

Novel Imaging Systems for in vivo Monitoring and Quality Control during Tumour Ion Beam Therapy: An Introduction

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Outline

1. The upcoming FP7 call
2. What do we have? In-beam PET
3. What do we need?

1. The upcoming FP7 call

HEALTH-2008-1.2-4: Novel imaging systems for in vivo monitoring and quality control during tumour ion beam therapy.

Description: The focus should be to develop **novel imaging instruments**, methods and tools for monitoring, **in vivo** and preferably in **real time**, the **3-dimensional** distribution of the radiation dose effectively delivered within the patient during ion beam therapy of cancer.

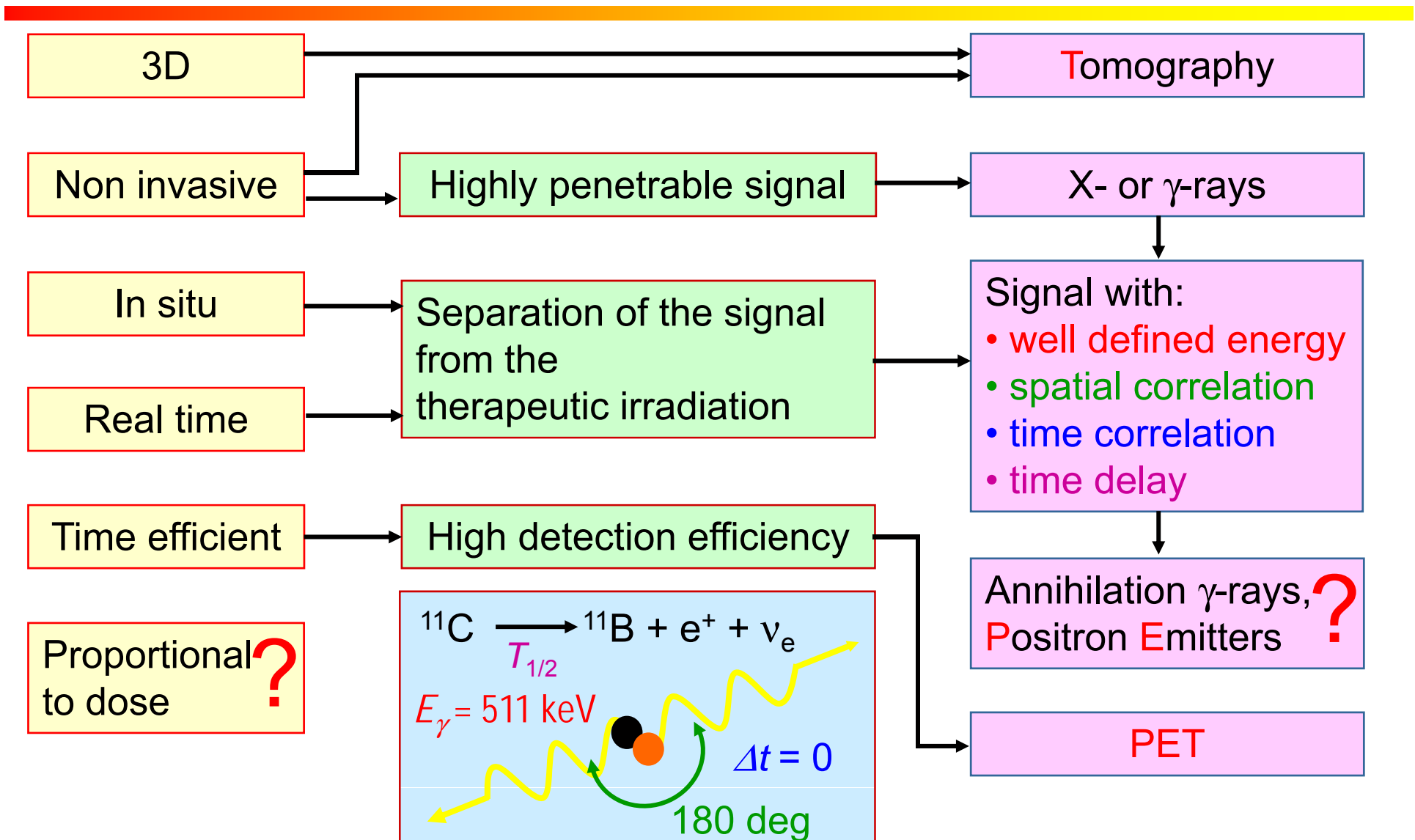
The ions should be **protons or heavier ions**.

The system should typically be able to **quantify the radiation dose delivered**, to **determine** the agreement between the **planned target volume** and the actually irradiated volume, and for **decreasing localisation uncertainties** between planned and effective positions (e.g. of tissues or organs), and between planned and effective dose distribution during irradiation.

It should aim at **improving quality assurance**, **increasing target site (tumour) to normal tissue dose ratio** and **better sparing normal tissue**.

2. What do we have? In-beam PET

Rationale



2. What do we have? In-beam PET Physics

Peripheral nucleus-nucleus-collisions, nuclear reactions (${}^AZ, xp, yn$), $\Delta\mathbf{p} \approx \mathbf{0}$

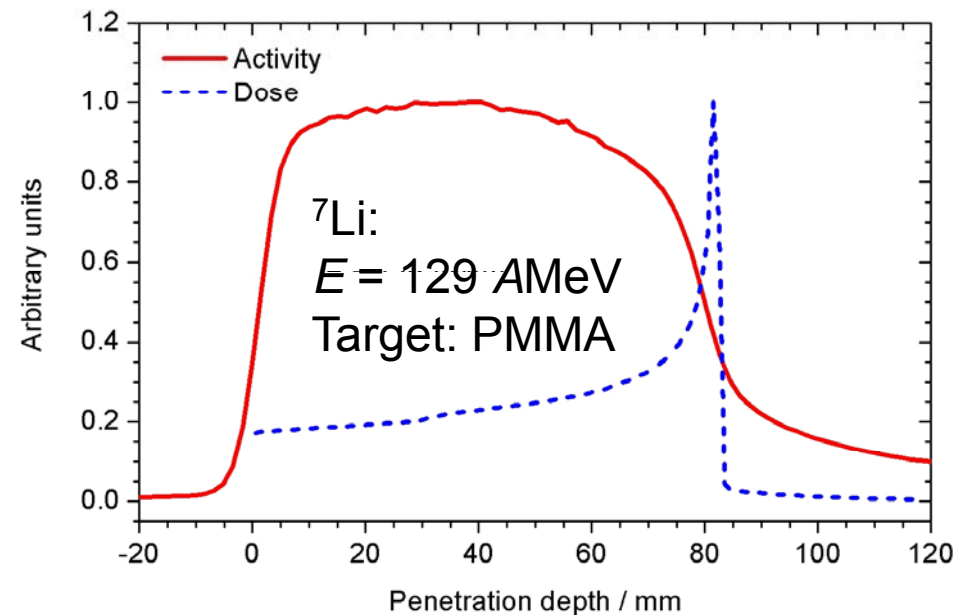
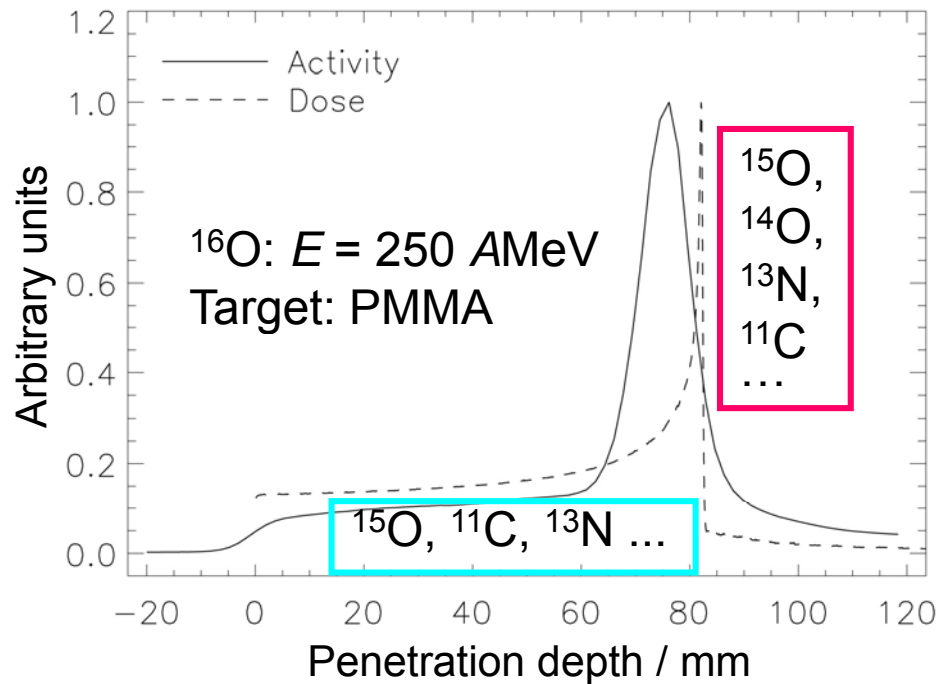
$Z \geq 6$

