

Development of  
innovative PET  
module with DOI  
and timing capability

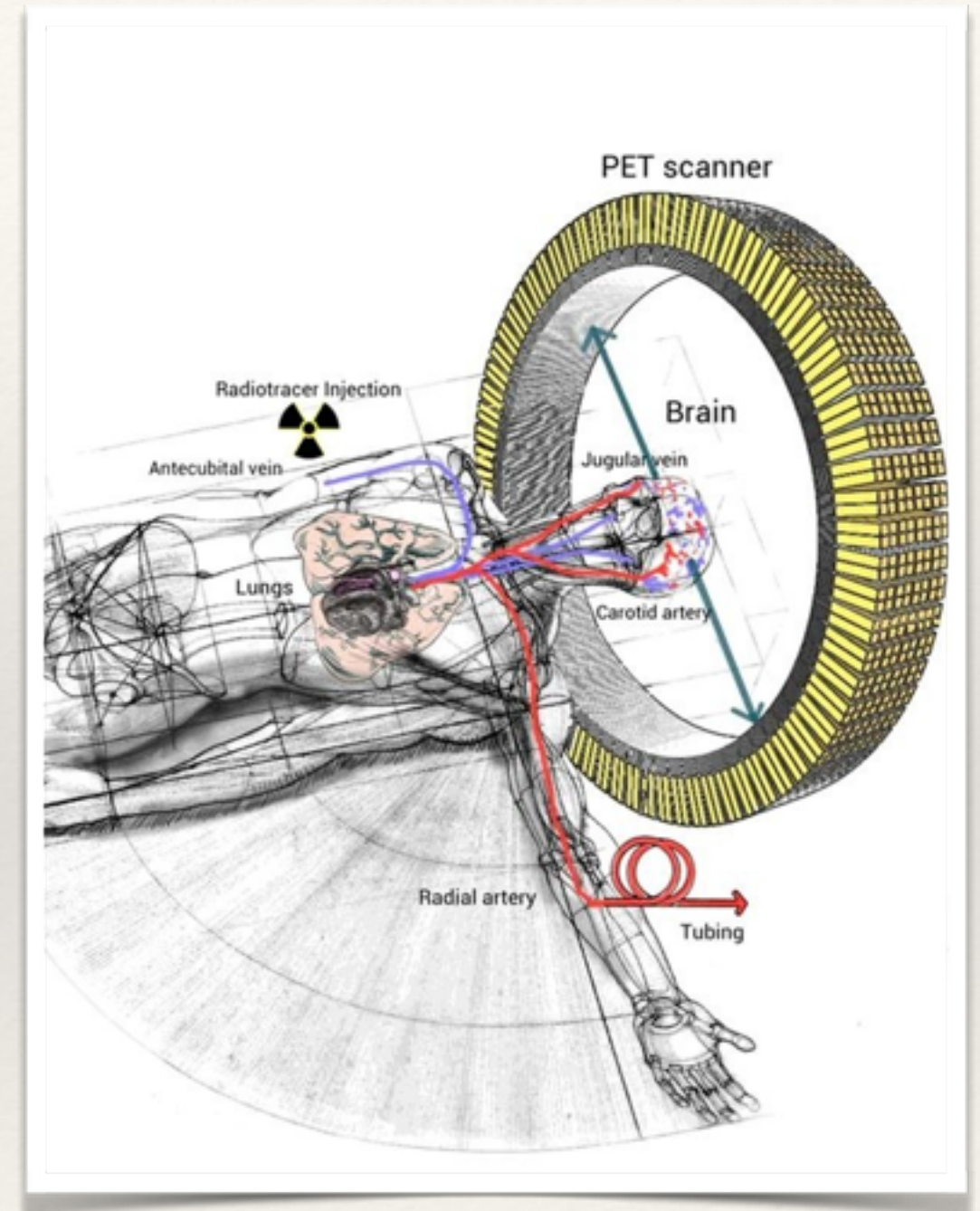
Gianluca Stringhini



CERN KT Project "New ClearPEM module"  
CERN KT Project "Detector module development for Whole  
Body PET"

# Positron Emission Tomography

- ❖ Radiotracer labelled with a positron emitter ( $^{18}\text{F}$ -FDG)
- ❖ Positron annihilation and production of two back to back gammas (511 keV)
- ❖ Detection of the two gammas in coincidence using detectors

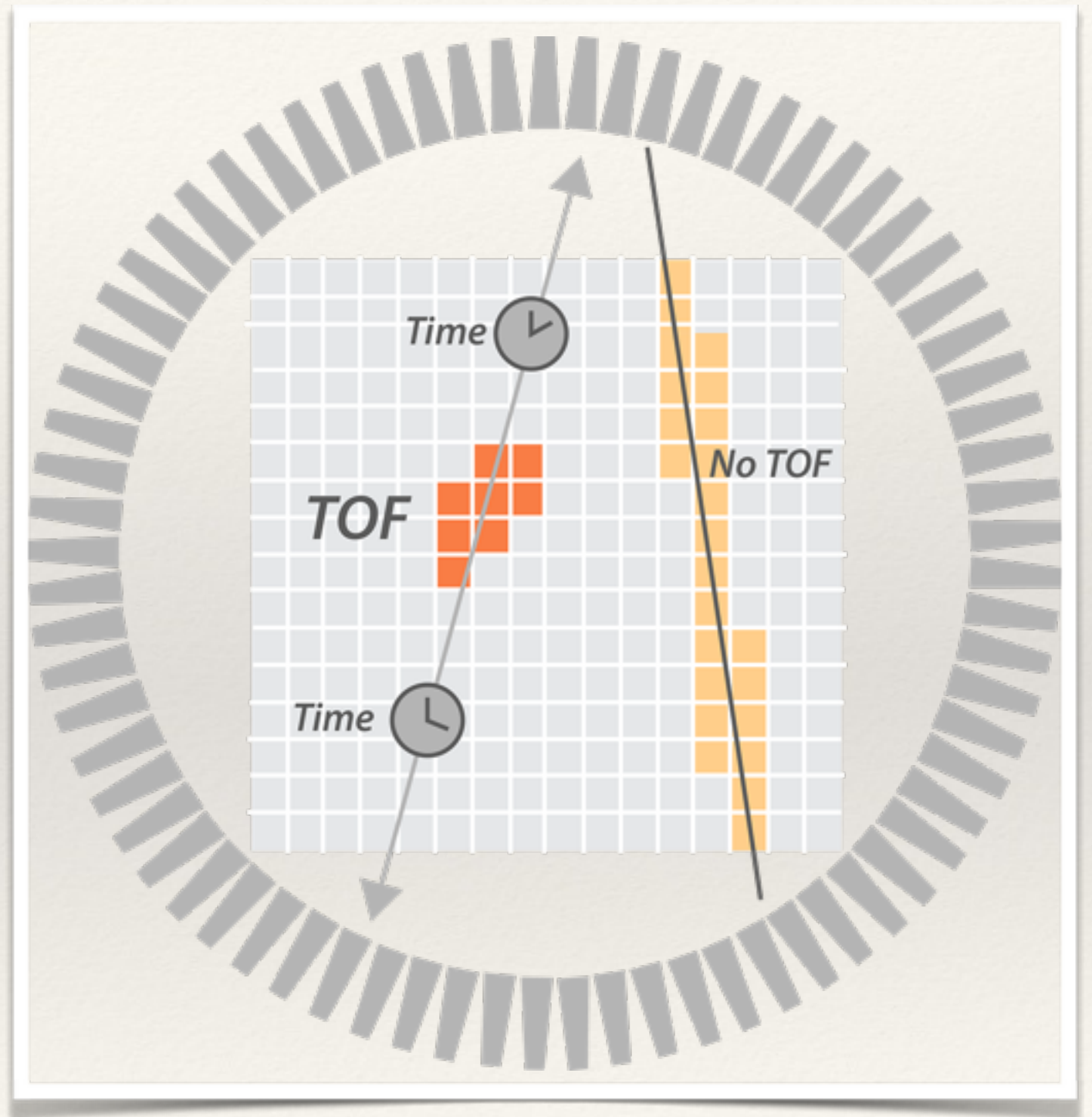




# Time of Flight

Knowing the arrival time of the two gammas, it is possible to reduce the region where the annihilation took place and increase the signal to noise ratio.

