# Using new digital SiPM from Philips with AX-PET a new geometrical concept for PET



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#### On behalf of the AX-PET collaboration

https://twiki.cern.ch/twiki/bin/view/AXIALPET





### Outline



- Introduction to Positron Emission Tomography
- AX-PET
  - The AX-PET concept
  - Detector components
  - Module characterisation
  - Results of tomographic reconstructions
  - Inter Crystal Scattering events
- AX-PET using digital SiPM from Philips
  - Energy resolution
  - Time resolution
  - Future





# Positron Emission Tomography

Unstable

parent nucleus

- ▶ basis of the PET system **Positron Emission**:
- $p \rightarrow n + e^+ + \nu_e$

positron

annihilation

positron emission

- ightharpoonup ho decay of different radionuclides
- Positron Annihilation:  $e^+e^-$  2 photons emitted "back to back" Ey = 511 keV

γ interact with matter:

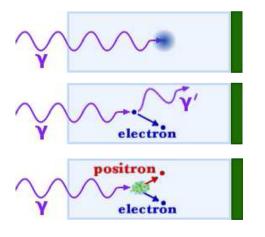
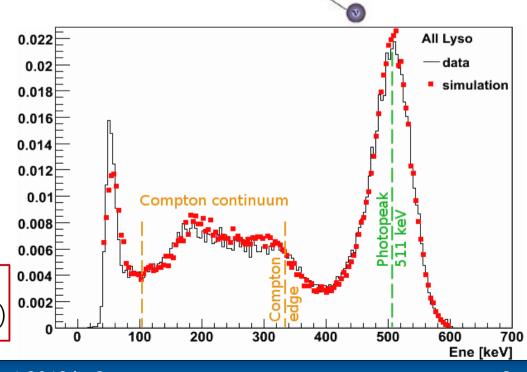


Photo-electric effect

Compton scattering

Pair production

To measure the positron emitter distribution : Measure the γ pair → build line of response (LOR)

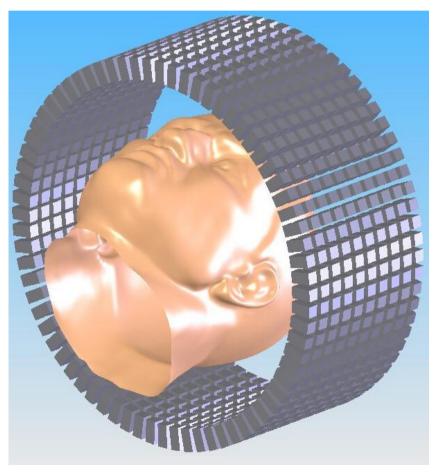




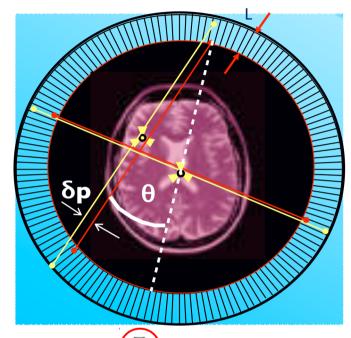




#### Standard PET scanners



Short crystals radially oriented Block readout



$$\epsilon = 1 - e^{-\mu L}$$
 Max. interaction efficiency  $\rightarrow \log L$   $\delta p = L \cdot sin heta$  Min. parallax error

$$\delta p = \stackrel{\textstyle \iota}{L} sin heta$$
 Min. parallax error  $\stackrel{\textstyle \iota}{
ightarrow}$  short L

Always a compromise between spatial resolution and sensitivity:

solution: add depth of interaction information

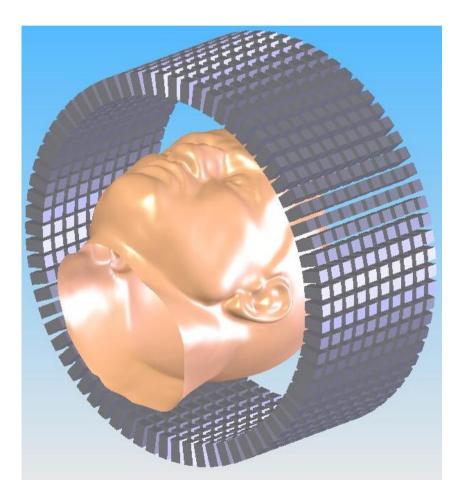


# The AX-PET concept

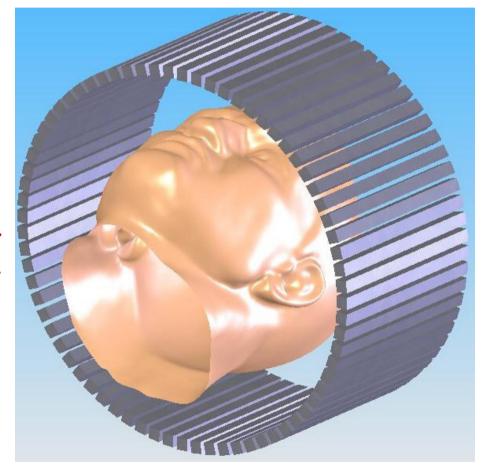


Standard PET scanners

AX-PET geometry proposal







Short crystals radially oriented Block readout

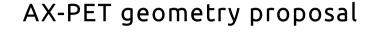
Long crystals axially oriented Single crystal readout

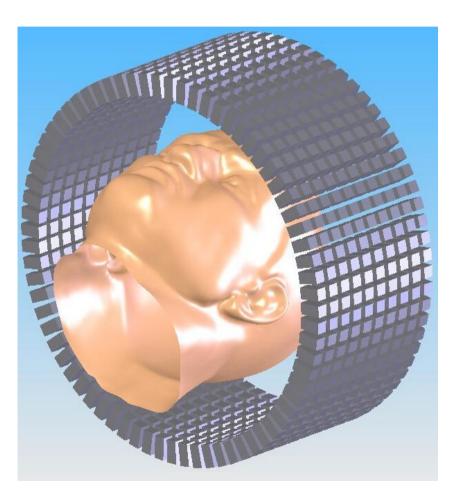


# The AX-PET concept



Standard PET scanners







Short crystals radially oriented Block readout

Long crystals axially oriented Single crystal readout

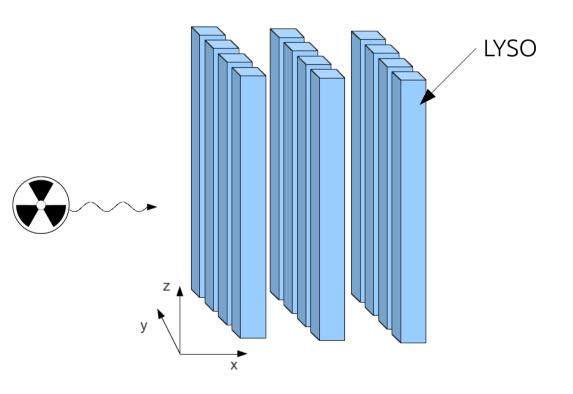






#### 3D measurement of the photon interaction point

- Transaxial coordinate and energy measurement with thin elongated scintillator LYSO crystals
  - The hit crystals gives the transaxial coordinate (x, y)



