

MedAustron

OMA SCHOOL ON MEDICAL ACCELERATORS

5-9 JUNE 2017

SYNCHROTRON

FADMAR OSMIĆ

SYNCHROTRON FOR MEDICAL APPLICATIONS

- **Occurrence and Examples**
- **Parameters**
- **Components**
- **Certification**
- **Challenges vs Possibilities**
- **Outlook**

FIRST SYNCHROTRONS FOR HADRON THERAPY

● Loma Linda University Medical Center

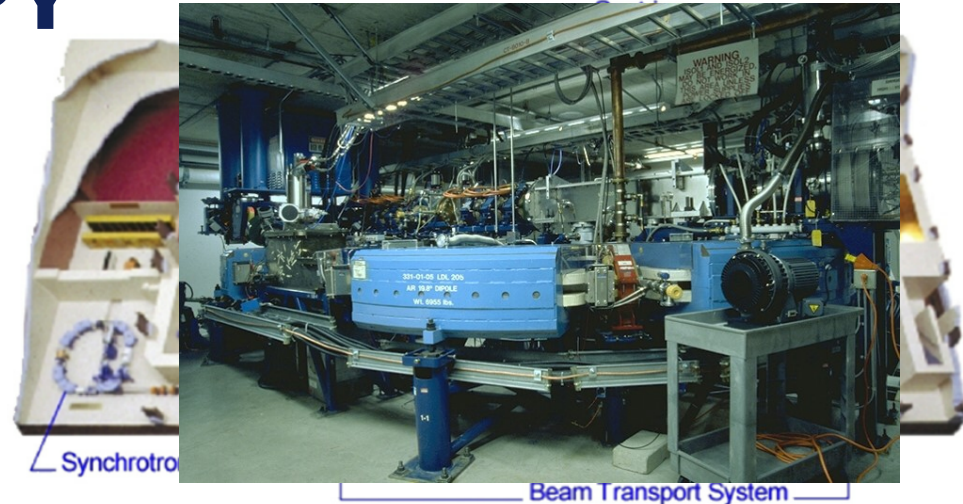
- Constructed in 1990 by Fermilab
- 7 m diameter

● Heavy-Ion Medical Accelerator in Chiba (HIMAC)

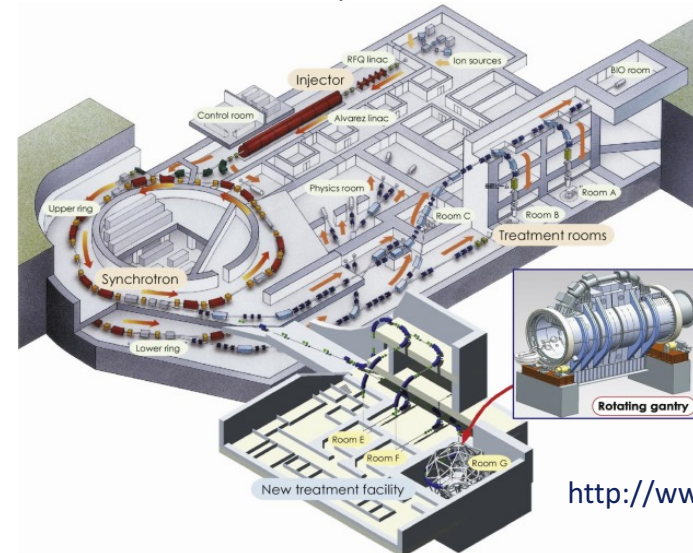
- Built by NIRS in 1993
- 2 synchrotrons
- Basis for Japanese centers

● Experimental Heavy Ion Therapy Facility at GSI

- Operational from 1997 to 2008
- Using the existing synchrotron SIS-18



<http://medical-center.lomalindahealth.org/>



<http://www.nirs.qst.go.jp>

OCCURRENCE

Austria	MedAustron, Wiener Neustadt	p	S 250	2 fixed beams**, 1 gantry** (under construction)	2017
		C-ion	S 430/u	2 fixed beams**	2017
China	IMP-CAS, Lanzhou	C-ion	S 400/u	1 fixed beam	2006
China	SPHIC, Shanghai	p	S 250	3 fixed beams**	2014
		C-ion	S 430/u	3 fixed beams**	2014
Germany	HIT, Heidelberg	p	S 250	2 fixed beams, 1 gantry**	2009, 2012
		C-ion	S 430/u	2 fixed beams, 1 gantry**	2009, 2012
Germany	MIT, Marburg	p	S 250	3 horiz., 1 45deg. fixed beams**	2015
		C-ion	S 430/u	3 horiz., 1 45deg. fixed beams**	2015
Italy	CNAO, Pavia	p	S 250	3 horiz., 1 vertical, fixed beams	2011
		C-ion	S 480/u	3 horiz., 1 vertical, fixed beams	2012
Japan	HIMAC, Chiba	C-ion	S 800/u	horiz.***, vertical***, fixed beams	1994
		p	S 230	1 gantry	2001
Japan	HIBMC, Hyogo	C-ion	S 320/u	horiz.,vertical, fixed beams	2002
Japan	PMRC 2, Tsukuba	p	S 250	2 gantries***	2001
Japan	Shizuoka Cancer Center	p	S 235	3 gantries, 1 fixed beam	2003
Japan	STPTC, Koriyama-City	p	S 235	2 gantries**, 1 fixed beam	2008
Japan	GHMC, Gunma	C-ion	S 400/u	3 horiz., 1 vertical, fixed beams	2010
Japan	MPTRC, Ibusuki	p	S 250	3 gantries***	2011
Japan	Fukui Prefectural Hospital PTC, Fukui City	p	S 235	2 gantries***, 1 fixed beam	2011
Japan	Nagoya PTC, Nagoya City, Aichi	p	S 250	2 gantries***, 1 fixed beam	2013
				3 horiz., vertical, 45 deg., fixed beams	2013
Japan	SAGA-HIMAT, Tosu	C-ion	S 400/u		2013
Japan	Hokkaido Univ. Hospital PBTC, Hokkaido	p	S 220	1 gantry	2014
Japan	i-Rock Kanagawa Cancer Center, Yokohama	C-ion	S 430/u	4 horiz., 2 vertical, fixed beams	2015
Japan	Tsuyama Chuo Hospital, Okayama	p	S 235	1 gantry	2016
Russia	ITEP, Moscow	p	S 250	1 fixed beam	1969
Russia	St.Petersburg	p	S 1000	1 fixed beam	1975
USA, CA.	J. Slater PTC, Loma Linda	p	S 250	3 gantries, 1 fixed beam	1990
USA, TX.	MD Anderson Cancer Center, Houston	p	S 250	3 gantries***, 1 fixed beam	2006
USA, MO.	S. Lee Kling PTC, Barnes Jewish Hospital, St. Louis	p	SC 250	1 gantry	2013
USA, FL.	Ackerman Cancer Center, Jacksonville	p	SC 250	1 gantry	2015
USA, MN.	Mayo Clinic Proton Beam Therapy Center, Rochester	p	S 220	4 gantries**	2015
	Laurie Proton Center of Robert Wood Johnson Univ. Hospital, New Brunswick	p	SC 250	1 gantry	2015
USA, NJ.	St. Jude Red Frog Events Proton Therapy Center, Memphis	p	S 220	2 gantries**, 1 fixed beam	2015
USA, TN.	Mayo Clinic Proton Therapy Center, Phoenix	p	S 220	4 gantries**	2016
USA, FL.	Orlando Health PTC, Orlando	p	SC 250	1 gantry	2016
USA, OH.	UH Sideman CC, Cleveland	p	SC 250	1 gantry	2016

26 operational synchrotron centers

- 15 protons
- 5 carbons
- 6 combined

4 in Europe

- all combined

13 in Japan

2 in China

5 in US

2 in Russia

→ About 1/3 of proton centers use synchrotrons

→ All carbon and dual centers use synchrotrons

<https://www.ptcog.ch/index.php/facilities-in-operation>

FURTHER CENTERS IN PROGRESS

● **9 under construction (according to PTCOG):**

- 8 proton synchrotrons
- 1 carbon synchrotron
- 1 combined → KIRAMS

● **4 in planning stage (difficult to estimate)**

- 2 proton synchrotrons (according to PTCOG)
- 2 combined (as far as I know) → CNAO/MEDAUSTRON

