Ultrasound advanced imaging: beyond anatomy

Ultra Fast imaging or High Frame Rate

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CREATIS

Examples and the corresponding evolution of ultrasound imaging

Part 1

- static elastography
- shear wave elastography
- ultrafast imaging
- photo-acoustic imaging

Tissue elasticity imaging - clinical motivation

- The objective of elastography is to prodcue a map of the stiffness of tissues
- There is strong correlation between stifness and some pathologies

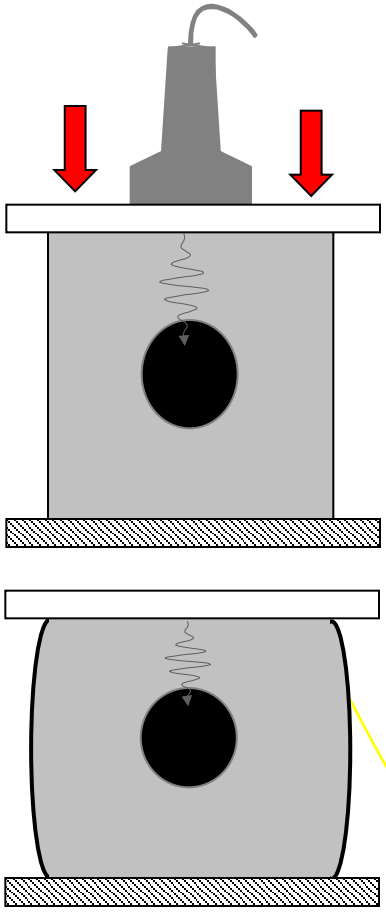
Young Modulus in Breast tissue (kPa)	
Normal fat	**: 18 ± 7**
Normal glandular	**: 28 ± 14**
Infiltrating carcinoma	**: 106 ± 32**

Young Modulus in Prostate tissue (kPa)	
Normal anterior	**: 60 ± 15**
Normal posterior	**: 68 ± 14**
Cancer	**: 230 ± 34**

[Krouskop-98]

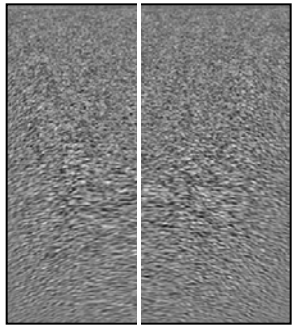
- The principle of static elastography is to image the deformation of a tissue under external load (palpation with the US probe)

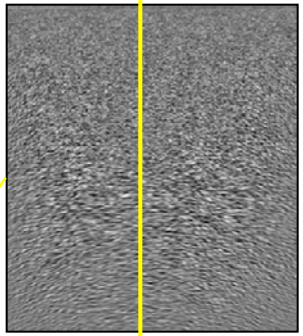
Elastography - Basic principle



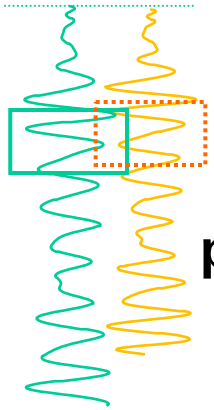
Ultrasound scatterrers positions are modified

US image at pressure P



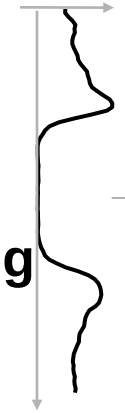


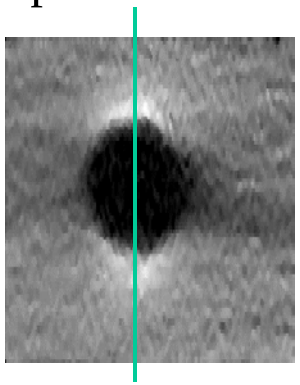
US Image at pressure P+dP



Signal processing

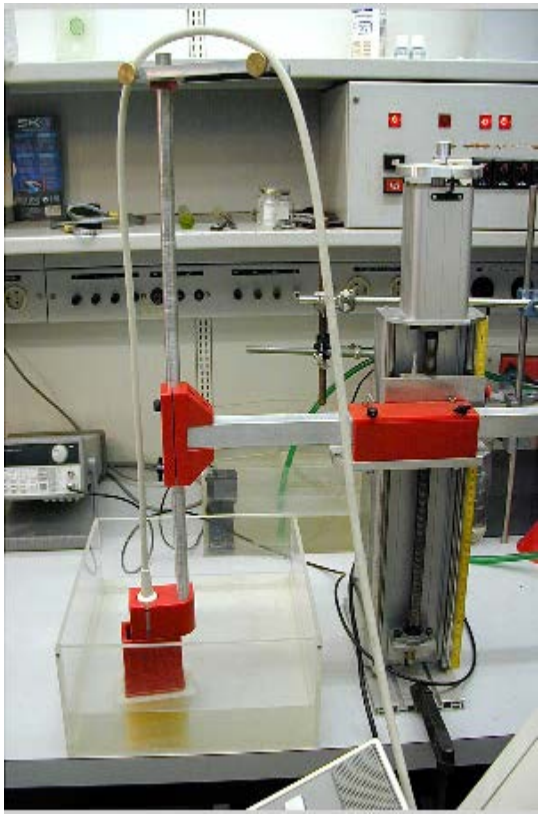
Local deformation map



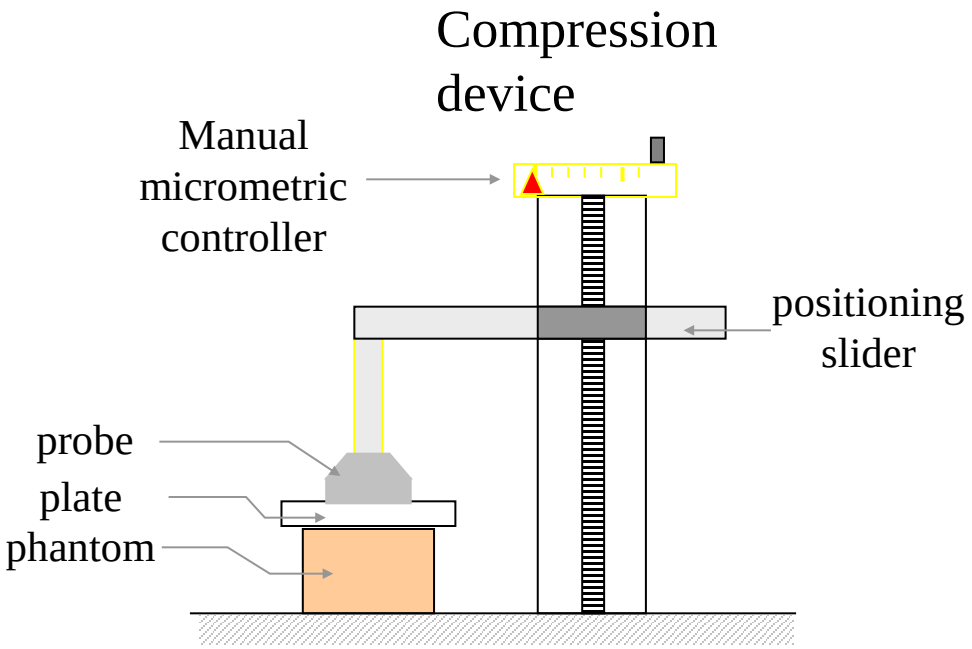


Strain field

In vitro results: experimental set-up

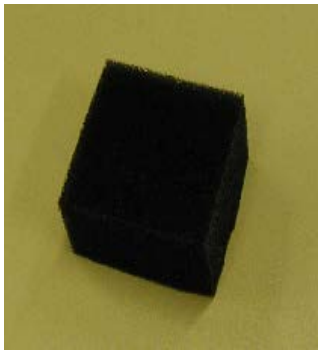


Bochum

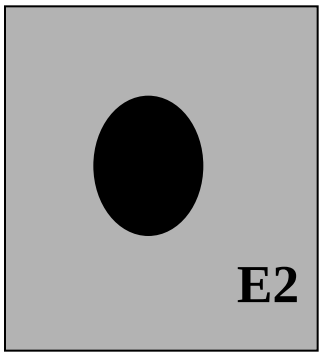


Central frequency: 7.2 MHz
Sampling frequency: 36 MHz
Displacement step precision: 0.05 mm

Results with a foam phantom



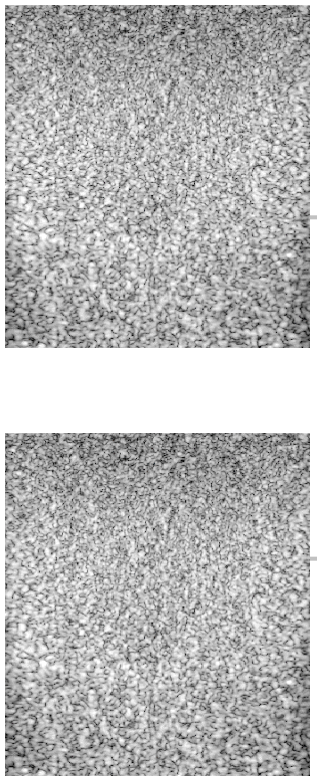
Test object

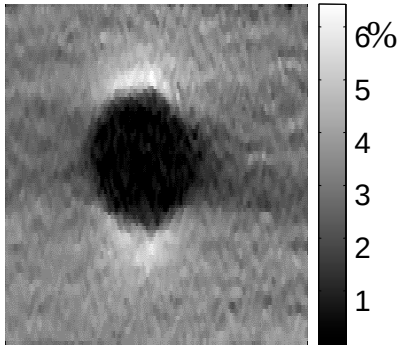


scheme

$E_1 > E_2$

$Z_1 = Z_2$

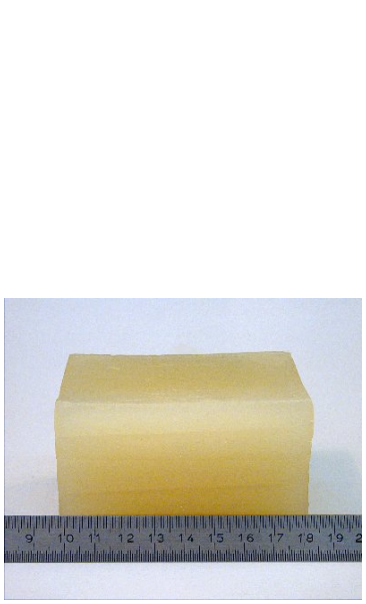




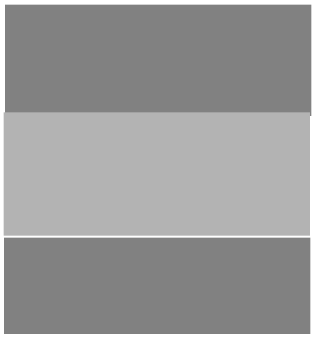
Computed strain field

- Foam phantom containing a spherical hard inclusion in agar (diameter: 1.5 cm)
- phantom characteristics: acoustical homogeneity; compressibility
- elastogram computation: window length = 1 mm, 60 % overlap