Projectile fragments

Target fragments

$Z < 6$

Target fragments



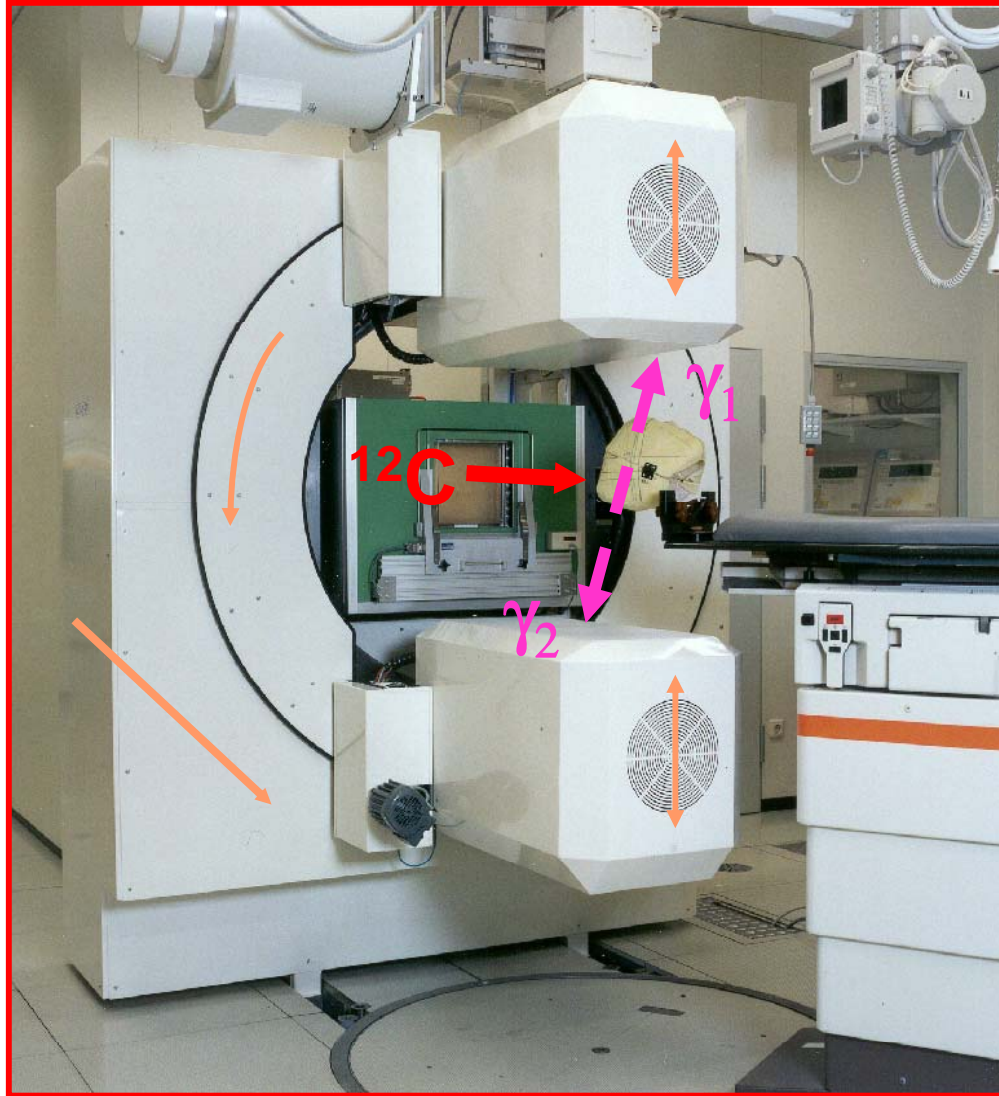
Therapy beam	${}^1\text{H}$	${}^3\text{He}$	${}^7\text{Li}$	${}^{12}\text{C}$	${}^{16}\text{O}$	Nuclear medicine
Activity density / $\text{Bq cm}^{-3} \text{ Gy}^{-1}$	6600	5300	3060	1600	1030	$10^4 - 10^5 \text{ Bq cm}^{-3}$

W. Enghardt et al.: Phys. Med. Biol. 37 (1992) 2127;
 K. Parodi et al.: IEEE T. Nucl. Sci. 52 (2005) 778;
 F. Sommerer et al.: Phys. Med. Biol. (to be published);

J. Pawelke et al.: IEEE T. Nucl. Sci. 44 (1997) 1492;
 F. Fiedler et. al.: IEEE T. Nucl. Sci., 53 (2006) 2252;
 M. Priegnitz et al.: Phys. Med. Biol. 53 (2008) 4443

2. What do we have? In-beam PET Instrumentation (I)

In-beam PET: ^{12}C -therapy at GSI Darmstadt



J. Pawelke et al.: Phys. Med. Biol. 41 (1996) 279
W. Enghardt et al.: Nucl. Instr. Meth. A525 (2004) 284



Off-beam PET: ^1H -therapy at MGH Boston

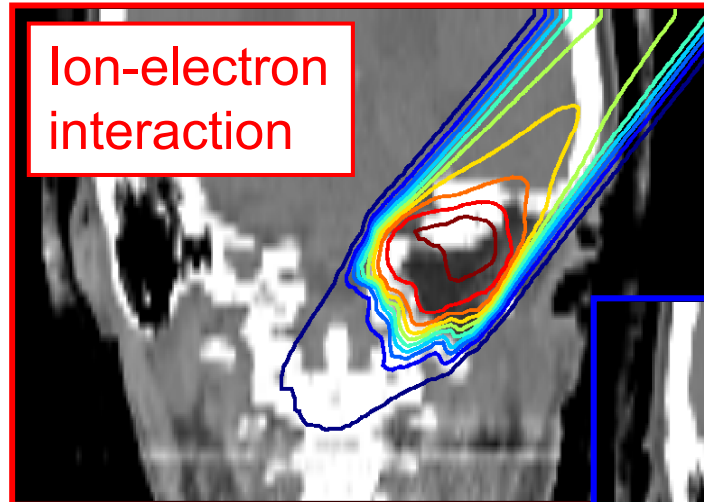
K. Parodi et al.:
J. Radiat. Oncol. Biol. Phys. 68 (2007) 920

