



# REVIEW on a few relevant techniques in super-res microscopy

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7<sup>TH</sup> NIC@IIT ADVANCED MICROSCOPY PRACTICAL WORKSHOP

# Point Spread Function

## IMAGE FORMATION

## SYSTEM RESOLUTION

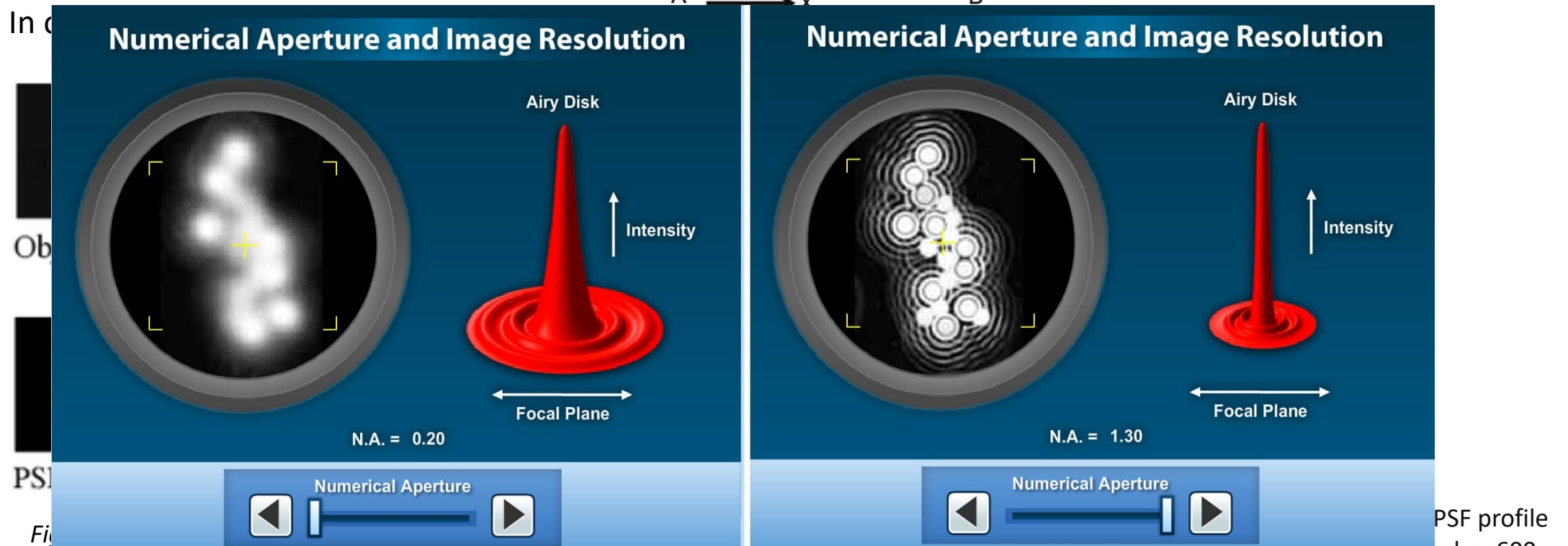


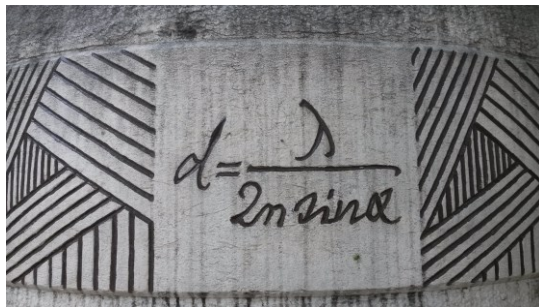
Fig. 1. PSF profile for a wide-field microscope.

for a wide-field microscope in the xy-plane (scale bar 200 nm) and xz-plane (scale bar 600 nm); **B** two particles at resolvable and unresolvable distances as seen in a microscope.

# SUPER-RESOLUTION MICROSCOPY

Microscopy techniques that allow to reach a **resolution higher** than the one imposed by the Abbe diffraction limit.

## Abbe diffraction limit



“Maximum resolution possible for a theoretically perfect, or ideal, optical system”

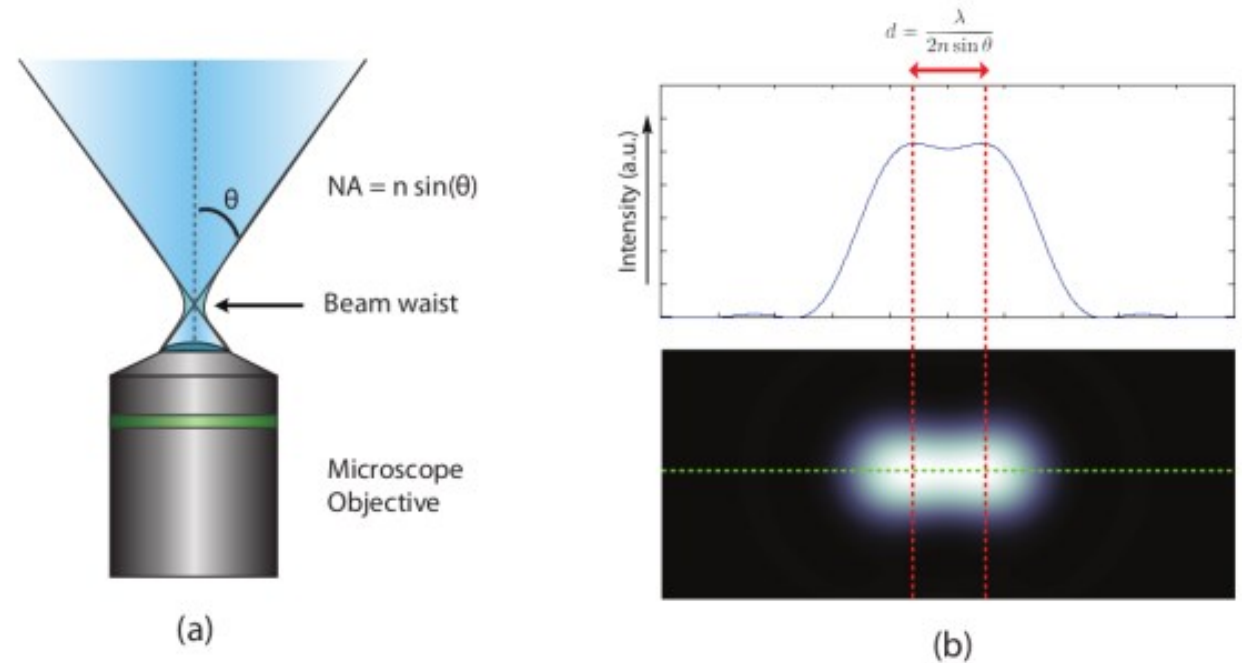


Figure 3 [10] – diffraction limit.  $d$  is the smallest resolvable distance between two points

# EXAMPLES of SUPER-RES TECHNIQUES

- *Structured Illumination Microscopy*
- *Stimulated Emission Depleted Microscopy*
- *Stochastic Optical Reconstruction Microscopy*

