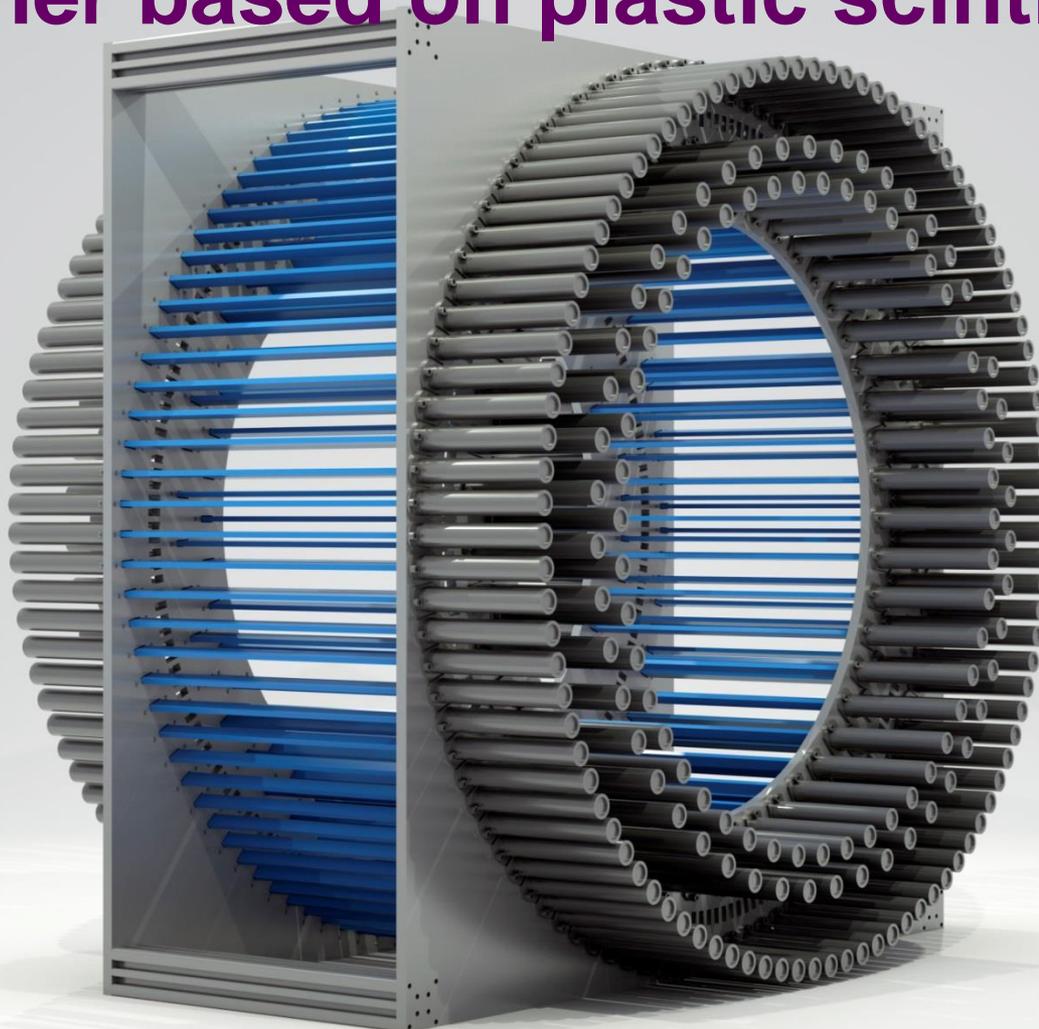


## scanner based on plastic scintillators

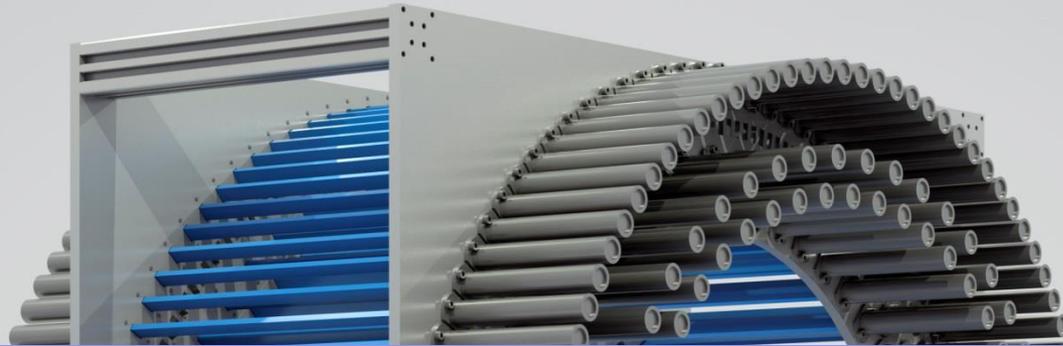


**ICTR-PHE-2016, 15-19 February 2016**

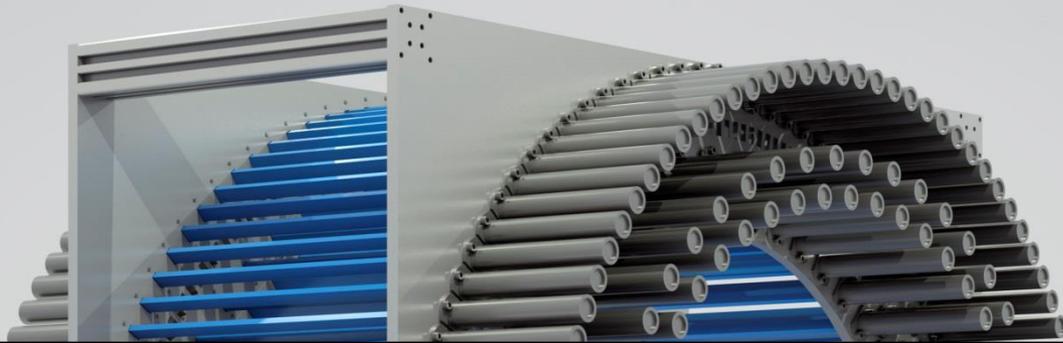
Paweł Moskal, Jagiellonian University  
on behalf and for the J-PET Collaboration

<http://koza.if.uj.edu.pl>





- **Jagiellonian PET**
- **NEMA characteristics**
- **Towards simultaneous J-PET and MRI imaging**



- **Jagiellonian PET**

**WHOLE BODY**

**LARGE ANIMAL**

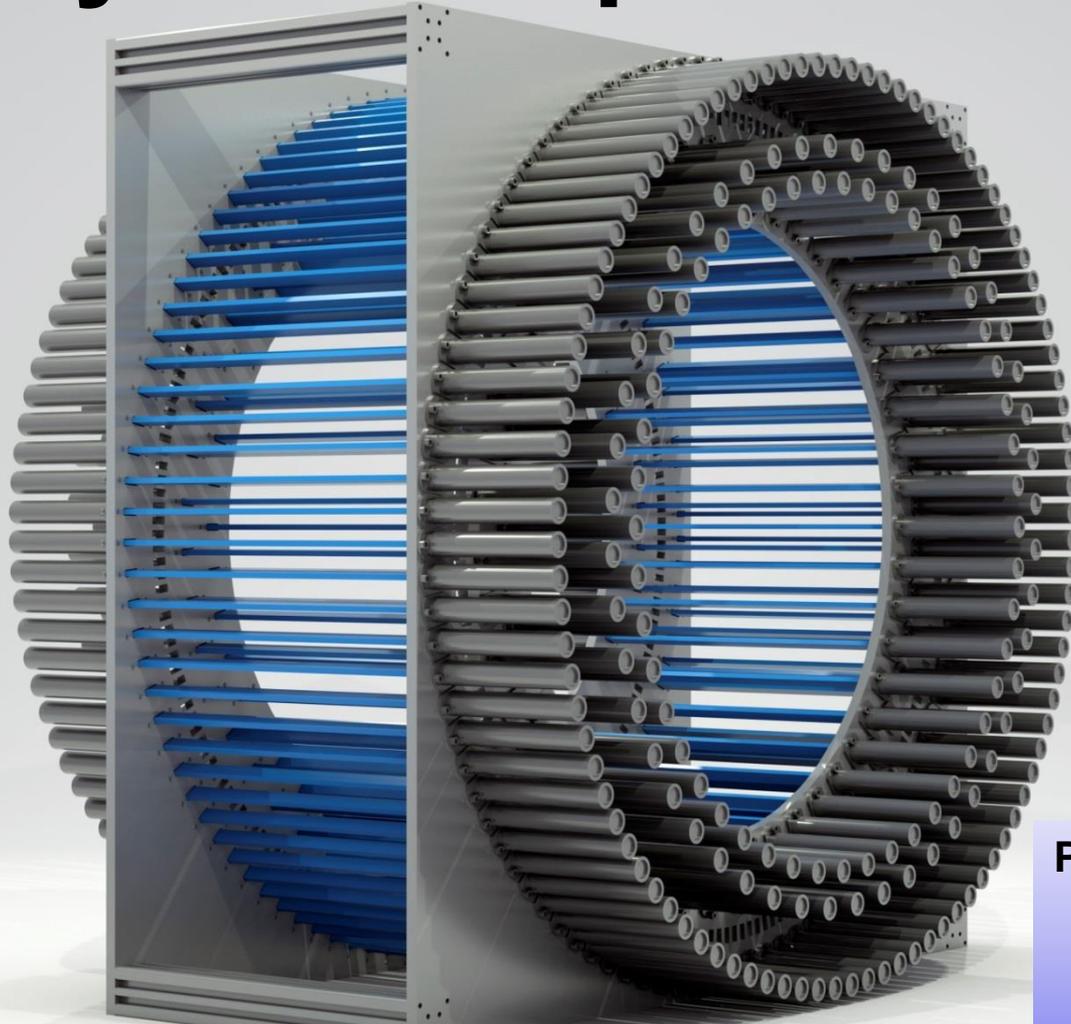
**COST EFFECTIVE**

**CONFIGURABLE**

**MRI COMPATIBLE**

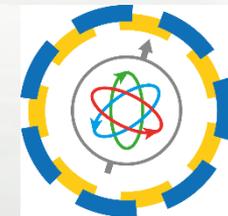
...

# crystals → plastics

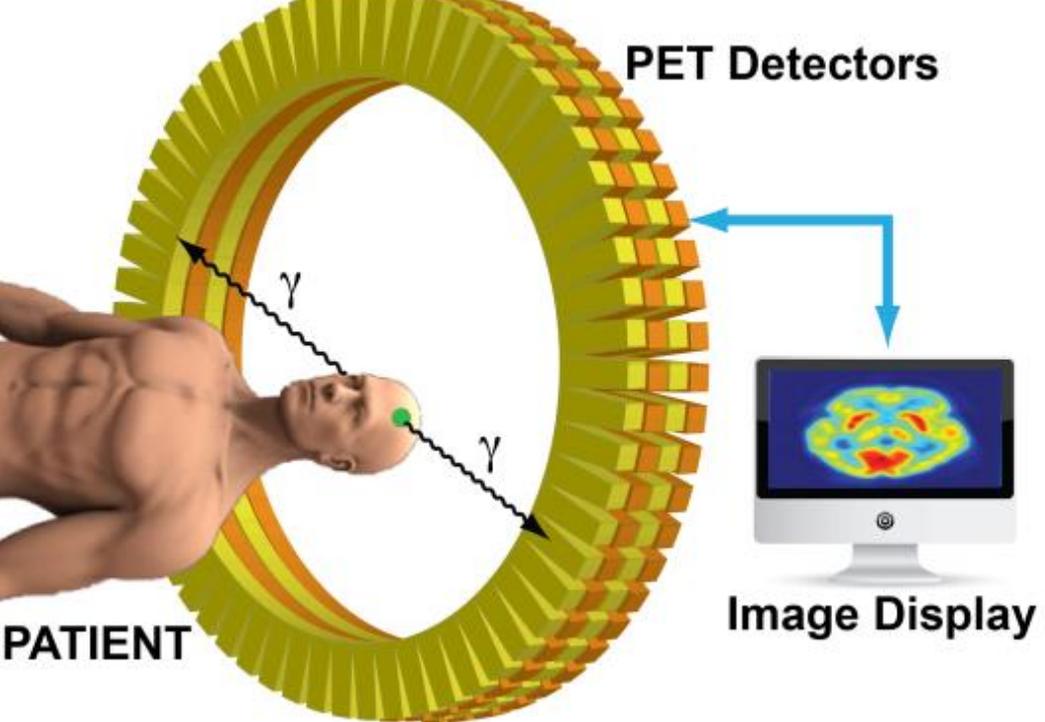


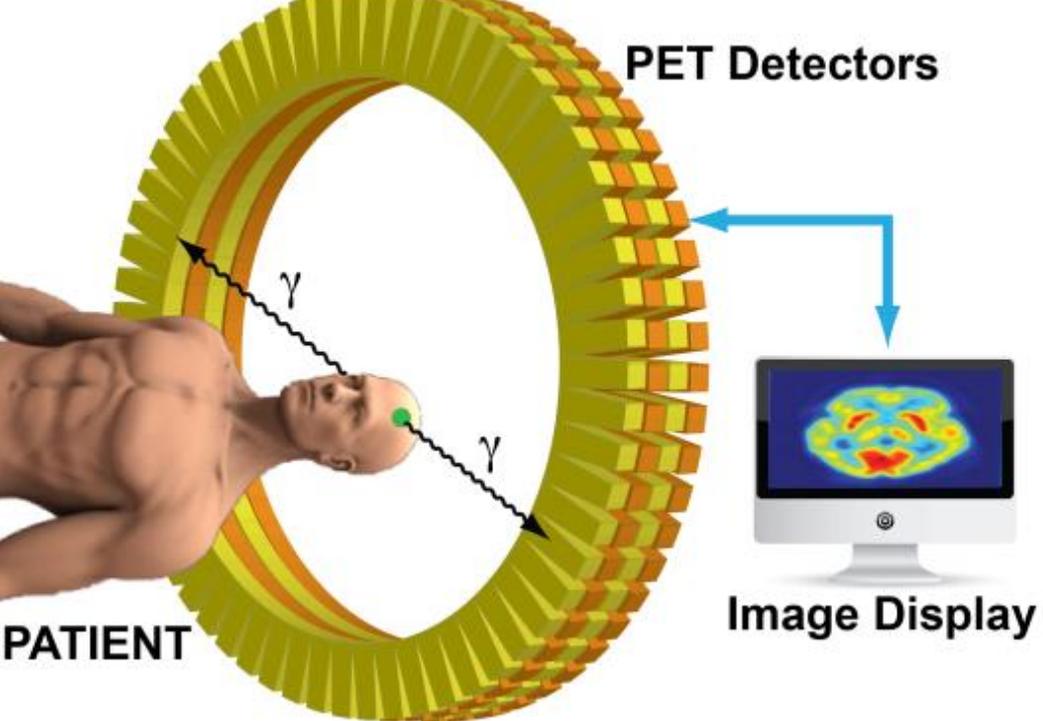
P. M., Patents (2014)  
WO2011008119,  
WO2011008118  
EU, JP, US.

