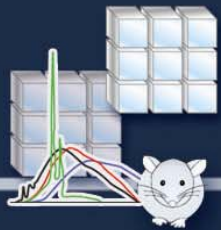


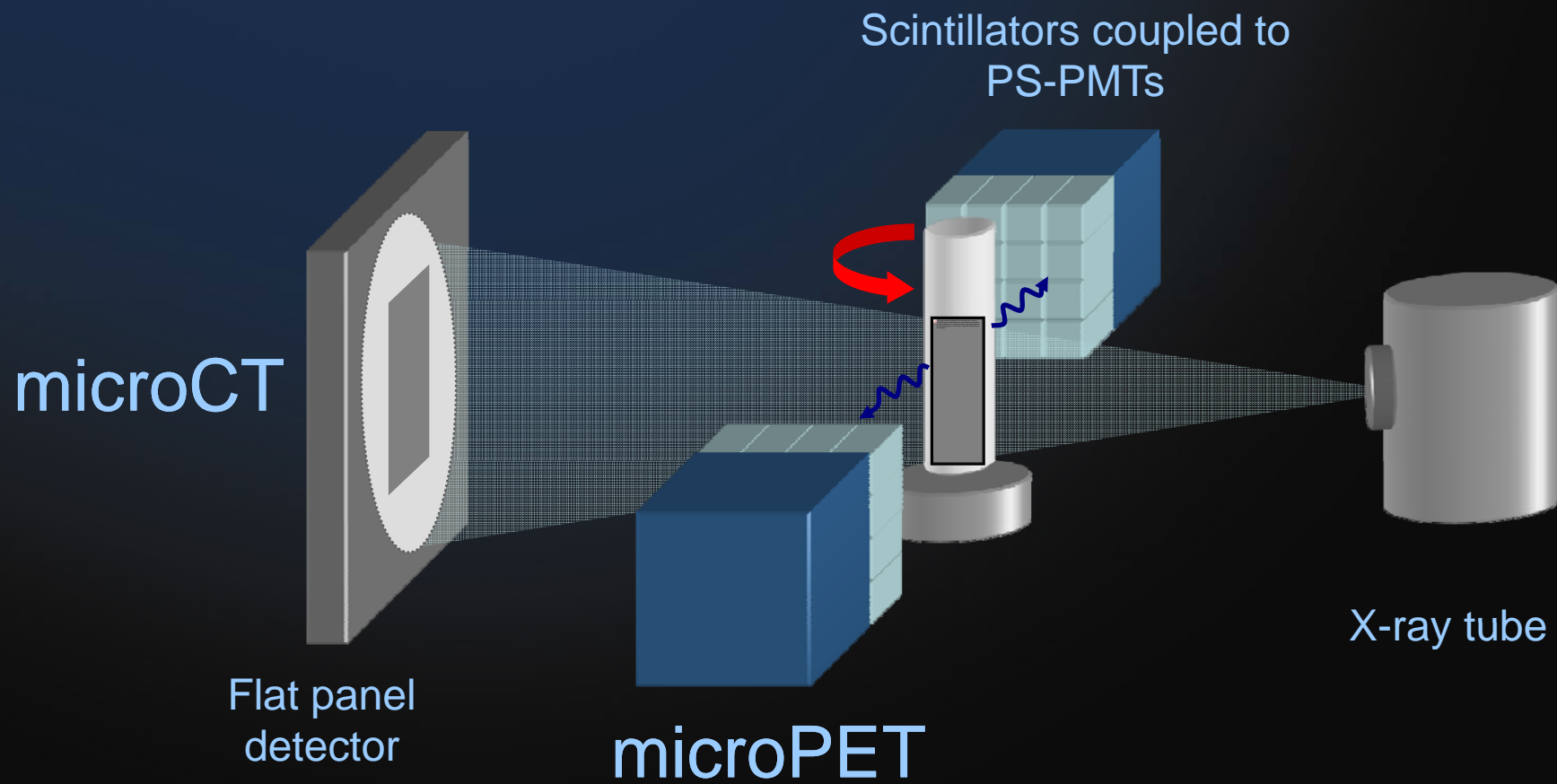
# Image-transfer properties of a microCT system based on a flat panel detector

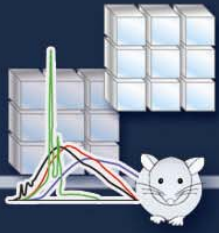
Arnulfo Martínez-Dávalos  
Instituto de Física, UNAM  
[arnulfo@fisica.unam.mx](mailto:arnulfo@fisica.unam.mx)





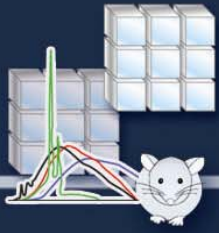
# Sistema Bimodal de Imágenes (SIBI)





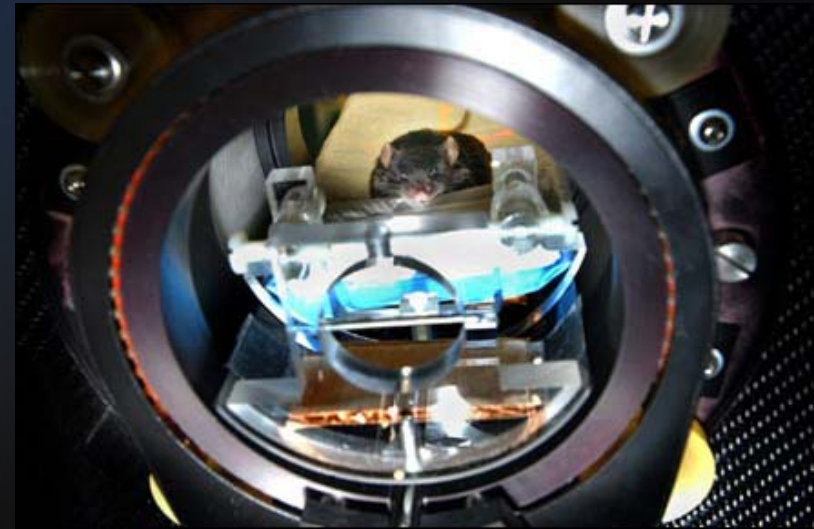
# Aims

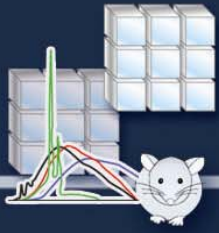
- ❖ To develop radiological imaging systems for small rodents using state of the art technologies
- ❖ To integrate different imaging techniques in order to provide both anatomical and functional information
- ❖ To provide advanced training in all related areas (radiation detection, nuclear techniques, imaging, preclinical studies, etc.)
- ❖ To collaborate in basic biomedical research using *in vivo* molecular imaging techniques



# Why study mice?

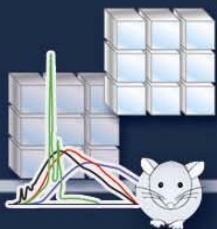
- ❖ Biological model *par excellence*
- ❖ Genetically modified strains
- ❖ Animal models of neoplastic or neurological diseases
- ❖ Non invasive *in-vivo* studies
  - Neurochemistry
  - Disease development
- ❖ Longitudinal studies





# The dose problem in microCT

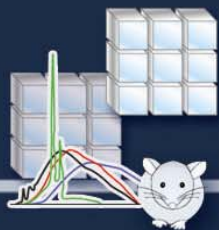
- ❖ In-vivo imaging allows longitudinal studies, but ...
  - only meaningful if the subject is not altered!
- ❖ Excessive dose can alter physiological functions:
  - 200 mGy *in-vivo* elevates gene expression level [Amundson et al. 2001]
  - 20-50 mGy *in-vitro* induces stress-response gene expression [Fornace et al. 2002]



