

# Enhancing InBeam PET with single Photon (Compton) Detection

CERN September 2nd 2008

VALENCIA GROUP, **IFIMED**

José M. Benlloch (PET hardware, speaker)

José Bernabeu (Valencia project leader)

Carlos Lacasta (proponent of the concept)

Magdalena Rafecas (MC and reconstruction expert)

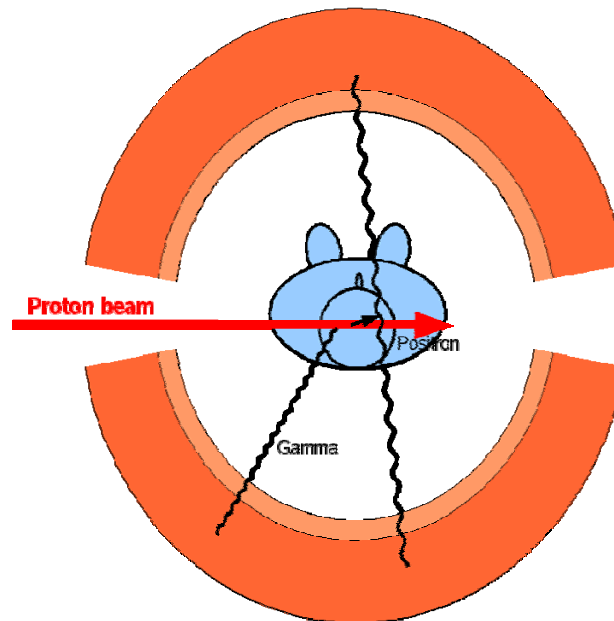


**IFIC**  
INSTITUTO DE FÍSICA CORPUSCULAR  
Centro Mixto CSIC – Universidad de Valencia



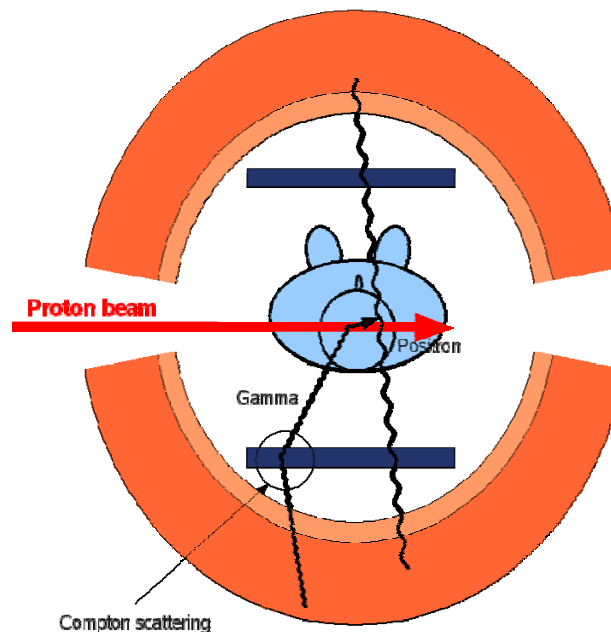
# Principle

- Current InBeam devices operate in PET mode
  - Only gammas from positron annihilation
- Being also sensitive to prompt gammas would increase the efficiency.