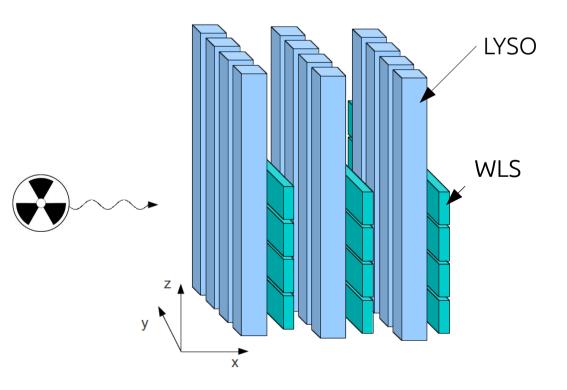




### The AX-PET concept

#### 3D measurement of the photon interaction point

- Transaxial coordinate and energy measurement with thin elongated scintillator LYSO crystals
  - The hit crystals gives the transaxial coordinate (x, y)
- Axial coordinates measured with Wave Length Shifter (WLS) strips



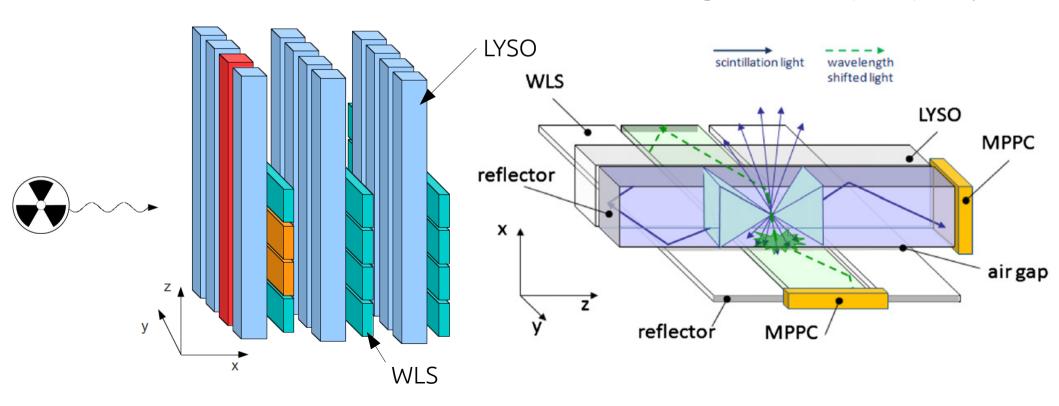




# The AX-PET concept

#### 3D measurement of the photon interaction point

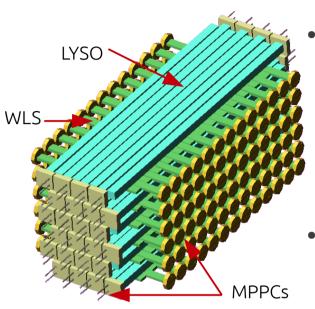
- Transaxial coordinate and energy measurement with thin elongated scintillator LYSO crystals
  - The hit crystals gives the transaxial coordinate (x, y)
- Axial coordinates measured with Wave Length Shifter (WLS) strips











- LYSO (Lu<sub>1.8</sub>Y<sub>0.2</sub>SiO<sub>5</sub>:Ce), Prelude 420 from Saint Gobain
  - 3x3x100 mm<sup>3</sup>
  - Light Yield LY=32 photons/keV
  - High density: 7.1 g.cm<sup>-3</sup>
  - Decay time τ = 41 ns
  - Attenuation length  $\lambda_{511} = 12 \text{ mm}$  @ 511keV
- Wave length shifting strips, ELJEN EJ-280-10x
  - 10 times higher dye concentration for better absorption

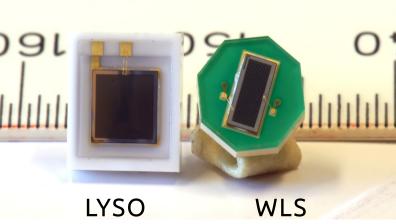
Expected LYSO light output@511 keV event : ~ 1000 photons

- 3 x 3 mm² area, 3600 cells 50 x 50 um²
- PDE ~ 40%
- Gain: 5.7 10<sup>5</sup>
- Bias voltage ~ 70 V

Expected WLS light output : ~ 50 photons

- 3. 22 x 1.19 mm<sup>2</sup> area, 782 cells of 70 x 70 um<sup>2</sup>
- PDE ~ 40%
- Gain: 4 10<sup>5</sup>
- Bias voltage ~ 70 V

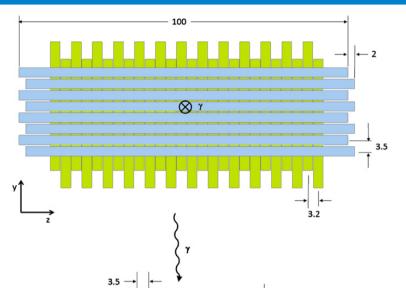


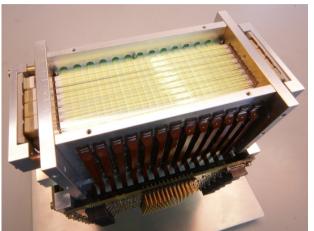




### Module assembly





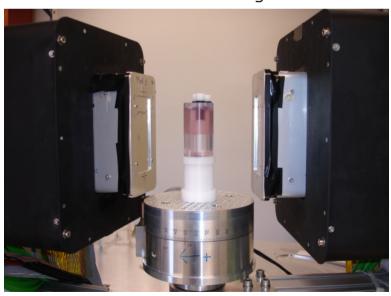


Assembled module

Module housing and services



- One fixed, one mobile
- Operated in coincidence
- Each module is composed by six layers
- Each layer is made of 8 LYSOs and 26 WLS both staggered to enable the readout
  - → 204 channels per module individually biased
- All layers are optically decoupled



Demonstrator gantry





### Demonstrator performance

For more explanations see publication: doi:10.1016/j.nima.2011.06.059

face-to-face

#### • Energy resolution :

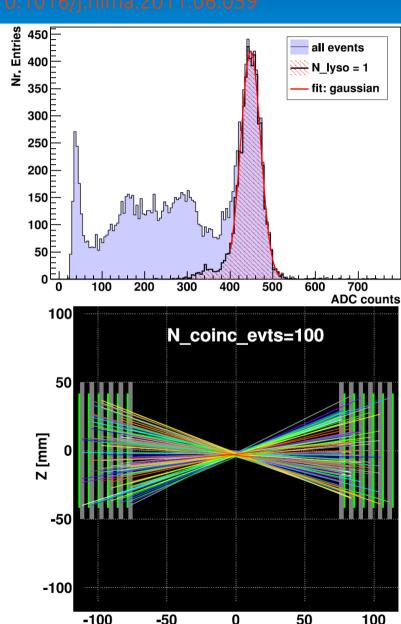
 Average value of the energy resolution of all the LYSO crystals for both modules is 11.8% FWHM at 511 keV