2. What do we have? In-beam PET Instrumentation (II)

	In-beam	Off-line
Positron camera	Double head	Conventional ring PET/CT
Workflow	(1) Portal 1 + 40 s decay (2) Repositioning (< 5 min) (3) Portal 2 + 40 s decay ...	(1) Portals 1, 2, ... (2) Transfer to PET (15 min) (3) PET-scan (30 min)
Relevant isotopes	^{11}C (20 min), ^{10}C (19 s) ^{15}O (2 min) ... ^8B (0.8 s)	^{11}C (20 min),
Influence of metabolism	Low to medium	Strong
Quantitative PET	Difficult	Possible
Image correlation planning-CT – PET	Stereotactic coordinates	Additional CT (PET/CT)
Range measurements	Portal 1 (no restrictions) Portals 2 ... (difficult)	Impossible for opposing portals

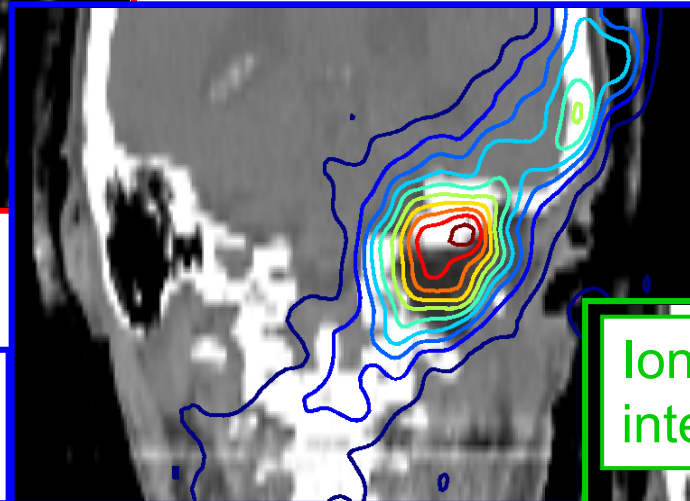
2. What do we have? In-beam PET

Clinical implementation (I)

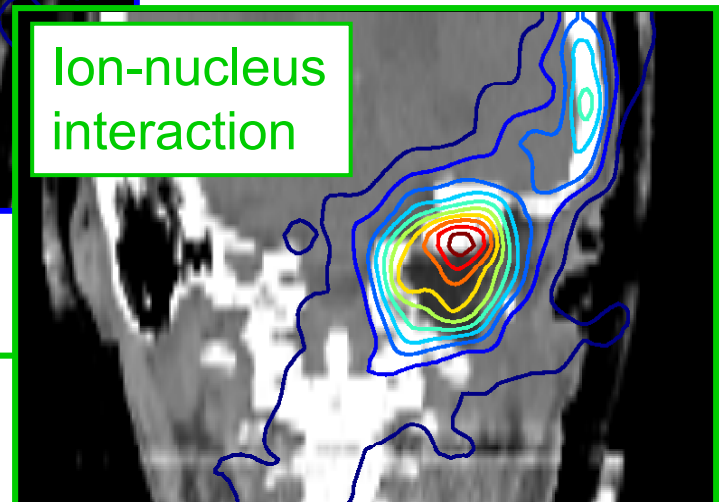


Treatment plan:
dose-distribution

Chordoma, 0.5 Gy, 6 min



β^+ -activity:
prediction



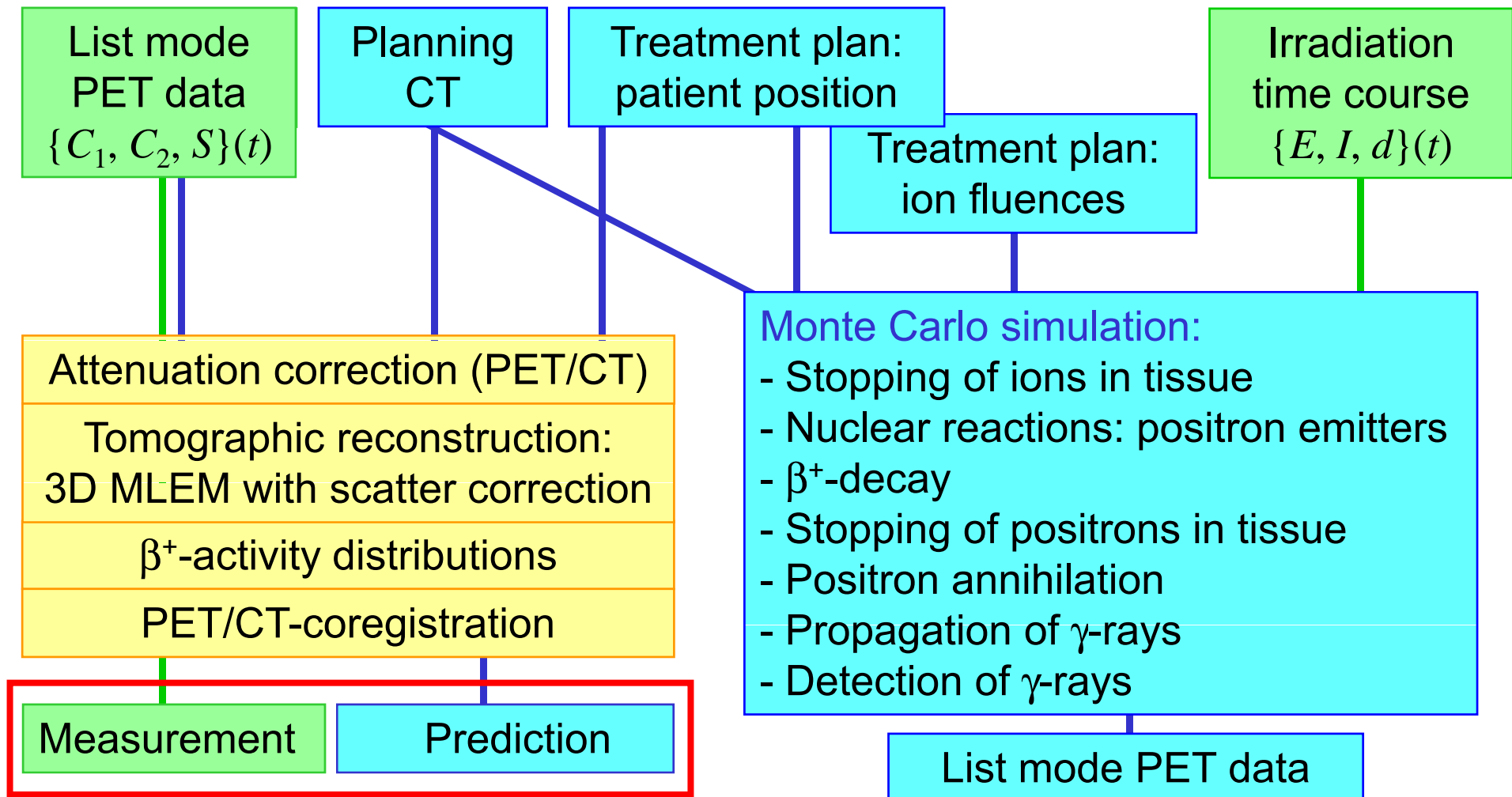
β^+ -activity:
measurement

W. Enghardt et al.:
Strahlenther. Onkol. 175/II (1999) 33;
F. Pönisch et al.:
Phys. Med. Biol. 48 (2003) 2419;
Phys. Med. Biol. 49 (2004) 5217