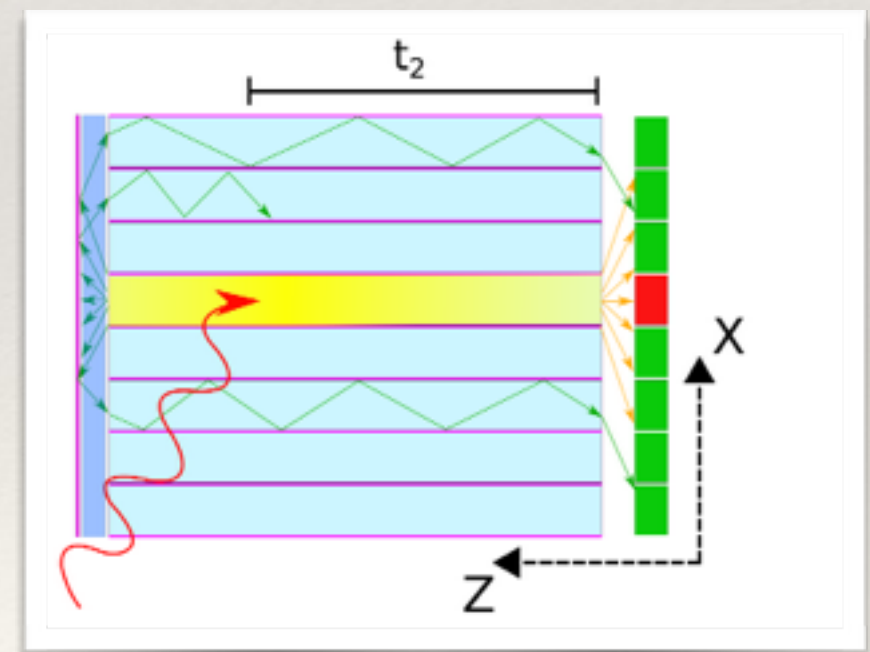
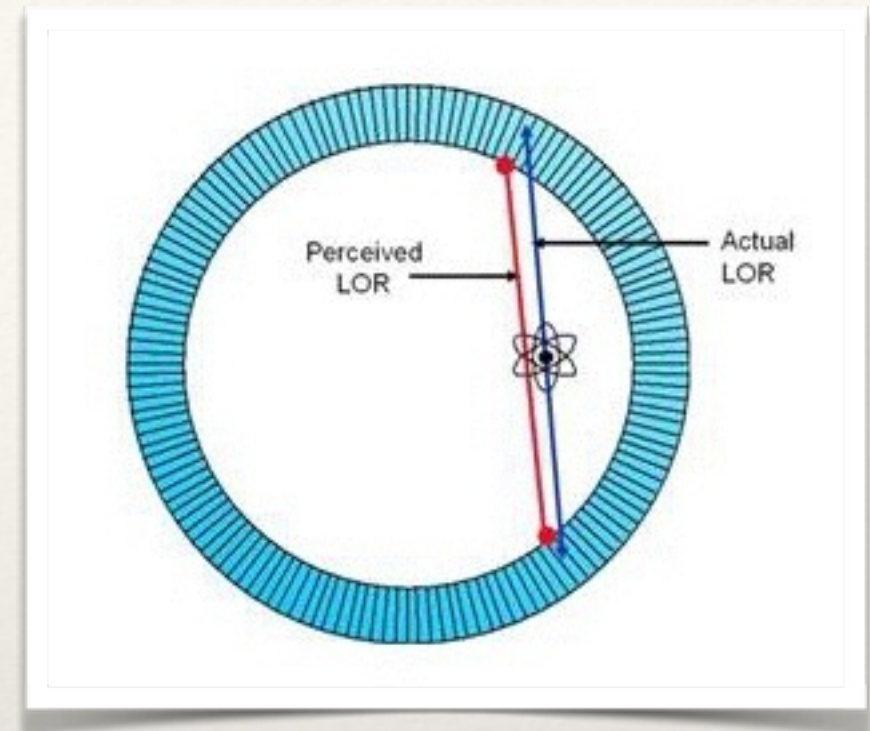
➡ Fast detector



# Depth of Interaction

Knowing the interaction point position along the main axis of the scintillator allow to reach high performances:

- ❖ Small animal and organ dedicated scanner: to avoid parallax error and obtain high quality images.
- ❖ Whole body scanner: to correct for the time jitter of the photon propagation along the crystal.





# Aim of our study

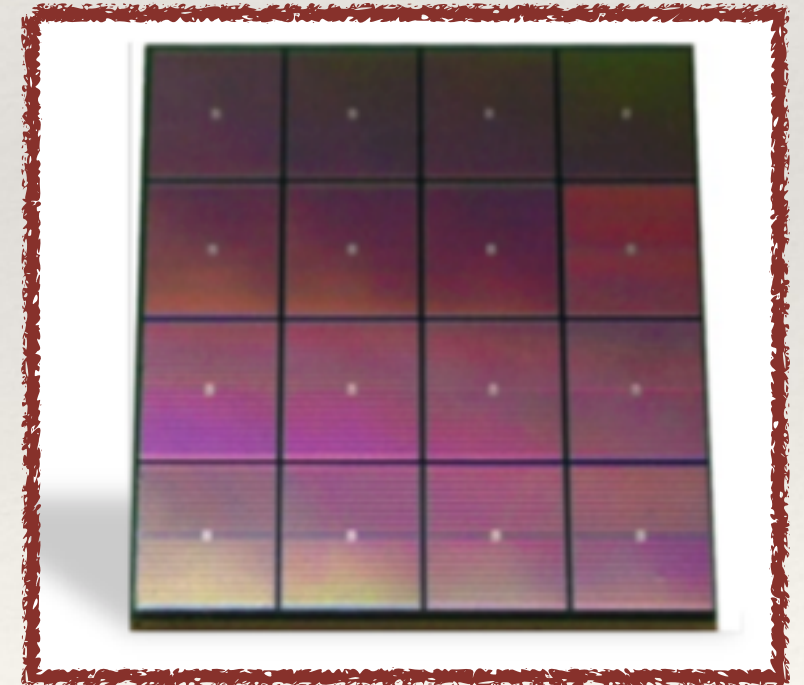
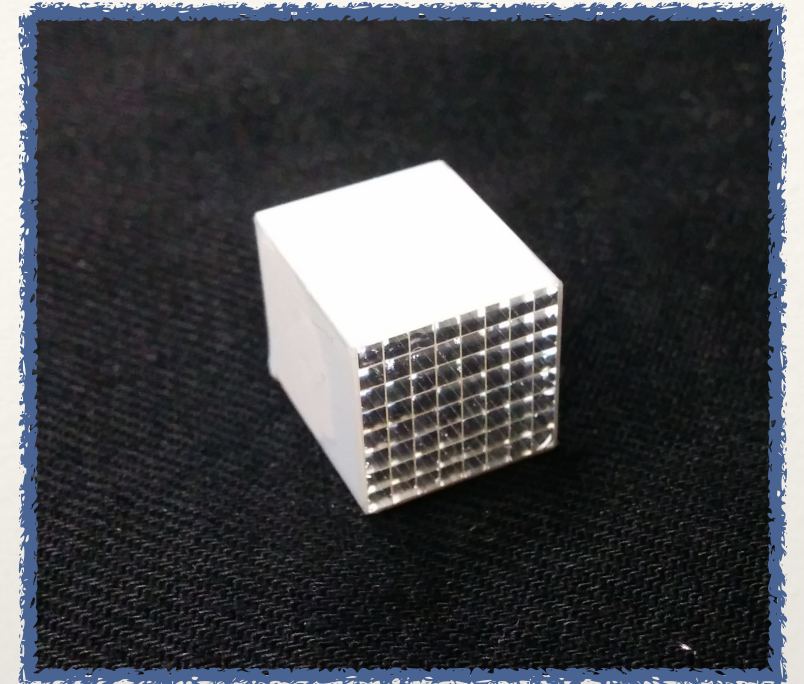
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To develop an innovative PET module that allows to reach high performances in term of spatial resolution and energy resolution while keeping the complexity of the system reasonably low.