# Oxford Instruments X-ray tubes

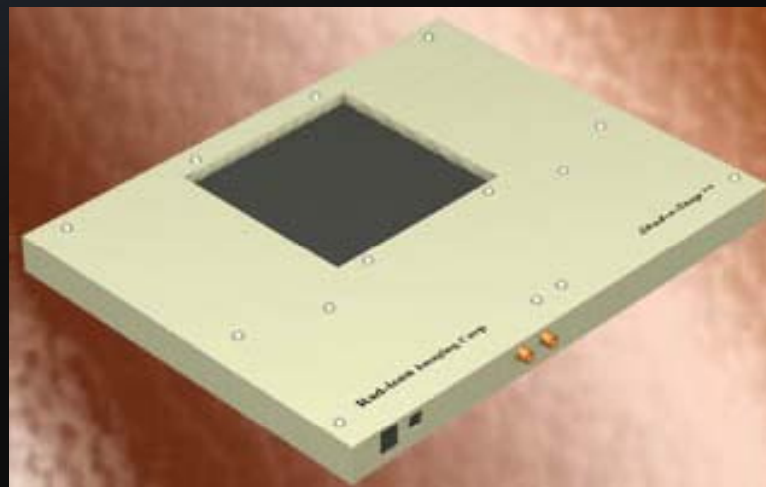


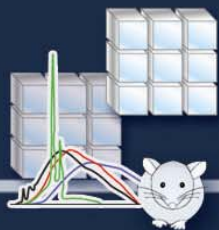
	Ultrabright	Apogee
Target	W	W / Mo
Current interval (mA)	0.1 - 2	0.1 - 1
Voltage (kV)	10 - 90	20 - 50
Focal spot ( $\mu\text{m}$ )	13 - 40	35
Beam angular aperture	$33^\circ$	$22^\circ$



# Flat panel detector

- ❖ Rad-icon Shad-o-Snap 4k
- ❖ 8 CMOS photodiode panels
- ❖  $\text{Gd}_2\text{O}_2\text{S}$  scintillator screen  
(Kodak Lanex fine,  $\sim 80 \mu\text{m}$  thickness)
- ❖  $2000 \times 2048$ ,  $48 \mu\text{m}^2$  pixels
- ❖  $96.1 \text{ mm h} \times 98.6 \text{ mm w}$
- ❖ 12 bits per pixel
- ❖ 4000:1 dynamic range
- ❖ USB data interface
- ❖ 540 ms readout period

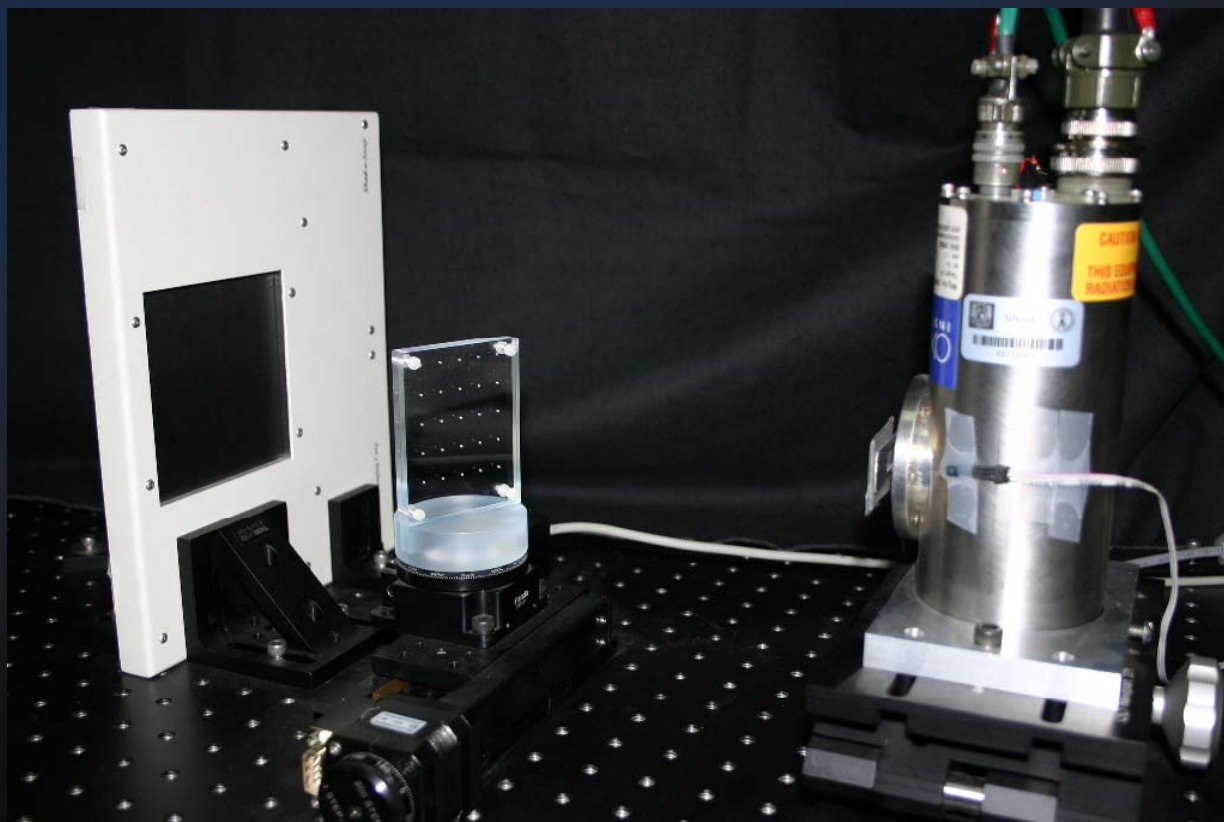




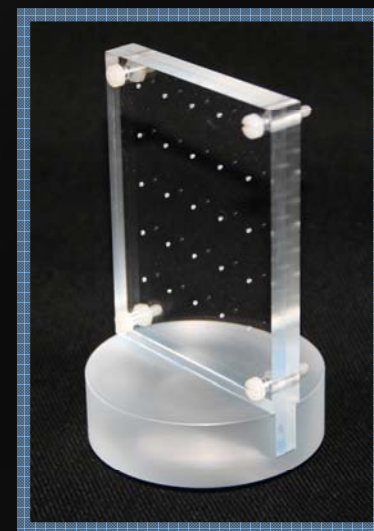
# Basic setup

Detector

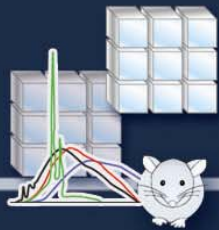
X-ray tube



X- $\theta$  stage







# mCT control panel

exposition\_motor\_temp\_shadobox2048\_05.vi

File Edit View Project Operate Tools Window Help

Image Save Path  
C:\Documents and Settings\All Users\Documents\2008-07-02 Rosita

Image Name  
rosi

High Voltage: 50 kV  
Current: 0.8 mA  
Degree Increment: 1  
Rotation Limit: 360  
Speed [°/seg]: 8

X-Ray: OFF  
Integration Time: 5min  
DAQ Name: PCI6024E

Full Acquisition: START STOP  
Single Acquisition: START

Linear stage: MOVE  
Rotational to zero: MOVE  
Warm Up: START  
microCT I/O: CHECK

50 kVp  
400 mAs

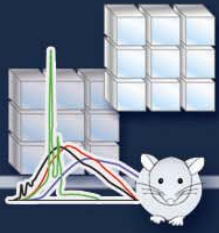
X-ray tube temperature: 27.2 °C

Left  
Up  
Right  
Image contrast level: 60

Image Number: 361  
Current Image: 182  
Current Position: 181

Message Window  
Single Acquisition Complete.  
Initializing Full Acquisition: Checking microCT blocks.  
-> Motorized rotation stage. Initialized OK.  
-> Shad-o-Box 2048 X-Ray Camera. Initialized OK.  
-> Folder path OK.  
-> KV & mA values reached. OK.  
Full Acquisition in progress . . .  
Full Acquisition Interrupted.