J-PET: L. Raczyński et al., Nucl. Instrum. Meth. A764 (2014) 186  
J-PET: P. M. et al., Nucl. Instrum. Meth. A764 (2014) 317  
J-PET: P. M. et al., Nucl. Instrum. Meth. A775 (2015) 54  
J-PET: L. Raczyński et al., Nucl. Instrum. Meth. A786 (2015) 105  
J-PET: P. M. et al., Phys. Med. Biol. (2016) in print; arXiv:1602.02058  
34 articles and 16 International patent applications

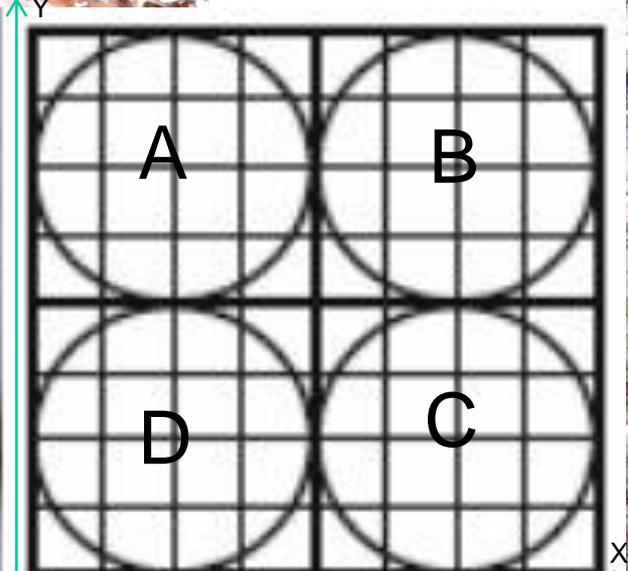
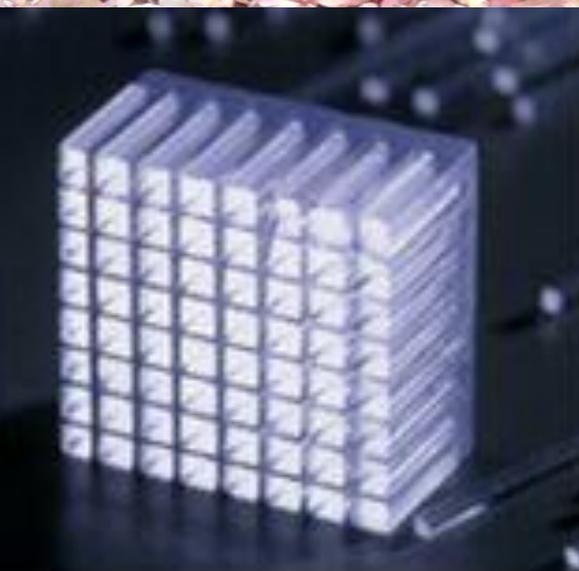


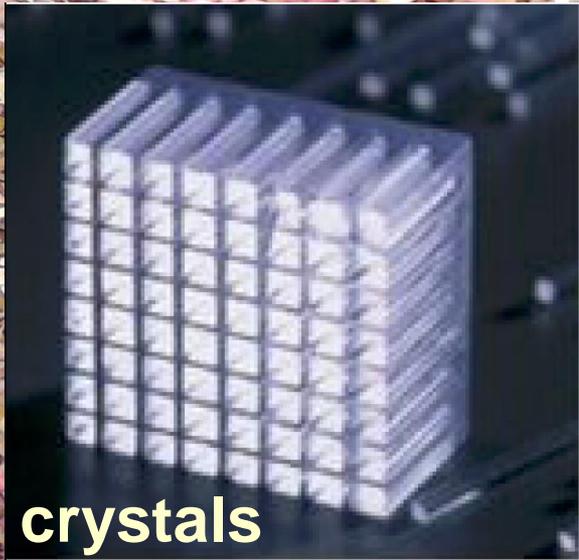
**J-PET**



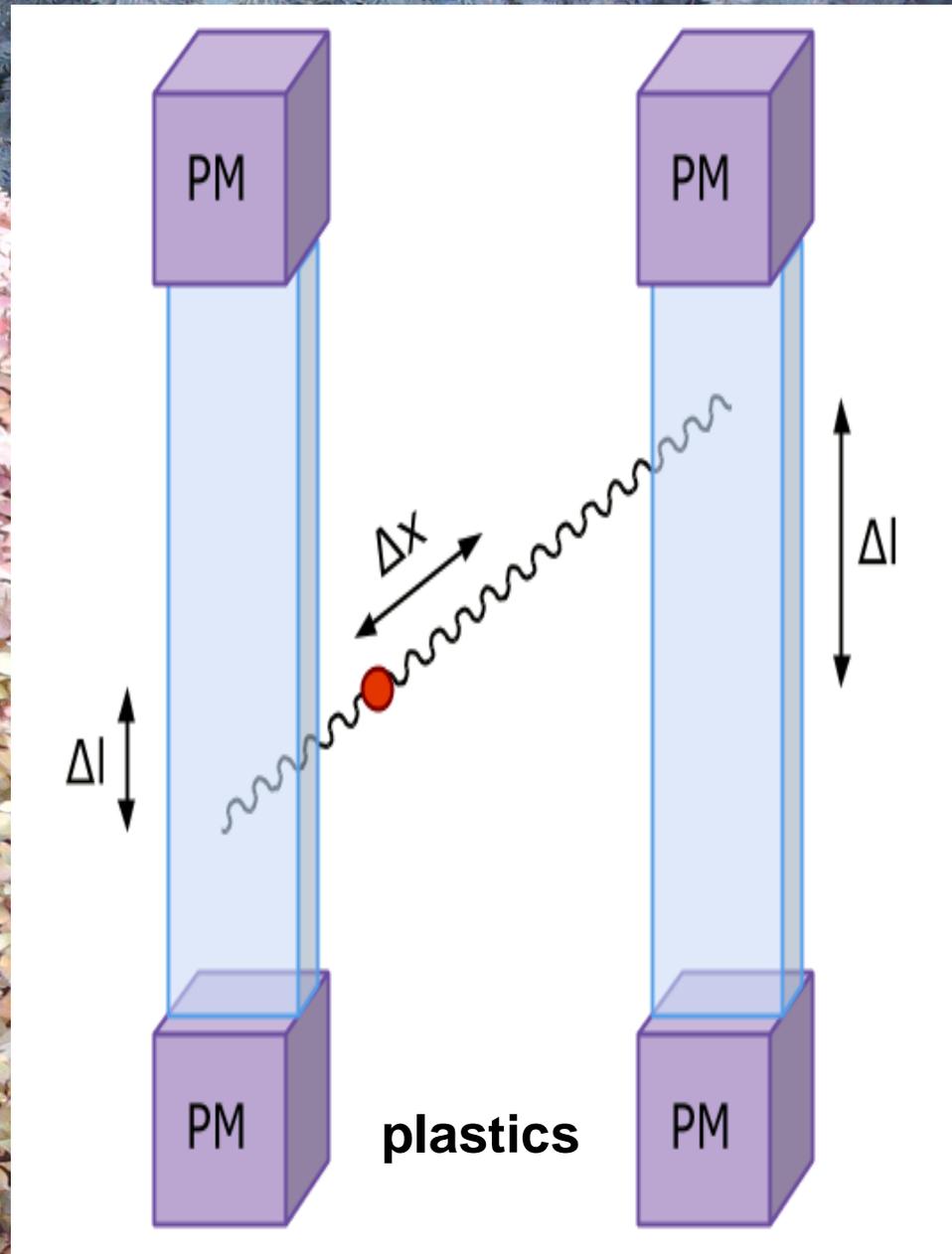


$$X = \frac{(B+C) - (A+D)}{A+B+C+D}$$



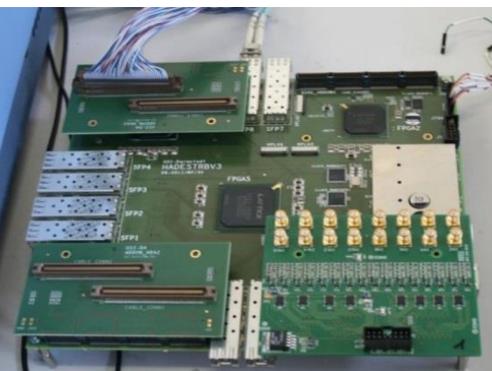


**crystals**



**plastics**

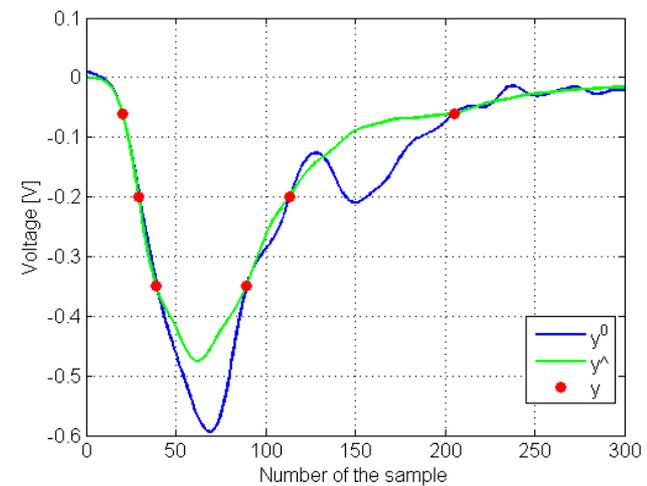
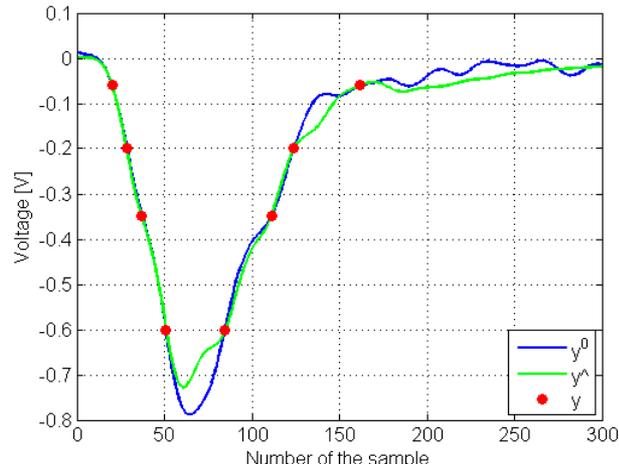
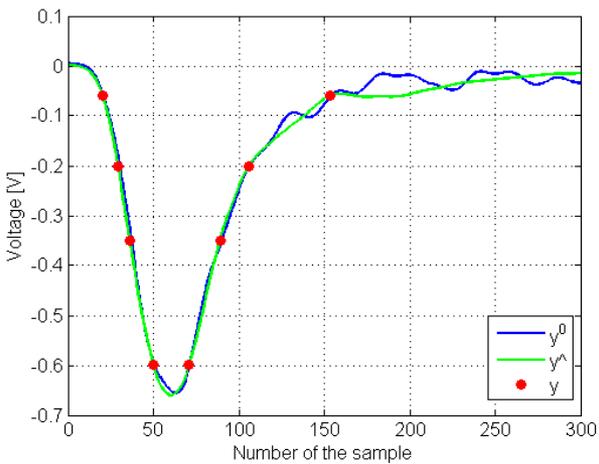
# New idea... BREAK THROUGH



**ONLY DIGITAL** in triggerless mode  
 FFE sampling & Readout electronics  
 precision of 21ps (sigma) for 10 Euro per sample

M.Pałka, P.M., **PCT/EP2014/068367**

G. Korcyl, P. M., M. Kajetanowicz, M. Pałka, **PCT/EP2014/068352**



Library of signals ; Principal Component Analysis; Compressive Sensing;  
 J-PET: L. Raczyński et al., Nucl. Instr. Meth. A786 (2015) 105  
 J-PET: P. M. et al., Nucl. Instrum. Meth. A775 (2015) 54

## Reconstruction

**Detector**

**FrontEnd electronics**

**Electronics controller**

**Hit along strip**

**Annihilation point**

**Image**

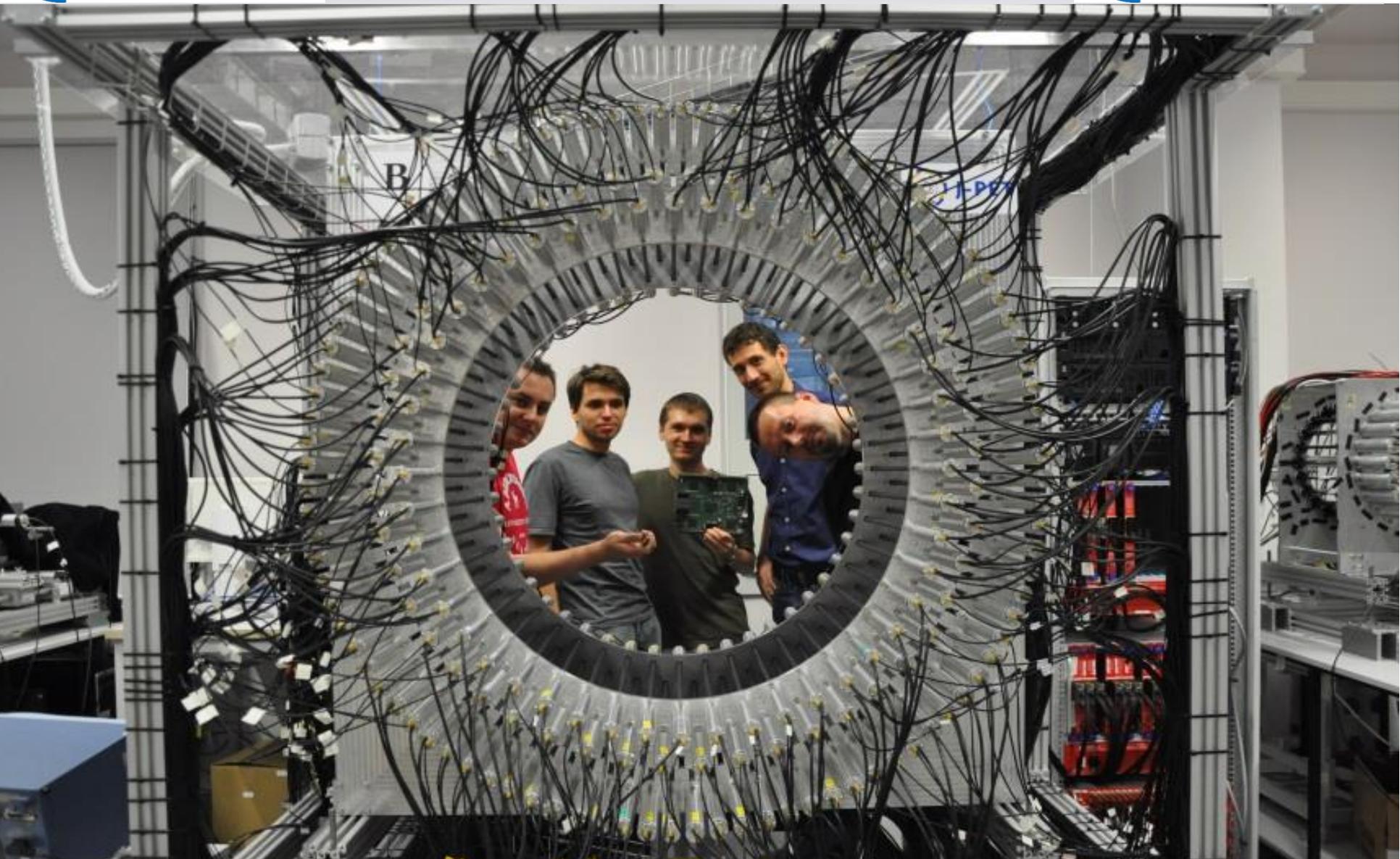


**J-PET**

# Jagiellonian PET

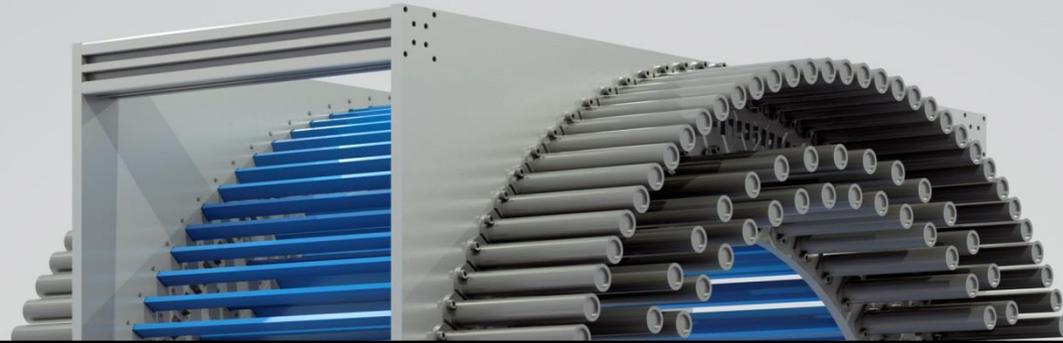


**J-PET**



**AFOV: 17 cm  $\rightarrow$  50 cm ; TOF: 520 ps  $\rightarrow$  300 ps**





- Jagiellonian PET
- NEMA characteristics
- Towards simultaneous J-PET and MRI imaging

