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# Recent developments in the FLUKA tools for treatment planning

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on behalf of the FLUKA group

#### **Treatment Planning Systems for Hadrontherapy**

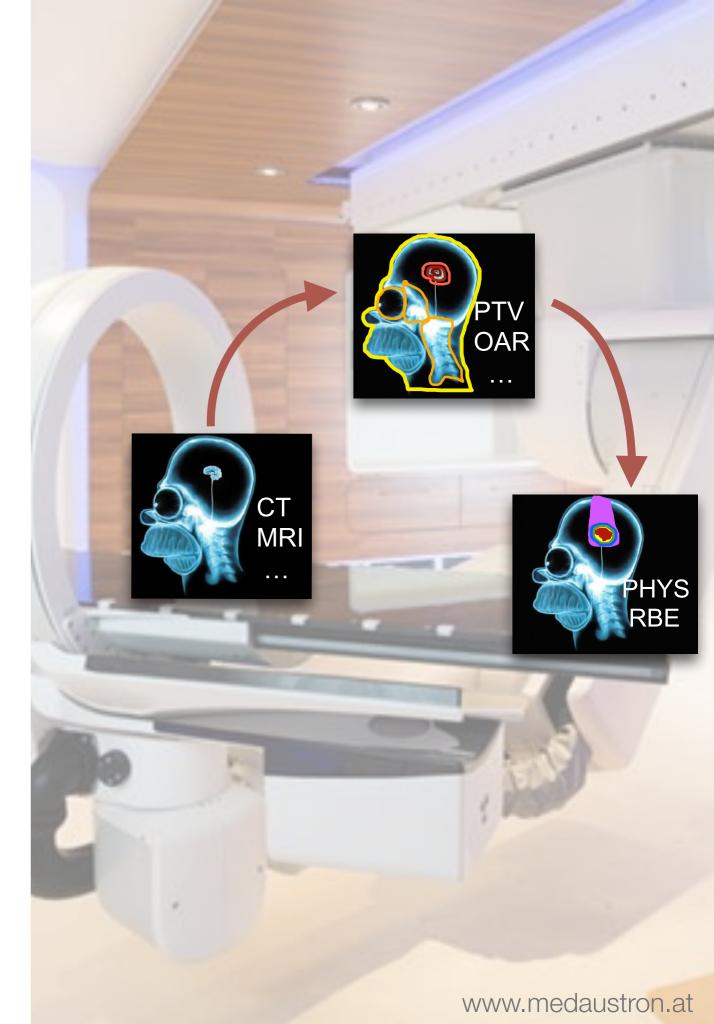
TPS are typically based on **pencil beam scanning algorithms** 

Range of the proton/ion beam is mainly based on the **water** equivalent depth

Lateral beam shape is described by Gaussian or double-Gaussian **parametrisation** 

Analytical TPS enables **fast** dose calculations and **fast** optimisation

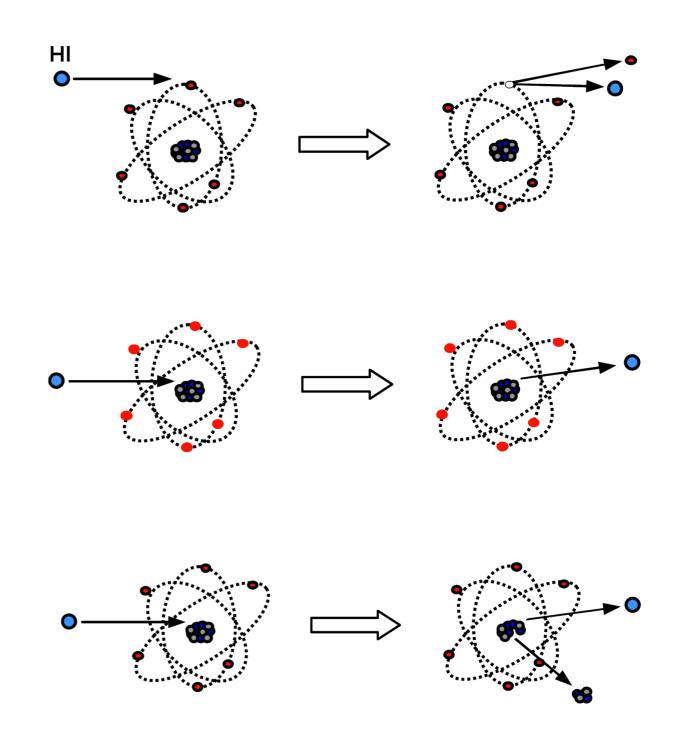
Why do we need Monte Carlo TPS?



## Monte Carlo Treatment Planning System

Faithful consideration of the **radiation transport and interactions with matter:** 

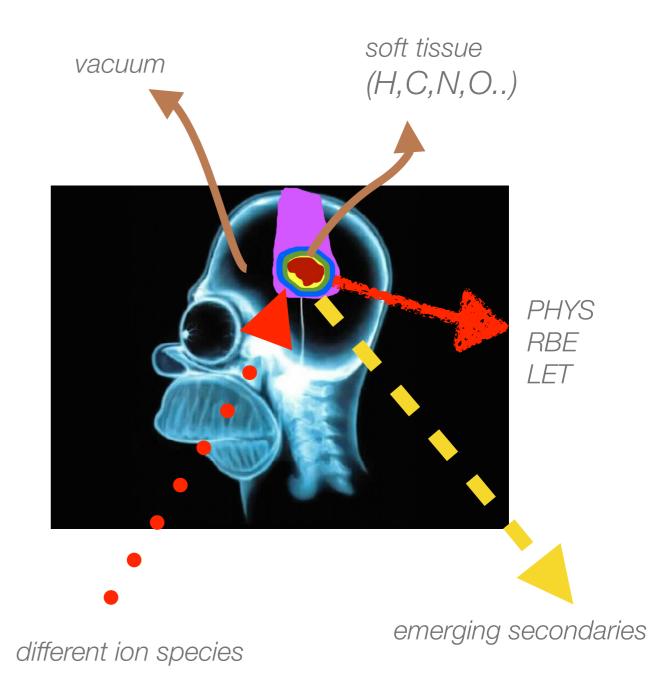
- Energy Losses through collisions with atomic electrons (Bethe-Bloch formula with its corrections)
- Nuclear Reactions (i.a. fragmentation tails, other secondary particles..)
- Multiple Coulomb Scattering (mostly elastic scattering deflection)



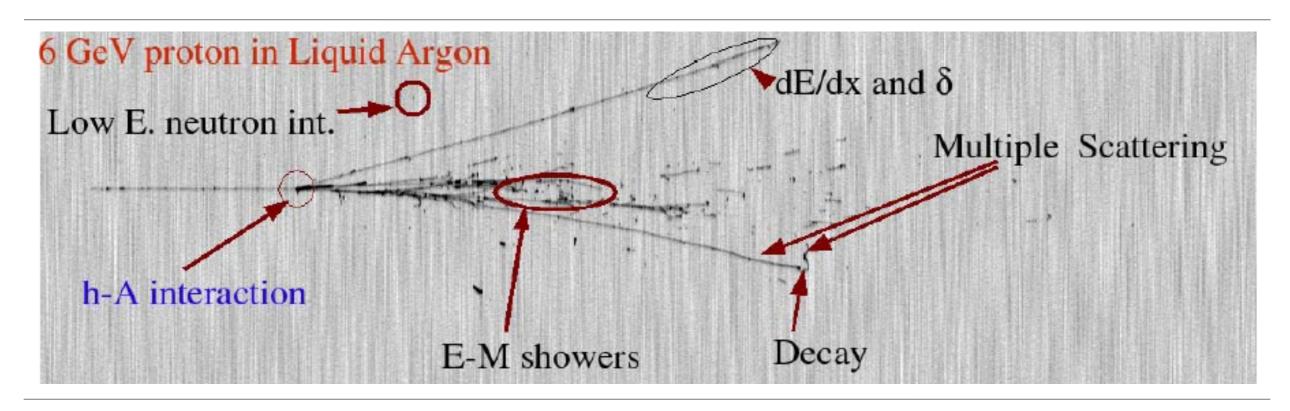
### Monte Carlo Treatment Planning System

Capable of handling all components of the expected radiation field

- Realistic atomic composition of the patient tissue, limited by the HU to tissue conversion
- Scoring not only physical dose, but also **RBE** dose, dose-weighted **LET**
- Accurate prediction of emerging secondaries for in vivo studies
- Protons and light ion beams



#### **Interactions and Transport Monte Carlo Code**



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- **FLUKA**<sup>[1][2]</sup> is a general purpose Monte Carlo code
- Joint CERN-INFN project, and is continuously undergoing development and benchmarking
- Maintained and developed under INFN-CERN
   agreement and copyright
- More than 9000 users worldwide

