

# Upstream Dosimetry using a Monolithic Active Pixel Sensor (MAPS)

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# Overview

 Radiotherapy.

 Motivation for online monitoring and verification.

 Current upstream system.

 Multi Leaf collimator edge reconstruction.

 Upstream dosimetry.

 Conclusion.

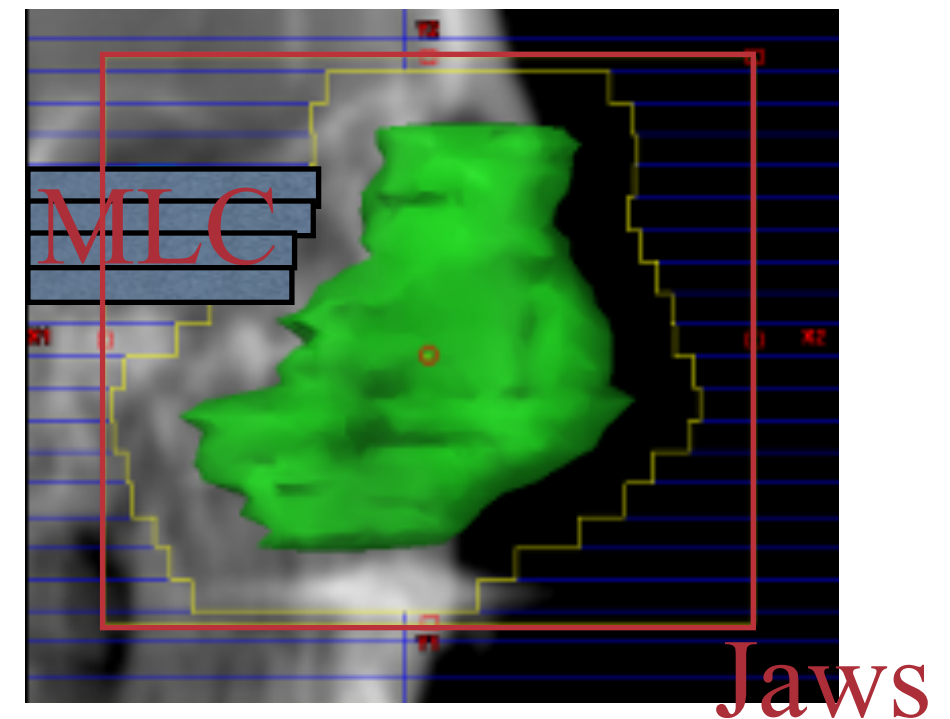
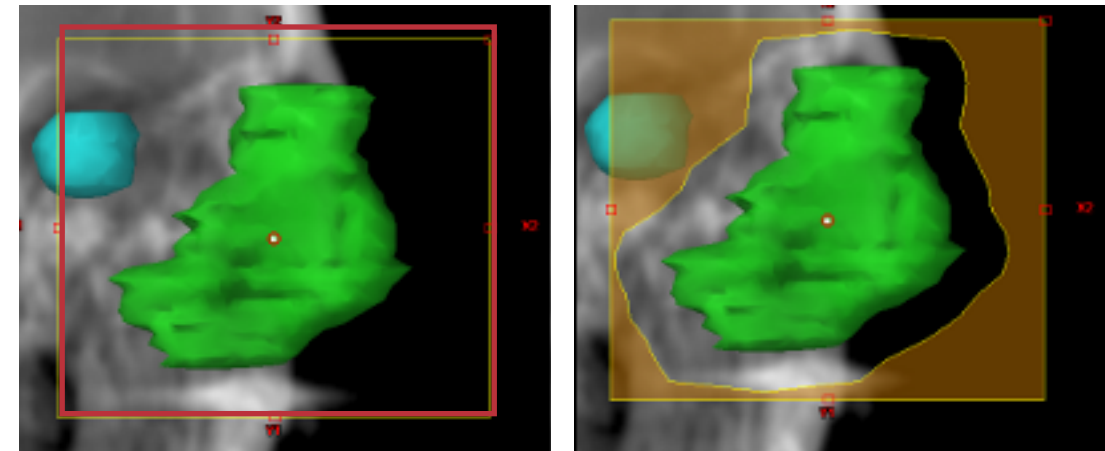
# Radiotherapy

✿ Important treatment for patients with cancer - used in 40% of curative cases.

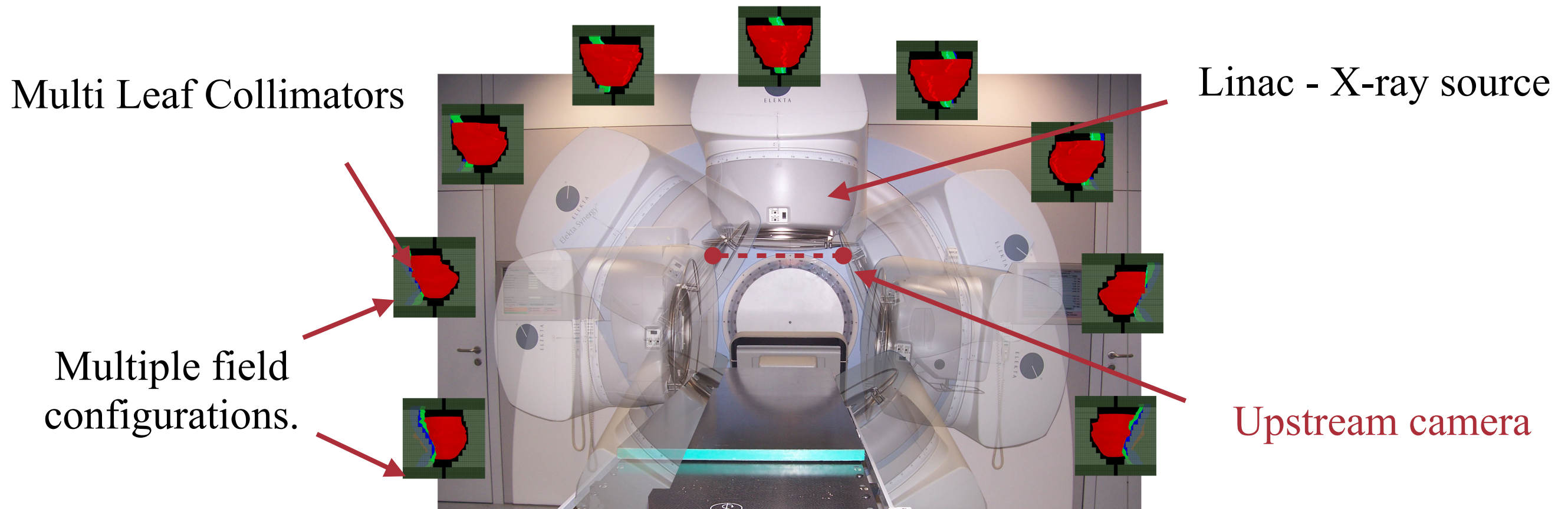
✿ Uses MeV X-rays to kill tumour cells.

✿ Intensity Modulated Radiotherapy uses Multi Leaf Collimators (MLC) to conform dose to the tumour.

✿ Spares the healthy tissue.



# Intensity Modulated Radiotherapy



**Measure:** Dose and Collimator Positions.



# Motivation for Online Monitoring

- ✦ **Safety:** Treatments are complex - Chief Medical Officer in the UK endorsed report calling for independent monitoring of IMRT.
- ✦ **AIM:** In case of gross error stop treatment.
- ✦ **Time:** Increase patient throughput through use of online verification - National UK Cancer Action Team strategy is to aim for 30% of radiotherapy courses to use IMRT by 2012.
- ✦ **AIM:** Increase efficiency up from the order few %.

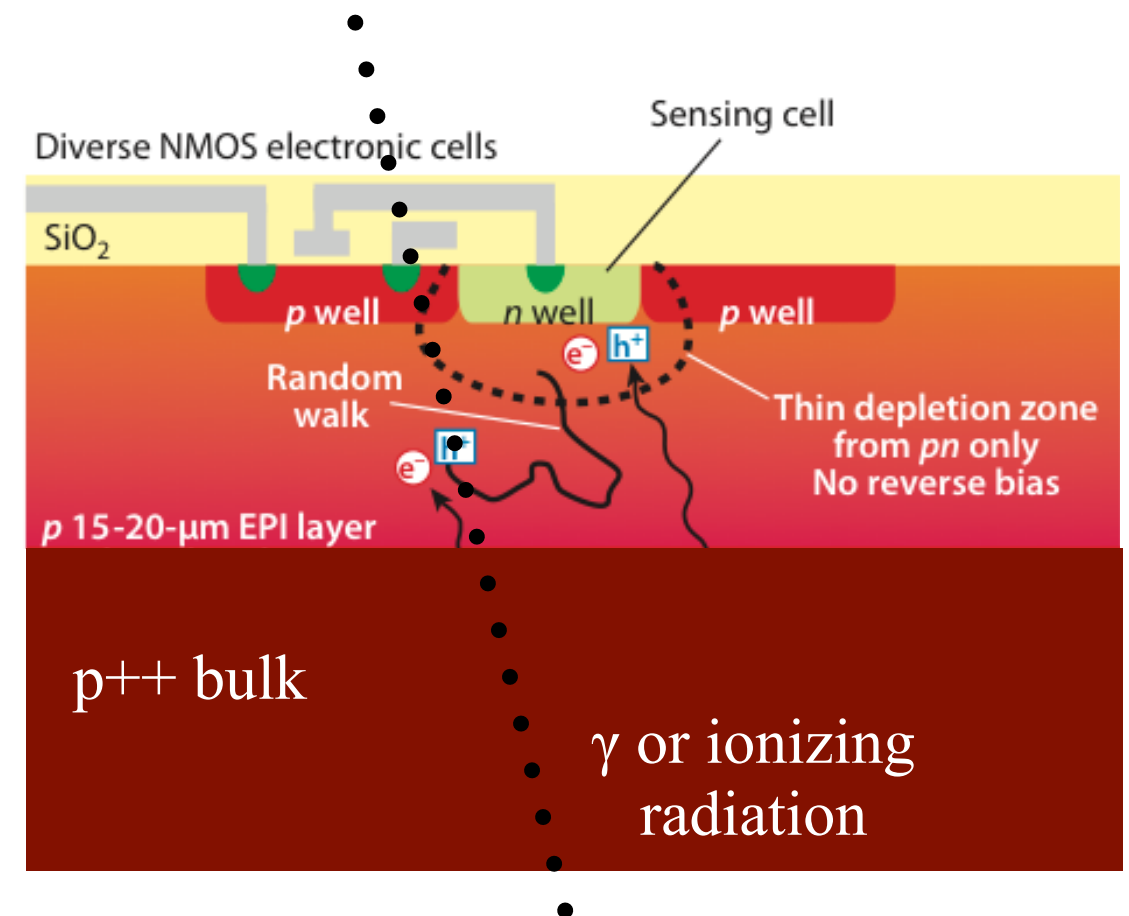
# Rationale for MAPS

🔥 Attributes:

🔥 Fast  $\Rightarrow$  Treatment time feedback.