● **In general: huge interest worldwide**

- A lot of tourism at MedAustron and other European centers

PROTON SYNCHROTRONS FOR TUMOR THERAPY



Hitachi:

- Operational in Tsukuba, Japan
MDACC, Texas
- 6 dipoles
- 7,8 m diameter

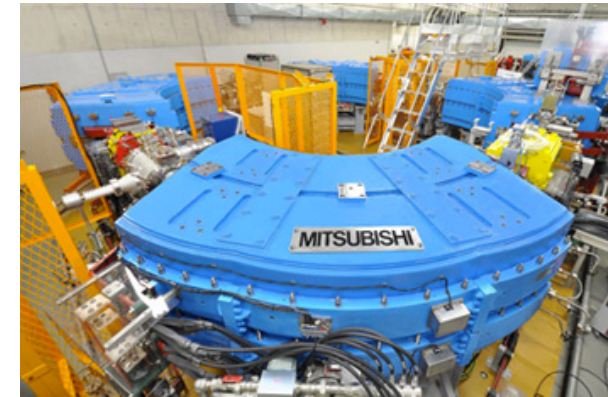
<http://www.hitachi.com/businesses/healthcare/products-support/pbt/>



ProTom:

- 8 dipoles
- 4,9m diameter
- 16 tons
- Protons up to 330 MeV → proton CT

<http://www.protominternational.com/>

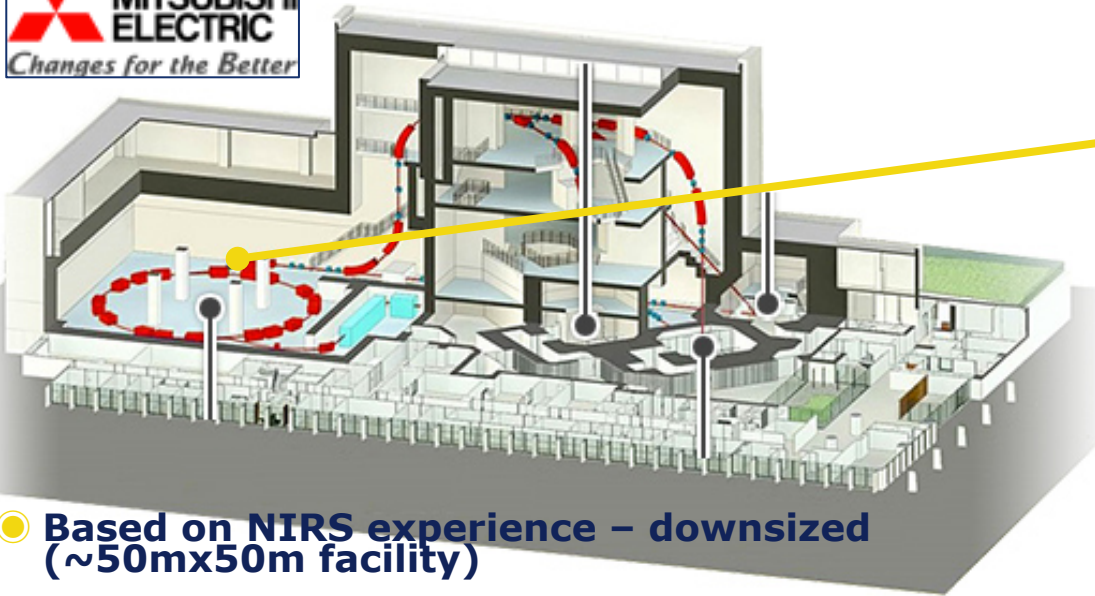


Mitsubishi

- 6 m diameter
- 4 dipoles

<http://www.mitsubishielectric.com/bu/particlebeam/products/index.html>

MITSUBISHI SYNCHROTRONS FOR TUMOR THERAPY



- **Based on NIRS experience – downsized (~50mx50m facility)**
- **Several installations in Japan**
- **Carbon and dual type available**
- **18 dipoles**
- **Turn-key solutions**
- **Other vendors (Hitachi and Toshiba) coming up with carbon facilities**

<http://www.mitsubishielectric.com/bu/particlebeam/products/index.html>

EUROPEAN SYNCHROTRONS ALL ARE DUAL TYPE



CNAO/MedAustron

- Based on PIMMS design at CERN
- Technical design variations
 - Injector position
 - Magnets
 - Power converters
- ~78 m circumference
- 16 dipoles a 10t

<http://fondazionecnao.it/en/>

Heidelberg

- Built by GSI
- He operation started
- 65 m circumference
- 6 dipoles a 25t

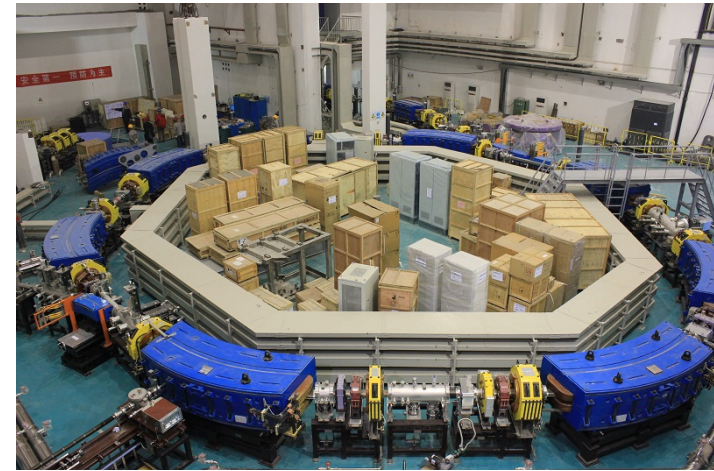
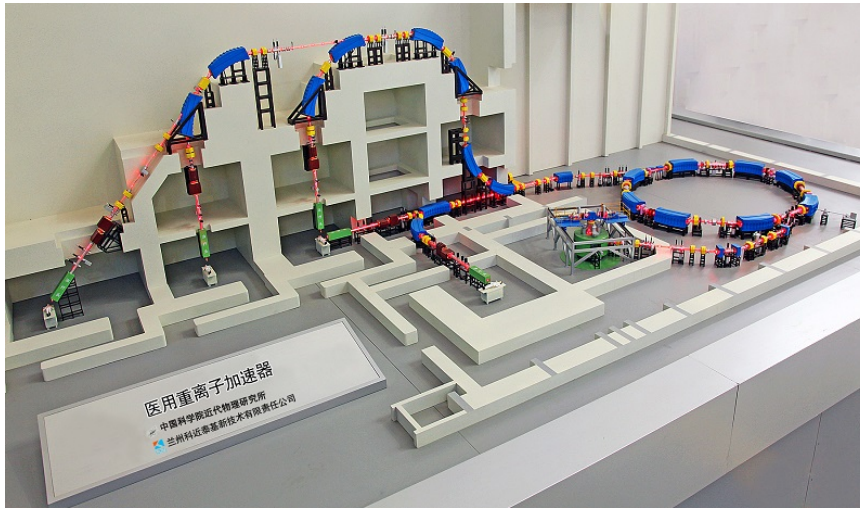
www.klinikum.uni-heidelberg.de

Siemens

- Installations in Marburg, Shanghai, (Kiel)
- Designed and built by Danfysik
- Modified HIT design → 65 m circumference
- 12 dipoles a 8t