Type: LSO / LYSO / BGO / polymer scintillator

Price per cm<sup>3</sup>: 86 / 86 / 35 / 1

Plastic scintillators can be easily produced in large sizes and various shapes

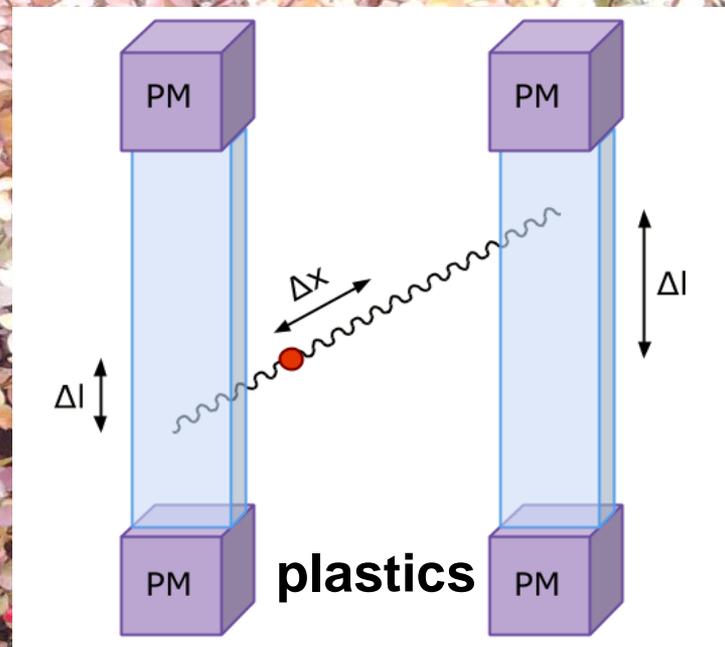
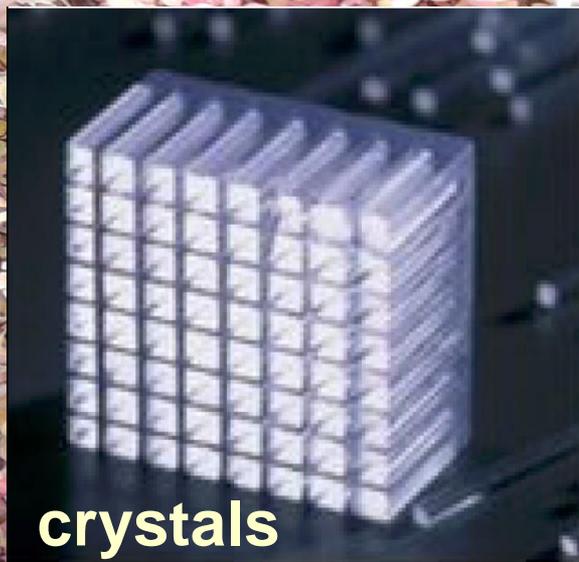
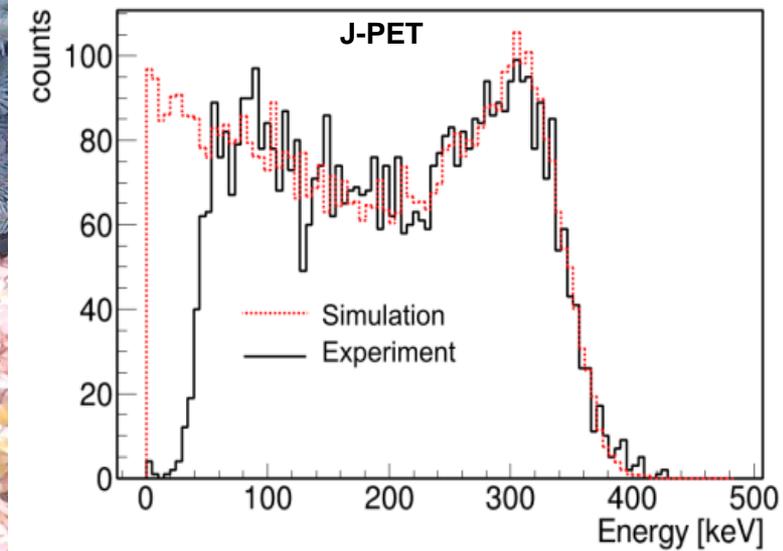
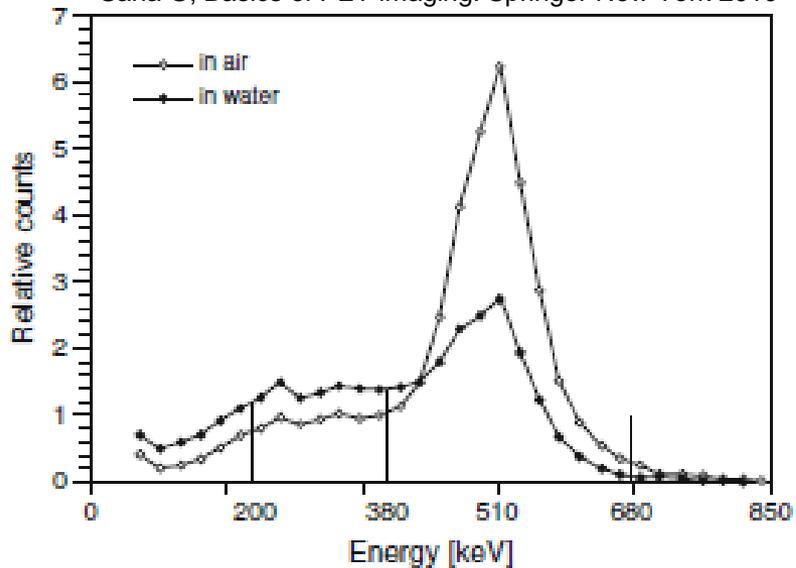
Why plastics were not considered so far as a material for PET detectors ?  
→ Low detection efficiency and no photeffect !

**Sensitivity ?**

**Scatter fraction ?**

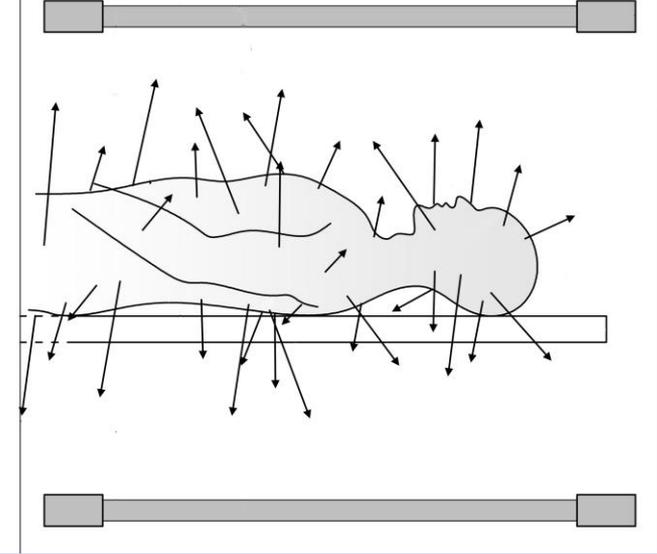
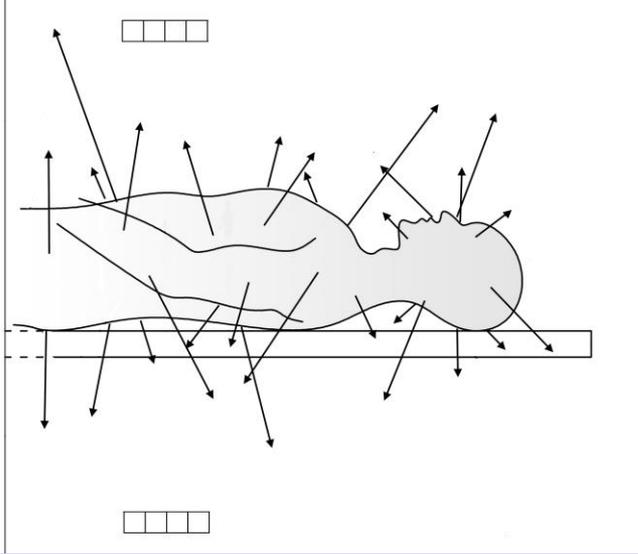
**Accidental coincidences?**

Saha G, Basics of PET imaging. Springer New York 2010



for the 2.5 cm layer the efficiency for the registration of events selected to reconstruct the image is for the plastic scintillator by  
**a factor of about 20 smaller in relation to the BGO crystals  
and about 40 times less compared to the LSO crystals**

<b>name</b>	<b>type</b>	<b>density [g/cm<sup>3</sup>]</b>	<b>decay time [ns]</b>	<b>photons/ MeV</b>	<b>mean free path [cm]</b>
<b>BGO</b>	<b>crystal</b>	<b>7.13</b>	<b>300</b>	<b>6000</b>	<b>1.04</b>
<b>GSO</b>	<b>crystal</b>	<b>6.71</b>	<b>50</b>	<b>10000</b>	<b>1.49</b>
<b>LSO</b>	<b>crystal</b>	<b>7.40</b>	<b>40</b>	<b>29000</b>	<b>1.15</b>
<b>NE102A</b>	<b>polymer</b>	<b>1.032</b>	<b>2.4</b>	<b>10000</b>	<b>10.2</b>
<b>BC404</b>	<b>polymer</b>	<b>1.032</b>	<b>1.8</b>	<b>10000</b>	<b>10.2</b>
<b>RP422</b>	<b>polymer</b>	<b>1.032</b>	<b>1.6</b>	<b>10000</b>	<b>10.2</b>

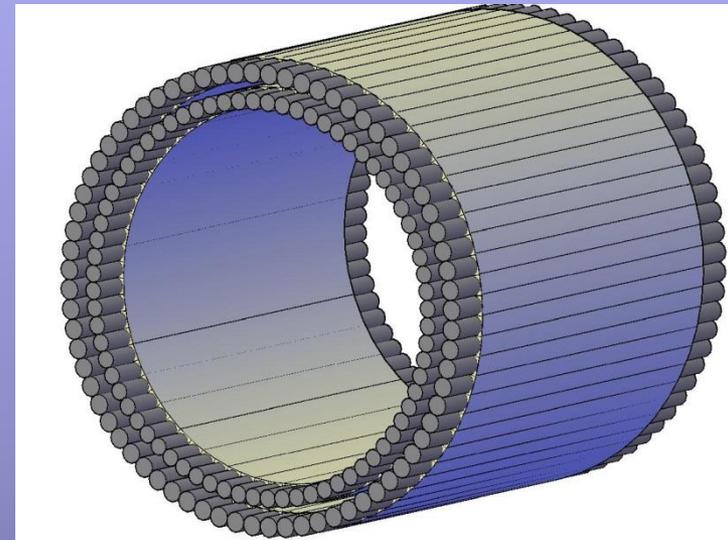


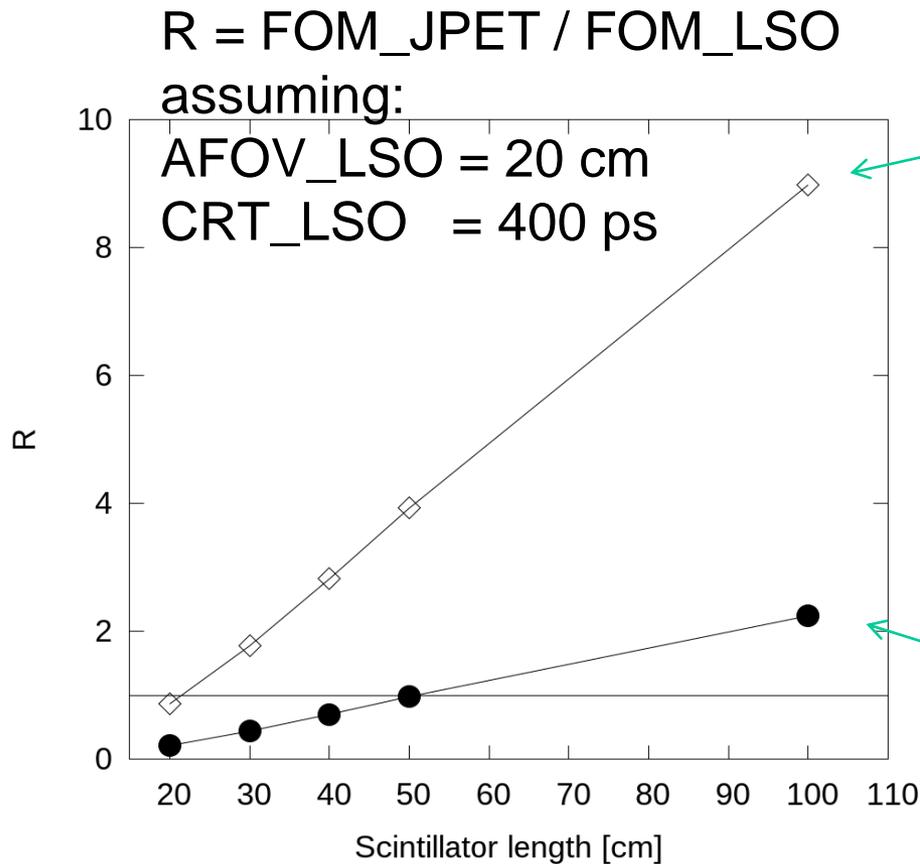
It is important to note that the cost of J-PET does not increase with the increase of the FOV  
 $\epsilon^2 = 20$  to  $40$  smaller efficiency

But

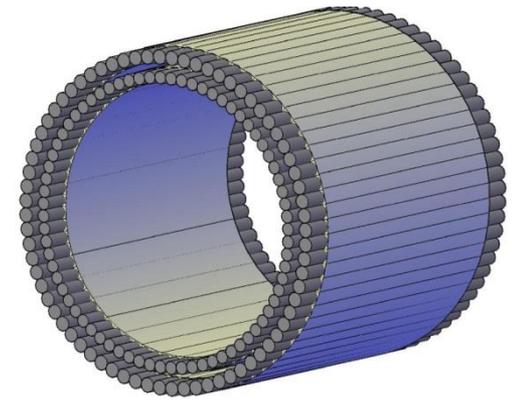
- Solid angle** ----- > factor of  $\sim 5$
- 600 ps --> 200ps – 300ps --> factor of 3 -- 2
- 1m instead of  $\sim 17$  cm -----> factor of 10
- N** layers in the strip-PET ----> factor  **$N^2$**

Conservatively:  
 for  $N=1$  ----> total factor of  $\sim 100$   
 Lower dose by factor of 3 (100 better / 30 worse)

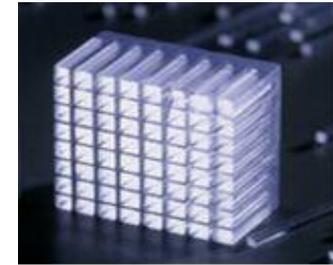
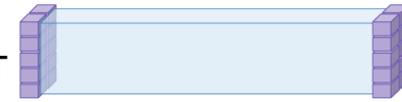