EXIT



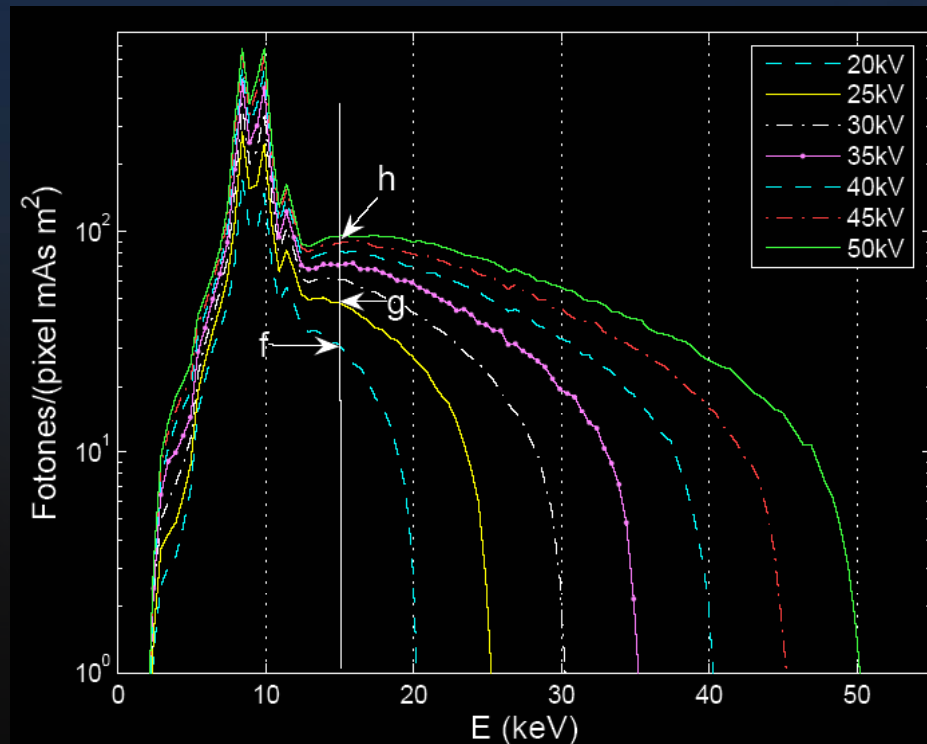
# Methods

- ❖ X-ray spectra: Amptek CZT detector
- ❖ FPN (flat field correction)
- ❖ MTF : Slanted edge technique
- ❖ NPS : 2D FT of relative noise distribution
- ❖ DQE :  $MTF^2 / (X \Phi_x NPS)$
- ❖ Dose performance : TLD & MC
- ❖ CT rec. : Feldkamp

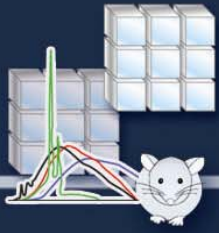


# X-ray spectra

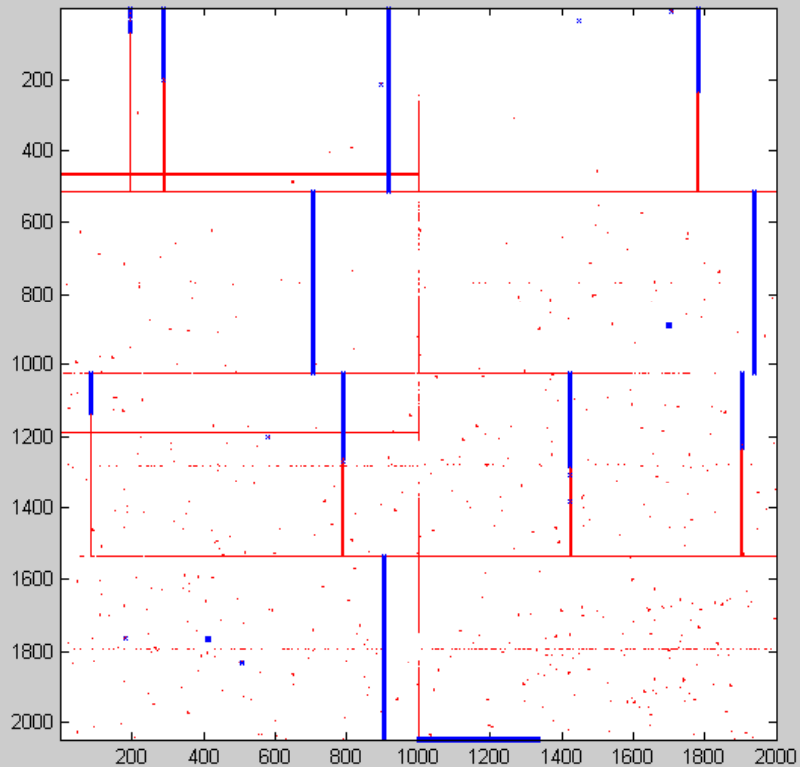
$$\Phi(E, V) = a(E)kV^3 + b(E)kV^2 + c(E)kV + d(E)$$



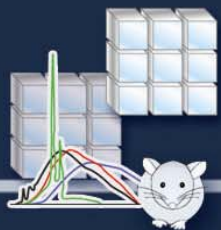
- ❖ Spectra
- ❖ Angular distributions
- ❖ Backscatter factors
- ❖ Output factors
- ❖ Half-value layers
- ❖ Parameterization