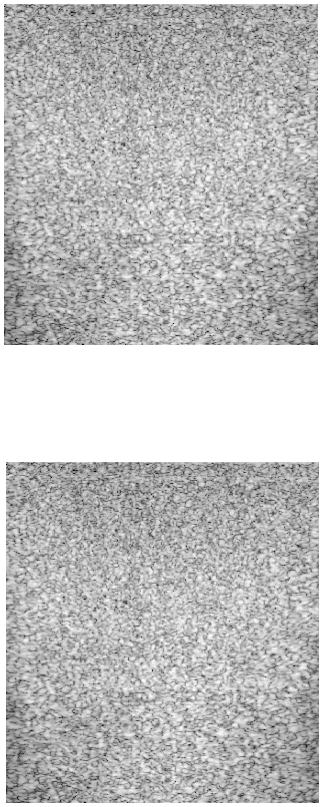
Results with a 3-layer tissue mimicking phantom

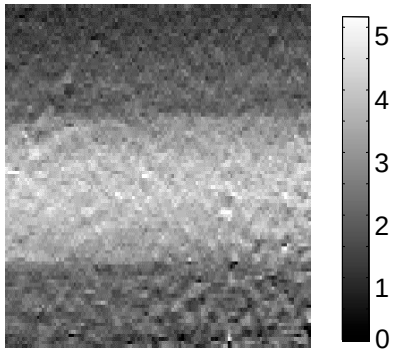


Test object



scheme



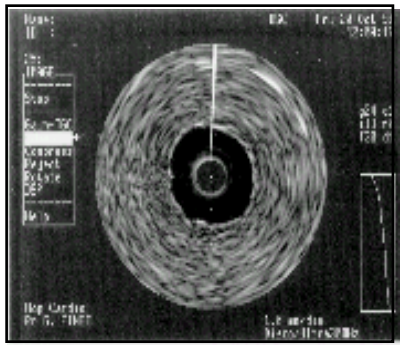


Computed strain field

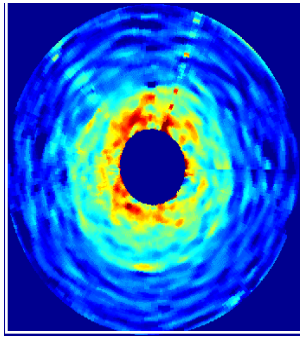
- 3-layer phantom
  - soft layer: 6% gelatine, 1% agar, 1% scatterers (SiC)
  - hard layer: 6% gelatine, 4.5% agar, 1% scatterers
- elastogram computation window length: 1 mm 60 % overlap

Results with a two layer cryogel phantom

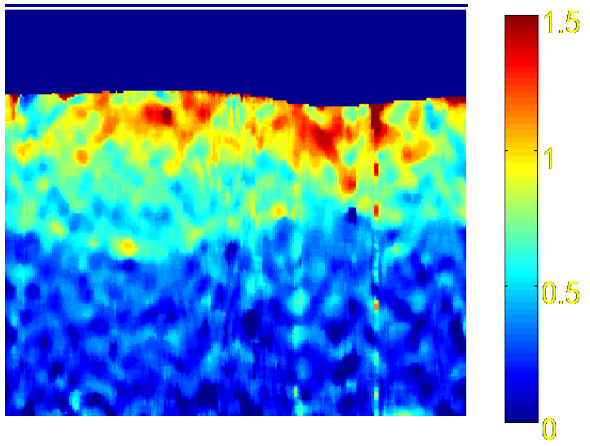
Photograph



B mode image

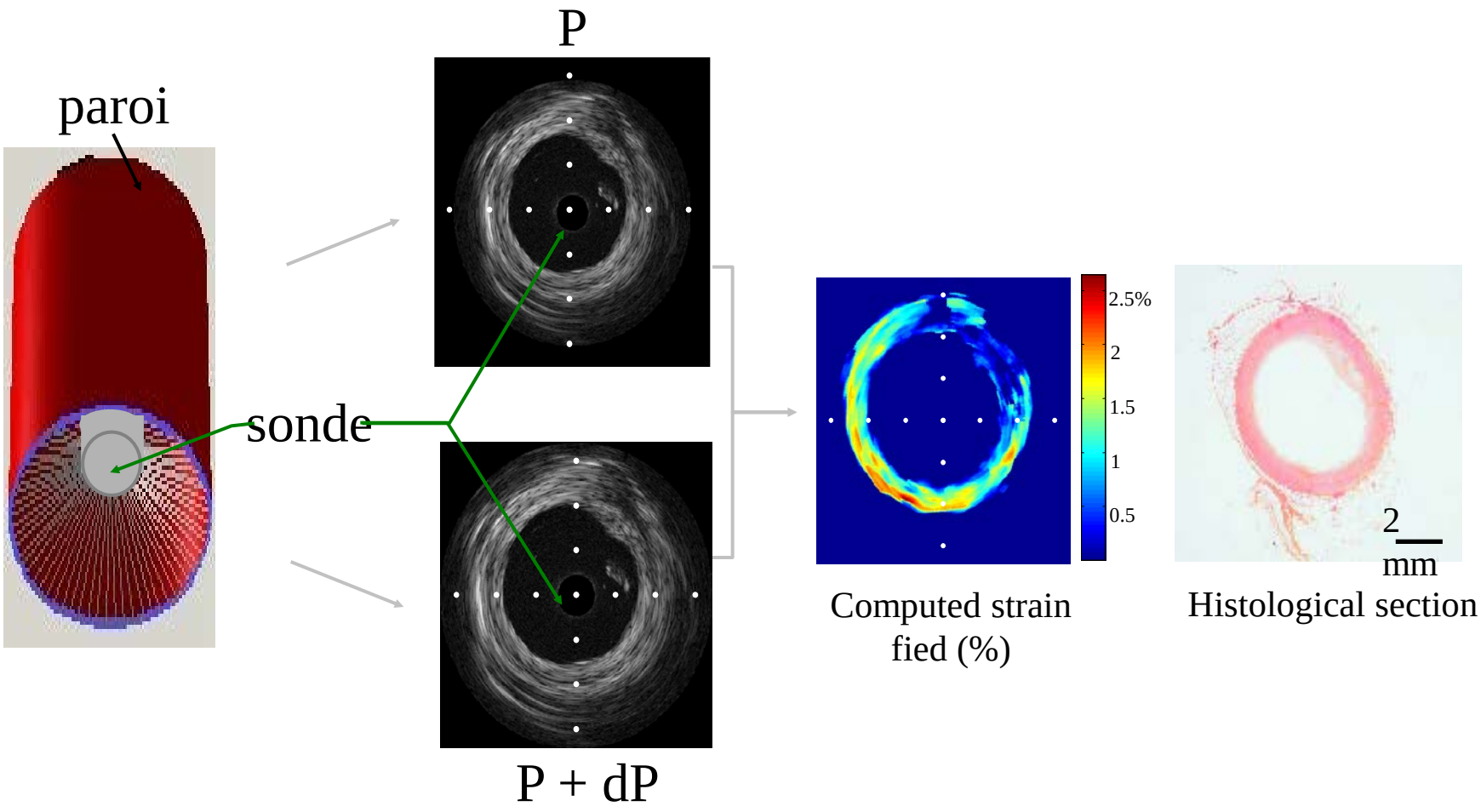


Elastogram



- Polyvinyl alcohol cryogel phantom
- 2 layers : soft = 1 freeze-thaw cycle, hard = 3 freeze-thaw cycle
- elastogram computation : window length = 0.25 mm, 80% overlap

Results with a fresh excised carotid artery



Limitation of static elastography

Only qualitative / relative stiffness

Depends on the applied load

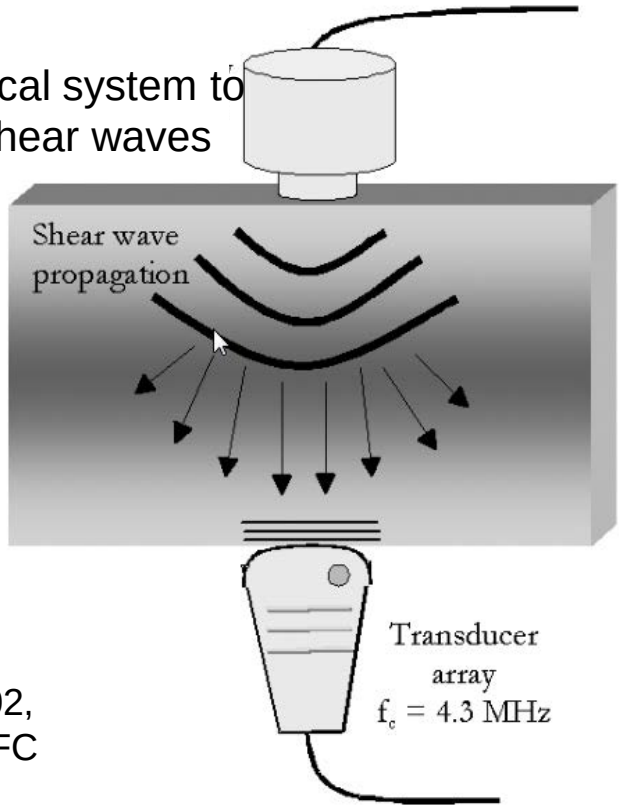
Not quantitative

➔ Shear wave elastography

The idea of shear wave elastography

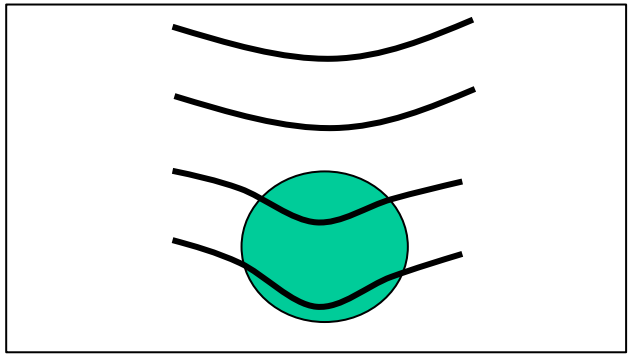
Shear wave propagation velocity is proportional to shear modulus

