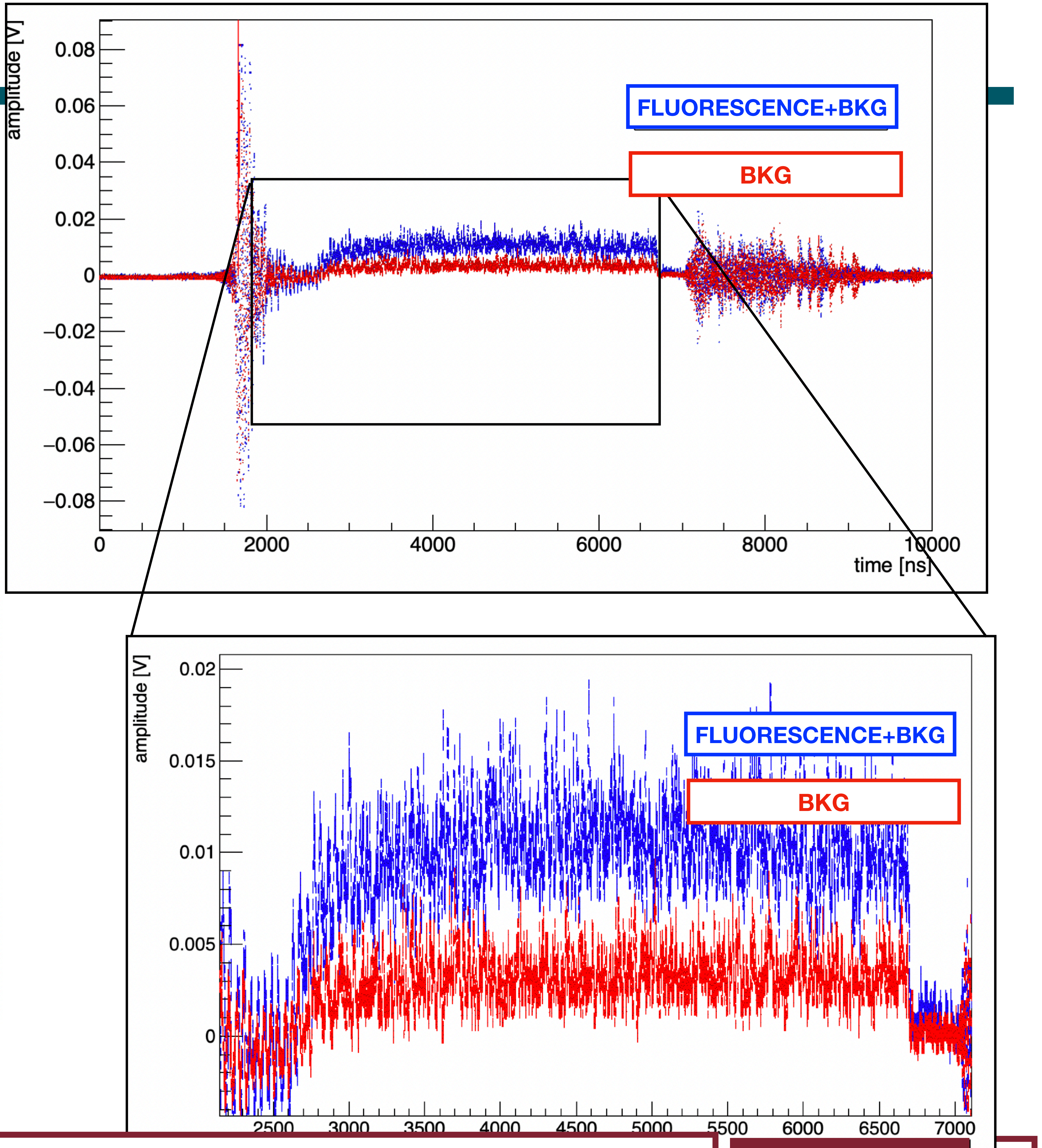
FLASH beam monitoring



- For our second round of testing at Pisa, we verified that, even at 2 m away from the machine, the fibers still produce background, so we remove them and put the PMT at 2 m from the beam exit window.
- The setup is, as usual, equipped with the possibility to measure also the background for each configuration and perform a background subtraction to evaluate the fluorescence contribution.