# Fixed Pattern Noise

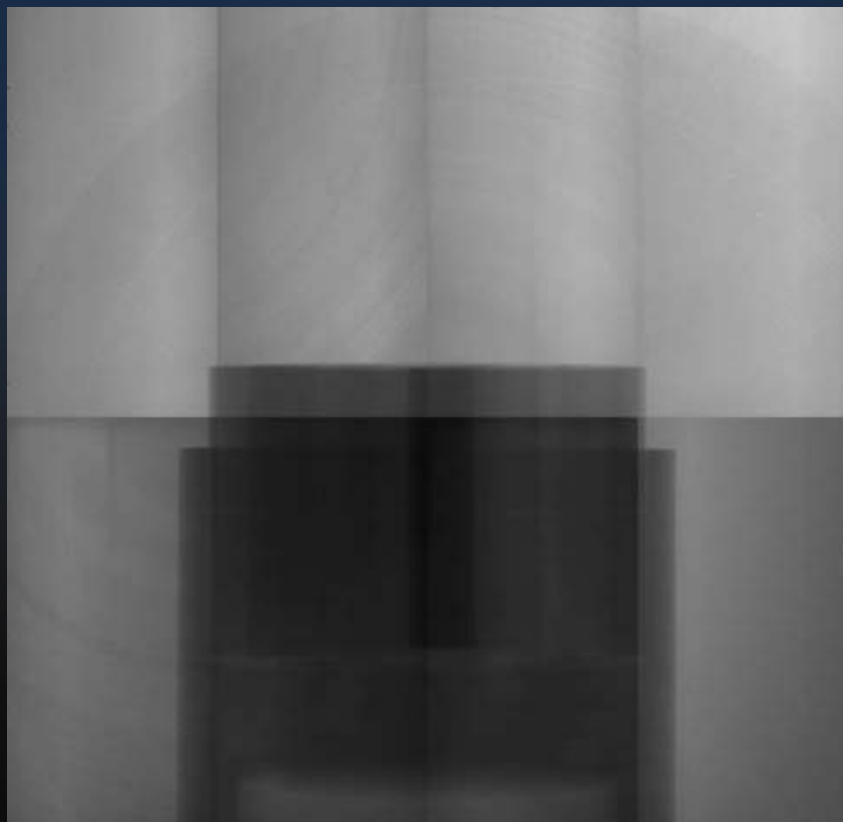


- ❖ **x** : dead pixels  
aprox. 0.1%
- ❖ **o** : outliers  
aprox. 1.0%

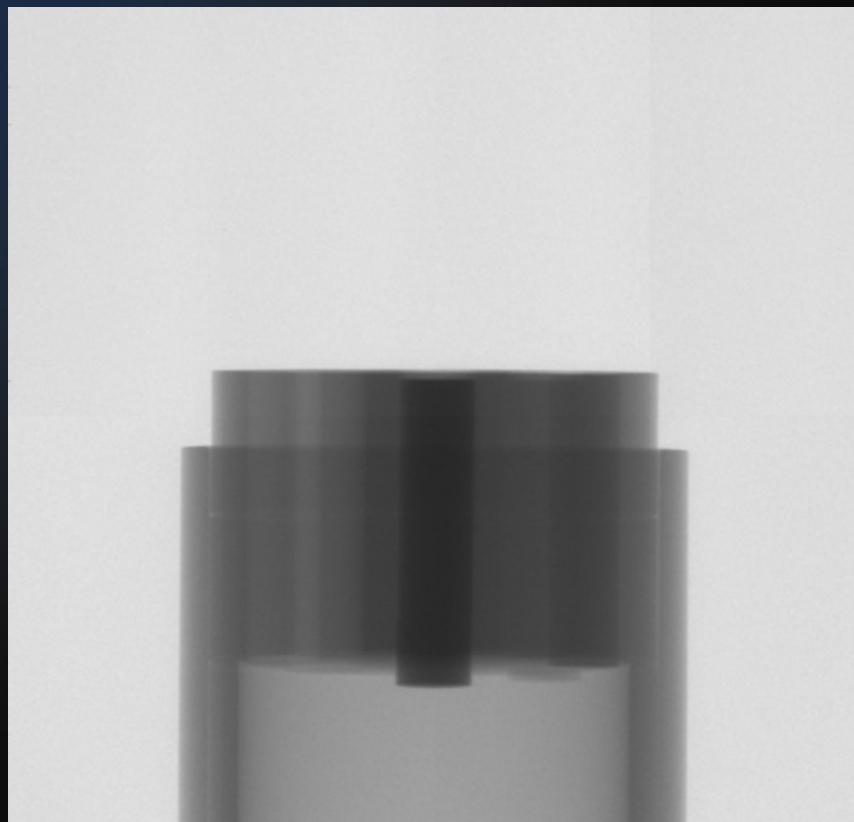


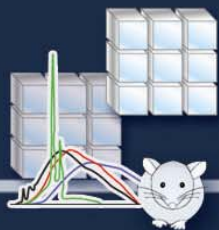
# Flat field correction

Non-uniform response

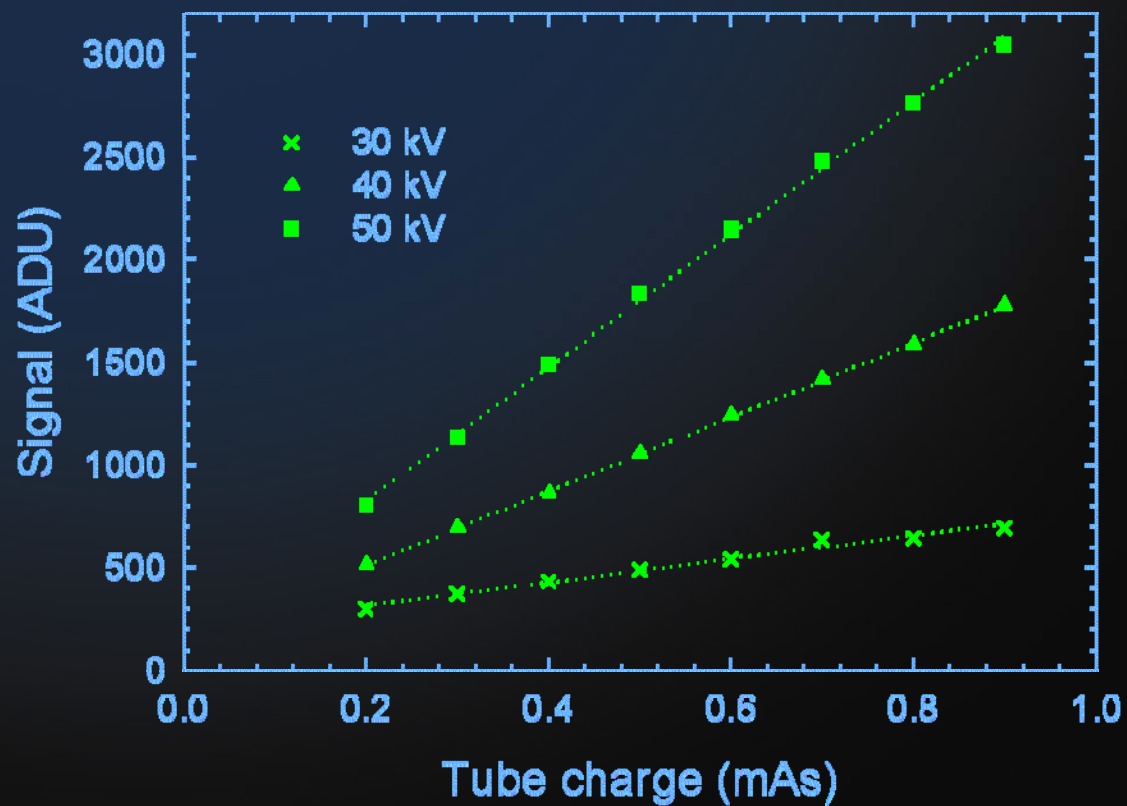


Corrected



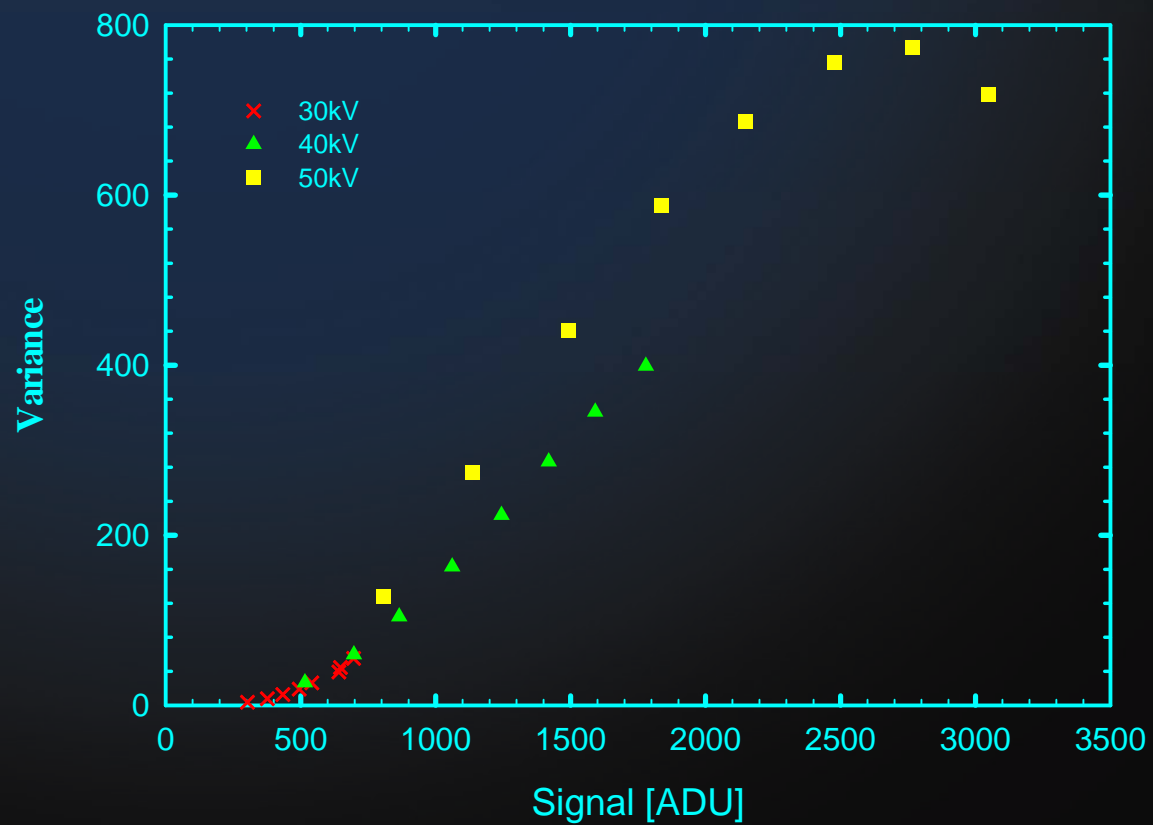
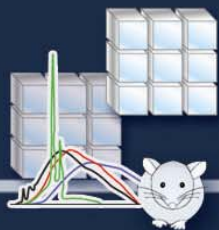


