



Ultrasonic Doppler Modes

Piero Tortoli

1



Outline

- Doppler effect
- CW/PW Doppler systems building-blocks
- Pulsed Wave (PW) mode:
PRF, sample volume, spectral broadening,
mean frequency estimation...

Advanced Doppler systems and methods:

- Single-gate (TCD, Duplex)
- Multi-gate
- Flow-imaging
- Power, Harmonic & Tissue Doppler imaging
- Doppler artefacts (aliasing, blooming...)



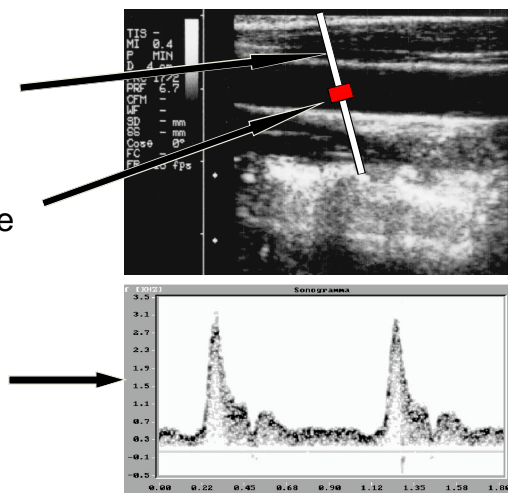
Outline of the 2nd part

- Pulsed Wave (PW) mode:
 - Duplex (Single-gate)
 - Multi-gate
 - Flow-imaging
 - Power and Harmonic Doppler
 - Tissue Doppler Imaging
- Doppler artefacts (aliasing, angle ambiguity, blooming...)




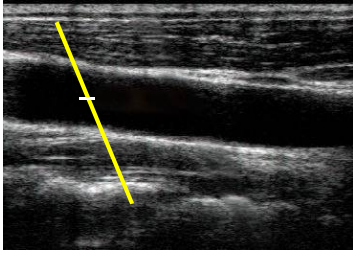
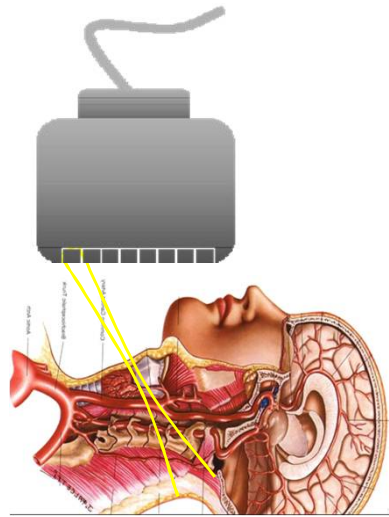
Duplex systems

- A (M-mode) scan line can be superimposed to a B-mode image
- Over the scan line, a specific sample volume can be selected
- The Doppler signal produced from the gated sample volume is analysed



UNIVERSITÀ DEGLI STUDI FIRENZE

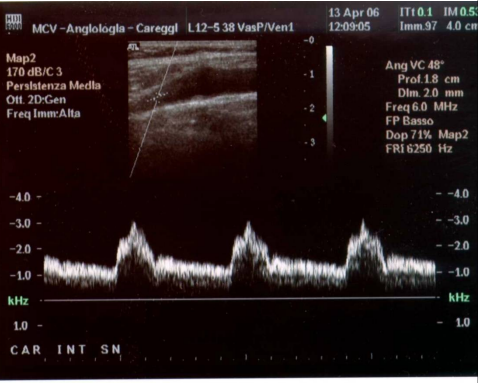
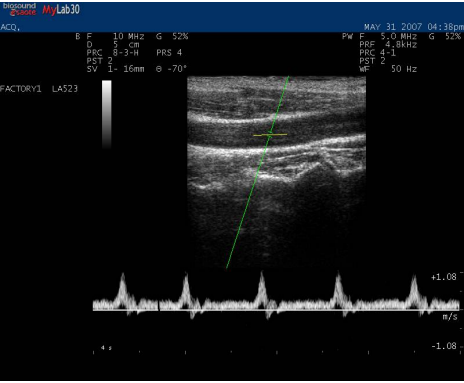
Duplex systems



Ideal for stenosis assessment

UNIVERSITÀ DEGLI STUDI FIRENZE

Duplex systems application



Healthy CCA

Stenotic Internal CA

UNIVERSITÀ DEGLI STUDI FIRENZE

Multigate spectral Doppler

The diagram illustrates the process of Multigate spectral Doppler. It starts with a B-mode ultrasound image on the left, showing a vessel lumen and vessel wall. A yellow line indicates the location of the Doppler gate. This gate is expanded into a 'Fast time' diagram, showing multiple parallel Doppler gates. Each gate's signal is processed by a Fast Fourier Transform (FFT). The resulting velocity profiles are then processed by another FFT to produce a spectral Doppler plot. The plot shows 'Depth (mm)' on the vertical axis and 'Freq/ Vel' on the horizontal axis. A yellow arrow points from the spectral plot back to the B-mode image, indicating the source of the data.