#### • Spatial resolution

- Axial:
  - Single module
    - Module 1: 1.75 mm FWHM
    - Module 2: 1.83 mm FWHM
  - Module in coincidences
    - F2F, OBL: 1.35mm FWHM
- Transaxial (single module)
  - F2F, OBL: 2 mm FWHM

#### Efficency/Sensitivity:

- Can always be improved by increasing the number of layers
- Time resolution: 1.9 ns FWHM



X [mm]

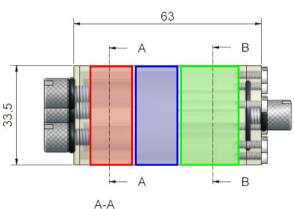


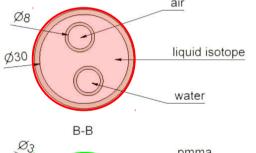
# Results from tomographic reconstruction

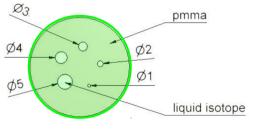


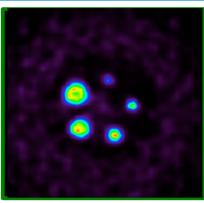
#### NEMA NU4

Image Quality Mouse Phantom



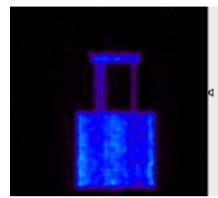




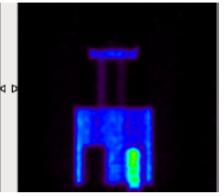












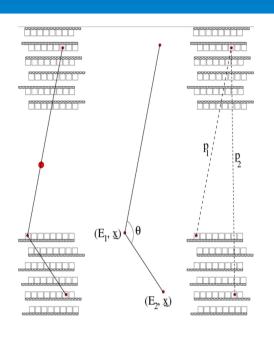
- Contrast region
- Homogenous region
- Spatial resolution region

Resolve 1 mm rod with 1.6 mm FWHM





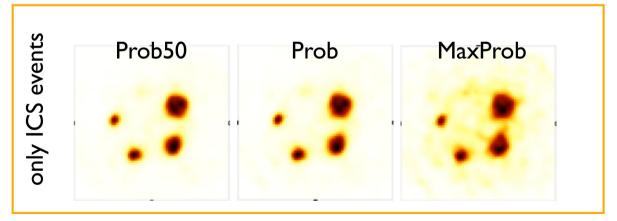


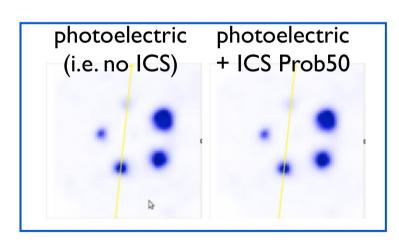


- So far only pure photoelectric events were used for the reconstruction
- ICS events are crucial in order to increase the detector sensitivity
- <u>Data sample used</u>: One photoelectric event in one module in coincidence with one ICS event in the other module

#### • Reconstruction method:

- Include both LOR (Prob50)
- Include both LOR weighted according to  $(d\sigma/d\Omega)_{Klein-Nishina}$  (Prob)
- Include only the LOR with max prob.  $(d\sigma/d\Omega)_{Klein-Nishina}$  (MaxProb)





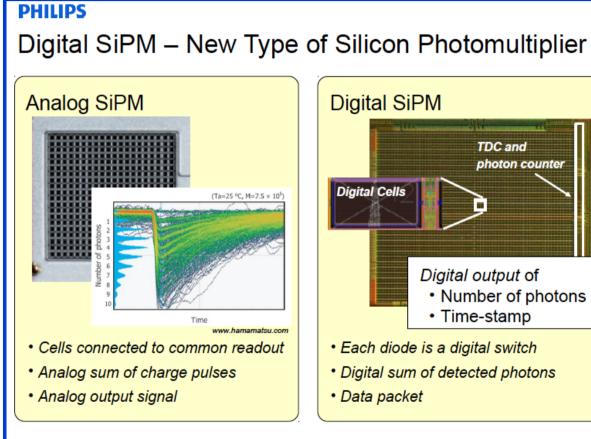
- For the NEMA phantom, ICS/photoelectric ~ 20 %, small gain
- Work still in progress. Improvement expected be more important for small data sample

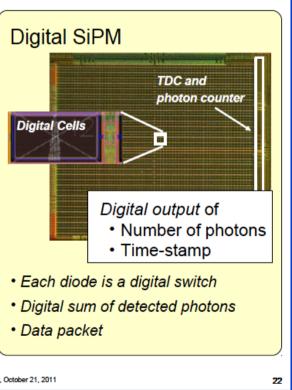


# Using Philips digital SiPM as alternative photodetectors



Web site: http://www.research.philips.com/initiatives/digitalphotoncounting/





- Sensitivity
- Lower dark count level compared to analog devices
- Speed
- Excellent timing resolution → Time Of Flight PET
- Robustness
- Against electromagnetic interference (Compatibility with MRI scanner)
- Low sensitivity to temperature variations
- High production yield due to the possibility of disabling individual cells

T. Frach, CERN detector seminar



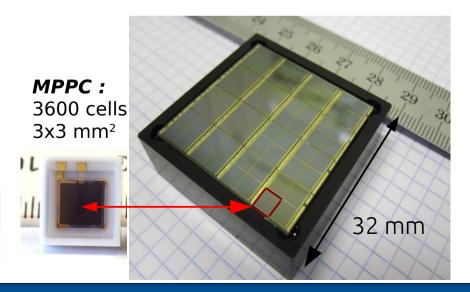
### Technical Evaluation Kit



- Our evaluation kit is made of:
  - 2 DLS 3200 sensor with 3200 cells per pixel
  - 2 DLS 6400 sensor with 6400 cells per pixel
  - 4 kapton cables
  - One base to connect the tiles
  - One power supply
  - One computer for detector configuration and data acquisition

Few characteristics	DLS 6400	DLS3200
Cell size [µm²]	30 x 50	59.4 x 64
Fill factor [%]	54	78 ( <b>→</b> 84)
PDE [%] @ 420 nm	30	43 (→ 47)
DCR [MHz/pixel] @20°C	<5	<10
Op. voltage [V]	< 35	
Temp. dep of PDE [% / K]	- 0.33	