2. What do we have? In-beam PET

Clinical implementation (II)

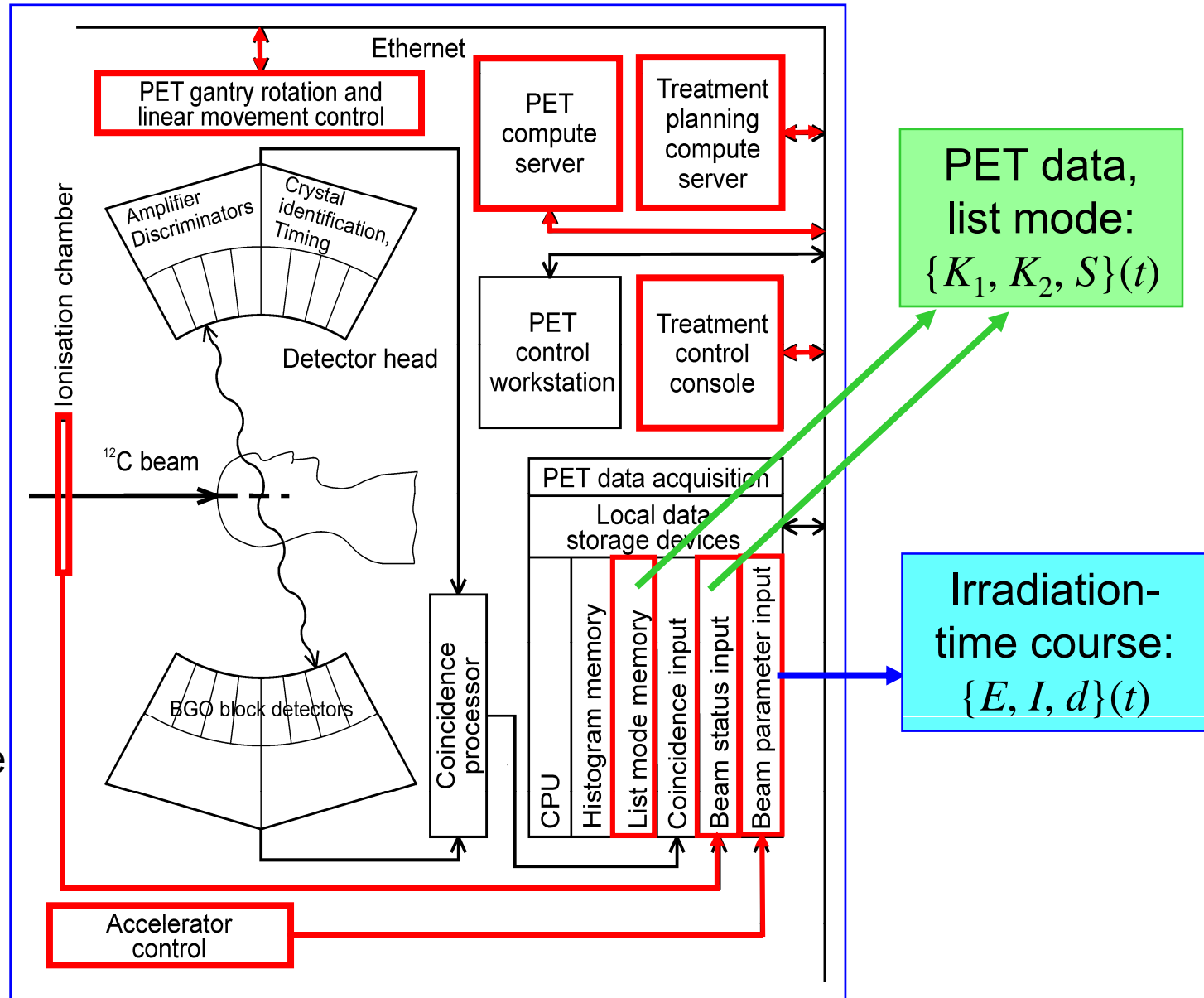
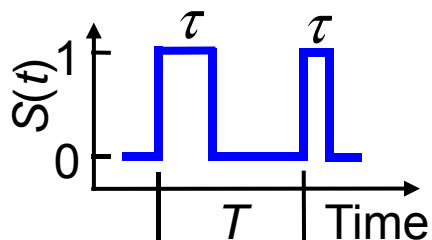
No proportionality between dose and activity: $A(\mathbf{r}) \neq D(\mathbf{r})$



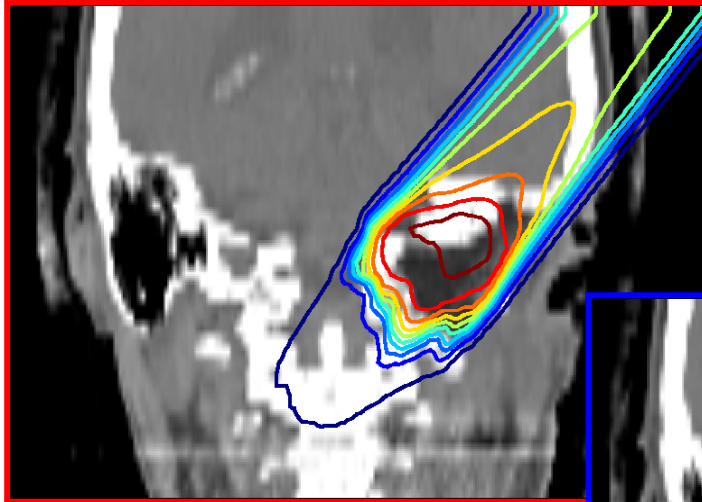
2. What do we have? In-beam PET Clinical implementation (III)

Accelerator:
Synchrotron
 $d \approx 60$ m

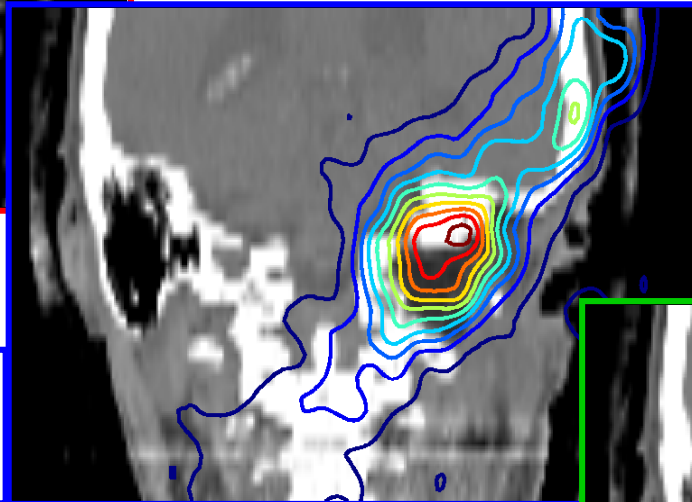
Particle beam:
pulsed
 $T \approx 5$ s, $\tau \leq 2$ s



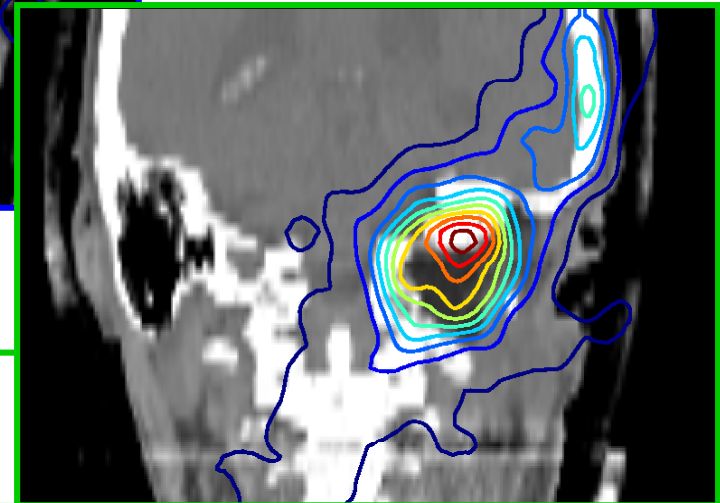
2. What do we have? In-beam PET Ion range verification