🔥 Good S/N  $\Rightarrow$  Precise monitoring.

🔥 Thin  $\Rightarrow$  Low attenuation of therapeutic photons.



# ACHILLES Sensor

✶ Thickness 100 $\mu$ m - 0.1 %  
attenuation for 2 MeV  
photons.

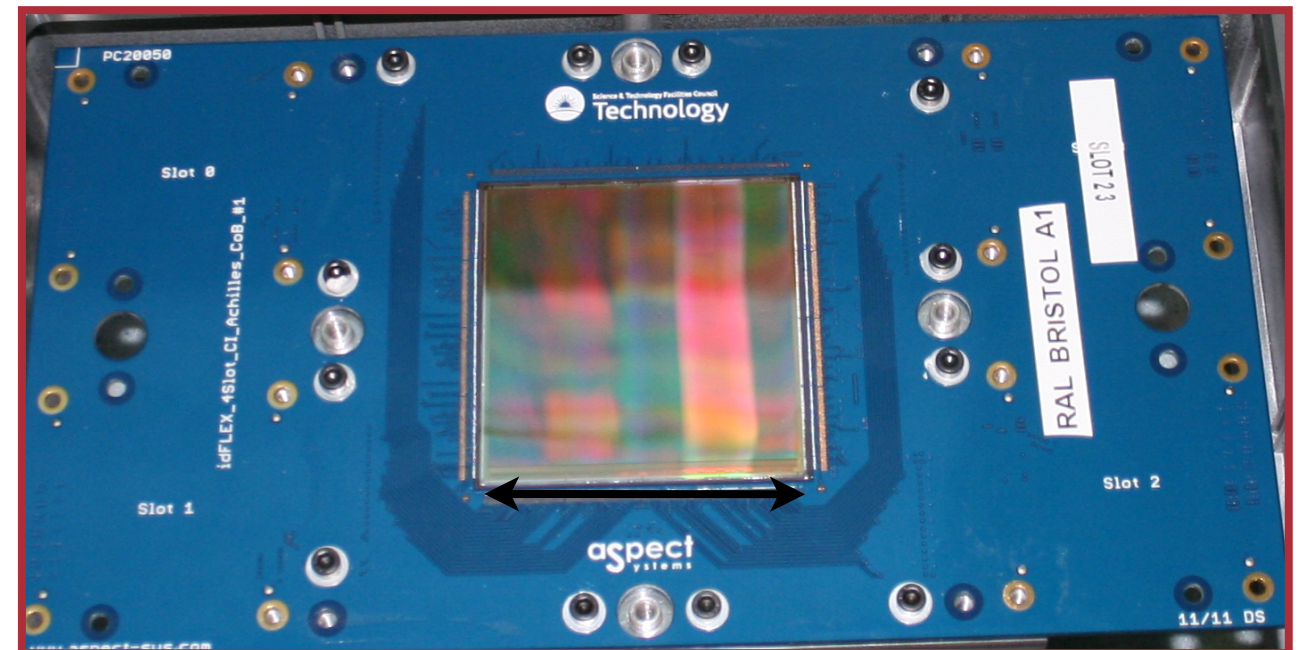
✶ 14 $\mu$ m epitaxial layer.

✶ 4096 x 4096 pixels.

✶ 3T pixels 14.5 $\mu$ m pitch.

✶ S/N for Fe<sup>55</sup> ~16.

✶ 40 fps - **Fast Readout.**



~ 6cm

N. Guerrini, R. Turchetta, and et al.

A High Frame Rate 16 million pixels radiation hard CMOS sensor.  
*Journal of Instrumentation*, Volume 6, March 2011.

Previously presented at IWORID, 11-15th July 2010.

# Current Upstream System

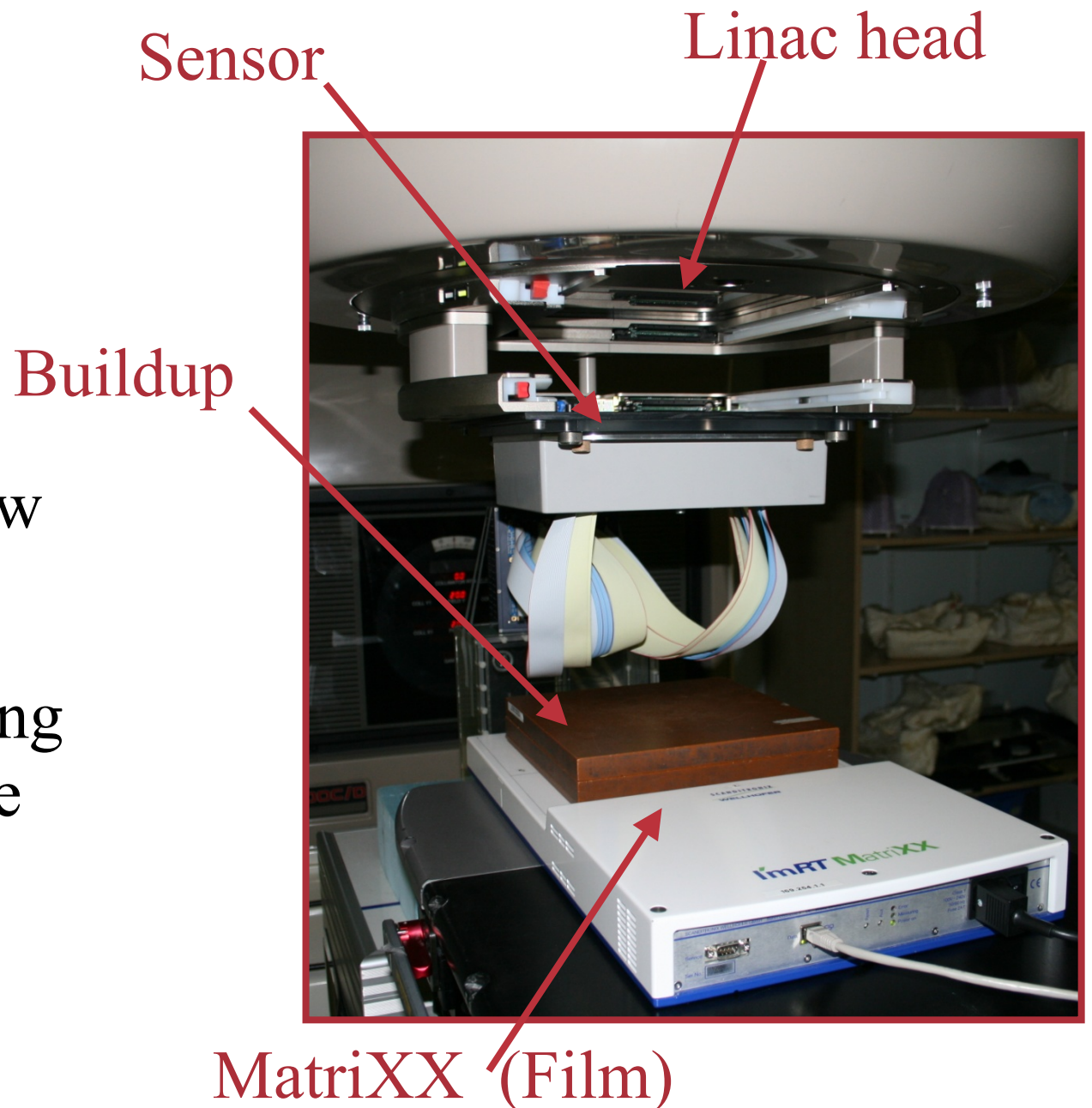
✦ Radiochromic film / MatriXX placed at 100cm from source (isocentre) with 5 cm of build up.

✦ Operational Settings:

✦ Specific MLC fields used to allow field reconstruction to be tested.

✦ Linac operated at nominal working conditions of 400 MU/min (Pulse Repetition Frequency  $\sim$  400Hz).

✦ Sensor running at 10 fps.