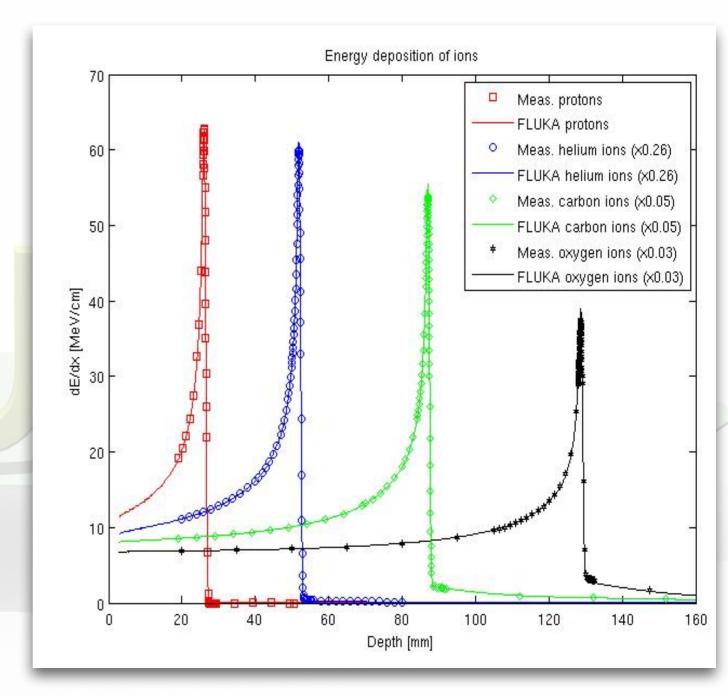
#### **FLUKA Short Description**

# FLUKA is a general purpose tool for calculations of particle transport and interactions with matter

- All Hadrons (p, n, K, pbar, nbar, (anti)hyperons...)
- Electromagnetic (, e+/-) and  $\mu$  and  $\nu$
- Nucleus-nucleus
- Low energy neutrons (0-20 MeV, multigroup, ENDF...)
- Full mixed field capability
- Transport in magnetic field
- Combinatorial (boolean) and Voxel geometries
- Double capability to run either fully analogue and/or biased calculations
- On-line evolution of induced radioactivity and dose
- Radiation damage predictions (NIEL, DPA)
- User-friendly GUI interface thanks to the Flair interface

# FLUKA for Medical Applications

- At HIT and CNAO (p and C-12)
  - TPS data generation, verification/optimization
  - Research: new beams, therapy monitoring
  - RBE model comparison NIRS
     vs. CNAO in carbon ion
  - **European Projects:** 
    - ENVISION/ENTERVISION (β+ emitters, prompt gamma, emerging charged particles
    - OMA Optimization of Medical Accelerators



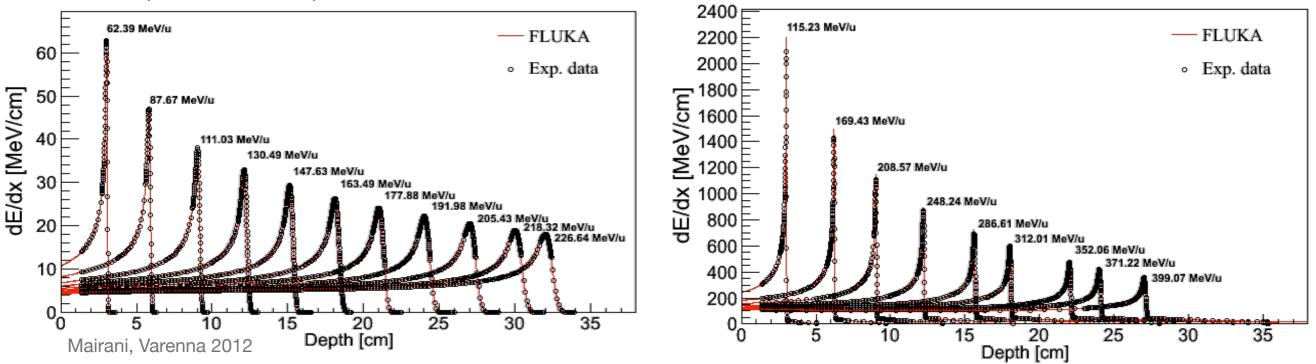
FLUKA simulations of depth–dose profiles of protons and light ions with therapeutic ranges in comparison with measured data at HIT [5]

#### Generating depth-dose distribution for TP database

Physics well established. Thoroughly **benchmarked** at single interaction level; i.a. **against depth–dose data and lateral-dose profiles** used for proton and ion-beam therapy

Depth-dose distribution of protons (CNAO) in water wo/with RiFi for the 147 energies in the initial phase of the operation

Depth-dose distribution of C-12 (HIT)



Courtesy of: Med Phys Group at CNAO and HIT



Flair<sup>[3]</sup> provides an IDE for all stages of FLUKA simulations (input, geometry editor, debugging, post-processing output visualization)

is more than a graphical Interface - it is a **complete integrated working environment** for FLUKA

#### **Front-end**

Fully featured Input file Editor;

Geometry: interactive visualization editing, and debugging;

Compilation of the FLUKA Executable;

Running (Spawning on multi-core) and monitoring of the status of one/many run(s)

**Back-end** 

Post processing of FLUKA output

Plot generations with gnuplot

Photorealistic 3D plots with USRBIN data superimposed

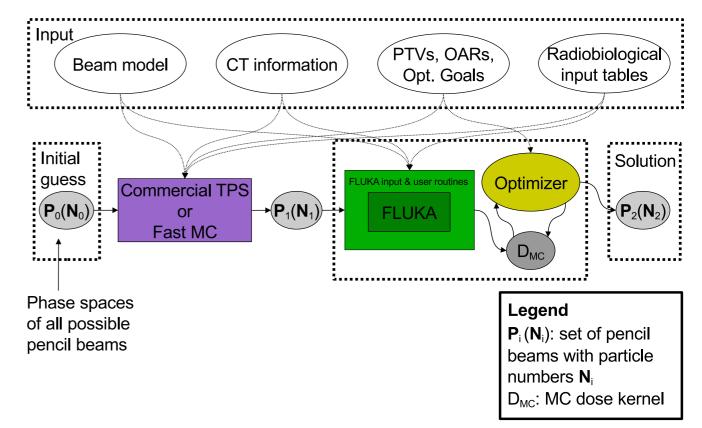
#### Other

Database of Materials, Isotopes FLUKA hypertext manual

. . .

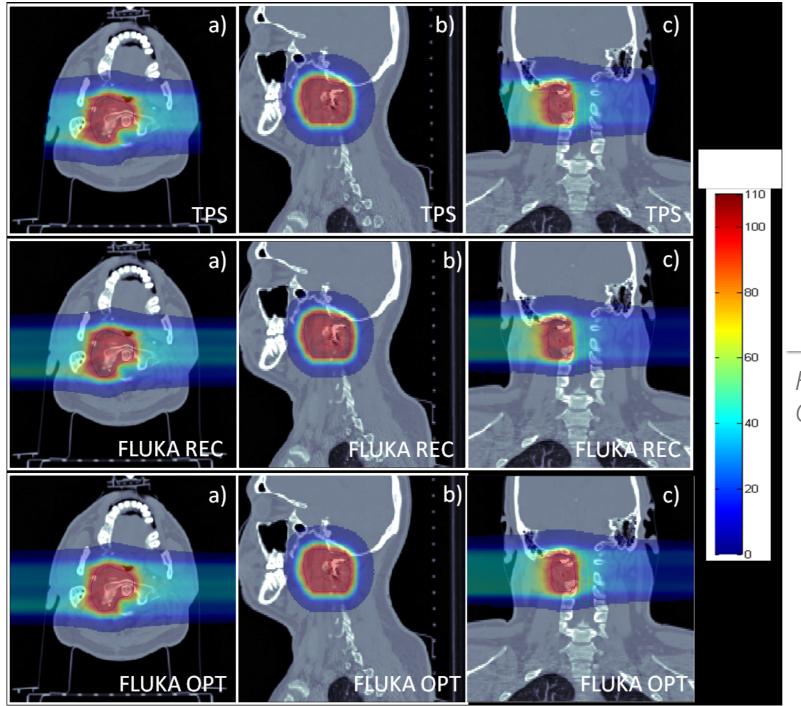
#### **FLUKA based MC Treatment Planing**

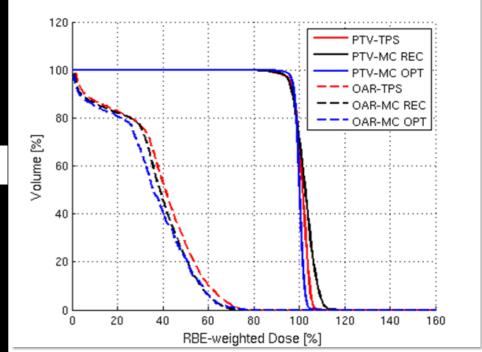
- To account for geometry and material details and applying realistic treatment conditions within acceptable CPU time
- To suggest a better solutions
- To be used stand-alone or as post re-optimization of TPS plans
- To be used in research: New ions and combined ion fields, testing of new biomodels



Software architecture of the FLUKA MC TPS [4]