Mechanical system to induce shear waves



Tanter-2002,
IEEE TUFFC

Shear wave propagation



Acceleration due to "harder" inclusion

US Imaging of the shear wave propagation + determination of local velcity ➔ shear wave modulus

Shear wave elastography

Shear wave have typical velocities ranging between 1-10 $m.s^{-1}$

➔imaging at frame rate >> 1 kHz is needed

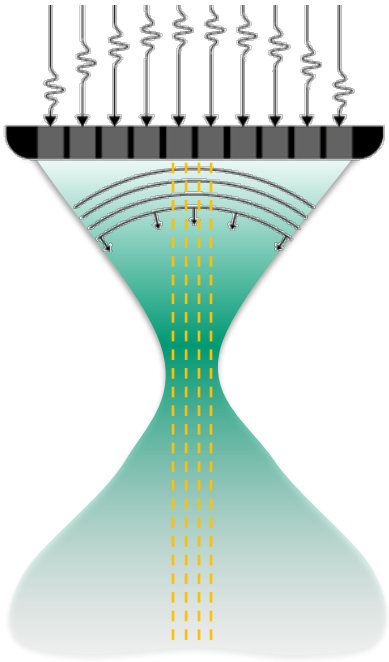
(classical imaging frame rage is 20 to 100 Hz)

How can ultrafast imaging be performed?

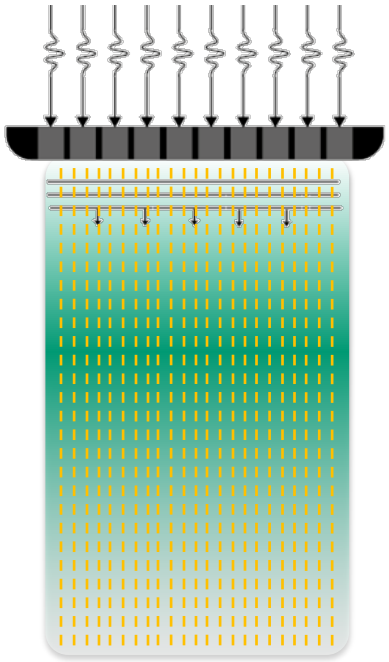
How to go faster?

Use **broad field-of-view transmit beams** with **full parallel receive beamforming:** 1 image per pulse => **4000 to 5000 fps!**

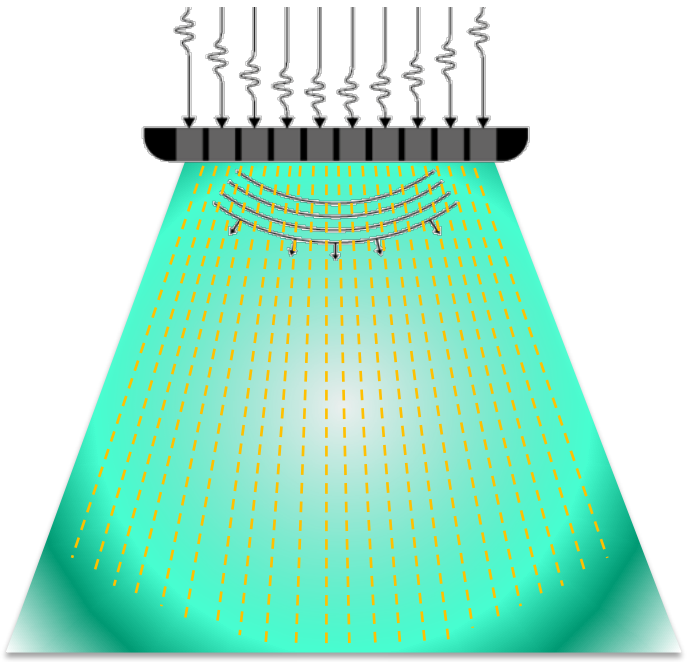
Focused pulses



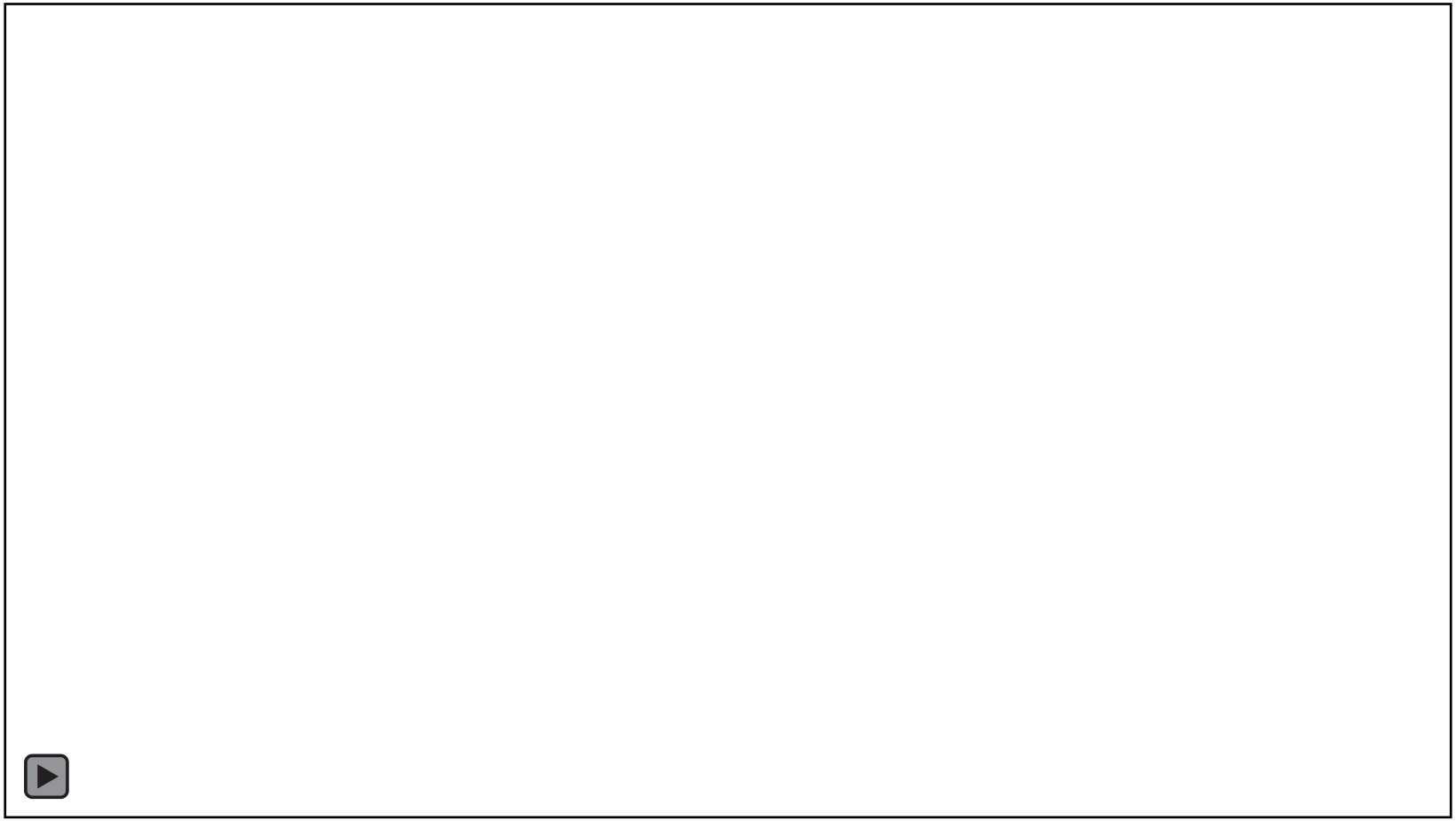
Unfocused pulses (plane waves)



Defocused pulses (diverging waves)