- ❖ 4 to 1 coupling between the scintillator and the detectors
- ❖ Depth of Interaction (DOI) capability with a single side readout
- ❖ High timing performances

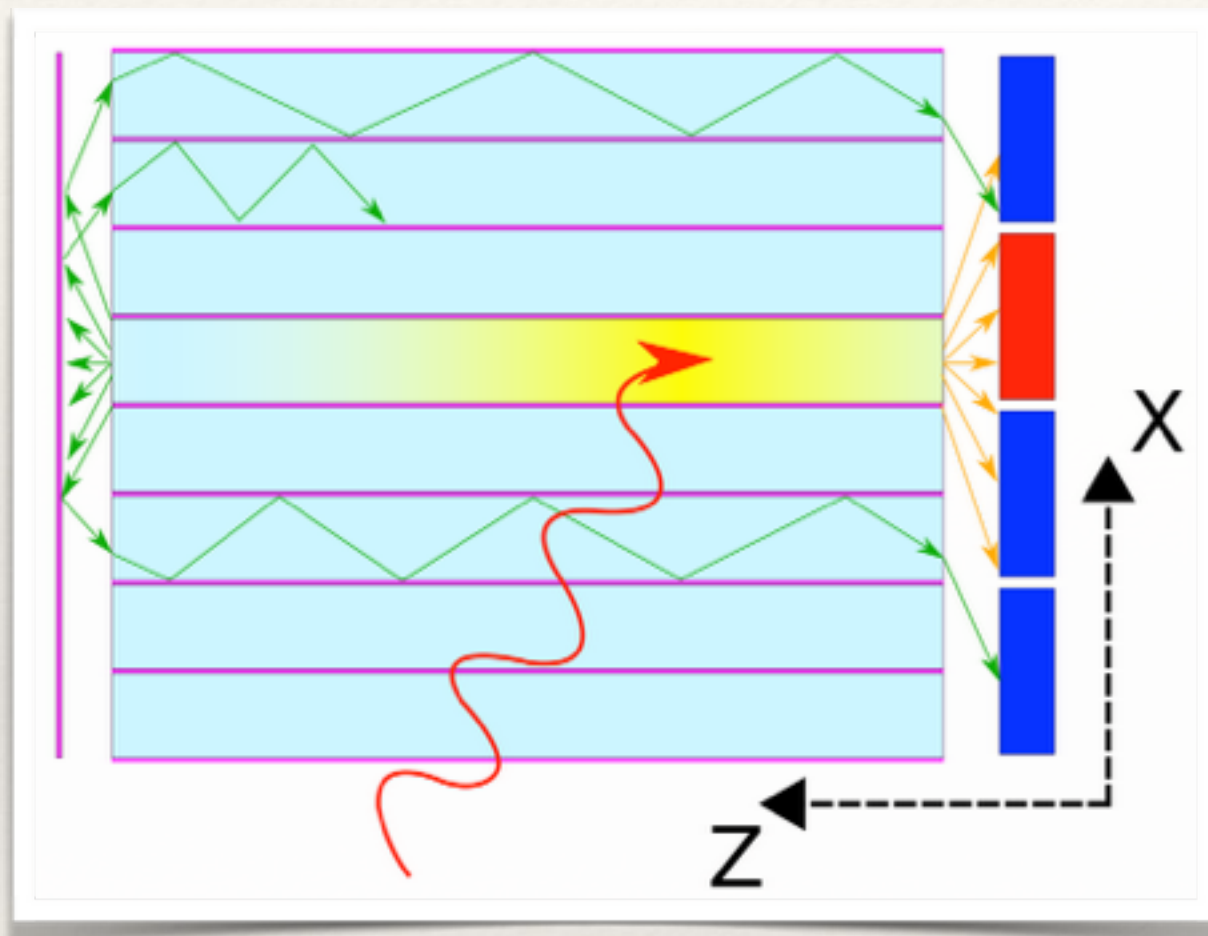
# Our innovative PET module

- ❖ LYSO crystals matrix (8x8)
  - ❖ Crystal dimensions:  $1.5 \times 1.5 \times 15 \text{ mm}^3$
  - ❖ Separation foil: ESR
  - ❖ Lateral surfaces of the crystals depolished
- 
- ❖ 4x4 MPPC array from Hamamatsu
  - ❖ Active area  $3 \times 3 \text{ mm}^2$
  - ❖ Pitch 3.1 mm





# A new approach to the DOI

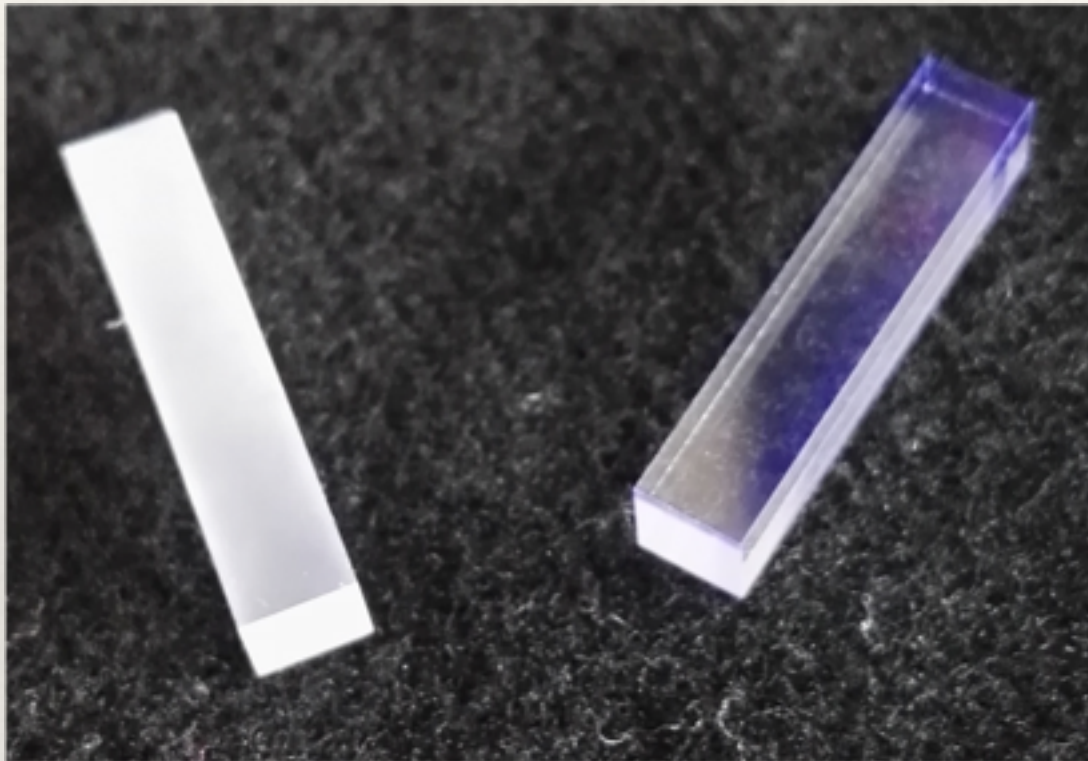


- ❖ Only one side readout
- ❖ Light guide on top of the module
- ❖ Reflector that redirects the light to the detector
- ❖ optical treatment of the lateral surface of the crystals

# A new approach to the DOI

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Optical treatment of the lateral surfaces of the crystals:  
**DEPOLISHING.**



The **DEPOLISHING** increases the probability for a optical photon to escape from the crystal during a lateral surface scattering.