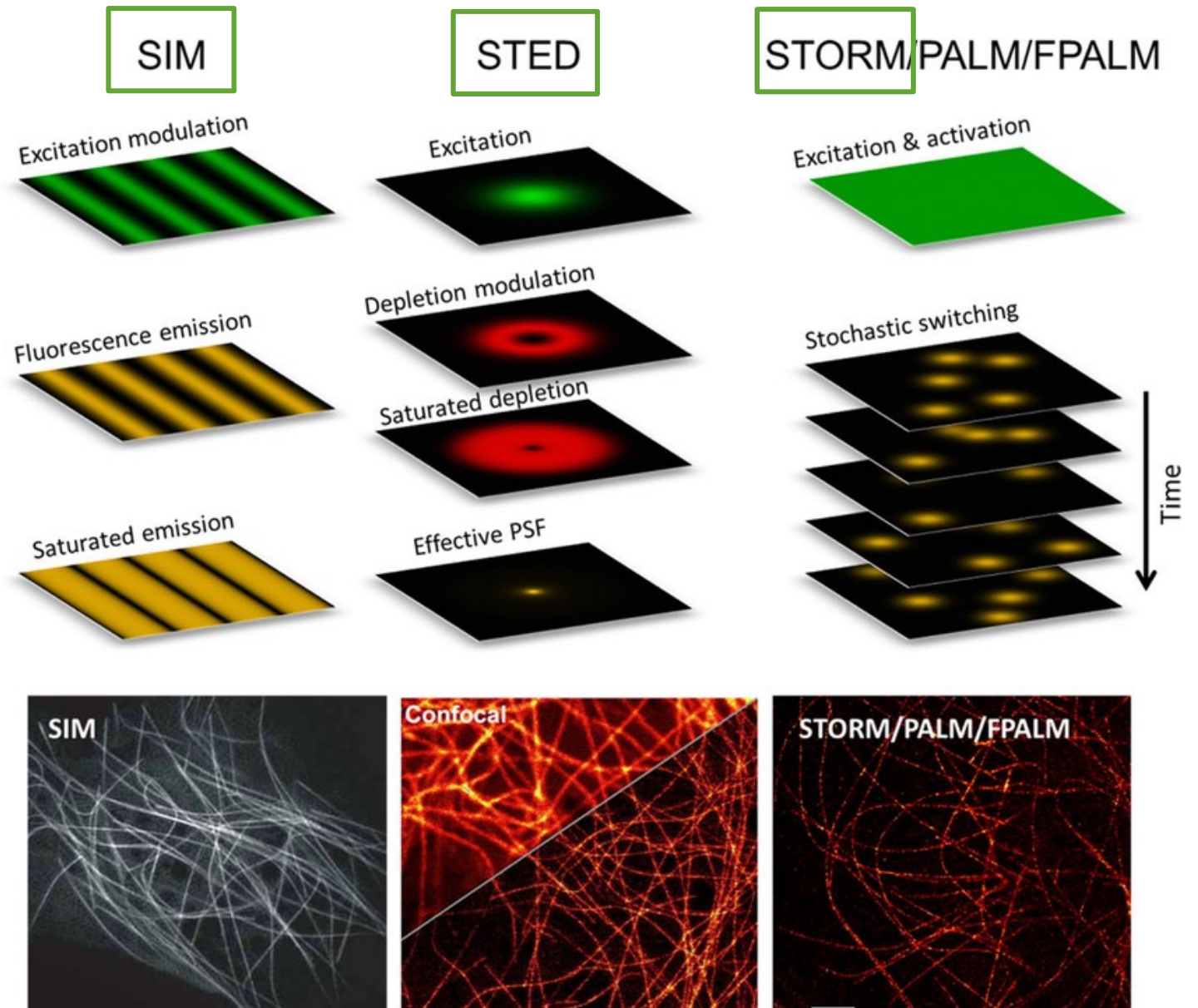
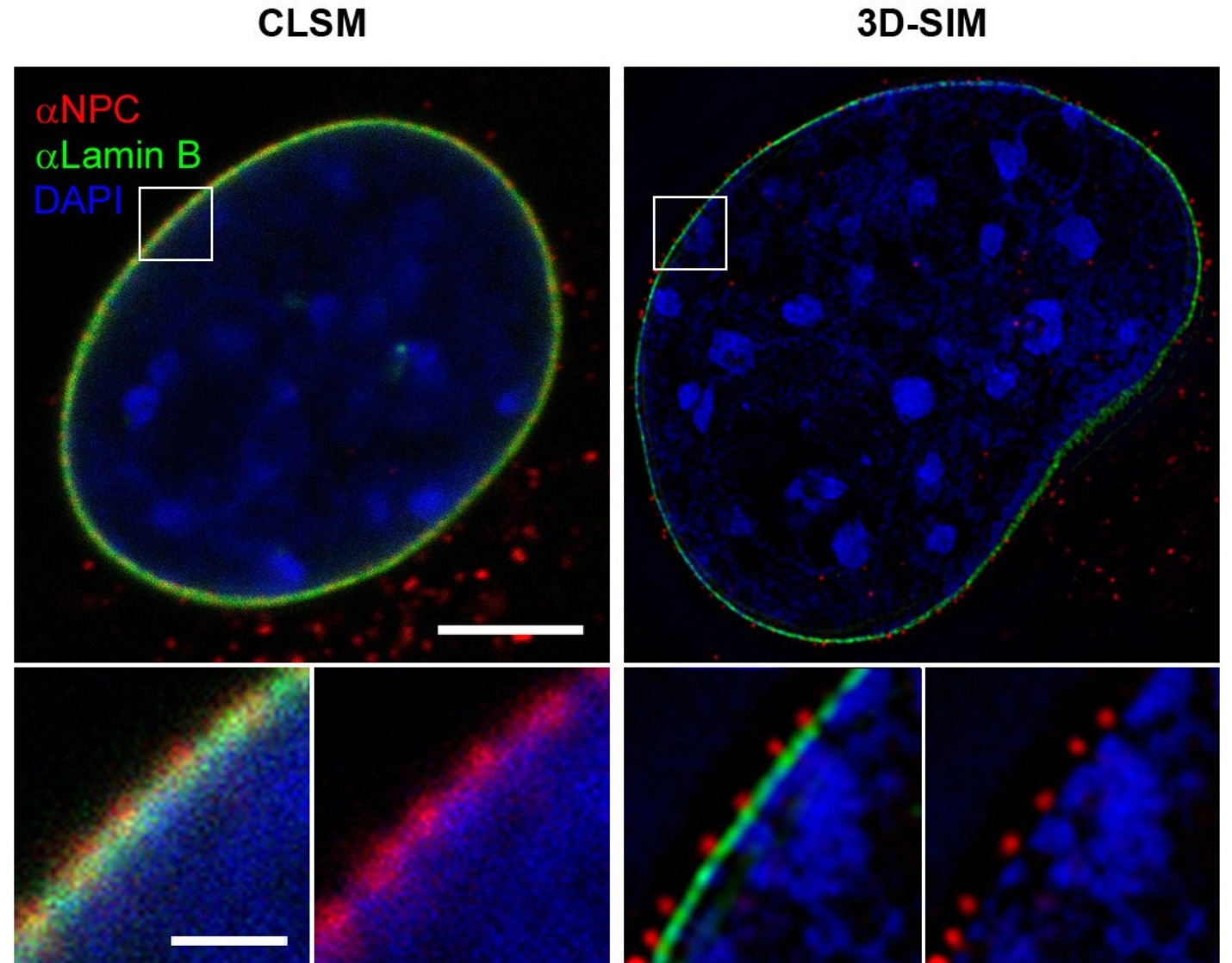


Figure 4 [11] – different super-resolution techniques

# SIM

## Structured Illumination Microscopy

**Principle:** sample excited with a known spatially structured pattern of light, it relies on the generation of **interference** patterns known as Moiré effect



*Figure 5* [12] – Simultaneous imaging of DNA, nuclear lamina, and NPC epitopes by 3D-SIM. C2C12 cells are immunostained with antibodies against lamin B (green) and antibodies that recognize different NPC epitopes (red). DNA is counterstained with DAPI (blue).

# GENERAL FEATURES

- Laser-based **wide-field** microscopy
- Movable diffraction **grating** into the excitation beam path
- Laser beams ( $\pm 1$ ) **interfere** with each other at the focal plane of the objective and create an illumination in stripes
- This **stripe pattern** by its superimposition with the **sample** generates a so-called **Moiré effect**

Overlap between the high frequency organization of the objects and the high frequency of the illumination stripes  $\rightarrow$  pattern of **lower frequency** well collected by the objective

