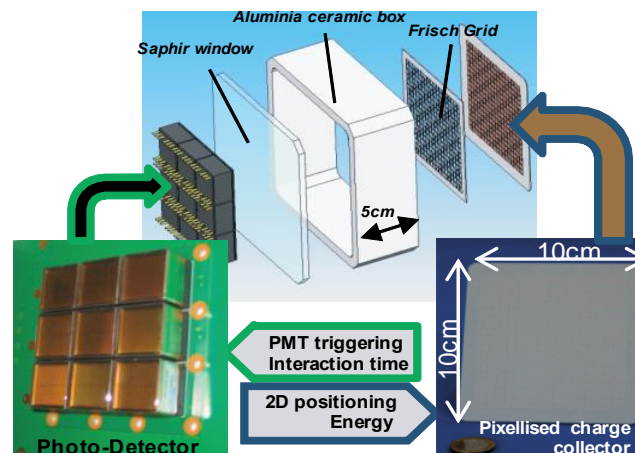
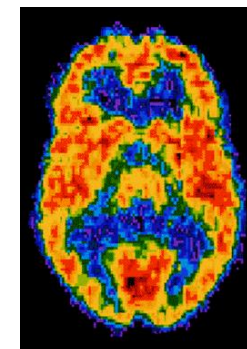
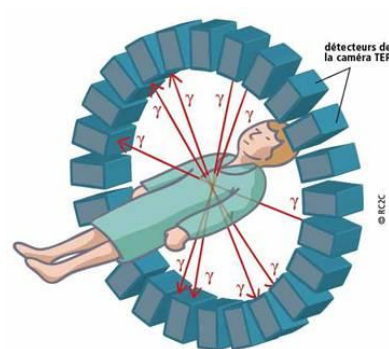


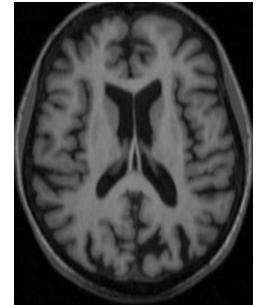
Status of the CaLIPSO High-Resolution PET Project

- I. Achieving 1 mm³ resolution for PET-scan
- II. Physical principle
- III. Optical detector
- IV. Ionization detector
- V. Full image simulation
- VI. Conclusion



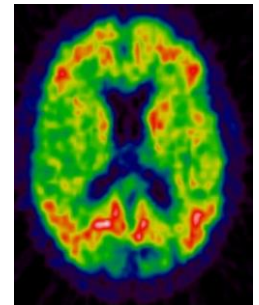
Magnetic Resonance Imaging (MRI)

- **Structure** visualization, 3D matter density
- **Excellent spatial resolution:** 1 mm³ over the whole brain
- **Low sensitivity** to cells biochemical activity $\sim 10^{-4}$ mol



Positron Emission Tomography (PET)

