

# WP2: 11Carbon PET-aided hadron therapy

Research objectives  
ESR positions  
Secondments

*L. Penescu, MedAustron  
On behalf of WP2*

# WP2 Scope. Presentation summary.

## Scope of WP2: $^{11}\text{C}$ PET-aided hadron therapy

- ✓ **Production** and **mass separation** of  $^{11}\text{CO}^+$ . (ESR11)
- ✓ Development of **charge breeding** scheme required for acceleration. (ESR3)
- ✓ Full **acceleration** and **treatment** -  $^{11}\text{C}$  hadron therapy test and planning. (ESR9)
- ✓ Further development of bioconjugates suitable for **imaging** and treatment of the ovarian cancer. New bifunctional fluorescent and radioactive bioligand. Tests with  $^{11}\text{C}$  as chelate. (ESR15)
- ✓ Development of multimodal **imaging** methodologies for the treatment planning. Methodology and preclinical techniques. Biological models. (ESR12)

## PARTNERS

<b>ESR11:</b> <u>University of Leuven</u> (Recruiting and Enrolment; 36 mo)		+ <u>CNAO</u> (Secondment; 10 mo)
<b>ESR3:</b> <u>CERN</u> (Recruiting; 36 mo)	+ <u>Chalmers University of Technology</u> (Enrolment)	+ <u>MedAustron</u> (Secondment; 5 mo)
<b>ESR9:</b> <u>CNAO</u> (Recruiting; 36 mo)	+ <u>University of Pavia</u> (Enrolment)	+ <u>CERN, HUG</u> (Secondment; 3 + 3 mo)
<b>ESR15:</b> <u>HUG</u> (Recruiting; 36 mo)	+ <u>EPFL</u> (Enrolment)	+ <u>AAA</u> (Secondment; 3 mo)
<b>ESR12:</b> <u>HUG</u> (Recruiting; 36 mo)	+ <u>University of Geneva</u> (Enrolment)	+ <u>CNAO</u> (Secondment; 3 mo)

## Presentation SUMMARY

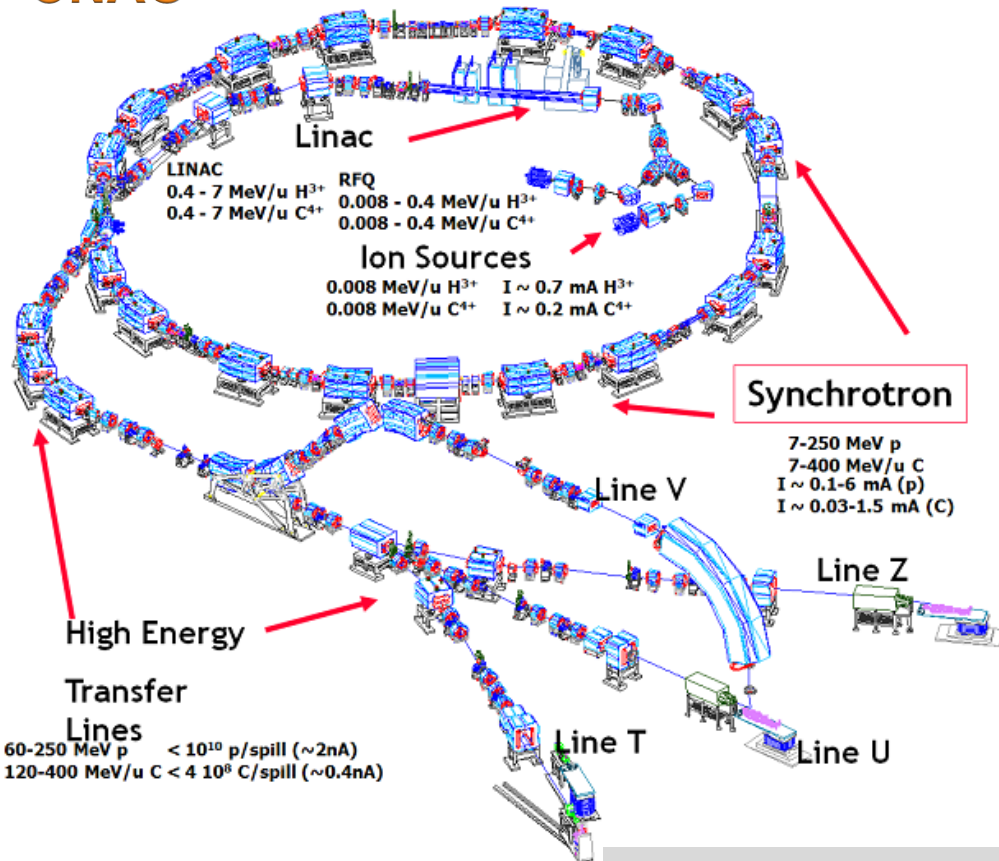
- Delivering a beam for treatment at an existing facility (MedAustron, CNAO, HIT).
- Possibilities for mixing/replacing  $^{12}\text{C}$  with  $^{11}\text{C}$ , for treatment and PET imaging.
- Open questions (to be addressed by the ESRs).

