

# Design Options of a 3-T 900-mm Whole Body MRI Magnet with Selected Commercial MgB<sub>2</sub> Wires

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## Abstract

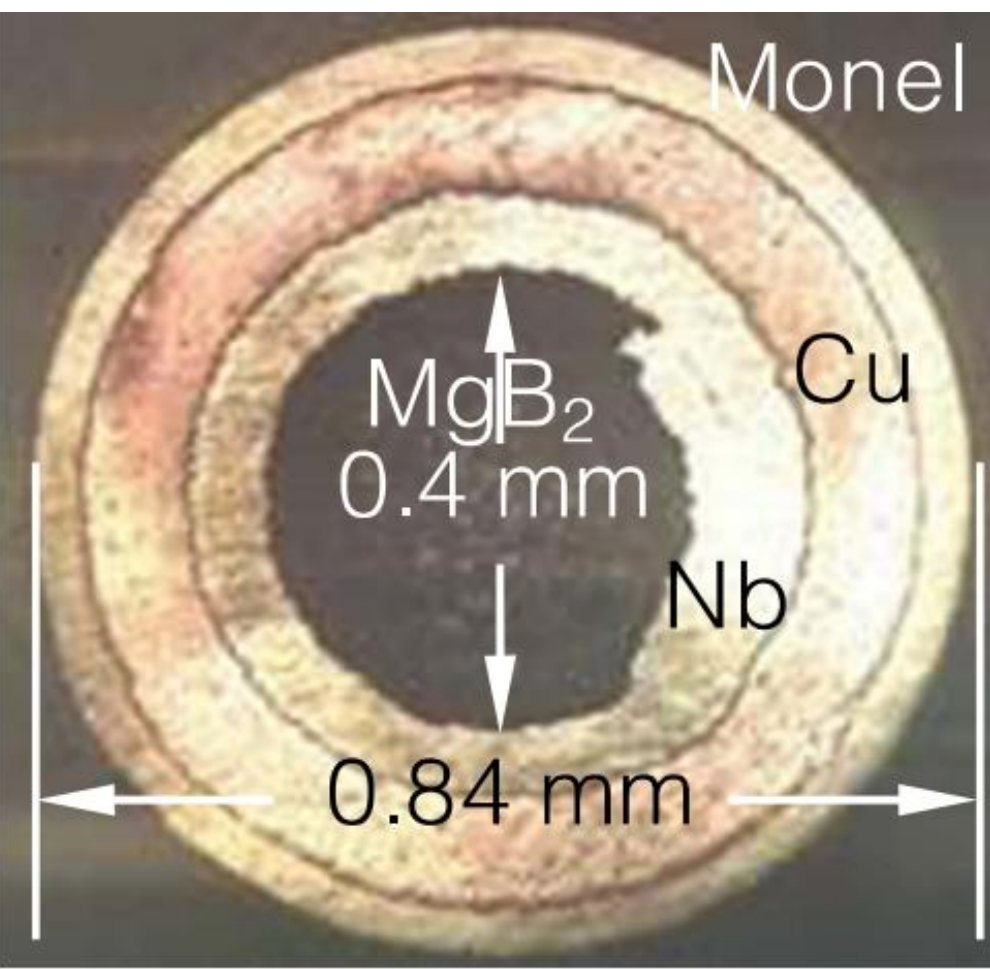
As the global helium crisis continues, the need for liquid-helium-free superconducting magnets continuously increases in the commercial sector of magnetic resonance imaging (MRI) systems. However, the conventional low temperature superconductor (LTS) magnets frequently experience unpredictable premature quenches, resulting in the extra usage of liquid helium before an MRI machine is delivered to its user site. The MgB<sub>2</sub> technology is expected to play an increasingly prominent role in the “next generation”, mainly because of a greater thermal stability of the wires than that of their LTS counterparts, making them essentially immune to the premature quench, as well as with their liquid helium (LHe)-free feature. To date, MgB<sub>2</sub> wires have been routinely produced by a few companies, such as Kiswire Advanced Technology that recently embarked on a collaborative R&D project with Korea University to design, construct, and operate an MgB<sub>2</sub> MRI magnet. This study presents the design options of a 3-T/900 mm MRI magnet employing selected commercial MgB<sub>2</sub> wires with a focus on: (1) conductor design and in-field performance; (2) coil volume and stray field; (3) mechanical stress and its tolerance; (4) cryogenic stability in various conductor options; (5) post-quench behavior and protection; and (6) field inhomogeneity due to manufacturing uncertainties of conductors.