FLASH beam monitoring

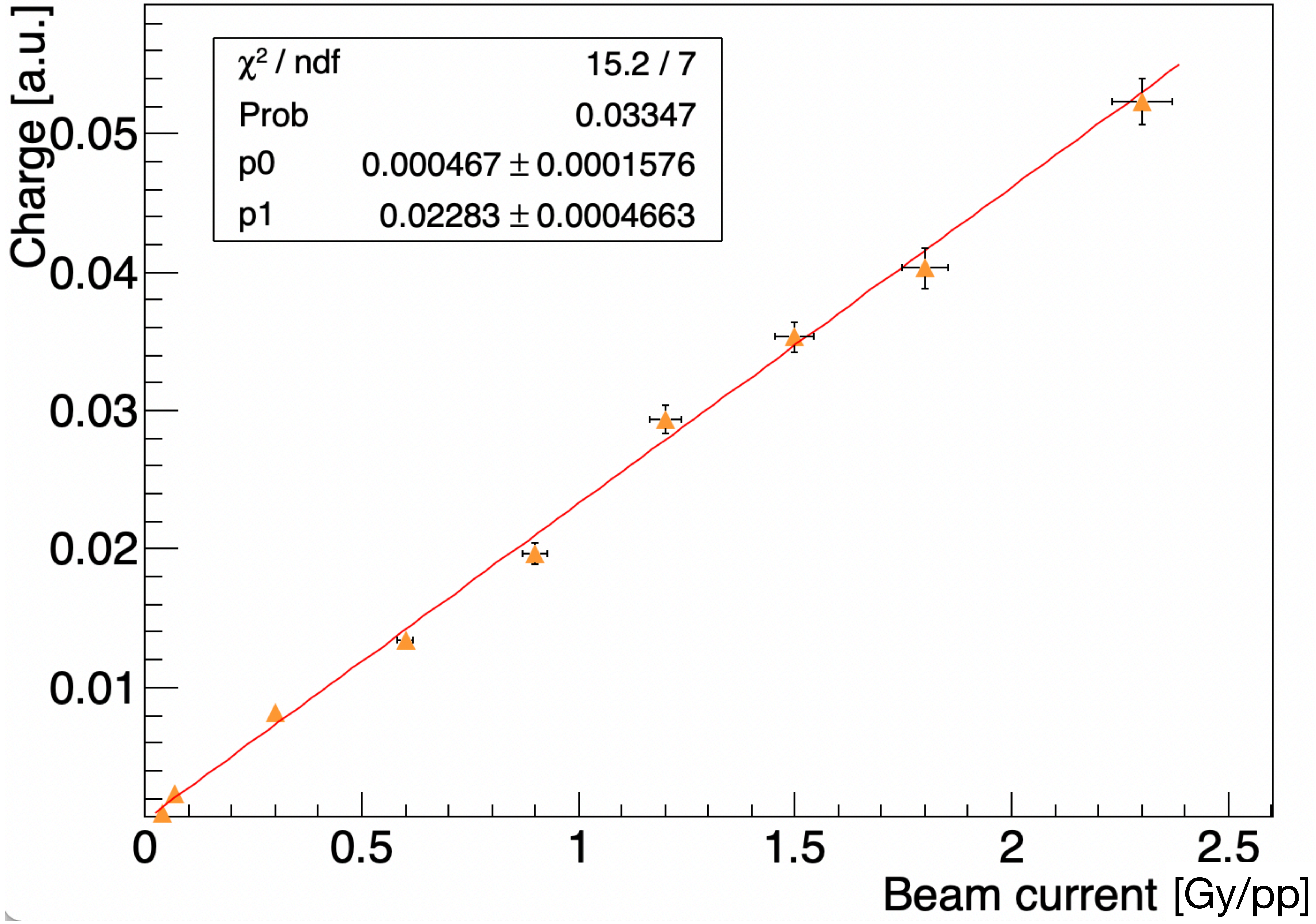


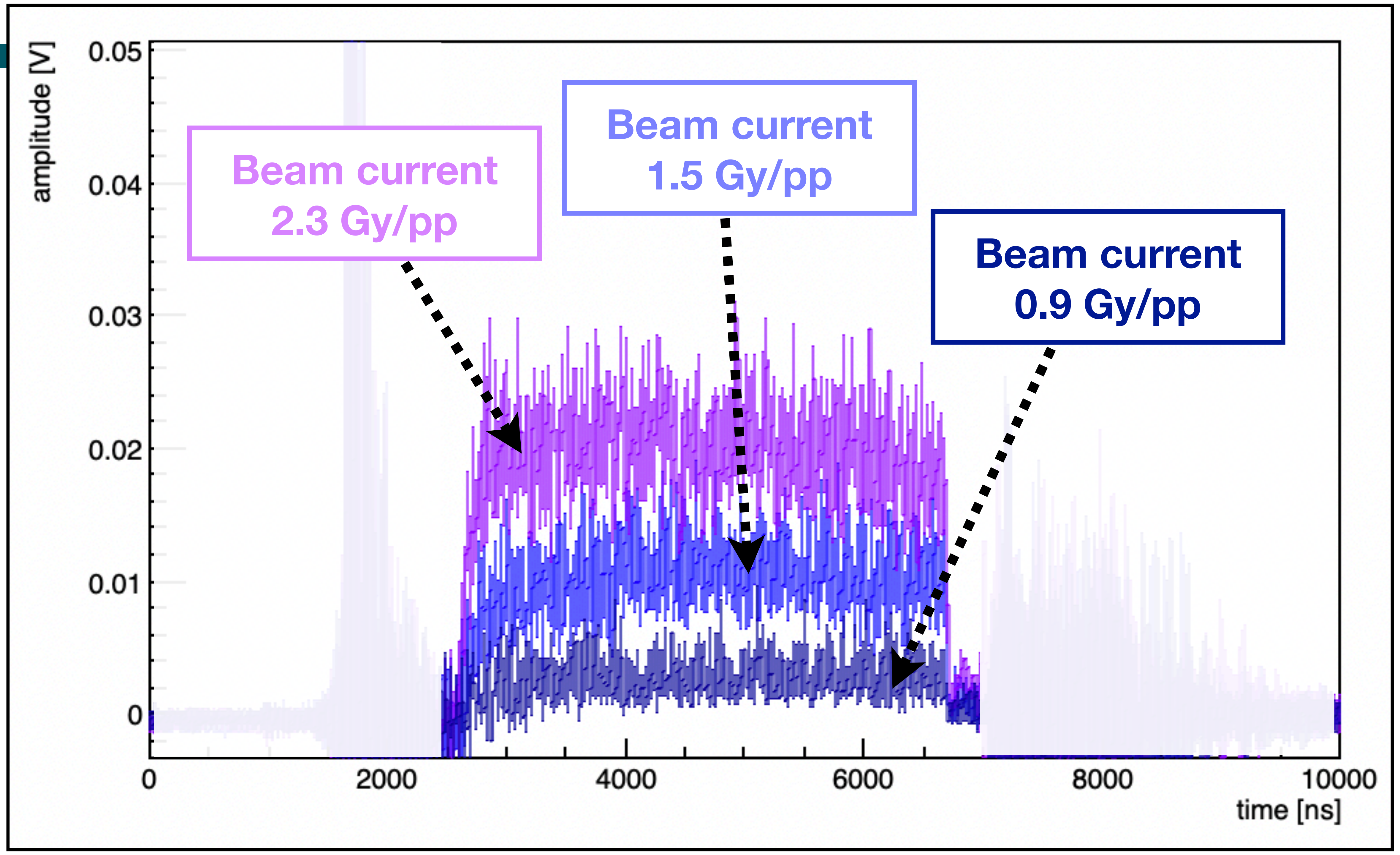


☑ S/N is still large.. but this is due to the readout system

FLASH beam monitoring

FLUORESCENCE



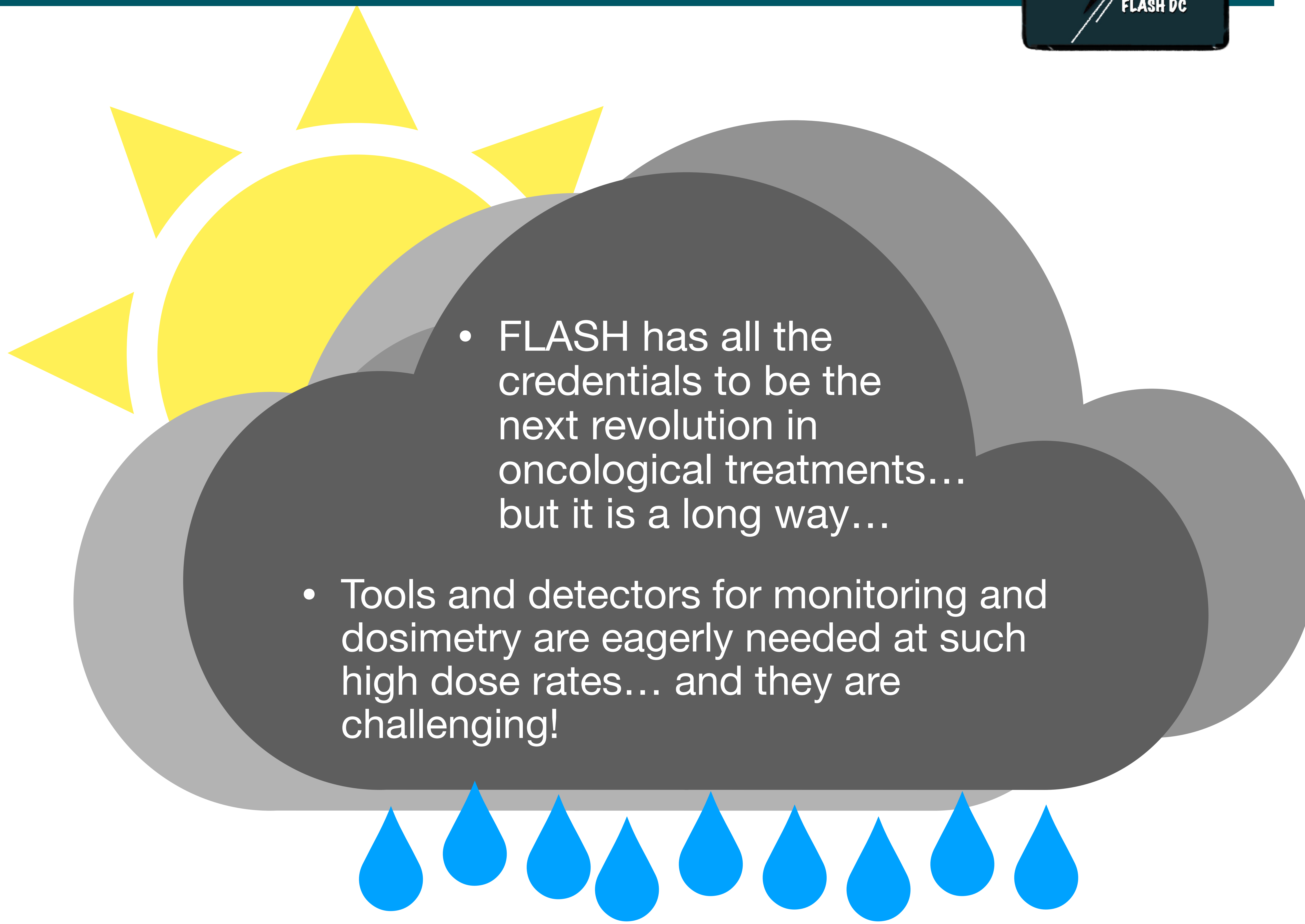


- ○ 3% syst. err on current
- ○ 3% syst.err$\oplus$stat.err on charge

- ☑ Fluorescence signal linearity as a function of the beam current is confirmed!
- ☑ The statistics is very low… only 30 pulses have been acquired (for each current).

Conclusions

- ☑ Definitely strong evidence that fluorescence signal has the expected linearity as a function of the beam current.
- ☐ The background in the readout system (PMT) is not negligible also at very large distances (only behind the wall of the room is zero).
- ☐ With this setup we have background of about 30%.
- ☑ Fluorescence is huge (we saturate easily at high currents).
- ☐ We had to reduce the acceptance with a diaphragm… this feature is necessary to avoid saturation of the PMT at high currents.
- ☑ We have a detector that has NO MATERIAL AT ALL on the beam line…



- FLASH has all the credentials to be the next revolution in oncological treatments… but it is a long way…
- Tools and detectors for monitoring and dosimetry are eagerly needed at such high dose rates… and they are challenging!