$N_{\text{JPET\_layers}} = 2$

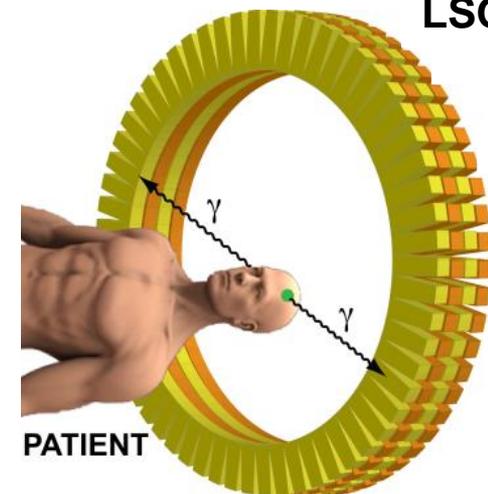


$$R = \frac{\text{FOM\_JPET}}{\text{FOM\_LSO}}$$



$N_{\text{JPET\_layers}} = 1$

LSO

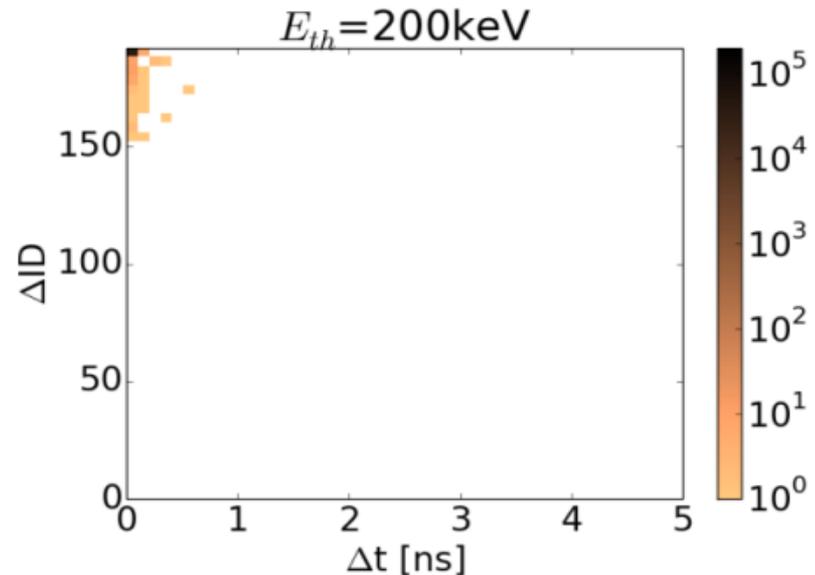
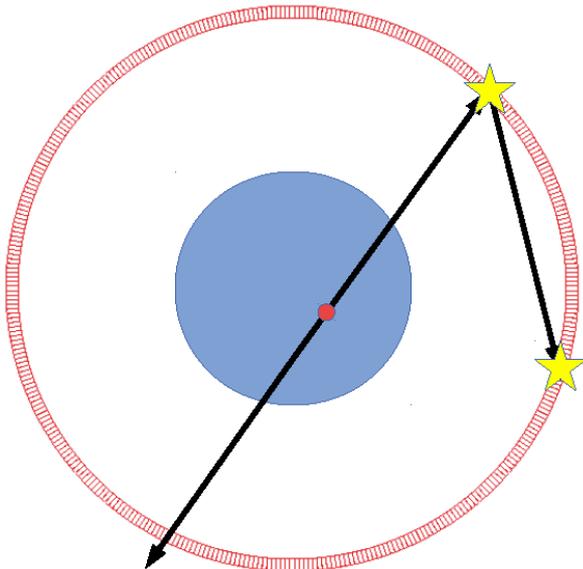
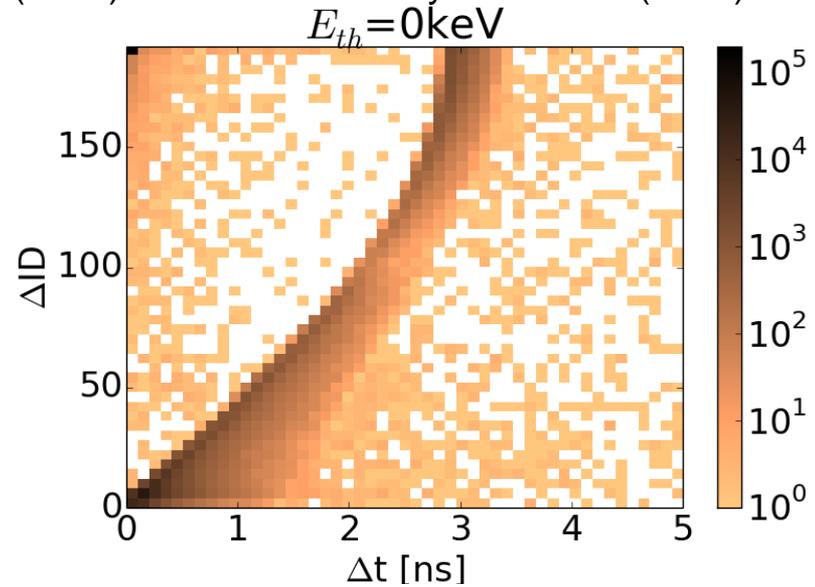
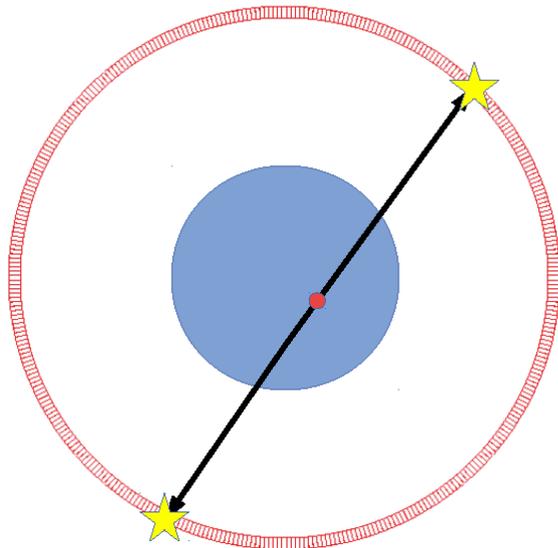


**Figure of Merit for whole body imaging:**  
 $\text{FOM} = \epsilon_{\text{detection}}^2 \cdot \epsilon_{\text{selection}}^2 \cdot \text{Acc} / (\text{CRT} \cdot N_{\text{steps}})$

# J-PET

## secondary scattering in the detector

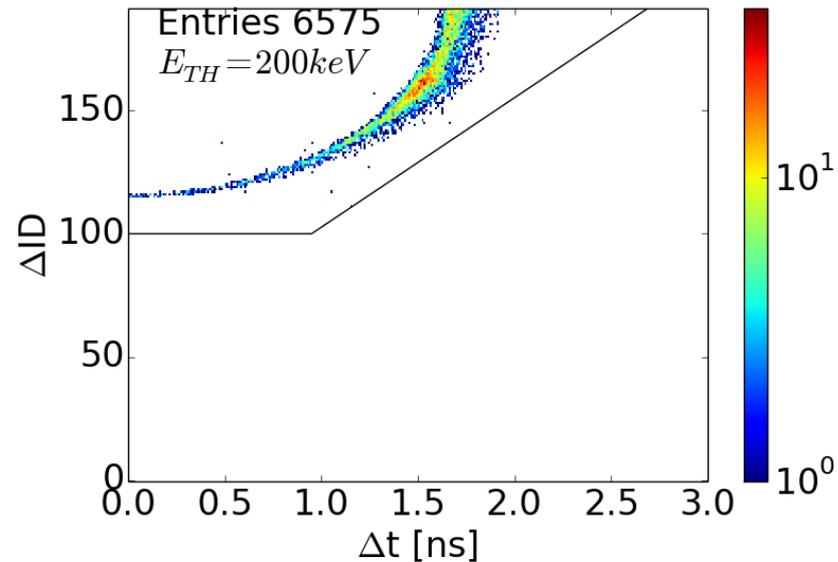
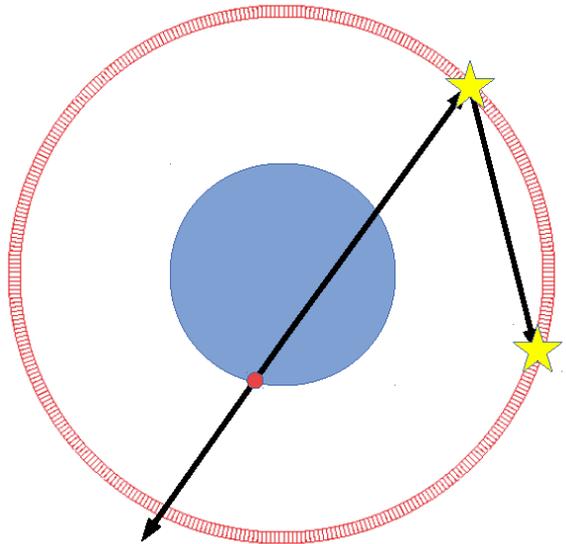
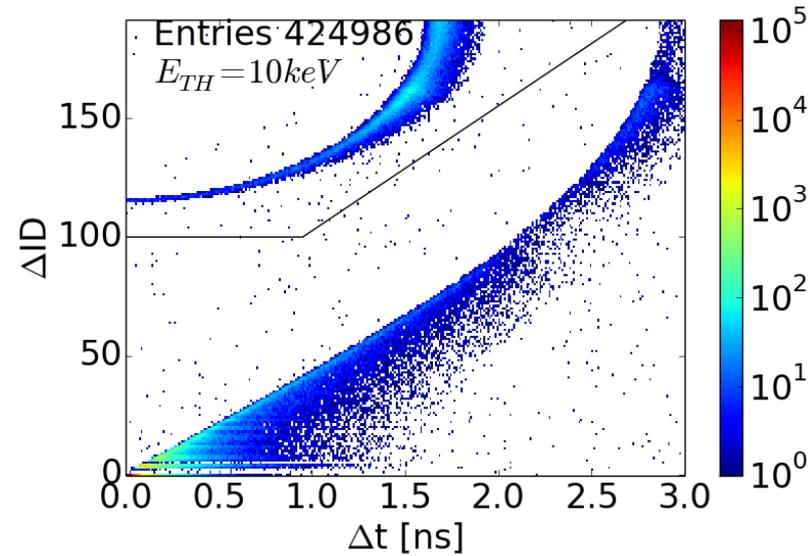
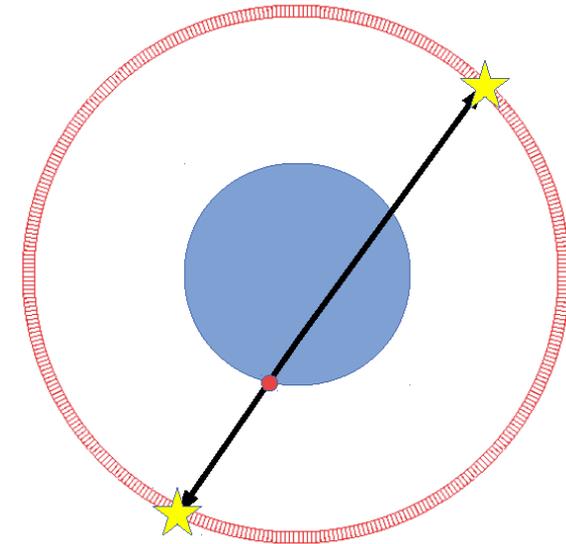
J-PET: P. Kowalski et al., Acta Phys. Pol. A127 (2015) 1505 and Acta Phys. Pol. B47 (2016)



# J-PET

## secondary scattering in the detector

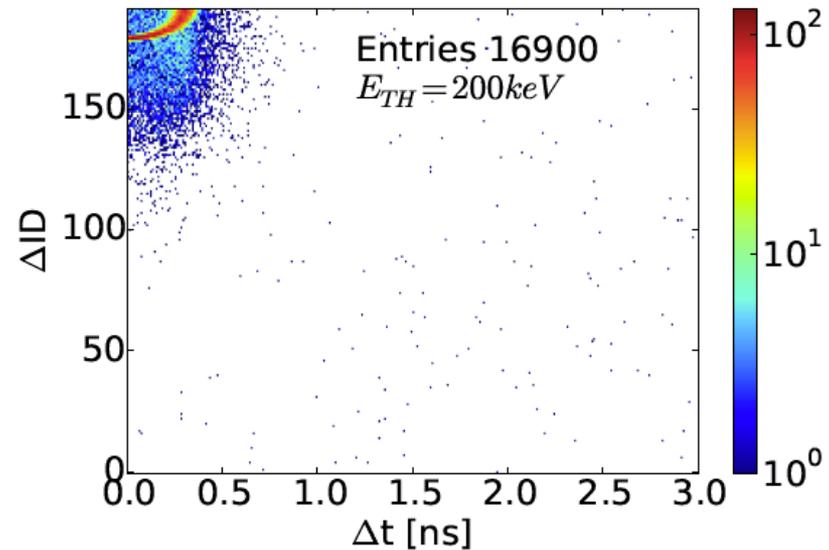
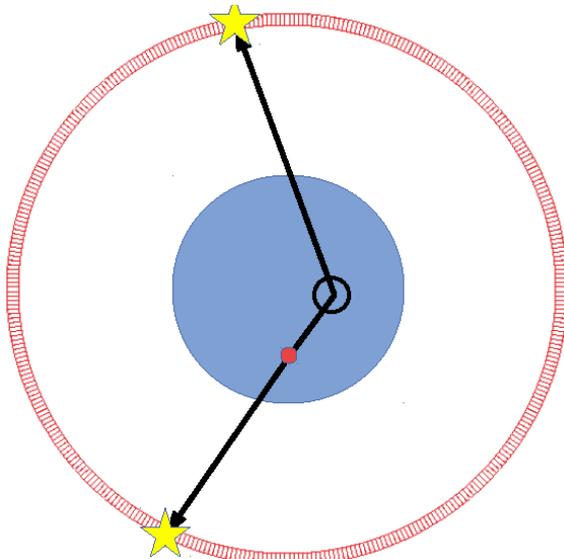
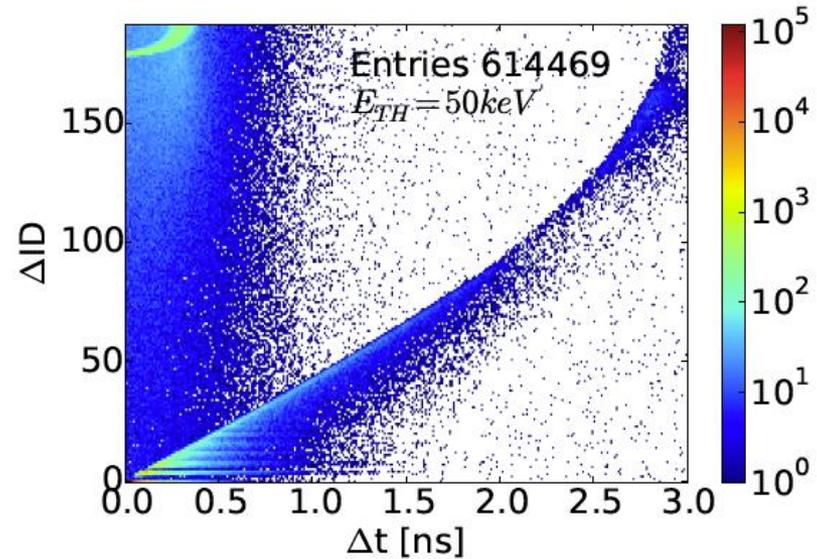
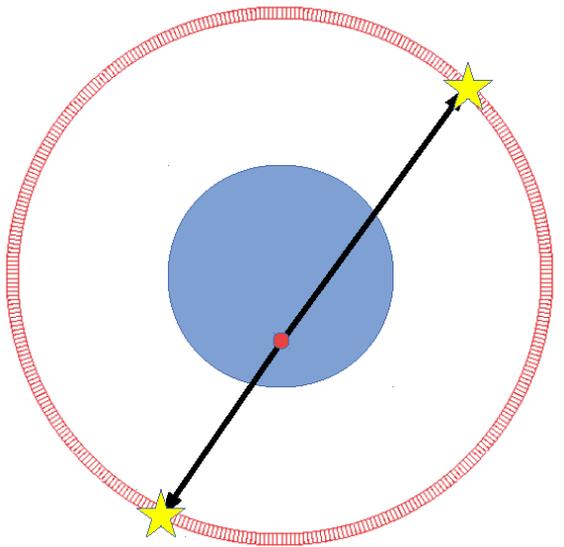
J-PET: P. Kowalski et al., Acta Phys. Pol. A127 (2015) 1505 and Acta Phys. Pol. B47 (2016)