Treatment plan:
dose distribution



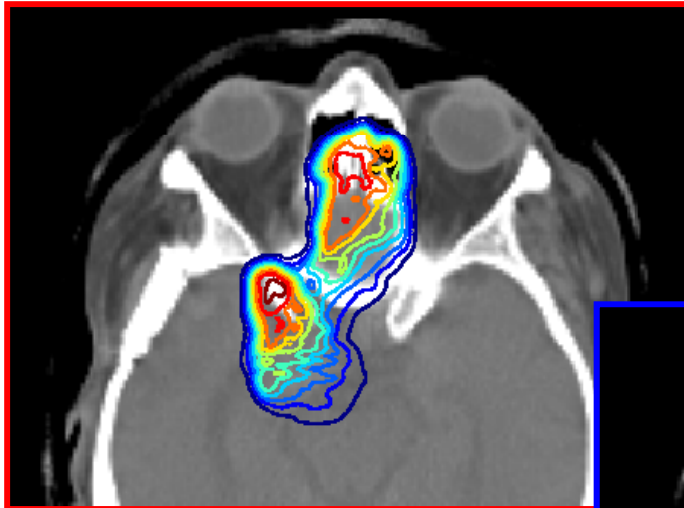
β^+ -activity:
prediction



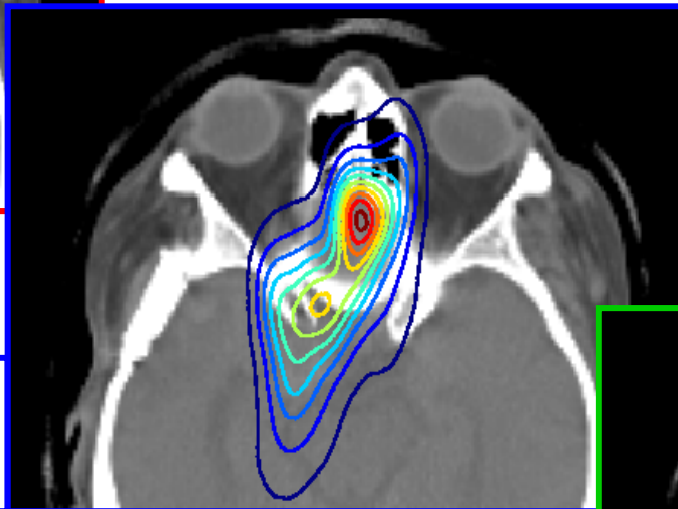
β^+ -activity:
measurement

2. What do we have? In-beam PET

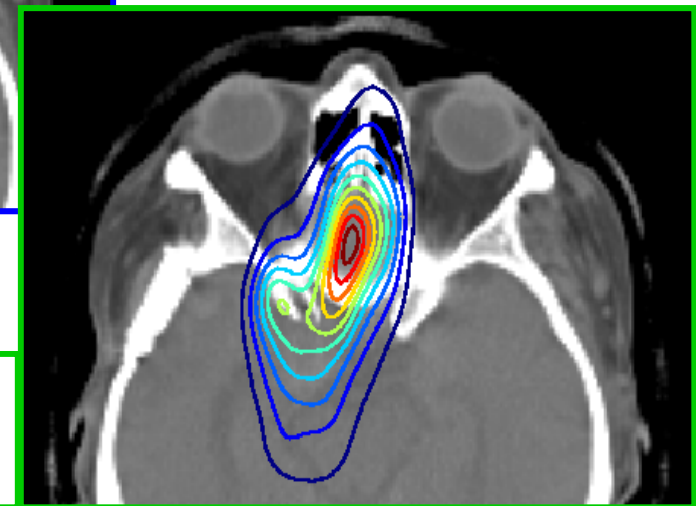
Field position verification



Treatment plan:
dose distribution



β^+ -activity:
prediction

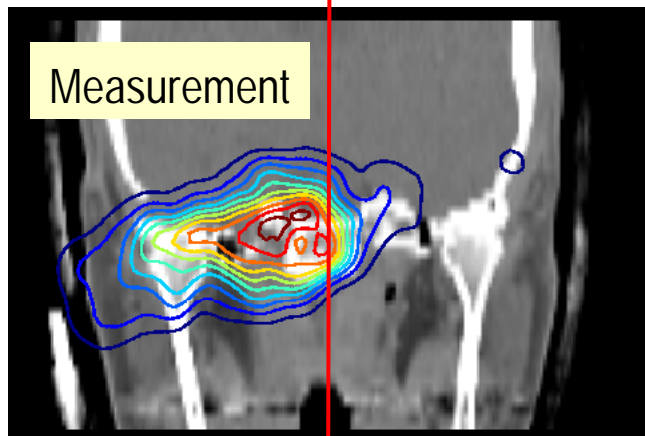
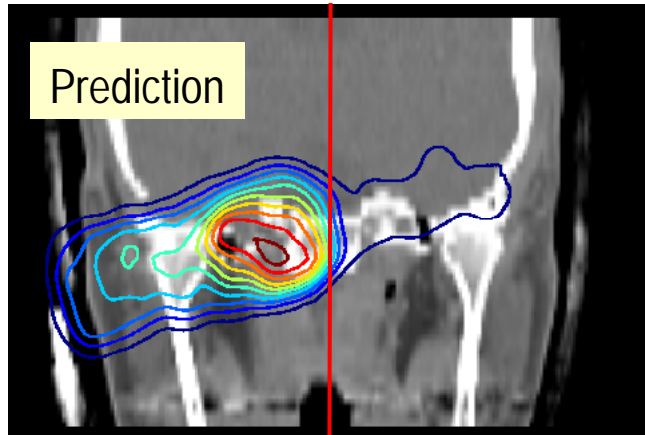


β^+ -activity:
measurement

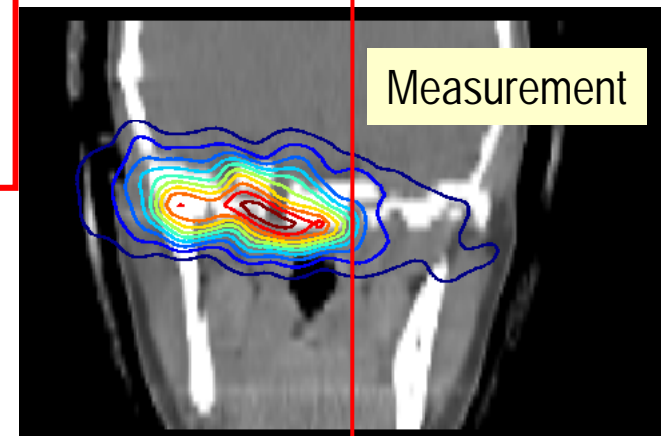
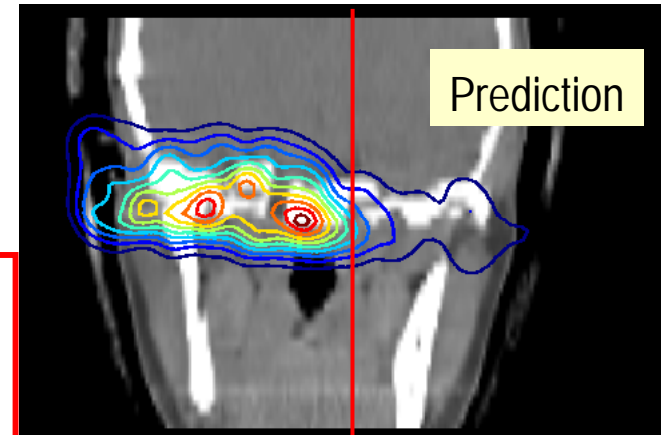
2. What do we have? In-beam PET