# Linearity of response

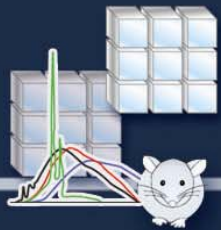


Oxford Instruments Apogee W, 1 mm Al, 1 mAs

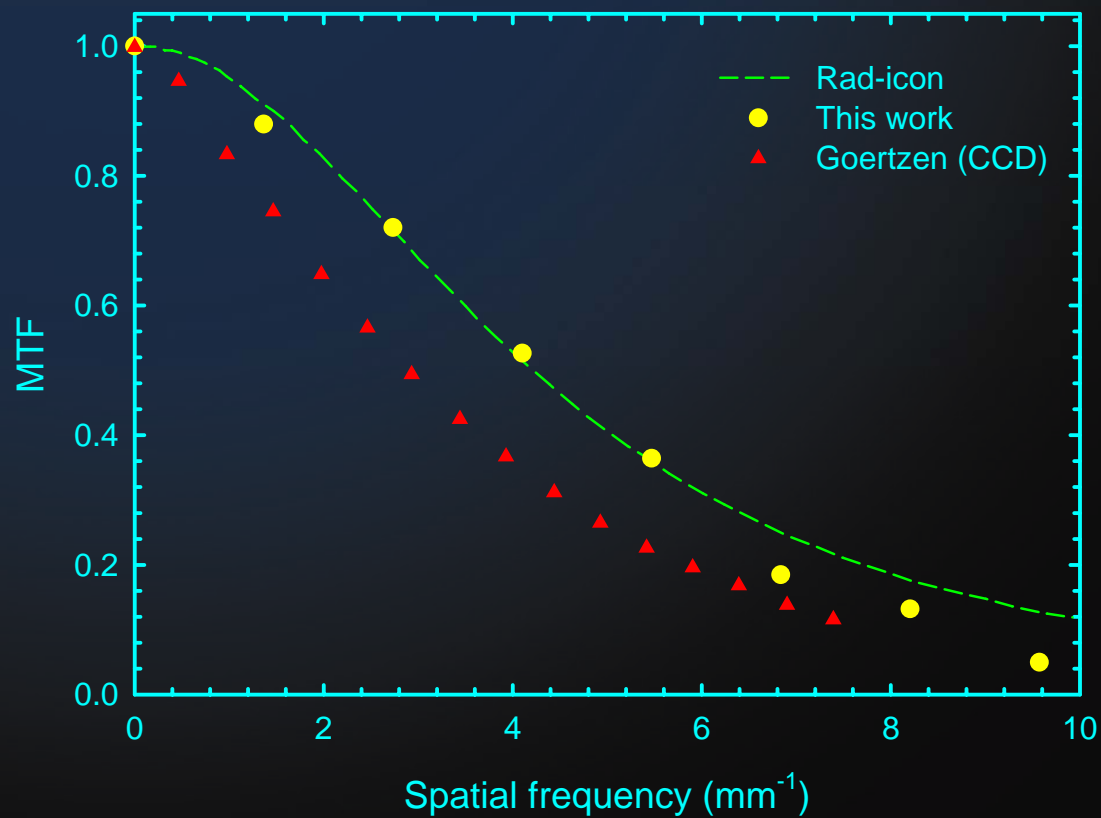
# Noise



Oxford Instruments Apogee W, 1 mm Al, 1 mAs



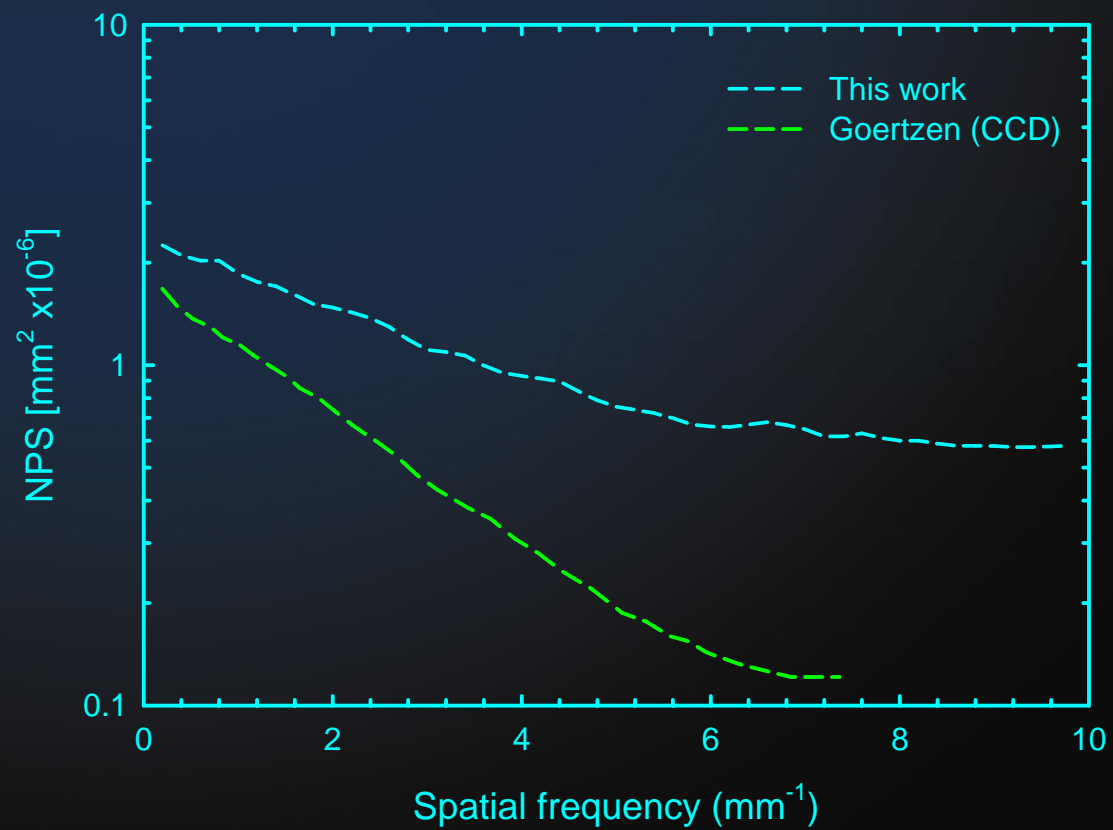
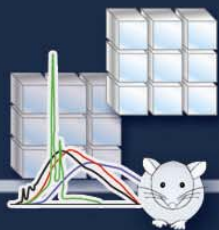
# Presampling MTF



