

# Design and characterization of pixelated needle probe for molecular neuroimaging on awake and freely moving rats

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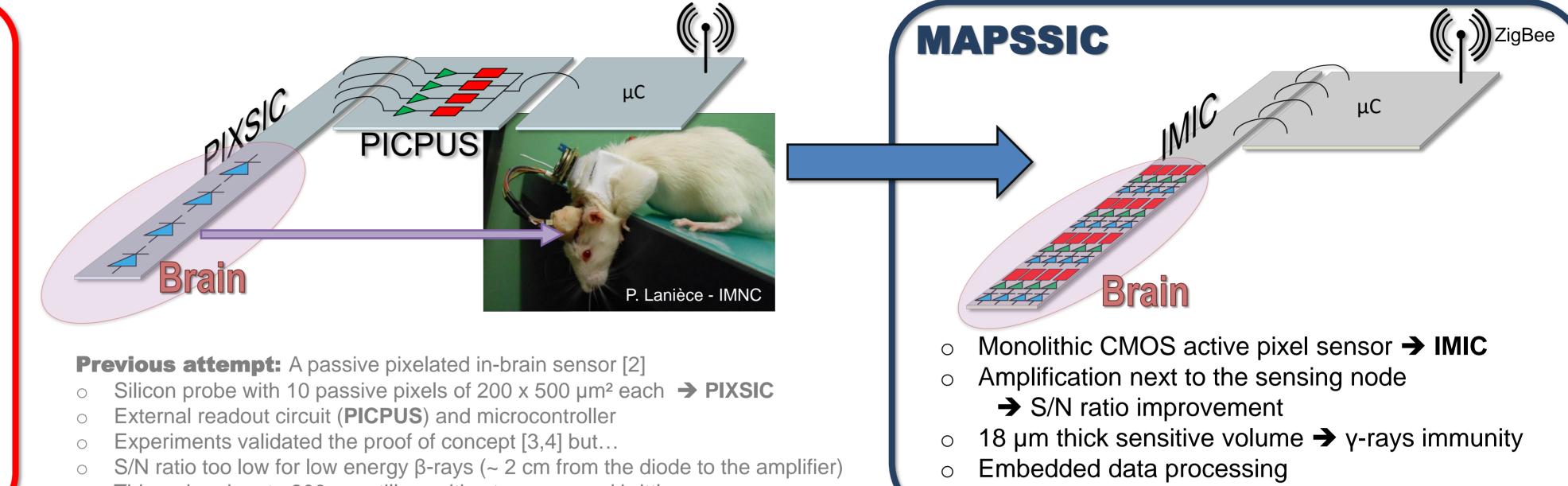
# I. MAPSSIC PROJECT

#### Motivation

- Neuroimaging on awake [1] and freely moving animals
- Localization of  $\beta$ + radiotracer clusters close to the pixelated sensor
- → Implantation of a pixelated needle-shaped sensor in the brain

### Requirements

- Sensor
  - Small size Limitation of the impact on the brain tissue
  - $\succ$  Immunity to the 511 keV  $\gamma$ -rays background
- o System
  - Compact with wireless data transmission
  - Autonomous



Limitation of the discomfort that may alter normal behavior

Thinned probes to 200  $\mu$ m still sensitive to  $\gamma$ -rays and brittle

- Dissipated power < 1 mW

**IV. SINGLE SENSOR VALIDATION** 

# II. IMIC SENSOR DESIGN

Size: 610 x 12000 µm<sup>2</sup> (pixelated needle-shaped sensor)

**Sensitive area:** 16 x 128 pixels → 480 x 6400 µm<sup>2</sup>

**Technology:** 0.18  $\mu$ m CMOS process on 18  $\mu$ m thick high resistivity (> 1 k $\Omega$ ·cm) epitaxial layer READOUT TIME (128 µs)