Physical beam model validation

1998



Since 1999



1. Precision measurements:

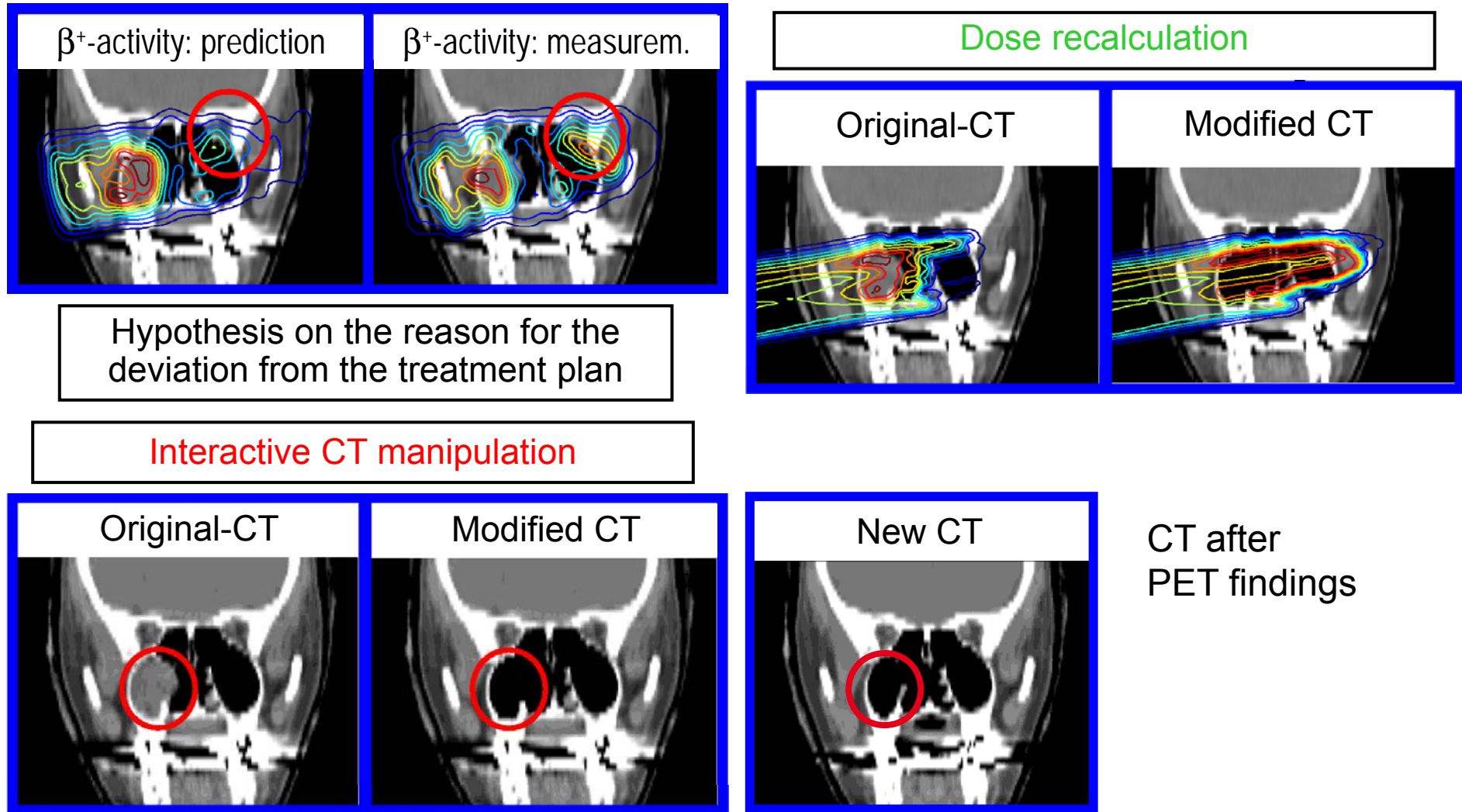
Range of
 ^{12}C -ions in tissue

2. Modification:

$$R = R(HU)$$

2. What do we have? In-beam PET

Estimation of dose delivery deviations



2. What do we have? In-beam PET

Estimation of dose delivery deviations

In-beam PET is not applicable to a precise dosimetry

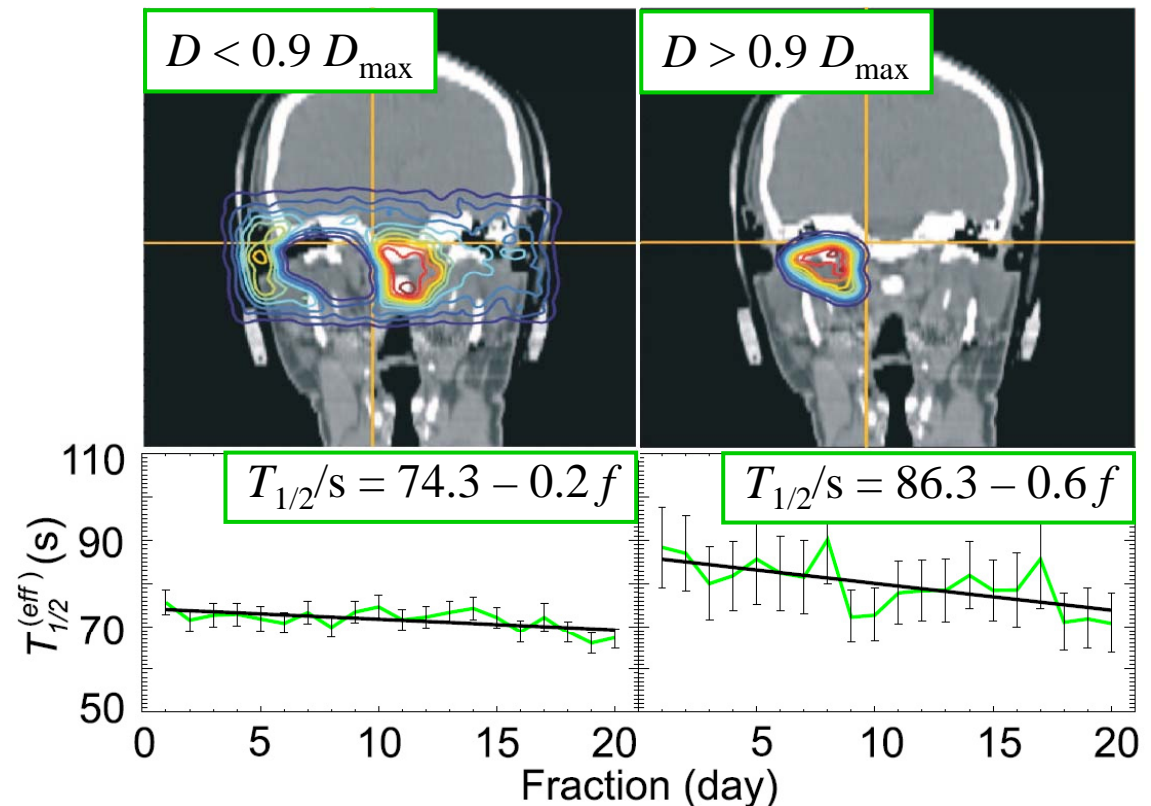
- it seems to be feasible to solve the inverse problem:

$$\mathbf{A}(\mathbf{r}) = \mathbf{T} \mathbf{D}(\mathbf{r})$$

$\mathbf{A}(\mathbf{r})$ – spatial distribution of activity
 $\mathbf{D}(\mathbf{r})$ – spatial distribution of dose
 \mathbf{T} – transition matrix