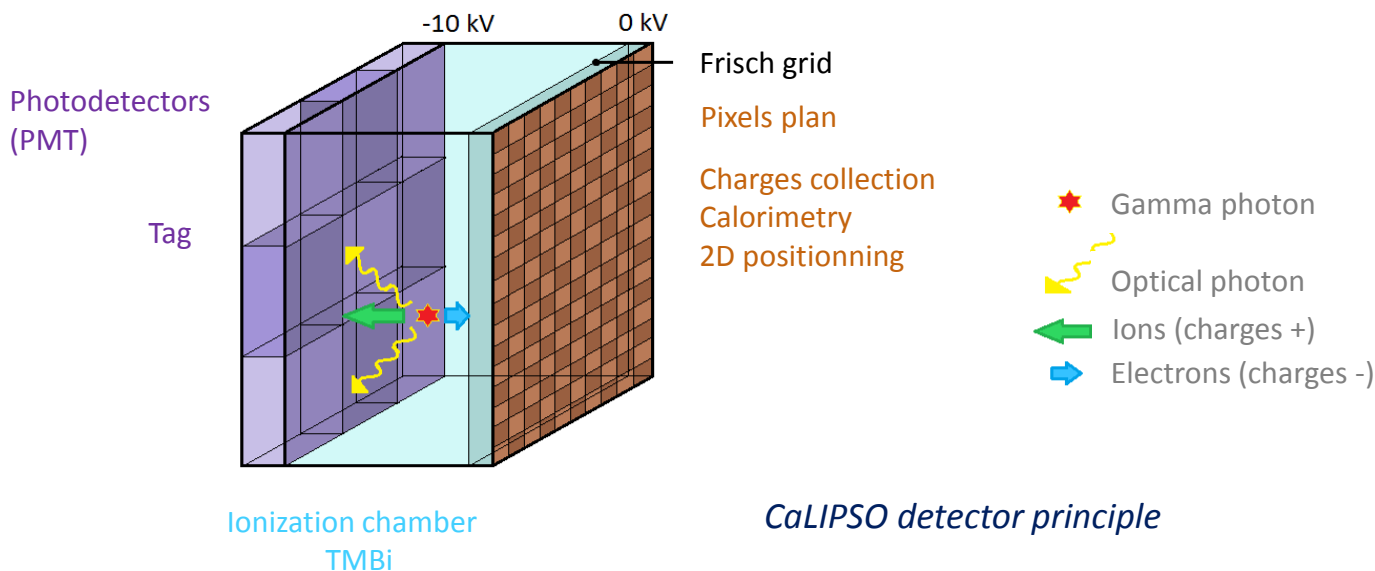
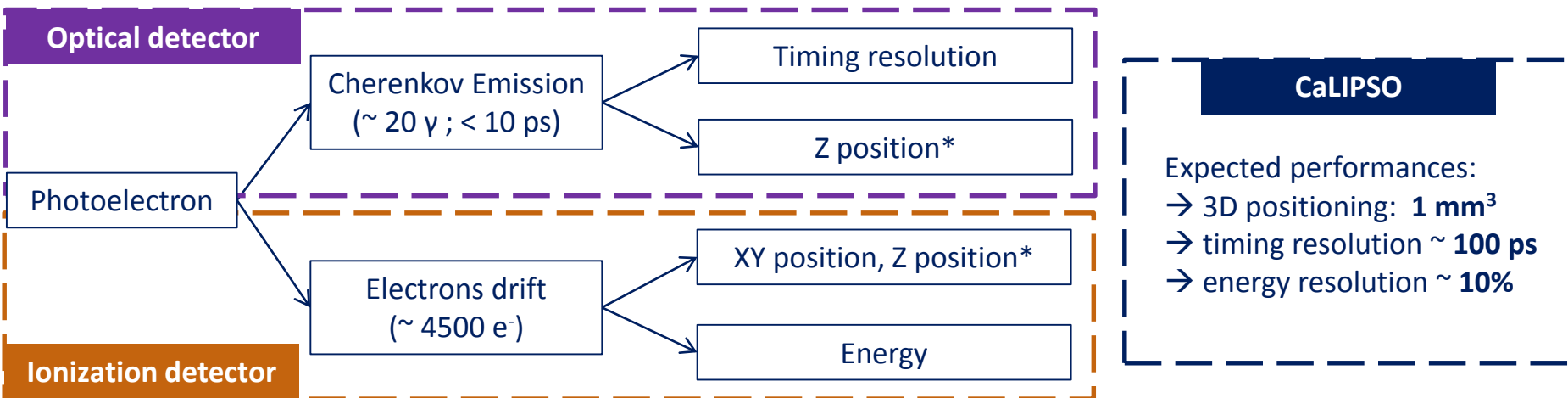
- Visualization and **quantification of biological activity**
- **Low spatial resolution,** (2.2 mm)³ at best over the whole brain
- **Excellent quantification** of the biochemical activity $\sim 10^{-12}$ mol
- Irradiation of the patient and the **operator** → Dose reduction

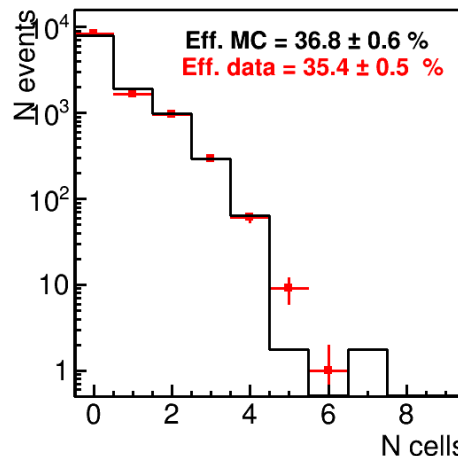
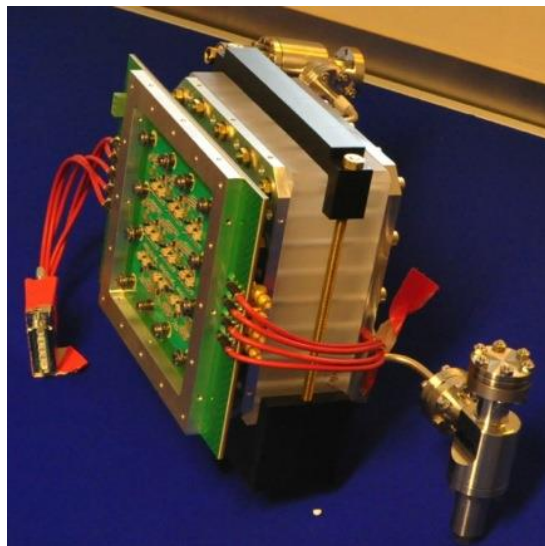