<http://www.danfysik.com/en/solutions/particle-therapy-accelerators/>

LANZHOU SYNCHROTRON

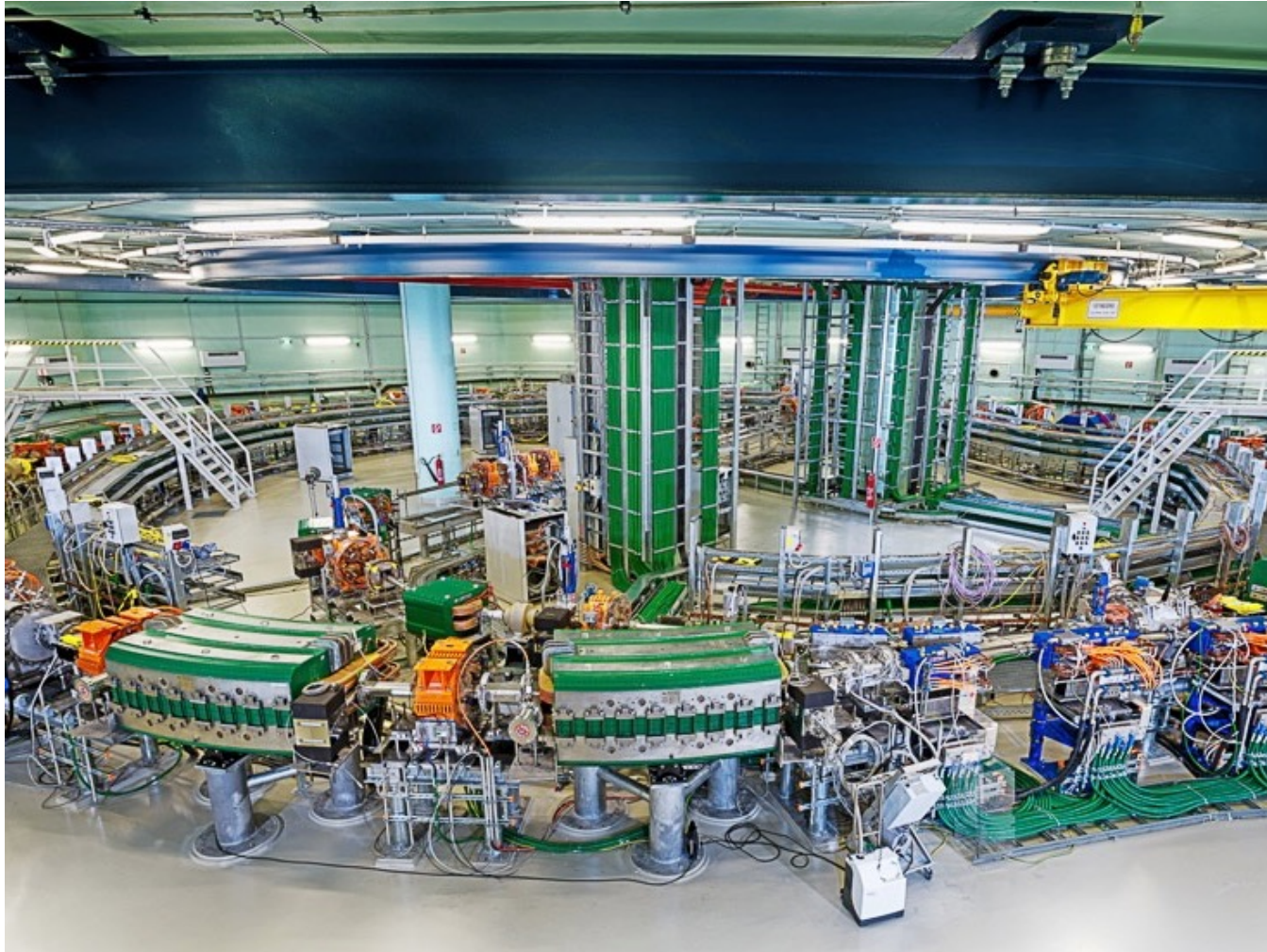


- Based on HIRFL research
- Heavy Ion Medical Machine (HIMM)
- Compact Carbon Synchrotron → 56,2 m circumference
- 8 dipoles
- Cyclotron as injector
- In construction
- Aiming at the Chinese market

<http://www.kejintj.com/en/cp/zlz/>

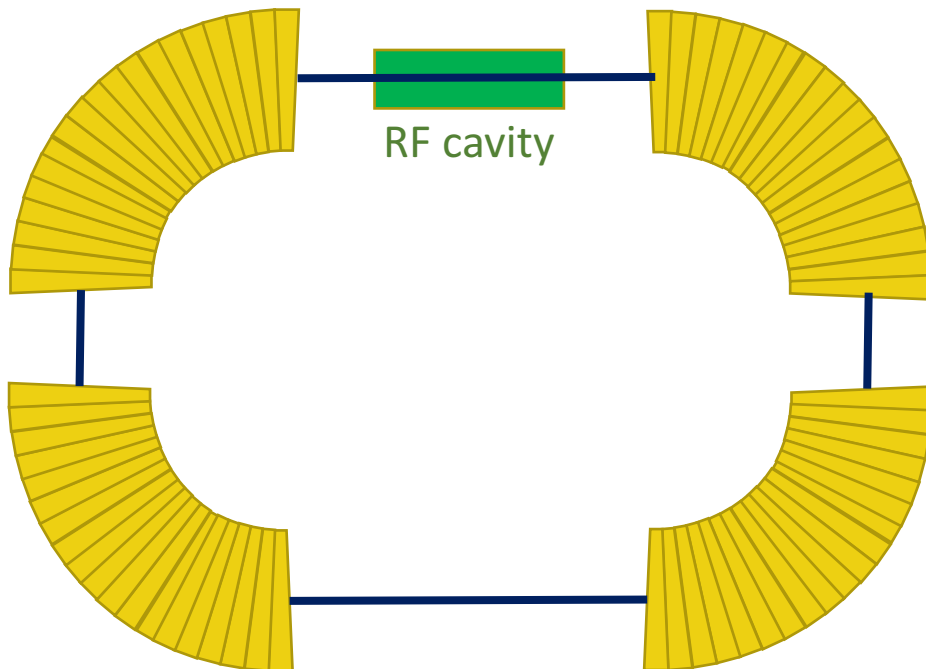
SYNCHROTRON IN DETAIL

CASE STUDY MEDAUSTRON



MEDICAL SYNCHROTRON

- Fixed radius → nominal path is constant
 - Magnetic field is adjustable
 - RF frequency is adjustable
- Variable energy
- Synchronous
- Customized lattice
 - Zero Dispersion sections for RF cavity and the minimum beam size at injection/extraction



- Multi-Turn Injection ~ 30 us
- DC beam at injection and after acceleration
- Slow extraction → see Adriano's talk
- Beam size \sim few cm
- Beam length : can be \sim half the circumference