2047

IT STORED

WAITING TIME

INTEGRATION TIME

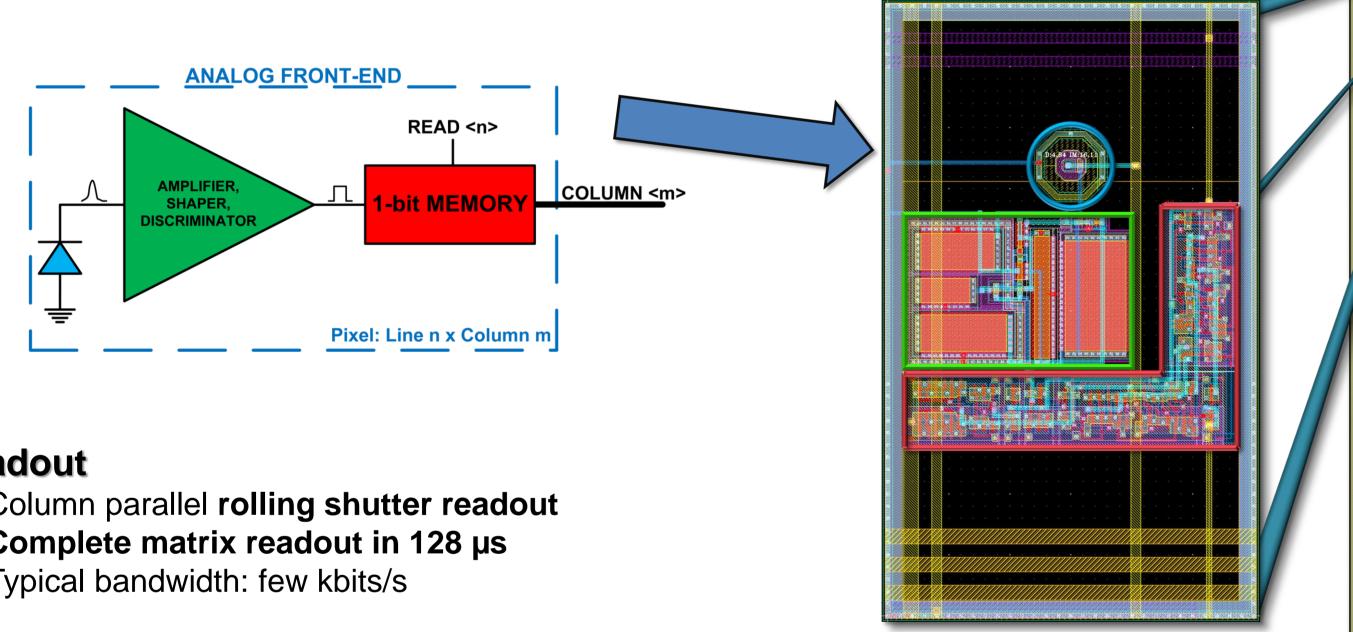
time

### Strategy for low power dissipation

- $\circ$  Very low readout rate (~ Hz)
- Information of the hit stored in the pixel between two readouts

### Pixel design

- Detection efficiency  $\rightarrow$  Small pixel pitch: 30 x 50  $\mu$ m<sup>2</sup>
- Based on a front-end amplifier of ALPIDE (ALice Plxel DEtector) [5]
  - Low power (55 nW/pixel)
  - Asynchronous operation
  - Memorization (on 1 bit) of the information of the hit until the readout 
     Synchronization

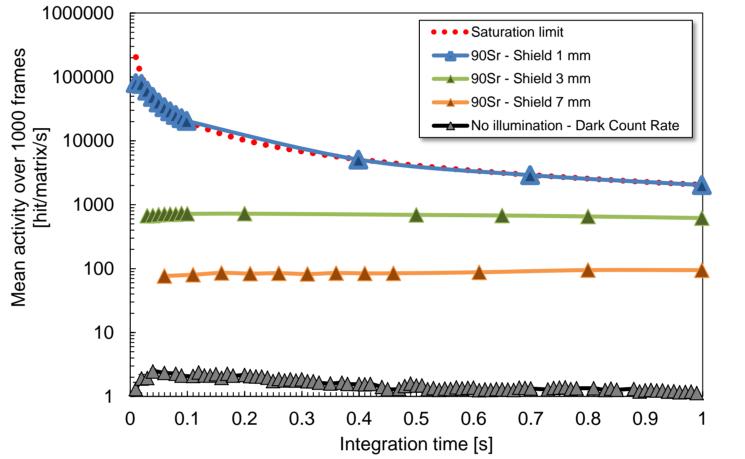


### Laboratory tests

- $\circ$  Power consumption of the whole sensor: 161  $\mu$ W
- Integrated DACs fully operating