Issues

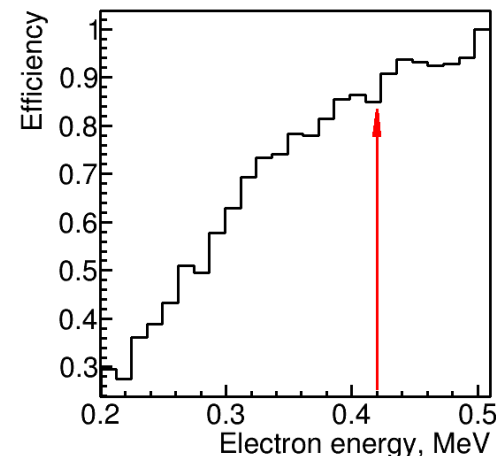
- **Localization** of γ interactions within the detector to **1 mm³**
- **Gain** in detection/imaging **efficiency** of a **factor 10**

- **Neuro-degenerative diseases research**
- **Positron annihilation spectrometry**



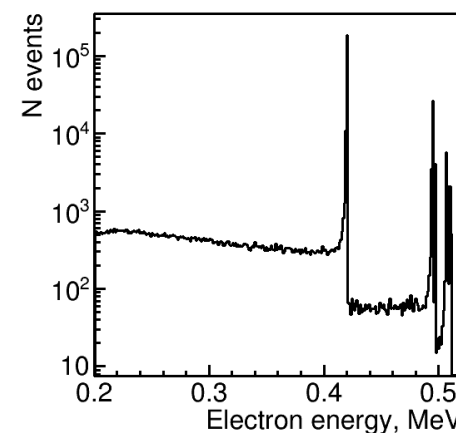


Cherenkov photons detected



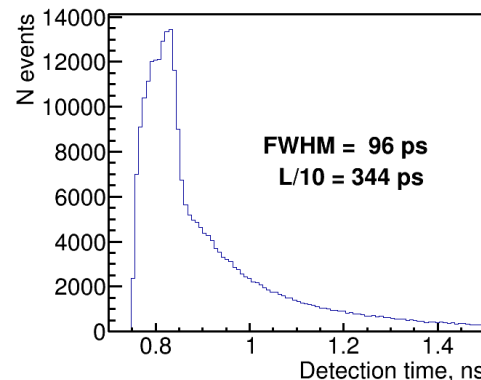
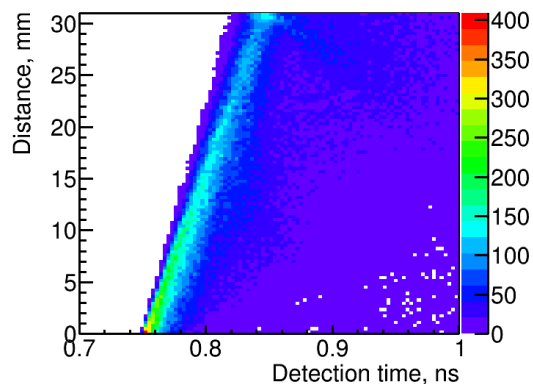
Detection efficiency

- **Fully efficient** on 511 keV γ through PE conversion
 - **90%** detection efficiency at 420 keV
 - 27 % expected / 34,5 % experimental \rightarrow few Compton interactions detected
- Monte Carlo matches data

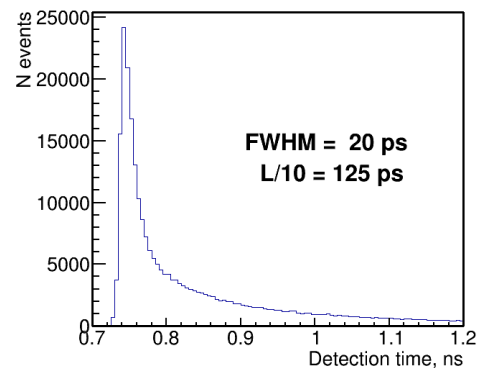
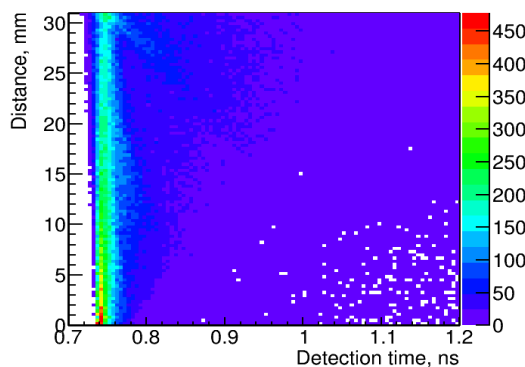