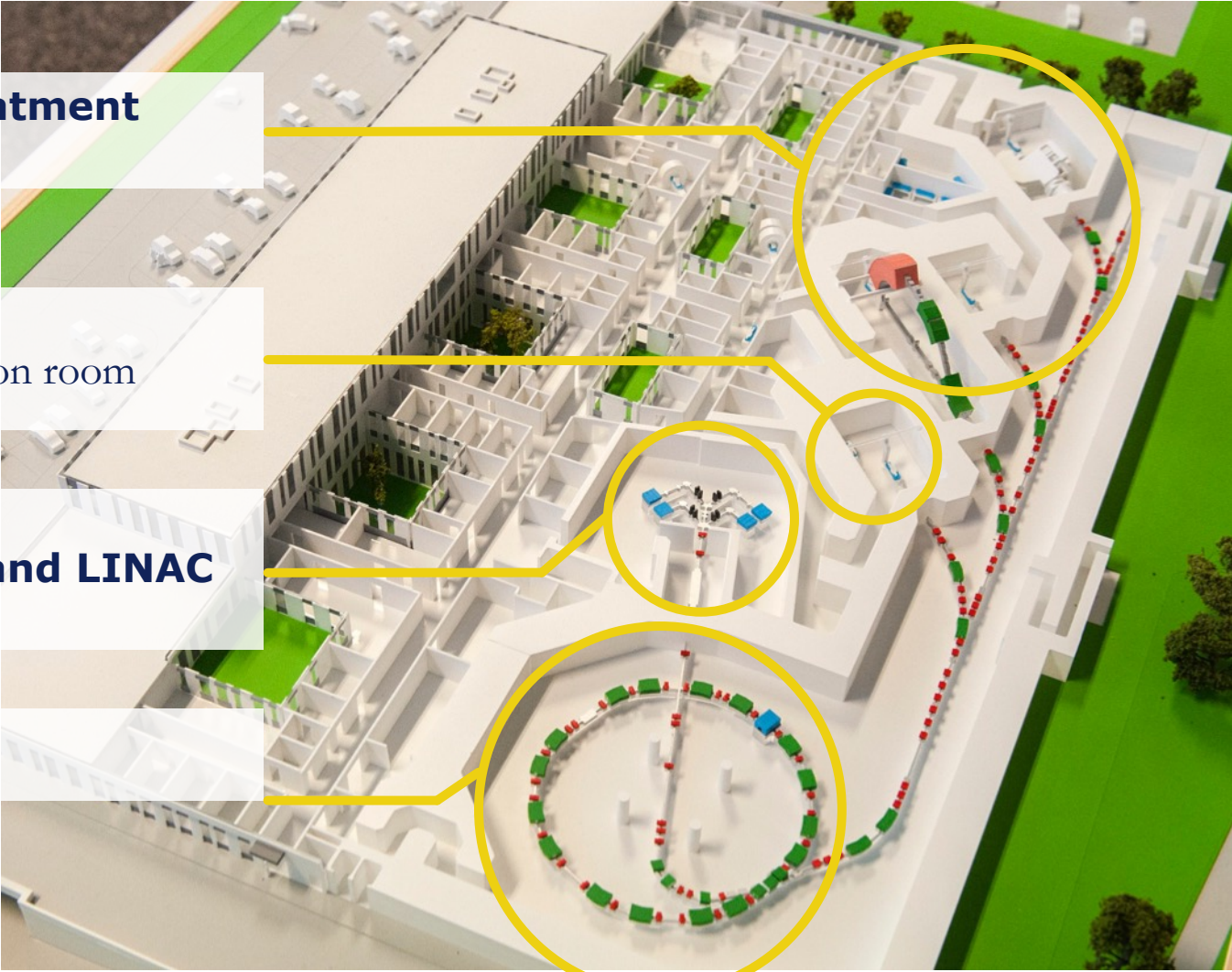
MEDAUSTRON FACILITY

3 patient treatment rooms

Research
An own irradiation room

Ion sources and LINAC

Synchrotron



BEAM PARAMETERS

MEDAUSTRON

Performance	
Particle Species	p, C (other light ions possible)
Energy	P: 60 – 250 (800) ; C: 120 – 400 MeV/u
Possible energy levels	255 per particle
Ramping speed	3 T/s
Scanning speed	20 m/s (– 100 m/s)
Maximal scanning field size	20 x 20 cm ²
Intensity	p: 1E10, C: 4E8
Width	4 – 10 mm (assuming vacuum up to Iso Center)

BEAM PARAMETERS

MEDAUSTRON

Stability	
Minimal energy step size	0,1 MeV
Beam energy precision	0,25 MeV
Relative beam energy spread dE/E	Approx 1.1E-3
Position precision	+/- 0,5 mm
Beam profile stability spill to spill	+/- 20%
Intensity	+/- 20%
Particle current extraction stability in the 100 Hz range	0 to 2 times the requested beam current
Particle current extraction stability in the kHz range	0 to 5 times the requested beam current

IMPORTANT: Long-term reproducibility of beam properties (QA!)

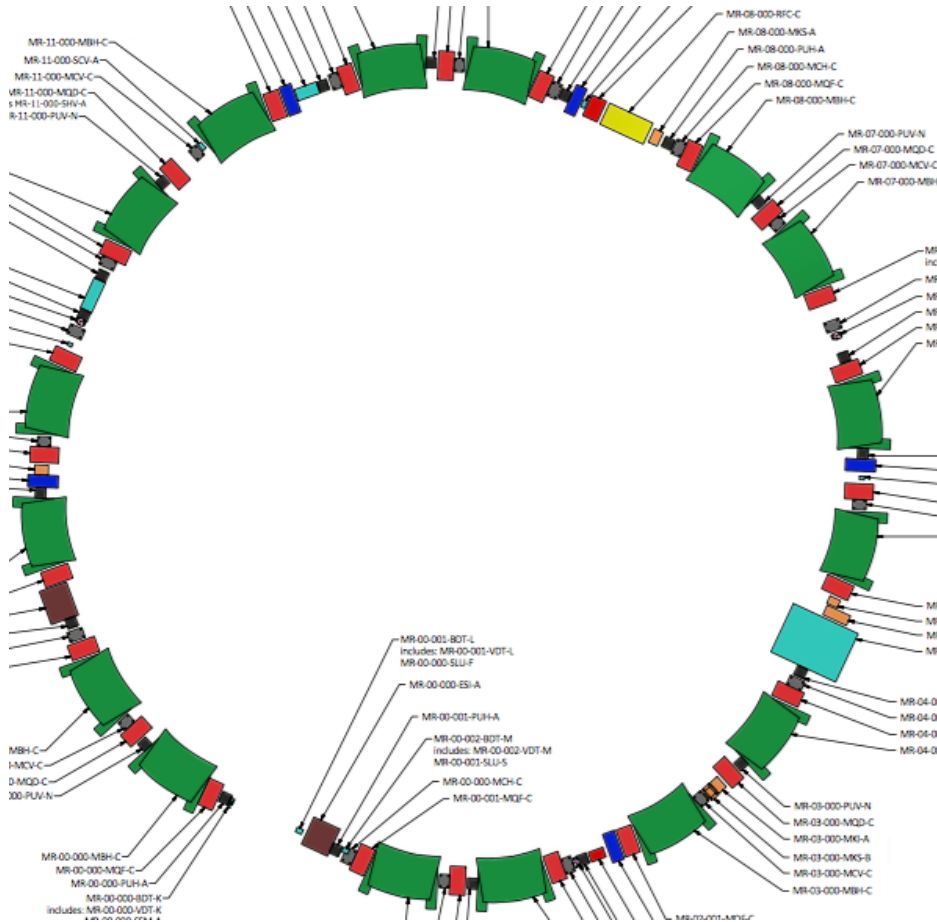
BEAM PARAMETERS

MEDAUSTRON

Availability	
Dead time between cycles	<2 s
Room switching time	<20 s
Beam Particle switching time	~2 mins
Maximal cycle time	120 s
System Uptime	95-98 %
Time of cycle excluding extraction	<2s
Room occupancy time	25 mins (can be 13)

SYNCHROTRON COMPONENTS

EXAMPLE MEDAUSTRON

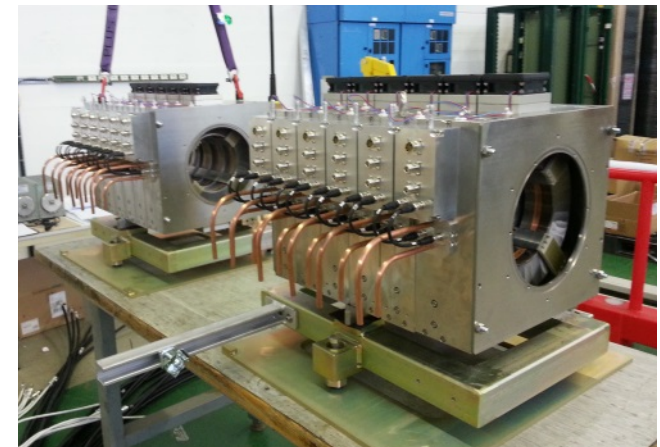
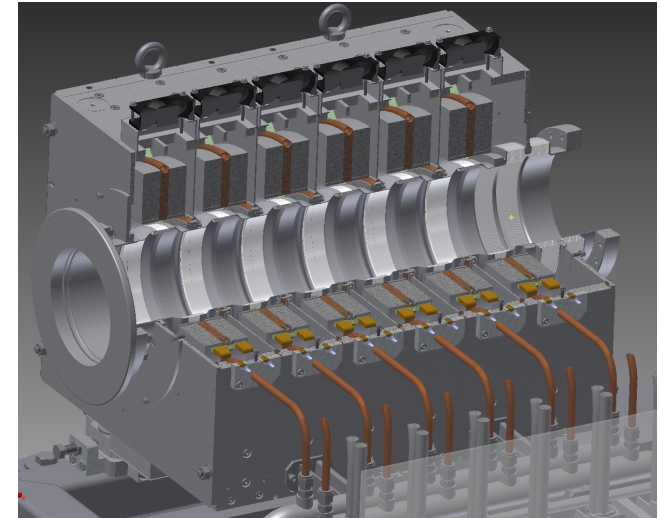