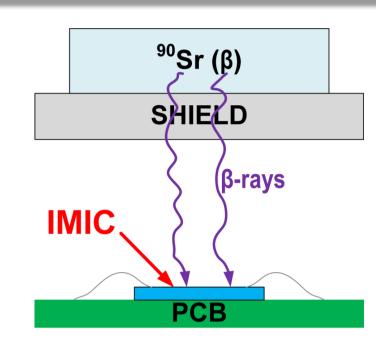
### Measurements with $\beta$ - source (<sup>90</sup>Sr)

- Integration time between 10 ms and 1 s
- Room temperature operation
- $\circ$   $\beta$  source activity regulated with various shield thickness



#### Measurements with $\beta$ + emitter (<sup>18</sup>F)

 $\circ$  <sup>18</sup>**F**: β+ and γ emitter in aqueous solution (100 MBq max. allowed in the laboratory)



#### **Detection performances**

- For long integration time (~1 s)
  - Dark Count Rate ~ 1.15 hits/matrix/s
- For short integration time (< 20 ms) Ο
  - Max. activity ~ 80 000 hits/matrix/s
  - Dark Count Rate ~ 2-3 hits/matrix/s
- For expected activities (<< 100 hits/matrix/s) No hit losses with longer integration times (~1 s)



#### Readout

- Column parallel rolling shutter readout
- $\circ$  Complete matrix readout in 128 µs
- Typical bandwidth: few kbits/s