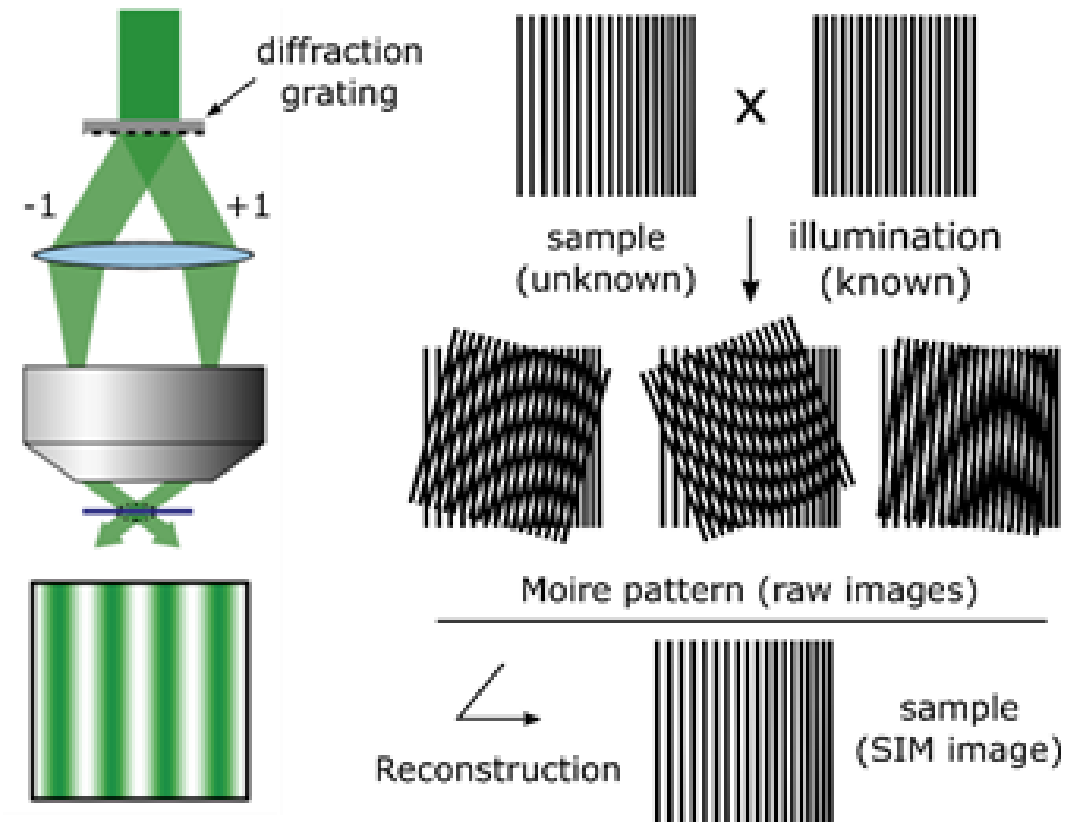


Figure 6 [13] – Moiré pattern formation

# IMAGE RECONSTRUCTION

- Shift and change of the orientations of the illuminating bands → **image reconstruction**
- Number of shifts and rotations depends if 2D or 3D, in order to cover a certain Fourier Space

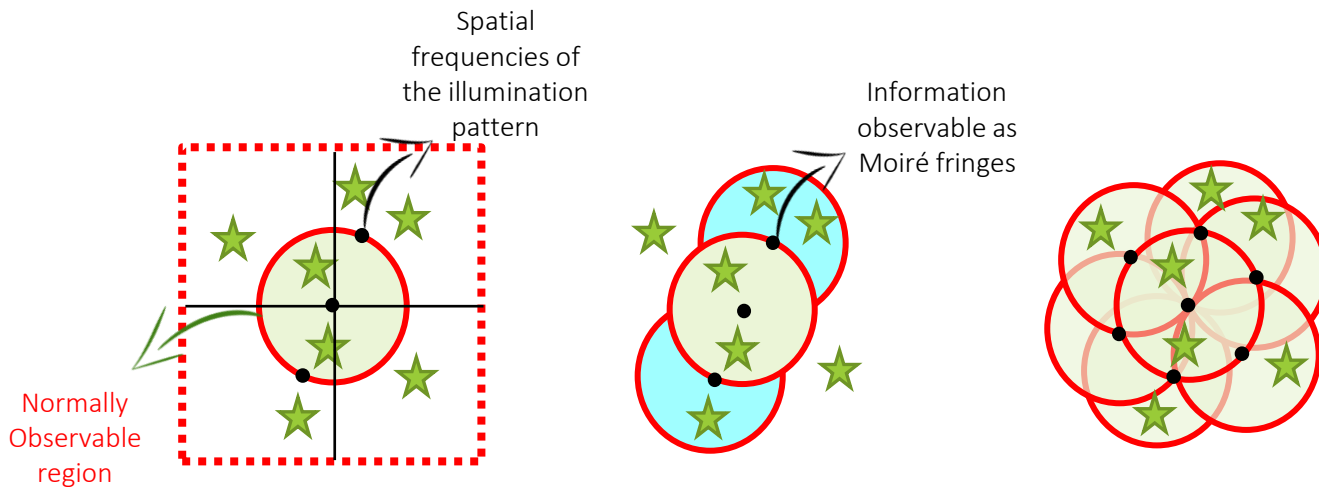
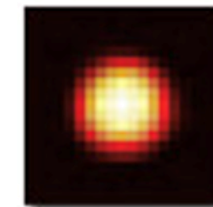
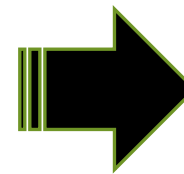
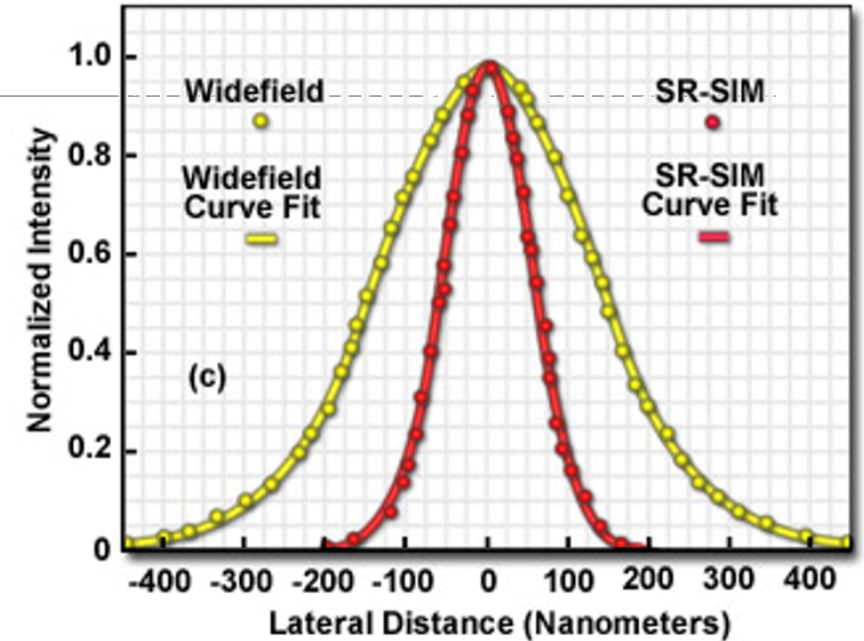


Figure 7 [6] – comparison between widefield and SR – SIM PSFs



Widefield PSF



SR-SIM PSF

# OPTICAL SETUP

- **Laser** source directed into the microscope optical train
- The light is directed through a polarizer and a **diffraction grating** and is then projected onto the specimen
- The rays are **collimated** by the objective in the specimen focal plane where they **interfere** and generate a three-dimensional illumination pattern
- Fluorescence emission is captured by a **CCD camera**