# PIMMS-based accelerators: HIT, CNAO, MedAustron

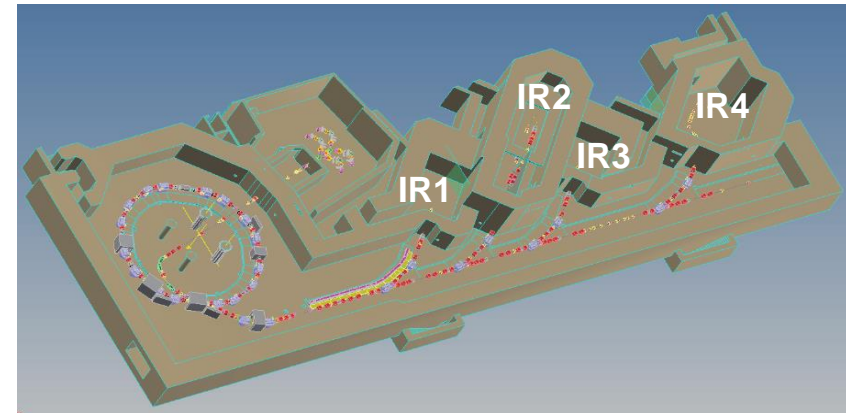
PIMMS: Proton-Ion Medical Machine Study, CERN 2000-006