Detection of velocity profiles in arteries and veins

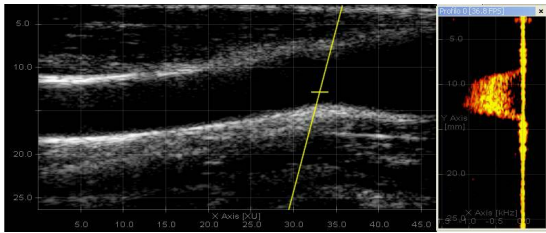
UNIVERSITÀ DEGLI STUDI FIRENZE

MSD stenosis assessment

The screenshot shows the 'MSD stenosis assessment' software interface. It features two main windows: 'Frame browser' and 'Frame viewer'. The 'Frame browser' window displays a series of frames with a color-coded stenosis assessment. The 'Frame viewer' window shows a detailed view of a frame, with a color-coded stenosis assessment and a corresponding B-mode image. The software includes various control panels for gain, zoom, and other parameters. A yellow arrow points from the 'Frame viewer' window to the B-mode image below, indicating the source of the data.

UNIVERSITÀ DEGLI STUDI FIRENZE

Dual (B+MSD) Mode

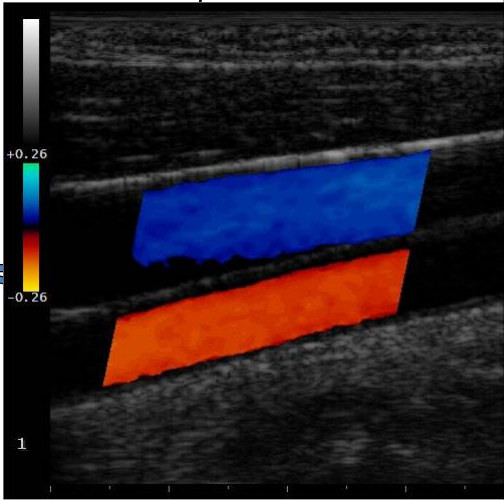


UNIVERSITÀ DEGLI STUDI FIRENZE

Flow imaging Mode (Color Doppler)

- By firing several pulses for each scan line
- By estimating the mean frequency (velocity) detected at each depth
- By color-coding consecutive pixels according to the detected mean frequencies
- By scanning a 2-D region

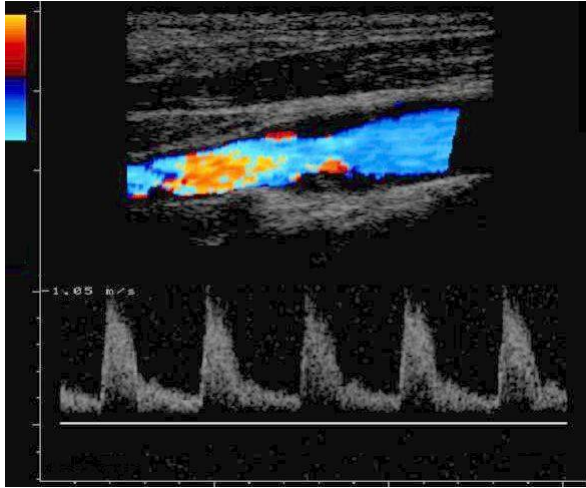
Frame rate limitations
Poor sensitivity
Unsuitable for low velocities