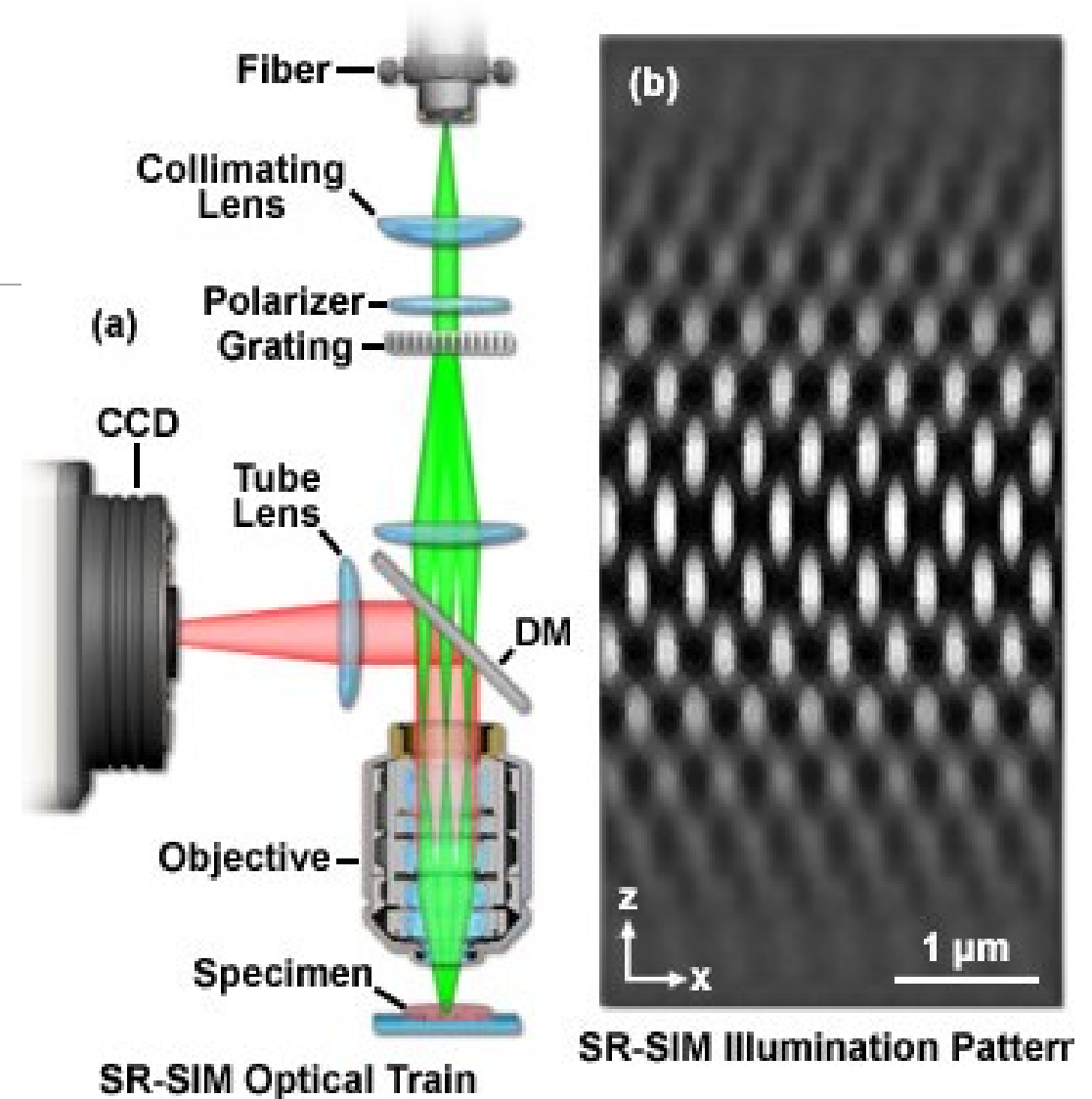


Figure 8 [6] – SR – SIM optical setup



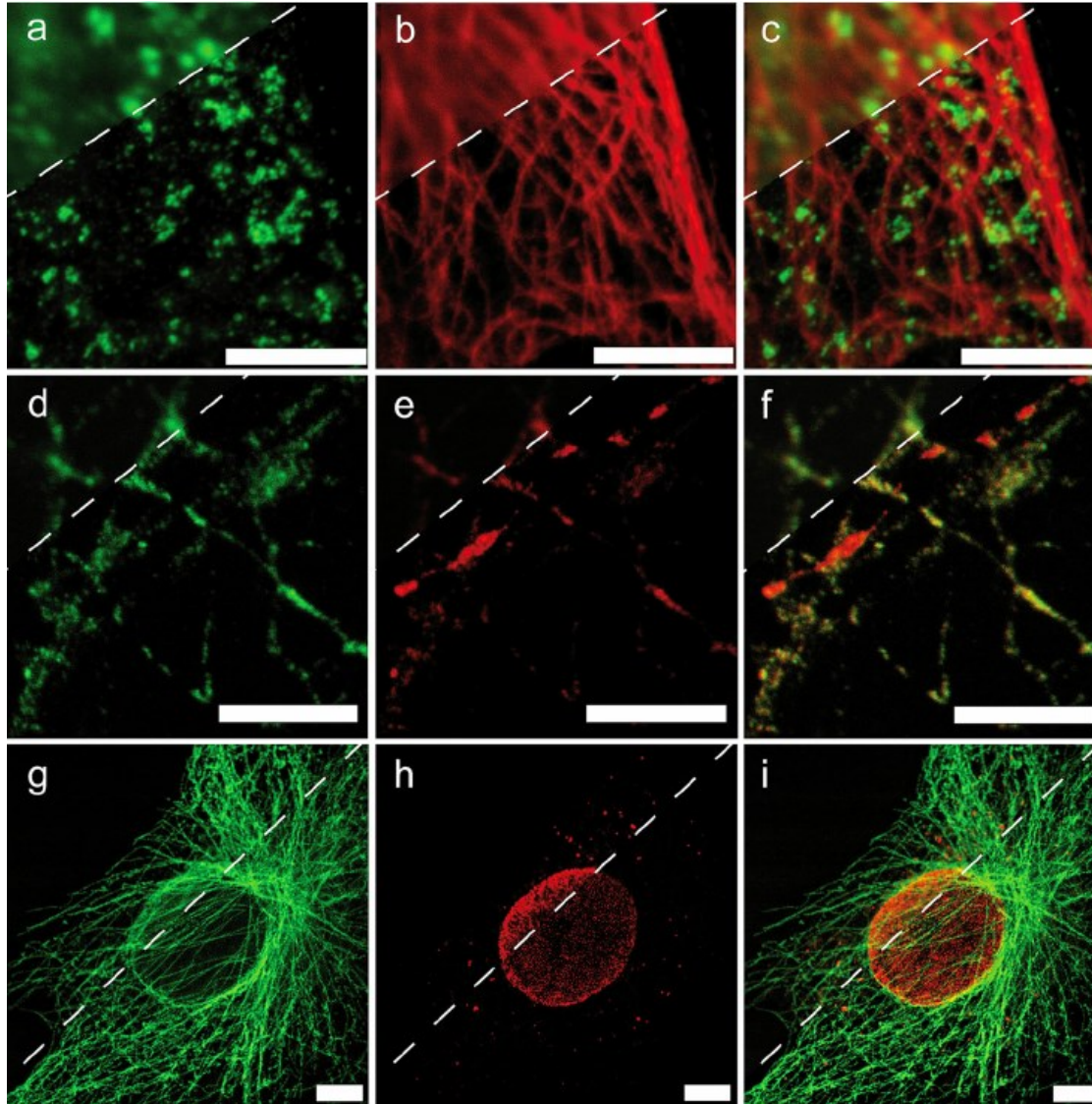
# PROS & CONS

- Increased resolution (100nm lateral and 250nm axial)
- Fast frame rate of imaging (high **temporal resolution**), being wide-field
- Use of **conventional** fluorophores

- Obtained resolution not as good as STORM/PALM and STED (~20nm)
- Possible **artefacts** during image reconstruction
- Sensitive to out of focus light → difficult with dense/thick samples



*Figure 9 [14] – Capture multiple images with structured illumination that is shifted in phase. Repeat this process for three different angles. These images are then processed using advanced algorithms to obtain super-resolution images.*



**Principle:** switching off the fluorescence of dye molecules by **stimulated emission** using intense laser light in the outer regions of the diffraction limited excitation focus, and detecting the **fluorescence** from dye in the center

# STED

*Stimulated Emission  
Depletion Microscopy*

Figure 10 [8] – Multicolor STED imaging.  
Confocal – STED.  
a – c: **HeLa cells** in which clathrin is stained by ATTO 590 ( green ) and tubulin by ATTO647N ( red )  
d – f: Culture of **hippocampal neurons** in which Syn1 is labeled with ATTO 594 ( green ) and vGAT with Abberior STAR635p ( red )