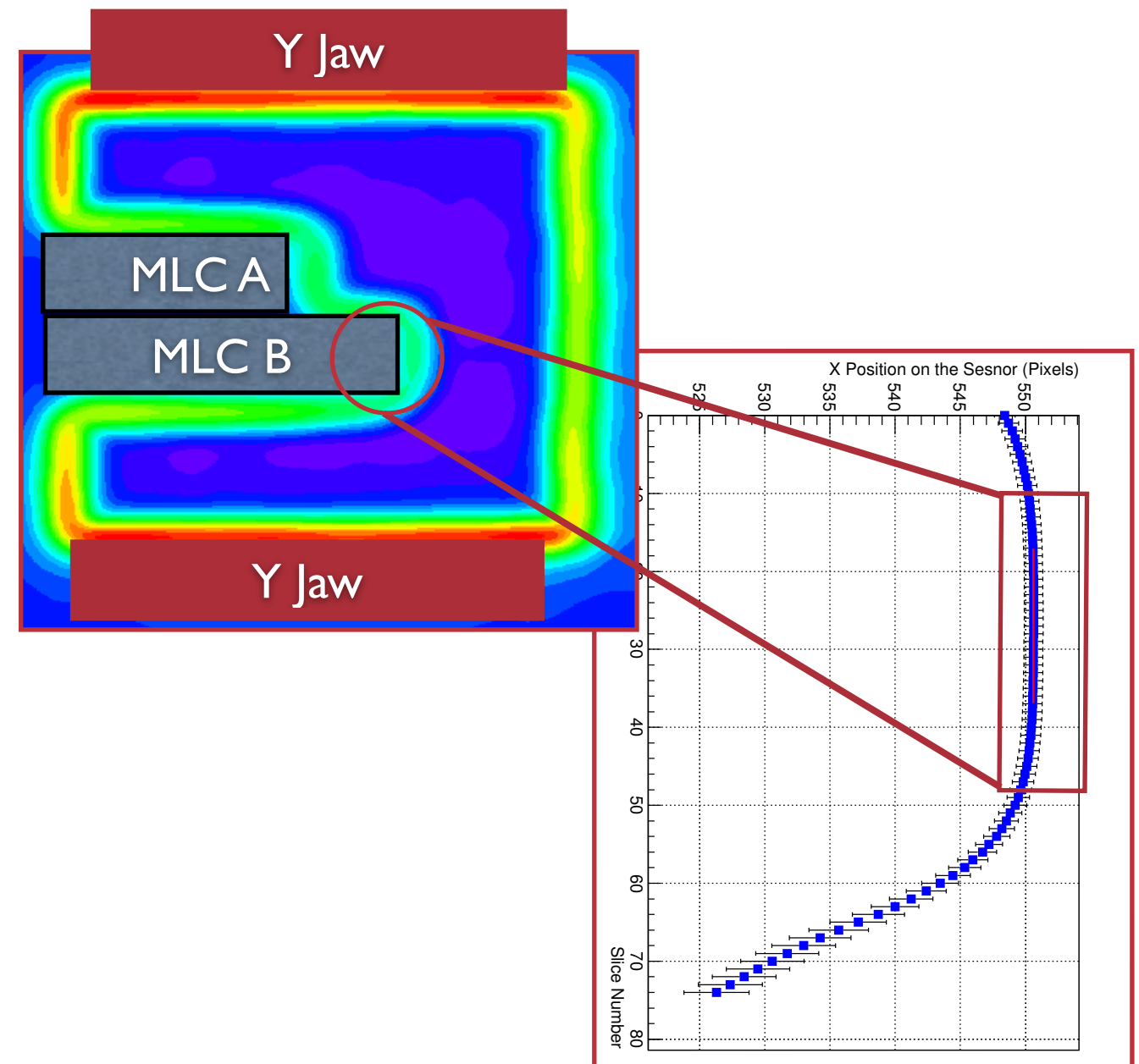




# Leaf Edge Reconstruction

## Image Processing:

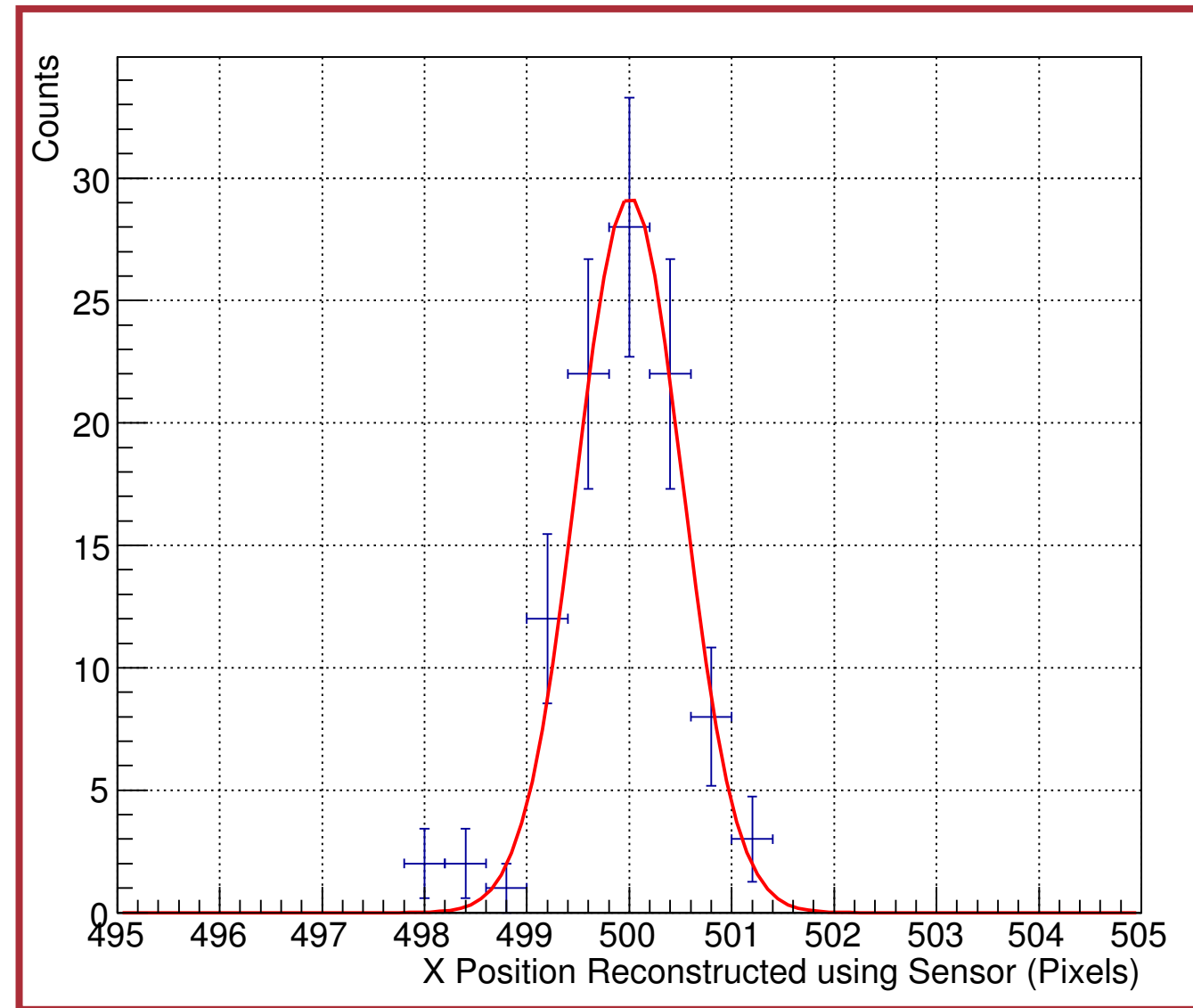
- Resize image to 1024 x 1024, Smooth image with gaussian kernel, convolute with Sobel gradient kernel.
- Combine images using the magnitude.
- Use points with minimum change along contour to define leaf position.





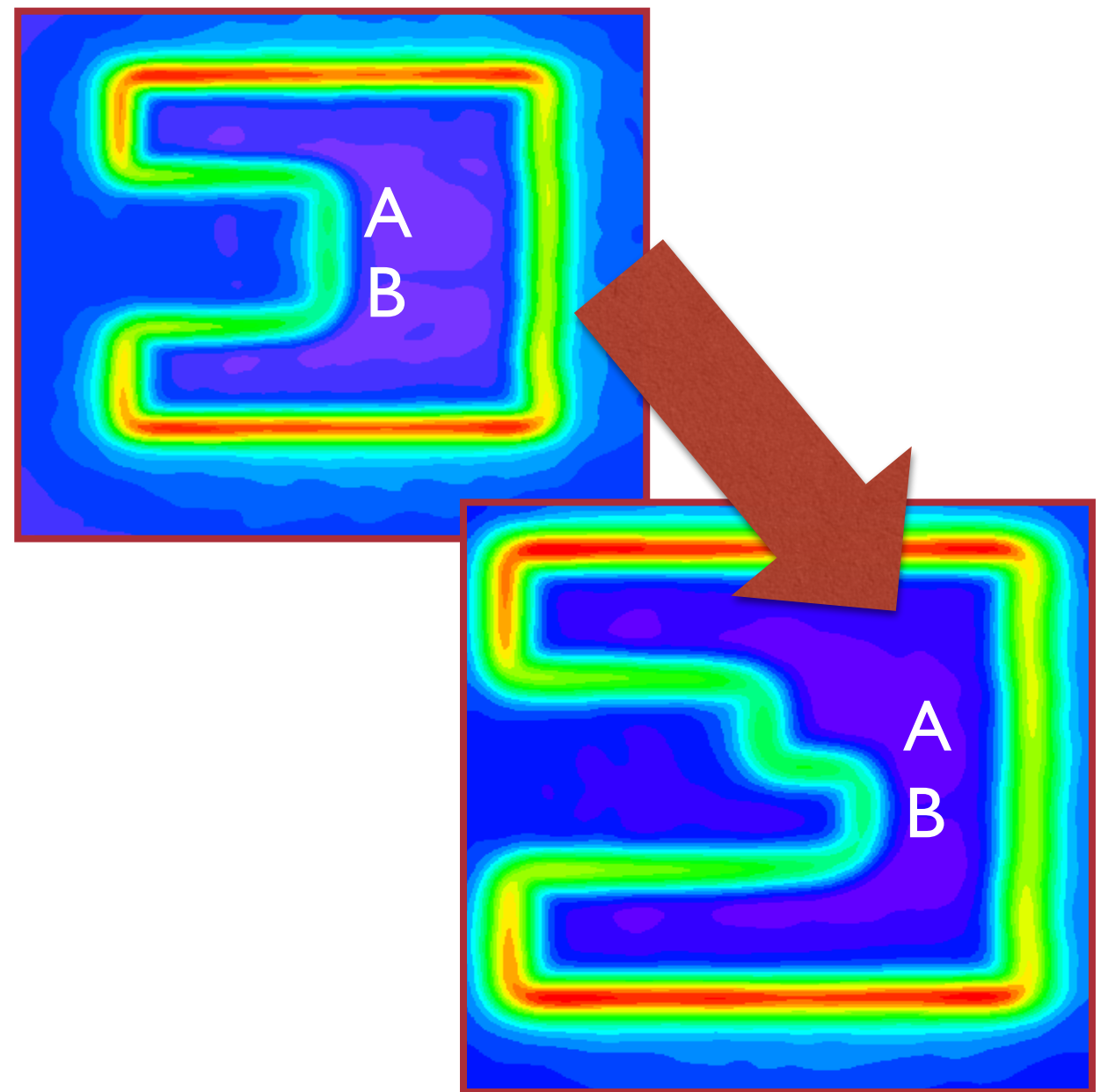
# Leaf Reconstruction Precision

- Quantise the precision of reconstruction using the distribution for 100 single frames.
- Results in precision at the iso-centre of  **$52 \pm 4 \mu\text{m}$**  and  **$6 \mu\text{m}$**  for **10 seconds** of data.