Conclusions

<u>**Thanks to:**</u>
Angelica De Gregorio, Valerio Di Domenico, Gaia Franciosini, Marco Garbini, Michela Marafini, Riccardo Mirabelli, Vincenzo Patera, Alessio Sarti, Angelo Schiavi, Adalberto Sciubba, Marco Toppi, Giacomo Traini

But it is so much fun!

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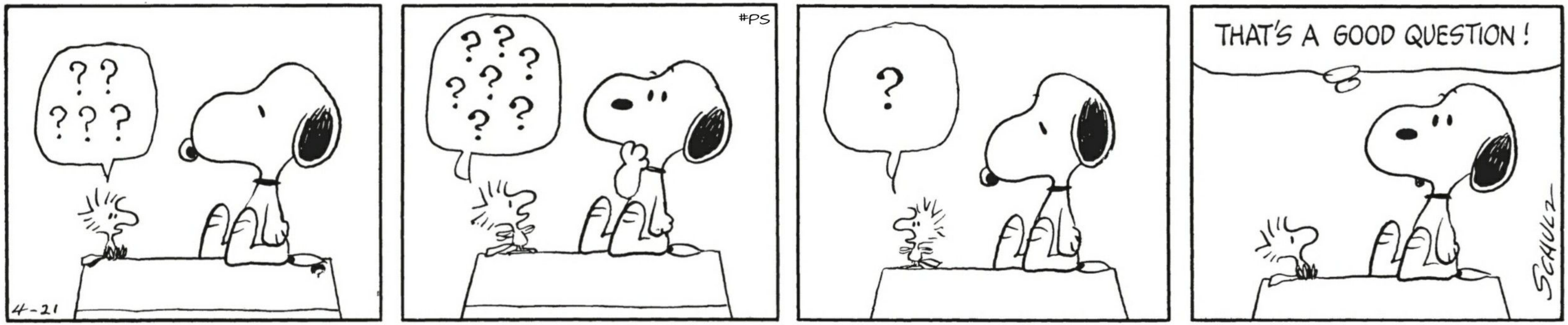
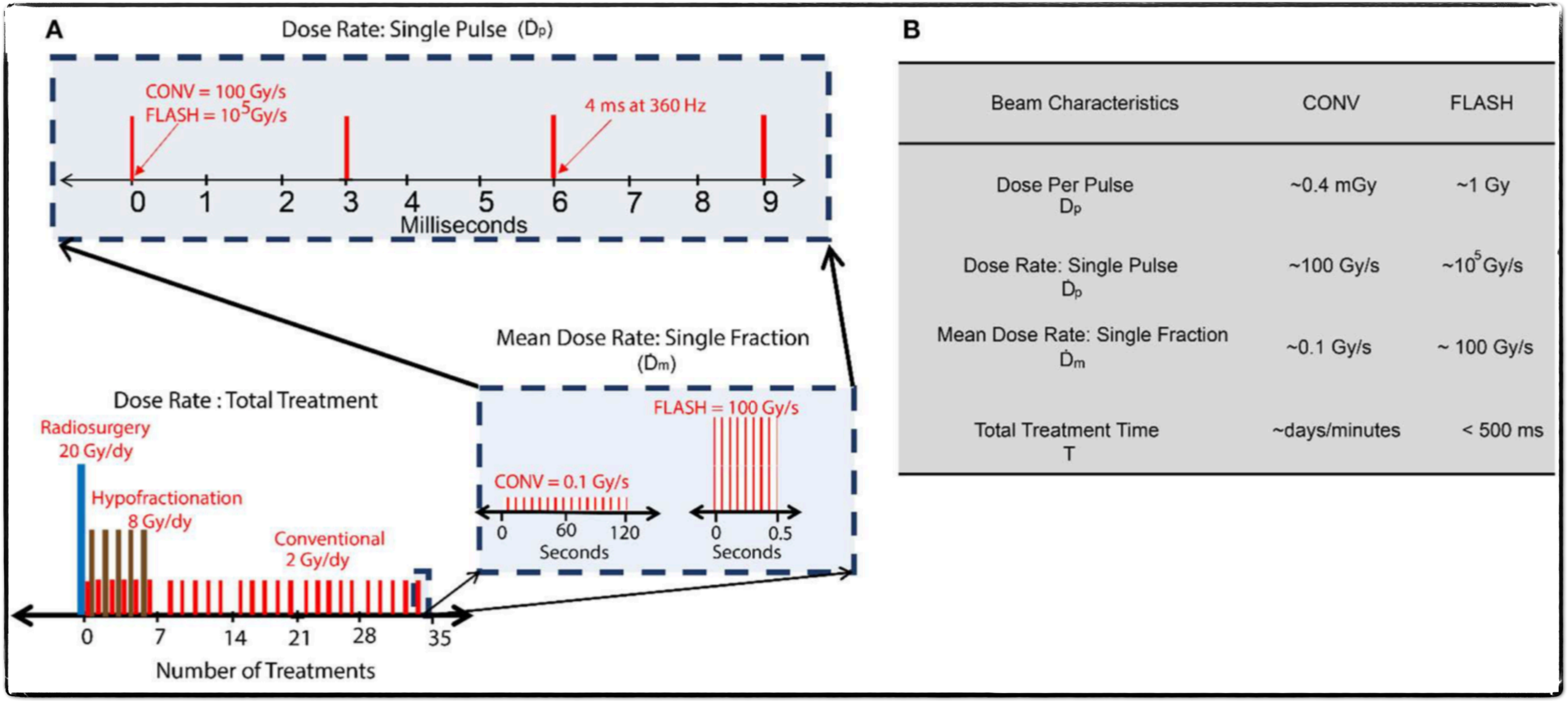
Thank you for your attention!