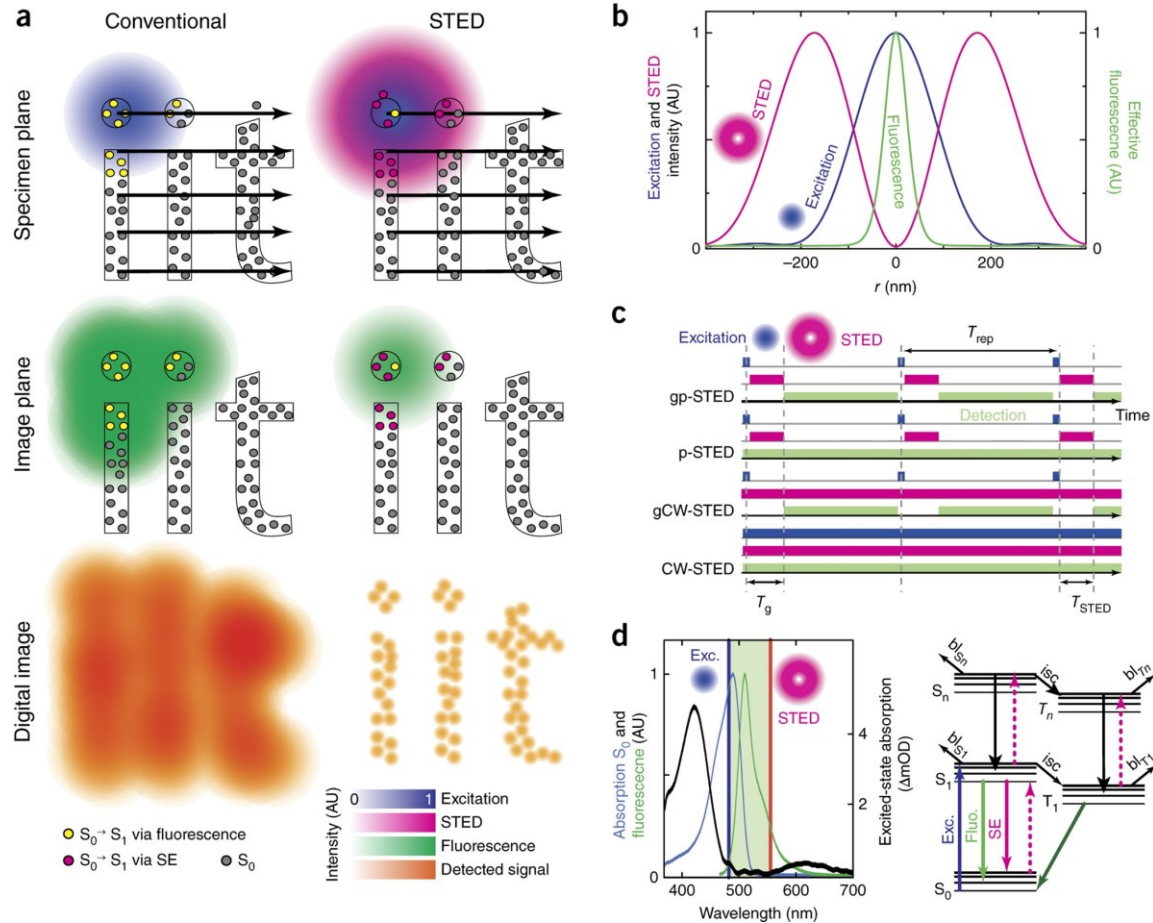


Figure 11 [7] – (a) Conventional scanning microscope (left) and a STED microscope (right). (b) Spatial conditions. (c) Temporal conditions (d) Spectral conditions.

# GENERAL FEATURES

- Pulsed lasers in relation to the time scales for **molecular relaxation** → radially symmetric depletion zones (**non-linear depletion**)
- **Phase modulator** modifies the STED beam → zero-intensity node at the center of focus with exponentially growing intensity toward the periphery
- Fluorophores within the **zero-node** region → fluorescence
- Fluorophores exposed to the STED beam → back to their ground state by means of **stimulated emission**
- High depletion laser powers (often  $>250 \text{ MW/cm}^2$ ) → **instantaneously** to the ground state
- Reducing laser power → formation of a **non-fluorescent state** different mechanisms (metastable triplet state, formation of charge-transfer states, or photoswitching)

# OPTICAL SETUP

- Synchronized ultrafast **lasers** pulses: the STED beam is red-shifted, 10-300 ps width (exc. shorter)
- **Phase plates** for the doughnut shape → quenching of the molecules at the periphery
- **Raster scanning** across the sample
- Single photon **detectors** (Single Photon Avalanche Diodes, SPADs)
- **Dichroic mirror**, to overlay excitation and depletion lasers and to separate fluorescence signal from excitation light
- Objective

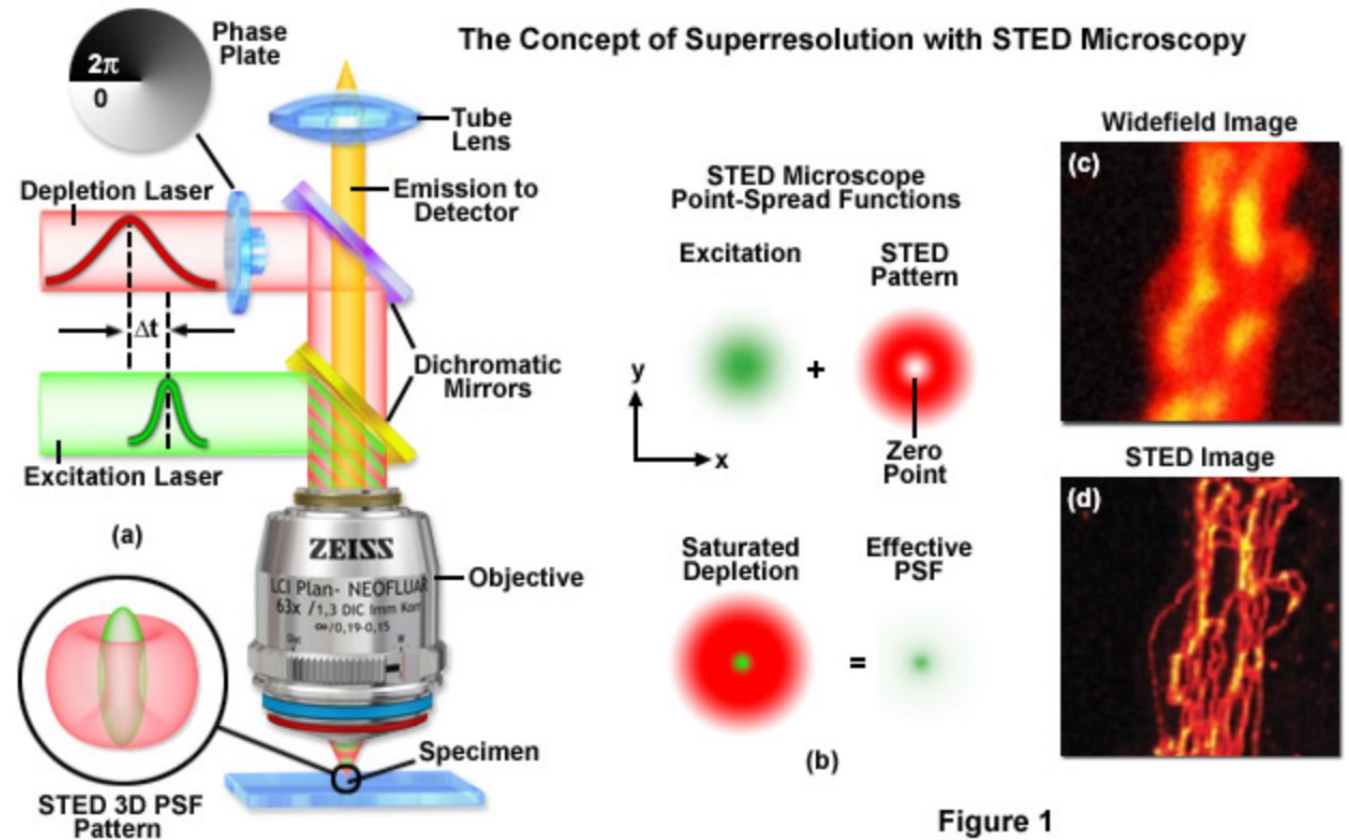
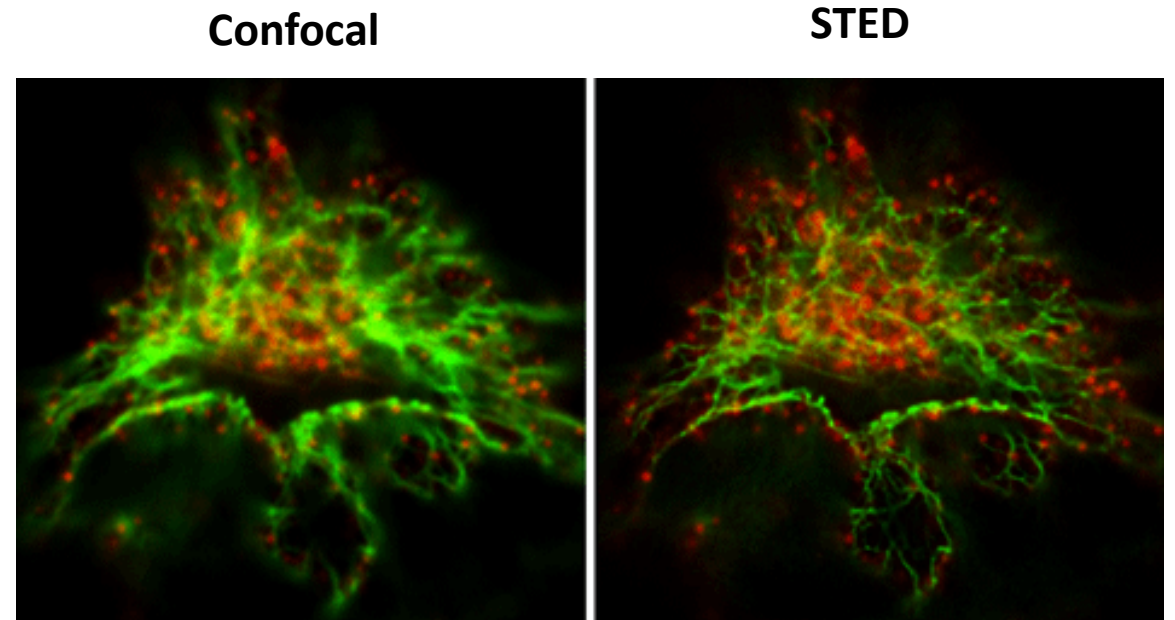