511 keV γ spectrum in TMBi

Detection time / position correlation



Detection time after decorrelation



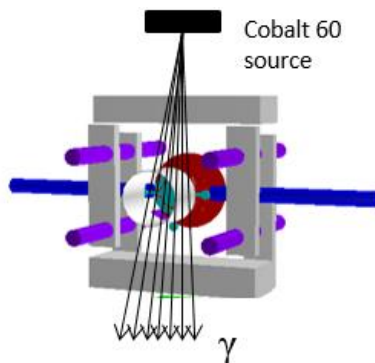
- 540 ps experimental due to R11265 PMTs
- Simulation shows correlation between detection time and interaction position
 - 96 ps correlated / **20 ps after decorrelation**
- Current fastest PMT → MCP-PMT with 70 ps FWHM resolution
 - Near future → **Coincident Resolution Time of 150 ps**

- **Ionization chamber**
- Our goals :
 - **10% energy resolution**
 - **200 ns timing resolution** on charge collection
- Ionization current → 3 main factors :
 - Charge production yield (number of free electrons / 100 eV)
 - Electron mobility → proved by ionization current / electric field dependency
 - Electron lifetime
- Charge measurements → closer to final detector
 - Electron mobility / lifetime values
- Very low signals (pA, fC) → eliminate noise sources

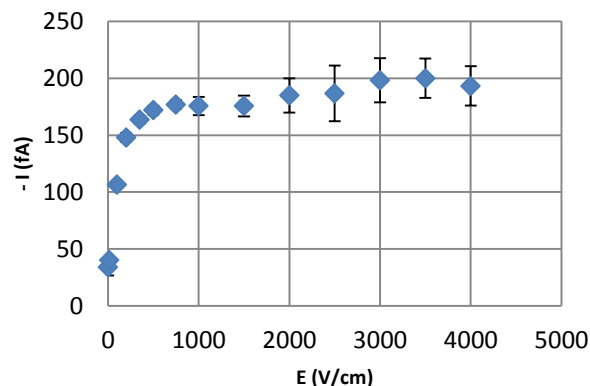


Single pixel detector

Ionization current measurements



$$I = f(E)$$



- Energy information lost by electronegative impurities capturing secondary electrons
- Electrons lifetime $> 20 \mu\text{s}$ needed
 - Electrons scavengers $< 0,1 \text{ ppm}$ oxygen equivalent
 - Molecular sieves, getter materials, silica gel, activated alumina...
 - **Large effort**
- Ultra-high vacuum cleaning procedure