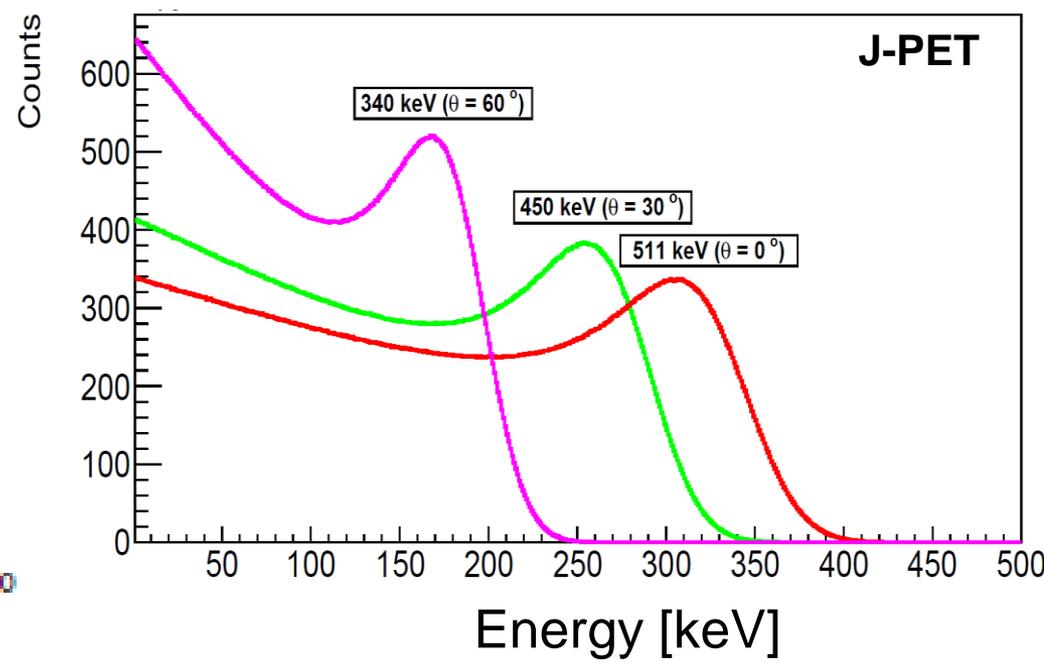
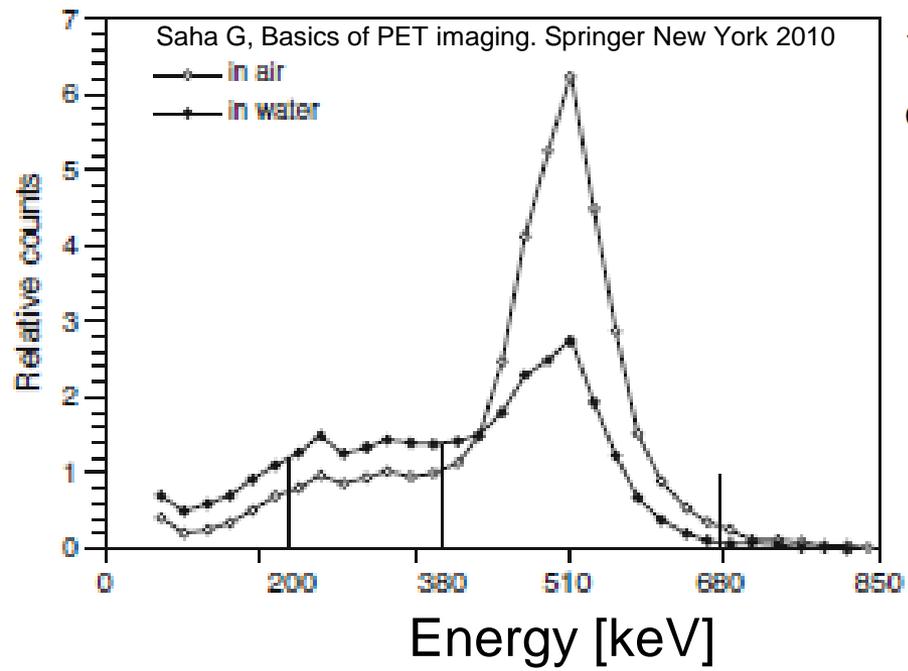
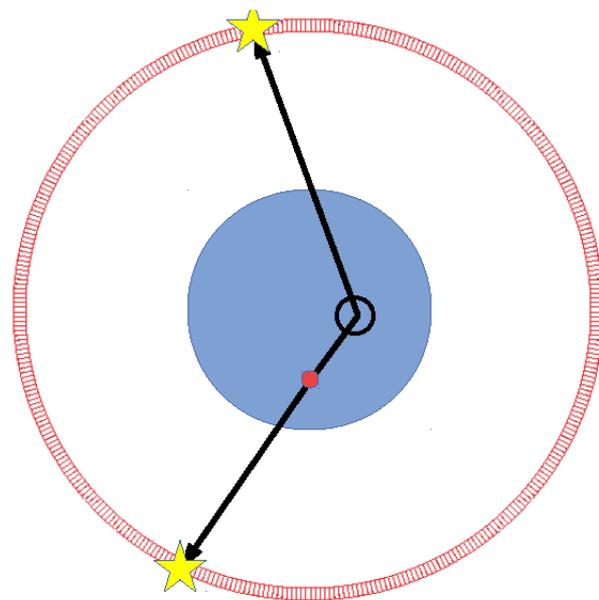
# J-PET

## secondary scattering in the detector

J-PET: P. Kowalski et al., Acta Phys. Pol. A127 (2015) 1505 and Acta Phys. Pol. B47 (2016)



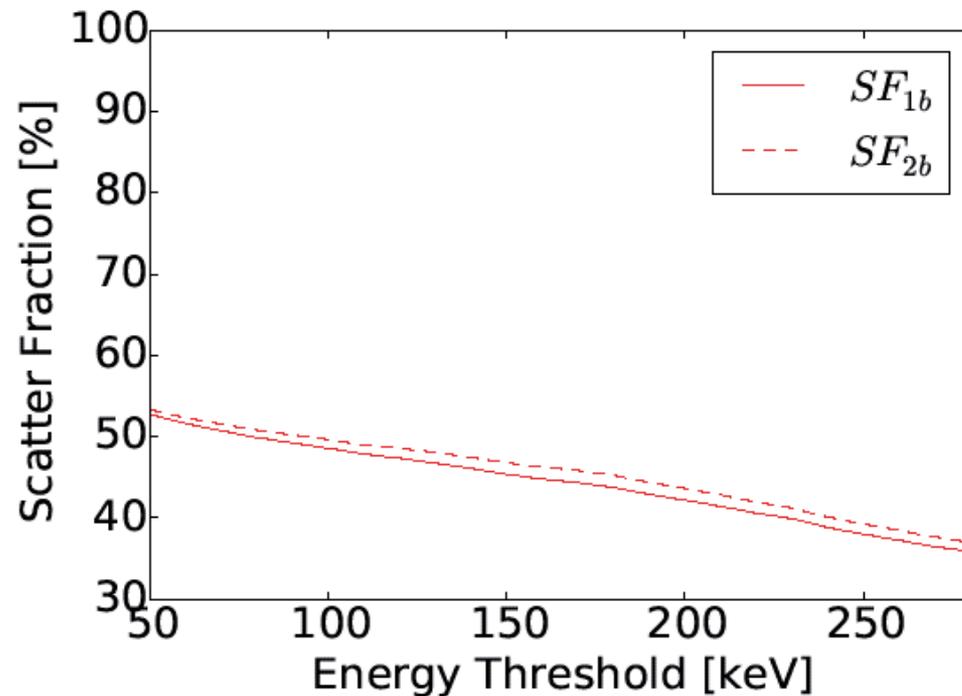
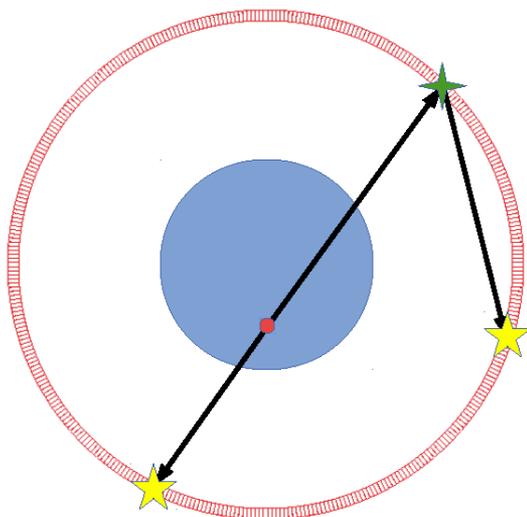
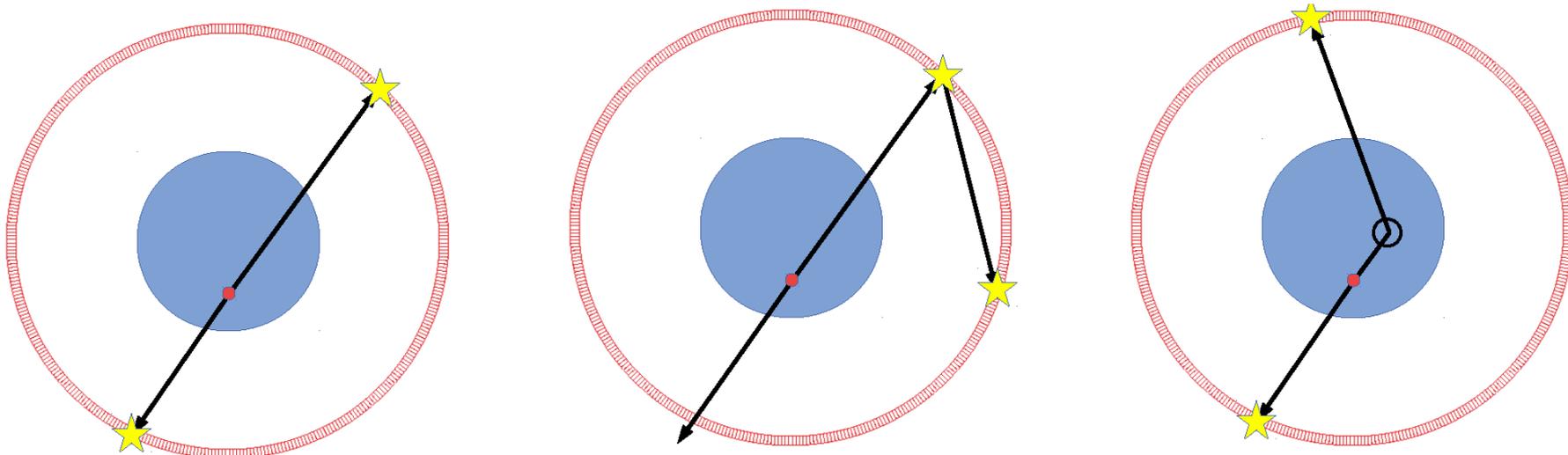
# J-PET scattering in the patient



# J-PET

# Scatter Fraction

J-PET: P. Kowalski et al., Acta Phys. Pol. A127 (2015) 1505 and Acta Phys. Pol. B47 (2016)



# J-PET CHARACTERISTICS

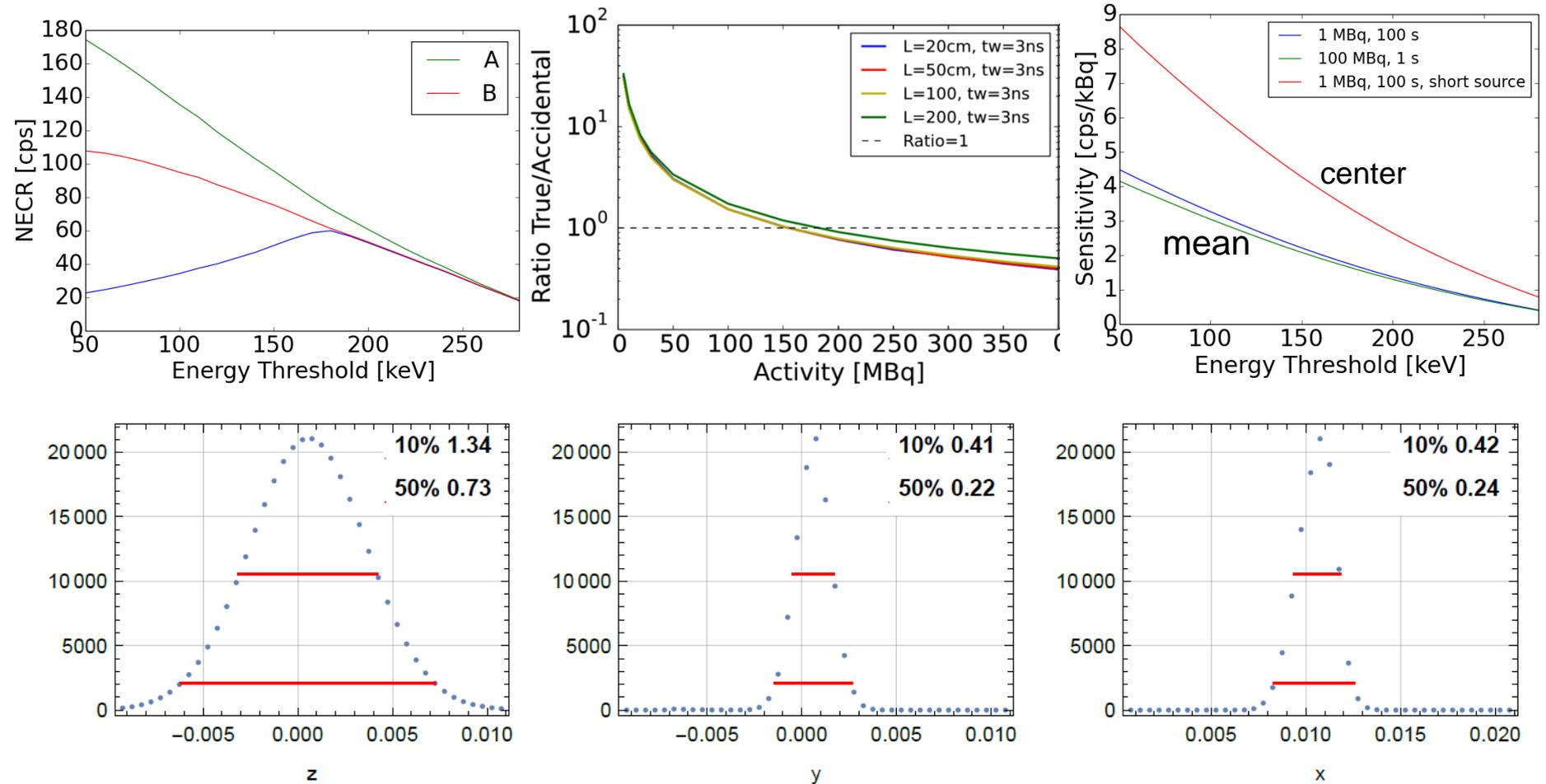
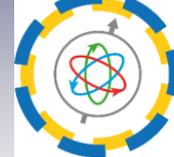


Figure 27: Reconstruction of the 1mm source located at (1, 0, 0) cm after 020 iterations. FullRing length 050 cm.