Figure 12 [8] – excitation and depletion lasers, focal spots produced by those lasers and comparison of widefield and STED images of microtubules (with Alexa 594)

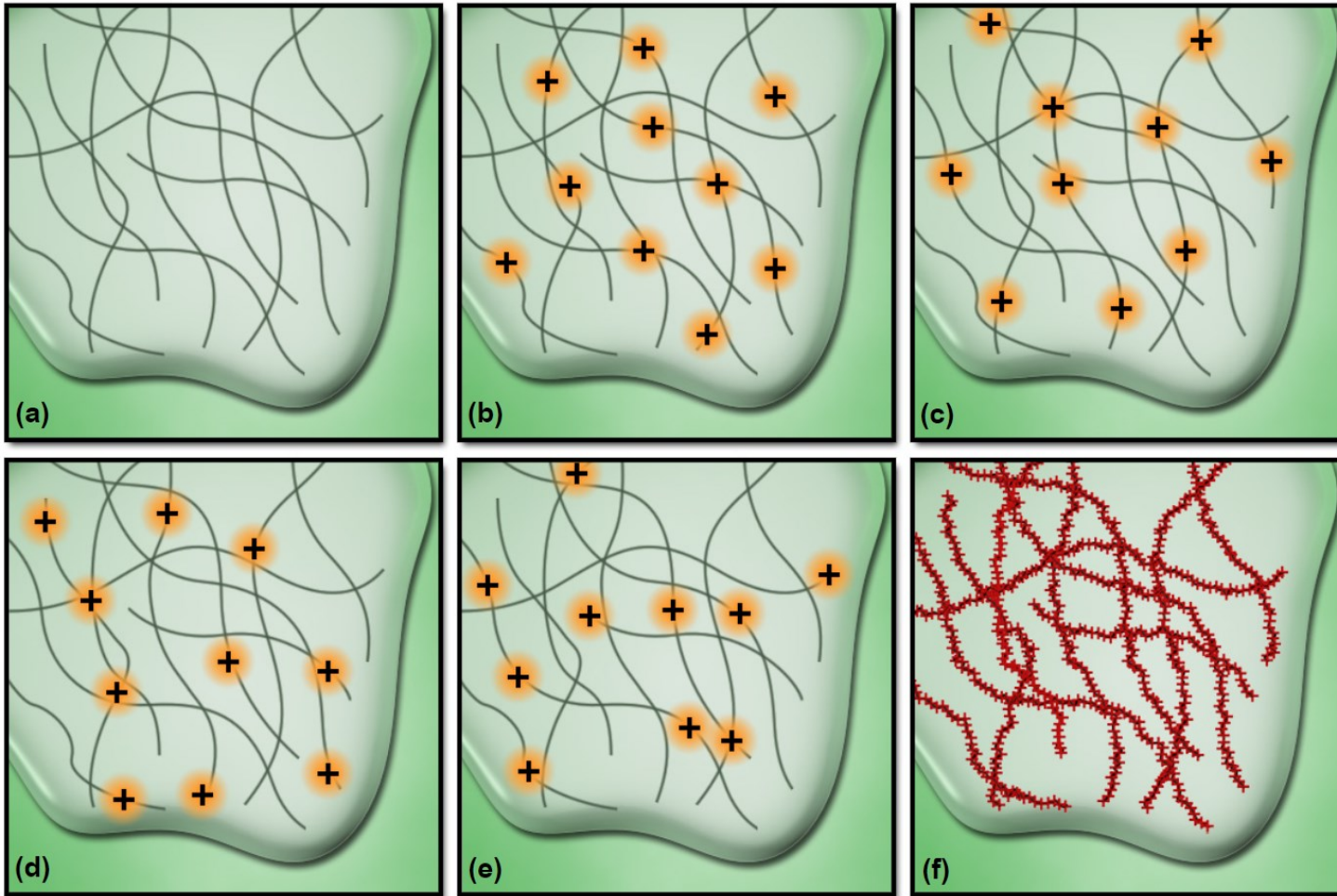
# REMARKS

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- Further resolution enhancement → **time gates** to the collected data (gSTED)
- Another benefit: resolution increased only due to the **experimental configuration and laser power**
- Image **acquisition times** can approach the speed of any laser scanning confocal microscope
- The effective resolution increase is proportional to the **power** of the depletion laser → problematic at extremely high laser powers
- Wide range of fluorophores have been successfully used with STED, including fluorescent proteins, ATTO dyes, Alexa Fluors, DyLights, and several other synthetics.



*Figure 13* [16] – Comparison of confocal microscopy and STED microscopy. Vimentin and clathrin were visualized by immunohistological co-staining.



**Principle:** the activated state of a *photoswitchable* molecule must lead to the consecutive emission of sufficient photons to enable *precise localization* before it enters a dark state or becomes deactivated by photobleaching

# STORM

*Stochastic Optical  
Reconstruction Microscopy*

Figure 14 [1] – Basic principles of STORM Superresolution Imaging

# GENERAL FEATURES

**Methodology:** turn on and off single fluorophores (stochastically) then **fit** the PSF to find their center, until they are all exhausted