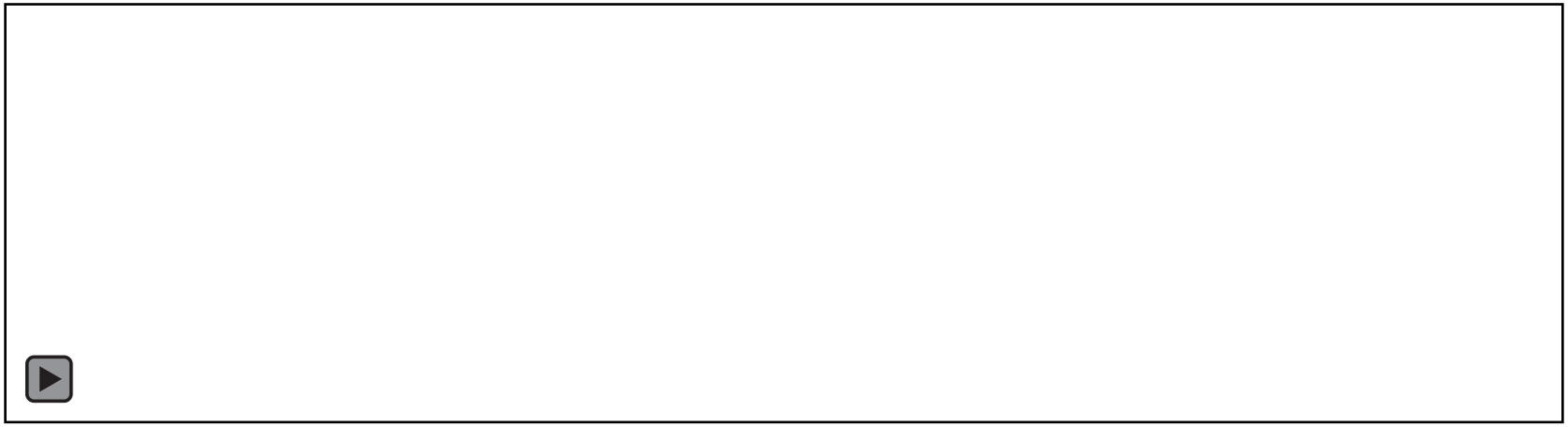


Conventional vs ultrafast imaging



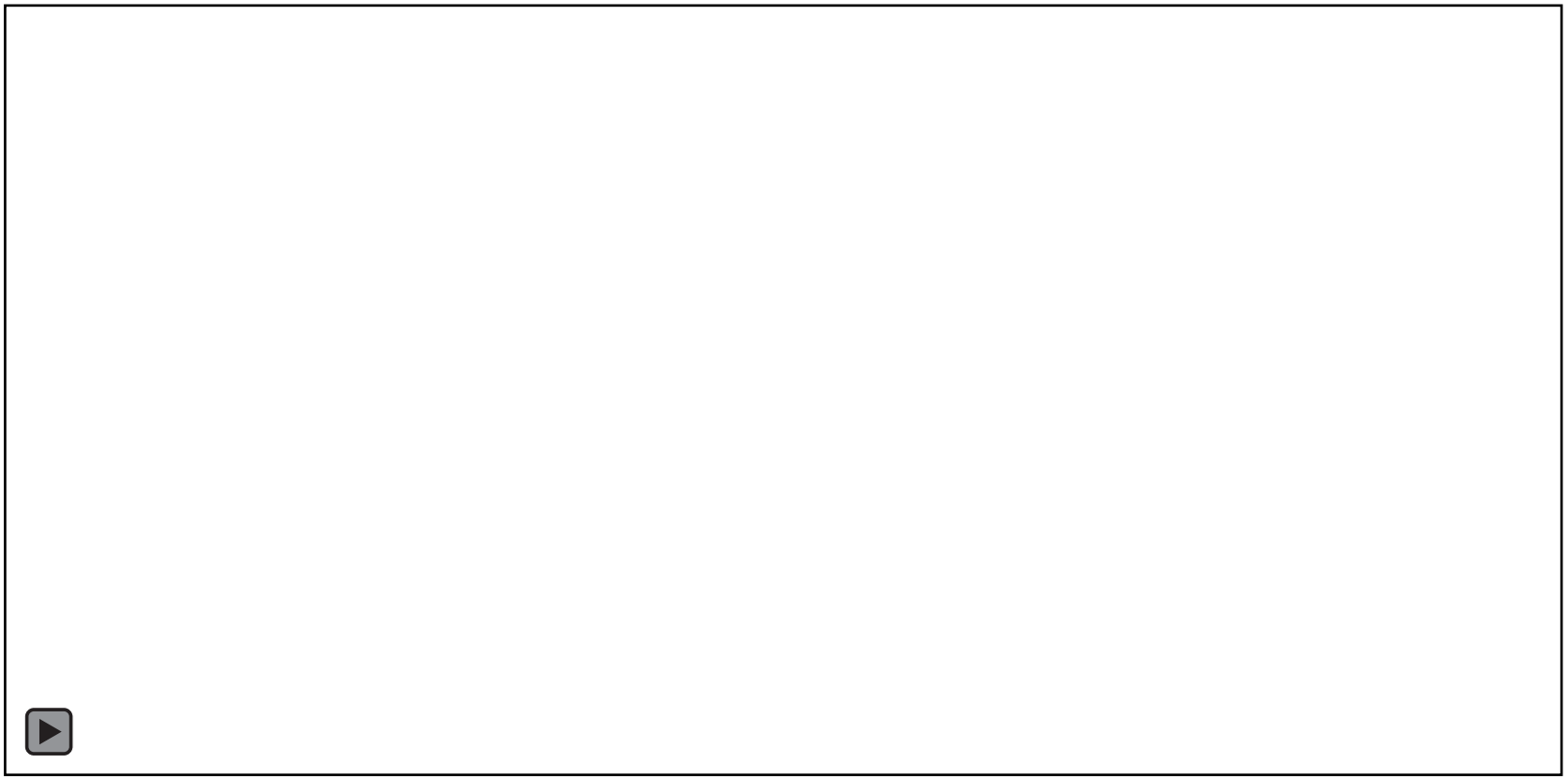
➔ Using ultrafast imaging one can image shear wave propagation