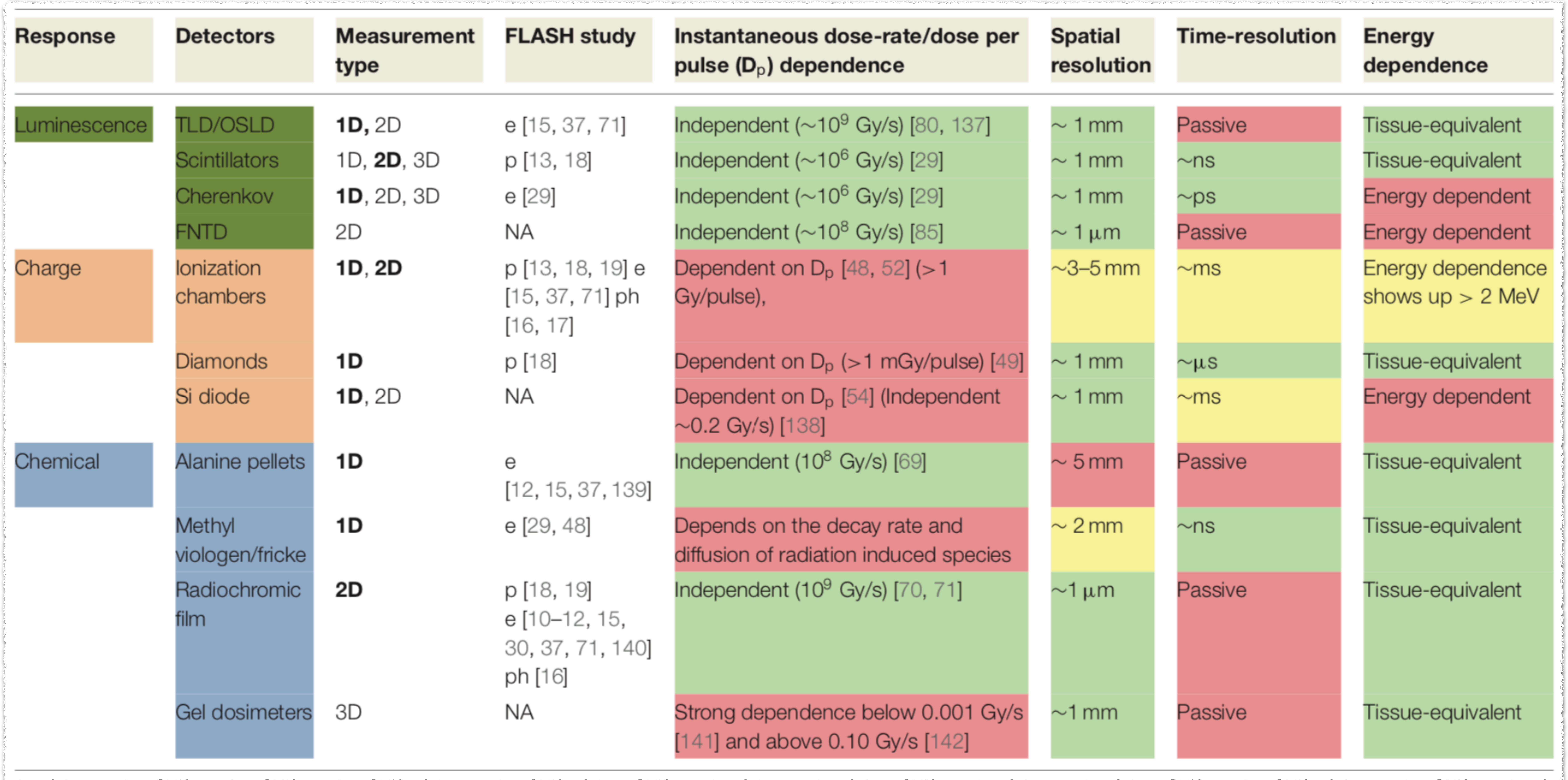
Backup

Ashraf MR, Rahman M, Zhang R, Williams BB, Gladstone DJ, Pogue BW and Bruza P (2020) Dosimetry for FLASH Radiotherapy: A Review of Tools and the Role of Radioluminescence and Cherenkov Emission. Front. Phys. 8:328. doi: 10.3389/fphy.2020.00328