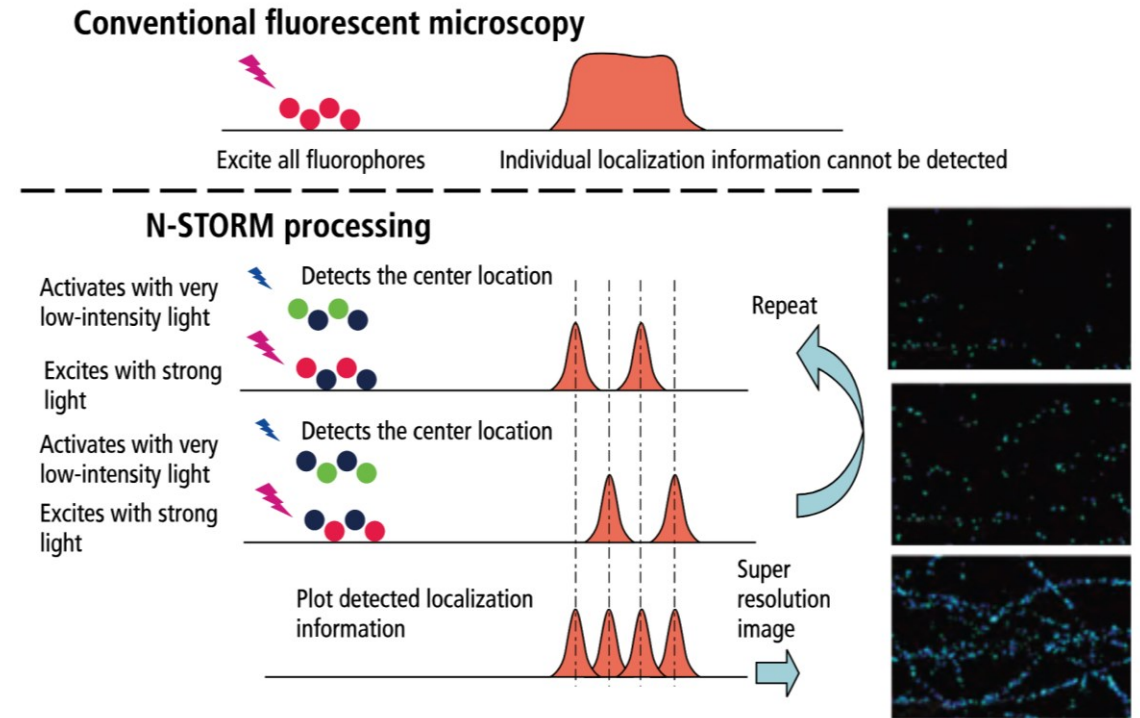


Figure 15 [2] – STORM process

- » **Widefield microscopy** → faster than a confocal, good for the membrane
- » Distance between molecules must exceed the Abbe diffraction limit ( $\approx 250nm$ ) → **parallel recording** of many individual emitters
- » The dye needs to have a short **duty-cycle** (es. Cy3-Cy5) → lots of photons for high resolution
- » **3D-storm**: exploits a cylindrical lens that modifies the shape of the focus → easier to recognize the location

# OPTICAL SETUP

- Widefield microscope
- 2 **continuous lasers** at different wavelengths
- Dichroic mirror
- Digital camera

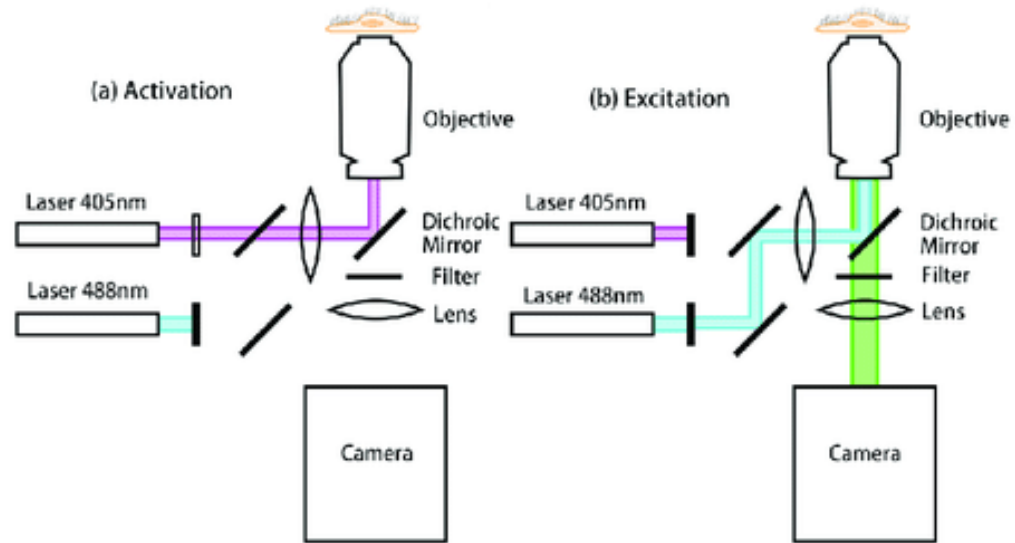


Figure 16 [3] – STORM optical setup

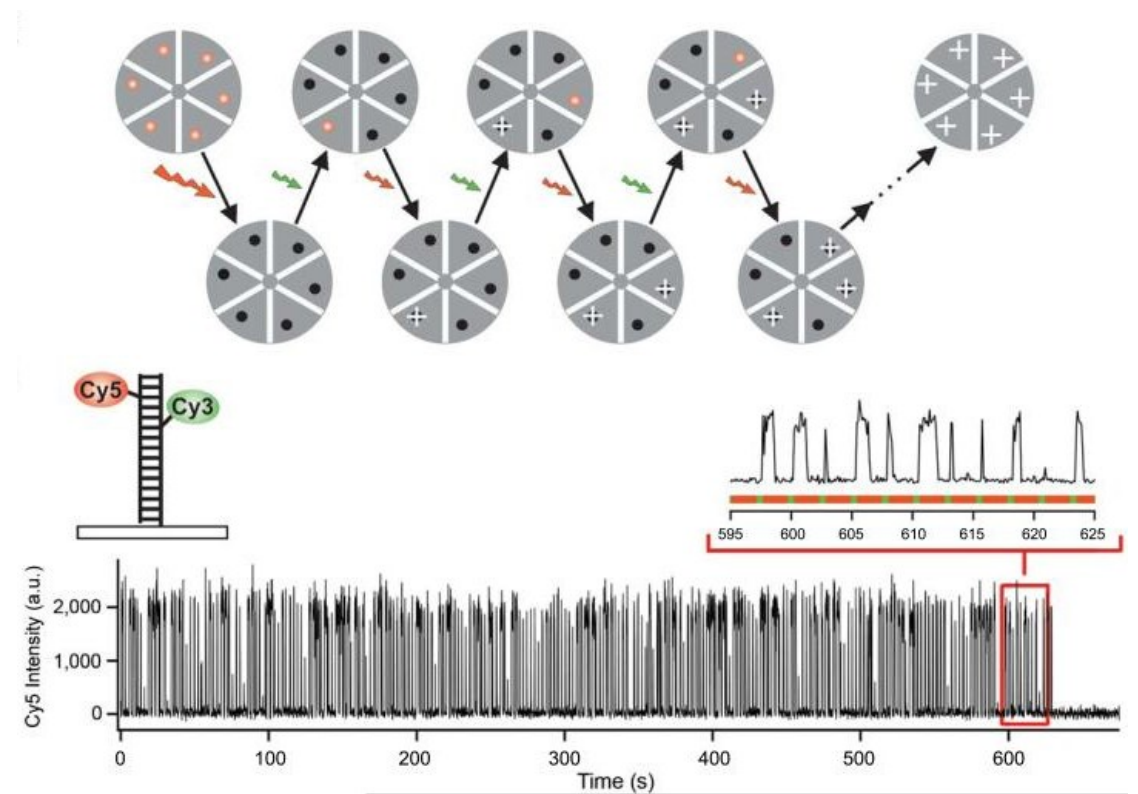


Figure 17 [4] – imaging sequence and example with Cy5 switch on DNA

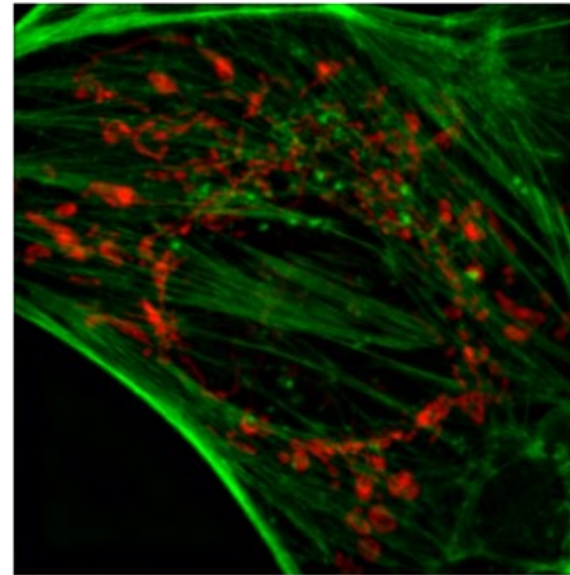


# REMARKS

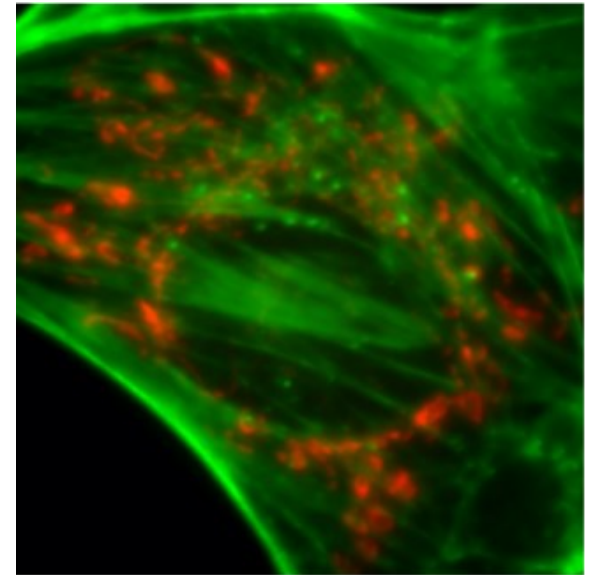
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- Most widely used super-resolution microscopy technique for **single-molecule imaging** or for structures like cytoskeletal biopolymers
- Limited uses *in vivo* because of its **toxicity** (PALM is better, also for particle tracking)
- There can be problems with **localization** and structure if you consider the dimension/uncertainty of the labels