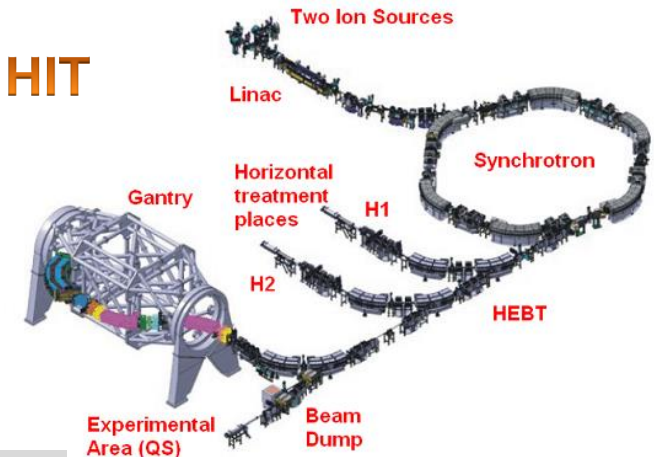
## CNAO



## MedAustron

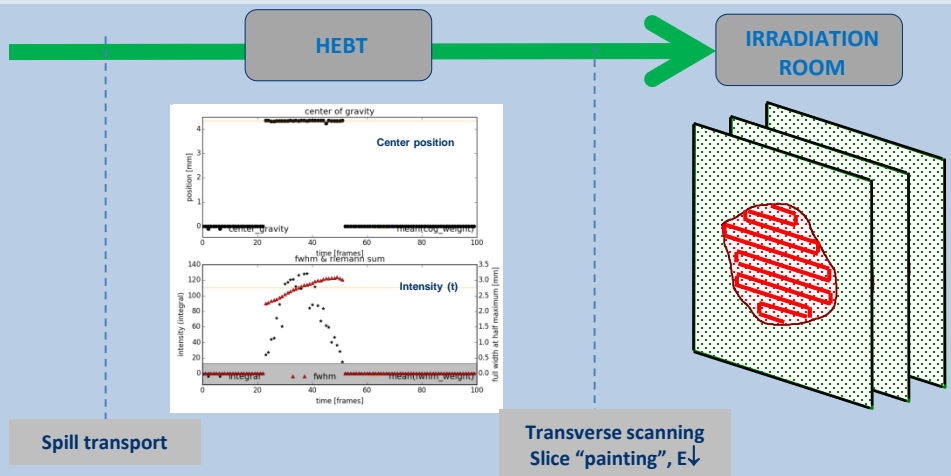
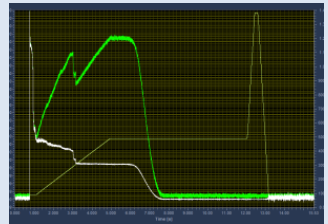
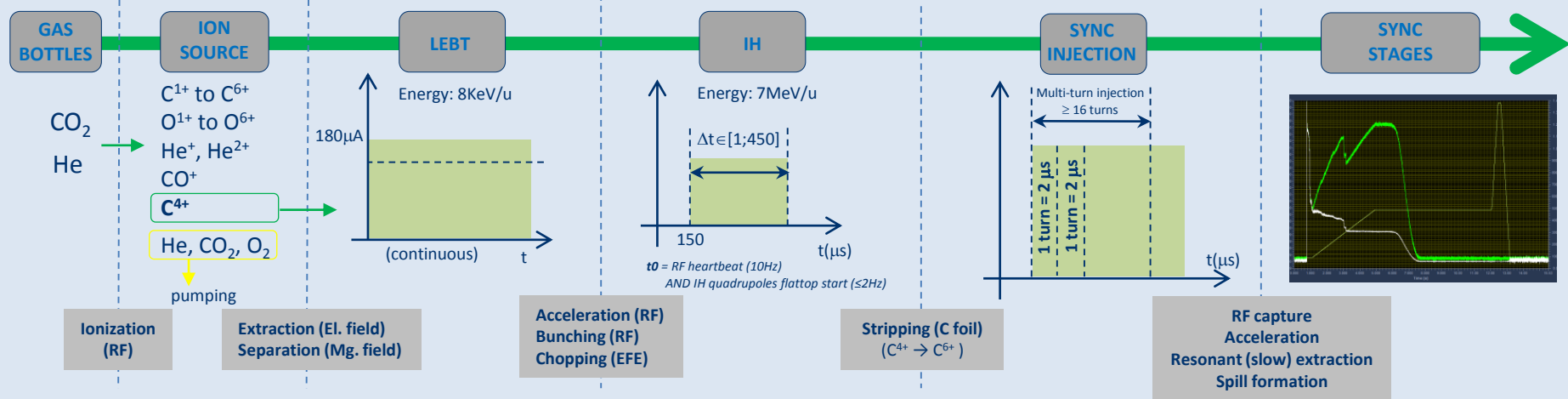
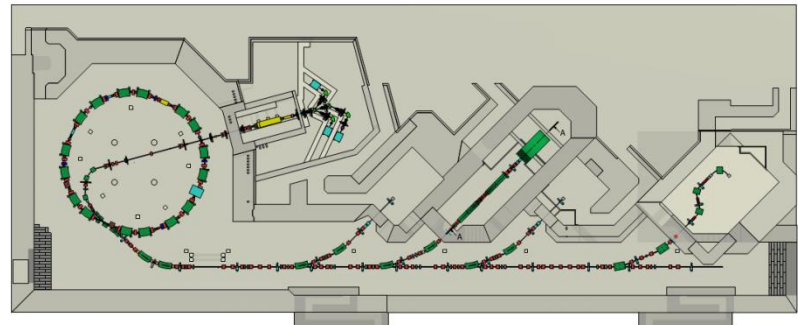


## HIT



- ✓ Same main ideas
- ✓ Different implementation choices

# The $^{12}\text{C}$ beam path at MedAustron



- Pencil beam: 4 to 10 mm FWHM in vacuum
- Fast magnetic deflection, H and V (20 m/s)
- Scanning field size: 20 x 20 cm<sup>2</sup> (IR 1 to 3)
- Beam position accuracy:  $\pm 0.5$  mm
- $\leq 1 \cdot 10^{10}$  protons/spill;  $\leq 4 \cdot 10^8$  C-ions/spill
- Energies corresponding to 3-37 cm penetration depth in human tissue
- $\sim 1$  minute to deliver 2 Gray in 1 L tumor volume

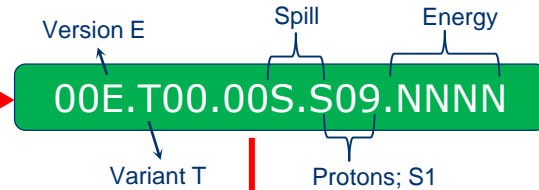
# Requesting a beam

Treatment plan = a sequence of cycle codes

The bits of a cycle code contain information on:

- Extraction Energy
- Spill length
- Beam size
- Irradiation room
- MEBT degrader used
- Particle type.
- Ion Source.
- Variant.
- Version.