Multigate processing applied to multiple scan lines



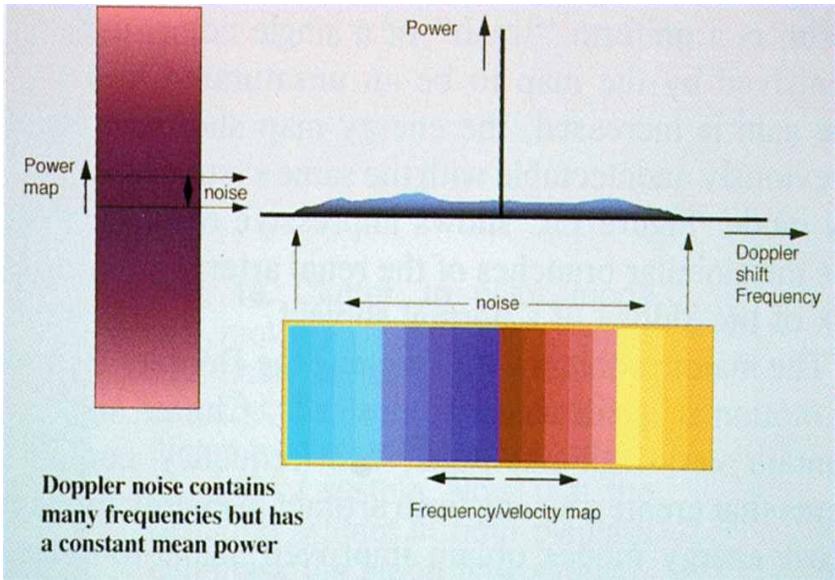
Color Doppler application



non-hemodinamic internal carotid stenosis



Power Doppler



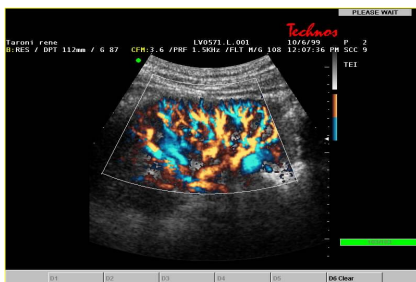
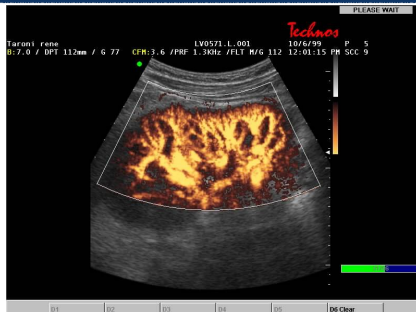


Power Doppler

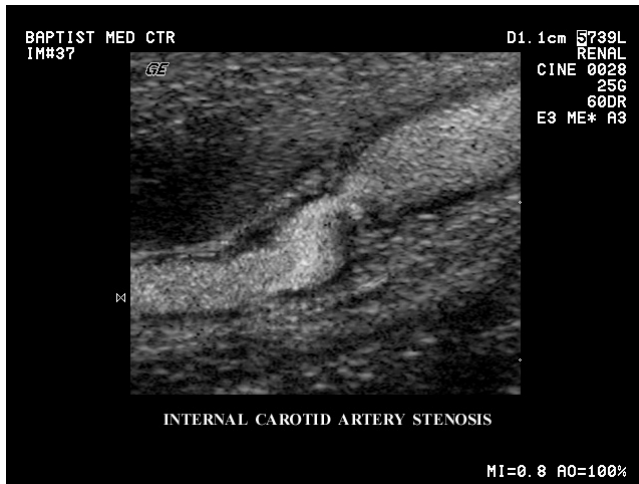
- For each scan line, the power of Doppler echoes is detected and integrated (persistence)

- ☺ High S/N
- ☺ Ideal for small vessels
- All movements (including "slow" blood and tissue movements) are detected
- Qualitative (velocity magnitude is ignored)

Same hardware as for Doppler imaging: software differences



B-Flow Mode

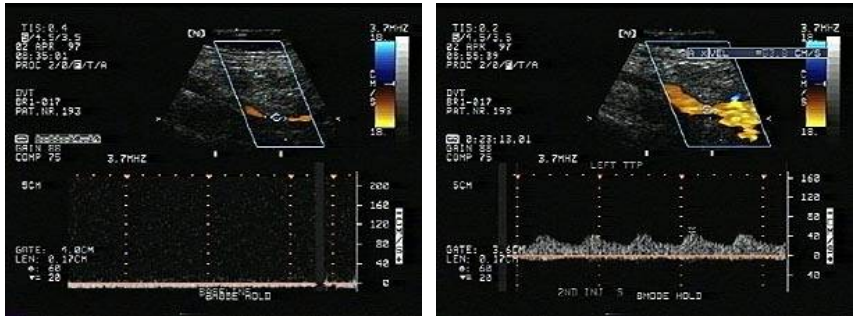


High resolution; High blood/tissue ratio

Doppler modes with Contrast agents

Echo enhancement

Injection of US contrast agents (microbubbles in a shell) generates strong backscattering (*echo enhancement*)



Useful for small, deep, hardly accessible vessels (eg: TCD analysis)





UNIVERSITÀ
DEGLI STUDI
FIRENZE

Harmonic Doppler Mode

- Non-linear behaviour of US contrast agents yields 2nd harmonic ($2 \times f_t$) components much stronger than those generated by tissue