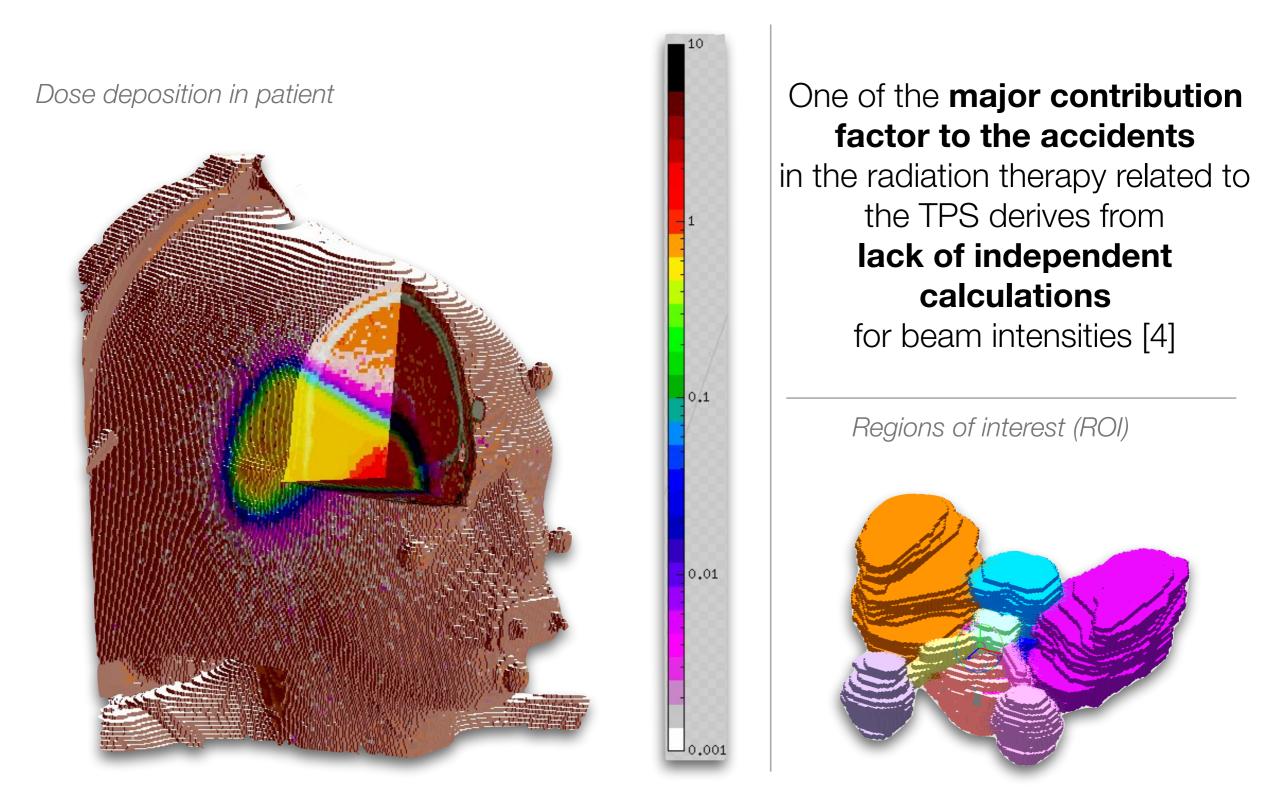
#### **FLUKA based MC Treatment Planning**



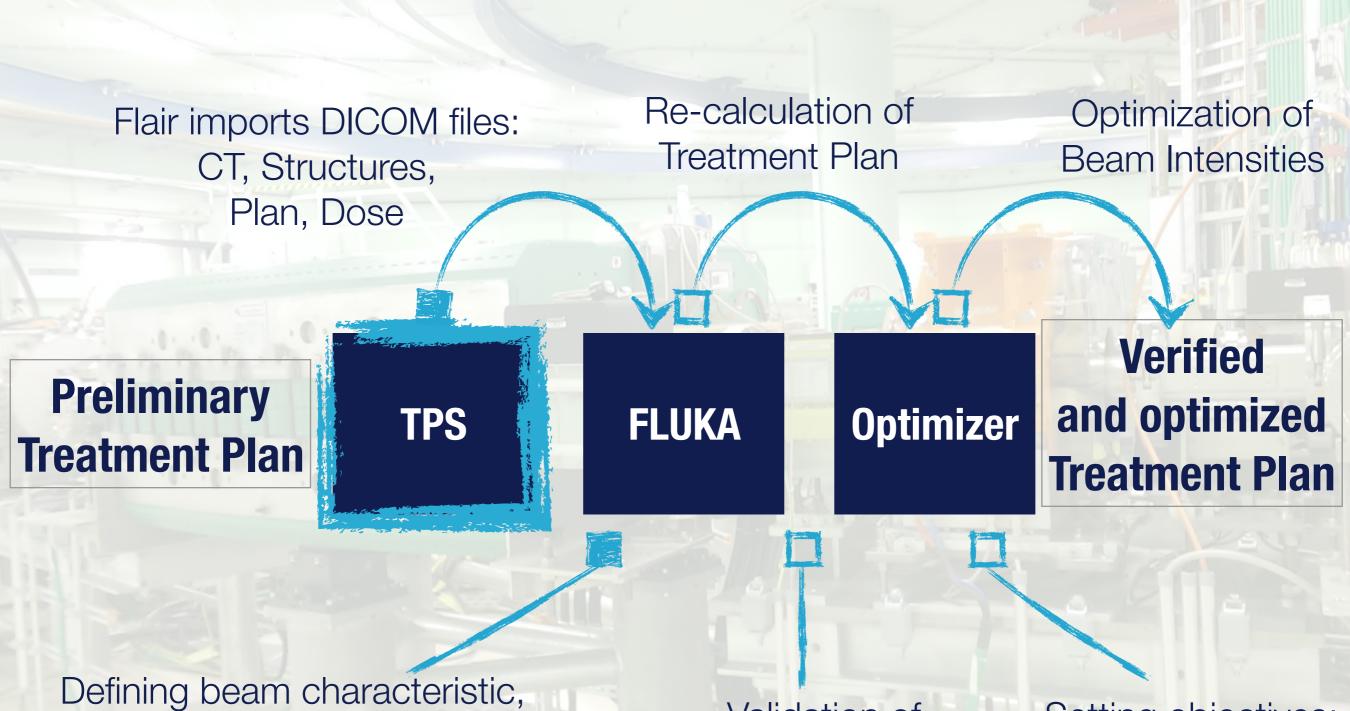


FLUKA RECalculation and FLUKA OPTimization of proton TPS at CNAO<sup>[4]</sup>

Monte Carlo Simulations are considered as a gold standard for dosimetric calculations in medical physics, although time is the main issue



#### **FLUKA** and its GUI Flair for Hadrontherapy TPS



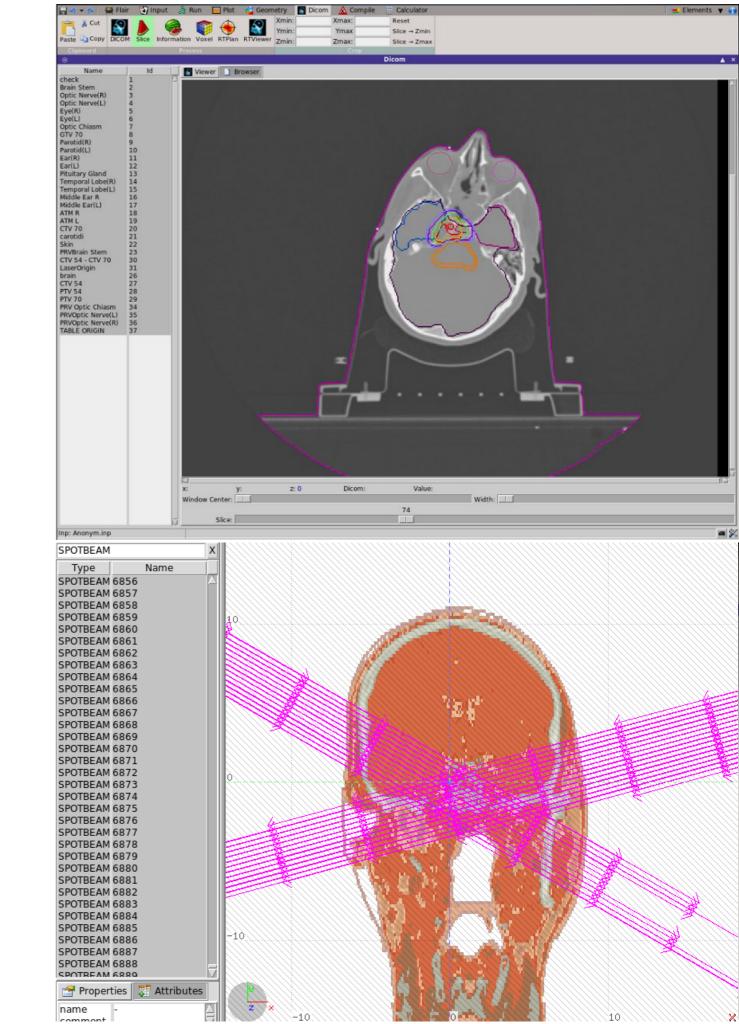
nozzle design

Validation of treatment plan

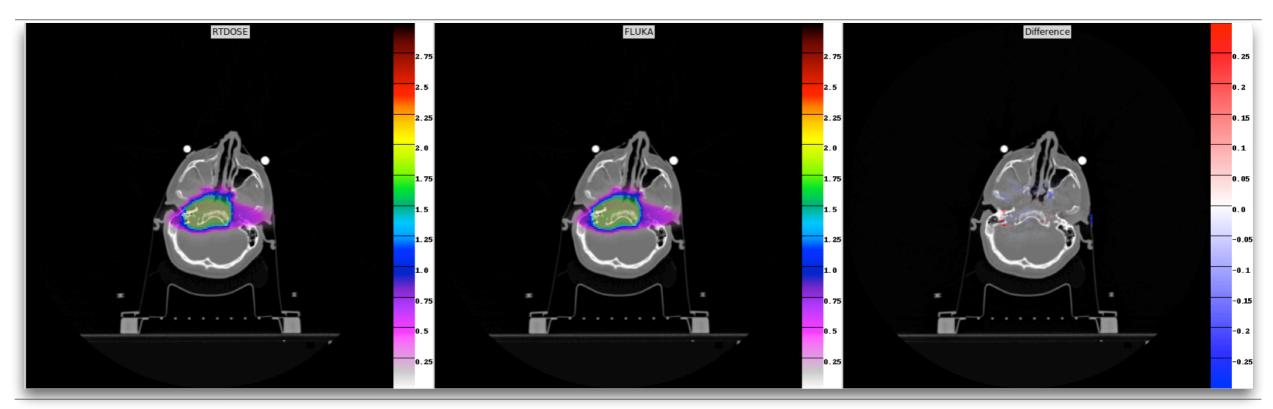
Setting objectives; Dose, LET<sub>d</sub>