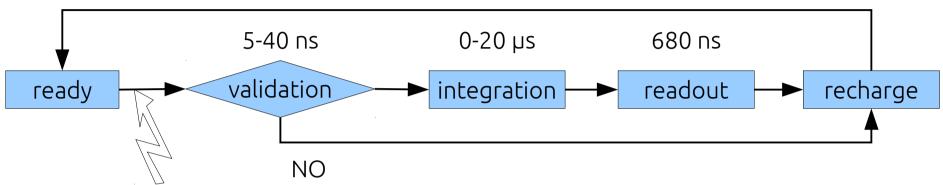




### DSiPM state machine



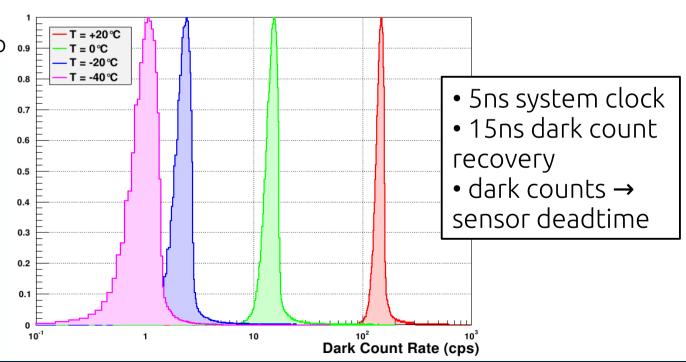




Trigger generated by the 1<sup>st</sup>, 2<sup>nd</sup>, 3<sup>rd</sup> or 4<sup>th</sup> photon arriving, this latter gives the time stamp

# 1.

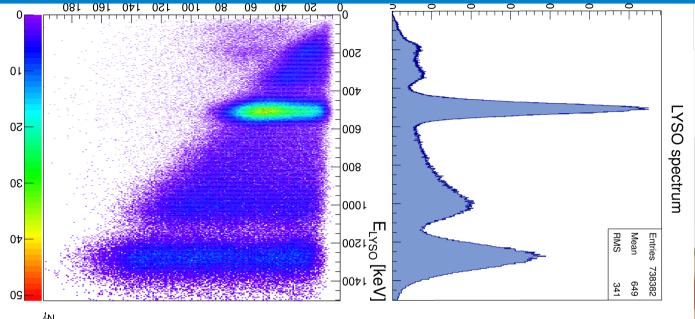
#### **SPAD Dark Count Rate Distribution**





### Energy resolution with the DLS 3200





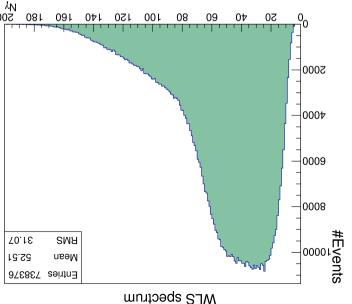
#### Minimal AX-PET like set-up

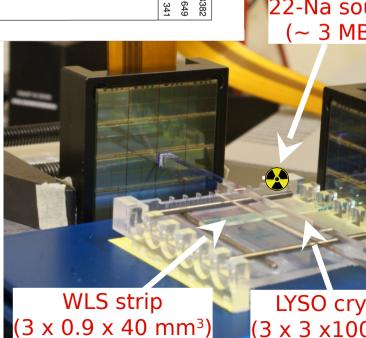
#### <u>Light yields:</u>

LYSO: 1500 – 1800 pe

WLS: 20-100 pe

### Energy resolution @511 keV: 12.3 % after saturation correction

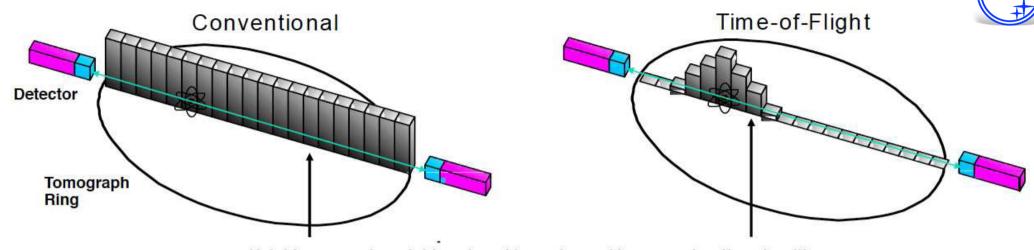




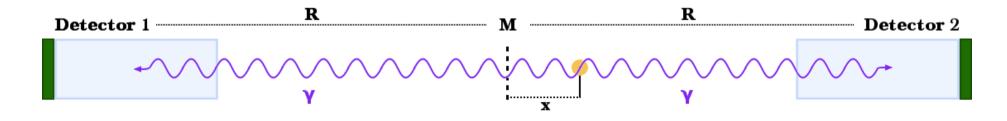


# Towards Time Of Flight PET





Height represents weight assigned to each voxel by reconstruction algorithm

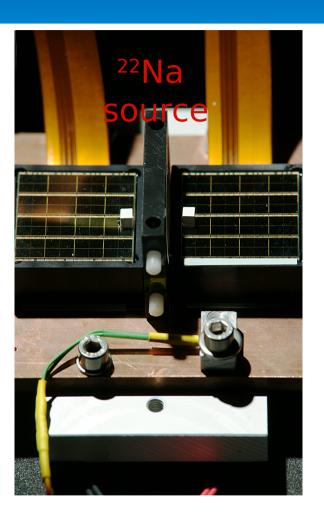


$$x = \frac{\Delta t \cdot c}{2}$$
  $\longrightarrow$   $\sigma_x = \frac{\sigma_t \cdot c}{2}$   $\longrightarrow$   $\sigma_x = 1 \text{ cm} \rightarrow \sigma_t = 65 \text{ ps}$ 

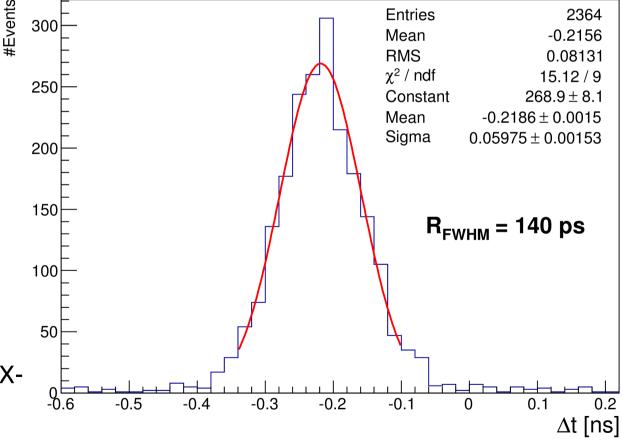


#### Time resolution with the DLS 3200





time difference between the two tiles for photopeak coincident events (coincidence window = 5 ns, Peltier cooling @ 10°C)



 $R_FWHM = 140 \text{ ps} \rightarrow R_FWHM = 2 \text{ cm}$ 

- 2 LYSO scintillator crystals **non AX-**PET standard (3x3x3) mm<sup>3</sup>
- Reflective white paint
- coupling done with optical grease