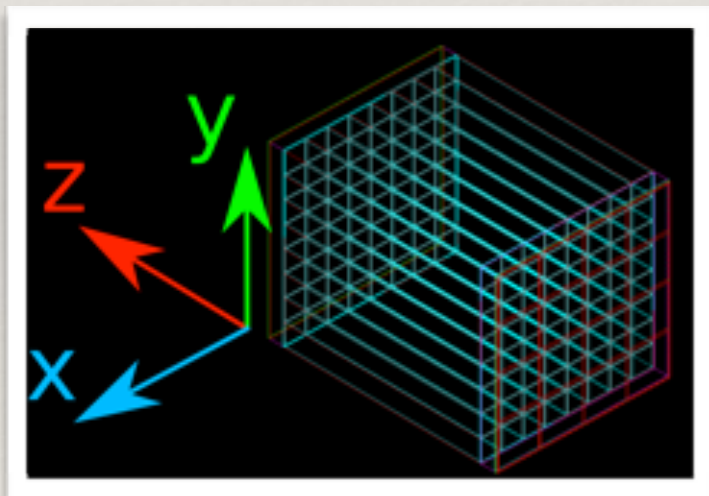
It leads to a correlation between the light collected by the detector and DOI.



# The procedure

Obtain the  $(x,y,z)$  interaction point for each event using combinations of the detected charges information:

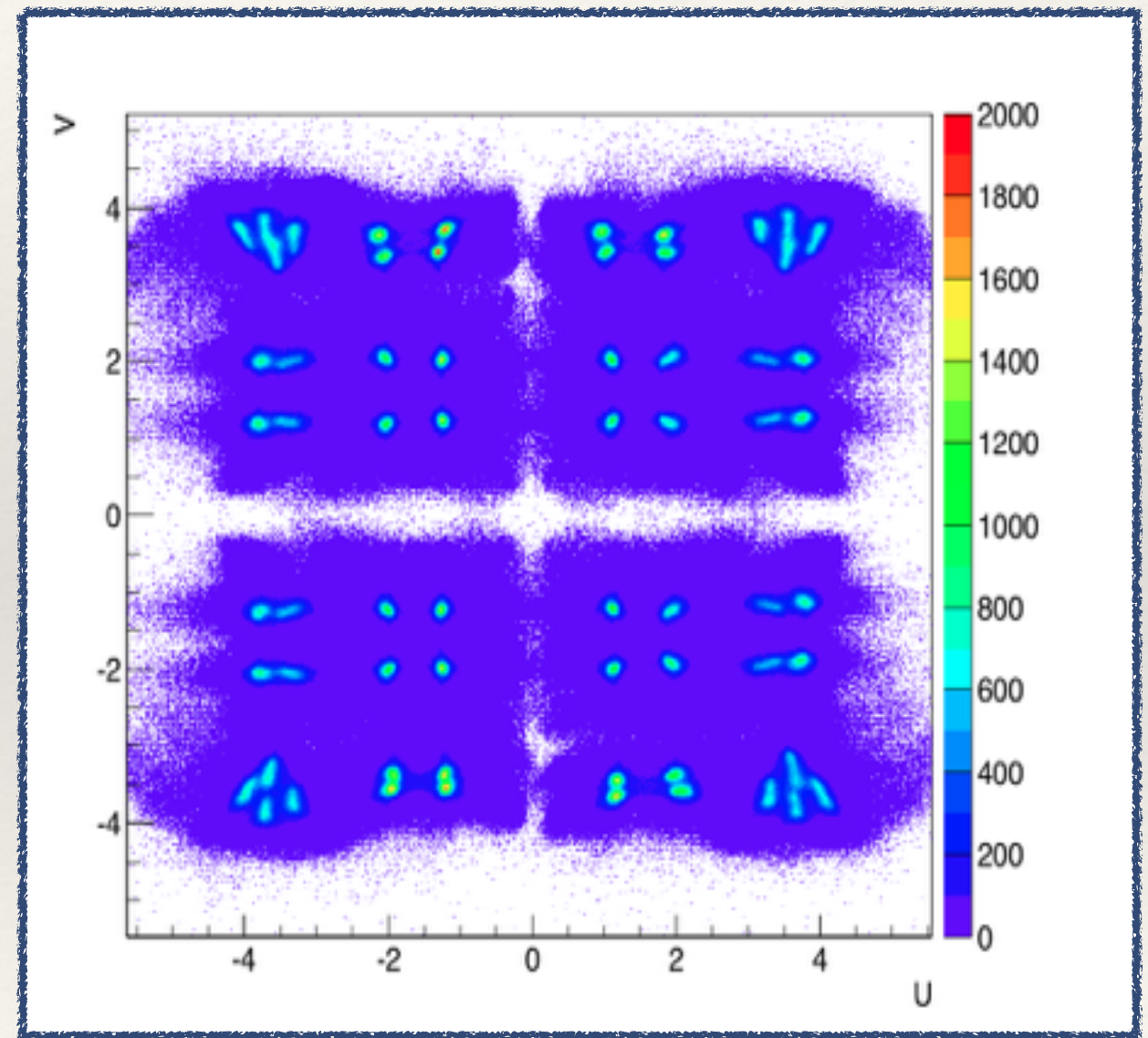
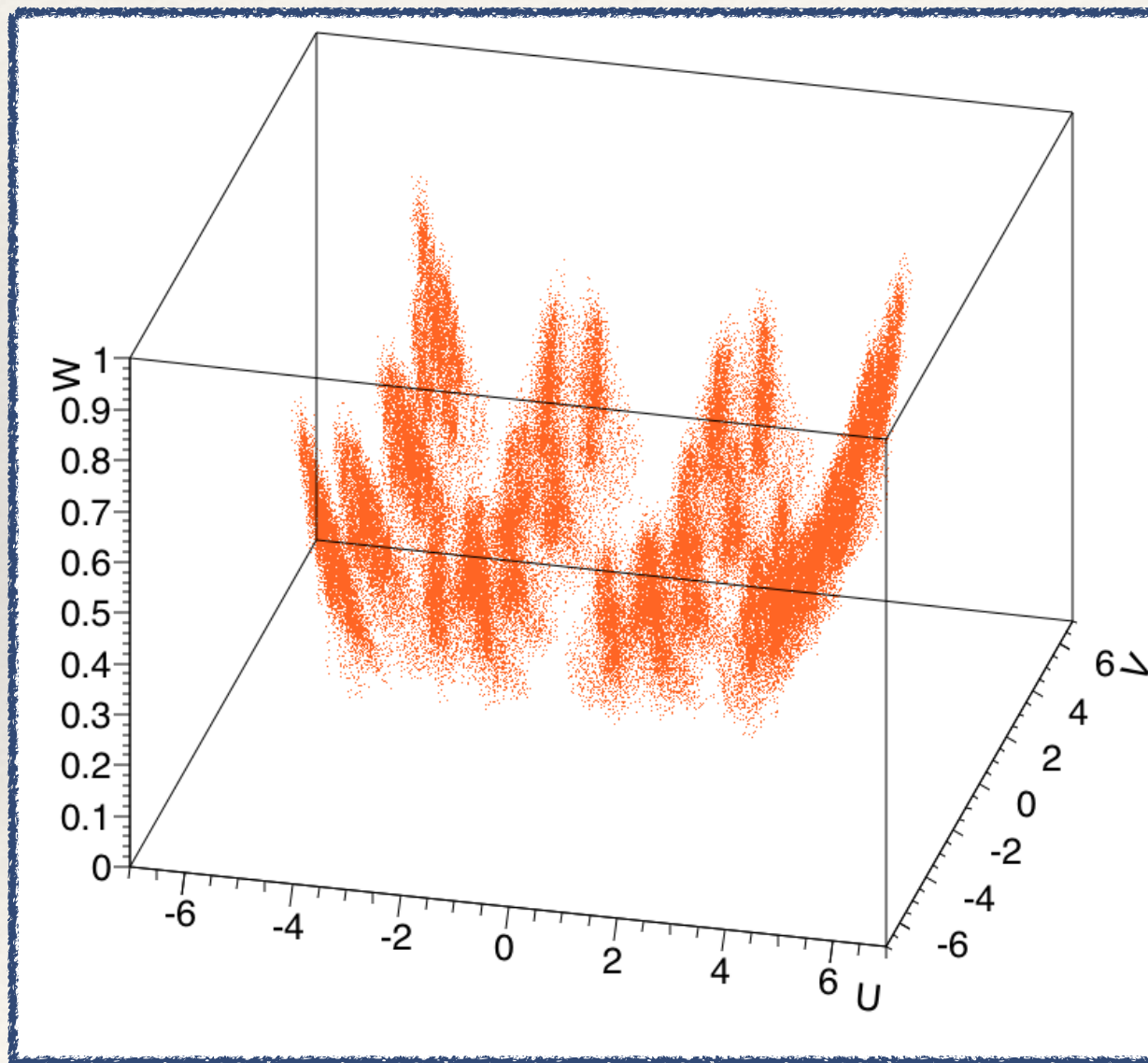
$$u = \frac{1}{P} \sum_i^{16} p_i X_i \quad v = \frac{1}{P} \sum_i^{16} p_i Y_i \quad w = \frac{p_{max}}{P}$$