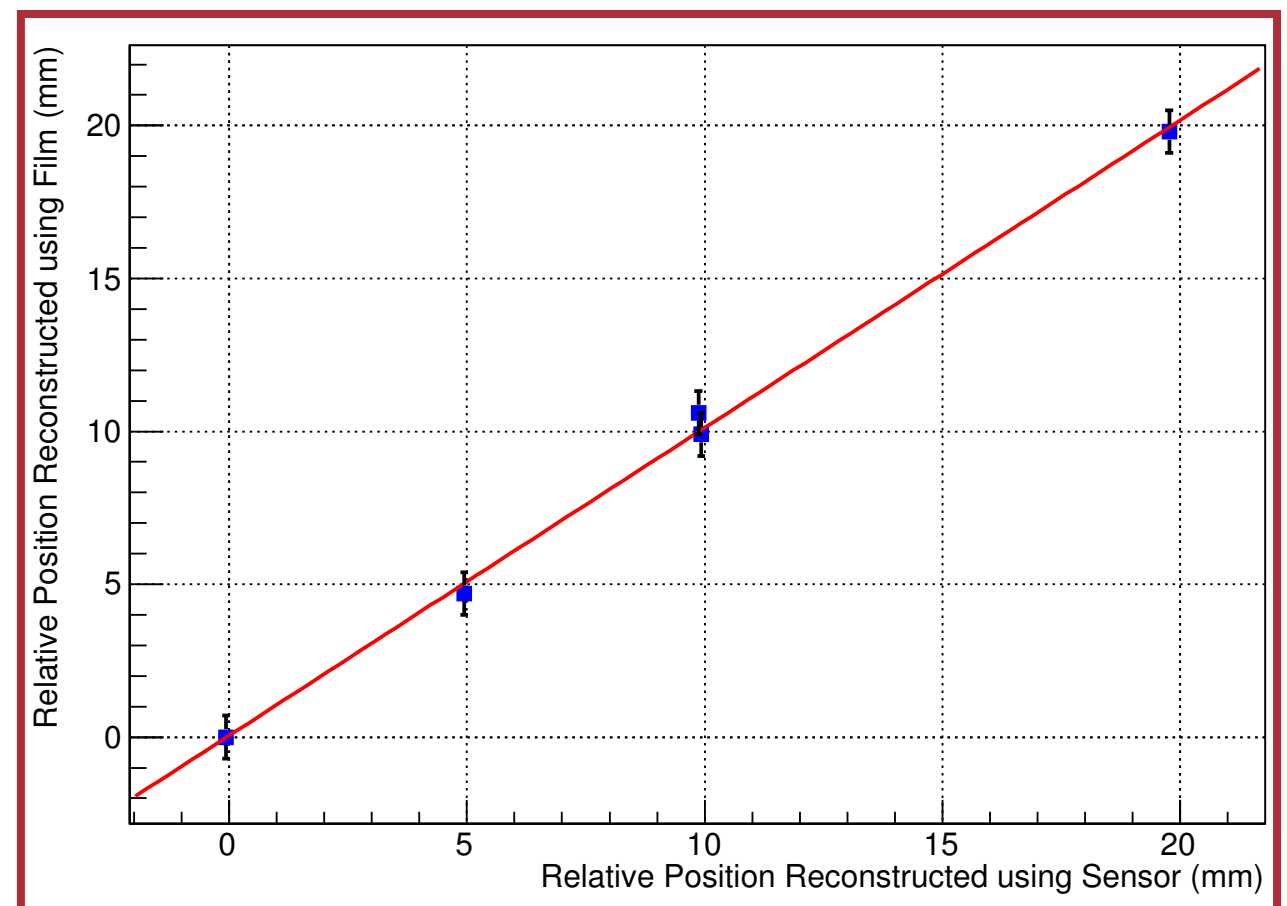
# Leaf Reconstruction Accuracy

- ✦ Analysed accuracy using radiochromic film as a benchmark.
- ✦ **Test:** Move MLC B with respect to MLC A and reconstruct difference.
- ✦ Compare reconstructed difference with film measurement.



# Leaf Reconstruction Accuracy

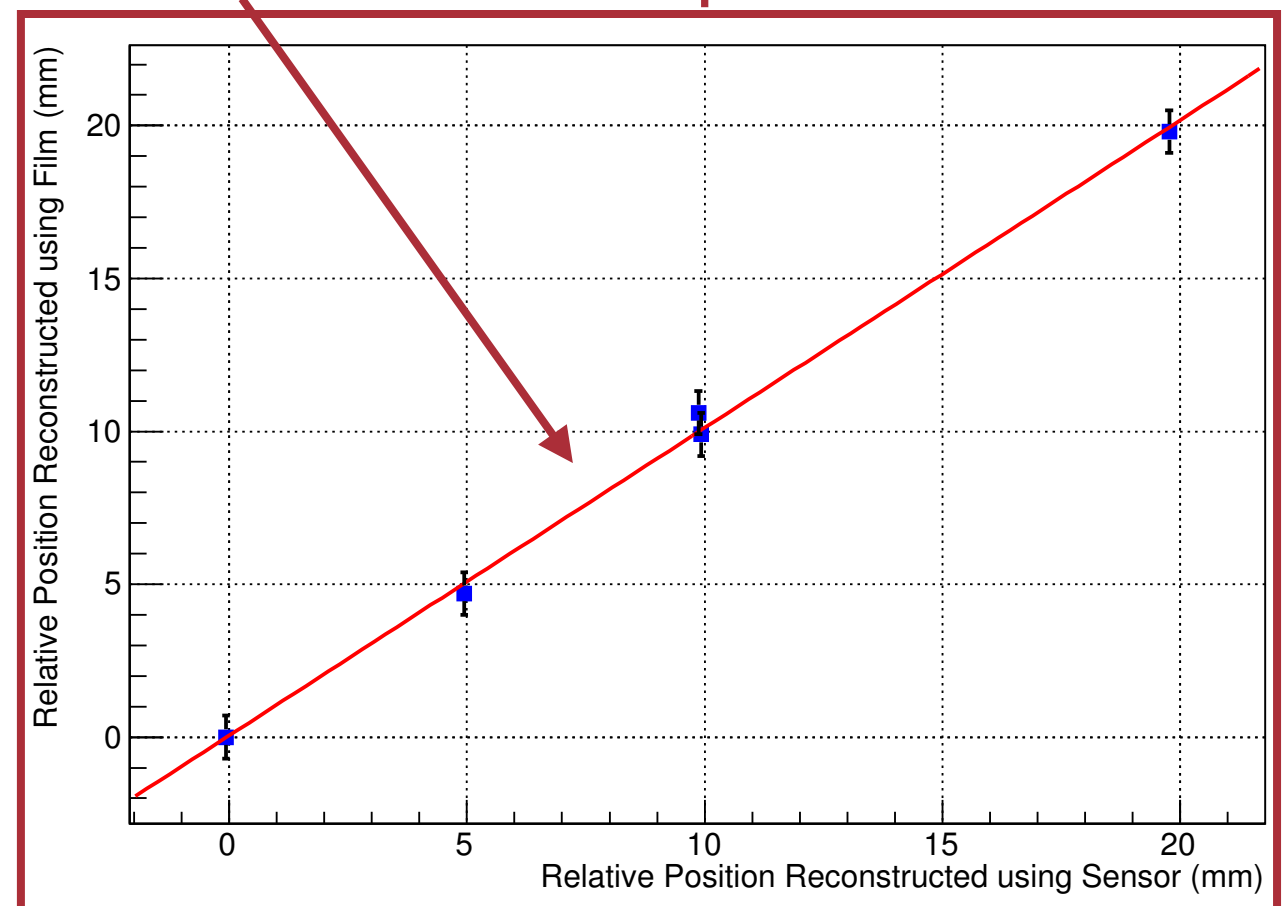
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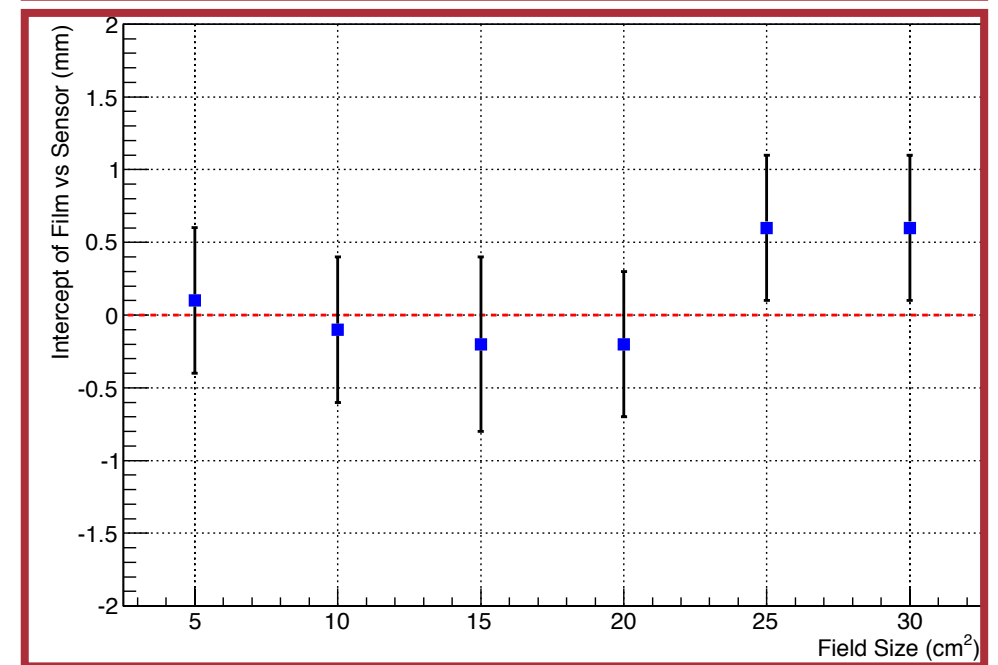
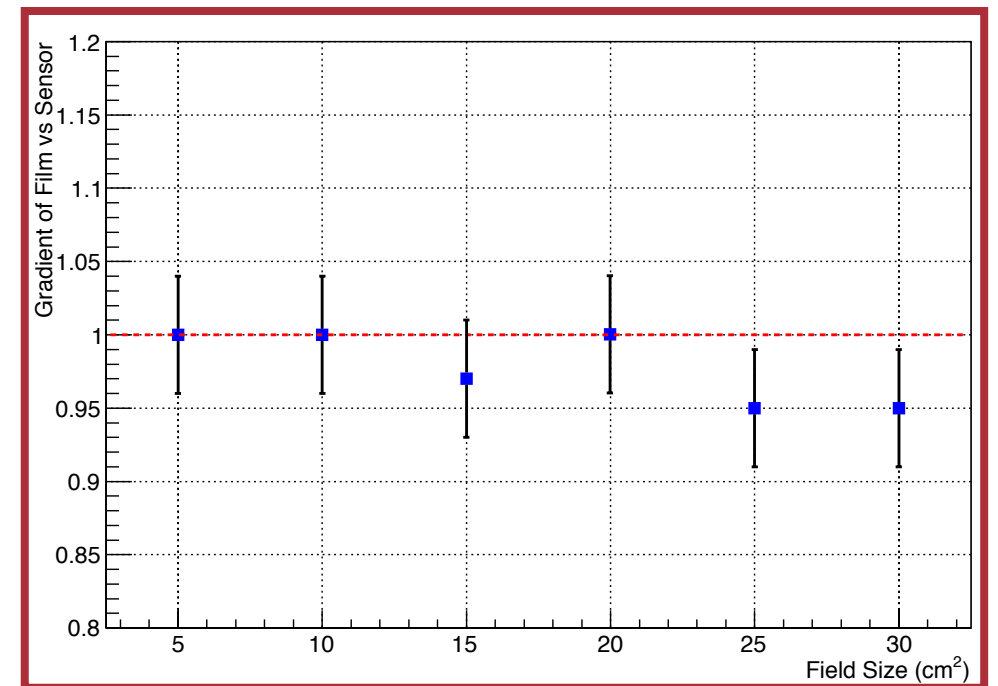
Expect linear relationship with gradient of 1 and intercept of 0