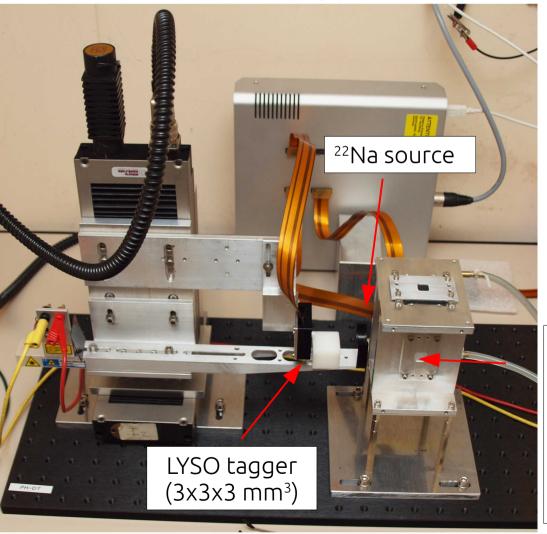


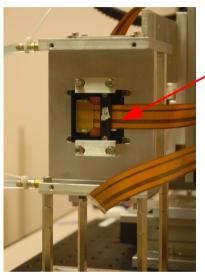
# AX-PET ongoing and future activities



AX-PET performance demonstration with dSiPM

axial resolution through WLS readout



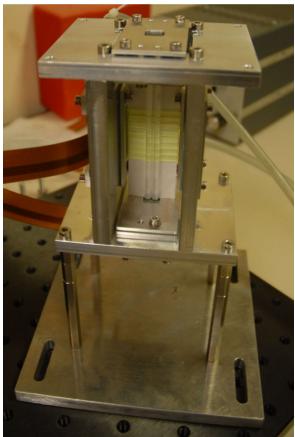


DLS 3200

Mini AX-PET module : 2 layers made of :

- 2 Lyso crystals
- 8 WLS strips

Water cooling

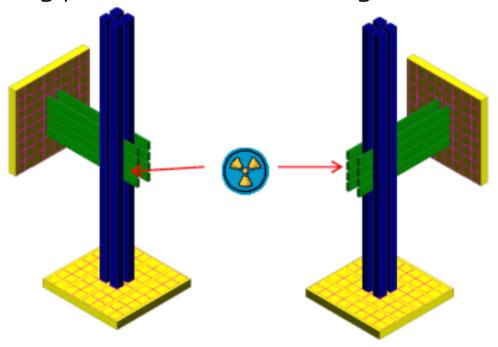


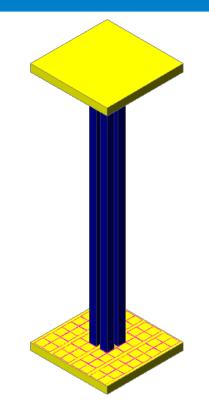


# AX-PET ongoing and future activities



Timing performances with long LYSO





Double side readout setup

AX-PET performance with small animals

Ongoing measurements with rats and mice using both <sup>18</sup>F and FDG at the Radio Pharmaceutical Institute at ETH Zurich

Stay tuned.... more results are coming very soon



# Thanks for your attention The AX-PET collaboration













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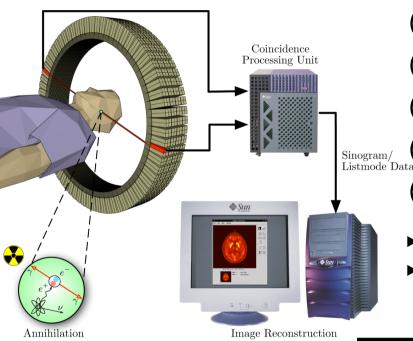




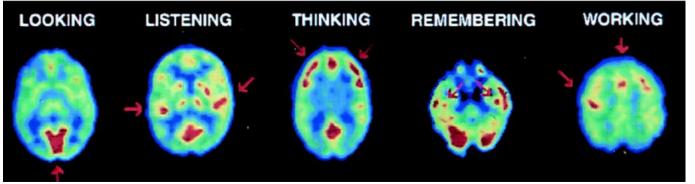


#### PET detector principle:

coincidence of 2 photons of defined energy (511 keV) and emitted on the same line

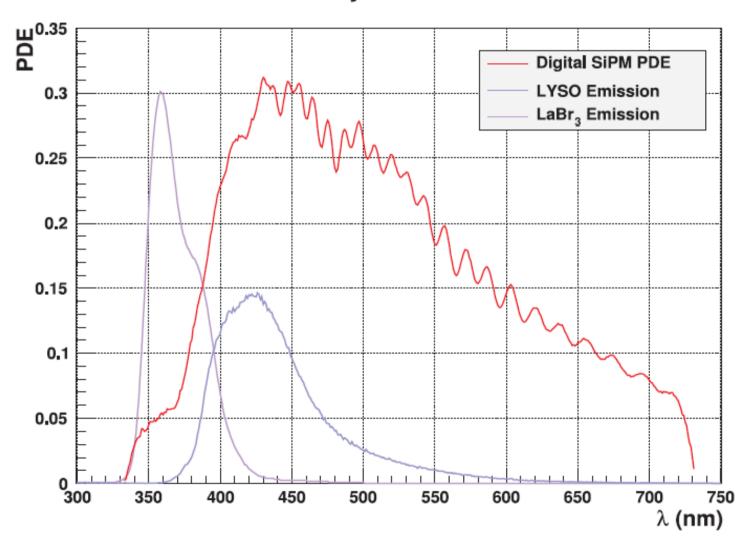


- (1) Inject the radiotracer into the body
- (2) Wait for uptaking period
- (3) Start the acquisition (i.e. detection of coinc. events)
- (4) Feed the data into the reconstruction algorithms
- (5) image of the activity concentration
- ► PET: "in-vivo" functional imaging technique
- get a (quantitative) image of the radio-tracer concentration