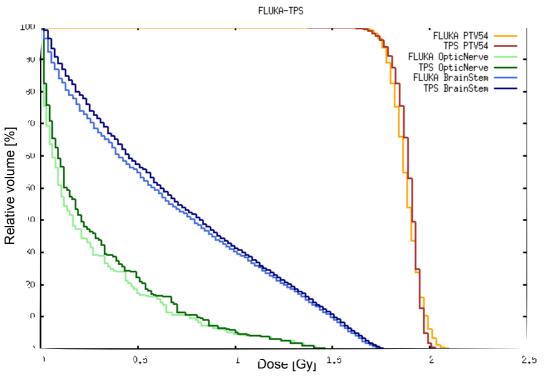
### FLUKA and its GUI Flair for Hadrontherapy TPS

- Process **DICOM standard files** for radiotherapy purposes
  - DICOM CT, MRI importer
  - Automatic material assignment using the Schneider parameterization
  - Importing ROI RTStructures
- Provides easy-to use tool for treatment plan re-simulation and quantitative comparison
  - Importing RTPlan
  - Generation of the DVH plots and comparison with the RTDOSe
  - Enables precise description of patient model and beam delivery system



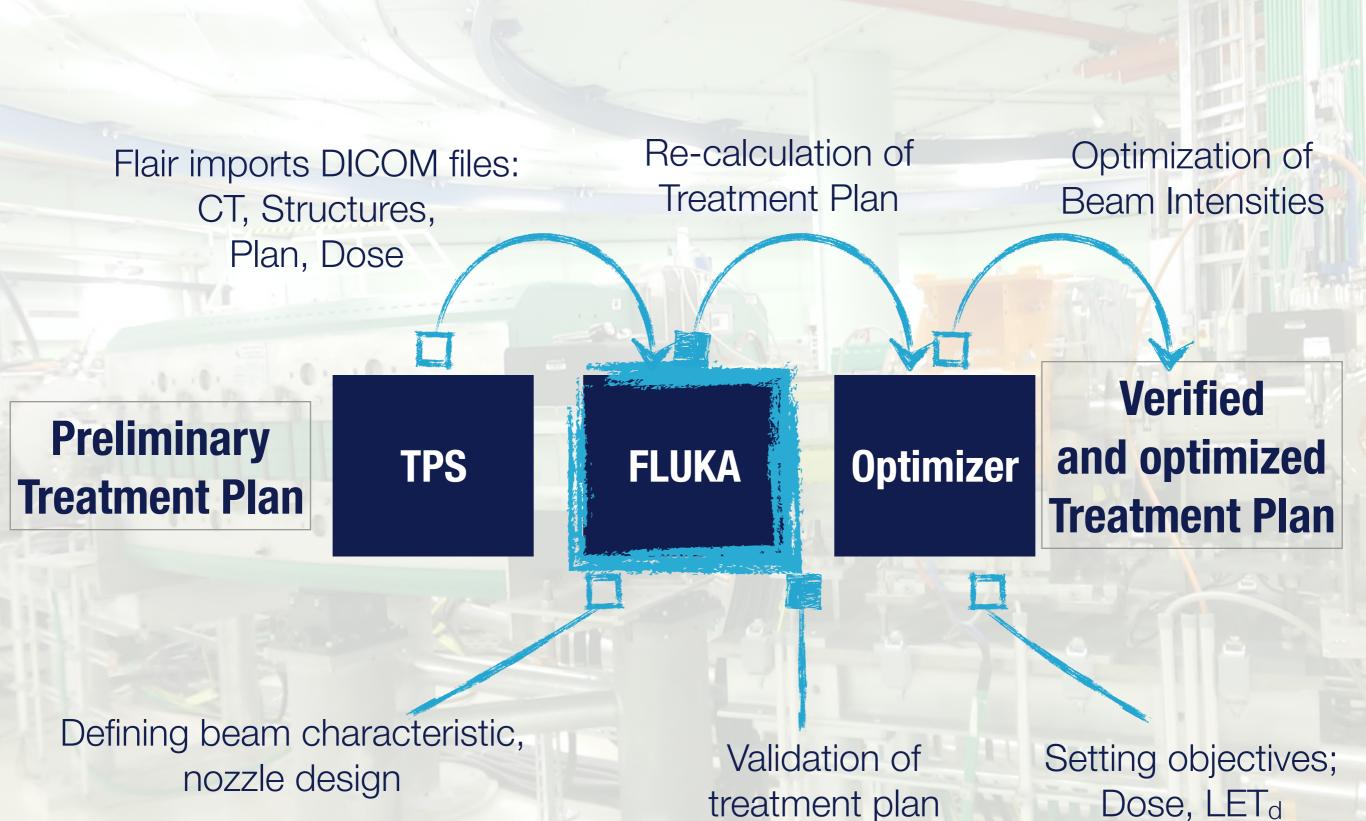
#### **Monte Carlo Treatment Plan recalculations**





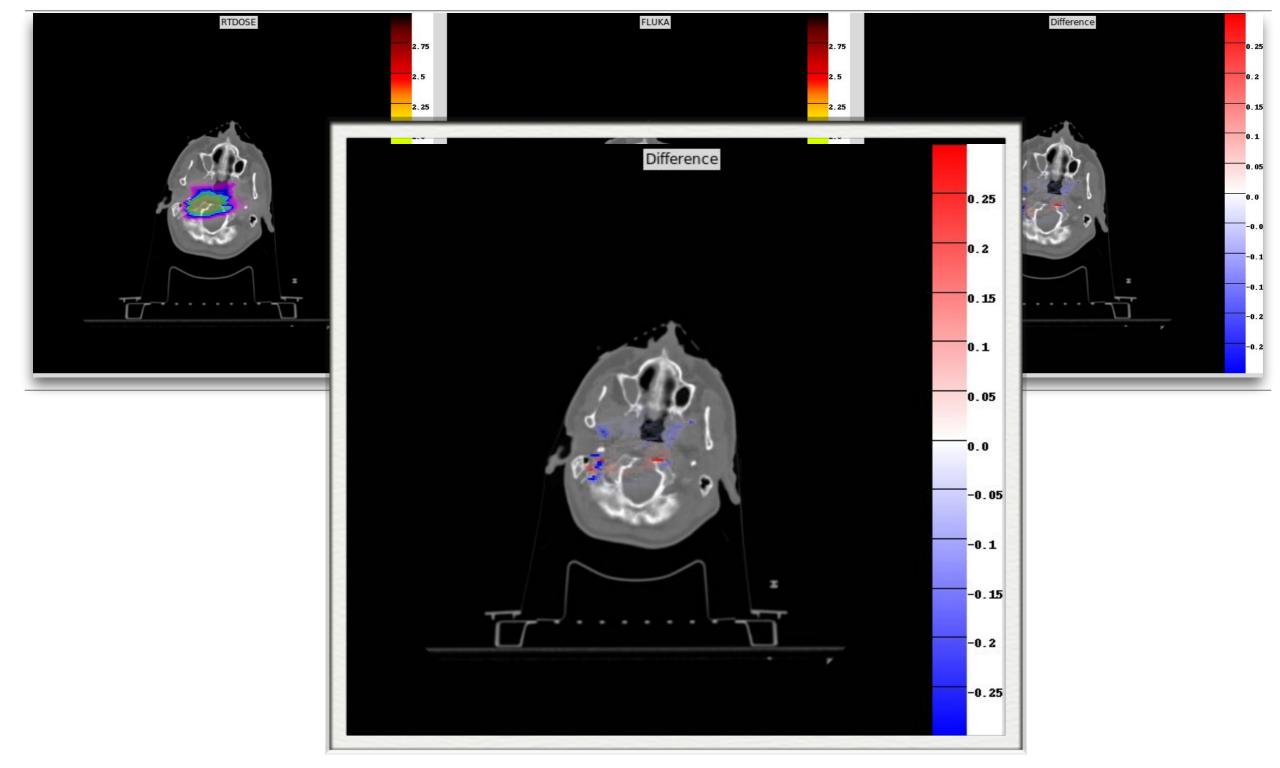
Proton chordoma patient case (CNAO)