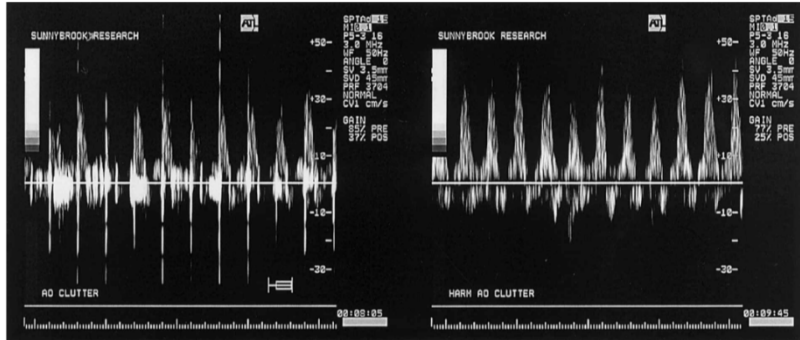


Figure 6. Clutter rejection with harmonic spectral Doppler. **A.** The abdominal aorta of an animal is examined with harmonic spectral Doppler. In conventional mode, clutter from the moving wall causes the familiar artifact, which also obscures diastolic flow. **B.** In harmonic mode, the clutter is almost completely suppressed so that flow can be resolved. The

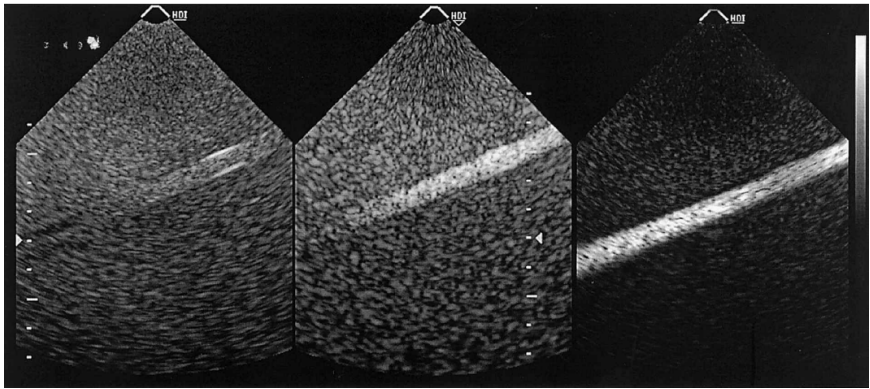
Need for wideband transducers – Suitable for perfusion assessment



UNIVERSITÀ
DEGLI STUDI
FIRENZE

Harmonic Doppler Mode

- Detection of 2nd harmonic echoes allows to reverse the roles of blood & tissue in US images
- More sophisticated TX-RX strategies (eg: *pulse inversion*) allow further increments of blood/tissue ratio to be obtained



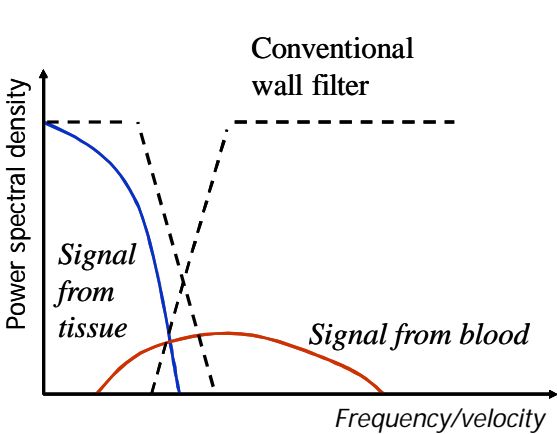
Conventional
US imaging

Harmonic
Doppler imaging

Pulse inversion
Doppler imaging

Tissue Doppler Imaging (TDI)

Tissue Doppler Imaging (TDI)