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# Leaf Reconstruction Accuracy

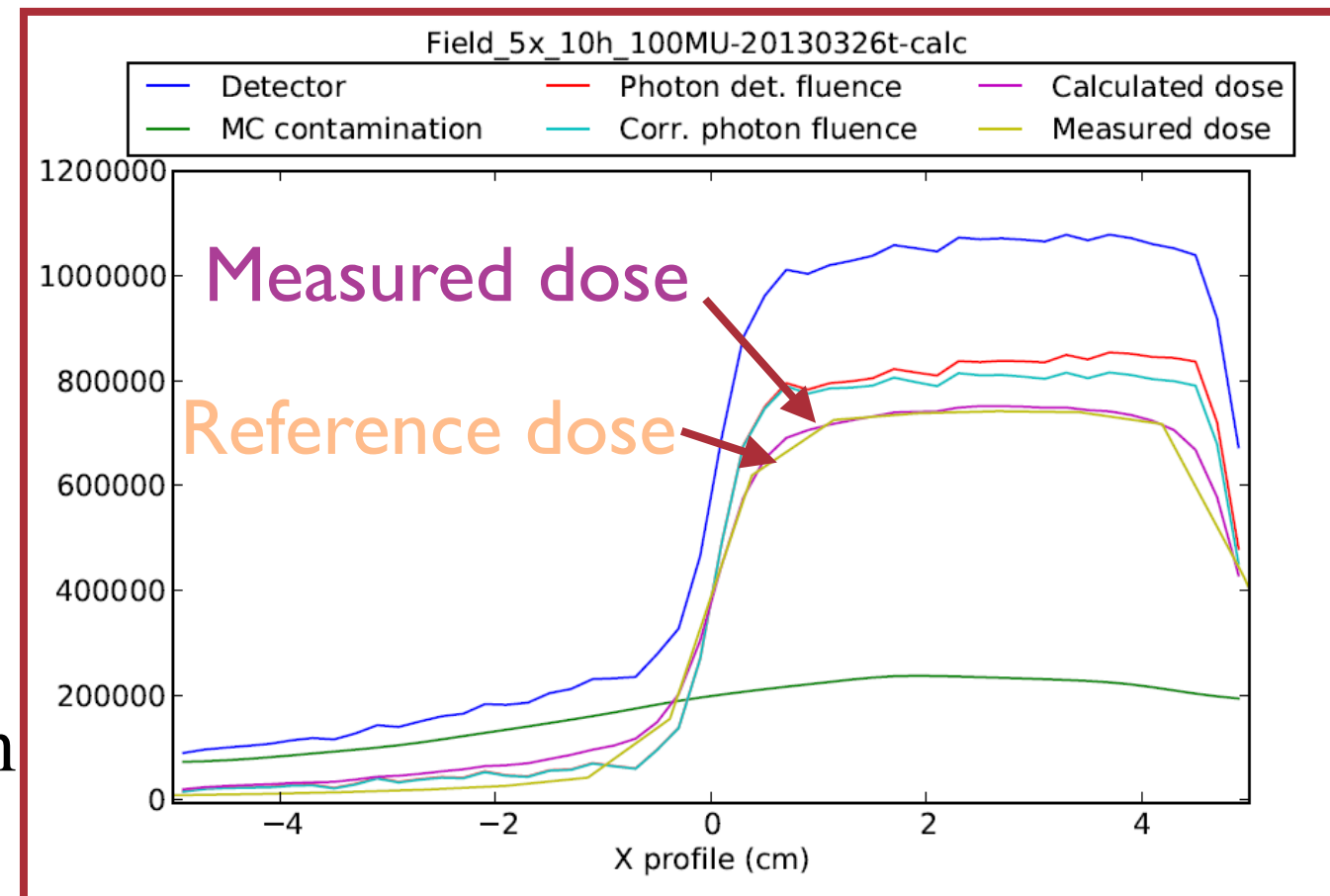
- Carried out test for six square fields.
- Excellent linearity - all measurements within 0.05 of 1.
- Method independent of field size and does not require MC modelling.





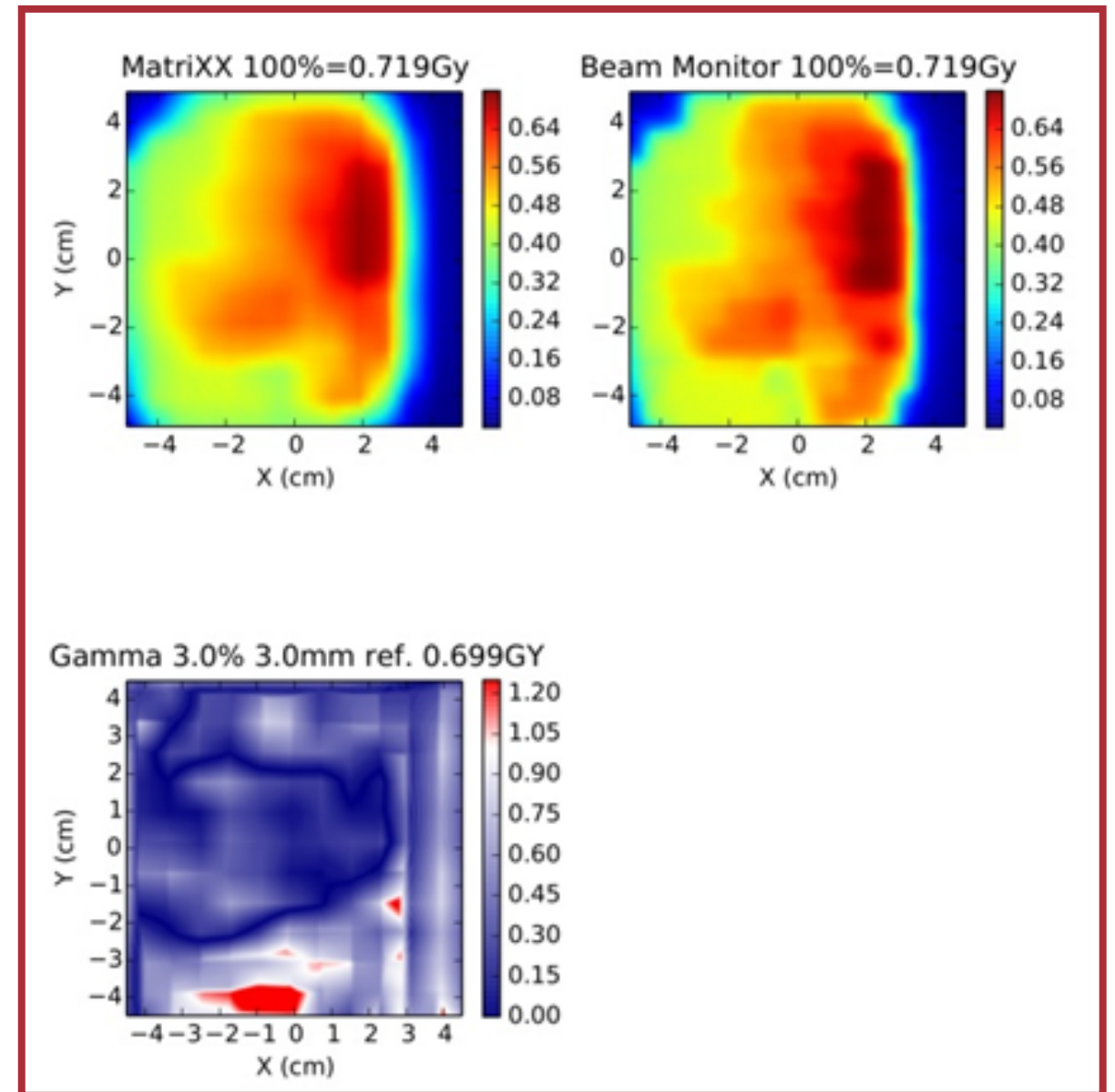
# Upstream Dosimetry

- ✦ Use MC model of linac and detector to convert signal in the detector into photon fluence.
- ✦ Use dose kernel to convert from fluence at the detector to dose in the phantom / patient.
- ✦ Compare with measured dose from the MatriXX.