- Calibration of HU to density
- HU to tissue conversion methods
- Ionization potentials of tissue materials
- Accuracy of primary beam description
- Biological dose and LET calculations



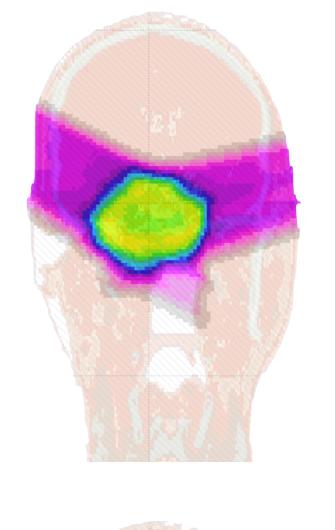
# Monte Carlo Treatment Plan recalculations for hadrontherapy / sensitivity studies

Proton chordoma patient case



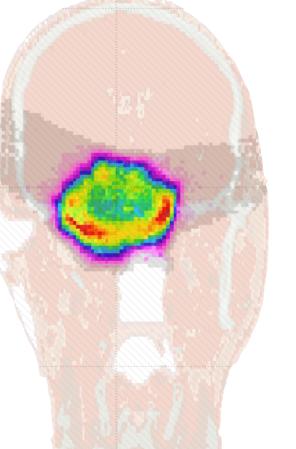
### Linear Energy Transfer (LET)

- LET is average amount of energy a particular radiation imparts to the local medium per unit length
- There is a significant correlation between the dose-averaged LET and RBE
- High-LET particles can reduce the response factor OAR (oxygen enhancement ratio) leading improvement of the treatment outcome for hypoxic radioresistive tumors



DOSE

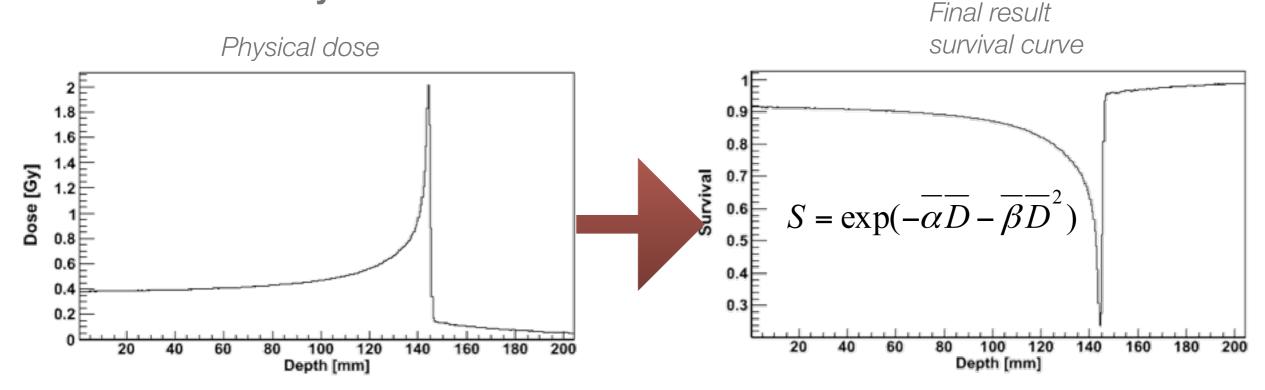
LET d



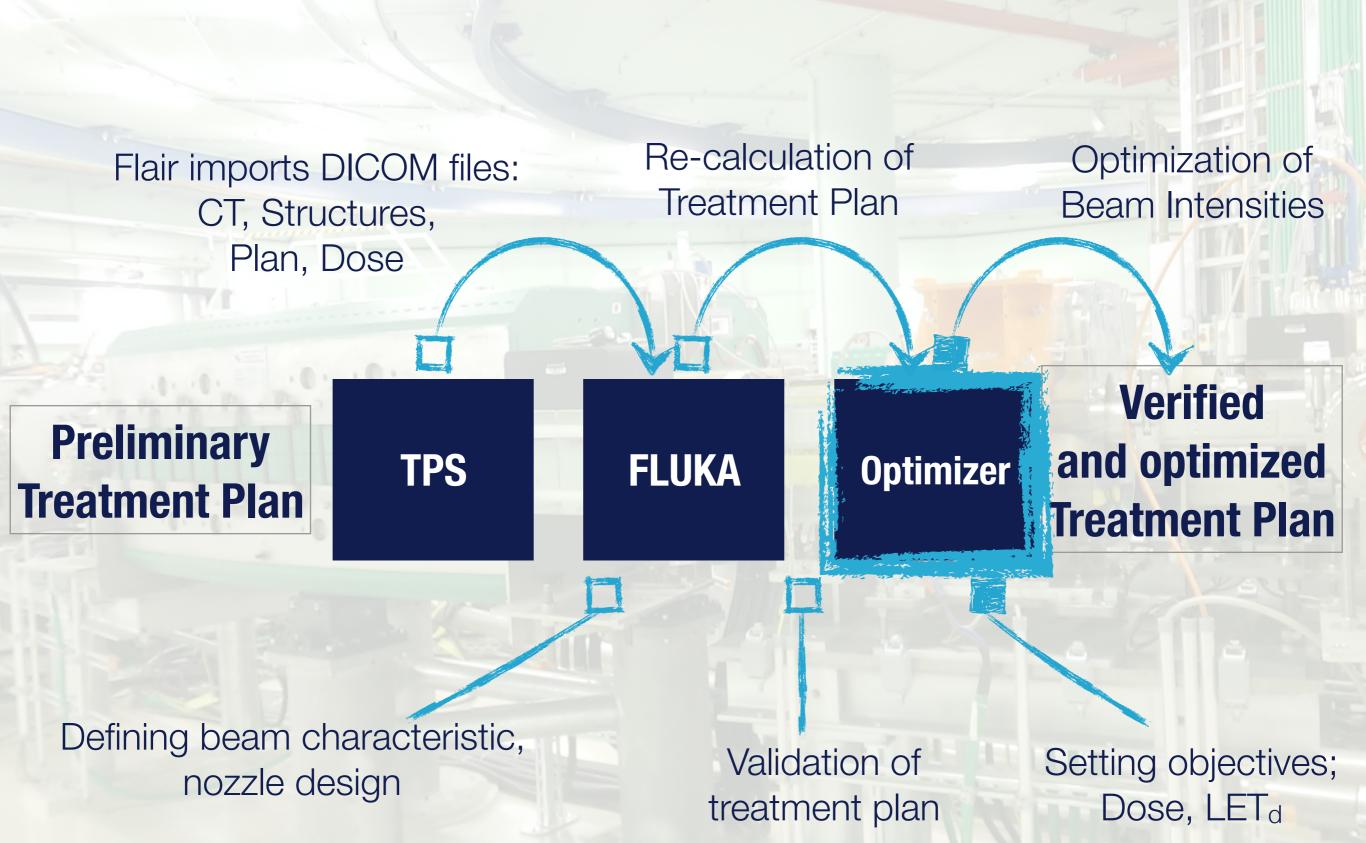
keV/um

#### **Biologically Oriented Scoring**

- Under the standard assumption of a linear-quadratic dose-effect relationship, for each energy deposition i, FLUKA interpolates from a radiobiological database the αD,i and βD,i parameters for the specific ion with a certain charge at a certain energy.
- Then FLUKA sums up properly the mixed radiation effect applying the Kellerer
   and Rossi theory of dual radiation action

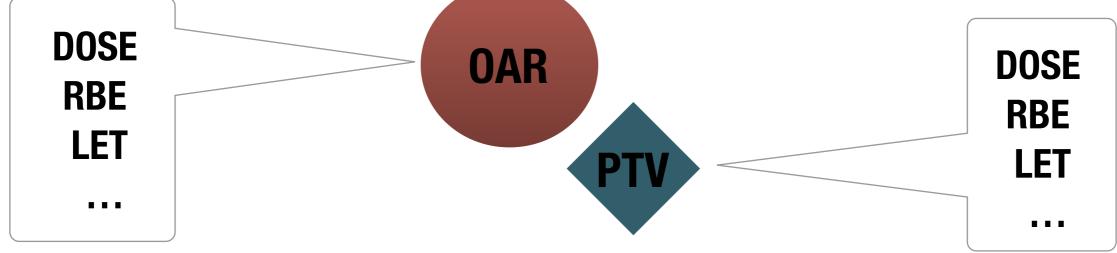


270 MeV/u C-12 ions on V79 cell line



#### **Goals of the MC Treatment Plan Optimization**

Re-simulation and validation of the Treatment Plan

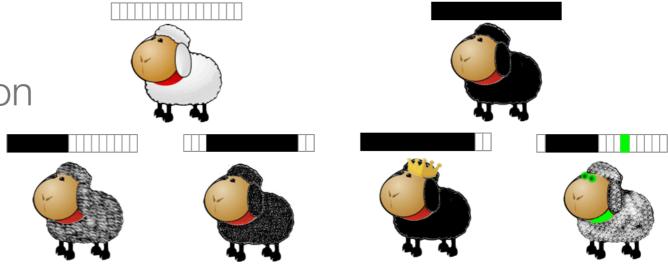


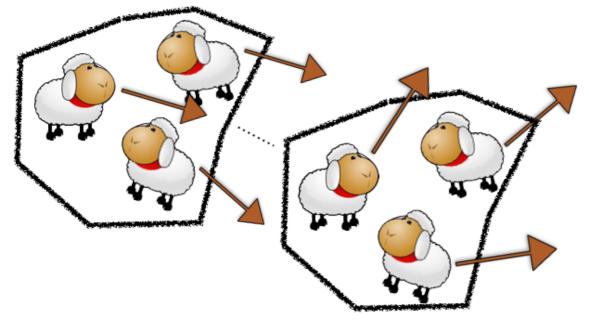
- Development of the framework for quick comparison of algorithms for dose/RBE/LET optimization based on MC output
- Evolutionary based algorithm for better space search: Genetic Algorithms, Particle Swarm Algorithm ..
- Development of the MultiObjective optimization algorithms