## Results & discussion

### ★ MgB<sub>2</sub> wire

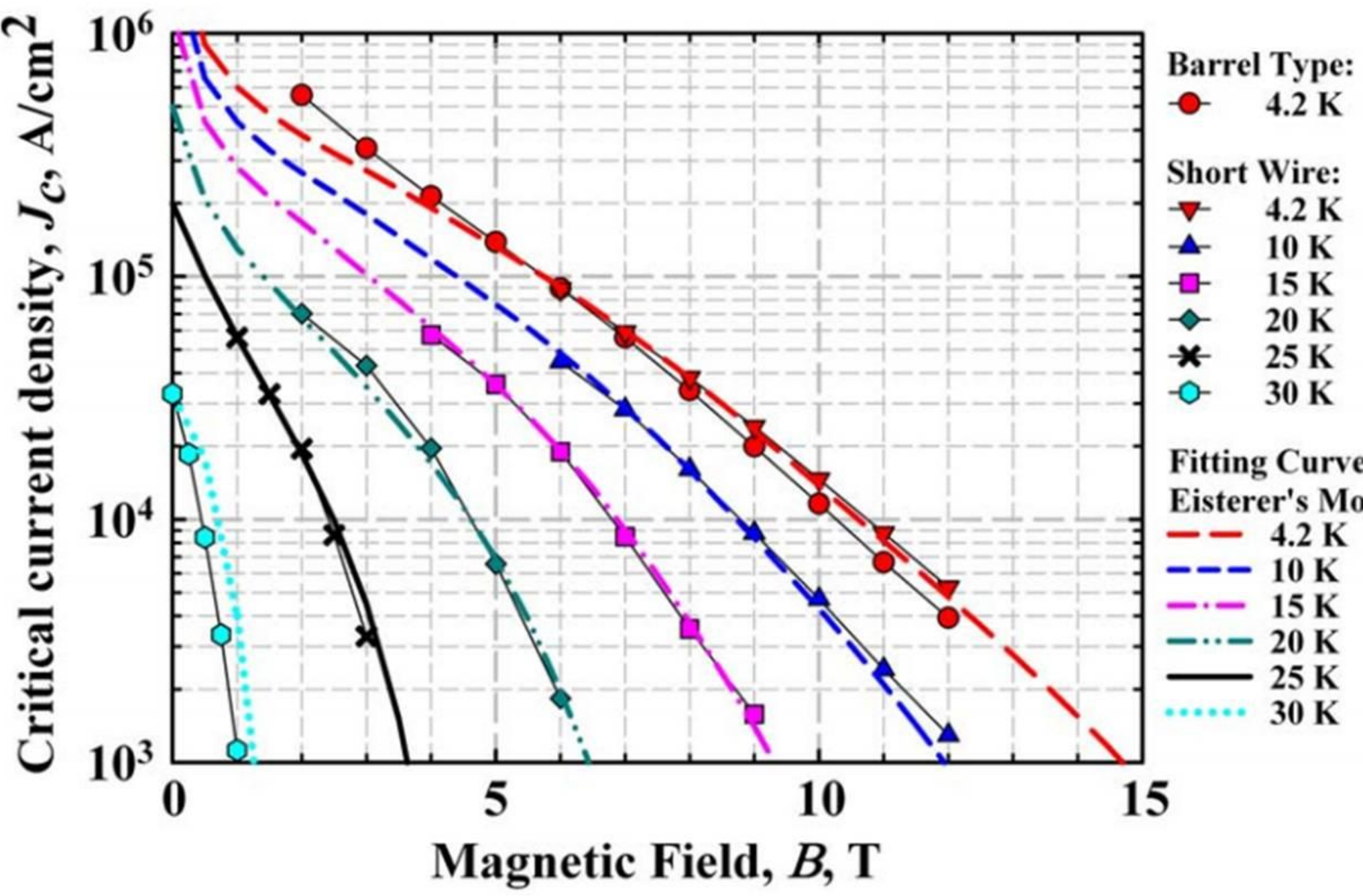
< Specifications of the MgB<sub>2</sub> wire used in this study >

Parameters	Values
Manufacturer	Hyper Tech Research Inc.
No. of filament	24
Barrier material	Nb
Sheath material	Monel
Dopant material	C
Insulation material	S-glass
Diameter of wire	[mm] 0.83 (w/o insulation) 1 (with insulation)
SC/non-SC ratio	[%] 11.7



< Photograph of the cross-section of the MgB<sub>2</sub> wire >

REF: Li et. al., Transport Critical Current Densities and n-Values of Multifilamentary MgB<sub>2</sub> Wires at Various Temperatures and Magnetic Fields, *IEEE Trans. Appl. Supercond.*, Vol. 24, No. 3, 6200105 (2014).