- **16 dipoles (+1 reference)**
- **24 quadrupoles (3 families)**
- **5 Sextupoles**
- **Power converters**
- **RF cavity**
- **Injection**
 - Electrostatic septum
 - ??? bumpers
- **Extraction**
 - Betatron
 - Electrostatic septum
 - Magnetic septum
- **Orbit correctors**
- **Beam Diagnostics**
 - Tune kickers
 - 20 Pickups
 - 2 CTs
 - 2 Schottkys
 - ...

SYNCHROTRON COMPONENTS

CASE STUDY: MEDAUSTRON RF CAVITY

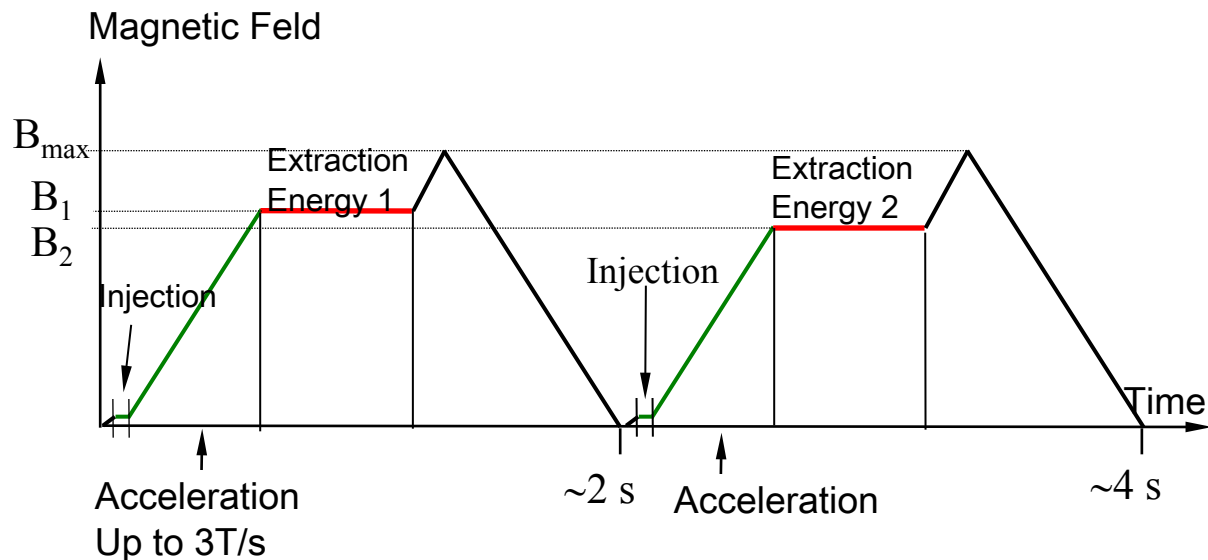
- Runs on 1st harmonic
- Finemet loaded co-axial resonator
- 2 blocks à 6 cells (82-121 mm)
- 2 Finemet FT-3L rings per cell (per gap)
- 12 x 1 kW
- Water cooled Cu disc
- Air cooling (cell: 58 m³/h)
- $f = 0.46 - 3.25$ MHz
- 5 kV total



C. Schmitzer
MedAustron

SYNCHROTRON CYCLE

- Injection 80us
- RF-capture: beam bunching 40 ms
- Acceleration <0,5 s
- Prepare Extraction 100 ms (Energy verification)
- Extraction 0,1 – 120 s
- Ramp Down Reset 0,5 s



CE: CONFORMITY ASSESSMENT STRATEGY

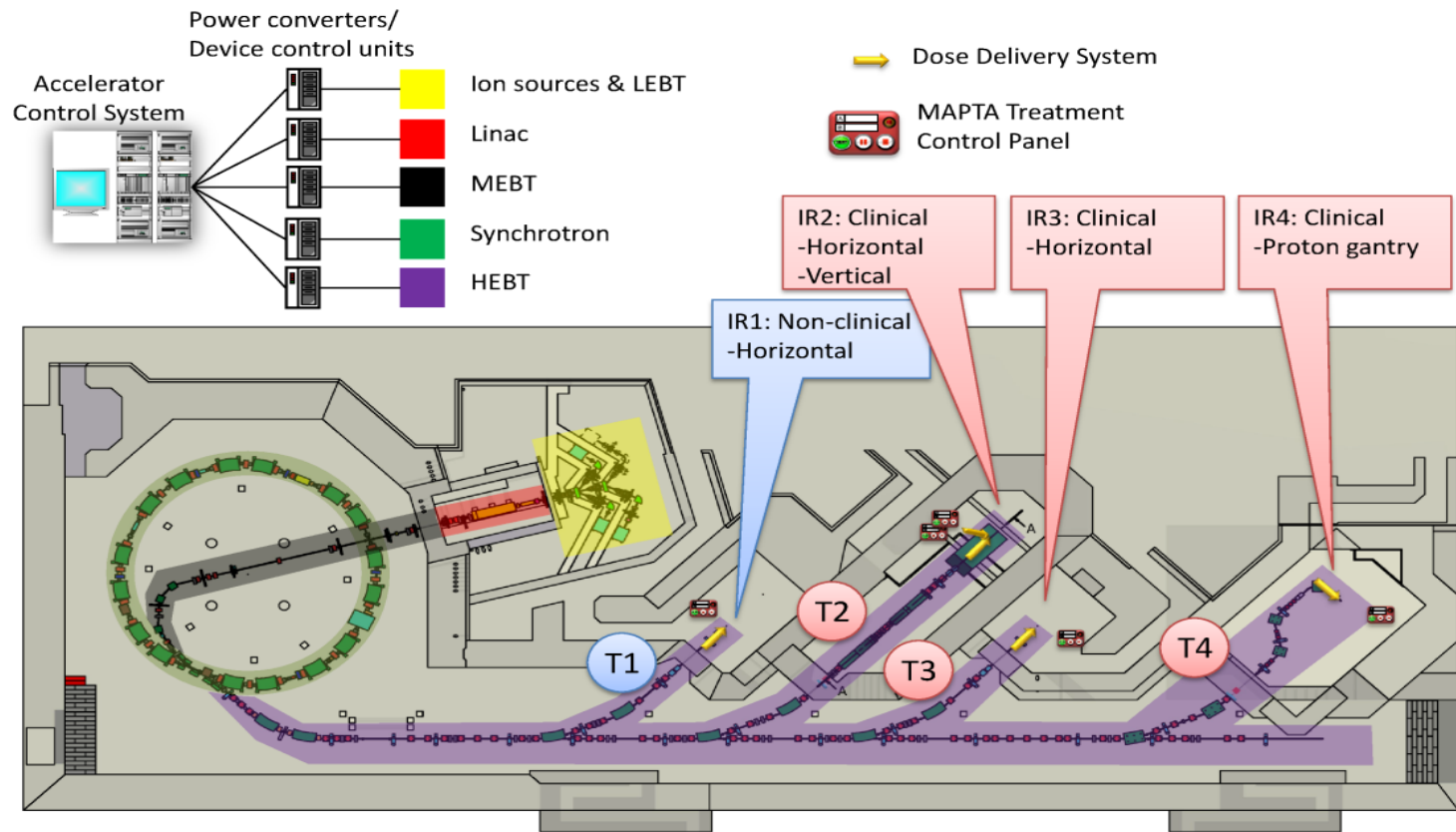
- **Starting Point:**

- Statement of Austrian Ministry of Health:

The Therapy Accelerator of the Particle Therapy Center MedAustron is to be classified as a medical product and is to be handled in accordance with the Medical Product Law and the European Medical Device Directive 93/42/EEG.