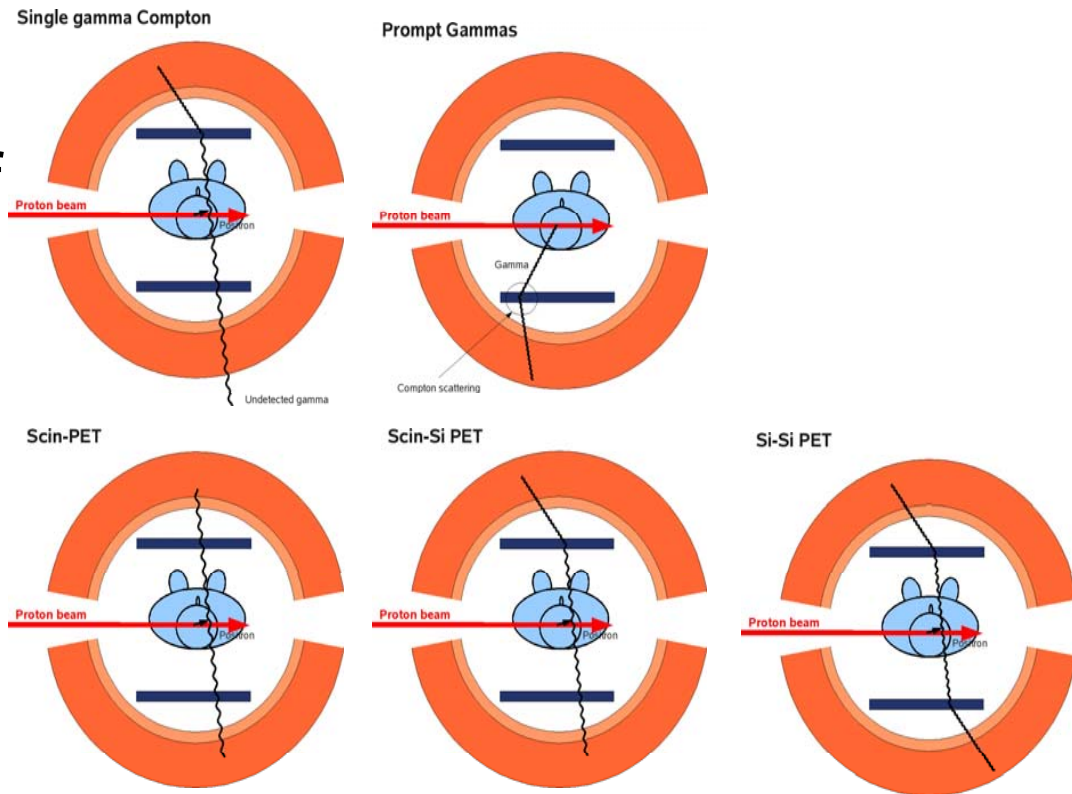
# The Compton PET

- We can augment the InBeam PET performance and efficiency by adding a scatterer in front of the PET scintillator.
- Our PET is now **also a Compton Camera**



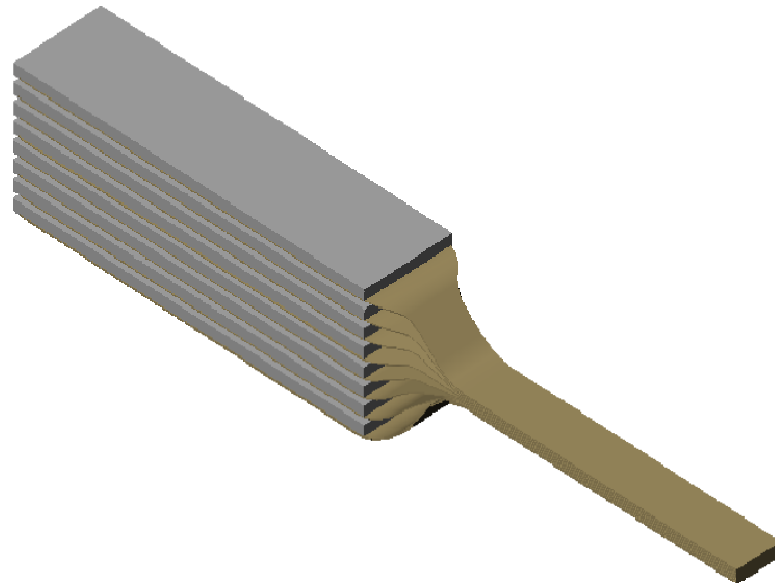
# The Compton PET

- Topologies
  - It can operate in PET mode with the combination of scatterer and scintillator
  - And also in single gamma mode.
- We certainly need some simulation to see the real gain



# The scatterer

- We propose a stack of silicon pad (big pixels 1x1 mm) sensors as building block for the scatterer.



# The scatterer

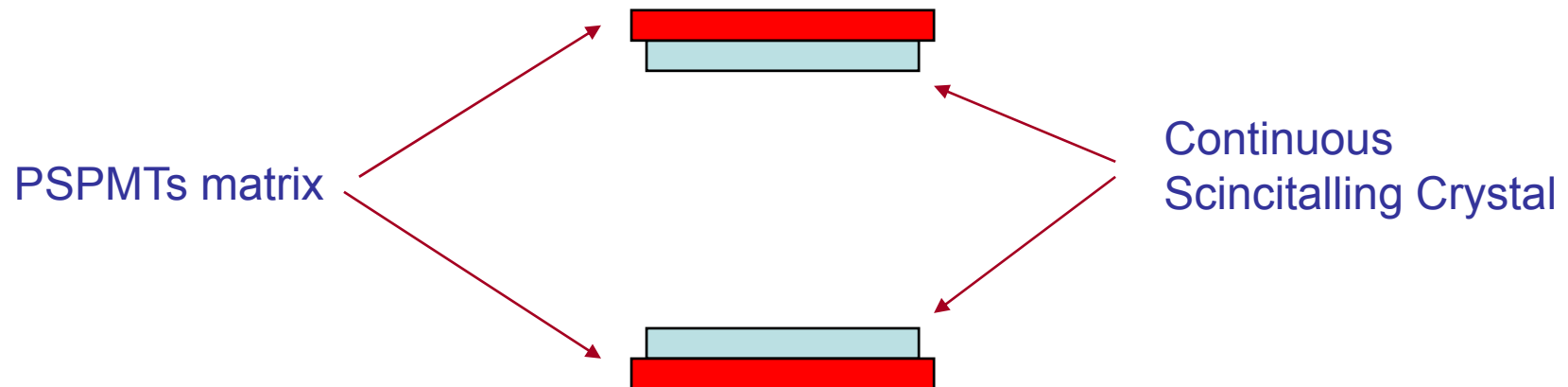
- Silicon is probably one of the best materials
  - Right Compton cross section
    - no absorption
    - Second Compton has low probability
  - Smallest tail produced by Doppler broadening compared to other materials
    - Only relevant for low energy photons (<300 keV)
- Mastered technology (detectors + r/o electronics) in High Energy Physics
- Some prototypes already built in Valencia for other applications