# Upstream Dosimetry Results

- ✧ 2D IMRT distributions reconstructed from sensor and MatriXX.
- ✧ Anterior H&N fields compared.
- ✧ Gamma Factor -
  - ✧ 97% of points  $\leq 1$  for 3% and 3mm.
  - ✧ Excellent agreement.

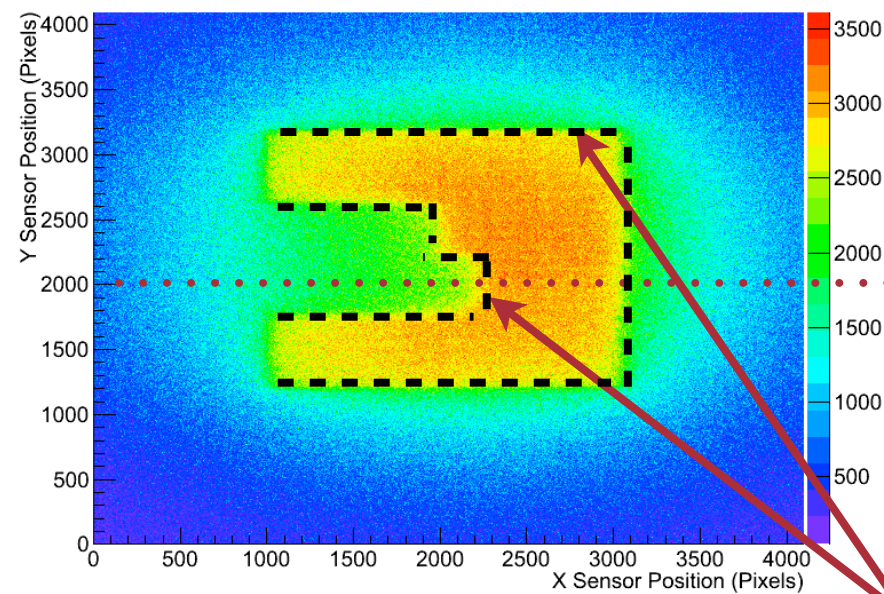
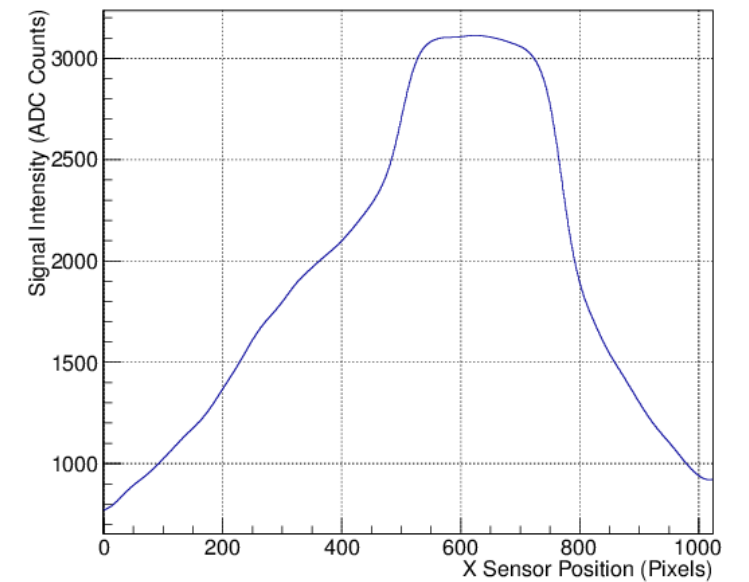
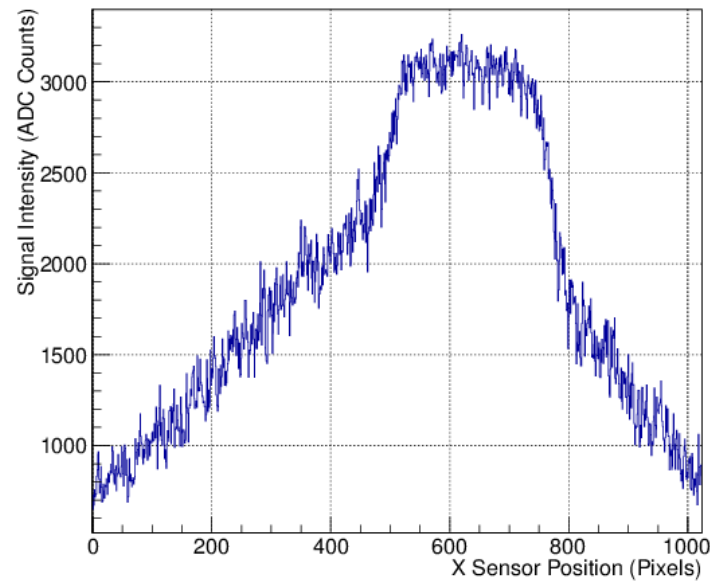
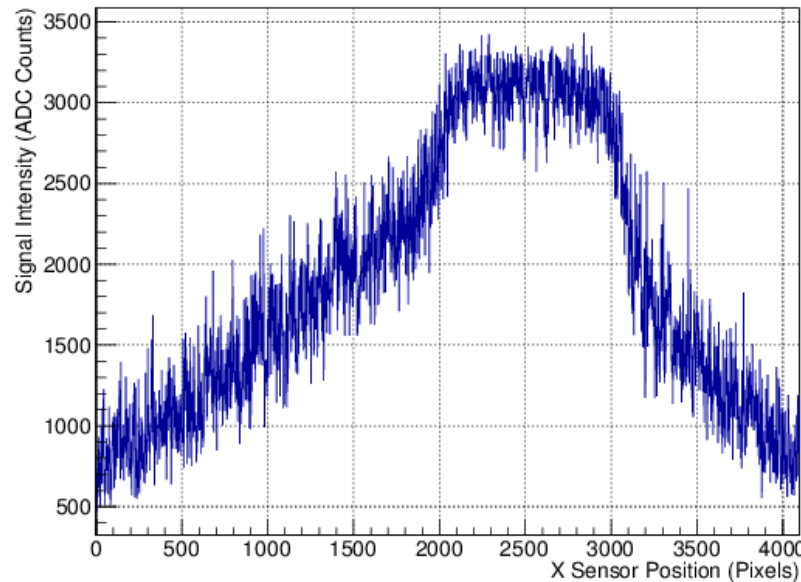


# Conclusions

- ✧ Demonstrated proof of concept upstream dosimetry system.
- ✧ Excellent leaf edge position resolution.
- ✧ Verification of IMRT fields demonstrated.
- ✧ Going through final round for funding to build a clinical prototype.