- The principal core process is safe operation of the product (the product is produced only once).

THERAPY ACCELERATOR MAPTA



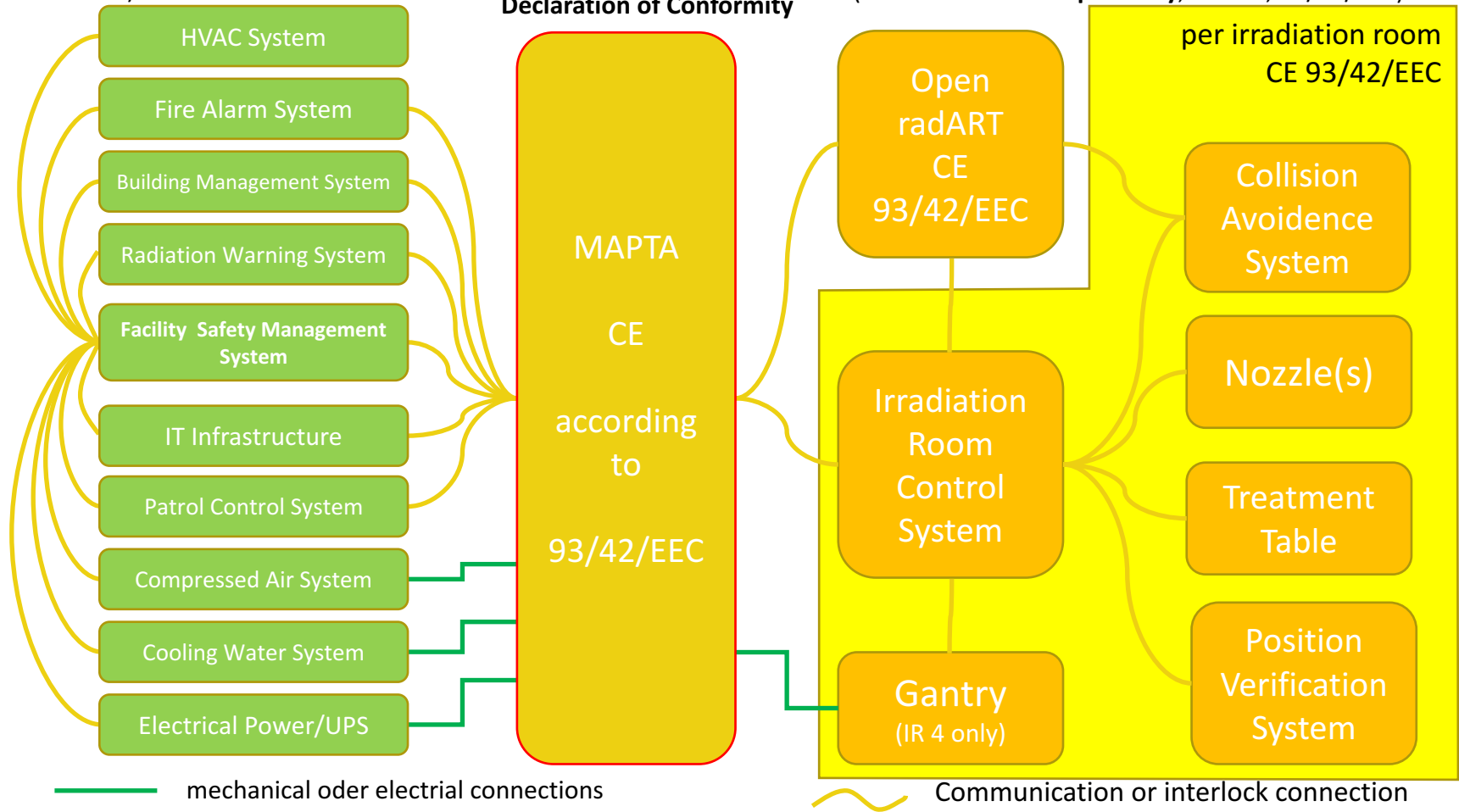
INTERFACE OVERVIEW

MAPTA

Interface to technical infrastructure (industrial standards)

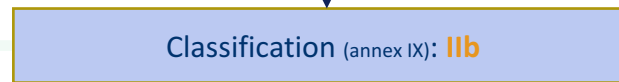
Interfaces to Medical Products
(Declaration of Compatibility, Art. 12, 93/42/EEC)

Declaration of Conformity

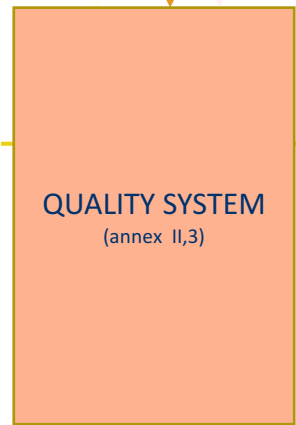
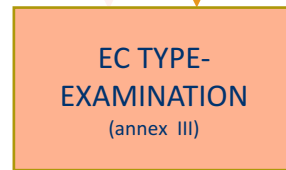
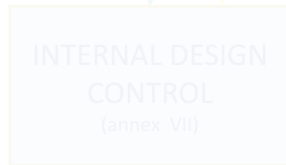


CE: PATHS FOR LIGHT ION BEAM MEE

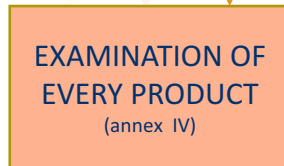
Medical Device Directive
93/42/EEC



Design Phase



Production Phase



Declaration of Conformity by Manufacturer



Declaration of Conformity by Manufacturer/Notified Body + Tests, Control, Examinations by Notified Body

CE: CONFORMITY ASSESSMENT STRATEGY

● Activities related to entire MAPTA:

- EMC regulation → EMC concept/report
- Functional safety w.r.t intended use
- Usability → User Manual
- ETG/ETV → OEnorm E8001 (initial commissioning)
- ISO 14971 (risk management for medical products)

● Additionally:

- Test management (incl. 60601-2-64)
- Technical documentation

CYCLOTRON VS. SYNCHROTRON

Cyclotron	Synchrotron
Fixed Energy Energy Selection System	Variable energy
Radiation protection	Low radiation
High current Current manipulation	Low current
Small footprint	Large footprint
No carbons	Different ions easy possible
No Injector	Injector needed
Lower cost	Higher cost

Don't forget the business case!