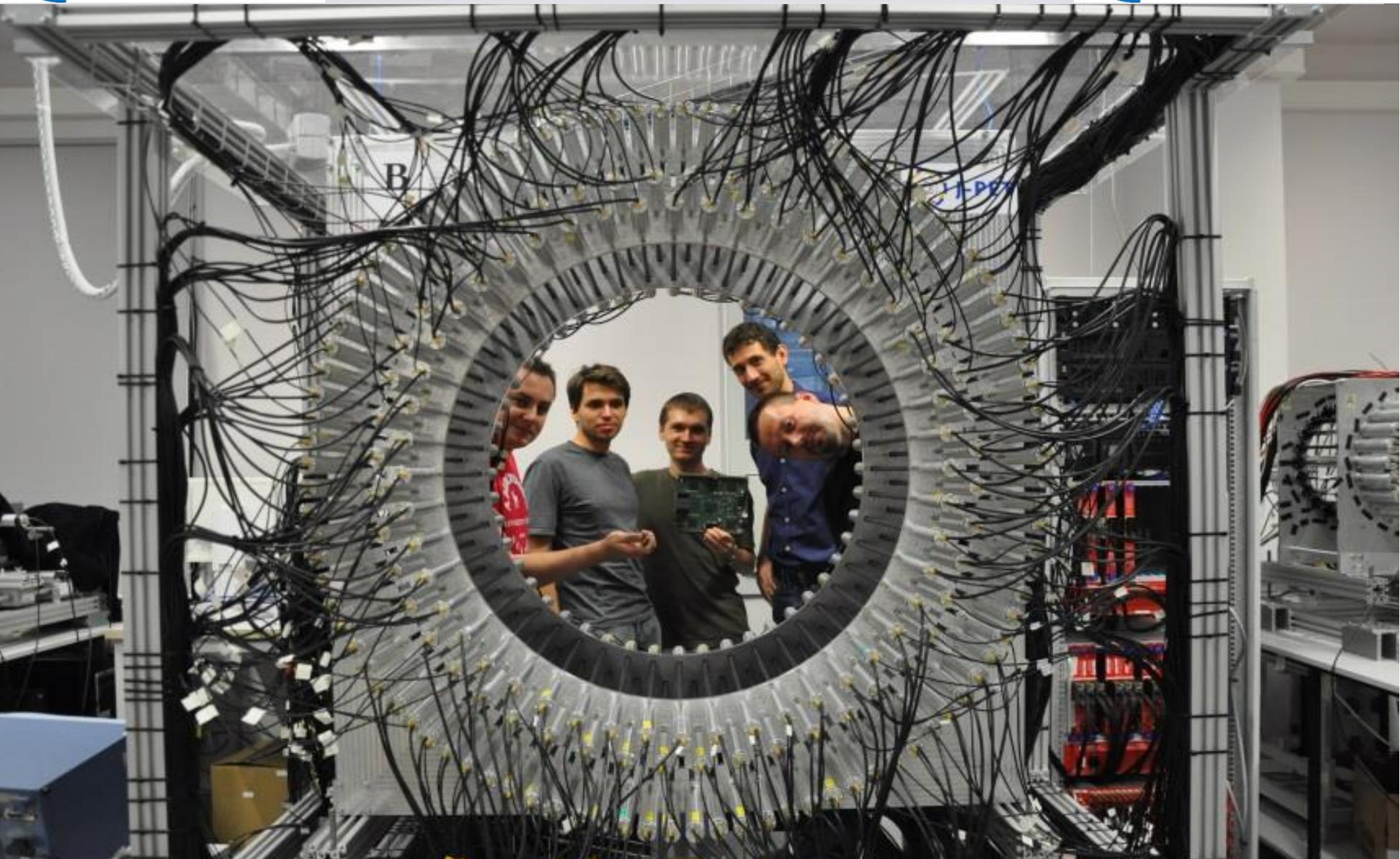


**J-PET**

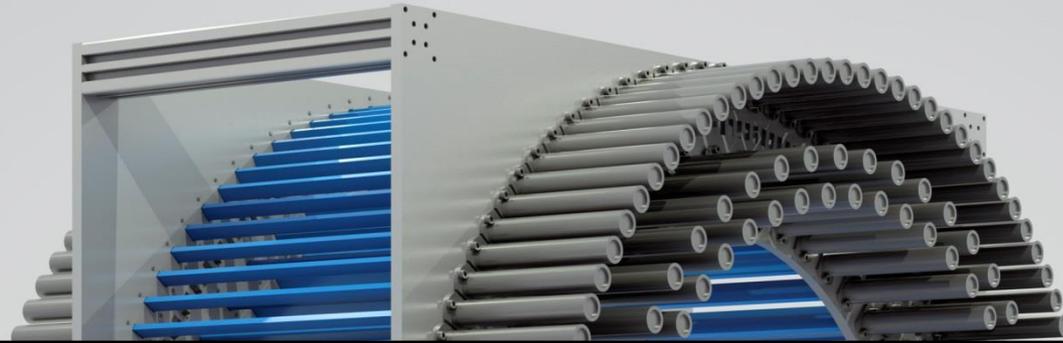
# Jagiellonian PET



**J-PET**

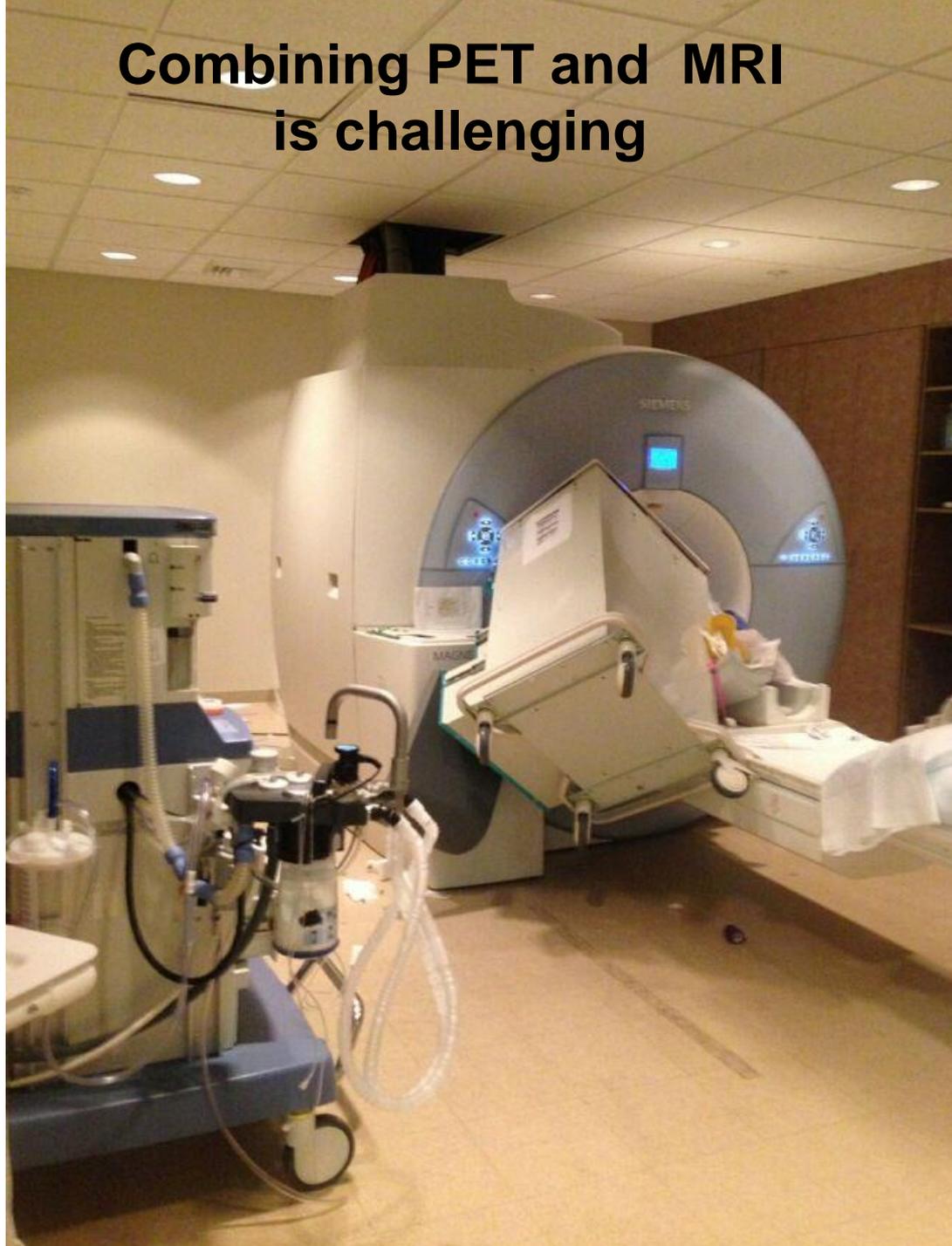


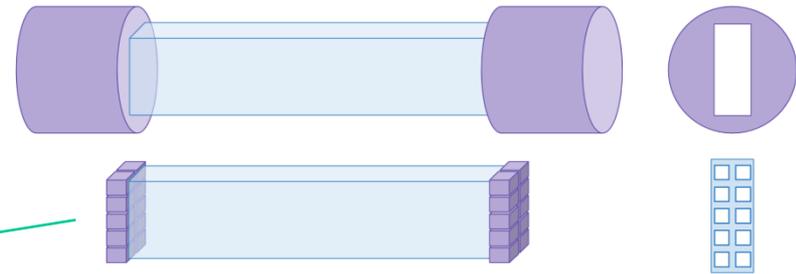
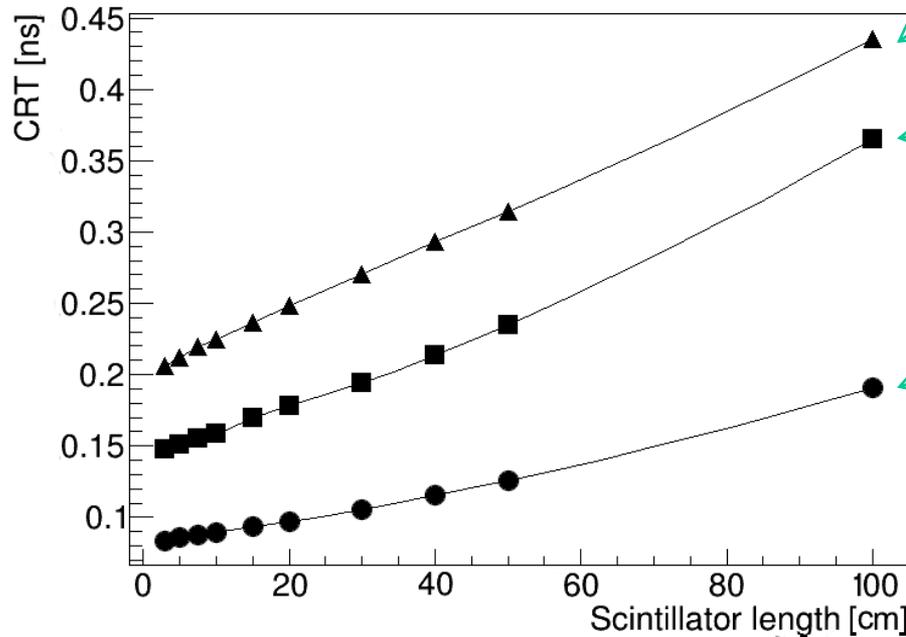
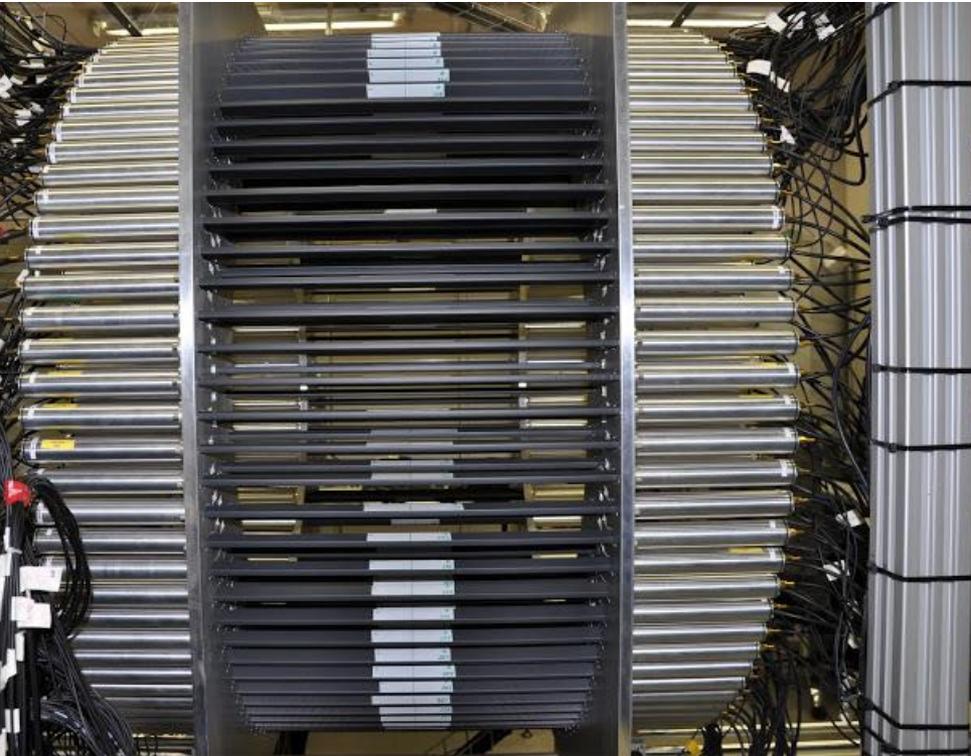
**AFOV: 17 cm  $\rightarrow$  50 cm ; TOF: 520 ps  $\rightarrow$  300 ps**



- Jagiellonian PET
- NEMA characteristics
- Towards simultaneous J-PET and MRI imaging

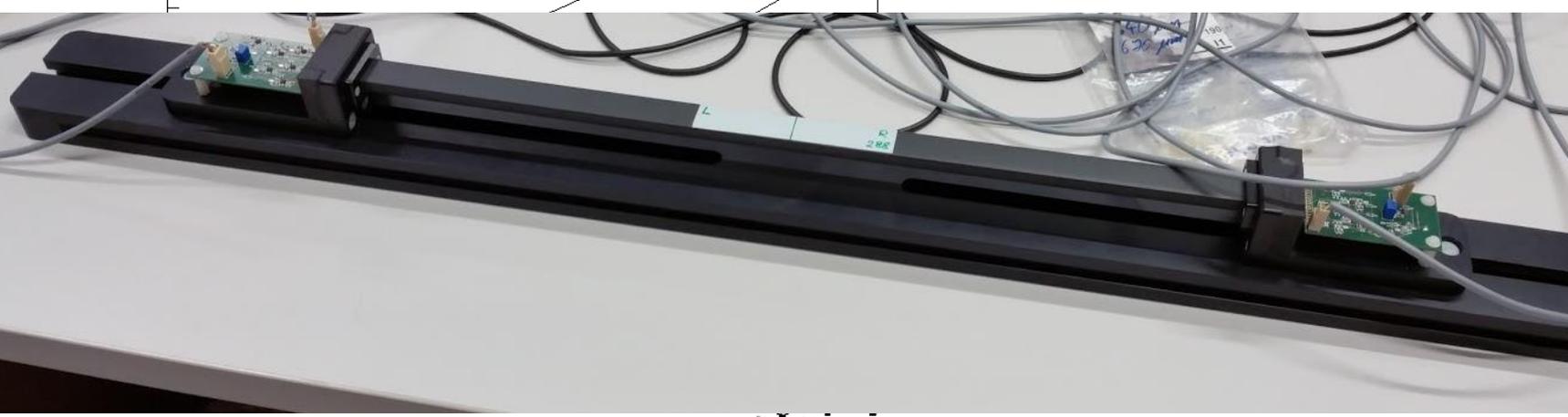
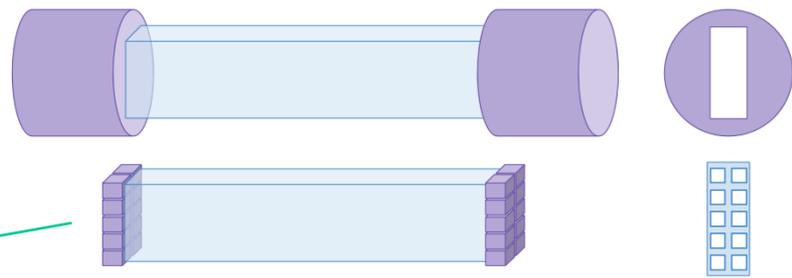
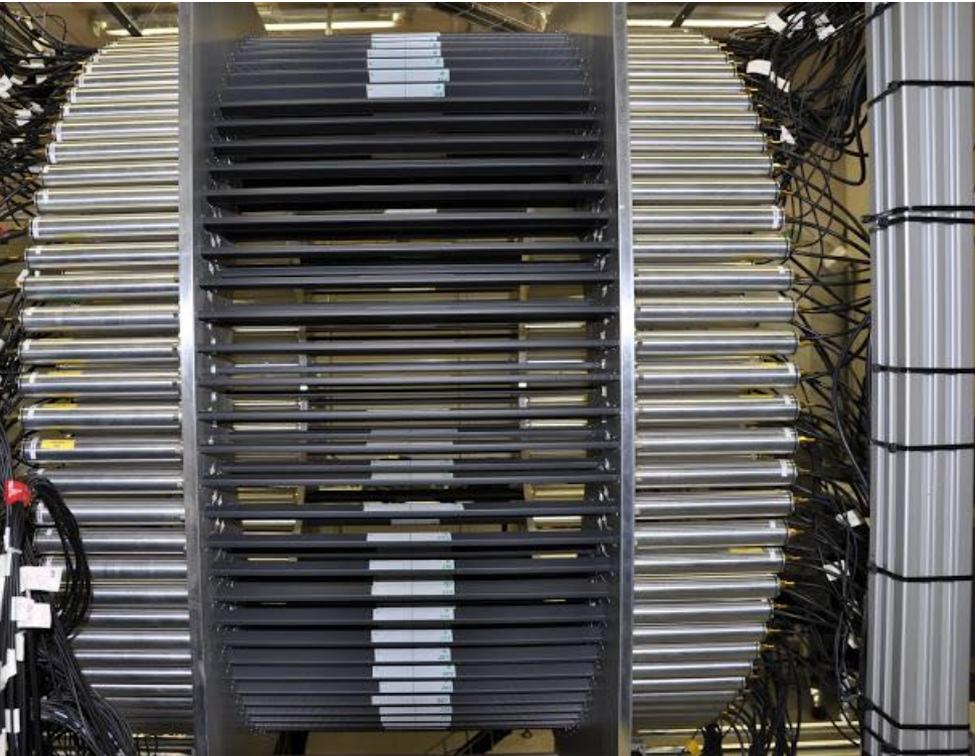
# Combining PET and MRI is challenging