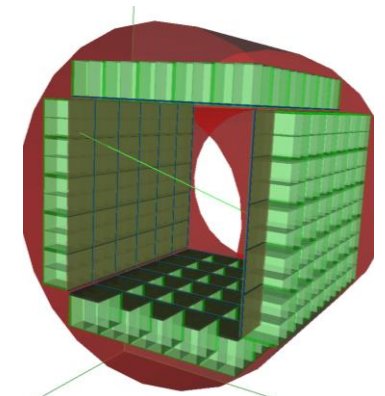
*Ultrapurification
stations*



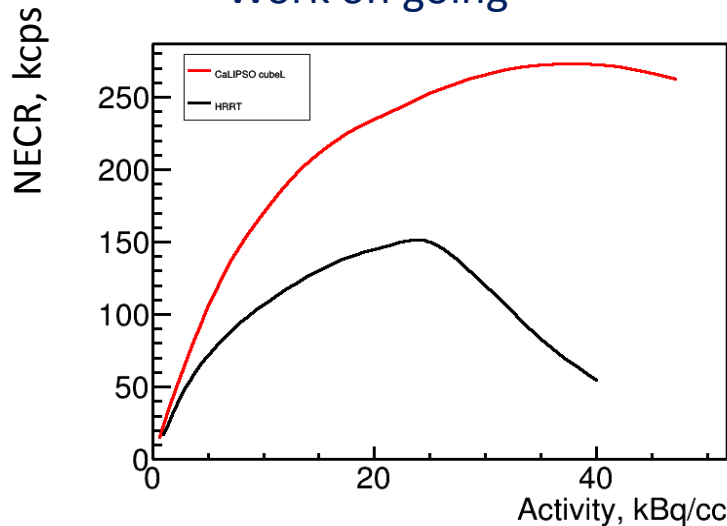


Olga Kochebina

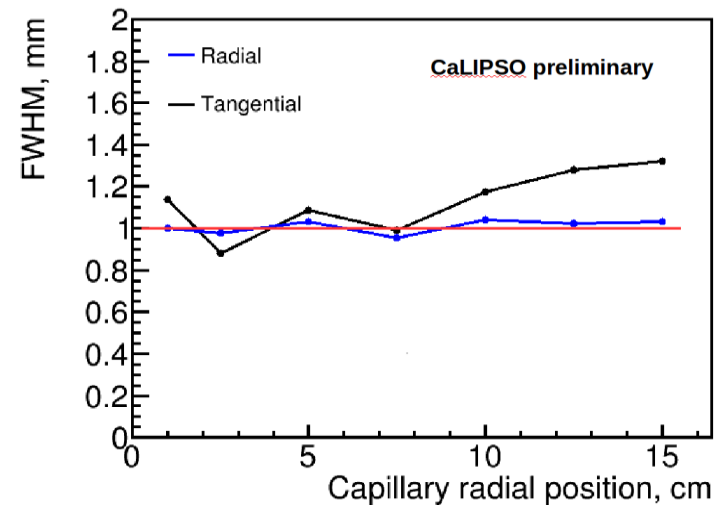
- GATE software (led by CEA/SHFJ)
- Improve NECR → improve efficiency
 - Better than Siemens HRRT (before TOF information)
- Improve resolution
 - ~ 1 mm at FOV center (2,3 mm for HRRT)
 - No significant Depth Of Interaction effect (2,3 - 3,2 mm for HRRT)
- Work on going



PET CaLIPSO geometry



NECR comparison HRRT / CaLIPSO



Spatial resolution regarding radial position

O. Kochebina, IEEE NSS/MIC, conf. record, San Diego, Nov 2015, in Press.

- CaLIPSO Project : Ambitious technology for High-resolution PET-scan
 - Excellent efficiency (photofraction, solid angle, TOF) → reduced dose
 - Foreseen spatial resolution : 1 mm³
 - Coincident Resolution Time < 150 ps → TOF information
- Now Operational
 - Optical detector fully efficient for photoelectron detection
 - Single pixel detector (ionization)
 - Efficient purification achieved on reference liquid tetramethylsilane
- On going
 - TMBi ultrapurification
 - Optical detector upgrade with MCP-PMT
 - Full PET-scan simulation with GATE → foreseen performance



D. Yvon

Responsable scientifique



G. Tauzin

Chef de projet



P. Verrecchia

Physique du détecteur



S. Sharyy

Physique du détecteur



X. Mancardi

Thèse Démonstr. ionisation



O. Kochebina

Post. Doc. Simu. PET Optimisée



J.P. Mols

Mécanique



P. Starzynski

Mécanique et Ultra-Vide



J.P. Bard

Électronique et labo



Ph. Abbon

Elec. Analog. Rapide



M. Kebbiri

Techno. Détec. Avancées



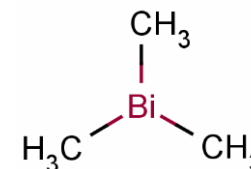
C. Canot

Thèse Détec. Opt. rapide.

- D. Yvon, J-Ph Renault, « Détecteur de photons à haute énergie » (High energy photon detector), Patent, Ref: FR 1 052 047, 22 March 2010, and WO2011/117158 A1.
- D. Yvon al., “The CaLIPSO detector project for enhanced PET imaging”, IEEE TNS-MIC conf. record. Anaheim, Nov. 2012, 10.1109/NSSMIC.2012.6551441
- P. Verrecchia, et al., « CaLIPSO: TMBi properties for particles detection », IEEE TNS-MIC conf. record, Anaheim, Nov. 2012, 10.1109/NSSMIC.2012.6551104
- D. Yvon, « Détecteur de photons à haute énergie », Patent, 12 novembre 2013 Reference: 13 61037 au nom du CEA.
- D. Yvon, J-Ph. Renault, G. Tauzin, et al., “CaLIPSO: An novel detector concept for positron annihilation detection”, ANNIMA conf. record June 2013, 10.1109/ANIMMA.2013.6728041
- D. Yvon, J-Ph. Renault, G. Tauzin et al., “CaLIPSO: An novel detector concept for PET imaging”, IEEE TNS, vol. 61 (2014) 60.
- E. Ramos, D. Yvon, P. Verrecchia, G. Tauzin et al., « Trimethyl Bismuth Optical Properties for Particle Detection and the CaLIPSO Detector », IEEE Trans. on Nuclear Science, Vol. 62 (2015) p. 1326 - 1335
- O. Kochebina, IEEE NSS/MIC, conf. record, San Diego, Nov 2015, in Press.
- E. Ramos, et al., « Efficient, Fast 511-keV γ detection through Cherenkov radiation: the CaLIPSO optical detector », J. of Instr., in prep.