Ultrafast imaging of shear wave propagation



Local velocity estimation

Ultrafast imaging of shear wave propagation

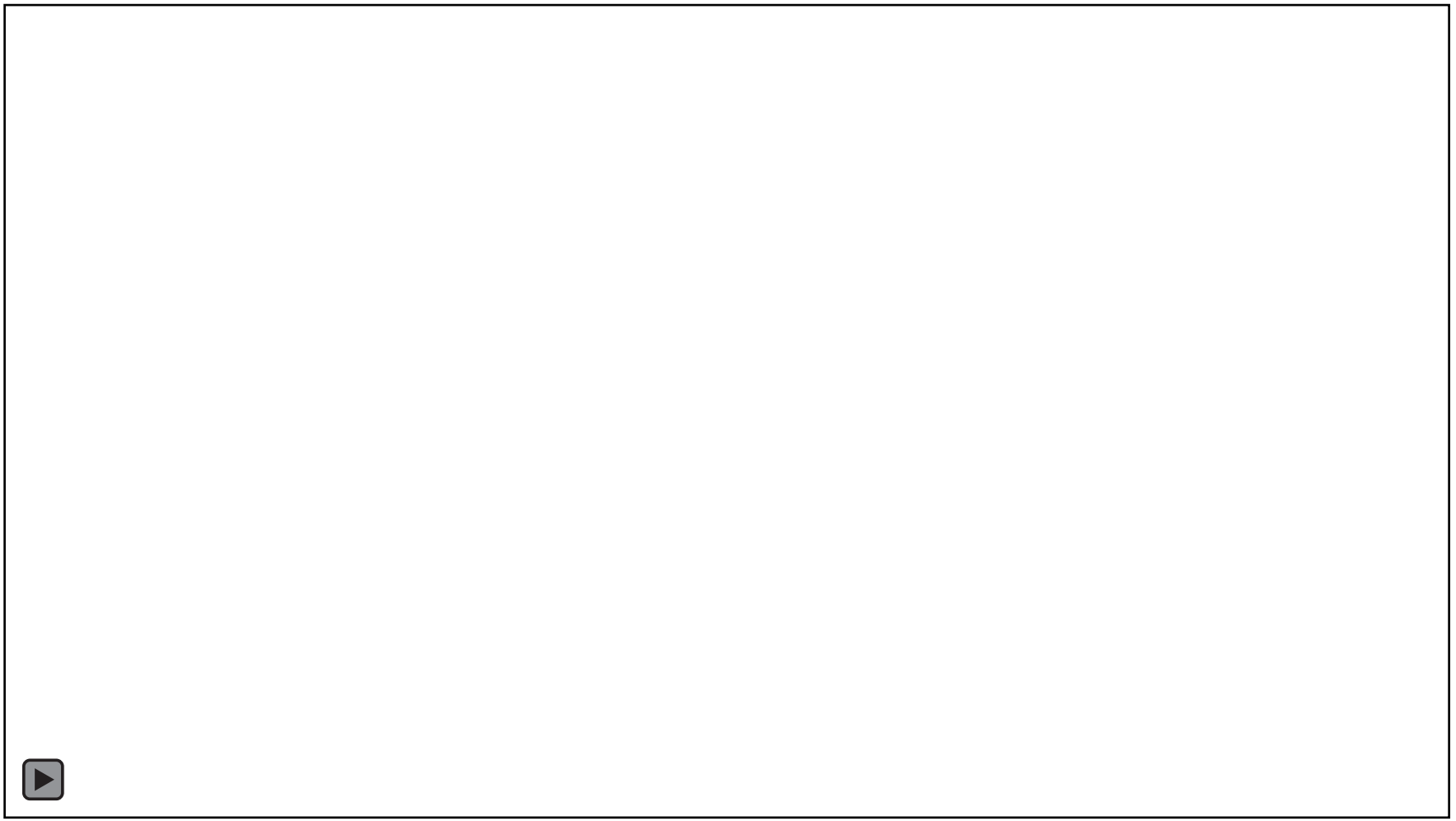


Shear wave elastography in the Supersonic Imagine system

The shear wave is induced using the US probe and the so-called push-beam

Ultrafast imaging is performed to image the shear wave propagation

http://www.supersonicimagine.fr/



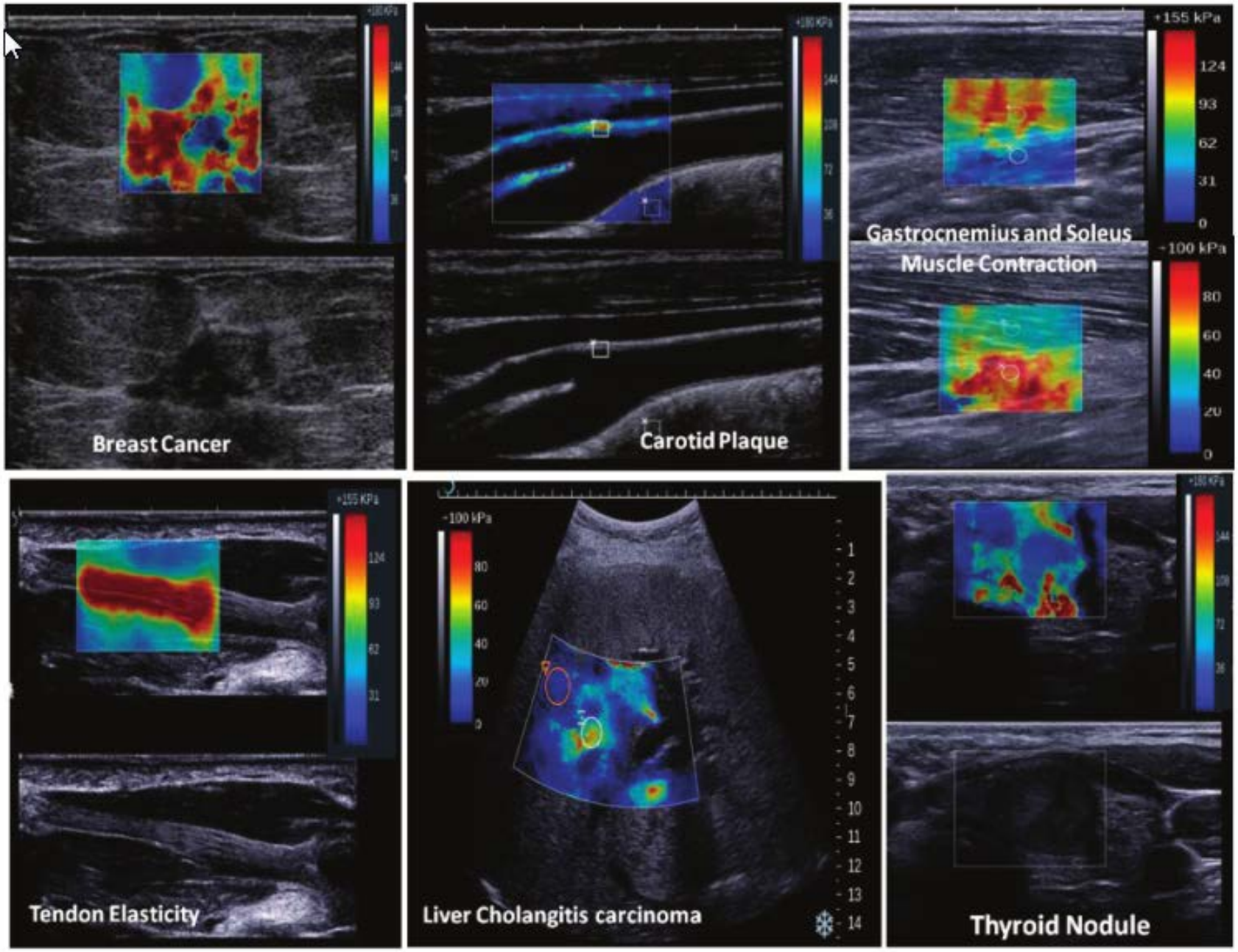


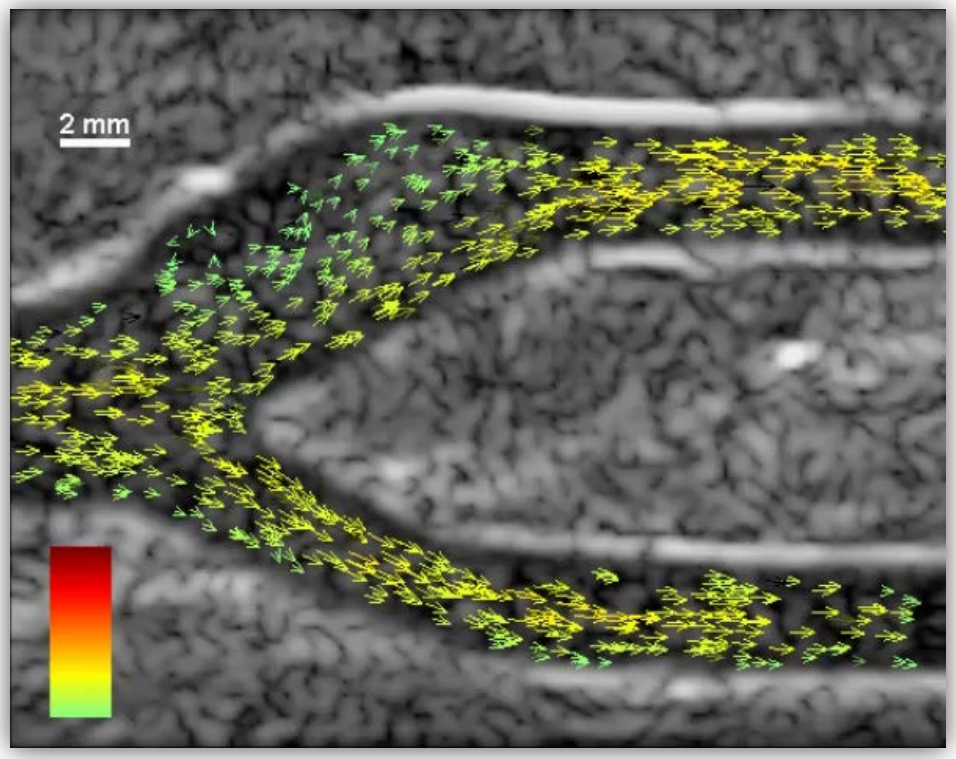
Fig. 6. Clinical examples of shear wave elastography based on the supersonic shear wave imaging (SSI) method (courtesy of Supersonic Imagi
France).

Use of Ultrafast imaging

Example: complex motion visualization:

- Blood flow
- Cardiac flow
- Arterial wall motion

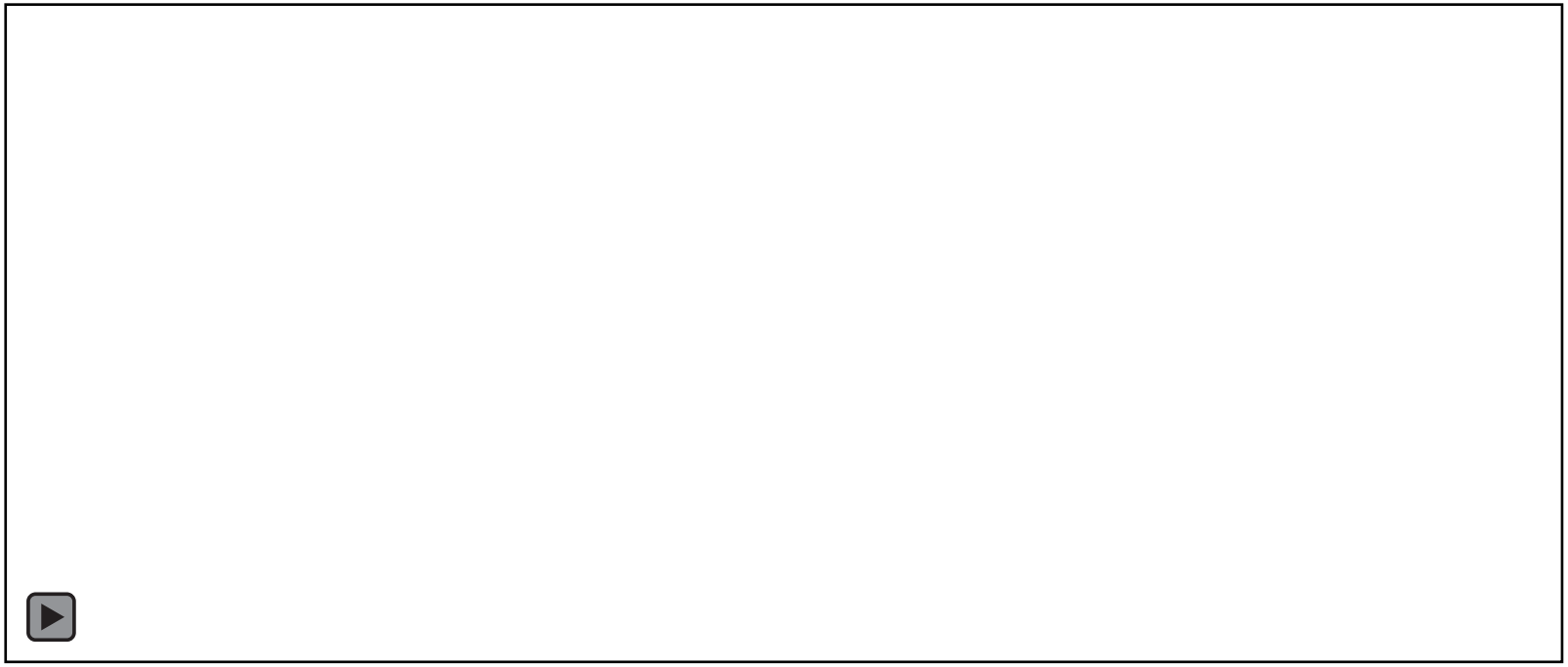
1) Complex motion visualization: blood flow



Ultrafast vector flow in the carotid bifurcation of a healthy subject

Courtesy of Alfred Yu, Hong Kong University

1) Complex motion visualization: blood flow



Ultrafast vector flow in the carotid bifurcation of a subject with 50% eccentric stenosis

Courtesy of Alfred Yu, Hong Kong University

1) Complex motion visualization: cardiac flow

- Perimembranous ventricular septal defect (significant shunt)
- 36 days old, 4259 gr.