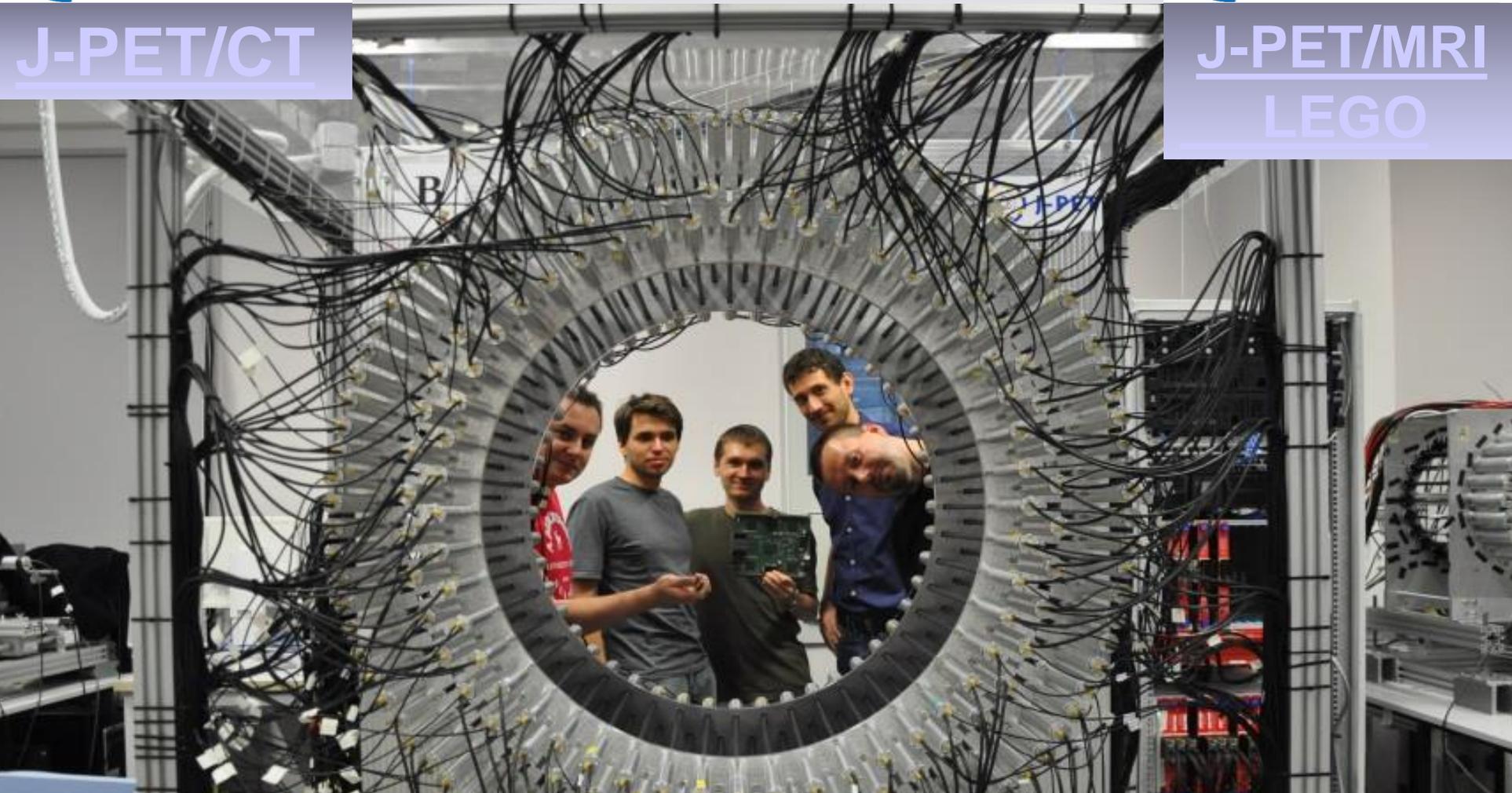
J-PET: P.M. et al., Phys. Med. Biol. (2016) in print ;  
arXiv:1602.02058

Limit of the J-PET



J-PET/CT

J-PET/MRI  
LEGO



**J-PET/CT:** P. M., PCT/EP2014/068363 (2013)

**J-PET/MRI:** P. M., PCT/EP2014/068373 (2013)

**J-PET/MRI insert:** B. Głowacz, P.M., M. Zieliński, P 413150 (2015)

**AFOV: 17 cm → 50 cm ; TOF: 520 ps → 300 ps**



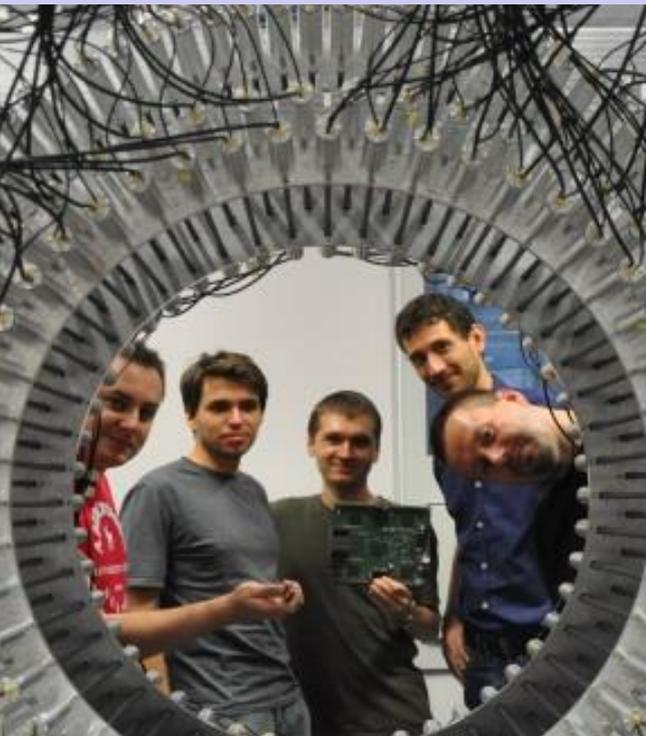
**J-PET**

# Jagiellonian PET



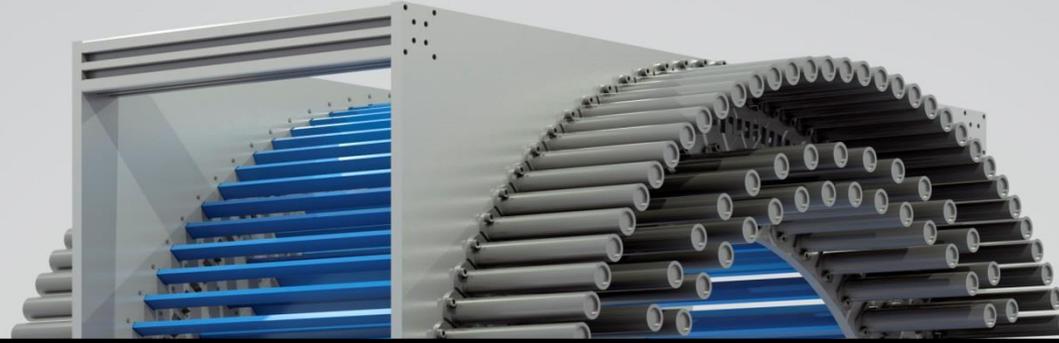
**J-PET**

**KING SIZE PET FOR LARGE ANIMALS**



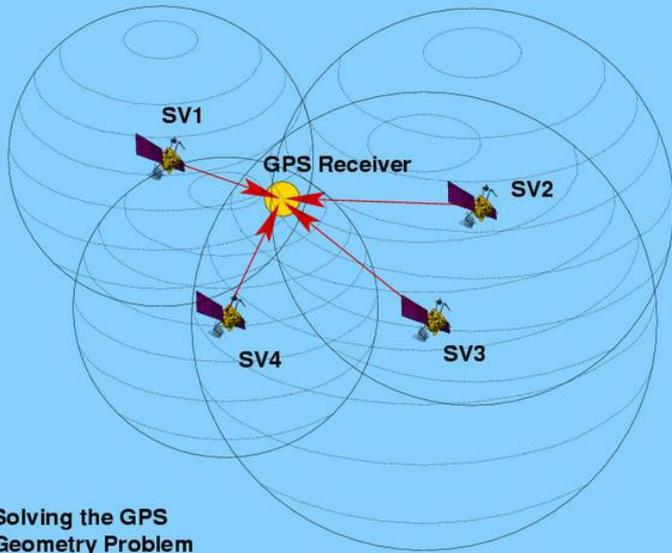
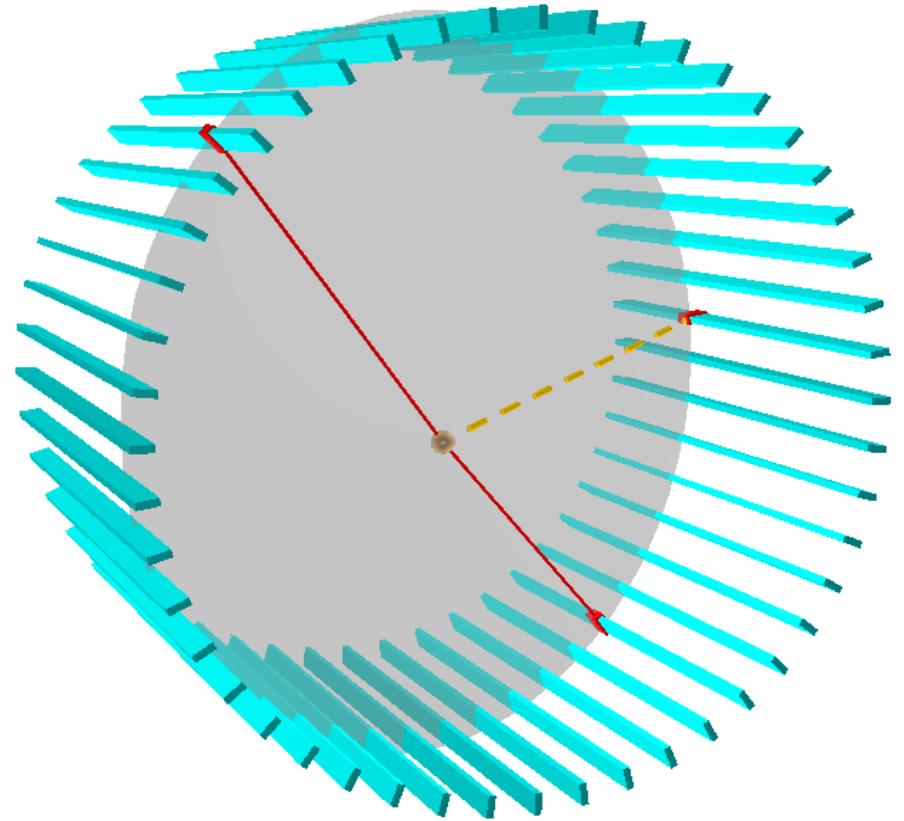
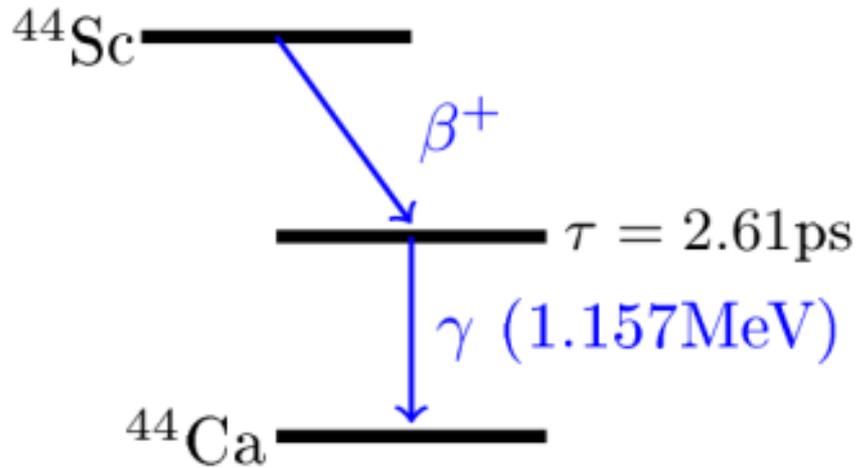
**THANK YOU  
FOR YOUR ATTENTION**

**AFOV: 17 cm  $\rightarrow$  50 cm ; TOF: 520 ps  $\rightarrow$  300 ps**



- Jagiellonian PET
- NEMA characteristics
- Towards simultaneous J-PET and MRI imaging
- **MULTI-PHOTON PET**

# 3-gamma tomography

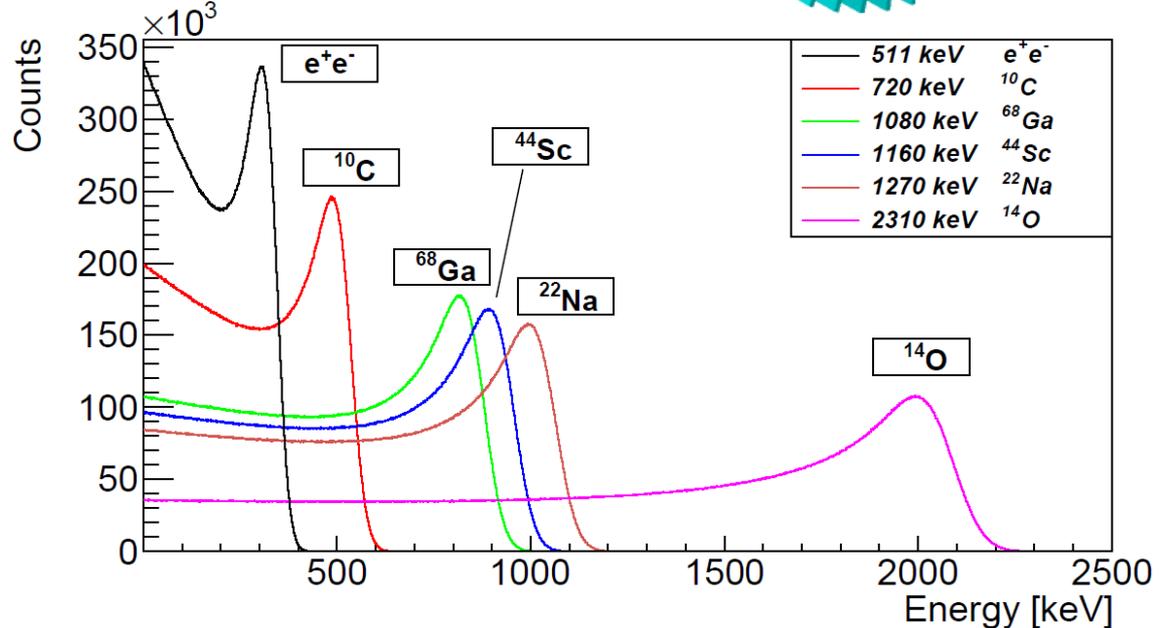
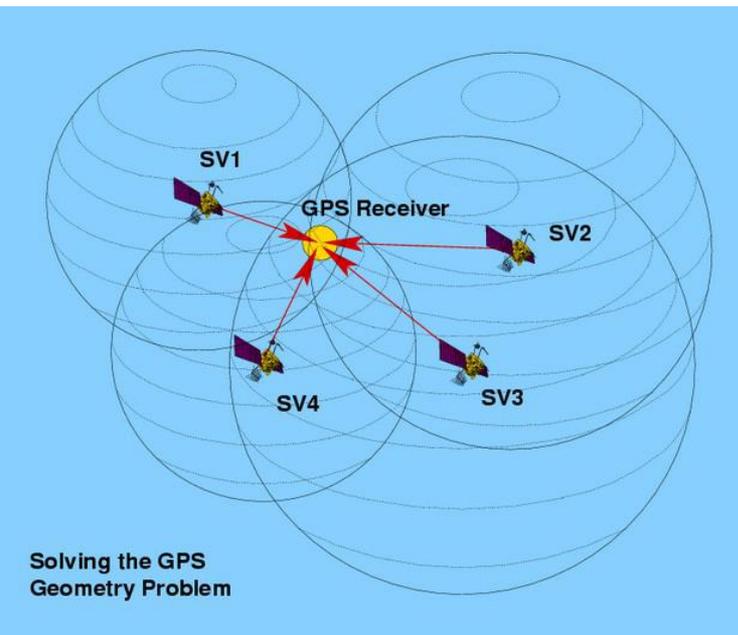
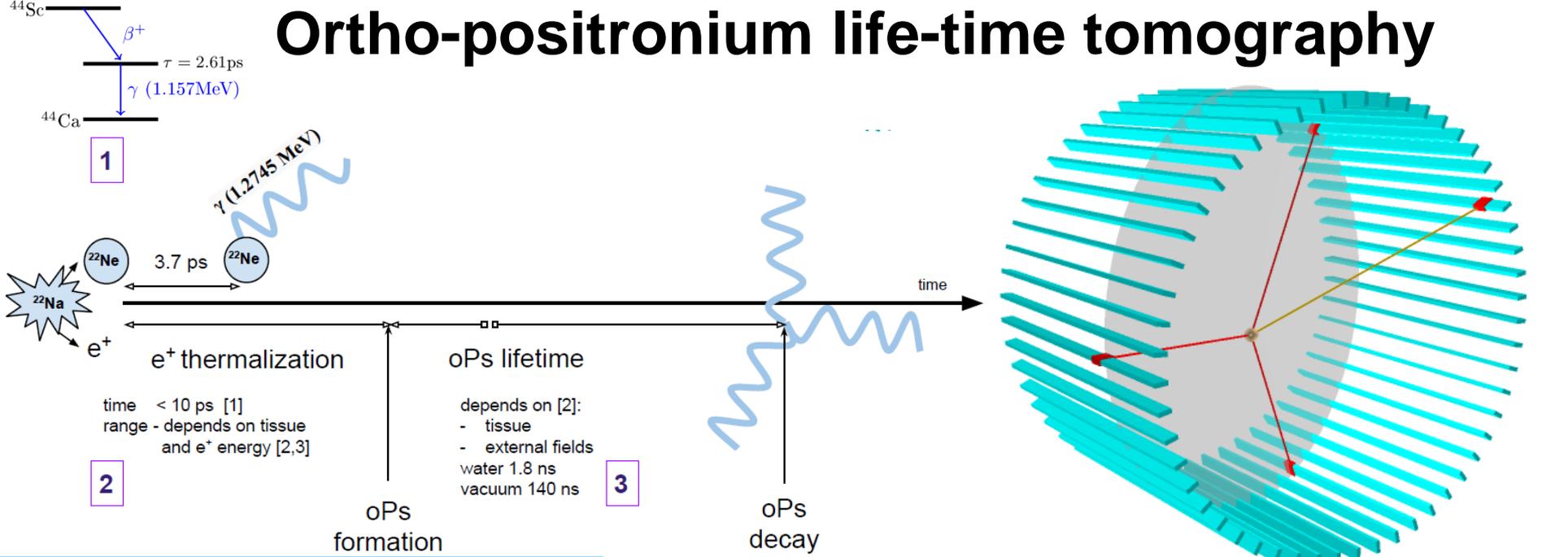