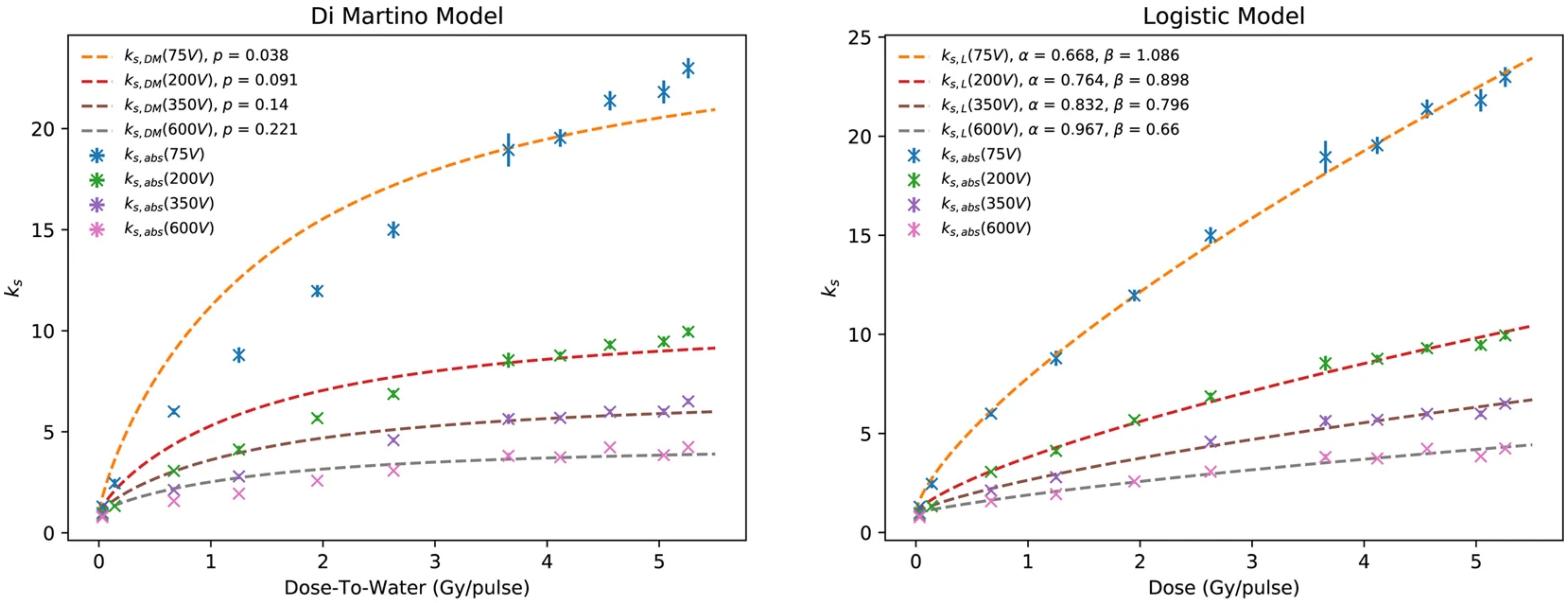
Beam Characteristics	CONV	FLASH
Dose Per Pulse D_p	~0.4 mGy	~1 Gy
Dose Rate: Single Pulse $\dot{D}_p$	~100 Gy/s	~10^5Gy/s
Mean Dose Rate: Single Fraction $\dot{D}_m$	~0.1 Gy/s	~ 100 Gy/s
Total Treatment Time T	~days/minutes	< 500 ms

Backup



Response	Detectors	Measurement type	FLASH study	Instantaneous dose-rate/dose per pulse (D_p) dependence	Spatial resolution	Time-resolution	Energy dependence
Luminescence	TLD/OSLD	**1D,** 2D	e [15, 37, 71]	Independent (~10^9 Gy/s) [80, 137]	~ 1 mm	Passive	Tissue-equivalent
	Scintillators	1D, **2D**, 3D	p [13, 18]	Independent (~10^6 Gy/s) [29]	~ 1 mm	~ns	Tissue-equivalent
	Cherenkov	**1D**, 2D, 3D	e [29]	Independent (~10^6 Gy/s) [29]	~ 1 mm	~ps	Energy dependent
	FNTD	2D	NA	Independent (~10^8 Gy/s) [85]	~ 1 μm	Passive	Energy dependent
Charge	Ionization chambers	**1D**, **2D**	p [13, 18, 19] e [15, 37, 71] ph [16, 17]	Dependent on D_p [48, 52] (> 1 Gy/pulse),	~3–5 mm	~ms	Energy dependence shows up > 2 MeV
	Diamonds	**1D**	p [18]	Dependent on D_p (>1 mGy/pulse) [49]	~ 1 mm	~μs	Tissue-equivalent
	Si diode	**1D**, 2D	NA	Dependent on D_p [54] (Independent ~0.2 Gy/s) [138]	~ 1 mm	~ms	Energy dependent
Chemical	Alanine pellets	**1D**	e [12, 15, 37, 139]	Independent (10^8 Gy/s) [69]	~ 5 mm	Passive	Tissue-equivalent
	Methyl viologen/fricke	**1D**	e [29, 48]	Depends on the decay rate and diffusion of radiation induced species	~ 2 mm	~ns	Tissue-equivalent
	Radiochromic film	**2D**	p [18, 19] e [10–12, 15, 30, 37, 71, 140] ph [16]	Independent (10^9 Gy/s) [70, 71]	~1 μm	Passive	Tissue-equivalent
	Gel dosimeters	3D	NA	Strong dependence below 0.001 Gy/s [141] and above 0.10 Gy/s [142]	~1 mm	Passive	Tissue-equivalent