CYCLE CODE



RUNFILE

```
000.000.000.008.0001
000.100.000.008.0002
00E.T00.00S.S09.NNNN
000.100.000.000.0000
000.100.000.000.0000
```

00F.F00.001.E07.FFFF

Applied timing sequence



00E.T00.00S.S01.NNNN

(some bits will be filtered out in the different sections of the machine, depending on their "mask")

Mask:

000.100.000.03F.0000



Filter:

000.T00.000.009.0000  
(Protons, S1)



000.100.000.007.0000



000.T00.000.001.0000  
(Protons; Variant T)



00F.F00.000.070.0000



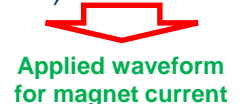
00E.T00.000.010.0000  
(Protons; Version E; Variant T)



00F.F00.001.E07.FFFF

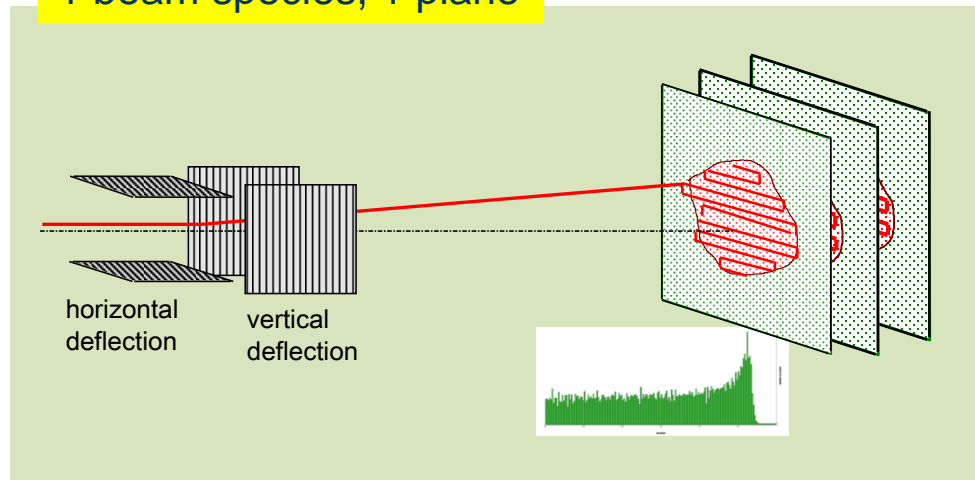


00E.T00.00S.S10.NNNN  
(Protons; Version E; Variant T; Spill SS; Acceleration energy NNNN)

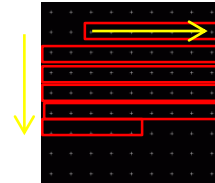


# Delivering 2 beam species

## 1 beam species, 1 plane



- 3D matrix of intensities defined by treatment plan
- Point by point scanning of slices
- A spill can cover a full slice
- From high E to low E



12C and/or 11C

- ✓ Treatment
- ✓ PET imaging

## 2 beam species, 1 (or 2) planes

- Treatment plan with dose splitting between species.
- Different penetration depths (=energies) for the 2 species.
- Full scan in 1 plane, followed by full scan in 2<sup>nd</sup> plane.
- Scan in 1 plane as above.
- (hysteresis of cw magnets)
- Scan in 2<sup>nd</sup> plane following same strategy as above.

## 1 beam species, 2 planes (H and V)

- Treatment plan with dose splitting between planes.
- Different penetration depths (=energies) for the 2 planes.
- Full scan in 1 plane, followed by full scan in 2<sup>nd</sup> plane.
- Scan in 1 plane as above.
- (hysteresis of cw magnets)
- Scan in 2<sup>nd</sup> plane following same strategy as above.