**Chip configuration:** SPI protocol to steer on-chip DACs → Polarization of the front-end

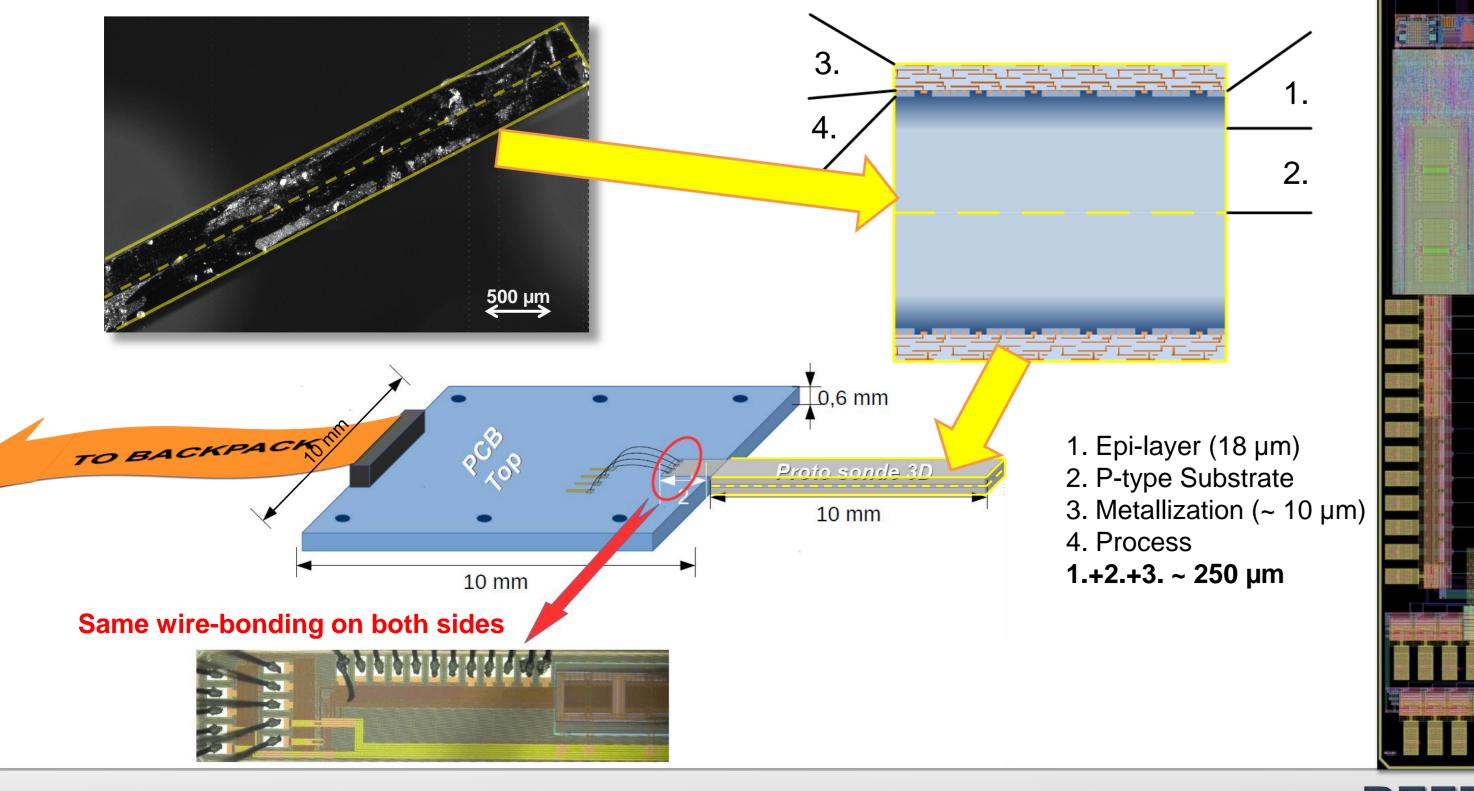
# **III. BACK-TO-BACK INTEGRATION**

#### Concept

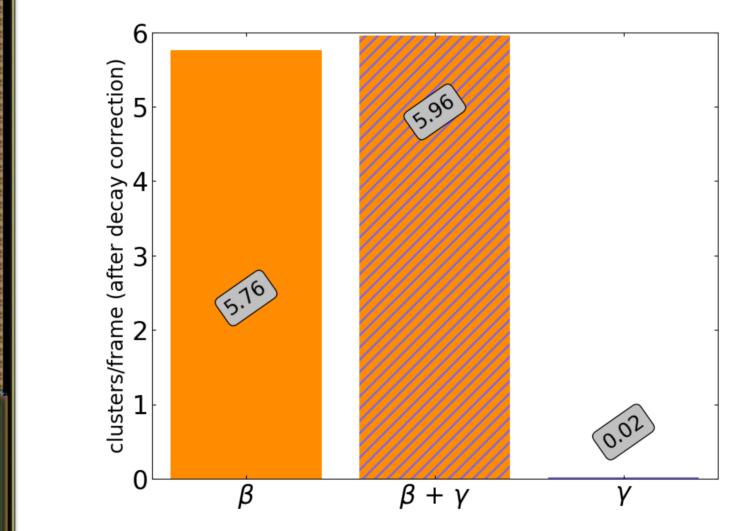
- Two sensors back to back
  - Robustness for manipulation and implantation Ο
  - Large two-sided sensitive area Ο
- Easy connection between the sensors and the backpack containing the microcontroller with wireless transmission and the battery