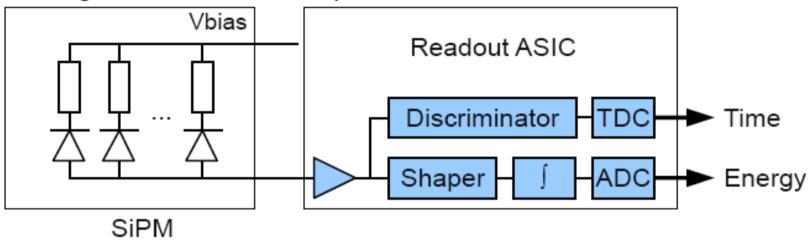
### dSiPM Photon detection efficiency

#### **Photon Detection Efficiency**

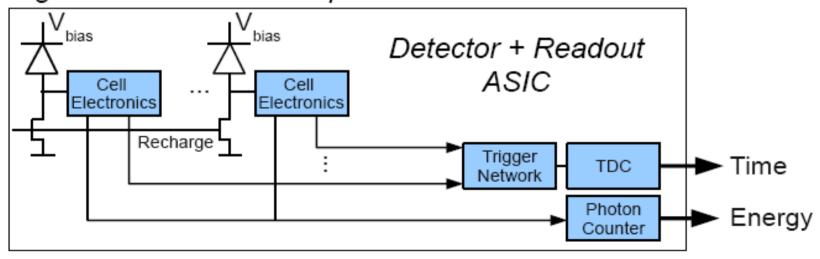


# Analog vs. Digital SiPM concept

#### Analog Silicon Photomultiplier Detector

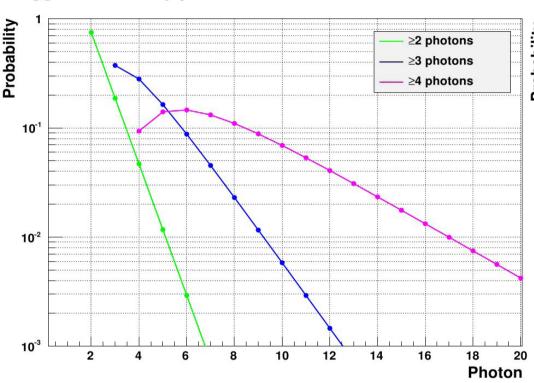


#### Digital Silicon Photomultiplier Detector



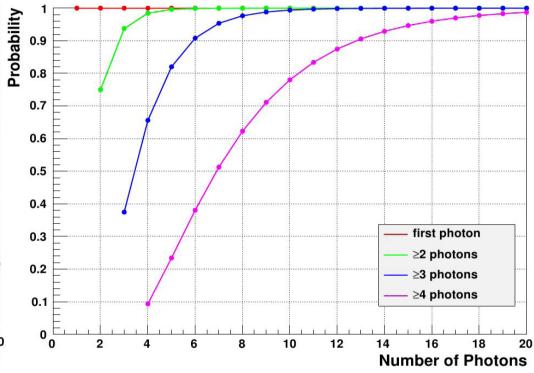
# dSiPM Trigger probability

#### **Trigger Probability per Photon**



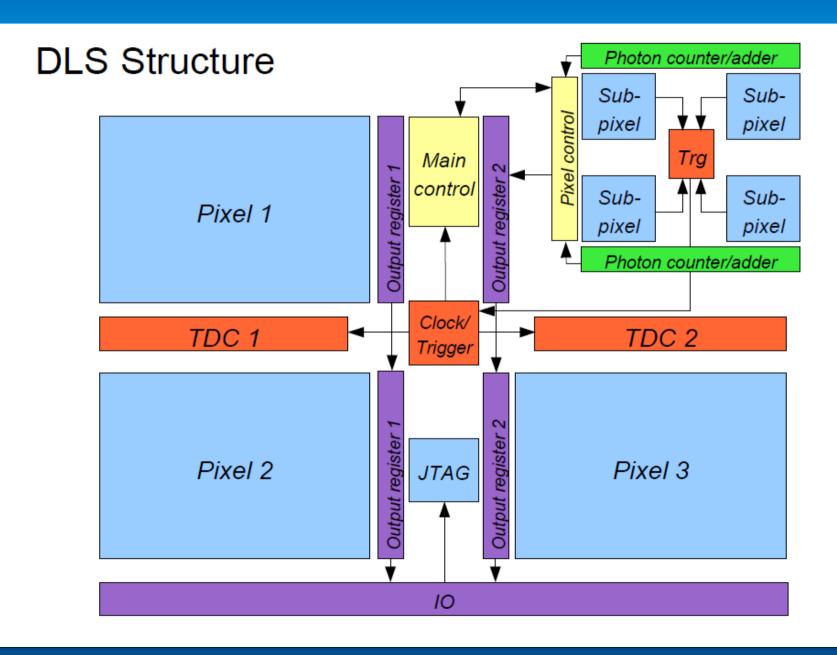
Probability for the n<sup>th</sup> photon to provide the trigger

#### **Cumulative Trigger Probability**

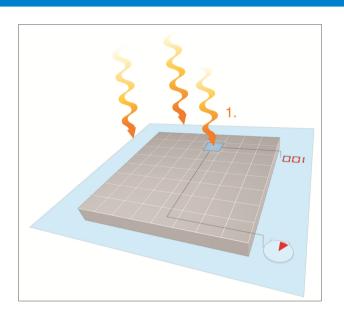


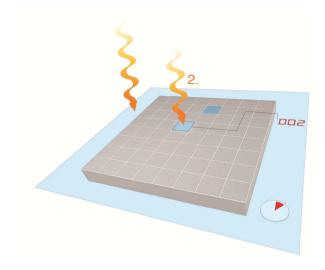
Probability to trigger as function of the amount of inpinging photons