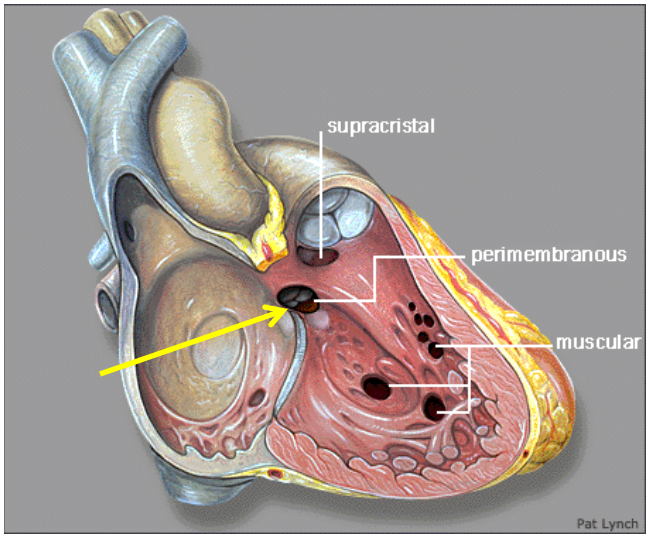
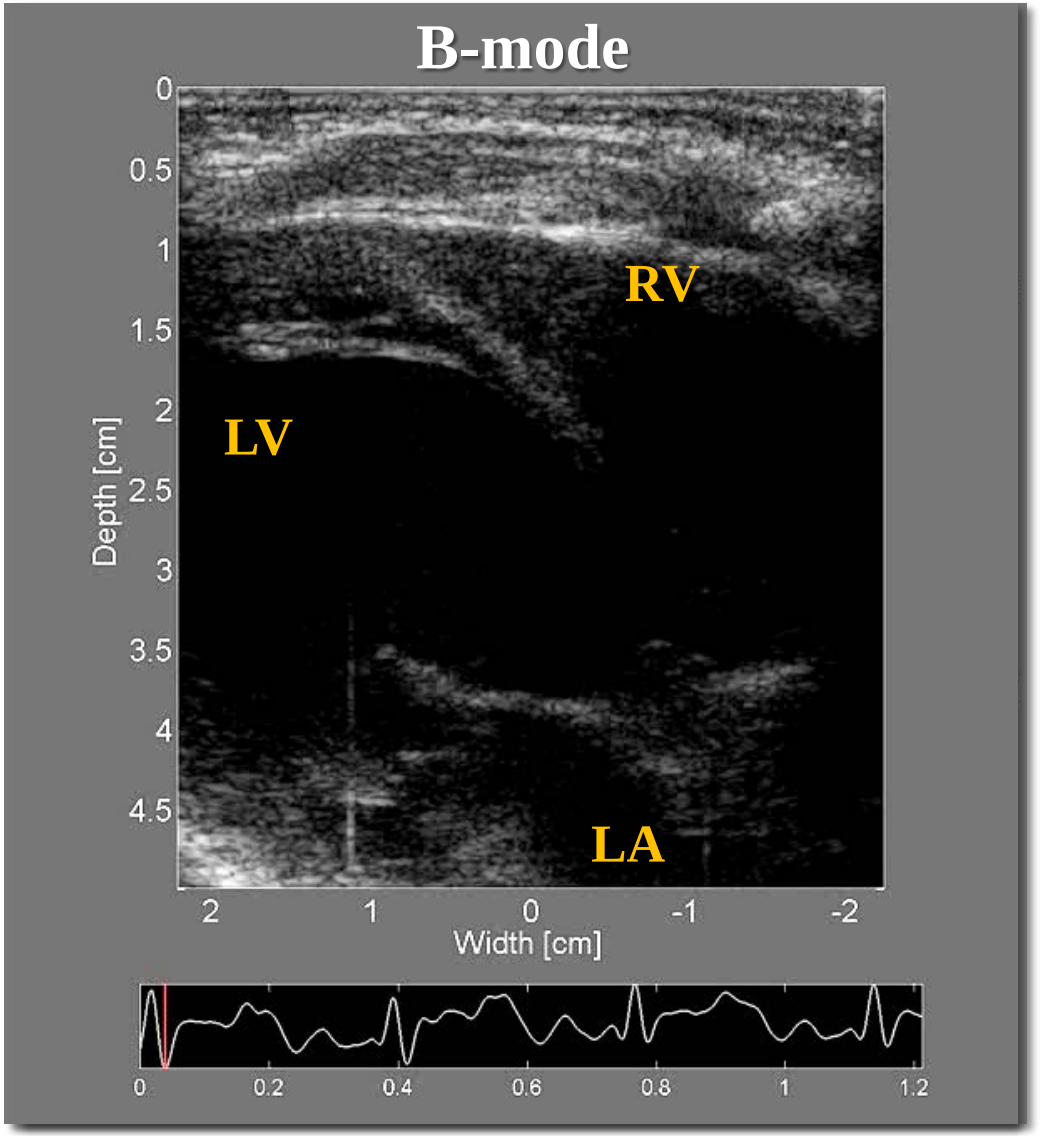


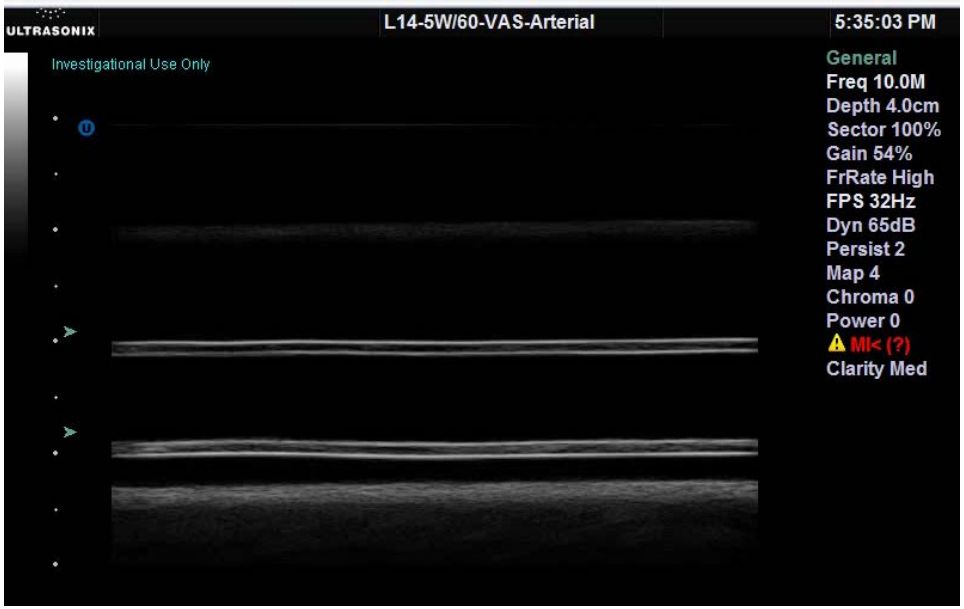
Image source: *Wikipedia, Pat Lynch*



Courtesy of Lasse Lovstakken, NTNU Trondheim, Norway

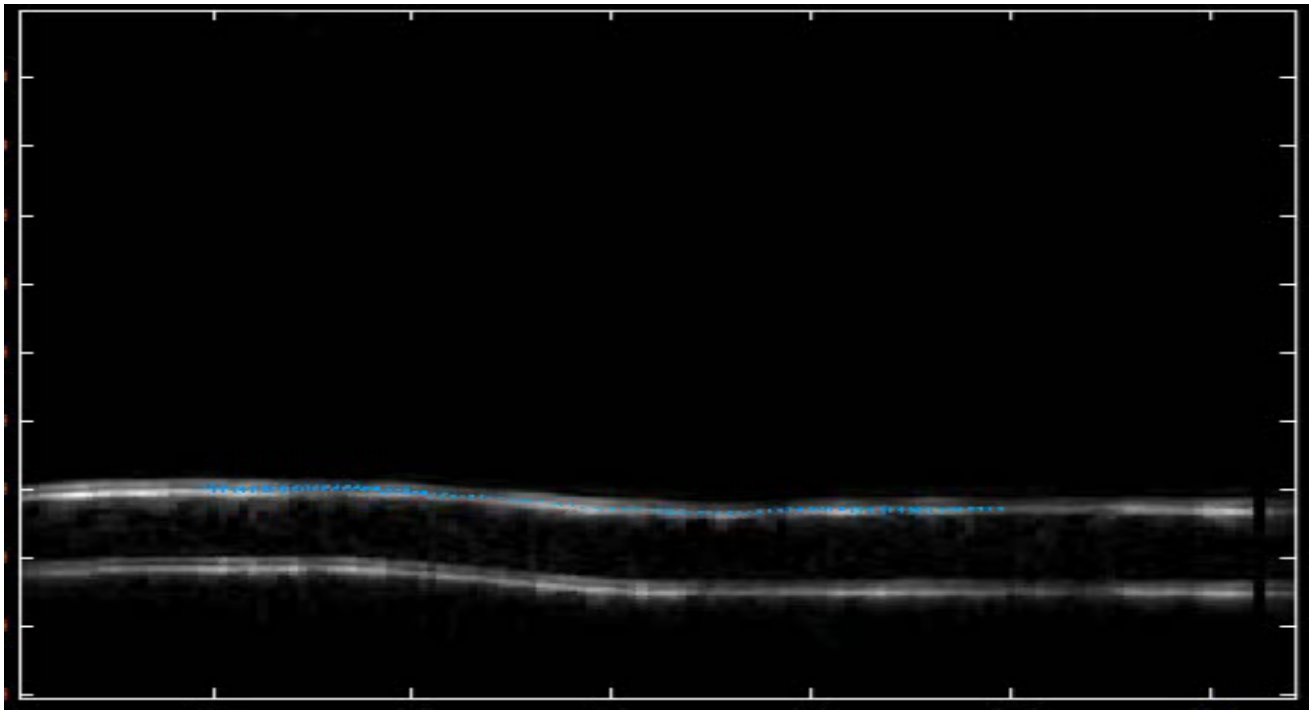
1) Complex motion visualization: arterial wall motion

Phantom: **An PVA Cryogel artery phantom**	**Acquisiton:** **Ultrasonix MDP**
Outer / inner diameter = 9.0 mm / 7.0 mm	128 channels Sonix Daq
peak flow rate = 8.0ml/s	Linear array L14-5W/60 128 elements ; pitch = 472 µm ; f_0 = 5MHz
duty cycle = 10%	PRF = 5000 Hz No compounding → 5000 images/s