# The PET detector

FIRST APPROACH: 2 PANELS.

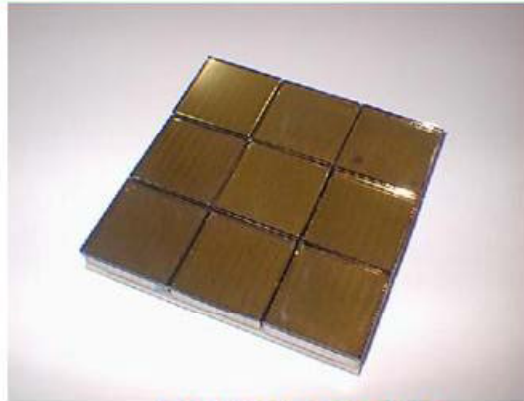
EACH PANNEL MADE OF:

- **FOTODETECTOR**: matrix of PSPMTs (HAMMAMATSU H8500).
- **CRYSTAL**: continuous scintillating crystal.



# The PSPMT matrix

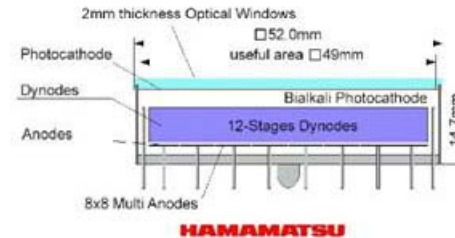
## Flat Panel PMT



**HAMAMATSU**

## Cross Section of Flat Panel PMT

PMT Type Number : R8400-M64  
Hybrid Assembly : H8500



Resistor network to reduce the number of channels to be digitized and to join several PSPMTs in a common readout.

9 x 9 PSPMTs will cover an area of about 16 x 16 cm<sup>2</sup>



# The Scintillating Crystal

Two options:

- **LSO.**

**Advantage:** higher stopping power.

**Disadvantage:** high intrinsic rate (cannot be used for triggering in single mode).

- **LnBr.**

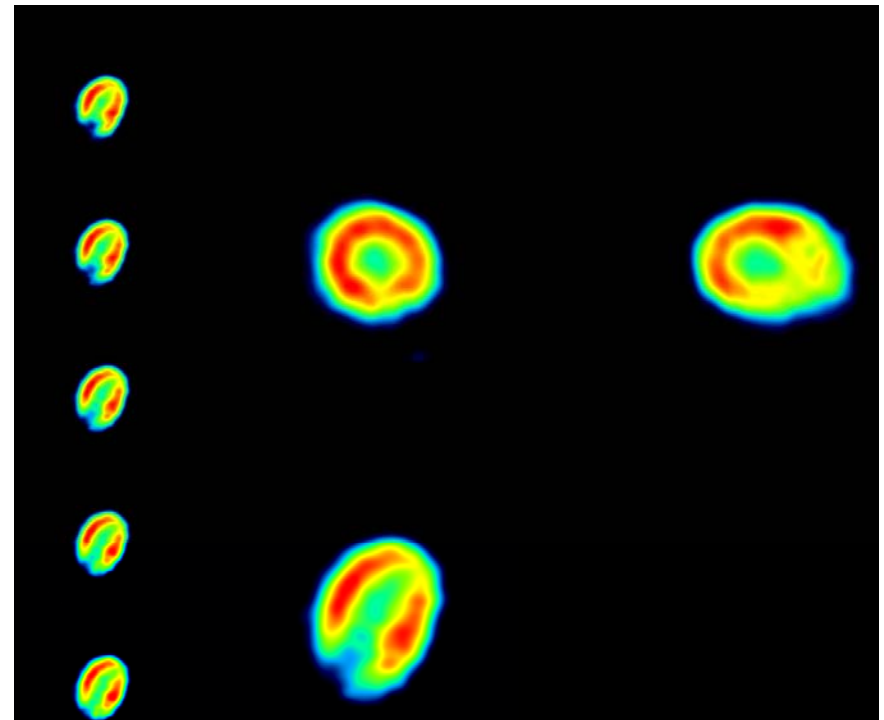
**Advantage:** fast and higher light yield (ideal for TOF-PET).