Spatial resolution at 10% MTF ~ 10 lp/mm

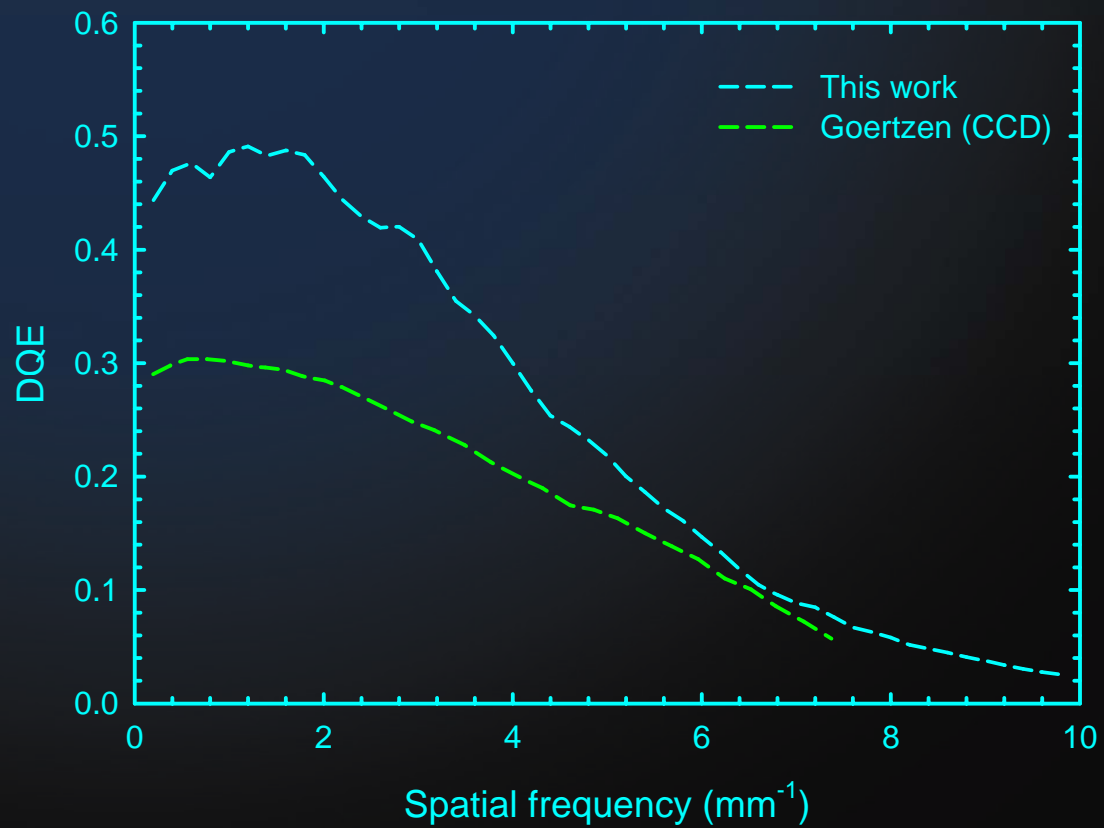
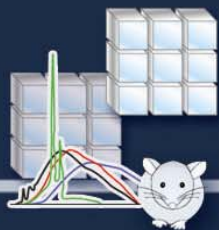


# NPS

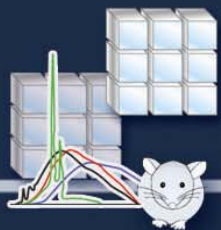


W 40 kVp, 0.5 mm Al, 30 mR

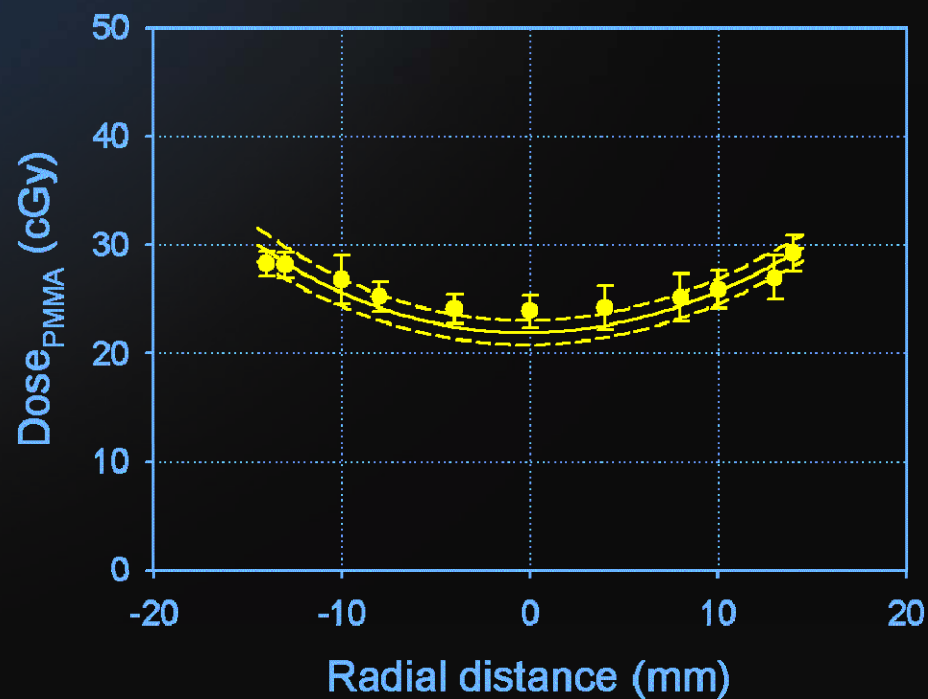
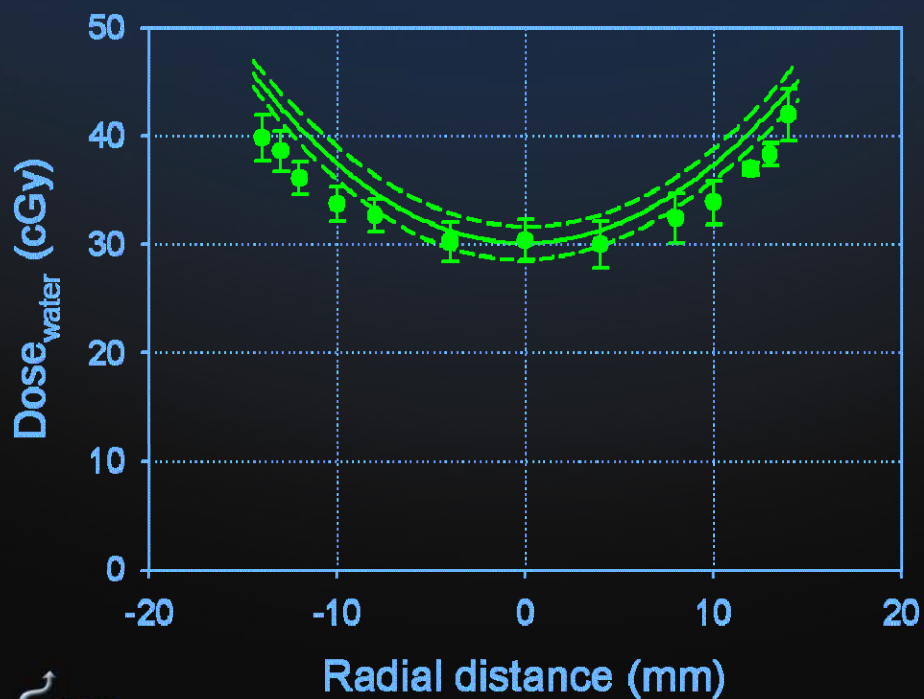
# DQE