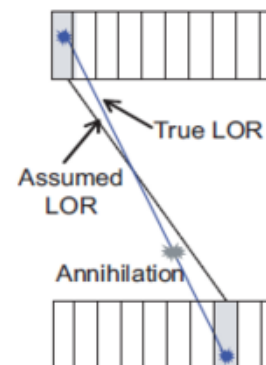
TMBi has the best coincident photoelectric conversion yield (47%)

- A factor 2 gain compared to the reference detector (LSO crystal)



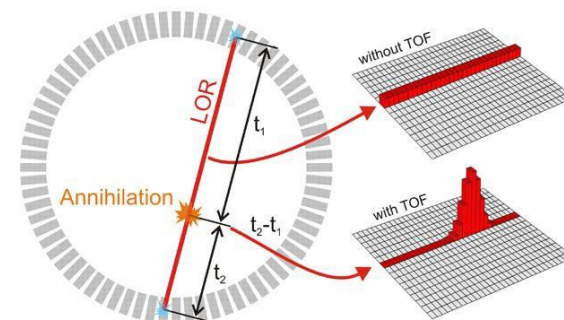
1mm³ 3D interaction positioning in detector

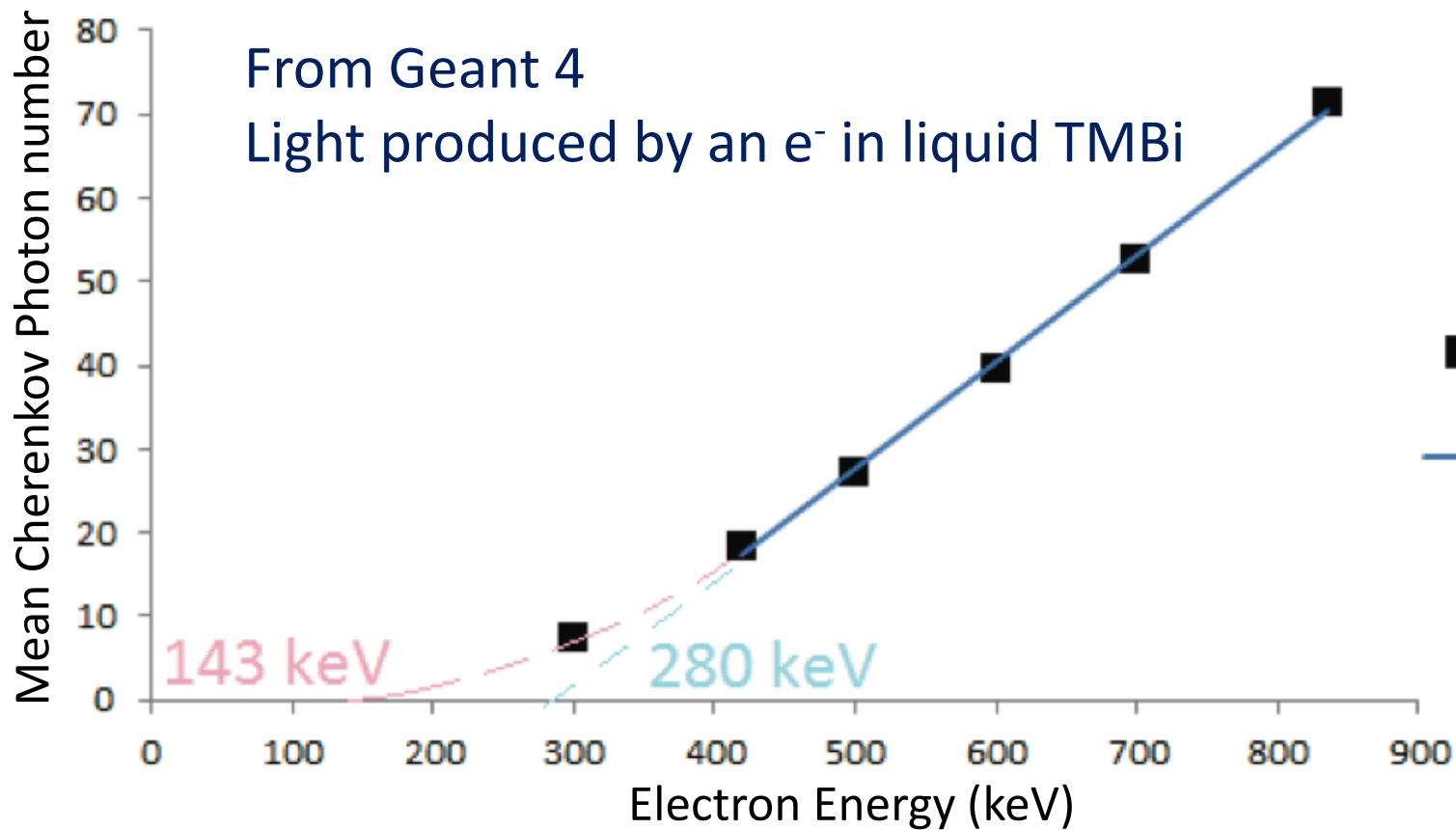
- Insensitive to the Depth Of Interaction effect
- Can be placed closer to the body
- Large gain in solid angle: **efficiency x ~ 4**