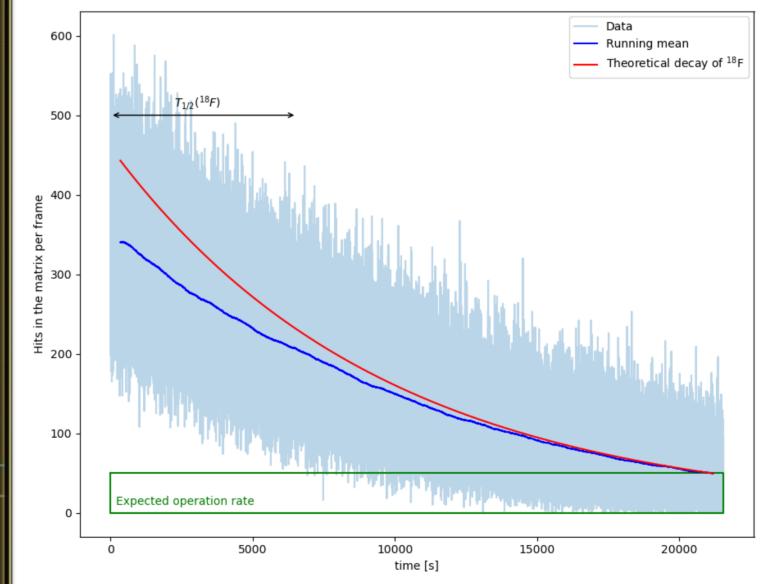
### Realization

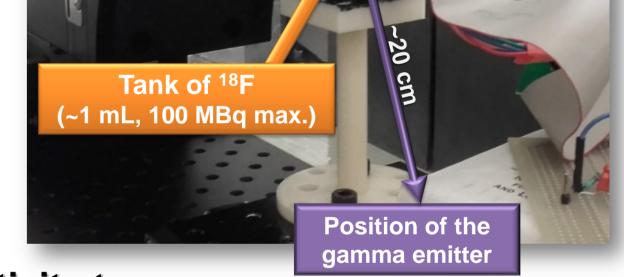
- Diced and thinned sensors glued back-to-back
  - Successful tests with individual sensors thinned to 150, 200, and 250 µm Ο
  - Total volume of the needle: 610 x 12000 x 500 µm<sup>3</sup> 0



### Produced at the Cyrcé cyclotron (IPHC)







### Sensitivity to y-rays

- <sup>18</sup>F solution with low activity close to the sensor: majority of positrons measured
- <sup>18</sup>F solution with high activity (~100 MBq) ~ 20 cm away from the sensor (head-bladder distance) : γ-rays only
- The y-ray contribution increases the mean #clusters/frame from positrons by 3.5 % only
- The beta+gamma measurement with the two sources at a time is 300x higher than for gamma only

### $\rightarrow$ IMIC is immune to 511 keV $\gamma$ -rays

### <sup>18</sup>F decay

- $\circ$  6 hours = 3 periods
  - Starting activity ~ 24 MBq
  - Ending activity ~ 2.5 MBq
- Integration time: 500 µs Ο
- Pile-up for high activity (counting limited to 1 bit) Ο
- Exponential decay measured at the expected operation activity

### **V. CONCLUSIONS & PERSPECTIVES**

• **Requirements reached:** functional CMOS monolithic active pixel sensor

- $\circ$  Low power: 161  $\mu$ W
- Compatible to the awaited activities of the radiotracers
- $\circ$  Immune to the 511 keV y-rays

### Outlooks

- Tests of the double-sided probe
- System integration (backpack)
- Coating with biocompatible polymer (Parylene) Ο
- In-situ experiments
- Tests and characterization of IMIC-LF: DMAPS version of IMIC (CPPM)

### REFERENCES

[1] Y. Gao et al. (2017) Time to wake up: Studying neurovascular coupling and brain-wide circuit function in the un-anesthetized animal. NeuroImage 153 : 382–398. [2] J. Godart et al. (2010) PIXSIC: A Pixellated Beta-Microprobe for Kinetic Measurements of Radiotracers on Awake and Freely Moving Small Animals. IEEE Trans. Nucl. Sci. 57 (3): 998-1007. [3] L. Balasse et al. (2015) PIXSIC, a pixelated β+-sensitive probe for radiopharmacological investigations in rat brain: binding studies with 18F-MPPF. Mol. Imaging Biol. 17 (2): 163-167. [4] L. Balasse et al. (2015) PIXSIC: a wireless intracerebral radiosensitive probe in freely moving rats. Mol. Imaging 14 (43): 484-489. [5] M. Mager. (2016) ALPIDE, the Monolithic Active Pixel Sensor for the ALICE ITS upgrade, Nucl. Instr. Meth. Phys. Res. A 824: 434-438.