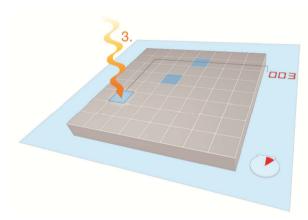
# dSiPM Trigger logic

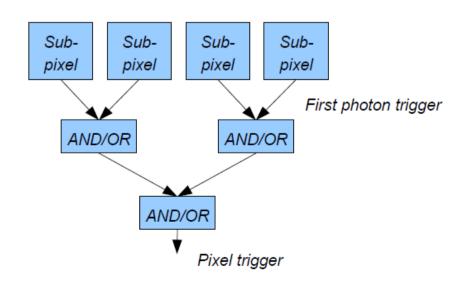


# dSiPM Trigger logic

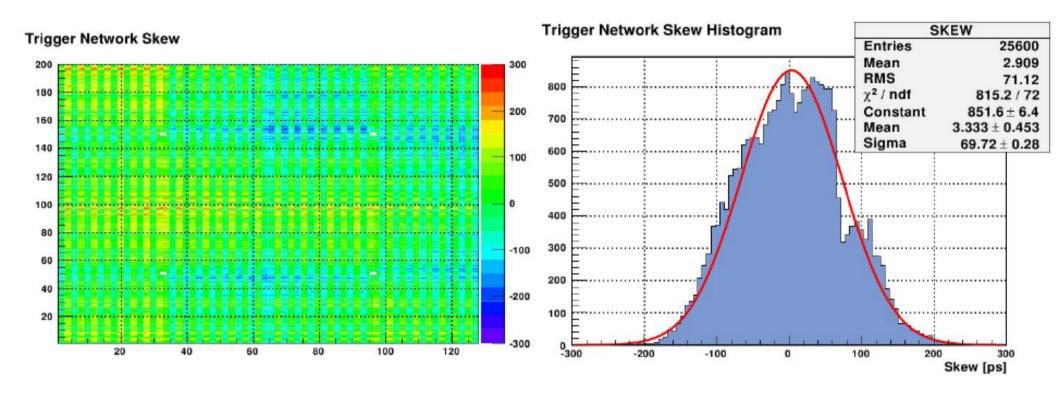




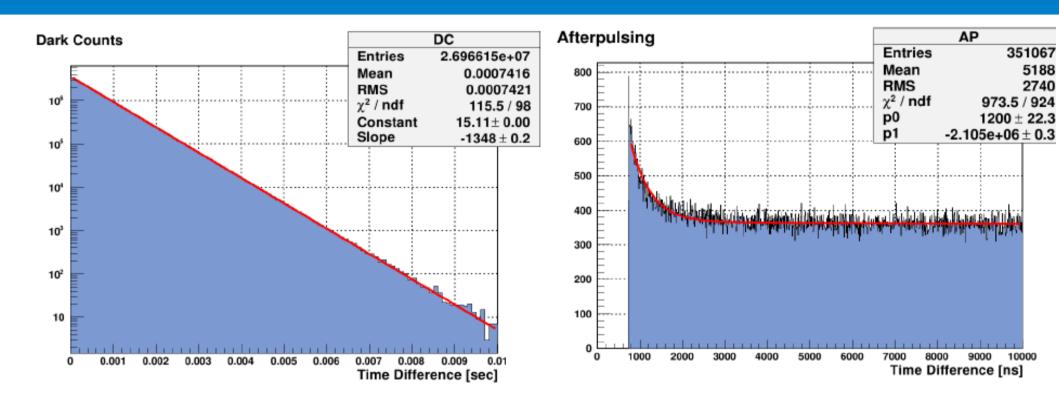




# dSiPM Trigger logic



# dSiPM DC and afterpulse



Time differences of two consecutive dark counts in a single diode.

Afterpulsing: deviation from the Poisson distribution in the first few µs.

Many diodes show afterpulsing probabilities of less than 0.1%, few are in the 2-3% range.



# Why going from analog to digital SiPM



Characteristic	dSiPM	aSiPM	APD	PMT
Sensitivity (PDE)	Max. ~70 % tbp	Max ~ 70% tbp	~ 70%	~ 35%
Intrinsic timing res.	~ 50 ps	> 150 ps	~ 1 ns	~ 400 ps
CRT on system level (depends also on scintillator)	Pot. ~ 150 ps 250 ps proven	~ 500 ps in literature	> 1 ns	~ 500 ps
voltage	35 V	35-70V	Up to 1500V	400-800V

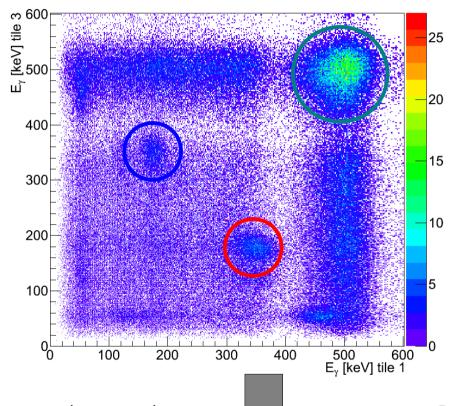
- Advantages of dSiPM wrt aSiPM
  - Lower DCR
  - Better CRT (triggering on the first photon) → TOF PET
  - Afterpulses does not affect the digital sum thanks to active quenching
  - No custom electronics needed



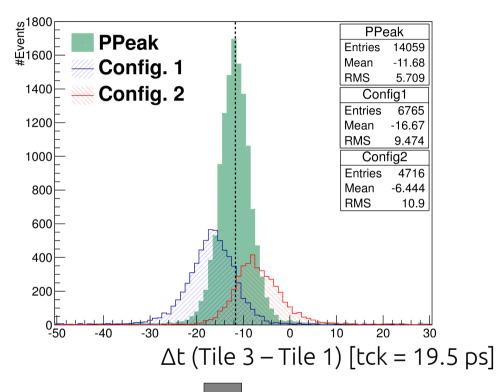
# Use of the DSiPM timing performance

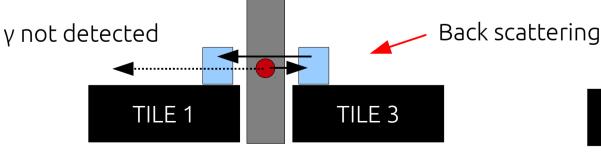




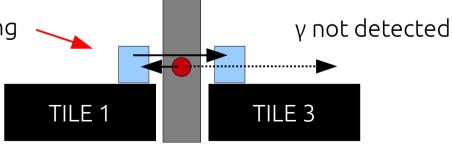


#### Time difference





Config 1  $\rightarrow \Delta t = t_3 - t_1 < 0$ 



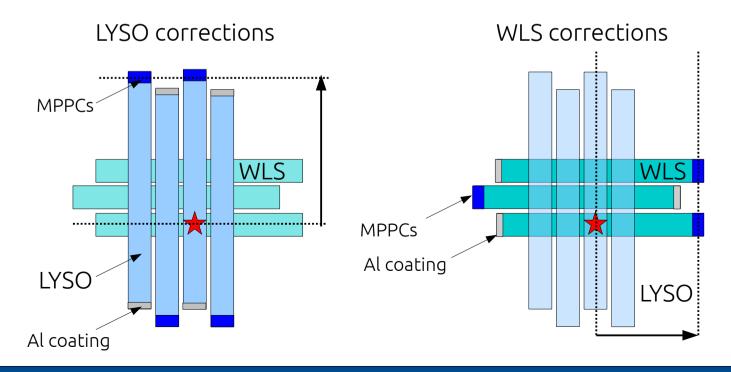
Config 2  $\rightarrow \Delta t = t_3 - t_1 > 0$ 







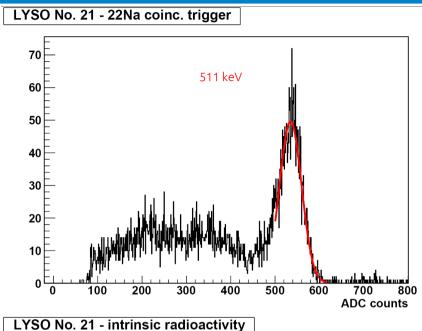
- The variation of the MPPC gain with the temperature is corrected to uniformize the response of all the LYSO and WLS
- WLS and LYSO are read out on one side, the other extremity being covered with a Al coating. Thus the light collected by the MPPCs depends on the position of the photoelectric interaction: Attenuation and reflexions
- This can be corrected using the spatial information from the WLS and LYSO





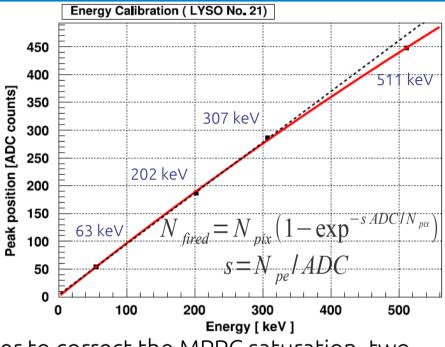
# MPPC saturation correction and Energy calibration