GPS-based trilateration reconstruction  
J-PET: A. Gajos et al.,  
Nucl. Instr. and Meth. (2016) submitted

P. M., **PCT/EP2014/068374 (2013)**

A. Gajos, E. Czerwiński, D. Kamińska, P. M., **PCT/PL2015/050038 (2015)**

# Ortho-positronium life-time tomography



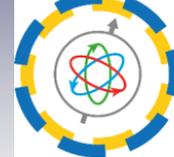
P. M., PCT/EP2014/068374 (2013)

A. Gajos, E. Czerwiński, D. Kamińska, P. M., PCT/PL2015/050038 (2015)



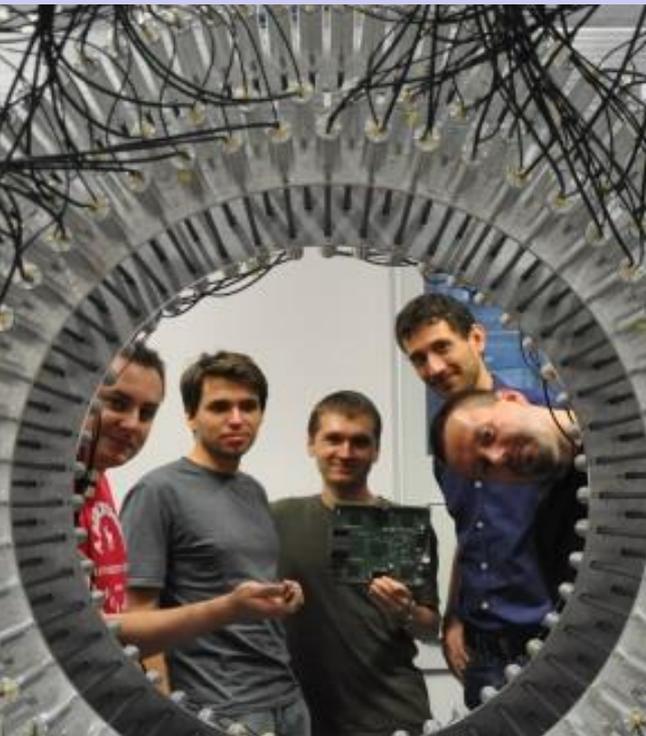
**J-PET**

# Jagiellonian PET



**J-PET**

**KING SIZE PET FOR LARGE ANIMALS**



**THANK YOU  
FOR YOUR ATTENTION**

**AFOV: 17 cm  $\rightarrow$  50 cm ; TOF: 520 ps  $\rightarrow$  300 ps**

Device	Sensitivity	SF	NECR	PSF	Diameter	AFOV
<b>GE Discovery STE and VCT</b>	2.3 cps/kBq (8.8 cps/kBq) (R0, centre of field of view) and 2.3 cps/kBq (8.9 cps/kBq) (R10) [1]	The system scatter fraction was 21.4% in 2D at an energy of 375 keV (33.9% in 3D mode at a higher energy of 425 keV).[1]	84.9 kcps at 43.9 kBq/ml (2D) and 67.6 kcps at 12.1 kBq/ml (3D) [1]	Transaxial resolution FWHM for 2D(3D) mode at 1 cm offset from the centre of the field of view (R1) was 4.87 mm (5.12 mm) and at 10 cm off centre (R10) radially 5.70 mm (5.89 mm) and tangentially 5.84 mm (5.47 mm). The axial resolutions were 4.4 mm (5.18 mm) (R1) and 5.99 mm (5.86 mm) (R10). [1]	88.6 cm [2]	15.7 mm [2]
<b>Philips Gemini TF PET/CT</b>	7 cps/kBq (NEMA) and > 14 cps/kBq (TOF) [3]	From 27% to 45% [4]	110 kcps (NEMA) and > 220 (TOF) [3]	FWHM r=1cm: transverse 4.8 mm axial 4.8 cm r=10cm: radial 5.2 mm tangential 5.2 mm axial 4.8 [4]	90 cm [4]	18 cm [5]
<b>Siemens Biograph TM</b>	4.2 cps/kBq [6]	From 31% to 34% [7]	9 kcps at 1 kBq/ml [7]		83 cm [7]	21.8 cm [5]

[1] Eur J Nucl Med Mol Imaging. 2007 Oct;34(10):1683-92. Epub 2007 Jul 28., <http://www.ncbi.nlm.nih.gov/pubmed/17661031>

[2] <http://www.medwow.com/med/petct/ge-healthcare/discovery-ste-16-petct/67494.model-spec>

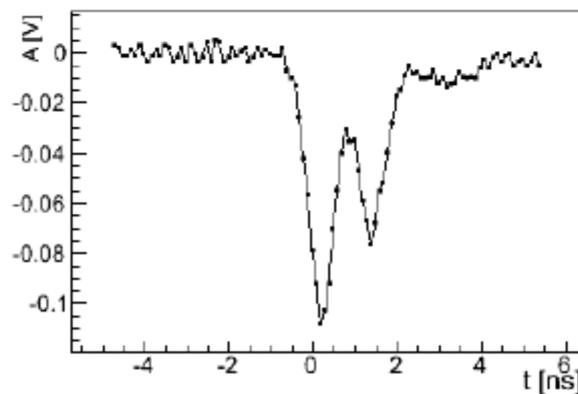
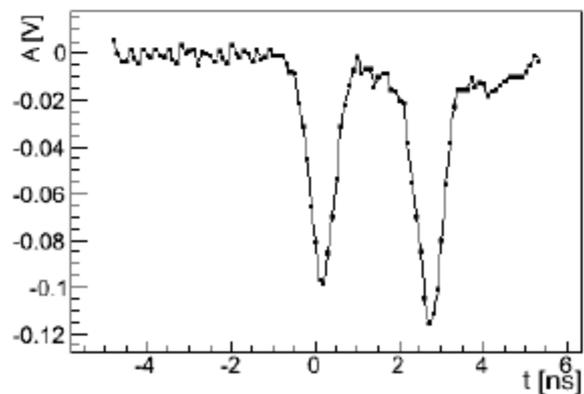
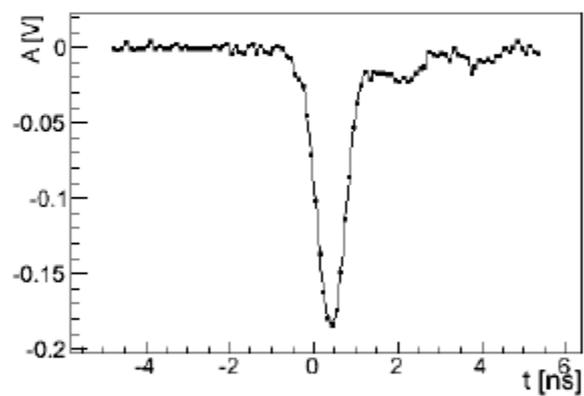
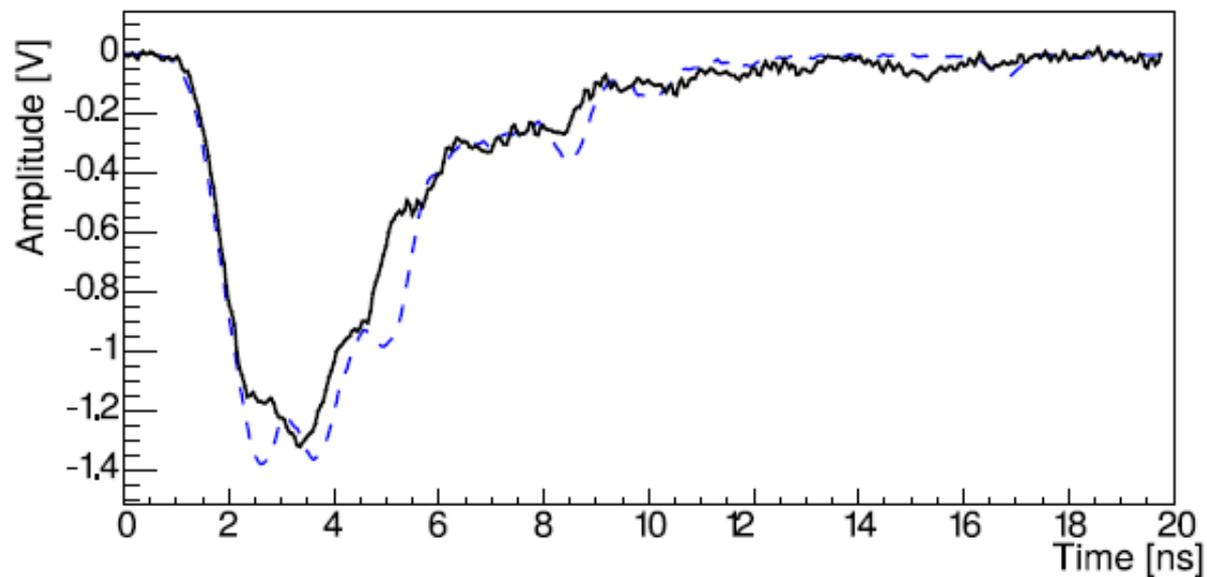
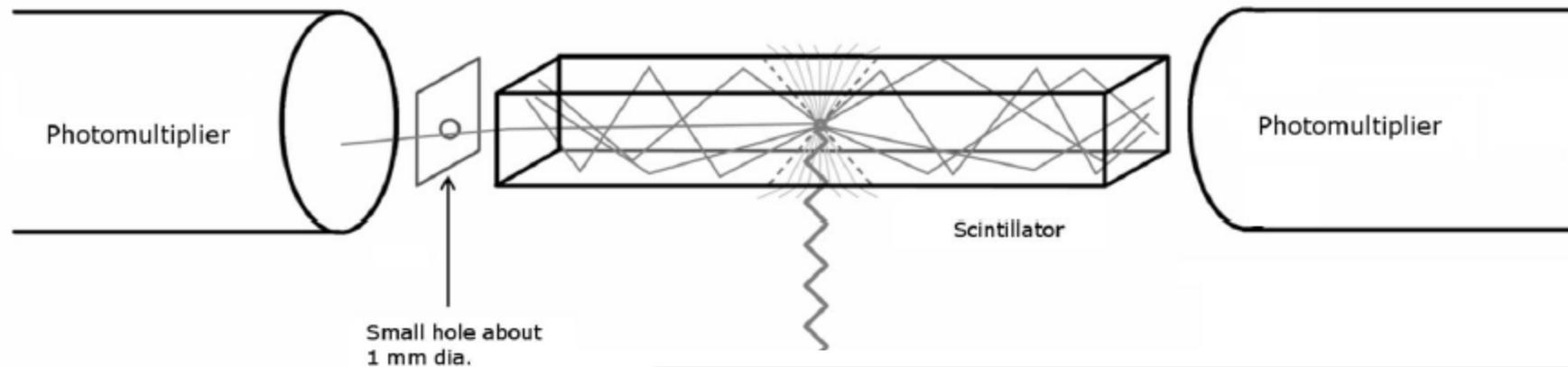
[3] <http://www.usa.philips.com/healthcare/product/HC882471/gemini-tf-pet-ct-scanner>

[4] S. Surti et al., J Nucl Med. 2007 Mar;48(3):471-80

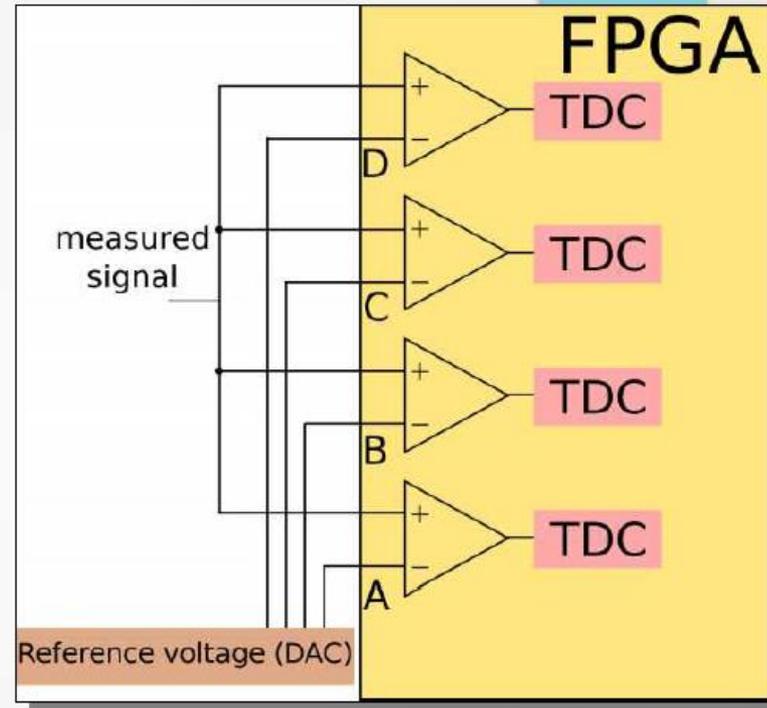
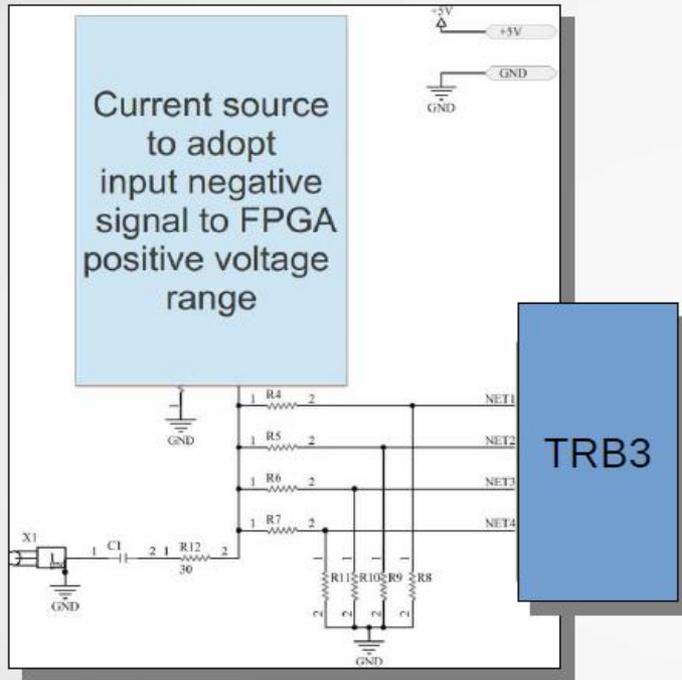
[5] <https://www.aapm.org/meetings/08SS/documents/Townsend.pdf>

[6] [http://www.activexray.com/pdf/Siemens\\_Biograph.pdf](http://www.activexray.com/pdf/Siemens_Biograph.pdf)

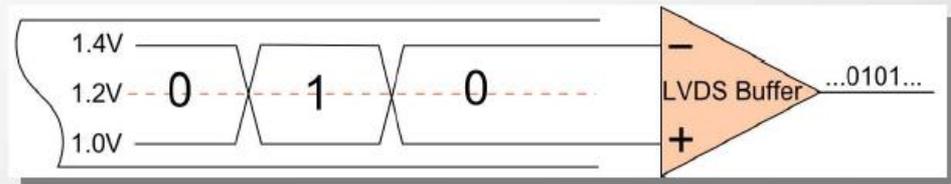
[7] P. Gonias et al., Nucl. Instrum. Methods Phys. Res. A, 571 (2007), 263



# FEE dive in



Discrimination of the signal is done with LVDS buffer which acts as a comparator. This innovative approach is the subject of **patent application**



**PCT/EP2014/068367 (2014)**

# TDC in FPGA

## FPGA