Backup

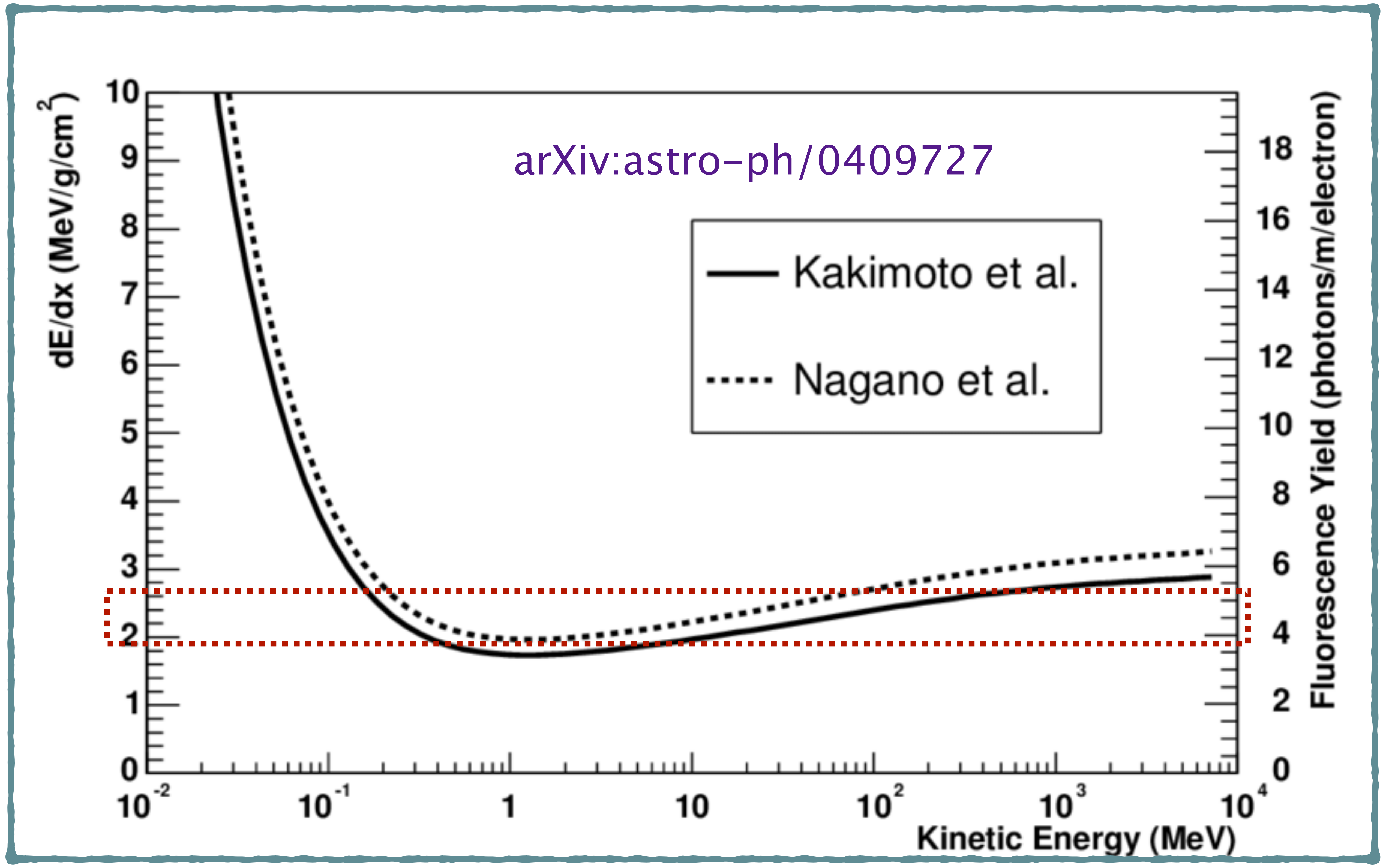


a doi: 10.1038/s41598-020-65819-y **b**

Backup

- How many photons we expect at typical IOeRT and VHEE energies?

E_K	ph./m (Fluor.)	ph./m (Ch.)
10 MeV	4 (@4π)	Under thr.
20 MeV	4 (@4π)	6 (@0.1°)
130 MeV	5 (@4π)	70 (@1.4°)