### **Evolutionary algorithms for TPS -MultiObjective Problems**

#### **Genetic Algorithm Optimization**

Each iteration creates new population using cross-over methods from parent individual solutions



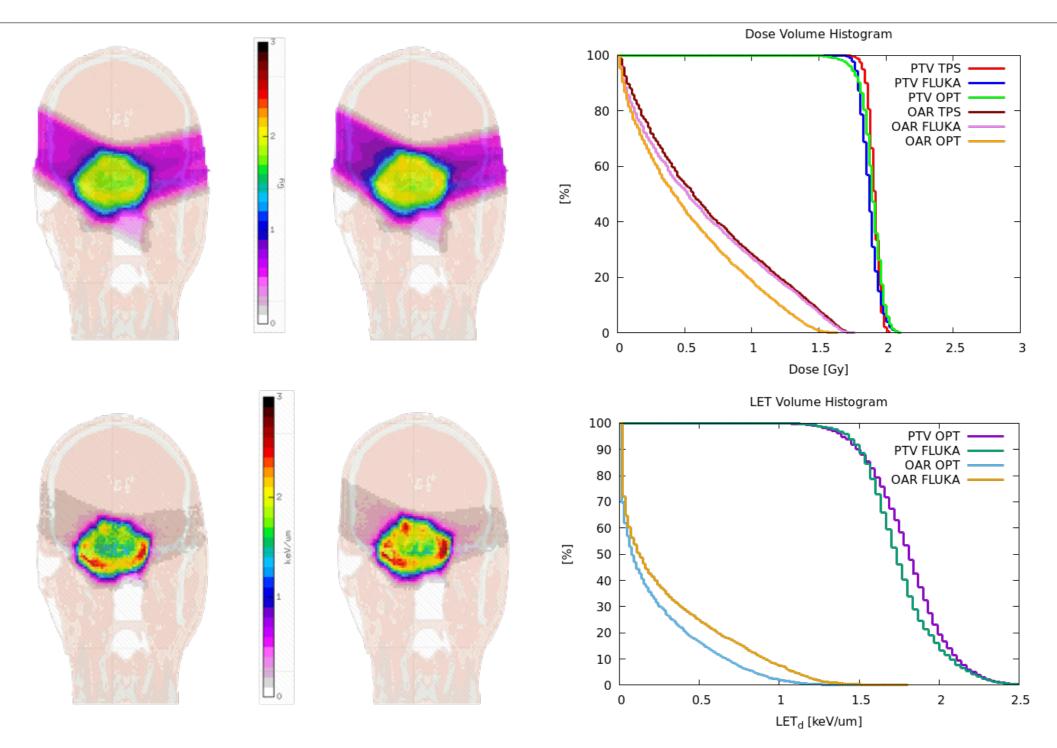


#### **Particle Swarm Optimization**

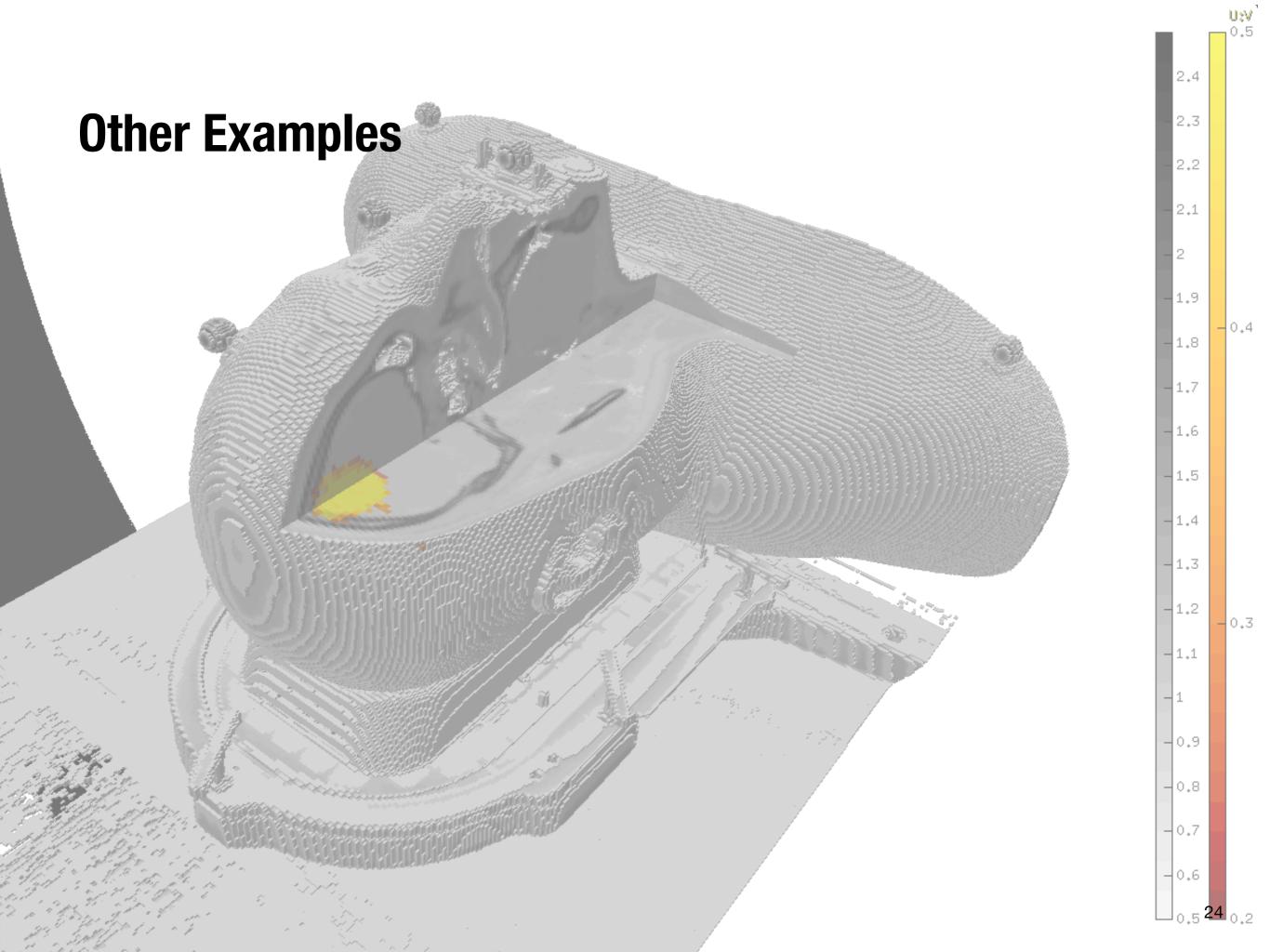
During iterations particles are moving in the search space of the optimization problem changing its position - solutions.

MultiObjective EA - ongoing work with preliminary results

#### Particle Swarm Algorithm for Dose/LET optimization



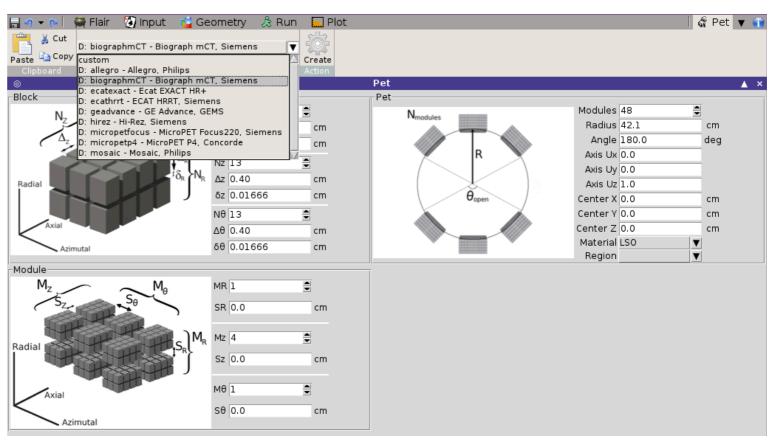
Proton TPS - physical dose distribution (top) and LETd distribution (bottom) for FLUKA TPS simulation (left) and FLUKA optimized recalculation (middle), with accompanying Physical Dose-Volume and LET-Volume Histograms 23

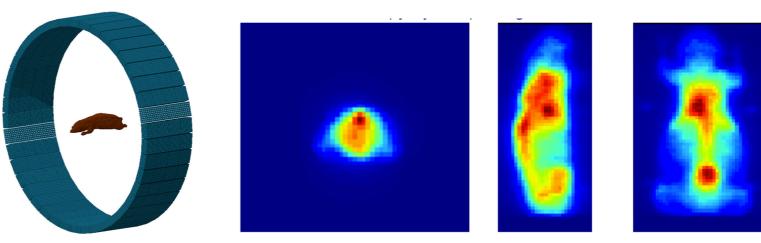


### **PET simulations**

Incorporated **dedicated PET scanner tool**, covering all steps from PET **ring creation** to the **reconstruction** of the image from coincidence events