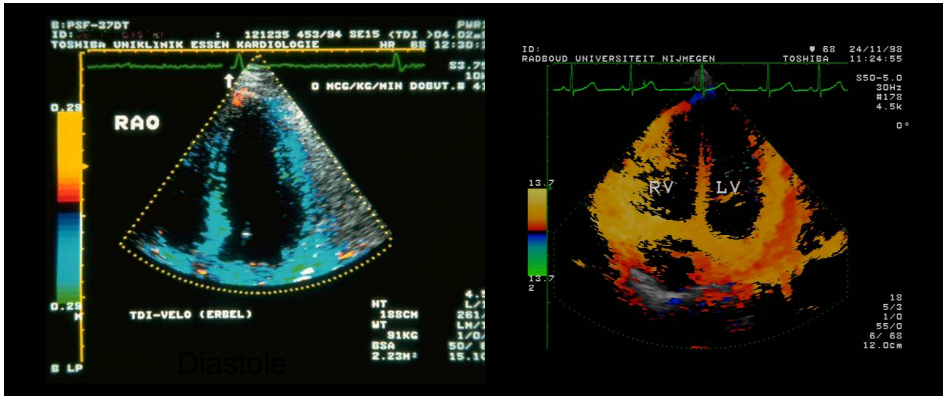


- The wall filter partially suppresses the echo-signal from tissue
- In TDI, the blood signal is suppressed!