**STORM**



**Wide-field**



*Figure 18 [17] – Comparison of wide-field microscopy and STORM microscopy.*

- Obtained resolution around **20nm**
- Non pumped lasers → fluorophore's duty cycle limits the signal time, no need for the pumped laser
- Cyanine dye, Cy5 and Cy3 have been used for the first experiments, having this switching properties

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# FLUORESECE & PSF

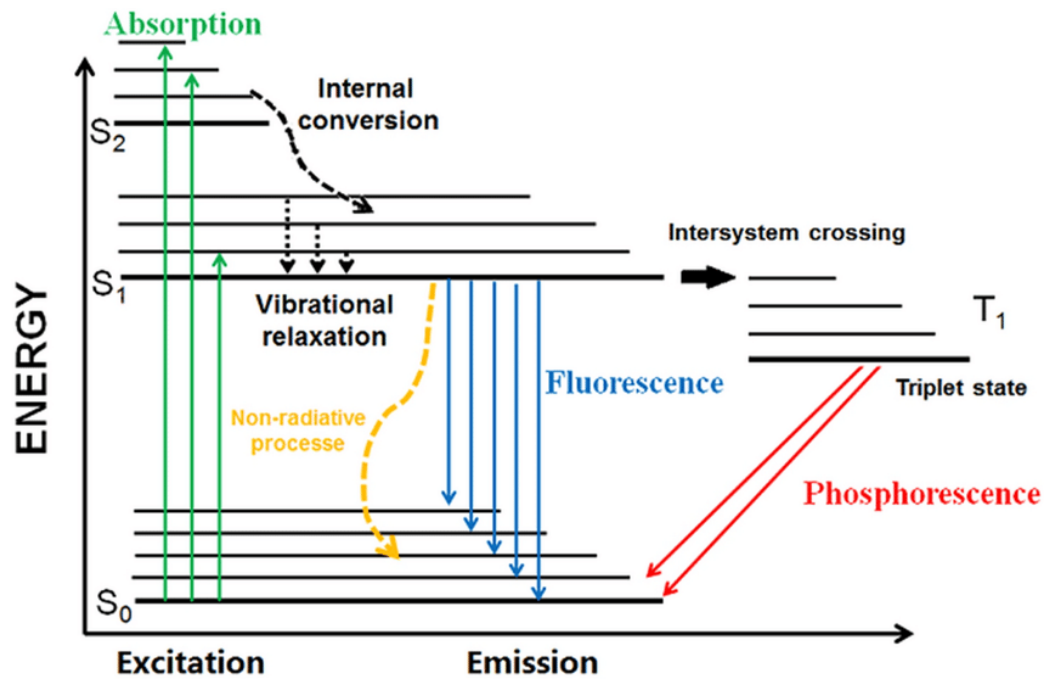
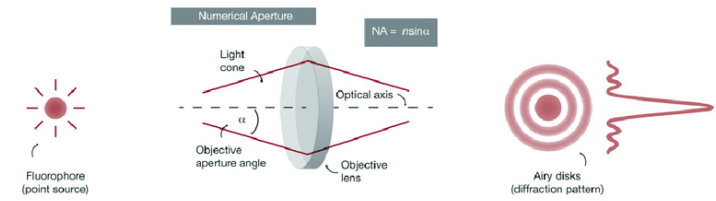
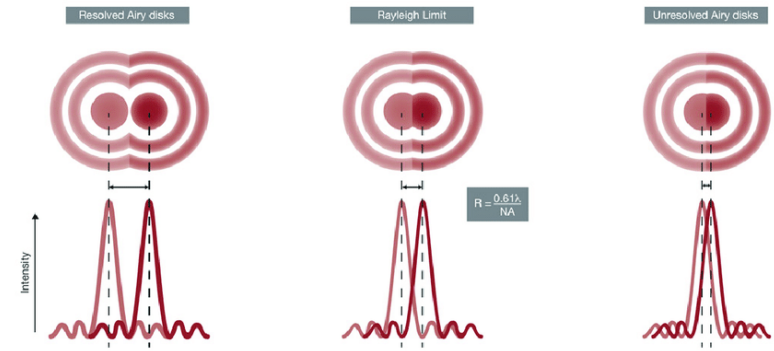


Figure 19 [18] – Jablonsky diagram

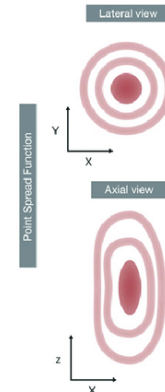
## A Numerical Aperture (NA)



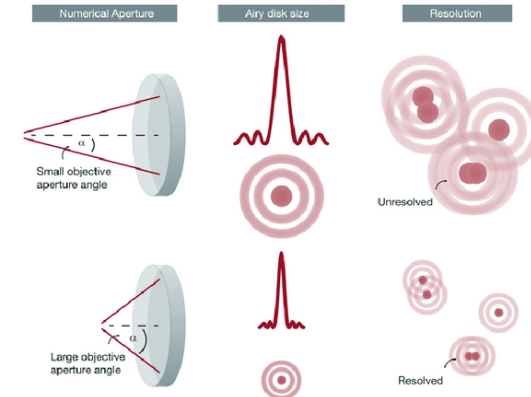
## B Resolution (R)



## C Point Spread Function (PSF)



## D Numerical Aperture, Airy disk size and resolution



# SIM mathematical explanation

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## Illumination pattern

$$I_{\theta,\varphi}(r) = \frac{I_0}{2} [1 + \cos(2\pi k_\theta \cdot r + \varphi)]$$

## Emission signal

$$\begin{aligned} D(r) &= (s(r) \cdot I_{\theta,\varphi}(r)) \otimes h(r) \\ &= D_0(r) + \cos(\varphi) \cdot D_C(r) - \sin(\varphi) \cdot D_S(r) \end{aligned}$$

## Fourier Transform of the emission signal

$$\begin{aligned} D_{\theta,\varphi}(k) &= [S(k) \otimes I_{\theta,\varphi}(k)] \cdot H(k) \\ &= \frac{I_0}{2} [S(k) \cdot H(k) + \frac{1}{2} e^{-i\varphi} S(k - k_\theta) \cdot H(k) + \frac{1}{2} e^{i\varphi} S(k + k_\theta) \cdot H(k)] \end{aligned}$$

## FT emission for each orientation

$$\begin{aligned} D_{\theta,\varphi_1}(k) &= \frac{I_0}{2} [S(k) \cdot H(k) + \frac{1}{2} e^{-i\varphi_1} S(k - k_\theta) \cdot H(k) + \frac{1}{2} e^{i\varphi_1} S(k + k_\theta) \cdot H(k)] \\ D_{\theta,\varphi_2}(k) &= \frac{I_0}{2} [S(k) \cdot H(k) + \frac{1}{2} e^{-i\varphi_2} S(k - k_\theta) \cdot H(k) + \frac{1}{2} e^{i\varphi_2} S(k + k_\theta) \cdot H(k)] \\ D_{\theta,\varphi_3}(k) &= \frac{I_0}{2} [S(k) \cdot H(k) + \frac{1}{2} e^{-i\varphi_3} S(k - k_\theta) \cdot H(k) + \frac{1}{2} e^{i\varphi_3} S(k + k_\theta) \cdot H(k)] \end{aligned}$$

## Image in the Fourier space

$$\begin{bmatrix} S(k) \cdot H(k) \\ S(k - k_\theta) \cdot H(k) \\ S(k + k_\theta) \cdot H(k) \end{bmatrix} = \frac{2}{I_0} M^{-1} \begin{bmatrix} D_{\theta,\varphi_1}(k) \\ D_{\theta,\varphi_2}(k) \\ D_{\theta,\varphi_3}(k) \end{bmatrix}$$