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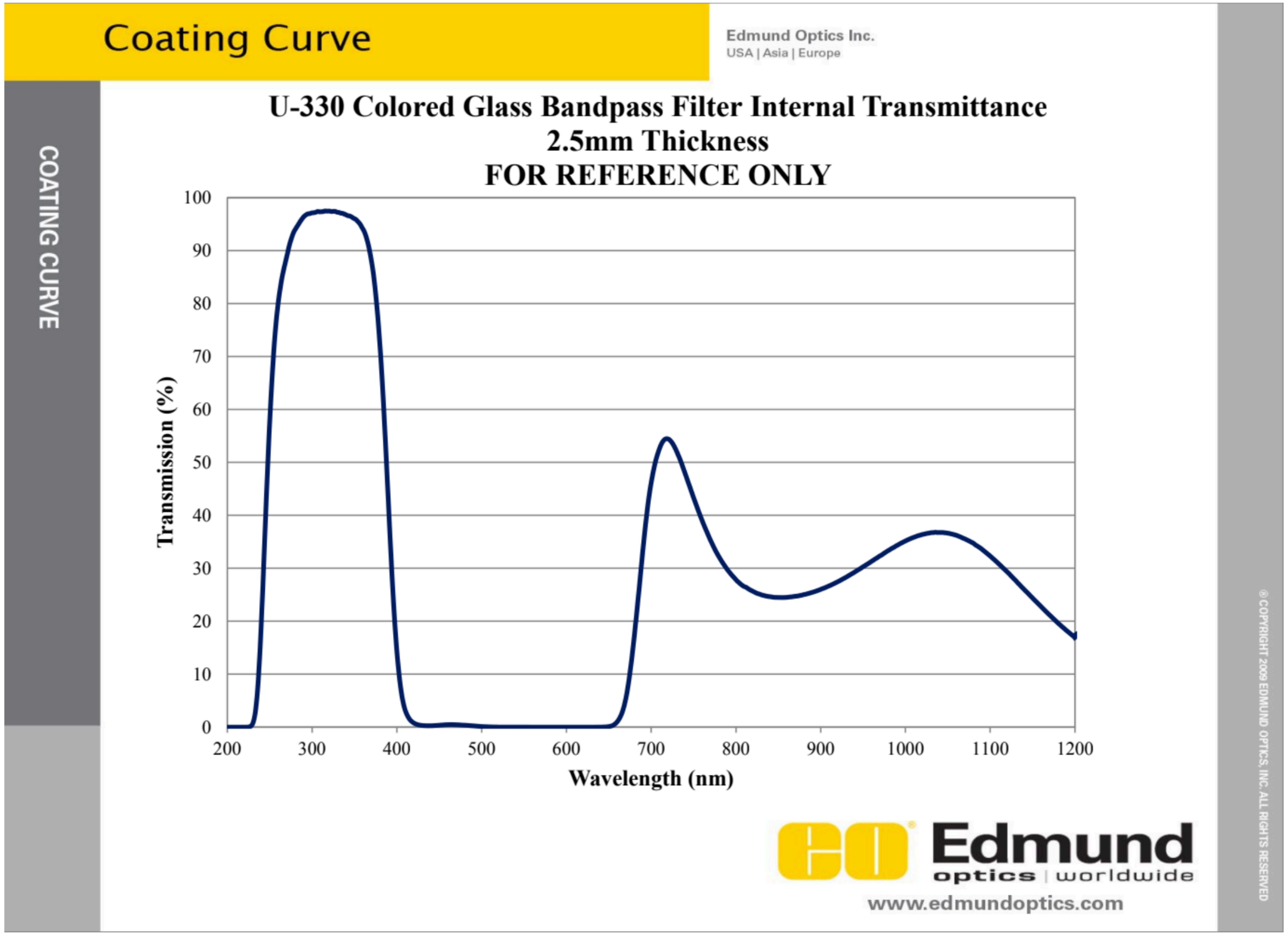
Coating Curve
Edmund Optics Inc.
USA | Asia | Europe
COATING CURVE
U-330 Colored Glass Bandpass Filter Internal Transmittance
2.5mm Thickness
FOR REFERENCE ONLY
Transmission (%)
100
90
80
70
60
50
40
30
20
10
0
200
300
400
500
600
700
800
900
1000
1100
1200
Wavelength (nm)
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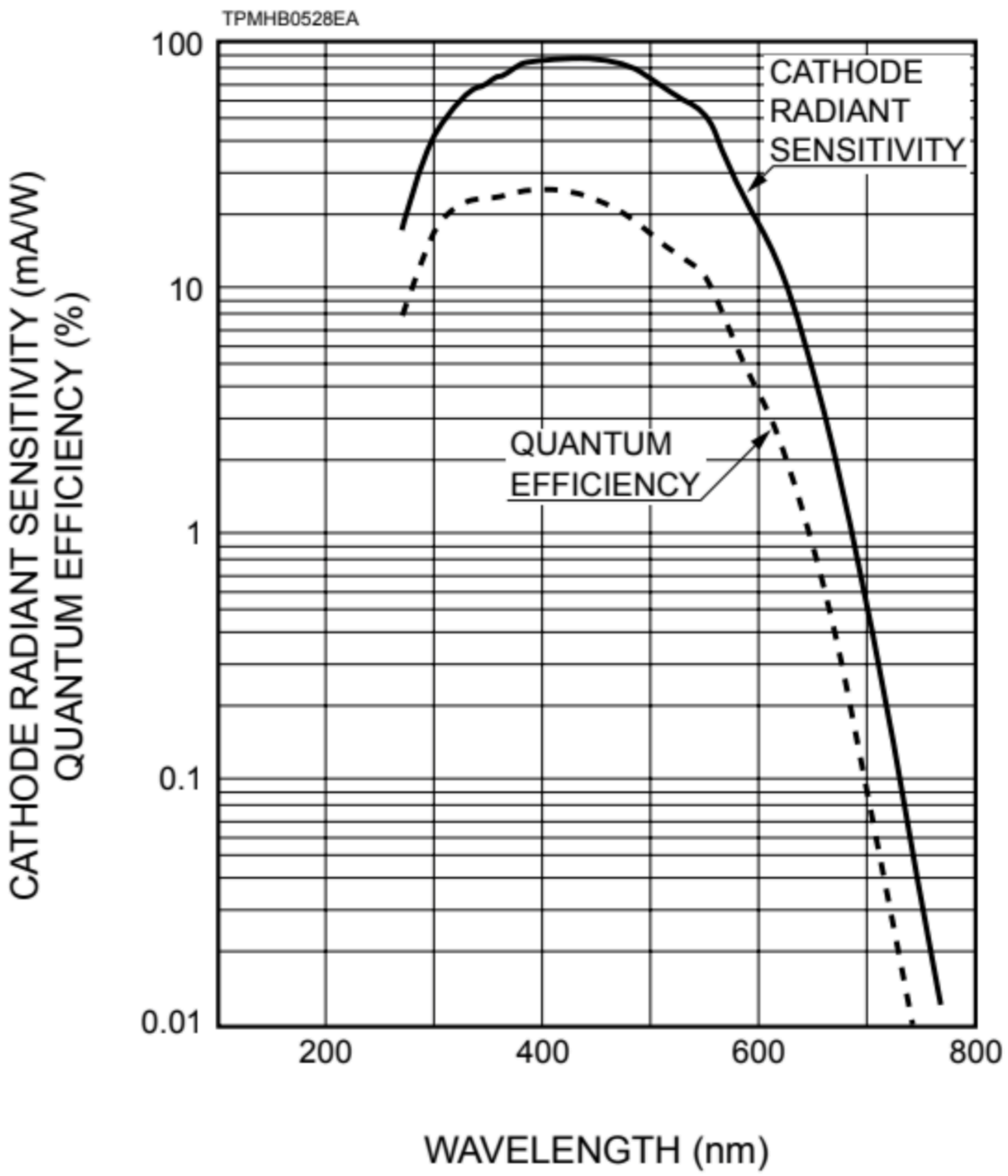
TPMHB0528EA
CATHODE RADIANT SENSITIVITY (mA/W)
QUANTUM EFFICIENCY (%)
100
10
1
0.1
0.01
CATHODE RADIANT SENSITIVITY
QUANTUM EFFICIENCY
200
400
600
800
WAVELENGTH (nm)

Backup

- A MC simulation has been developed to perform a model of the detection technique.
- It works well with the expected beam parameters (some of which are not present in the simulation, secondaries and uncertainties in the energy and angular divergence…)
- Introducing the measured parameters in this model we will continue with the optimization of the geometry.