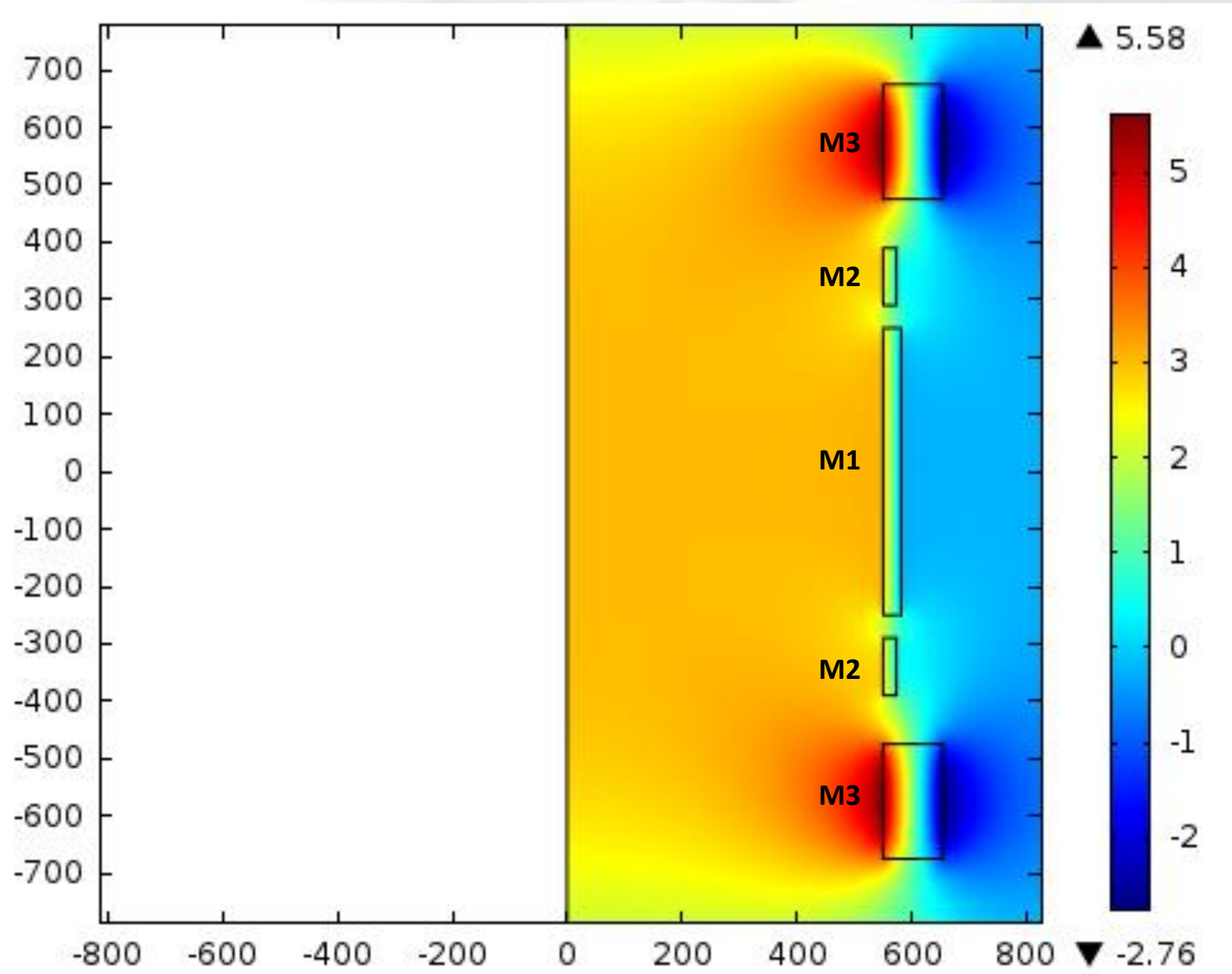
< Critical current density of the MgB<sub>2</sub> wire with respect to the magnetic field obtained at various temperatures >

REF: Li et. al., Transport Critical Current Densities and n-Values of Multifilamentary MgB<sub>2</sub> Wires at Various Temperatures and Magnetic Fields, *IEEE Trans. Appl. Supercond.*, Vol. 24, No. 3, 6200105 (2014).