- it seems to be difficult to quantify the metabolic washout of β^+ -radioactivity
 - individual
 - tissue dependent
 - dose dependent
 - fraction dependent
 - disturbed by the tumour
- in-beam PET images are corrupted by limited angle artefacts (non-quantitative)

K. Parodi, T. Bortfeld:
Phys. Med. Biol. 51 (2006) 1991
K. Parodi et al.:
Med. Phys. 33 (2006) 1993
F. Fiedler et al.: Acta Oncol. 2007



2. What do we have? In-beam PET

Advantages

- PET allows for a
 - beam delivery independent,
 - simultaneous or close to therapy (in-beam, offline, resp.),
 - non-invasivecontrol of tumour irradiations by means of ion beams
- an in-vivo **measurement of the ion range**
- the validation of the physical model of the treatment planning
- the evaluation of the whole physical process of the treatment from planning to the dose application
 - new ion species
 - new components, algorithms
 - high precision irradiations
- the detection and estimation of unpredictable **deviations** between planned and actually applied dose distributions due to
 - mispositioning
 - anatomical changes
 - mistakes and incidents (www.rosis.info, spotlight on in-vivo dosimetry)

2. What do we have? In-beam PET

Disadvantages and open problems

PET is not applicable to

- real time monitoring:

- too slow
- $T_{1/2}(^{15}\text{O}) = 2 \text{ min}$, $T_{1/2}(^{11}\text{C}) = 20 \text{ min}$
- dose specific activity: $\sim 1000 - 7000 \text{ Bq cm}^{-3} \text{ Gy}^{-1}$

- quantitative imaging, precise dose quantification, feedback to treatment planning and to IGRT

- limited angle artefacts
- degradation of activity distributions by the metabolism
- degradation of activity distributions by moving organs
- inaccurate prediction of activity distributions from treatment planning due to unknown nuclear reaction cross sections

3. What do we need?

Aim of this FP7-project

- PET: clinical application reached, further development: industry
- Development and proof of principle of **really new** solutions for
 - **non-invasive, real-time, in-vivo monitoring**
 - **quantitative imaging**
 - **precise dose quantification**
 - **feedback to treatment planning**
 - **real-time feedback to IGRT for moving organs**
- Preserve the leading European position in the field

3. What do we need?

WP1: Time-of-flight in-beam PET

- Aim: Remove the influence of limited angle tomographic sampling to quantitative imaging
- Subtask 1.1.: Development of a demonstrator of an in-beam TOF positron camera:
 - $2\tau < 200$ ps
 - $\eta_{\text{singles}} > 50$ %
 - $\Delta x < 5$ mm
 - ⇒ detector technology
 - ⇒ DAQ
- Subtask 1.2.: Tomographic reconstruction and prediction of measured activity distributions from treatment planning
 - ⇒ real-time TOF reconstruction
 - ⇒ simulation TP → TOF IBPET (WP5)

3. What do we need?

WP2: In-beam single particle tomography (IBSPAT) (I)

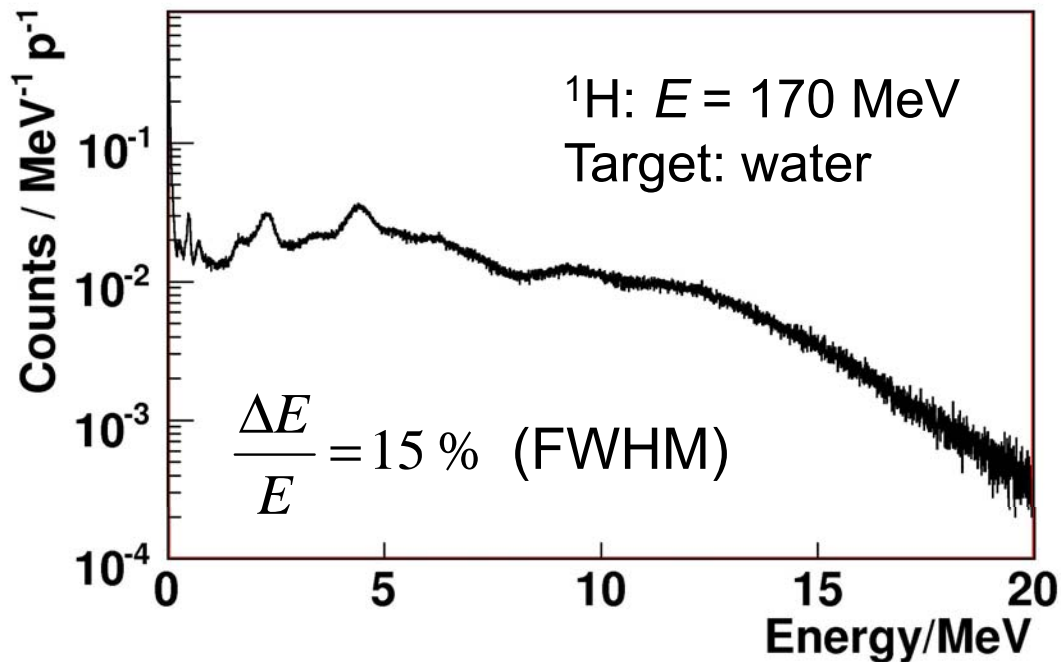
- Aim: Remove the influence of metabolism by detecting prompt nuclear reaction ejectiles (**photons**, neutrons, charged particles)
- Challenge: Signal acquisition during the huge background of therapy irradiation
- Subtask 2.1.: Development of a demonstrator of an in-beam single photon tomographic detection system (IBSPECT):
 - $\eta_{\text{singles}} > 10 \%$
 - $\Delta x < 5 \text{ mm}$
 - ⇒ detector technology (Anger camera, **Compton camera**: $\eta_{\text{CC}} \approx 100 \eta_{\text{AC}}$)
 - ⇒ discrimination of background radiation
 - ⇒ DAQ
 - ⇒ tomographic reconstruction (CC)
 - ⇒ simulation: TP → IBSPECT (WP5)
- Subtask 2.2.: Proof of principle of massive particle ($n, p \dots$) based in-vivo dosimetry
 - ⇒ simulation: TP → IBSPAT (WP5)
 - ⇒ decision on continuation

S. Chelikani et al.:
Phys. Med. Biol. 49 (2004) 1387

3. What do we need?

WP2: In-beam single particle tomography (IBSPAT) (II)