TDI images

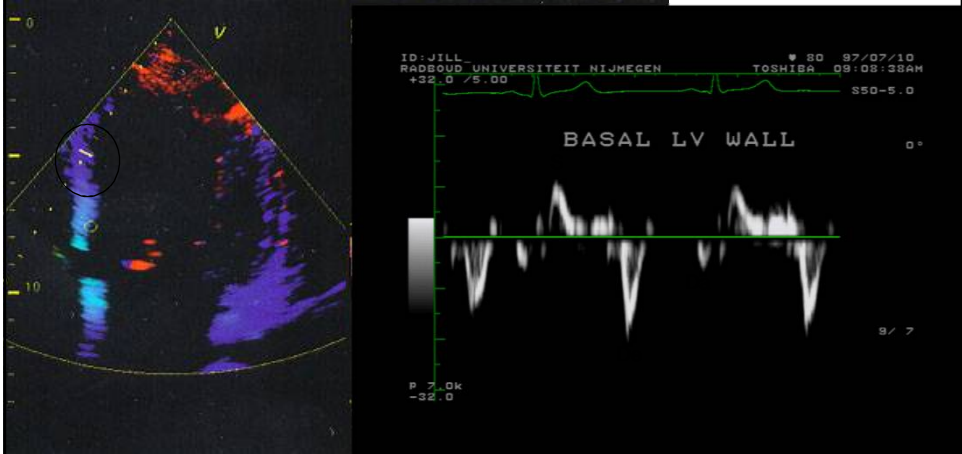
Left ventricle

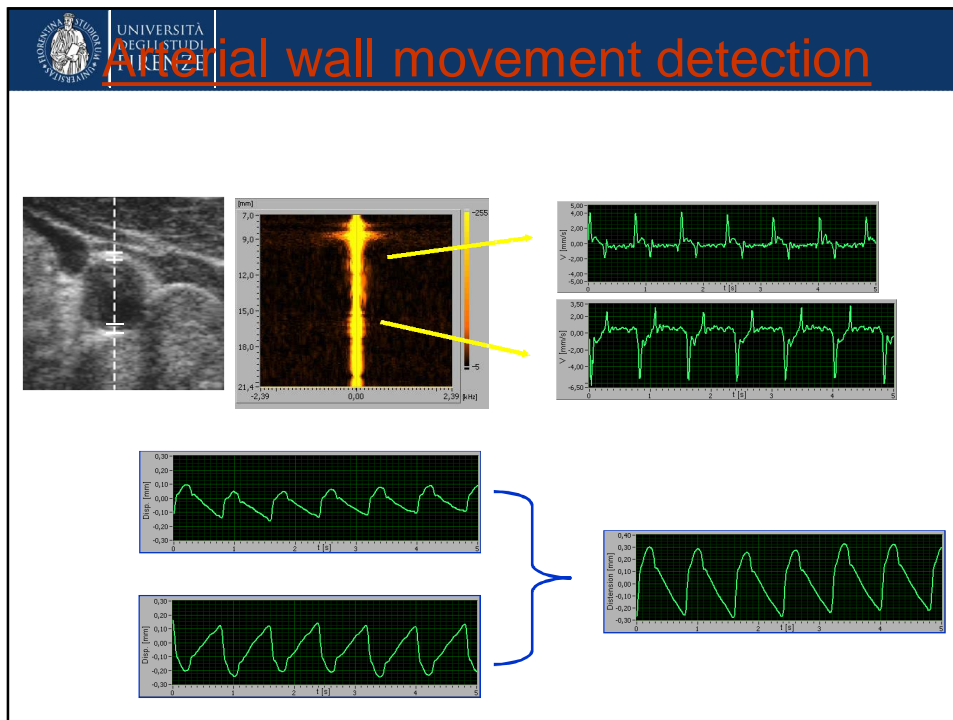


High signal, low velocity image



TDI waveforms





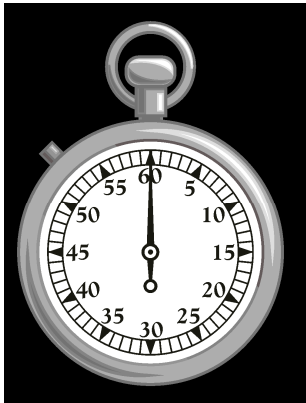
Doppler artefacts: Aliasing

- For each transmitted pulse, one sample of the Doppler signal at a given depth is obtained
- Doppler samples are produced at PRF rate
- If the sampling frequency, PRF, is too low with respect to the Doppler frequency, f_d (i.e. if $f_d > \text{PRF}/2$) \rightarrow



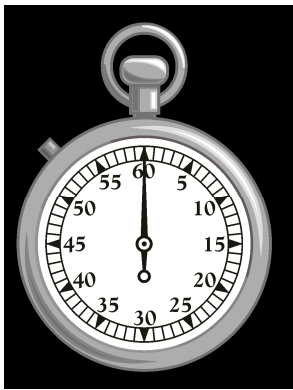
UNIVERSITÀ
DEGLI STUDI
FIRENZE

Aliasing example



UNIVERSITÀ
DEGLI STUDI
FIRENZE

Aliasing example



If subsequent pictures of the chronograph are taken too rarely, the hand seems to rotate into the wrong direction

UNIVERSITÀ DEGLI STUDI FIRENZE

Aliasing origin

Aliasing occurs for sampling frequency $f_s < 2B$, with B being the signal bandwidth (*Nyquist limit*).

For PW systems:

$$f_s = \text{PRF}$$

$$B = f_{d\max} \text{ (maximum Doppler frequency)}$$

→ Nyquist limit: $\text{PRF} > 2B = 2f_{d\max} = 4 \frac{v_{\max}}{c} f_0 \cos \vartheta$

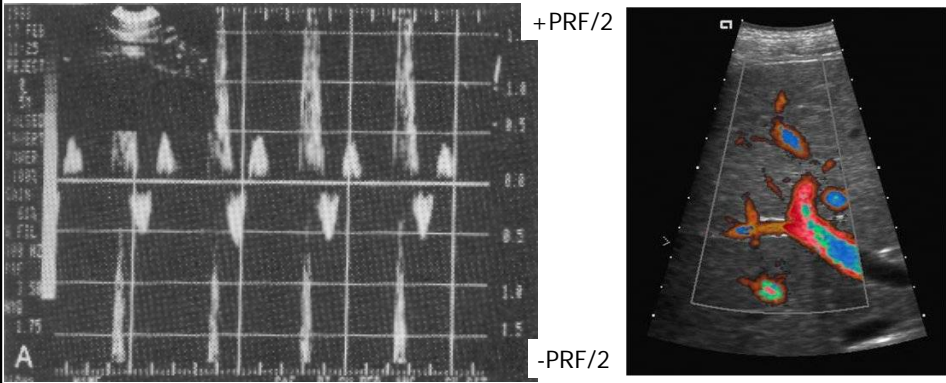
$$\text{PRF}_{\max} = \frac{c}{2d}$$

$$v_{\max} < \text{PRF}_{\max} \frac{c}{4f_0 \cos \vartheta} = \frac{c^2}{8f_0 d \cos \vartheta}$$

UNIVERSITÀ DEGLI STUDI FIRENZE

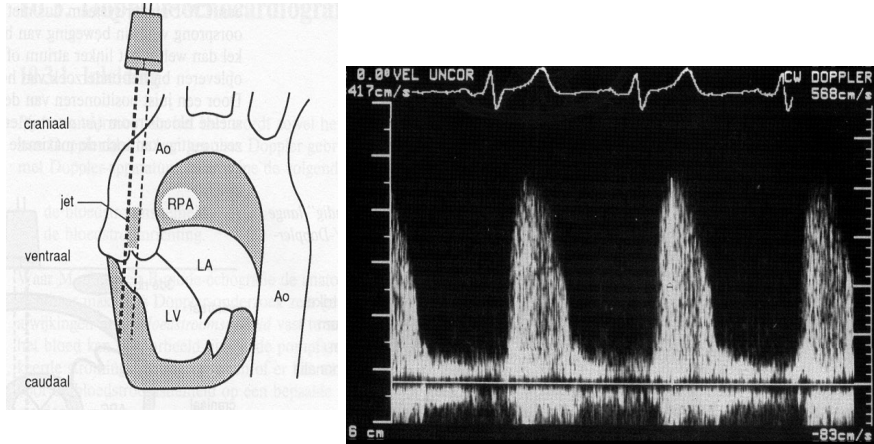
Aliasing effects

In PW Doppler systems, *aliasing* yields Doppler components in wrong positions, or wrong colors in 2-D flow maps