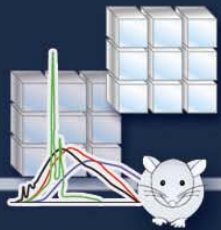


$$DQE = MTF^2 / (X \Phi_x NPS)$$

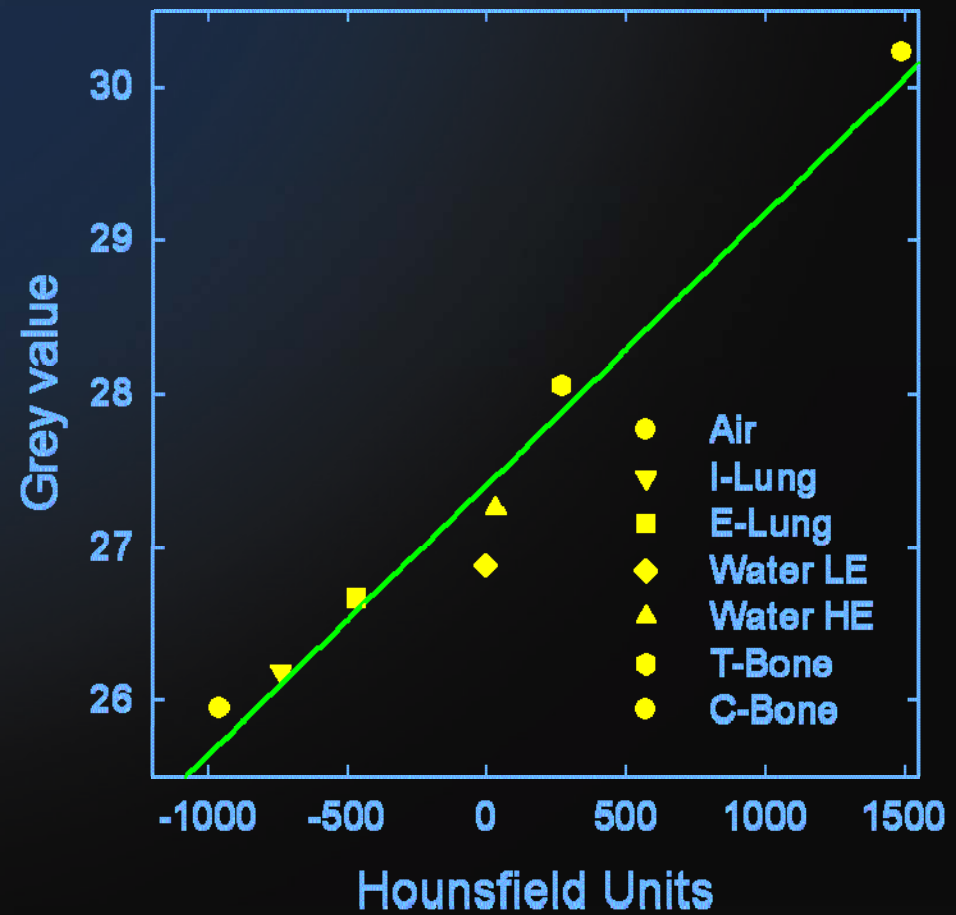
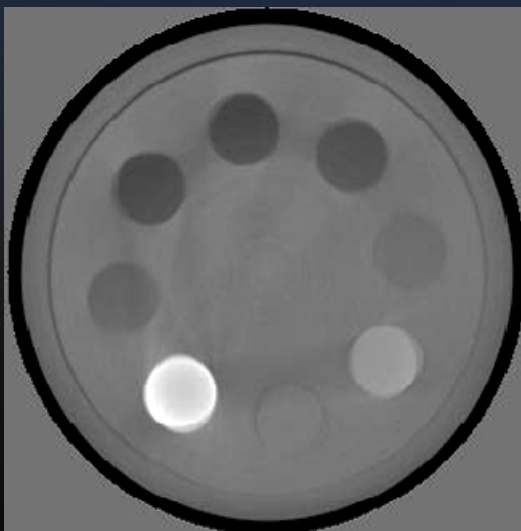