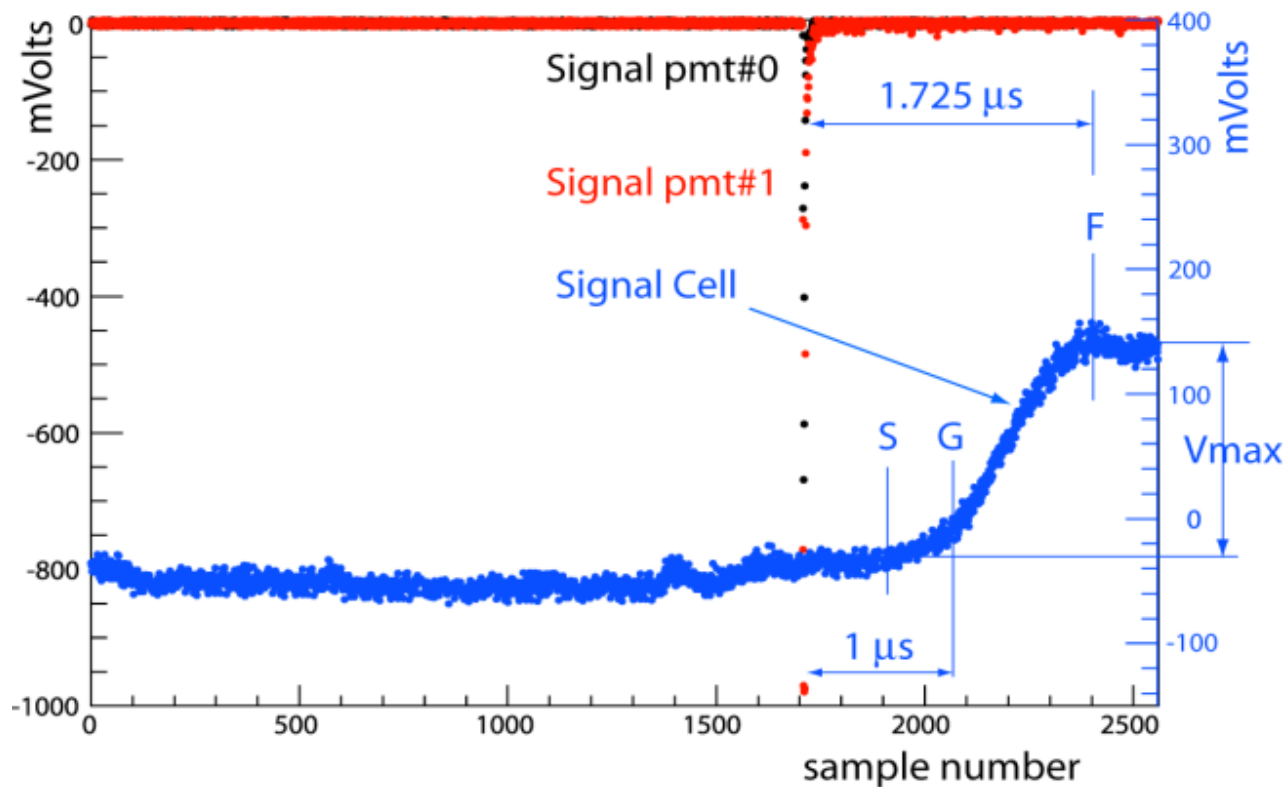
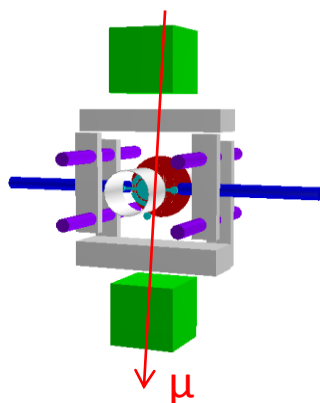


Time of Flight information enhances image contrast

- $G = (S/N_{\text{TOF}}) / (S/N_{\text{noTOF}}) = \alpha (2D / (c \delta t))^{1/2}$
- Δt Coincident Resolution Time, D typical organ size, $\alpha \sim 0.8$
- Brain ~ 20 cm, CRT of 150 ps (FWHM)
- $G \sim 2.4$, \Rightarrow Equivalent efficiency **gain of a factor of 5.7**