Salles et. al. IEEE IUS 2014

1) Complex motion visualization: arterial wall motion

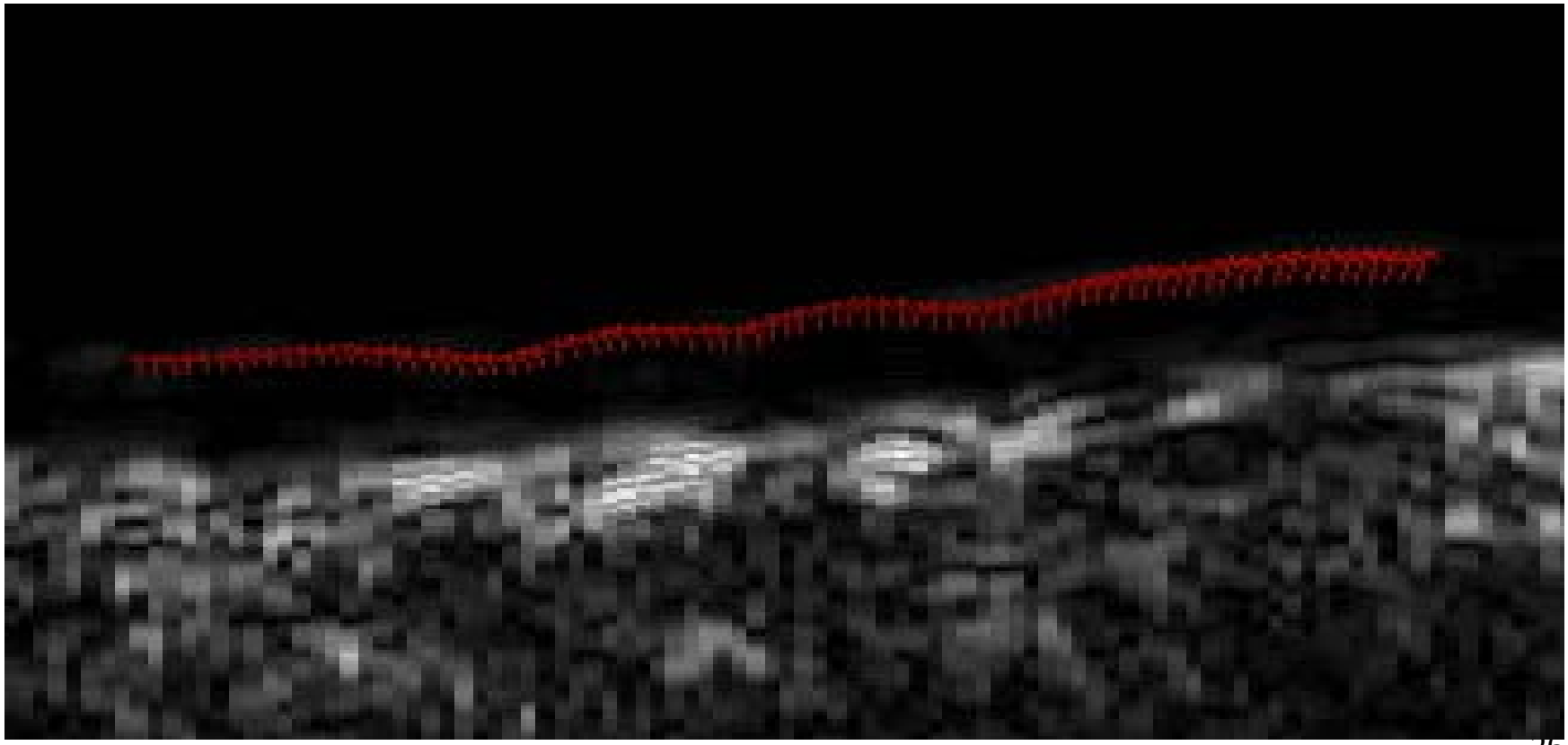


Velocity vector of the arterial wall

Salles et. al. IEEE IUS 2014

1) Complex motion visualization: arterial wall motion

In vivo heathly volunteer carotid artery



Salles et. al. IEEE IUS 2014

WHY Photo-acoustic imaging?

Optical imaging

- ⊕ Contrast
- ⊖ Resolution > ~ 1 mm
- ⊖ Investigation depth < ~ 5 cm
- ⊕ Functional information

Ultrasound imaging

- ⊖ Contrast
- ⊕ Resolution > ~ 100 µm
- ⊕ Investigation depth ~ 10 cm
- ⊖ No Functional information

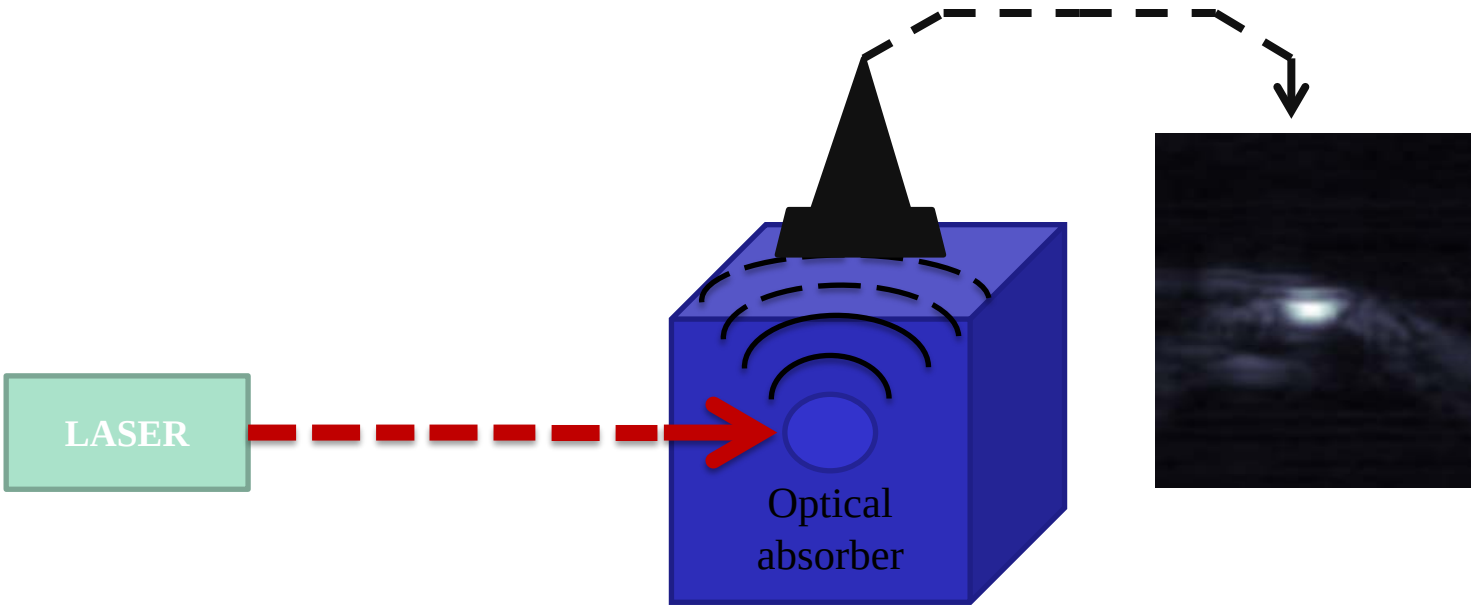
Photo-acoustic imaging

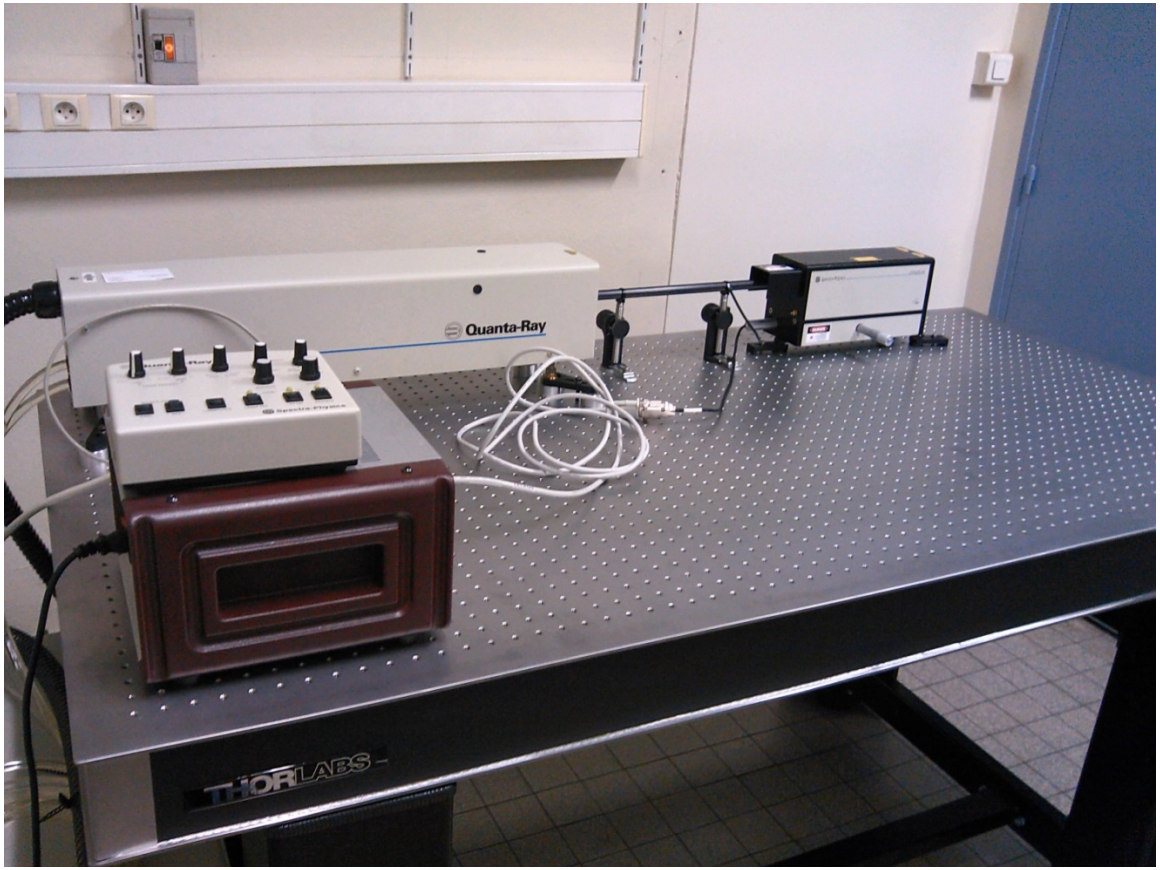
- ⊕ Contrast (optical abosption)
- ⊕ Resolution of Ultrasound
- ⊕ Depth of investigation
- ⊕ Functional information due to optical absorption
- ⊕ Non invasive, non inonizing

Physical principle

Ultrasound generation with light

Laser pulse → **Local absorption by tissues** → **Thermal expansion** → **Acoustic wave**