- ❖  $p_i$  : charge collected by the  $i$ -th detector
- ❖  $X_i$  and  $Y_i$  : positions of the center of the  $i$ -th detector
- ❖  $P$ : sum of the charges collected by the detectors for each event
- ❖  $P_{max}$ : maximum of the charge collected among the  $i$  charges collected

# The performances

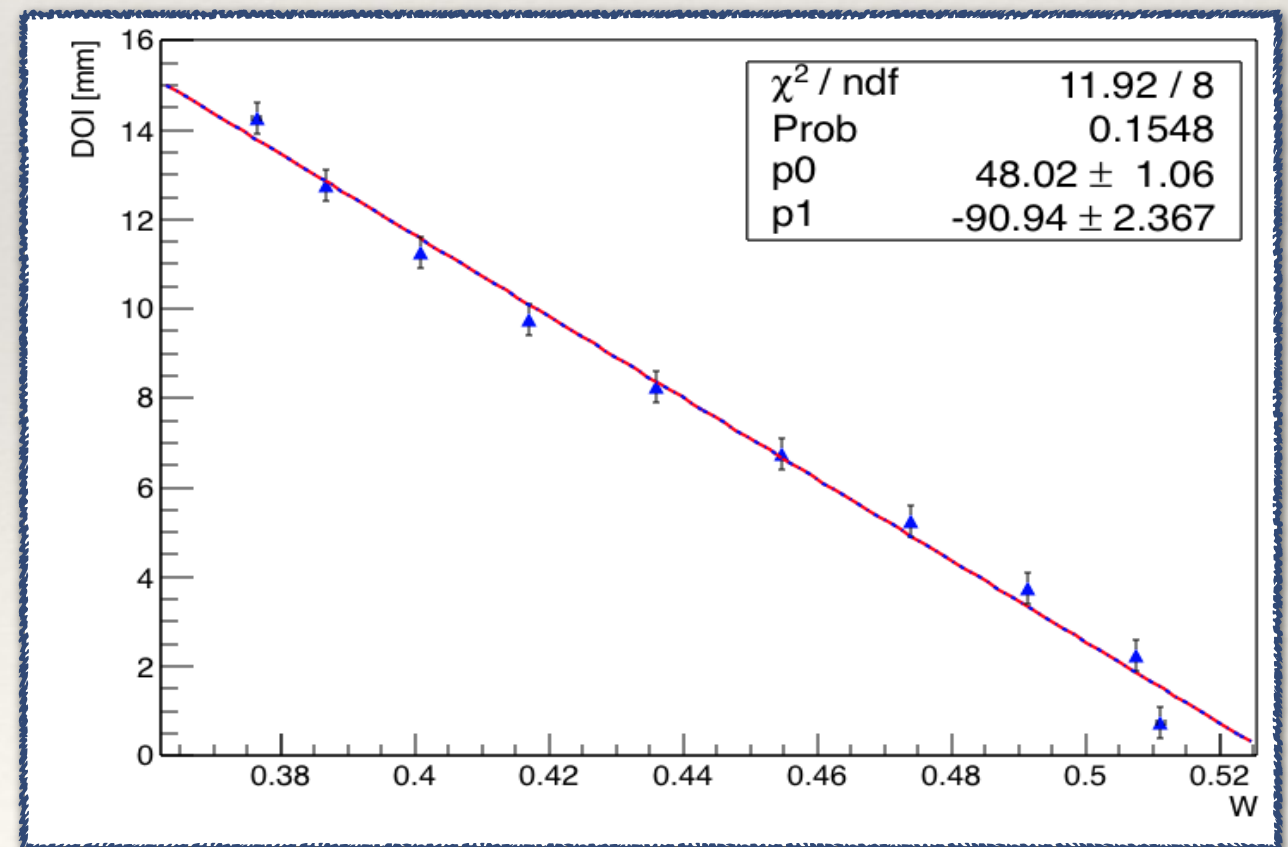
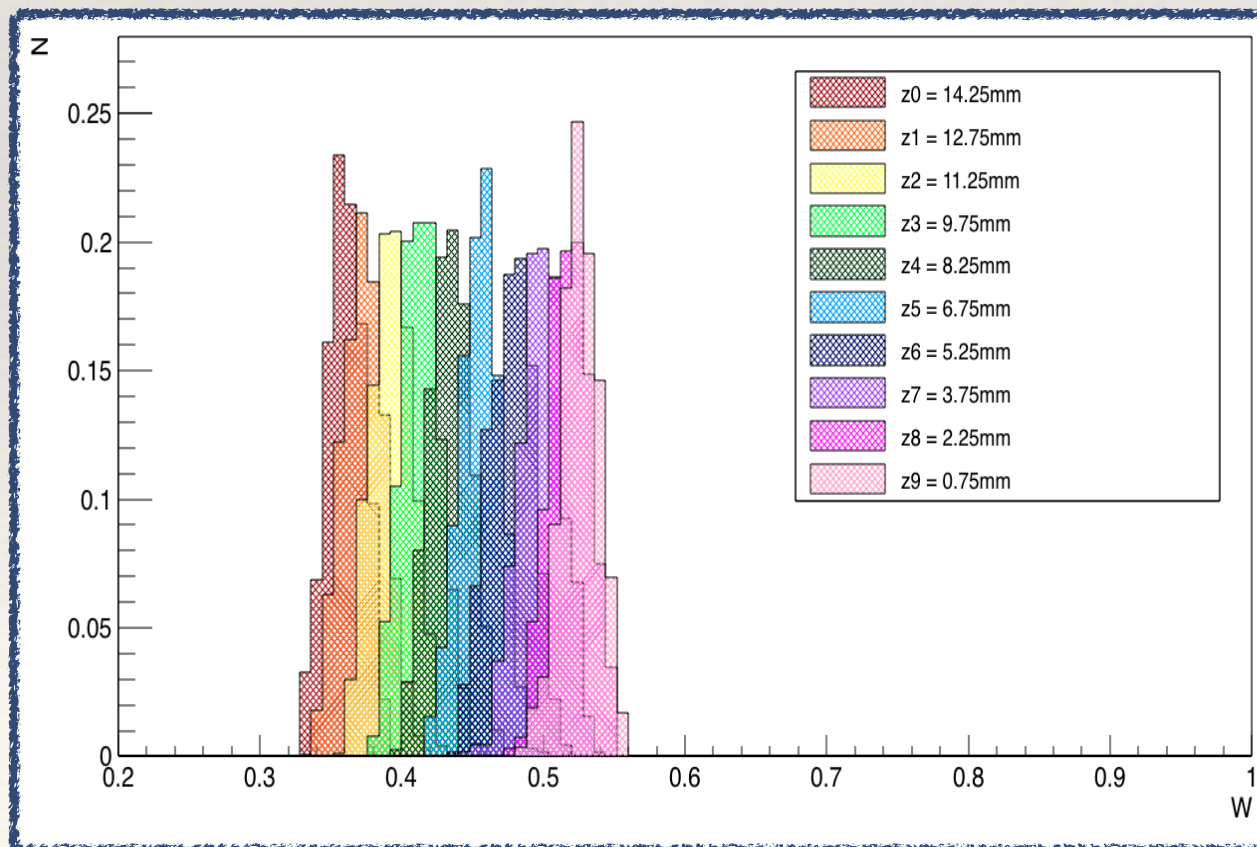
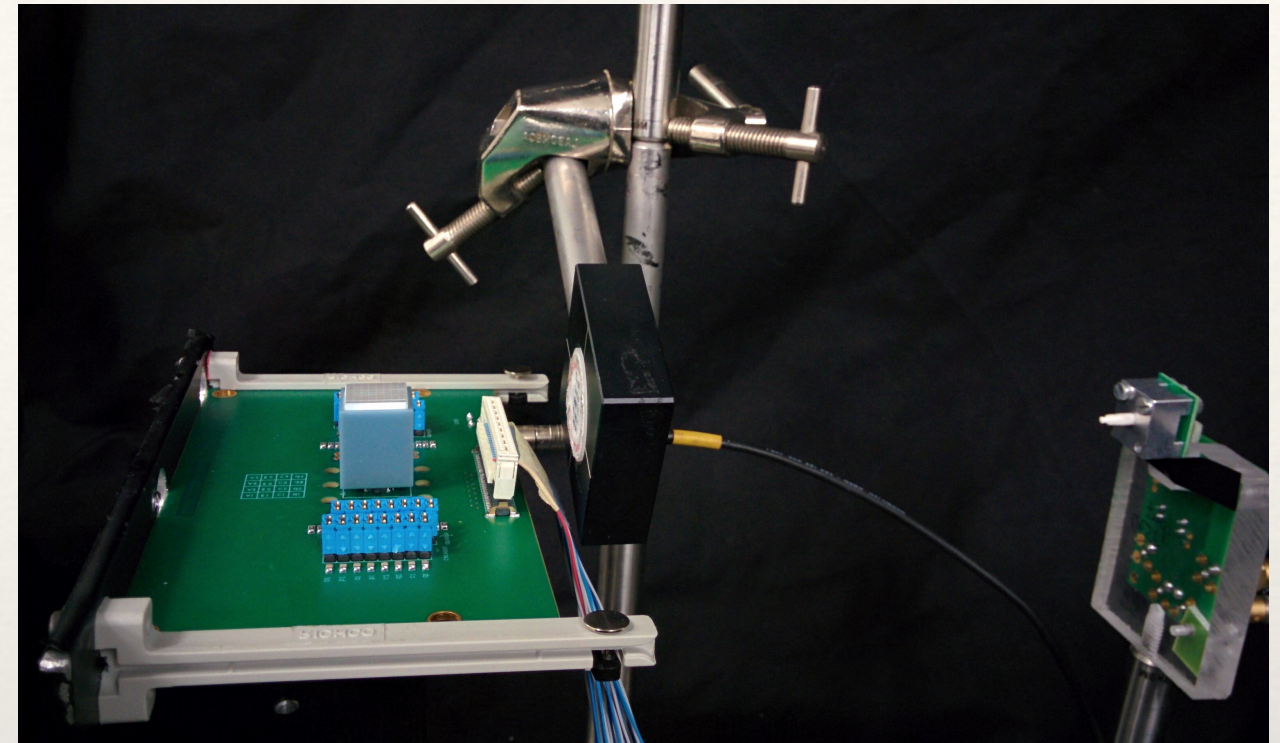
Excitation with a radioactive source  $\text{Na}^{22}$  placed 10 cm above the module