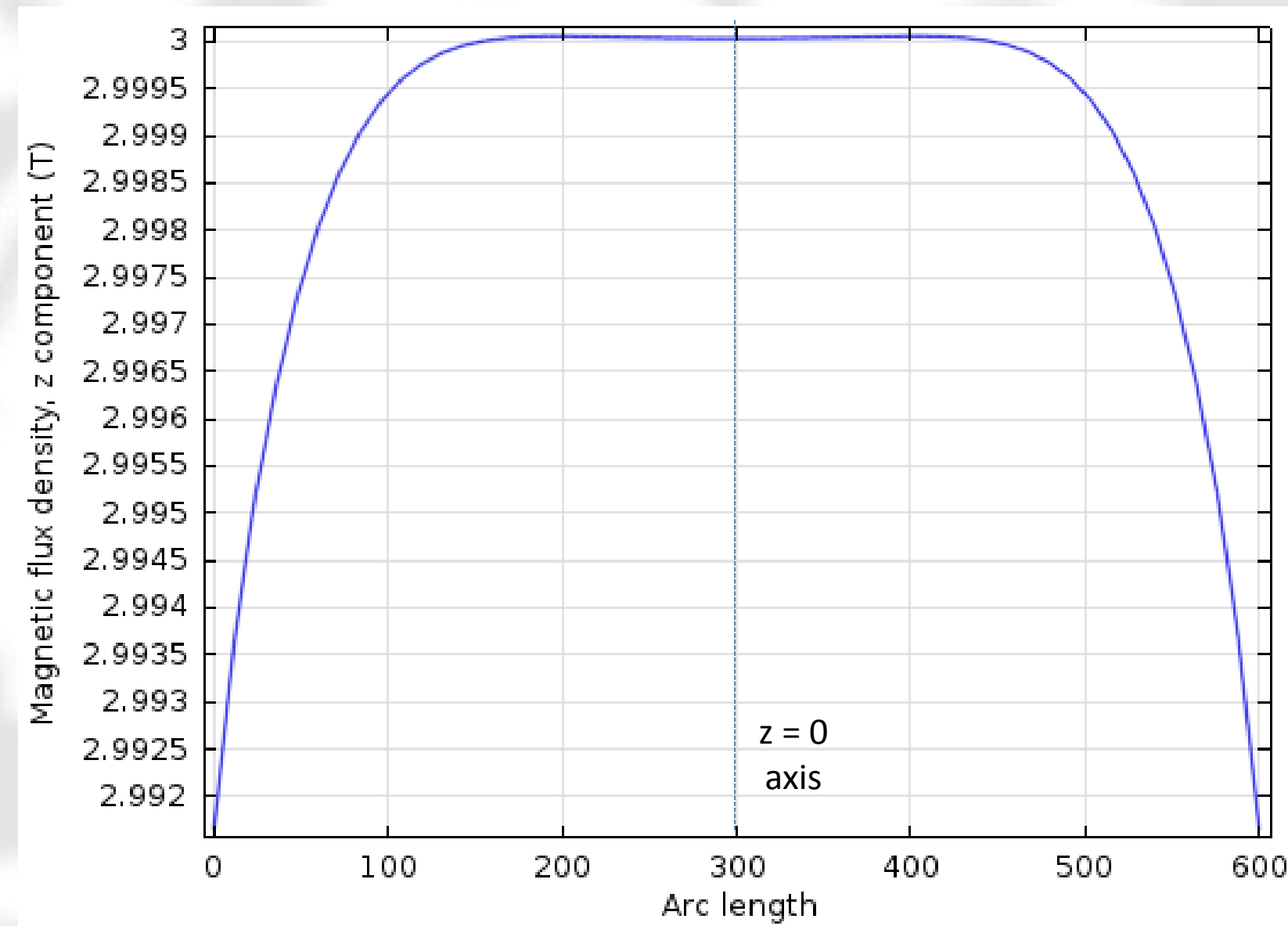
### ★ Electromagnetic design

< 1<sup>st</sup>-cut design parameters of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >

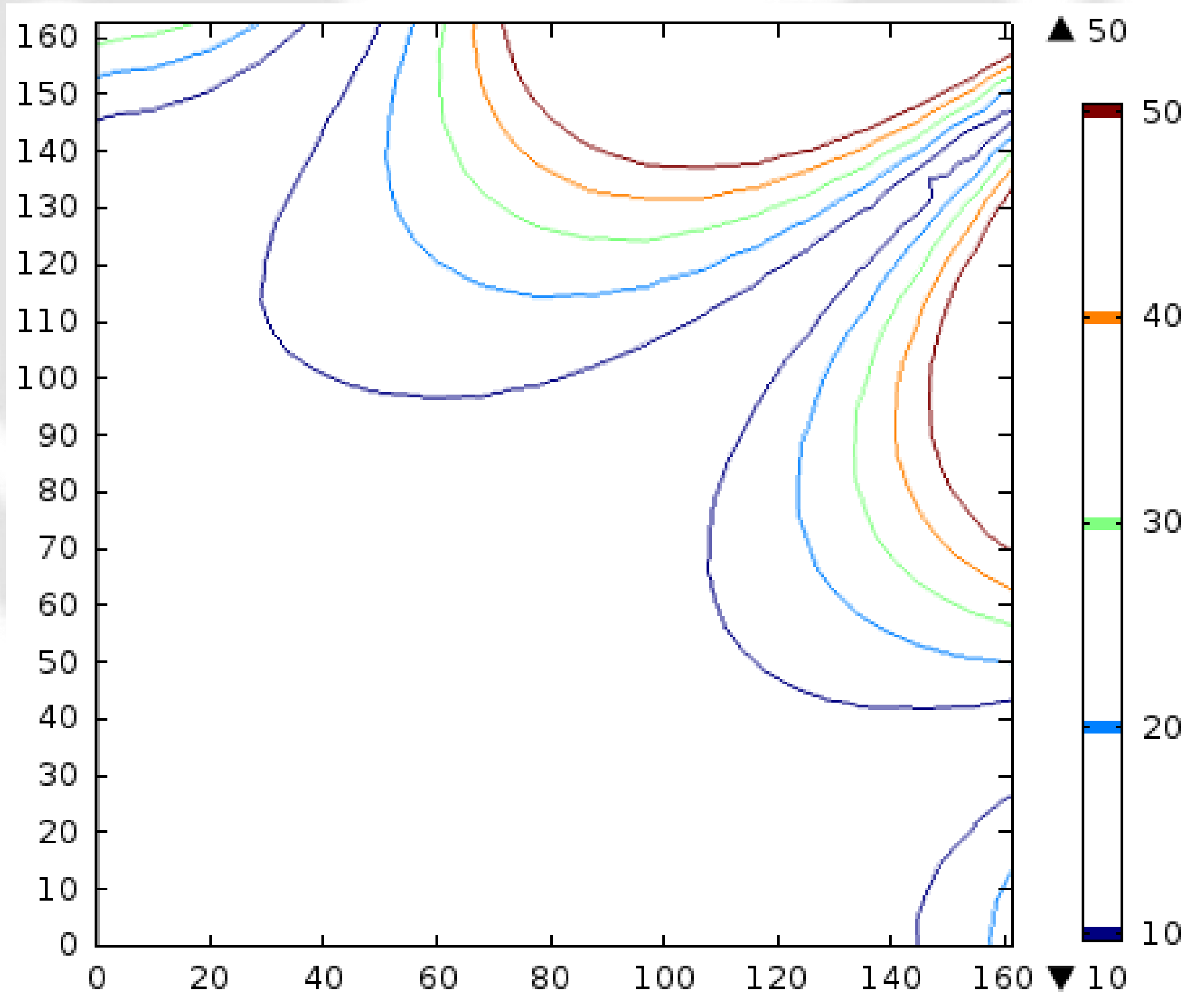
Parameters	M1	M2	M3
<b>Magnet</b>			
Inner diameter	[mm]	1100	
Outer diameter	[mm]	1147.03	1309.85
Height	[mm]	100	200
Total height	[mm]	1349	
Number of coil	[mm]	2	2
Turns/layer		500	200
Layers		36	121
Conductor length per coil	[km]	63.97	91.61
<b>Operation</b>			
Center field	[T]	3.0000	
Operating current	[A]	67.442	
Operating temperature	[K]	10	
Stored energy	[MJ]	9.41	
Field error at 30-cm DSV	[ppm]	< 20 (before shimming)	



< Magnetic flux density distributions of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >

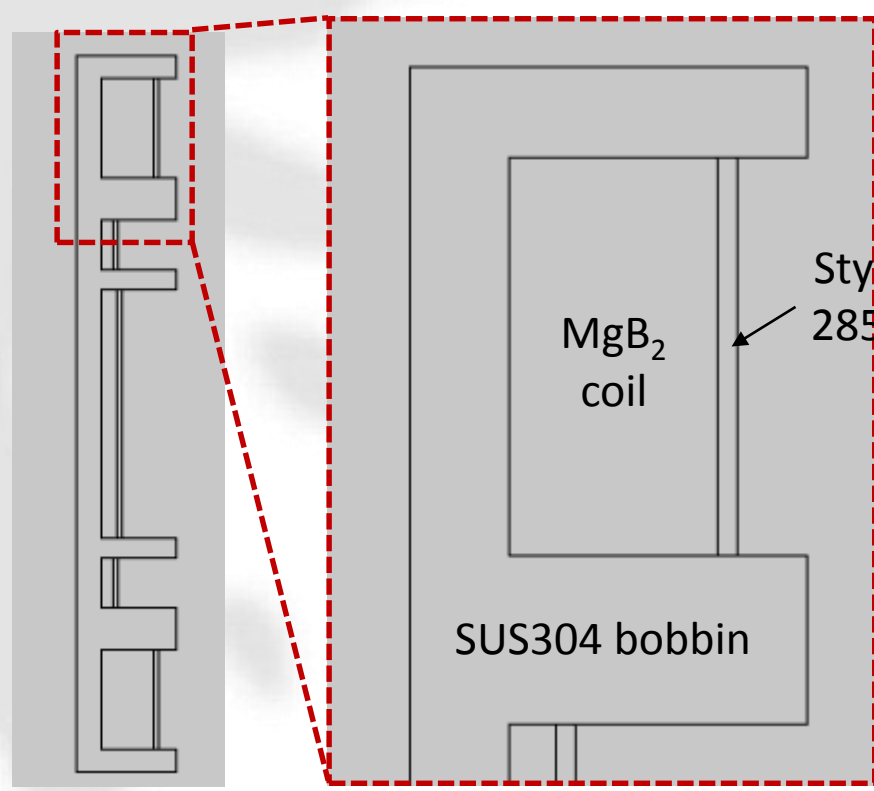


< Magnetic flux density distributions of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet along the z-axis >

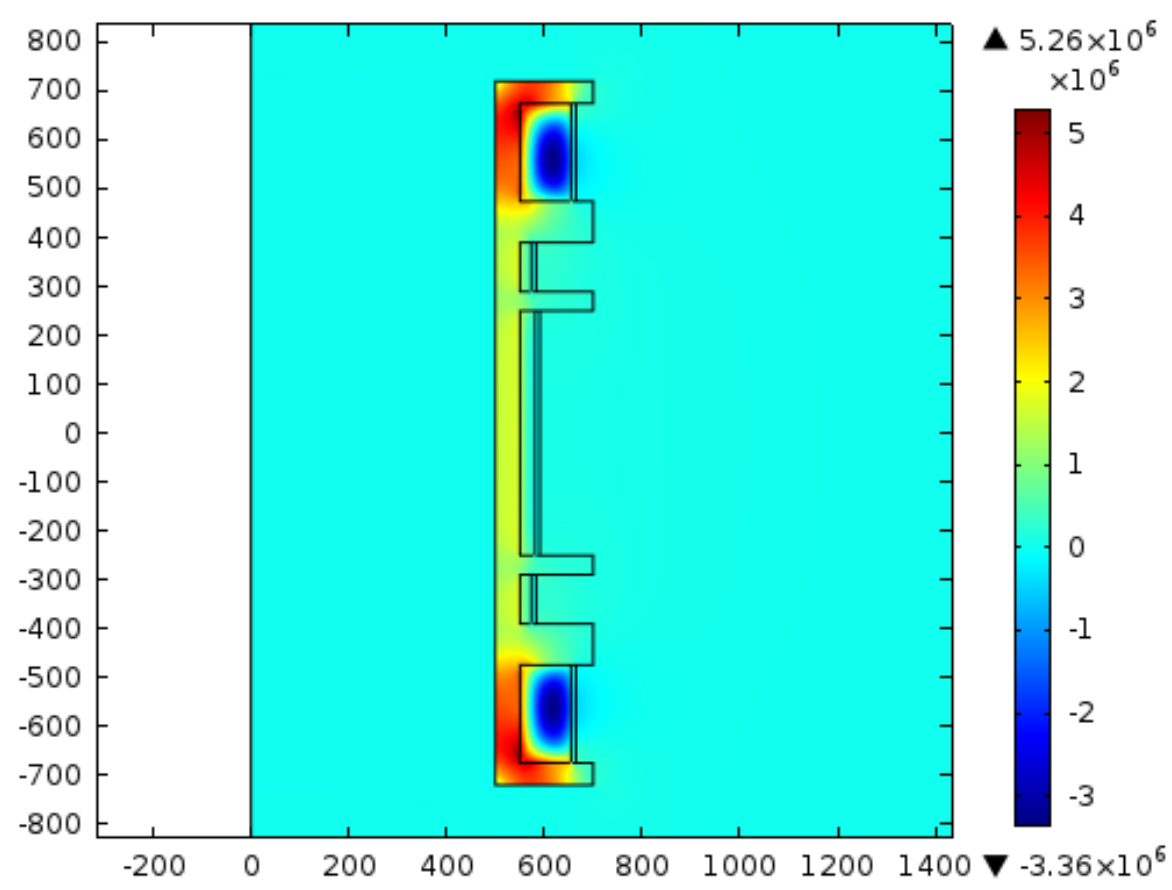


< Spatial field homogeneity distribution of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >

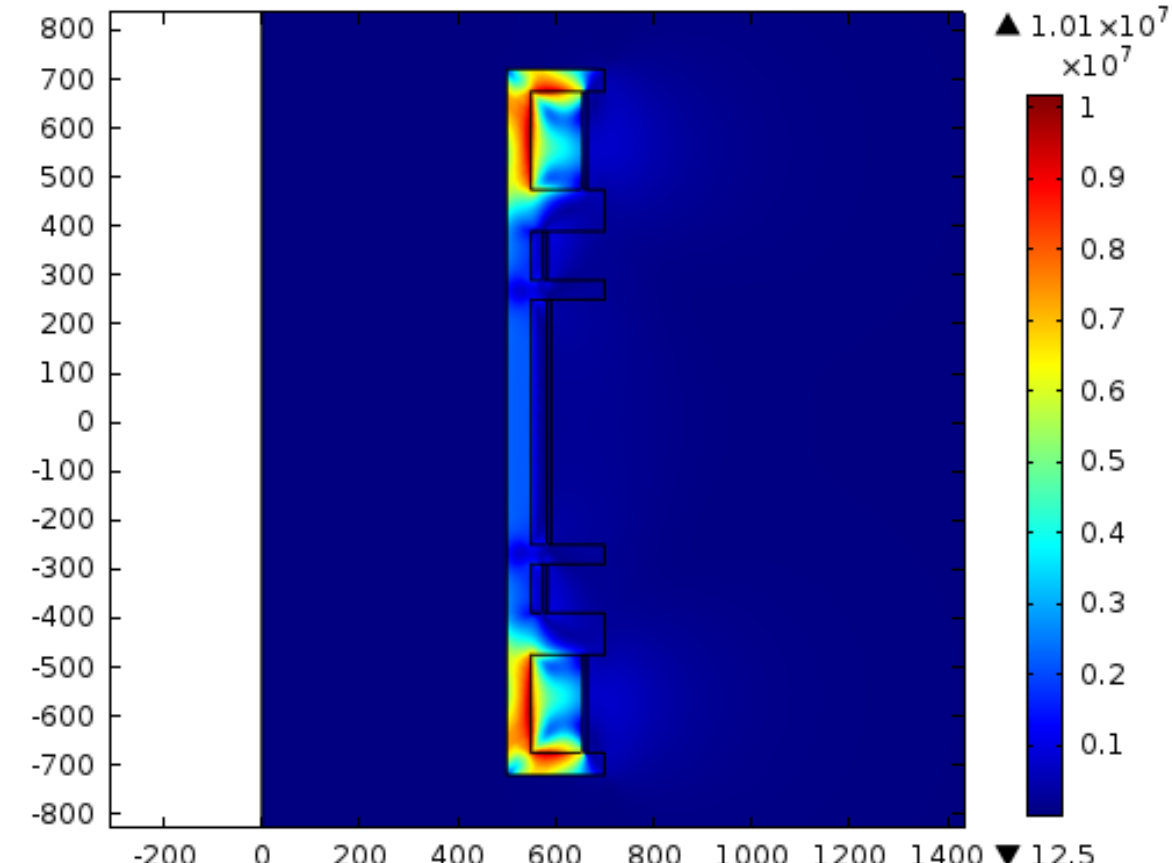
### ★ Stress-strain analysis



< Schematic drawing of a rigid body model for the stress-strain analysis of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >



< Stress tensor (phi component) distribution of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >



< Von Mises stress distribution of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet >

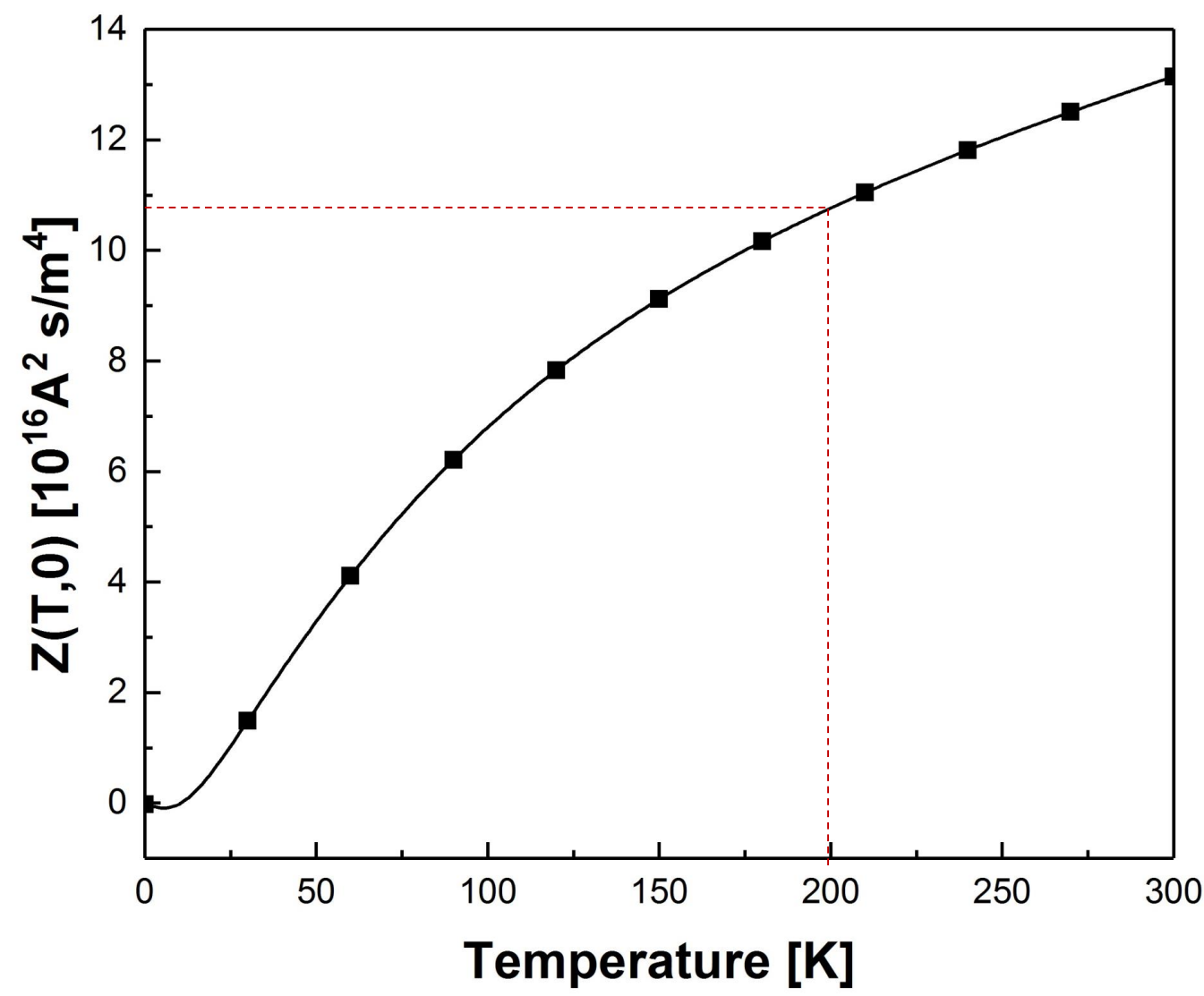
### ★ Z-function analysis

#### Assumptions

- Adiabatic heating
- Isolated magnet (no conduction heat input)
- No disturbance heat input (AC loss, flux jumping, wire motion, etc.)
- Constant current applied

$$Z(T_f, T_i) \equiv \int_{T_i}^{T_f} \frac{C_m(T)}{\rho_m(T)} dT$$

$C_m(T)$ : heat capacity of materials  
 $\rho_m(T)$ : electrical resistivity of copper



< Z-function of the winding pack including MgB<sub>2</sub> magnet, SUS304 bobbin, and Stycast 2850FT epoxy >

$$\int_{T_i}^{T_f} \frac{C_m(T)}{\rho_m(T)} dT = \left( \frac{A_m}{A_{cd}} \right) J_{m0}^2 \tau_{ah}$$

$A_m$ : cross-sectional area of matrix within the wire  
 $A_{cd}$ : cross-sectional area of conductor within the wire  
 $J_{m0}$ : current density within the copper matrix  
 $\tau_{ah}$ : time required to reach final temperature

$$\tau_{ah} = 1.47 \text{ s} \Rightarrow \text{Reach 200 K within 1.47 s}$$

Quench should be detected in ~ 0.5 s.

#### ★ Future works

- Optimization of the design of the 3.0-T whole-body MgB<sub>2</sub> MRI magnet will be performed to minimize the conductor consumption.
- Cryogenics, stability, and protection for the 3.0-T whole-body MgB<sub>2</sub> MRI magnet will be investigated with respect to the commercialized conductor options.