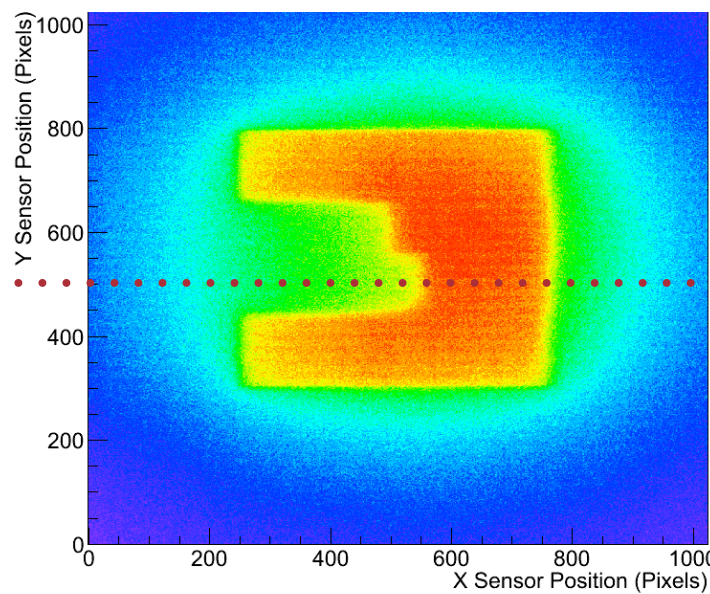
# BACK UP SLIDES

# Image Processing

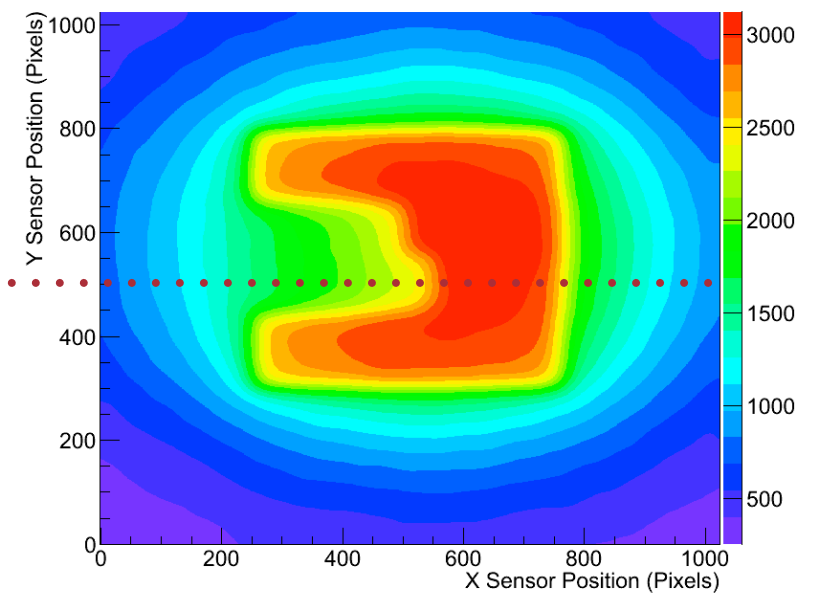


4096 x 4096

MLC and Jaws



1024 x 1024

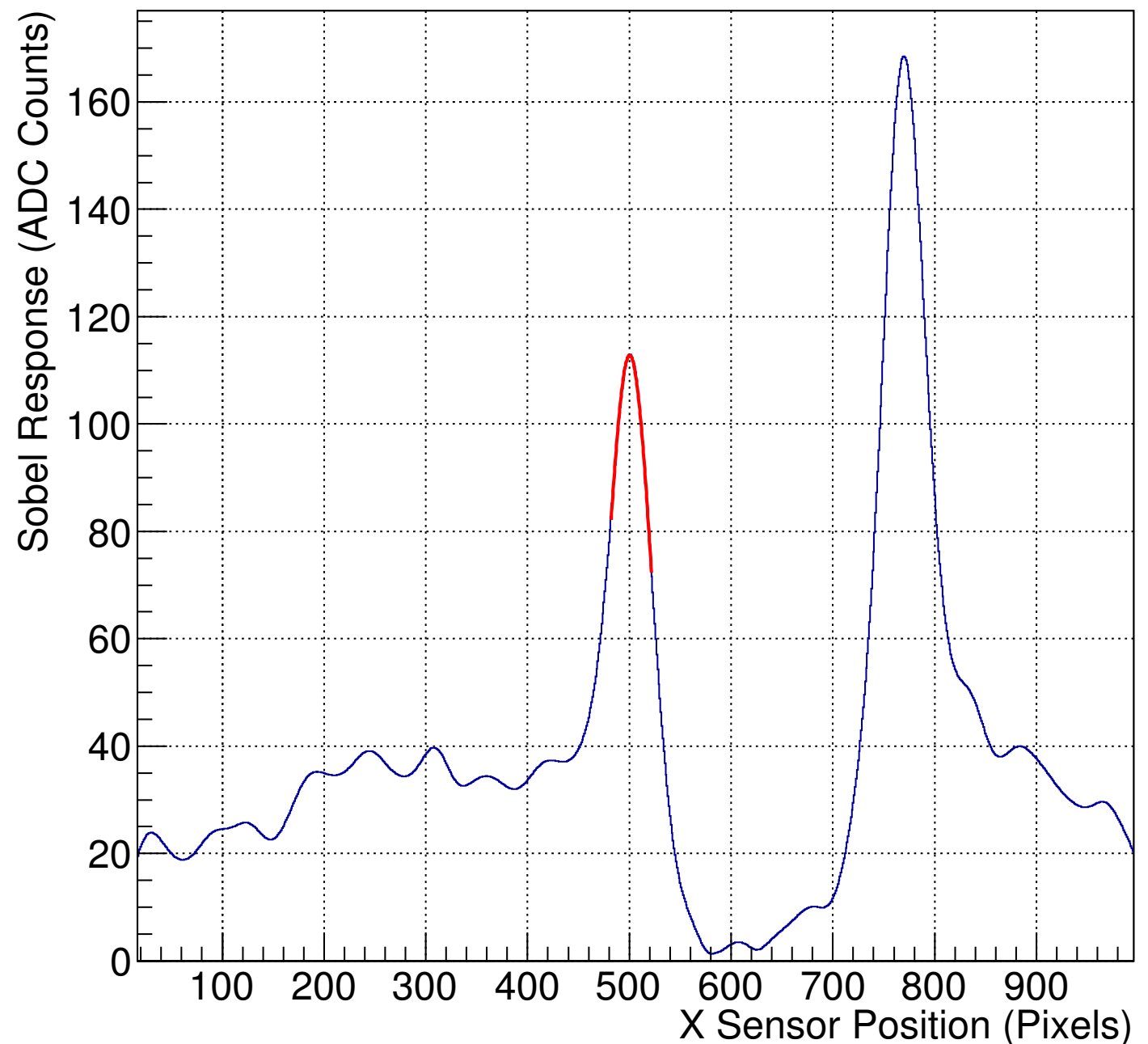


1024 x 1024 post Gaussian  
smoothing with a 15 pixel  
radius kernel



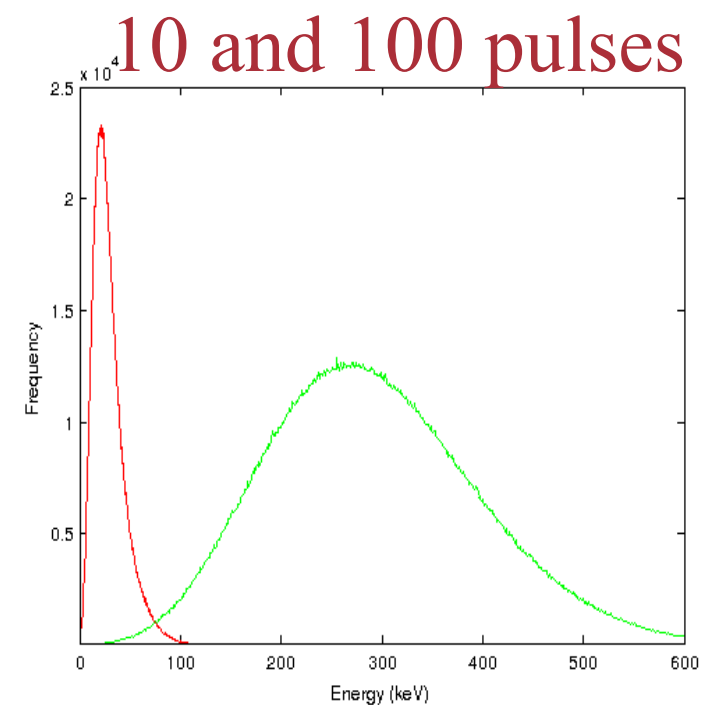
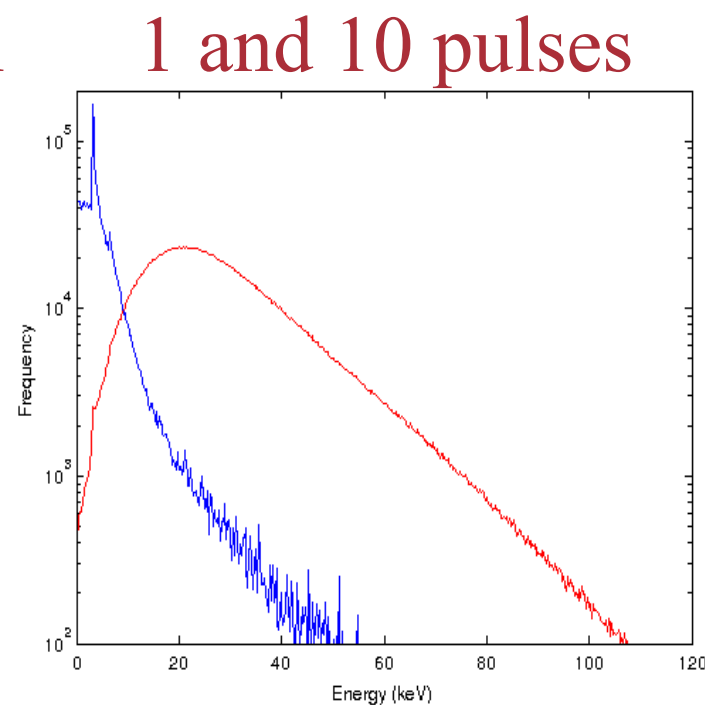
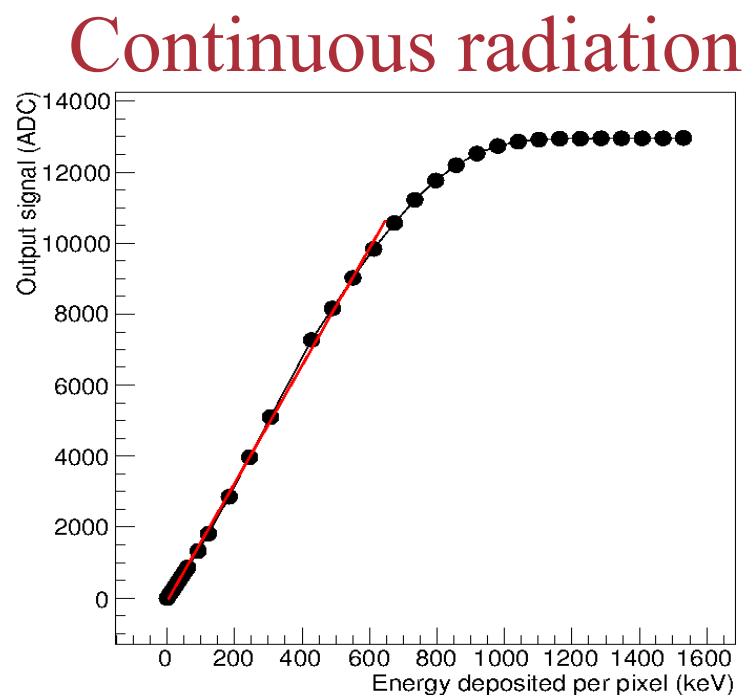
# Photon Field Reconstruction

- ✿ To extract a position from the edge response slices are taken across each leaf pair.
- ✿ The peaks in the response are fitted with Gaussian distributions.
- ✿ The mean of the distribution corresponds to a point along a contour of maximal gradient.



# Linearity

- ✶ Linearity tested using laser system.
- ✶ Energy deposited per pulse and multiple pulses determined using MC.
- ✶ Even for 100 overlapping pulses very few pixels would be in non-linear region.
- ✶ Aim to increase the frame rate.