UNIVERSITA' DEGLI STUDI FIRENZE

Methods for aliasing limitation CW Doppler measurement

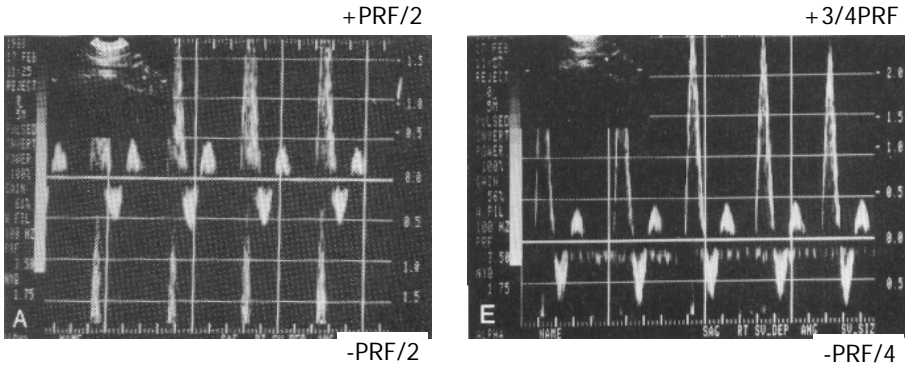


Jet stream through aortic valve stenosis

UNIVERSITA' DEGLI STUDI FIRENZE

Aliasing limitation

- ✓ Increasing the PRF (D_{max} decreases)
- ✓ Increasing the Doppler angle (f_D decreases)
- ✓ Using lower frequency transducers (*worst res*)
- ✓ *Baseline shifting:*



A: +PRF/2, -PRF/2

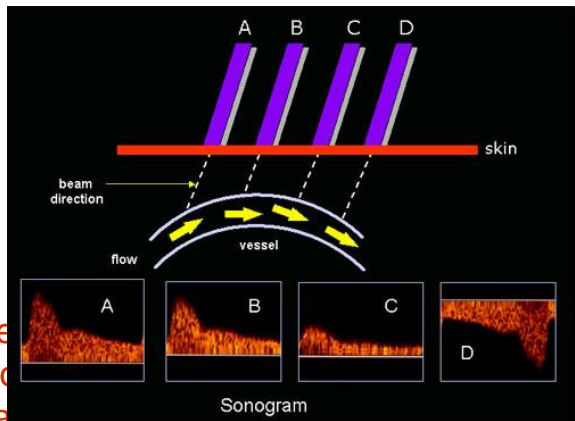
E: +3/4PRF, -PRF/4



Doppler angle ambiguities

The detected frequency depends on the Doppler angle

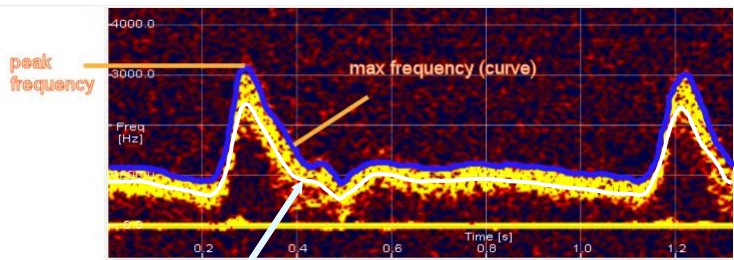
$$f_d = 2 \frac{v}{c} f_0 \cos \theta$$



- Frequency is dependent on the angle of the beam
- If the angle is not known, the frequency cannot be converted to velocity