- Useful for:
  - Inferring the dose map from the β+ emitter distribution
  - Test new PET design/ options





#### **Imaging potential of Radioactive Ion Beams**

#### Different Radioactive Ion

100000

10000

1000

100

5

8.5

11.5

Depth in water (cm)

15

Events per second

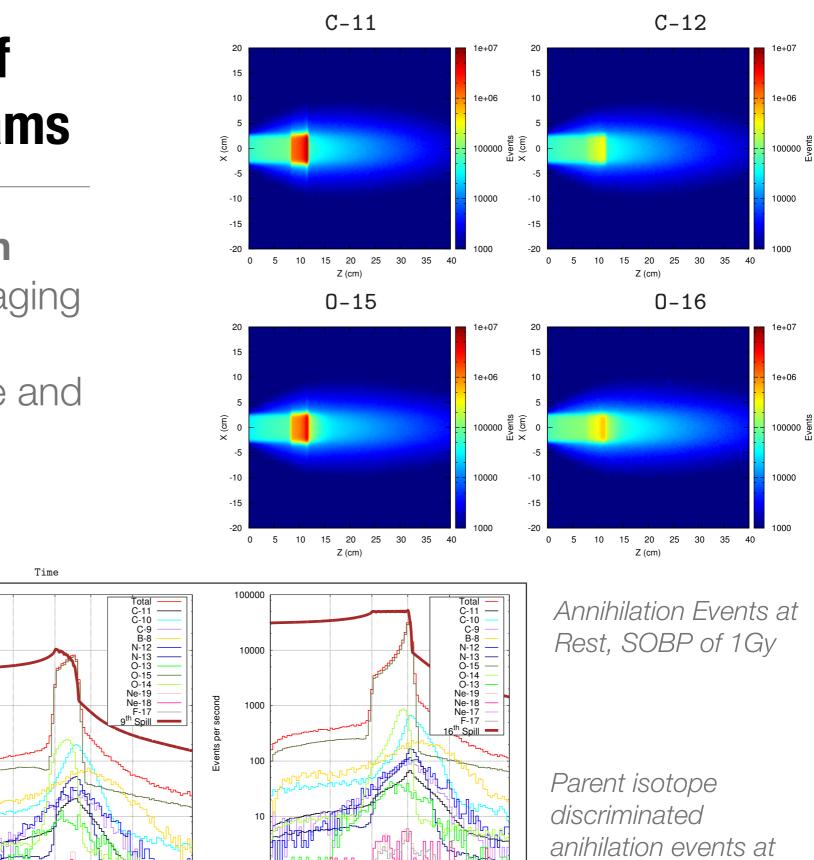
**Beams** have different imaging potentialities, depending of their half-life and the half-life of produced fragments

Tota

C-11 C-10 C-9 B-8

N-12

N-12 N-13 O-15 O-13 Ne-18 1<sup>st</sup> Spill



8.5

Depth in water (cm)

11.5

15

20

rest rate

Courtesy of: Ricardo dos Santos Augusto (CERN/LMU) 26

20

100000

10000

1000

100

8.5

Depth in water (cm)

11.5

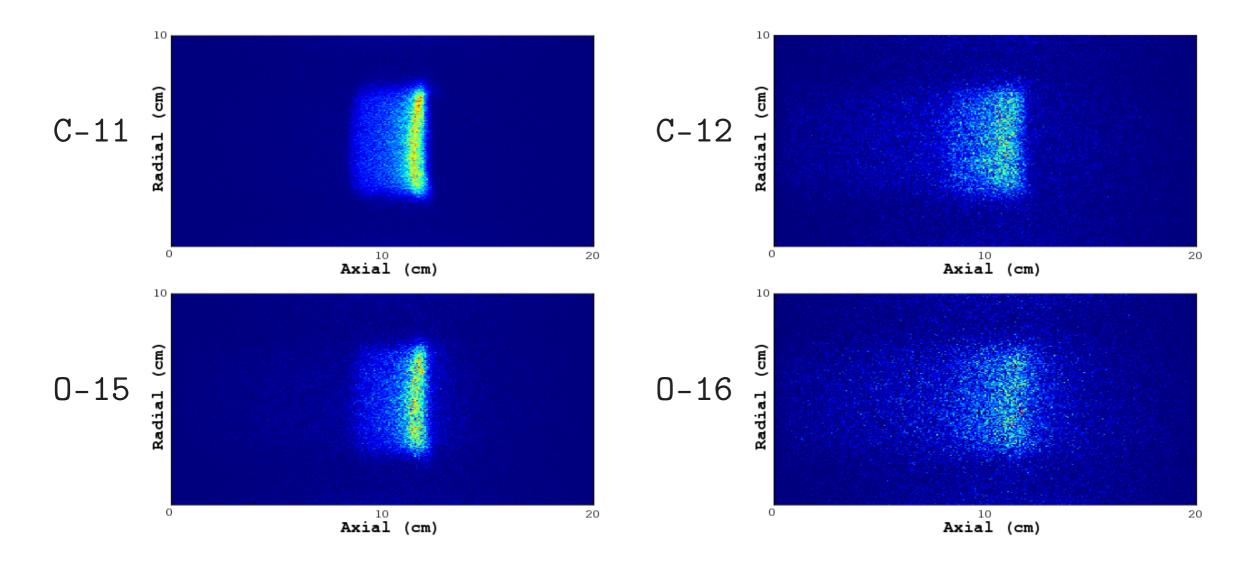
15

20

Events per second

# Range Monitoring Results - Offline Acquisition (from 5 to 30 minutes EOB)

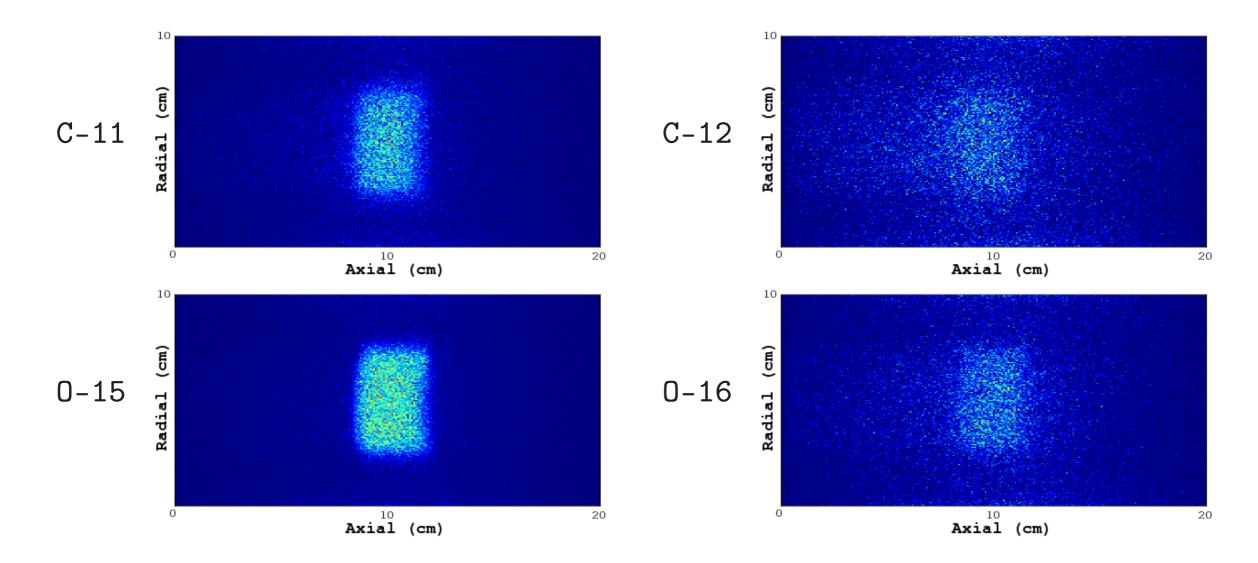
Due to the half-life difference between C-11 and O-15 (~20m & ~2m) - C-11 outperforms O-15 in longer acquisitions after irradiation.



Courtesy of: Ricardo dos Santos Augusto (CERN/LMU)

#### Range Monitoring Results -Online Acquisition (beam time duration of 130 s)

Online acquisition modalities are most advantageous for they mitigate the degradation of dose-PET correlation due to biological washout.