Courtesy of François Varray, CREATIS, University of Lyon

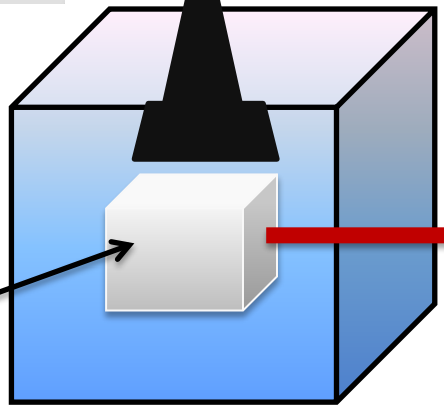
Acquisition setup

All raw RF signals are collected for beamforming

Sonix DAQ

Ultrasonix RP

Phantom



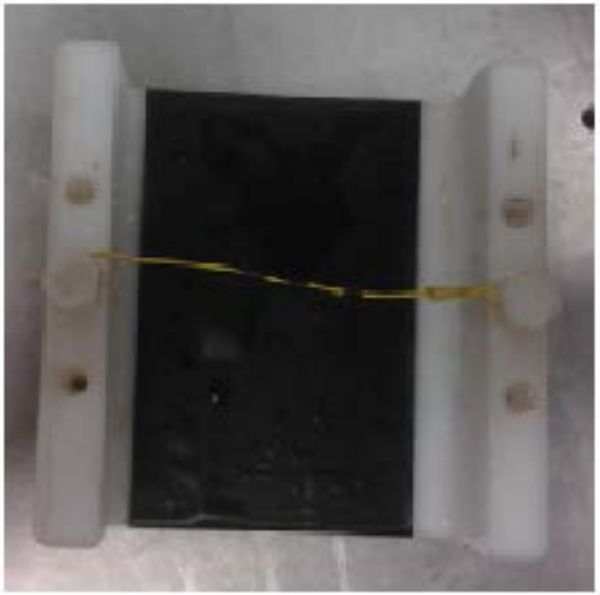
Water tank

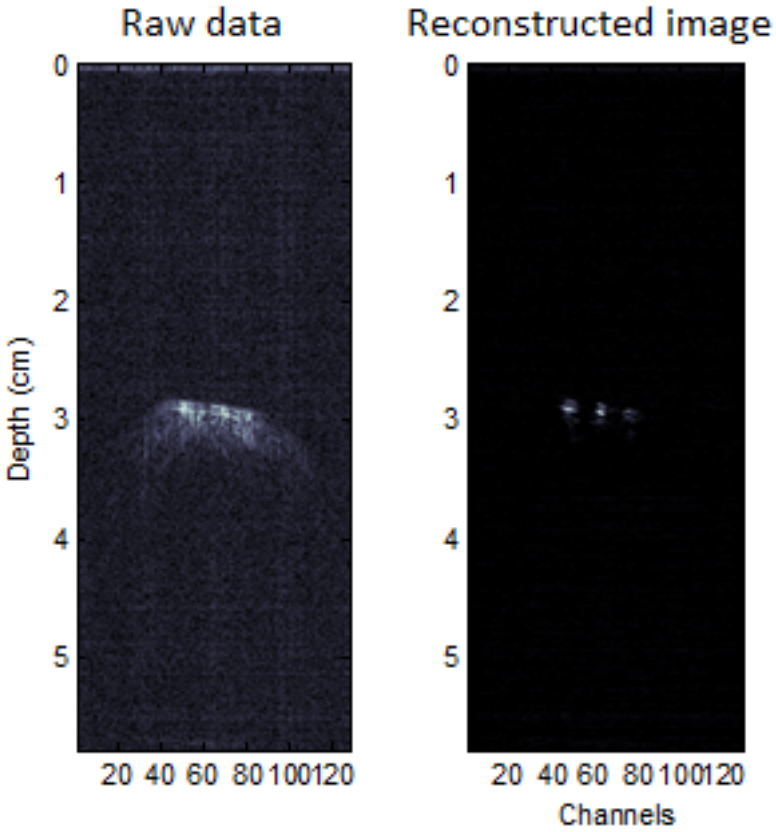
Laser pulse

Courtesy of François Varray, CREATIS, University of Lyon

Simple experiment with wires as absorber

- Several optical absorbers



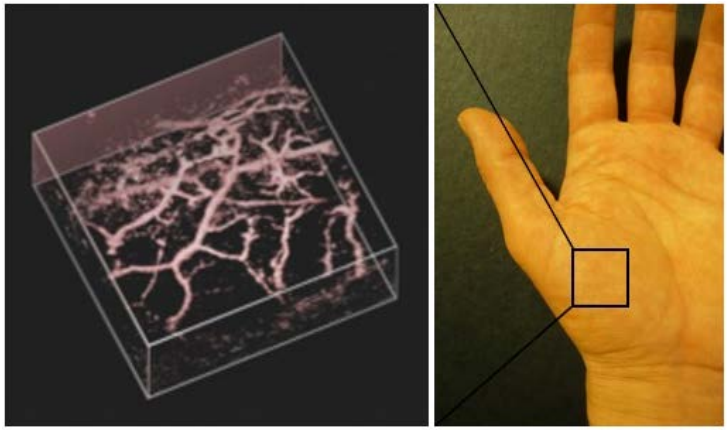


Courtesy of François Varray, CREATIS, University of Lyon

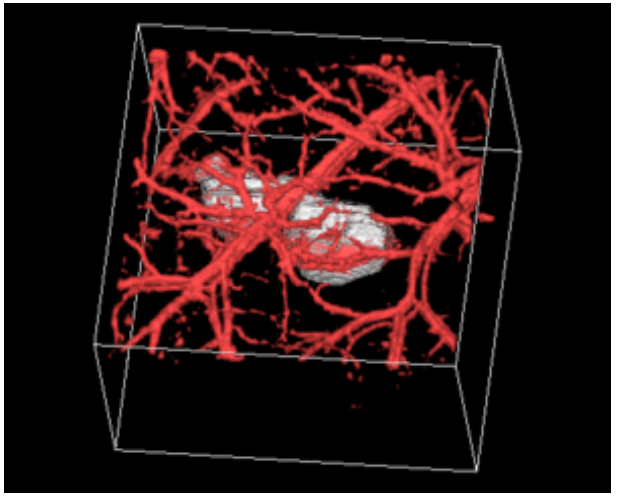
Applications

Vascularization

Cancer ➔ abnormal vascularization

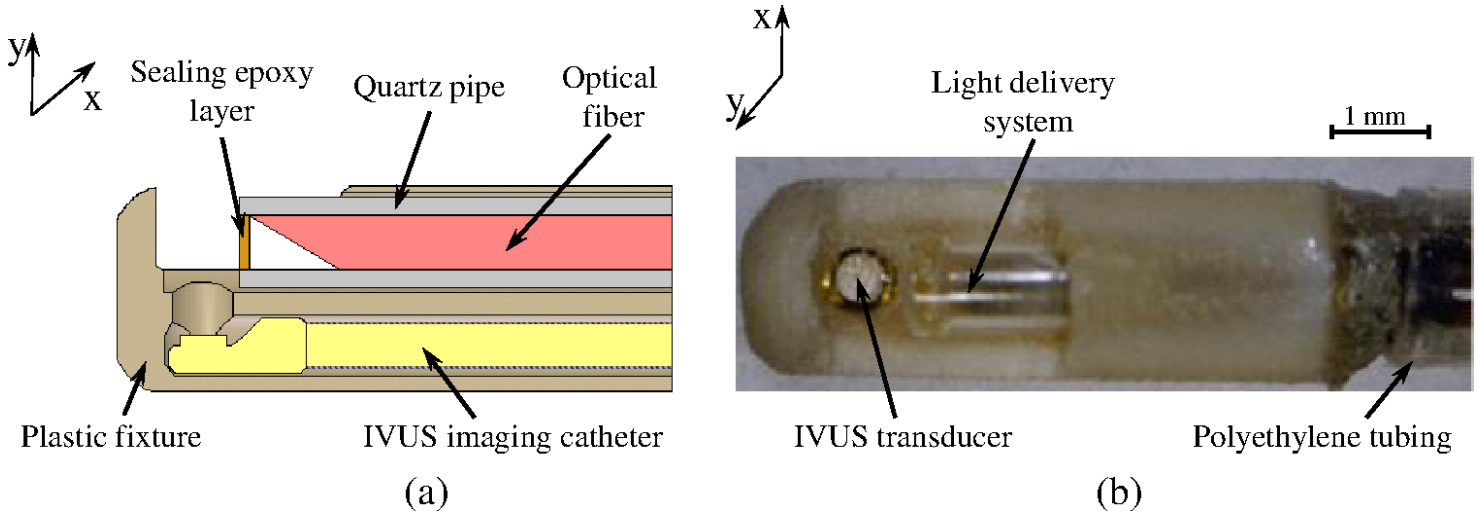


In vivo PA image of the hand vascularization. *UCL PA Imaging Group*



3D photoacoustic imaging of melanoma *in vivo. Zhang et.al. Nature Biotechnology 2006*

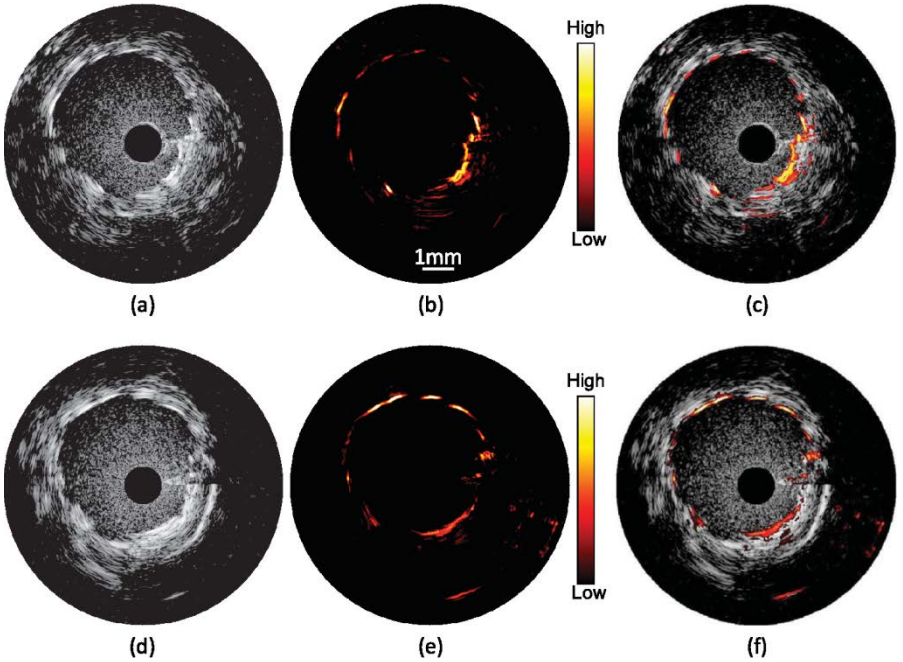
Applications



Karpiouk et.al, *J. Biomed. Opt.* 2012

Intra-vascular photo-acoustic,

vascularization of the plaque



Ultrasound advanced imaging: beyond anatomy!

- Elasticity
- Cardiac function
- Vector flow
- Arterial wall motion
- Functional imaging of the brain (ultrafast imaging or photo-acoustics)
- Vascularization using photo-acoustics