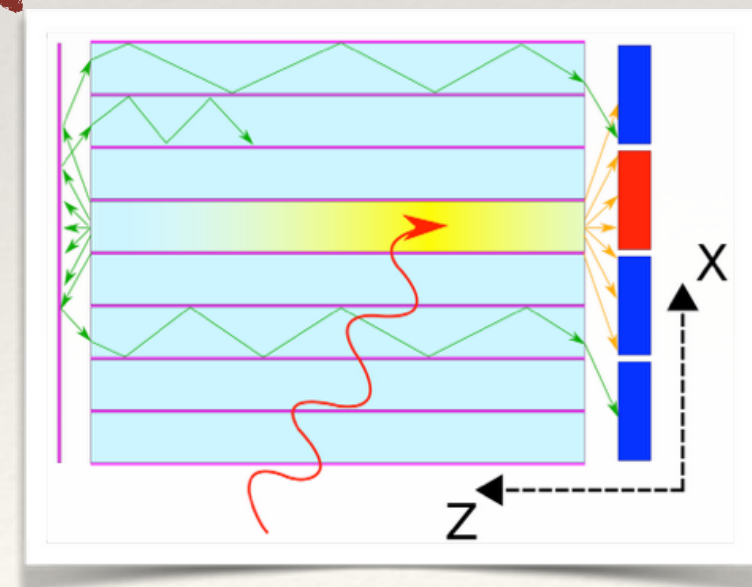
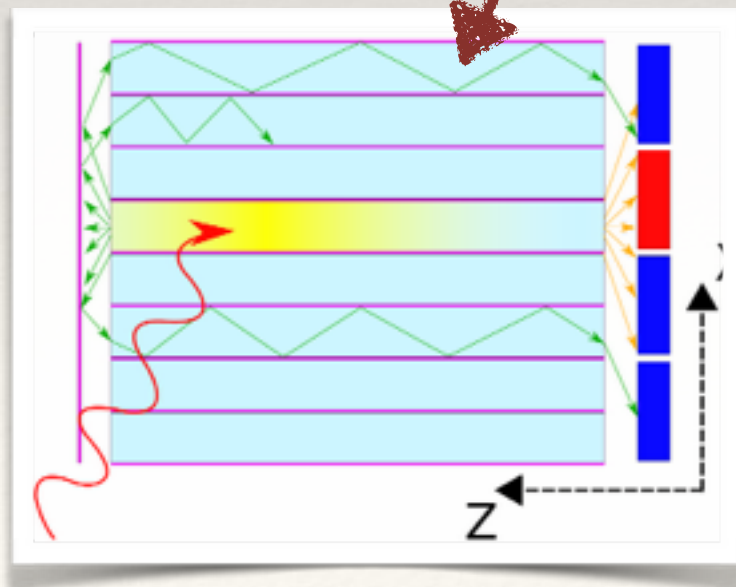
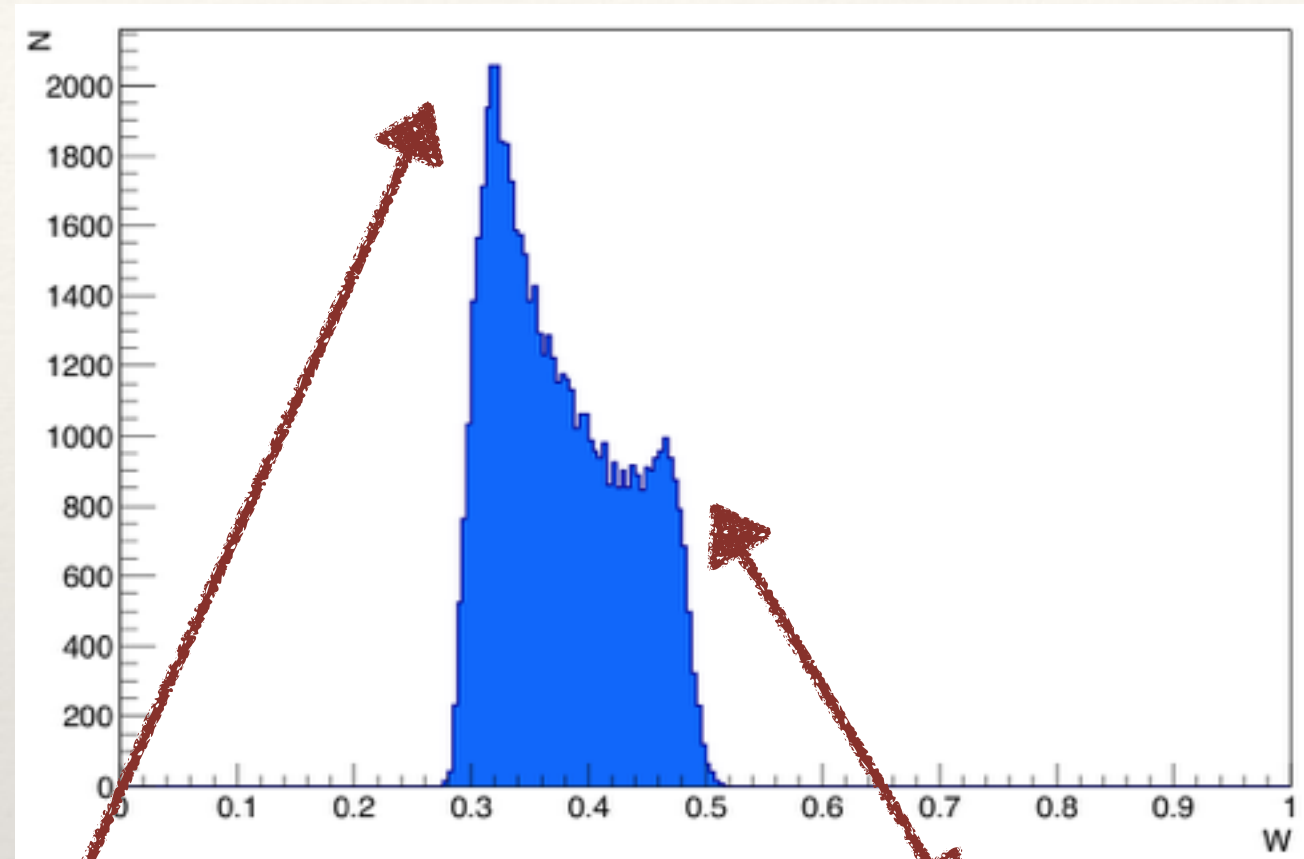
# The performances

- ❖ Energy resolution: 12% (FWHM)
- ❖ Spatial resolution: 1.5 mm (FWHM)
- ❖ DOI resolution: 3 mm (FWHM)