140 63 keV 202 keV 71Lu<sup>176</sup> 72Hf<sup>176</sup>

100 307 keV 30

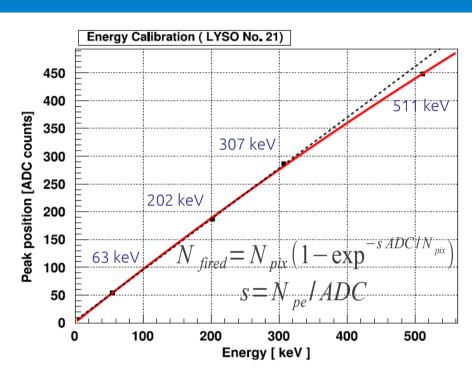


- In order to correct the MPPC saturation, two calibration sets are needed :
  - Photoelectric peak at 511 keV, acquired with the <sup>22</sup>Na source
  - "Integrated calibration source": Two of the peaks of the  $^{176}$ Lu decay spectrum at 202 and 307 keV (natural radioactivity of LYSO) and the Lutetium  $K_{\alpha}$  escape line at 63 keV
- The four data points are fitted to take into account the saturation effect in the MPPCs



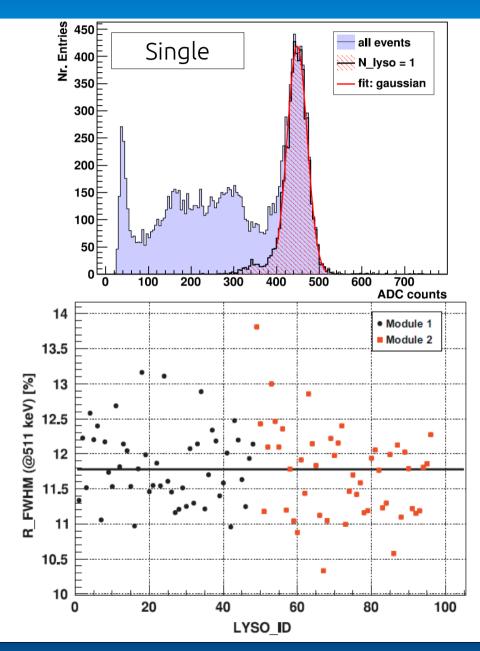






Even if the number of incoming photons is lower than the number of cells in the MPPC, the probability that two photons hit the same pixel is not zero → Saturation effect

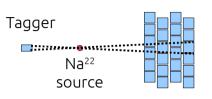
• The average value of the energy resolution of all the LYSO crystals for both modules is 11.8% FWHM at 511 keV





# Spatial resolution with point-like source





side view

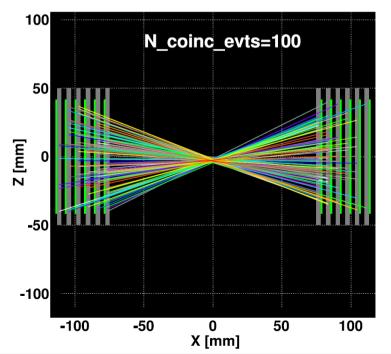
Collimated beam for precision scan

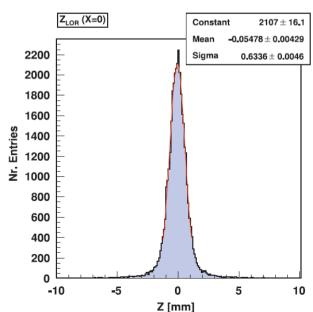
#### Taken into account:

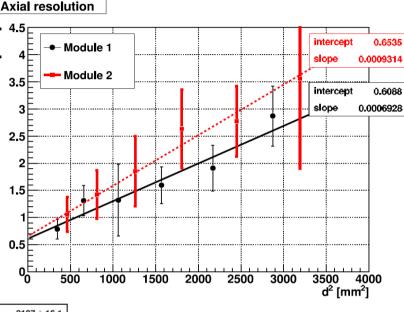
- positron range :  $\rho \sim 0.54$ mm
- non-collinearity : ~ 0.0022 x D ~ 0.33mm
- source dimensions : ø=250µm
- Beam divergence

#### Axial resolutions

- Module 1: 1.75 mm FWHM
- Module 2: 1.83 mm FWHM





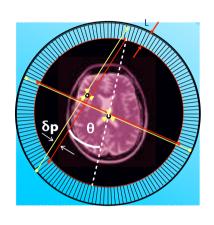


Axial resolution
• LOR of 100 coincidences in the axial plane. Intersection with plane x=0 gives R = 1.35 mm FWHM

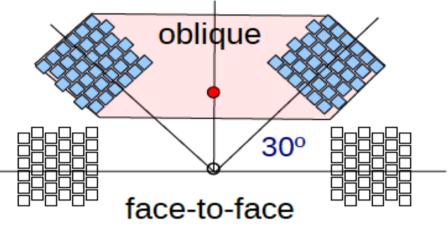


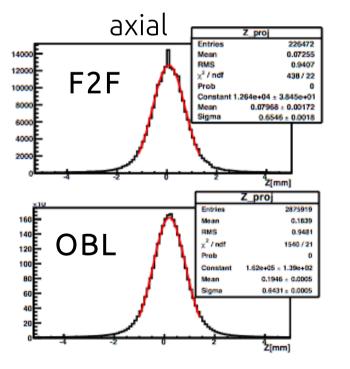
# Spatial resolution with point-like source

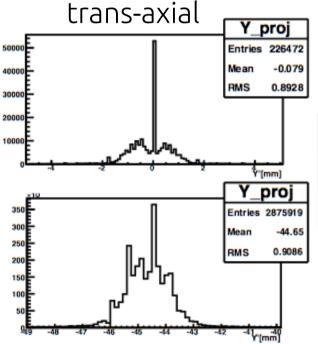




parallax error is more and more important outside the center of the FOV







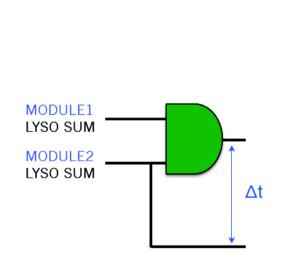
	Axial	Transaxial
F2F	σ=0.655	RMS=0.893
OBL	$\sigma$ =0.643	RMS=0.909

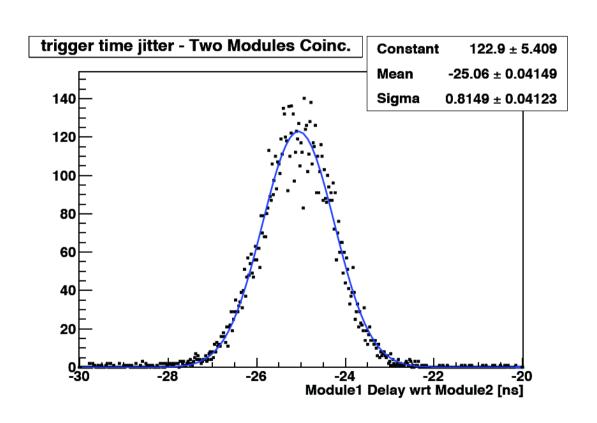






- measure delay of coincidence wrt Mod2
- measurement from the scope [Lecroy Waverunner LT584 L 1GHz]





Measured time resolution: FWHM ~1.9 ns