FURTHER CHALLENGES FOR SYNCHROTRONS

● Costs

- Due to foot print and complexity

● Timing structure

● Commissioning time

● Complex

- Especially the technical operation
- Large team to cover many disciplines needed

REASONS FOR SYNCHROTRONS

● High flexibility:

- Several ion species → exploiting the full potential of hadron therapy
(there are no carbon cyclotrons)

● Active energy selection

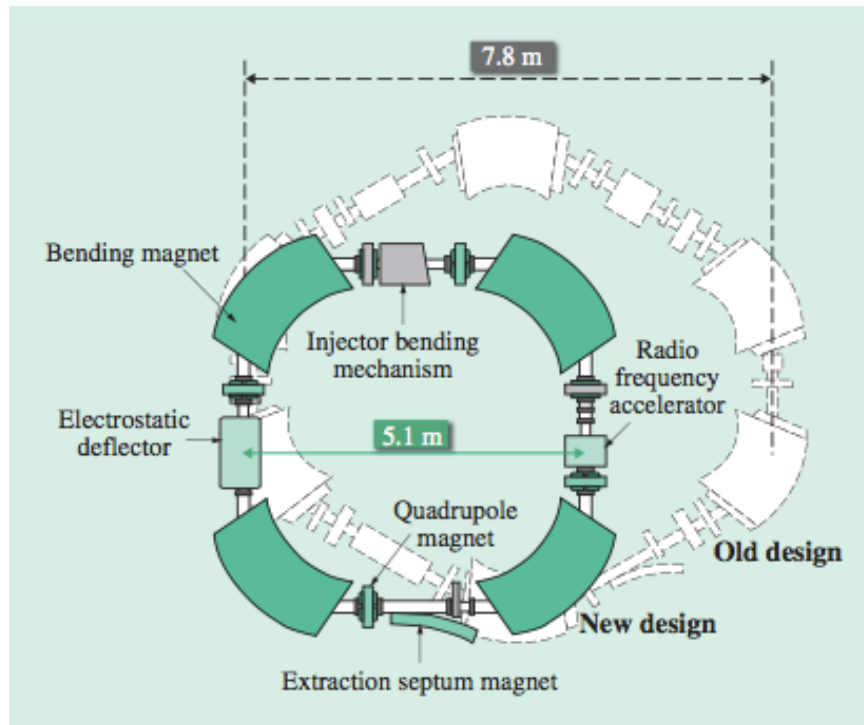
● Dose efficiency

- Carbon ions leave about 24 times more energy in a cell than protons
- Certain tumors can be treated
- Hypo-fractionations
- Benefit for patients

● Political aspects in decisions

- Importance of Know-how gain
- Research aspect

DOWNSIZING EXAMPLE HITACHI



● 6 → 4 dipoles

● 10 → 4 quads

● 7,8 m → 5,1 m

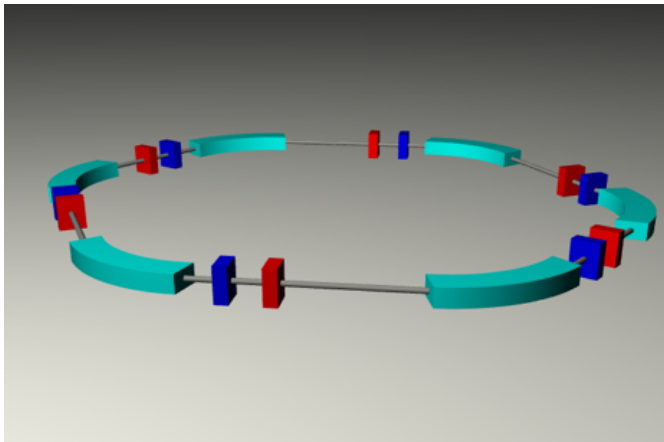
→ 30% smaller footprint

→ Thanks to a newly developed simulation technique for particle trajectory tracking

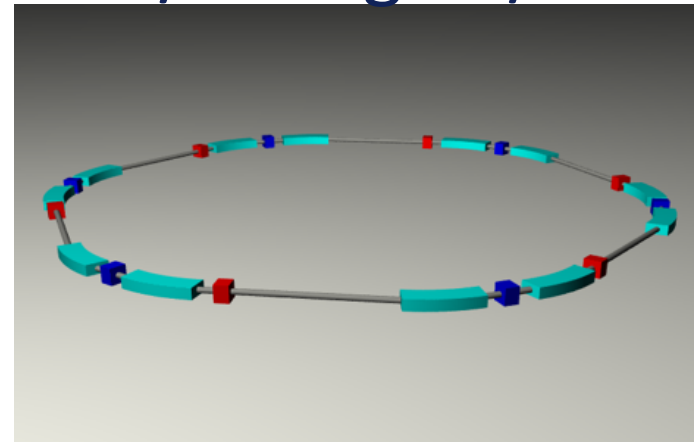
Umezawa et al.,
Hitachi Review Vol 64 (2015), No. 8

“DOWNSIZING” EXAMPLE SIEMENS/DANFYSIK

HIT



MIT/Shanghai/Kiel



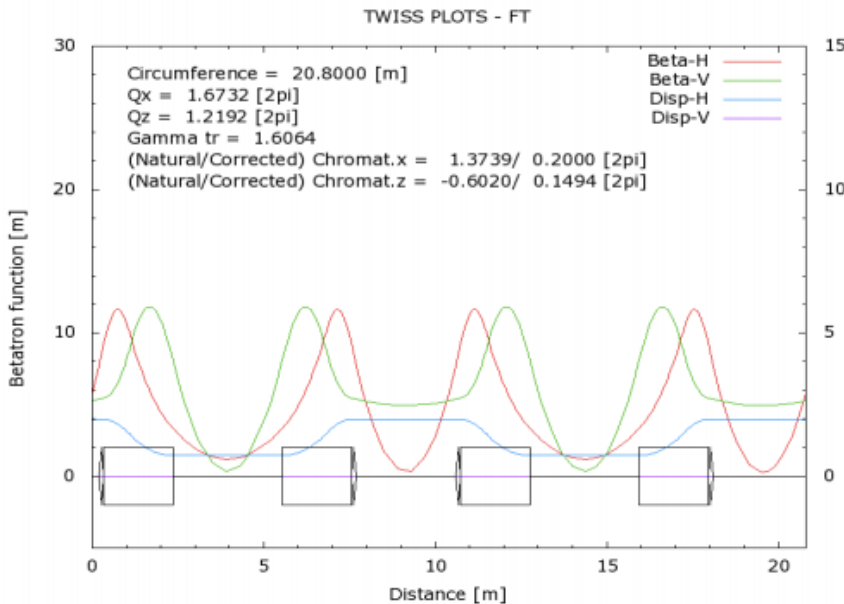
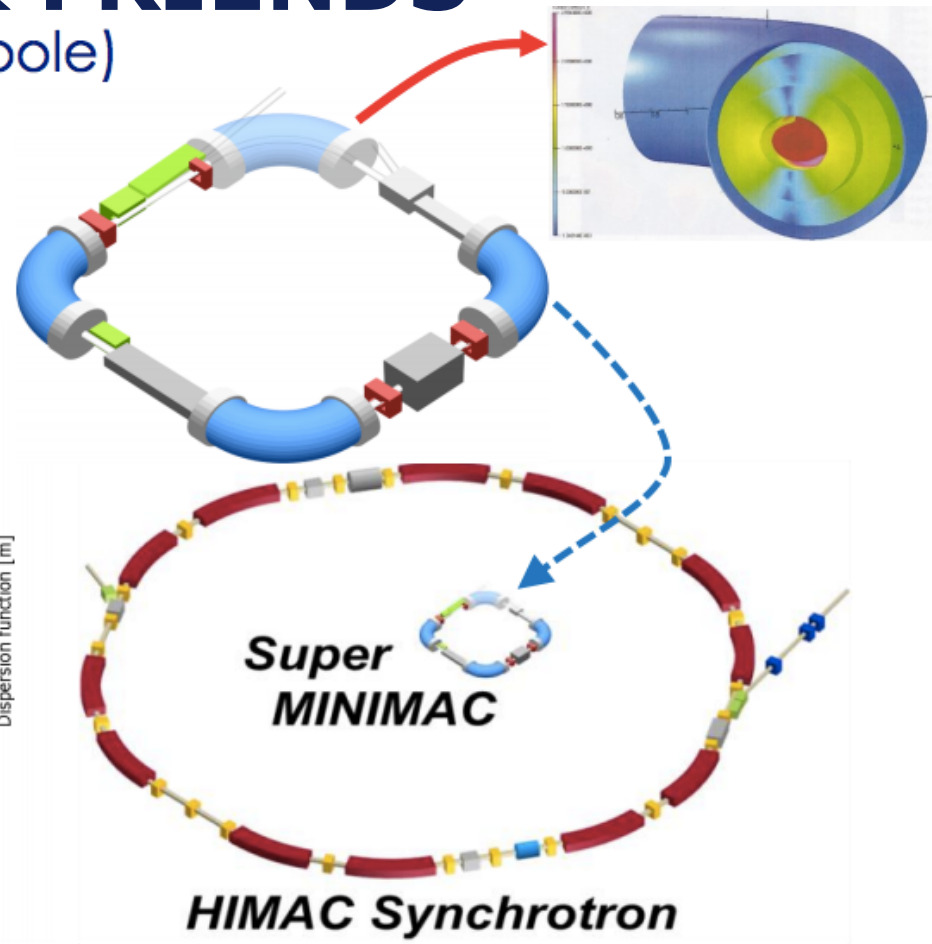
- **Reduced weight of heaviest component (installation, handling)**
- **Less space constraints in extraction region (smaller angle in magnetic septa possible)**
- **Higher symmetry (smaller beta function, larger dynamic aperture)**
- **Symmetric sextupole layout (flexibility)**

www.siemens.de

Heiko Rohdjess

FUTURE DOWNSIZING AIMED BY NIRS & FRIENDS

- SC magnets (Dipole+Quadrupole)
- $B_{\max} \sim 5$ [T]
- $dB/dt \sim 1+$ [T/sec]
- Circumference ~ 21 [m]