Maximum velocity

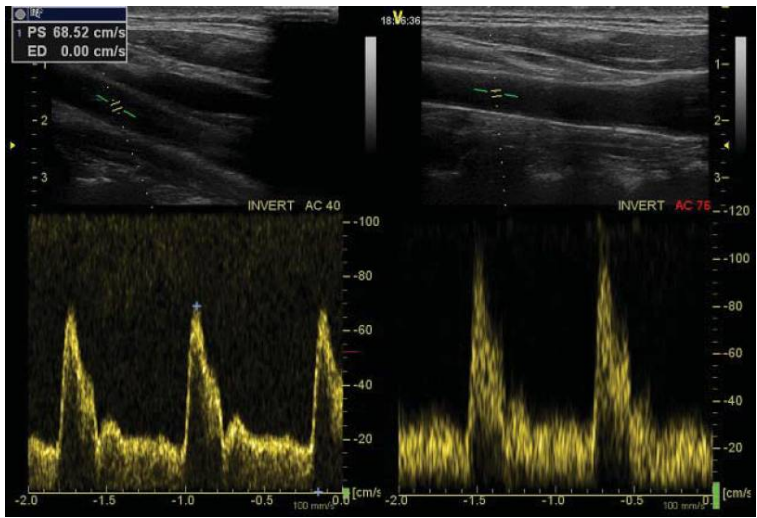


Mean frequency curve

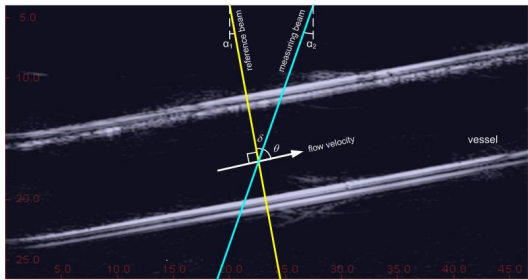
Does max frequency correspond to max velocity?



Angle ambiguity



Vector Doppler



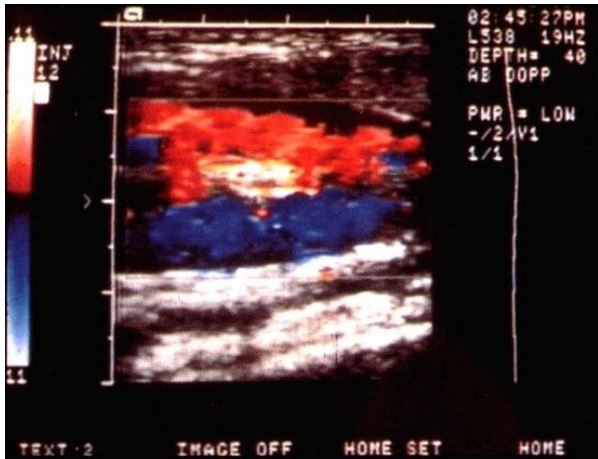
Two beams intercepting the same SV can solve the angle ambiguity

Two equations with two variables (v & θ):

$$f_{d1} = 2 \frac{f_0}{c} v \cos \vartheta \quad f_{d2} = 2 \frac{f_0}{c} v \cos(\vartheta + \delta)$$



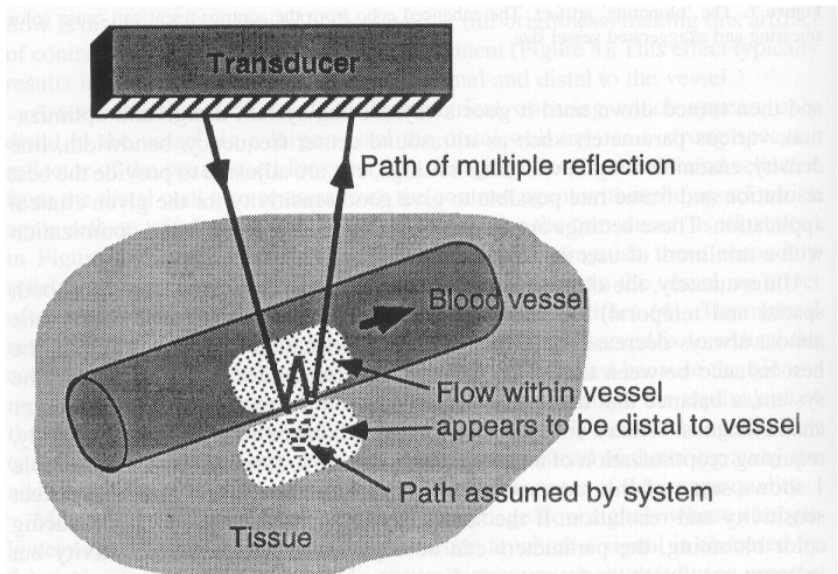
Blooming



Blooming corresponds to the presence of "color" in regions with no movement. It is due to excessive echogenicity of contrast agents



Blooming



Blooming risk is minimised by maintaining the Gain as low as possible



Summary

- CW mode is used only in cases where *aliasing* plays a major role (eg: *jets in cardiac valves*)
- All advanced Doppler systems work in PW mode
- PW mode allows range discrimination (flow mapping)
- In advanced Doppler modes, the key element is the transducer (wide bandwidth)
- Further enhancements in velocity detection and reduction of artefacts have to be expected through both technological (matrix probes, vector Doppler, plane wave imaging) and software advances