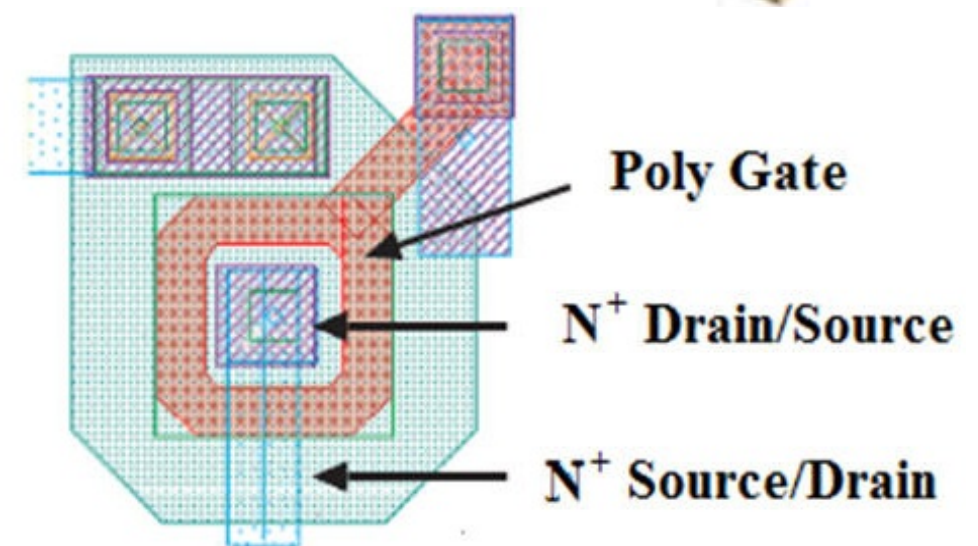
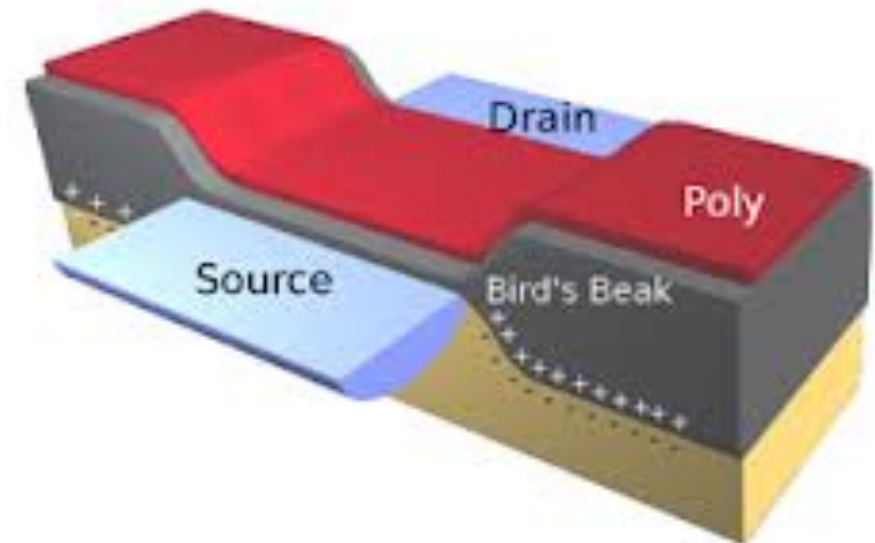


# Radiation Hardness

🔥 ACHILLES pixels:

🔥 Built in 0.35  $\mu\text{m}$  CMOS - thin oxide layer.

🔥 Uses gate geometry to reduce leakage current.



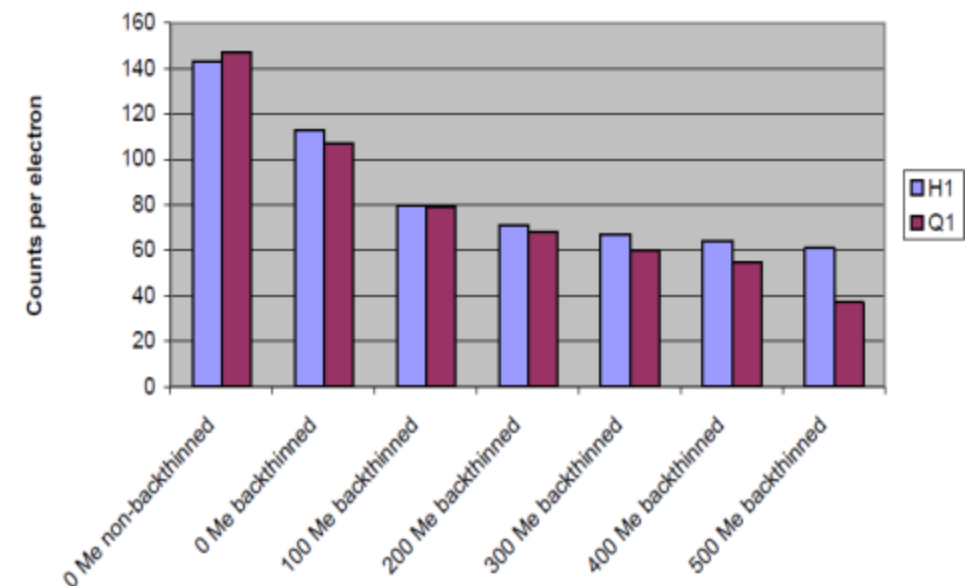
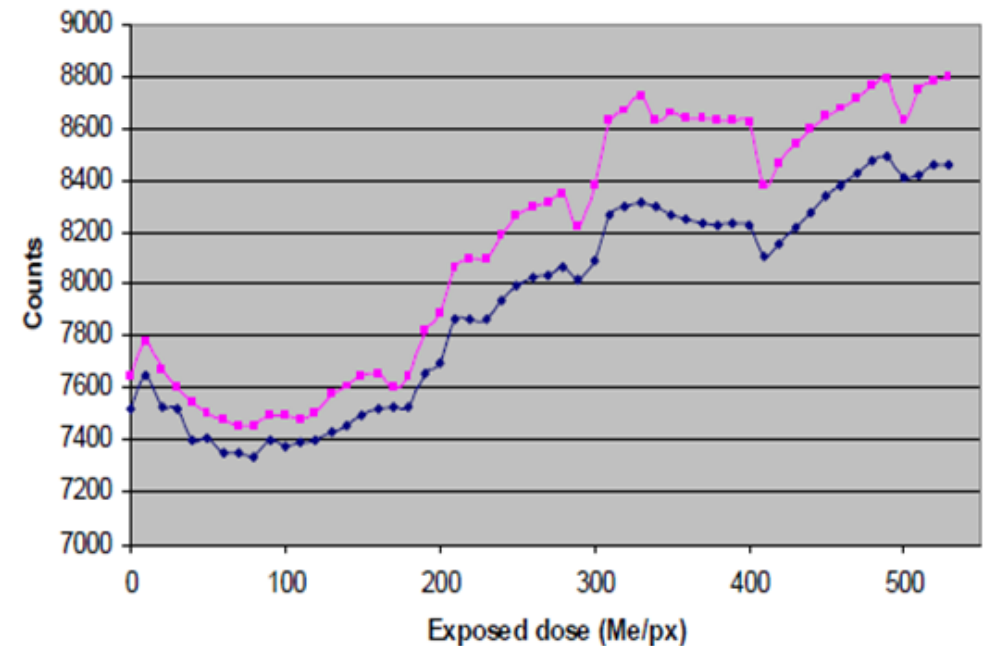
# Radiation Hardness

Two slightly different Achilles tested for radiation hardness.

The dark count changes slightly as function of the number of incoming 300 keV electrons. 500M 300 keV electrons corresponds to 20Mrad. Using 16 bit ADC, so no problem.

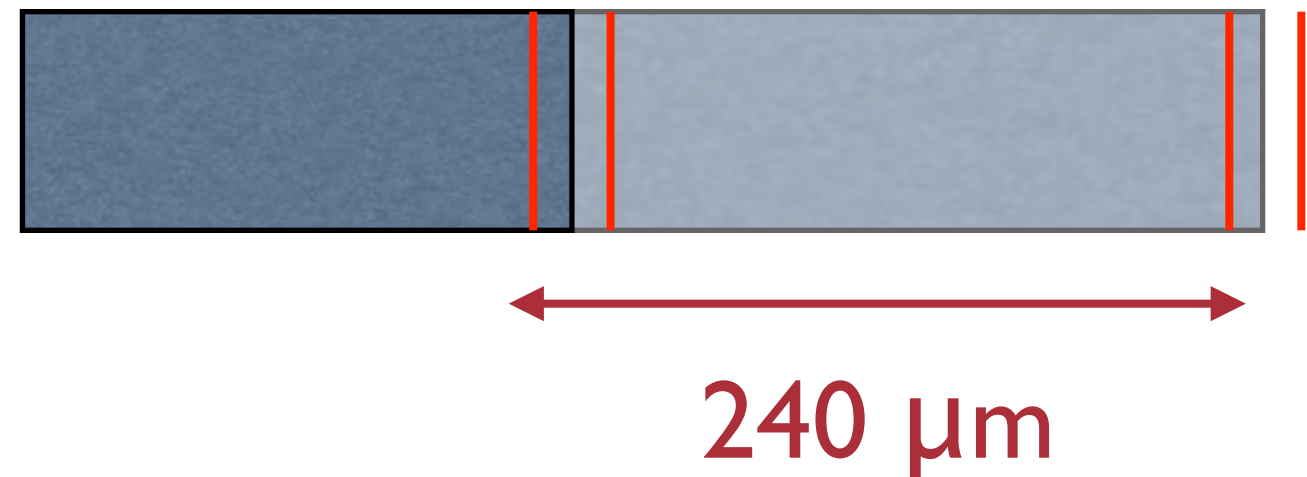
20 Mrad  $\approx$  500,000 fractions

Gain slowly decreases. No issue as our signals are big and can be calibrated and monitored.



# VMAT Considerations

- ✶ Maximum speed of the order 12 cm/s
- ✶ At 50 fps leaf would move 240  $\mu\text{m}$  with an error of 54  $\mu\text{m}$  on each position would have an uncertainty of  $\sim 75 \mu\text{m}$ .
- ✶ Don't see any issue for leaf reconstruction.
- ✶ Dose is determined from integrated signal.





# Characterisation

Used radioactive source:

Fe55.

Noise  $\sim 100$  e

Sr90.

MIP signal 990 e