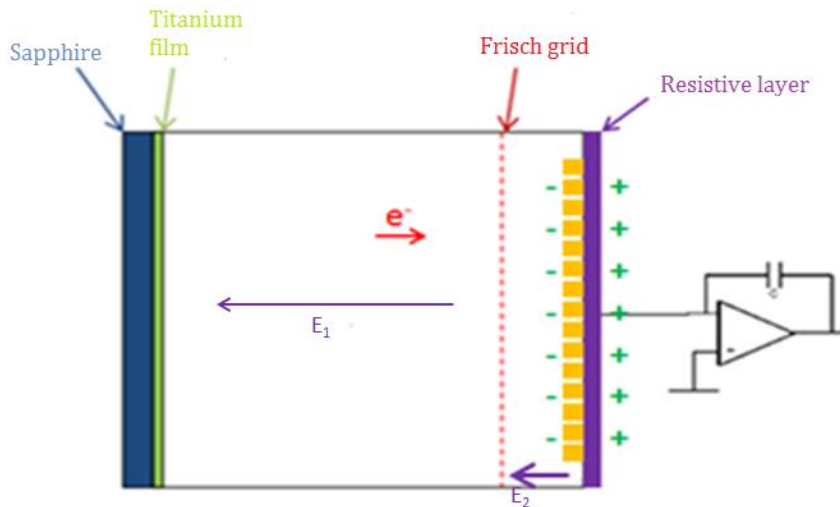
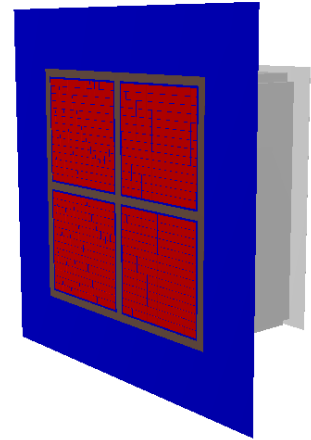




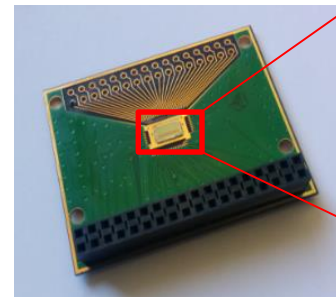


- Drift time = 725 ns = $\frac{\text{distance_anode}}{\text{drift speed}} = \frac{d}{\mu E}$

- No feedthrough
 - readout by capacitive coupling
 - Thin film deposits on alumine (IN2P3/CSNSM)
- Pixellized detector (1 mm²)
 - Low noise iDef-X multichannel ASIC electronics (CEA/IRFU)

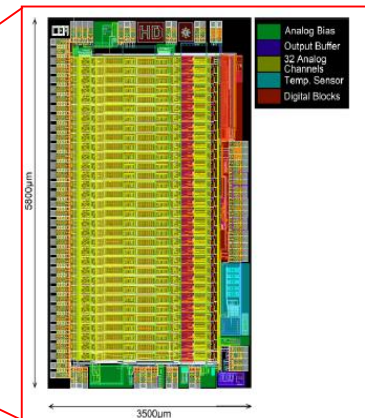


Capacitive readout principle



IDef-X chip

Pixelated detector



D. Attié and al.. Piggyback resistive Micromegas... JINST., 8 C11007, 2013.

O. Gevin and al.. IDef-X V1.0 : Performances of a New CMOS Multi Channel Analogue Readout ASIC for Cd(Zn)Te Detectors. Proc. IEEE NSS-MIC conf. rec, 2005.

Properties Detector	Atten Length (cm)	Coinc . PhotElecE Eff.(%)	Timing Resolution (ps, FWHM)	Energy Resolution (% FWHM)	G Interac. Postion. (mm)	End user friendly
LSO/LYSO	1.23	12	300 - 500	10	2 to 10	YES
LaBr ₃	2.3	1.9	100 - 300	3	4 to 10	YES
CdTe/CZT	2.0	2.2	slow	1- 3	0.1	YES
CaLIPSO	2.9	22	?150? - 380	10	0.15	Will be !

LSO/LYSO : The reference detector.

LaBr₃ : Excellent timing, poor PE Efficiency, fair positioning.

Only relevant for full body, Time of Flight PET config.

CdTe/CZT : Excellent position reconstruction, poor PE Efficiency.

Only relevant for single mouse PET imaging

CaLIPSO : Best PE efficiency, Excellent positioning, very good timing.

Take the best of all technologies – Needed for high-res efficient Brain PET