# The accelerator side: commissioning a “cycle code”

## The accelerator is able to generate:

- ✓ Number of ion species: **2**
- ✓ Number of different energies: **255**
- ✓ Number of beam sizes: **4**
- ✓ Number of intensities: **4**
- ✓ Number of extraction times: **8**
  
- Beam combinations per beam line:  
**65280**
- Gantry: different angles need to be considered
- Non-clinical research: extended energy range

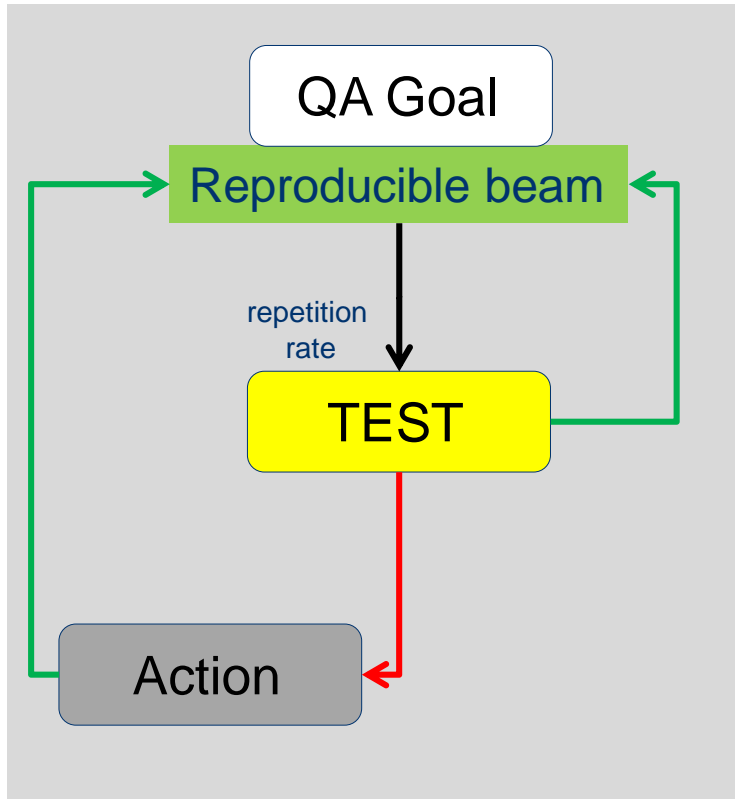
PARAMETERS which are NOT part of cycle code, but part of design + commissioning:

- Energy spread
- Spill quality (stability: intensity, position)
- Choices of beam optics (longitudinal and transversal)

DURATION OF A CYCLE – depends on accelerator performance:

- Injection time
- Acceleration time
- Short hysteresis time
- Hardware configuration time

# Preparation and QA of a medical beam



Reproducible  
BEAM

(A) Same applied settings  
(B) Reproducible  
machine performance

Understanding of:

- Hardware stability
- Hardware – Hardware interactions
- HW – Beam interactions
- Beam – Beam interactions
- Aging effects
- Maintenance effects
- Failure statistics

- ✓ **Spill formation:** defined in the synchrotron
  - Duration.
  - Intensity uniformity.
  - Position uniformity.
- ✓ **Spot formation:** defined in the HEBT line
  - Spot size
  - Position at isocenter
- ✓ **Restrictions on injector:** not critical
  - Most of the injected beam limitations can be corrected in the synchrotron



# Question marks vs. ESR topics

- 1) How to produce the  $^{11}\text{C}$  with needed intensity, reproducibility and stability?
- 2) Where to inject the  $^{11}\text{C}$  along the beam path? (answer correlated to 1...)
- 3) PET-related questions...

- 1) Compact PET cyclotron  $\rightarrow$   $\text{N}_2$  target  $\rightarrow$  release of  $^{11}\text{CO}_2$  into ion source  $\rightarrow$  beam path joining  $^{12}\text{C}$
- 2) ISOL production  $\rightarrow$  mass separation and charge breeding ( $\rightarrow$  post-acceleration?)  $\rightarrow$  beam path joining  $^{12}\text{C}$

- ✓ **Production** and **mass separation** of  $^{11}\text{CO}^+$  (ESR11)
- ✓ Development of **charge breeding** scheme required for acceleration (ESR3)
- ✓ Full **acceleration** and **treatment** -  $^{11}\text{C}$  hadron therapy test and planning (ESR9)
- ✓ Further development of bioconjugates suitable for **imaging** and treatment of the ovarian cancer. New bifunctional fluorescent and radioactive bioligand. Tests with  $^{11}\text{C}$  as chelate. (ESR15)
- ✓ Development of multimodal **imaging** methodologies for the treatment planning. Methodology and preclinical techniques. Biological models. (ESR12)

## TO HAVE IN MIND: The available intensity per spill is not a veto-condition.

Accelerator efficiency depends on all of the following:

- Intensity per spill
- Cycle time (acceleration time; hysteresis; re/configuration; injection of  $^{11}\text{C}$ ?)
- Strategy for using effectively all accelerated particles.
- Dealing successfully with machine limitations at higher intensities.