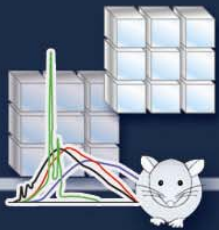
# Dose measurements & simulations





# Calibration in HU

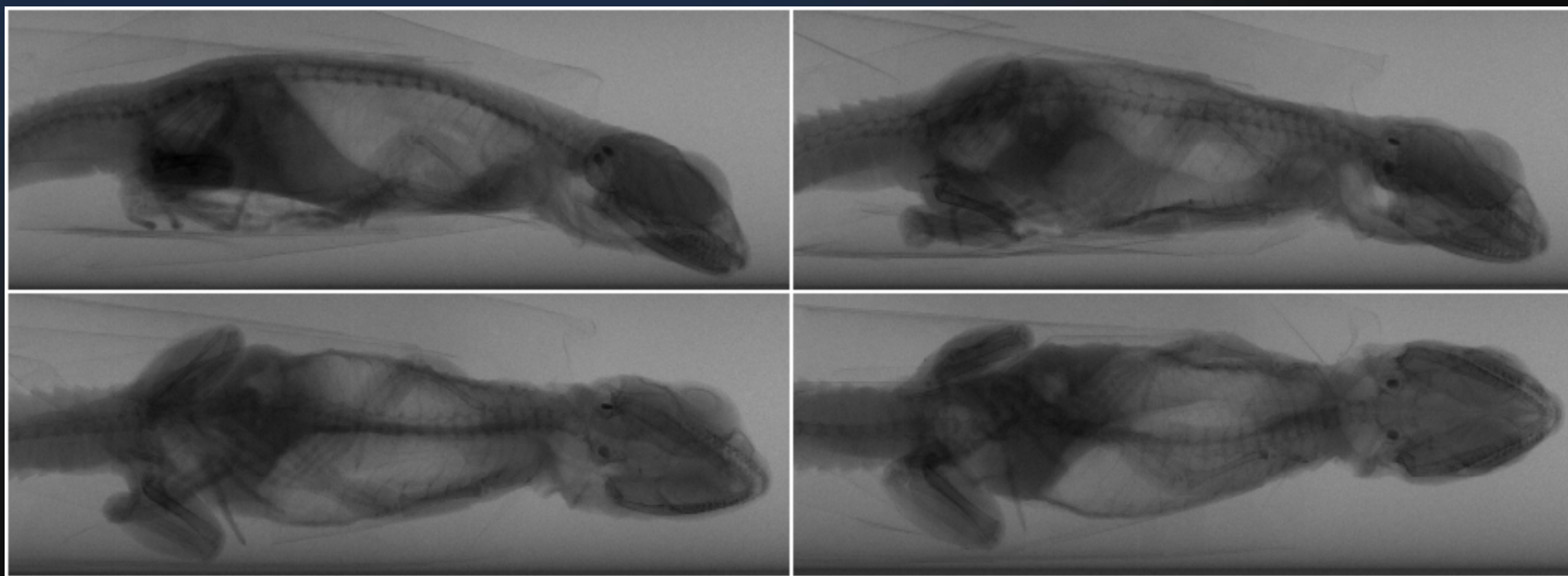


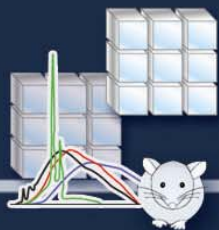


# Mexican Iguana

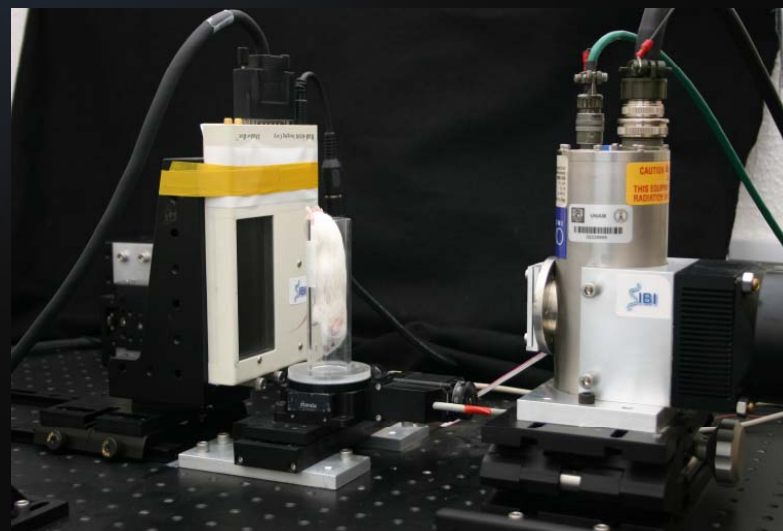
W target, 1.0 mm Al, 30 kVp, 0.5 mAs

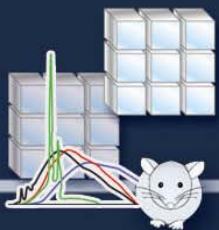
Body length ~ 4 cm





# First mCT of a mouse (*ex-vivo*)

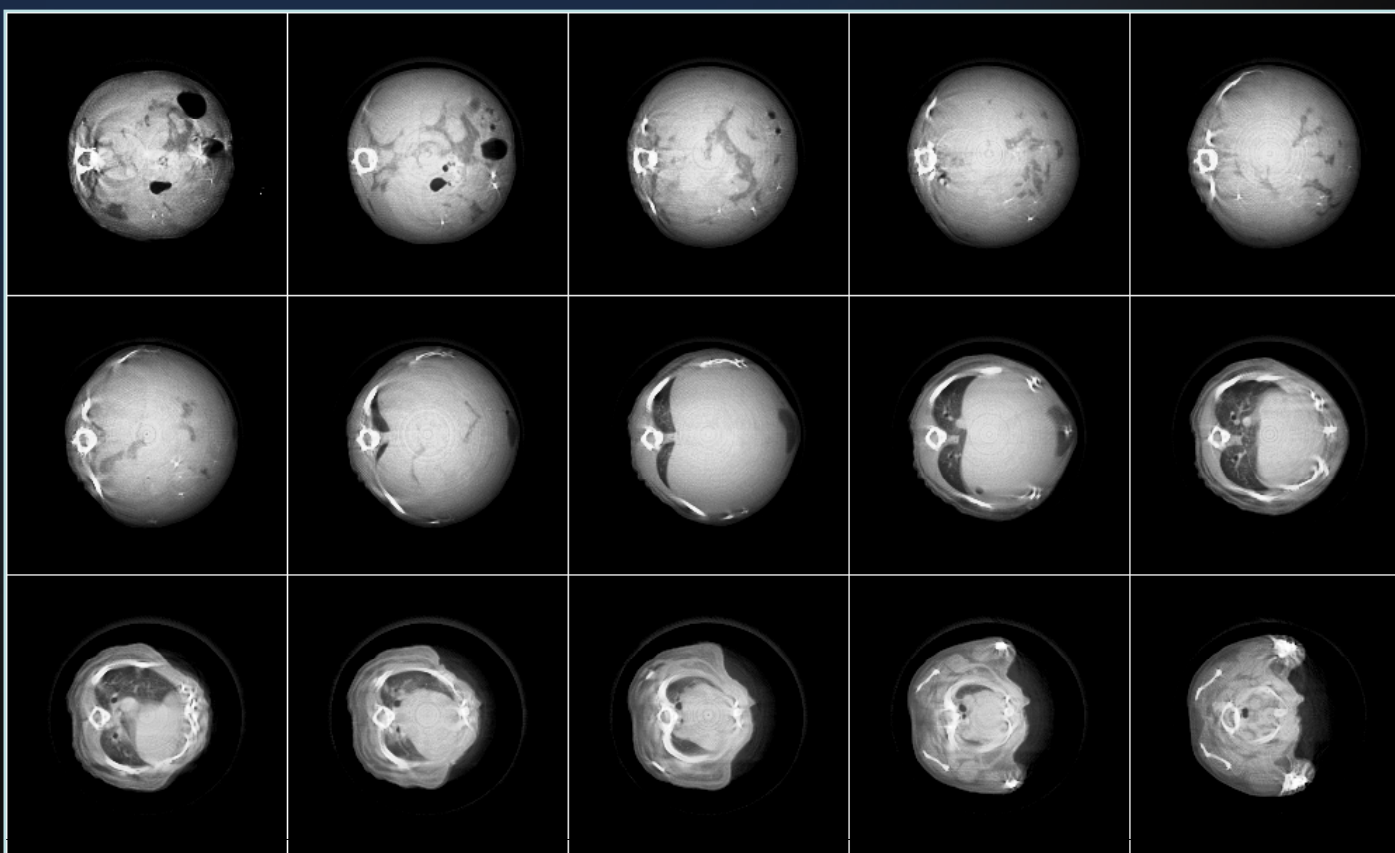


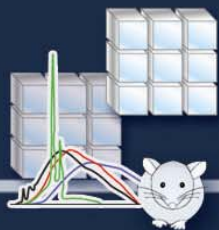


# CT reconstruction, axial slices

W 50 kVp, 0.5 mAs, 1 mm Al, 360° orbit, 1° steps

Feldkamp, Hann filter, 0.7 cutoff frequency





# Conclusions

- ❖ We have built and characterized a benchtop microCT prototype
- ❖ Detector performance:
  - Excellent spatial resolution ( $\sim 10$  lp/mm @ 10% MTF)
  - Good noise performance
  - Very good DQE (40-50% at low spatial frequencies)
- ❖ Successful image acquisitions and tomographic reconstructions

To do:

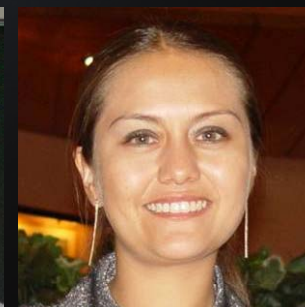
- ❖ New detector, faster data transfer
- ❖ Use of contrast media and/or dual energy techniques
- ❖ Integration of microCT with microPET





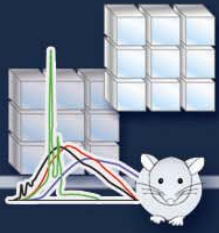
# Participants

## Faculty



## Students





# Human vs. mouse

## Human – 70 kg

### CT

- ❖ 100-120 kVp
- ❖ Spatial resolution ~0.4 mm
- ❖ Ring geometry
- ❖ Dose ~2-20 mGy

### PET

- ❖ Spatial resolution 2-3 mm
- ❖ Activity ~ 10-15 mCi
- ❖ Sensitivity ~ 2-4%

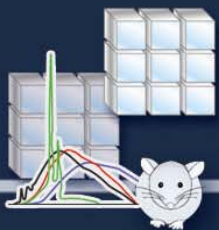
## Mouse – 30 g

### microCT

- ❖ 30-80 kVp
- ❖ Spatial resolution ~50  $\mu$ m
- ❖ Flat panel detectors
- ❖ Dose ~30-300 mGy

### microPET

- ❖ Spatial resolution 1-2 mm
- ❖ Activity ~ 0.5 mCi
- ❖ Sensitivity ~ 3.5%



# Reconstruction parameters

	Ramp	Shepp-Logan	Cosine	Hann	Hamming
SNR	24.7	22.9	25.8	25.2	26.7
CNR	3.5	3.9	4.8	5.2	5.1