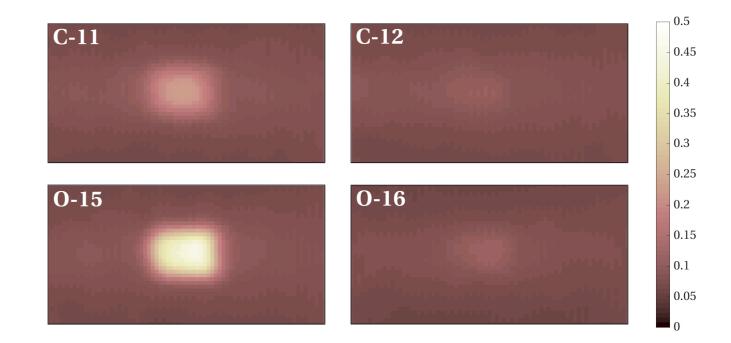


Courtesy of: Ricardo dos Santos Augusto (CERN/LMU)

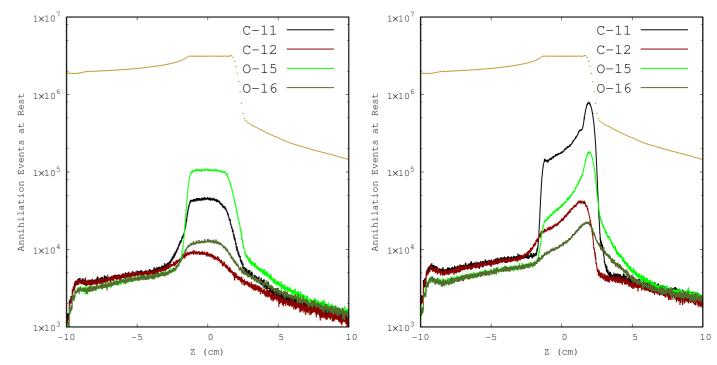
# Accounting for the beam time structure

**PET imaging can be significantly improved with RIBs**, in both online and offline PET modalities, without apparent dose drawbacks.

An attempt to validate the simulation results with experimental data from NIRS-HIMAC is ongoing - to be published in November



PET Sinogram file reconstruction using MLEM Code

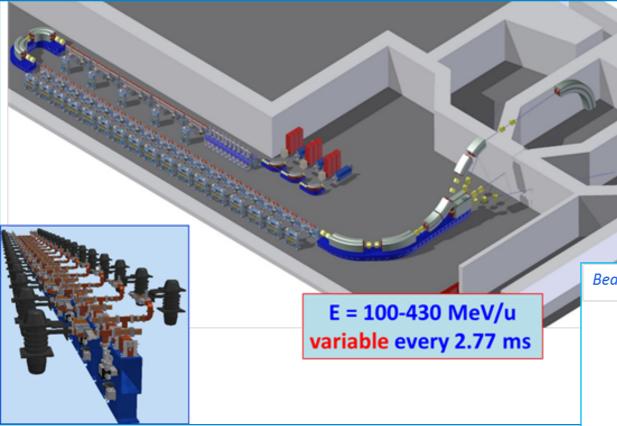


Annihilation events at rest produced during online (left) and offline (right) acquisition (SOBP dose in AU, golden points).

Courtesy of: Ricardo dos Santos Augusto (CERN/LMU)

#### **Two projects of TERA Foundation under development**







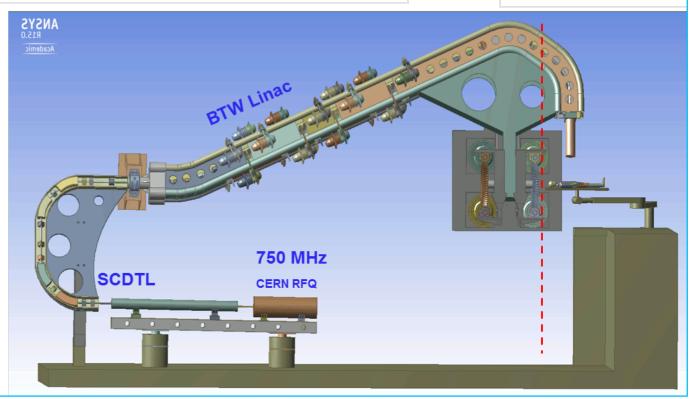
#### **TULIP- TUrning Linac for Protontherapy**

Beam production and transport system

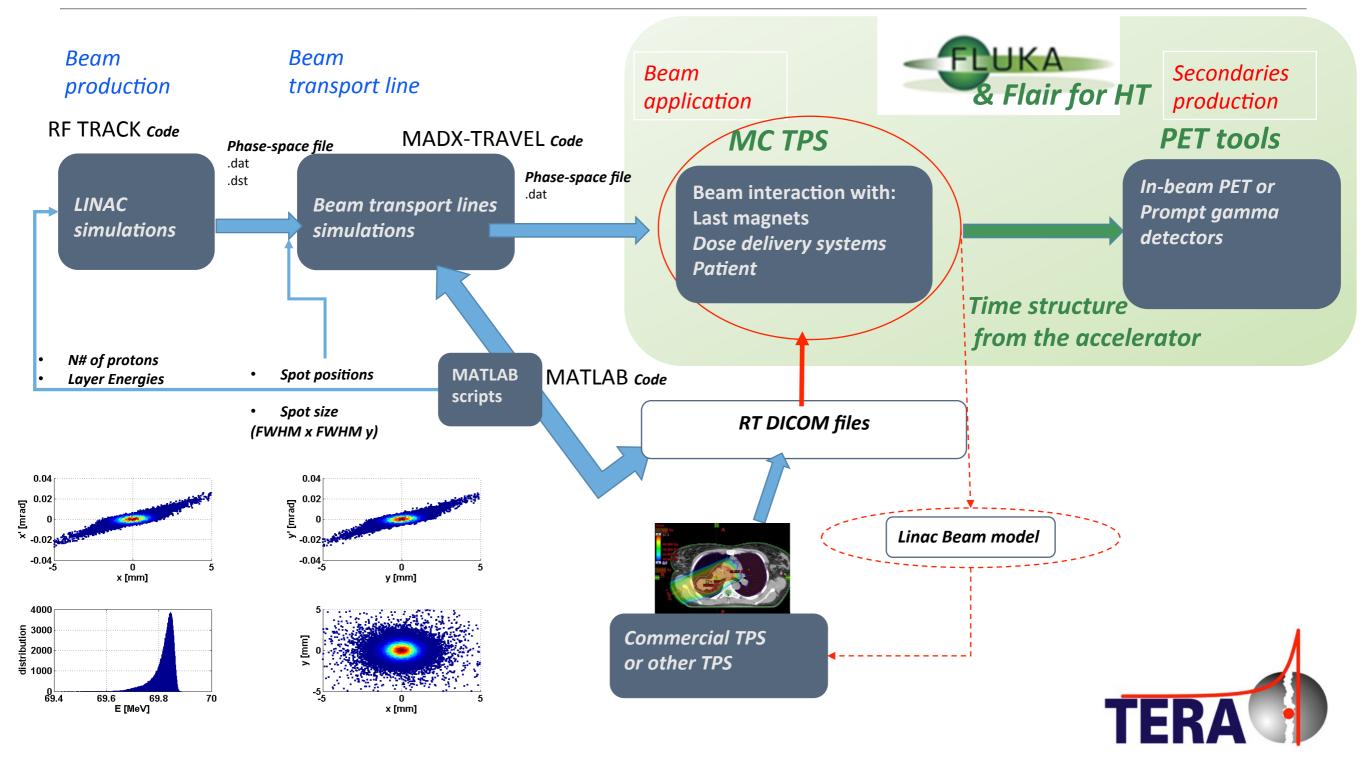
Beam application system

## The aim of the **full MC simulations** is to **characterize the linac beams** and

understand how the linac beam characteristics influences the DOSE and LET distributions in the patient .



#### Full Monte Carlo Simulations for new accelerator complex in Hadrontherapy TERA Foundation



Courtesy of: Caterina Cuccagna (TERA Foundation)

#### **Ongoing work**

- Ion fragmentation (also space radiation)
- Very light "special" ions: 3He, α, 6Li, 7Li, develop/check of the nuclear model physics
- Different radiobiological parameters/models (eg health tissue/tumor)
- Monte Carlo based TPS with MultiObjective Optimization techniques
- (Software) acceleration techniques



- [1] Böhlen, T. T., Cerutti, F., Chin, M. P. W., Fassò, A., Ferrari, A., Ortega, P. G., Mairani, A., Sala, P. R., Smirnov, G., Vlachoudis, V. (2014). *The FLUKA Code: Developments and challenges for high energy and medical applications*. Nuclear Data Sheets, 120, 211-214
- [2] Ferrari, A., Sala, P. R., Fasso, A., & Ranft, J. (2005). FLUKA: A Multi-Particle Transport Code. CERN 2005-10 (2005), INFN/TC\_05/11, SLAC-R-773
- [3] Vlachoudis, V. (2009). FLAIR: A Powerful But User Friendly Graphical Interface For FLUKA. Proc. Int. Conf. on Mathematics, Computational Methods & Reactor Physics (M&C 2009), Saratoga Springs, New York
- [4] Mairani, A., Böhlen, T. T., Schiavi, A., Tessonnier, T., Molinelli, S., Brons, S., Battistoni, G., Parodi K., Patera, V. (2013). *A Monte Carlo-based treatment planning tool for proton therapy*. Physics in Medicine and Biology, *58*(8), 2471– 2490
- [5] Battistoni, G., Bauer, J., Böhlen, T. T., Cerutti, F., Chin, M. P. W., Dos Santos Augusto, R., Ferrari, A., Ortega, P. G., Kozlowska, W., Magro G., Mairani A., Parodi K., Sala P. R., Schoofs P., Tessonnier T., Vlachoudis, V. (2016). *The FLUKA Code: An Accurate Simulation Tool for Particle Therapy.* Frontiers in Oncology, 6.