# DOI Calibration

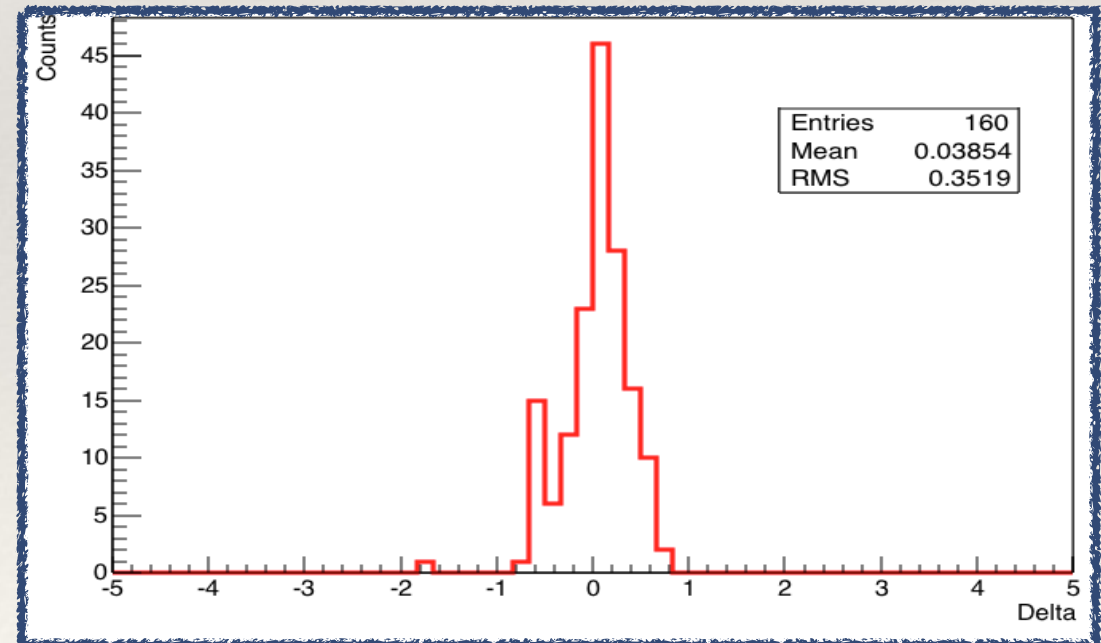
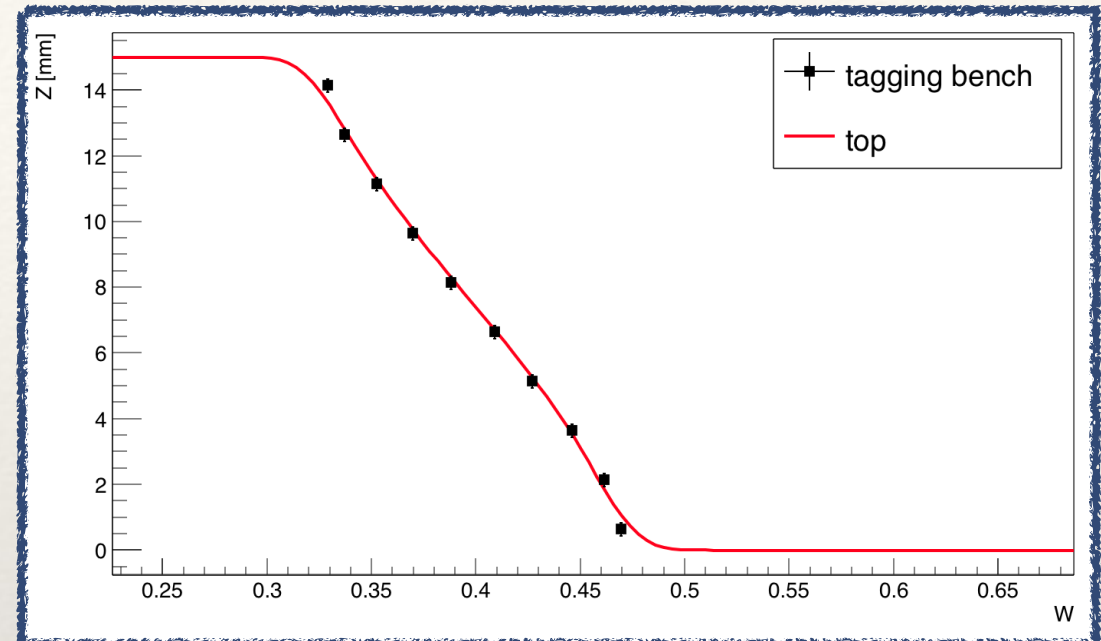
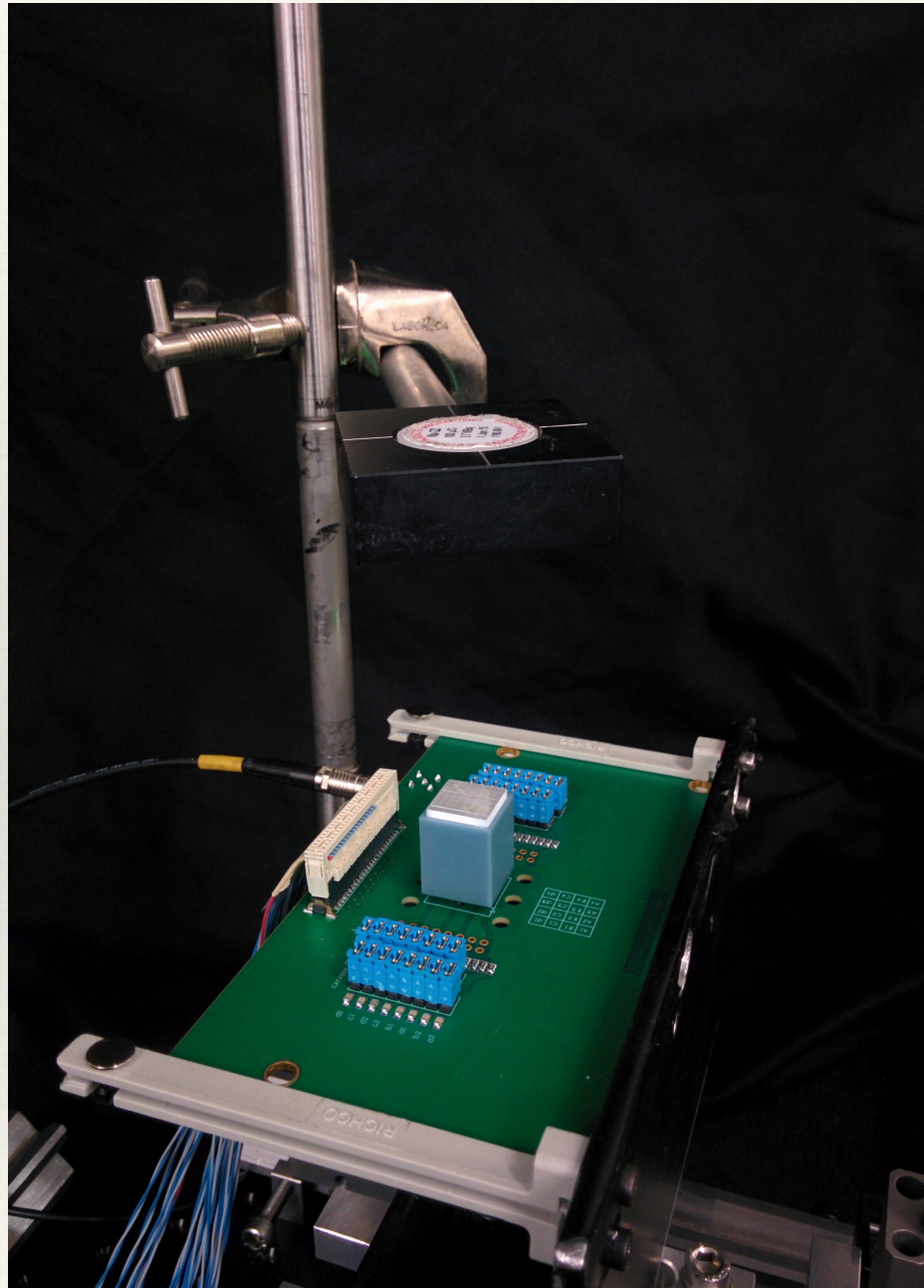