34

OBS: fast ramping curved, superconducting dipoles

Iwata et al., Nov 2016
Workshop at CIEMAT

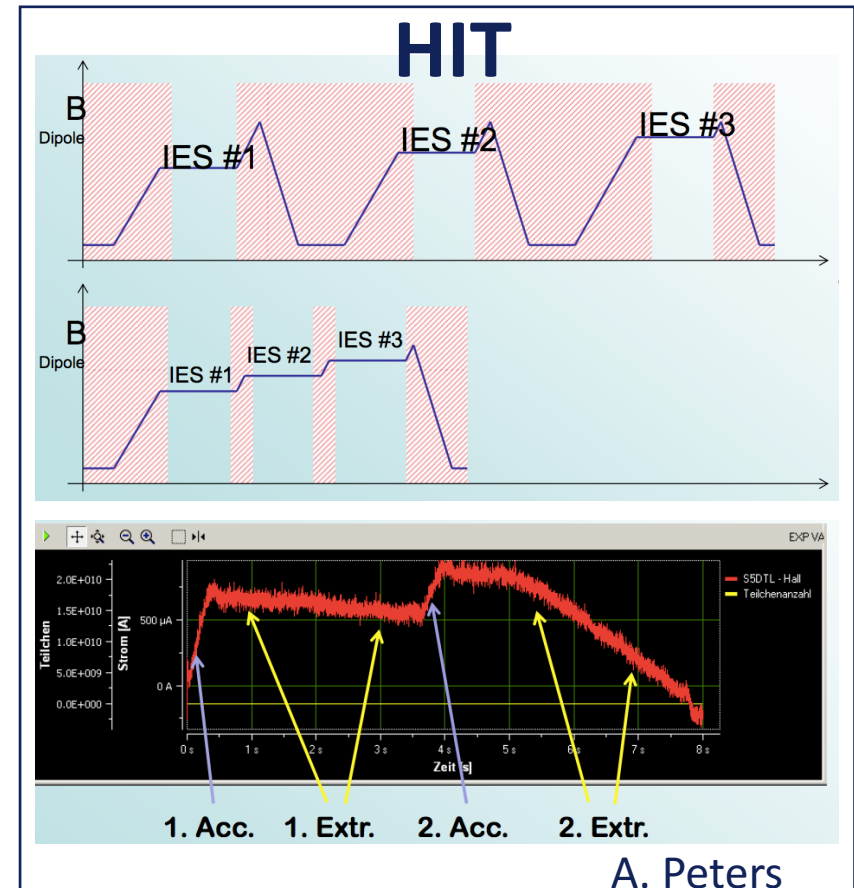
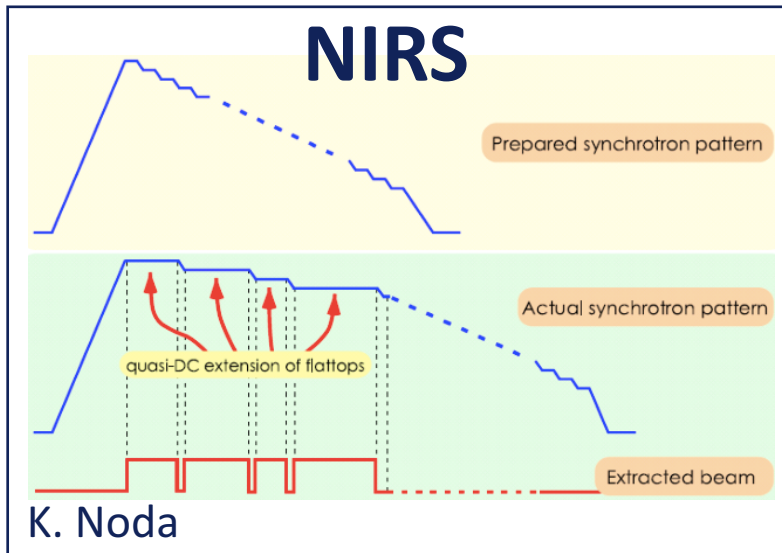
FUTURE DOWNSIZING AIMED BY NIRS & FRIENDS



<http://www.japantimes.co.jp/>
DEC 13, 2016

- **4 Japanese companies joined efforts with NIRS**
 - Hitachi Ltd., Mitsubishi Electric Corp., Toshiba Corp. and Sumitomo Heavy Industries Ltd
- **“... to share the research costs to develop a new heavy ion cancer treatment device in about 10 years”**
- **Goal: decrease the treatment costs by factor 2-3**

SPEEDING UP: MULTI-ENERGY OPERATION



- **NIRS approach: see slides by K. Noda**
 - Every energy level needs to be passed
- **HIT approach:**
 - Selective choice of energies
 - Shrinking the irradiation time by 50%
 - Proof of principle with 2 energies

OUTLOOK

● Downsizing is possible and ongoing

- Proton synchrotrons are already competitive with cyclotrons → small footprint
- Carbon facilities can fit in 50m x 50m

● Among others Danfysik has proven that slim carbon synchrotrons can be built

- Less components
- Easier service and operation

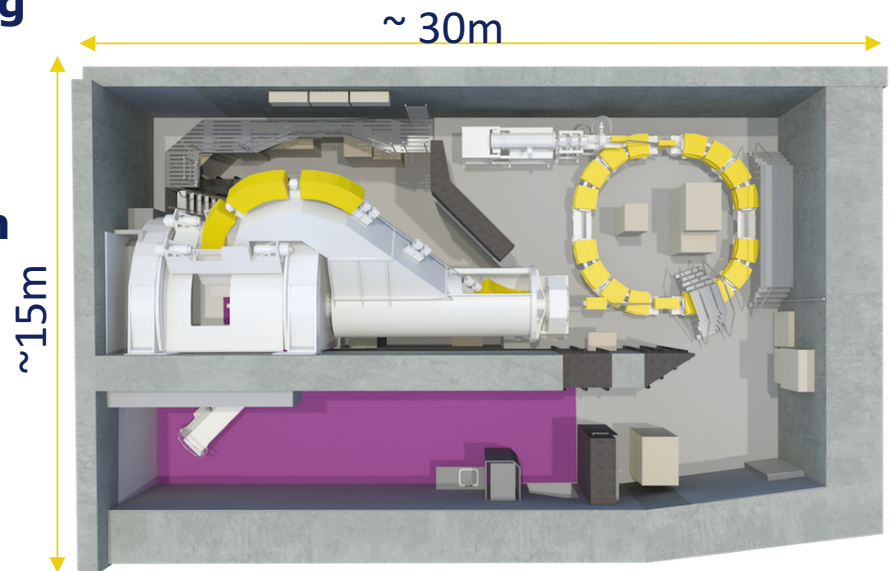
● Faster commissioning due to 1:1 copies

● Multi-Energy operation

● Faster cycle times

● Synchrotron as product

- Already available in Japan
- Was available in Europe (Siemens)
- European centers CNAO and MedAustron working now on this step



ProTom one gantry
room solution

THANK YOU!

MedAUSTRON