**Disadvantage:** currently still very expensive.

**We have also experience in building such PET technology.**

**Small animal PET**

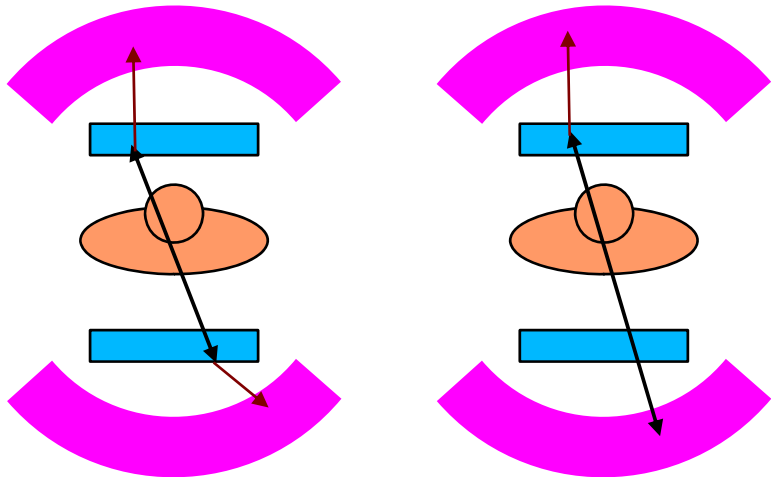
**Rat's Heart**



# Multichannel reconstruction

Goal: use and reconstruct all types of events

## High resolution channels

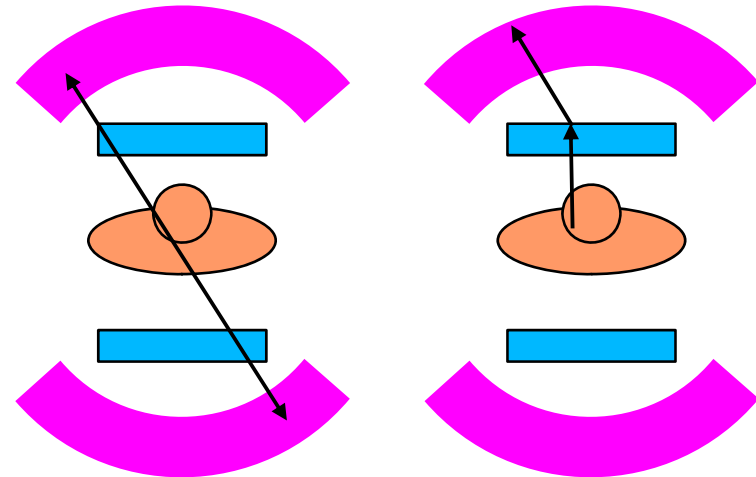


Si-Si

Si-Scintillator

Improve spatial resolution

## Low resolution channels



Scint.-Scint.

Single Compton

Improve sensitivity

# Multichannel reconstruction

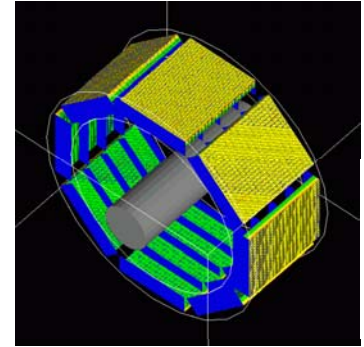
Dedicated reconstruction algorithms are needed

- Resolution channels considered in the system response matrix
- Dedicated modeling for each type of event
- Increased computational complexity

# Monte-Carlo simulations

## Goal:

- Optimization of system design
- Support modeling of physical response
- Evaluation of system performance and reconstruction algorithms



## Monte Carlo Simulation packages:

- Geant4
- GATE

## Resources:

- Grid infrastructure at IFIC
- PC Clusters



# Questions

- How much space do we have for PET and Compton PET?.
- How many prototypes in the project?
  - Only 1: Enhanced TOF-PET with Compton.
  - 2 prototypes: TOF-PET and enhanced PET.