GEANT4: H₂O (p, γ) X



- photon/proton = 0.25
- $N_p > 10^9$
- $N_\gamma > 10^8$

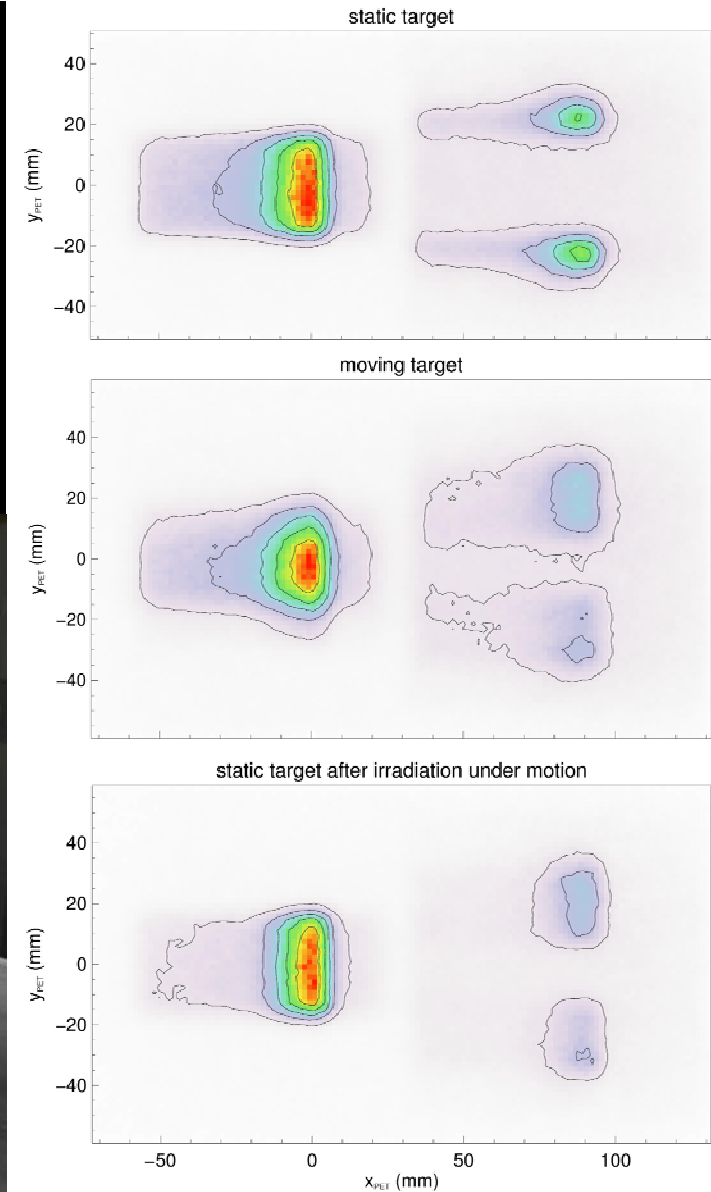
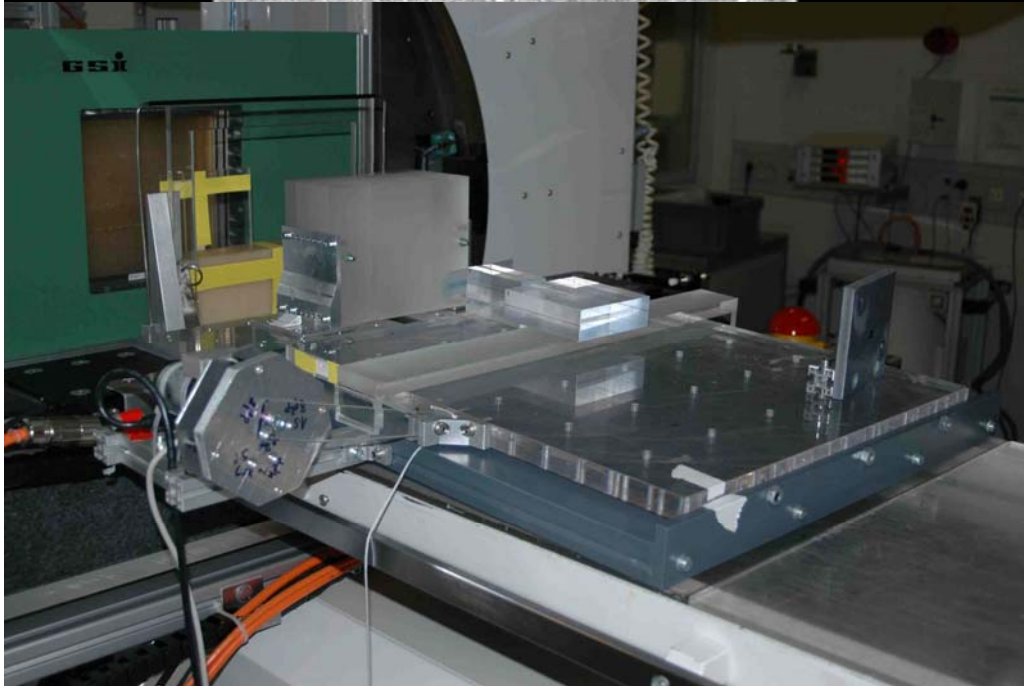
H. Müller:
www.fzd.de/FWK/MITARB/muellerh/G4/FF/index.htm

$$\frac{\Delta D}{D_{\max}} < 5\%$$

3. What do we need?

WP3: PT in-vivo dosimetry and moving organs (I)

C. Bert, C. Laube, K. Parodi. WE:
In-beam PET and ^{12}C -beam tracking. Experiment July 2008



3. What do we need?

WP3: PT in-vivo dosimetry and moving target volumes

- Aim: Establish in-vivo dosimetry methods for moving targets in combination with motion compensated beam delivery by gating and tracking
- Subtask 3.1.: Investigation of the potential of in-vivo dosimetry for irradiation of moving targets at the example of in-beam PET (GSI-facility)
 - ⇒ data acquisition schemes (4D IBPET)
 - ⇒ motion correction methods for 4D IBPET data
 - ⇒ time dependent simulation TP → 4D IBPET
- Subtask 3.2.: Extension of moving target methodology to the detection of single particles (feasibility study)
 - ⇒ influence of motion onto IBSPAT: simulation (WP5)
 - [⇒ data acquisition schemes (4D IBPET)
 - ⇒ motion correction methods for 4D IBPET data
 - ⇒ time dependent simulation TP → 4D IBPET (WP5)]

3. What do we need?

WP4: The combination of in-vivo dosimetry and treatment planning

- Aim: Development of fast and clinically applicable procedures for introducing in-vivo dosimetry results into adaptive treatment planning and beam delivery
- Subtask 4.1.: Development of **automatic** methods of identifying deviations between planned and actually delivered dose distributions:
 - ⇒ criteria for deviation detection (comparison with simulations)
 - ⇒ identification of reasons for deviations (patient mispositioning, anatomical reasons, incidents)
- Subtask 4.2.: Establishing the feedback between in-vivo dosimetry and treatment planning as well as beam delivery control:
 - fast
 - real time (IGRT), not feasible for IBPET
 - ⇒ methods of compensation (patient mispositioning, anatomical reasons, incidents)
 - ⇒ delivering information of deviation compensation to TP

3. What do we need?

WP5: Monte Carlo Simulation of in-vivo dosimetry

- Aim: Prediction of IBPET, IBSPECT, IBSPAT measurements from TP data for comparison with measured data
- Challenges: Dose prediction accuracy from in-vivo dosimetry data: $\Delta D/D_{\max} < 5\%$
Fast (reaction times of seconds)
- Subtask 5.1.: Development of fast and precise Monte Carlo tools for in-vivo dosimetry
 - ⇒ TP → TOF IBPET (WP1)
 - ⇒ TP → IBSPECT (WP2.1)
 - ⇒ TP → IBSPAT (WP2.2)
 - ⇒ TP → 4D IBPET, 4D IBSPAT, 4D IBSPECT (WP3.2)
- Subtask 5.2.: Compilation of basic physical data for the Monte Carlo tools of WP5.1:
 - ⇒ basis: experimental data, evaluated data bases
 - ⇒ generation of implicate data sets, e.g. yields
 - ⇒ concept for data to be measured (next EU-project)