DOI calibration with the external tagging crystal is unfeasible in a real PET scanner





# DOI Calibration

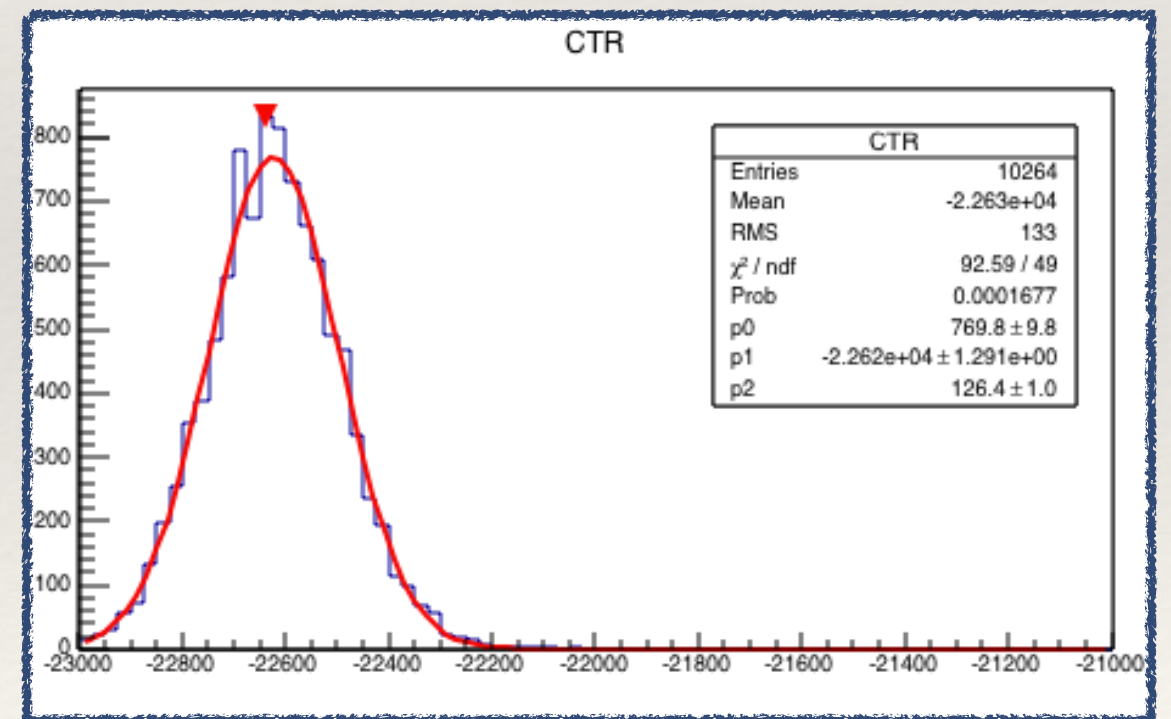
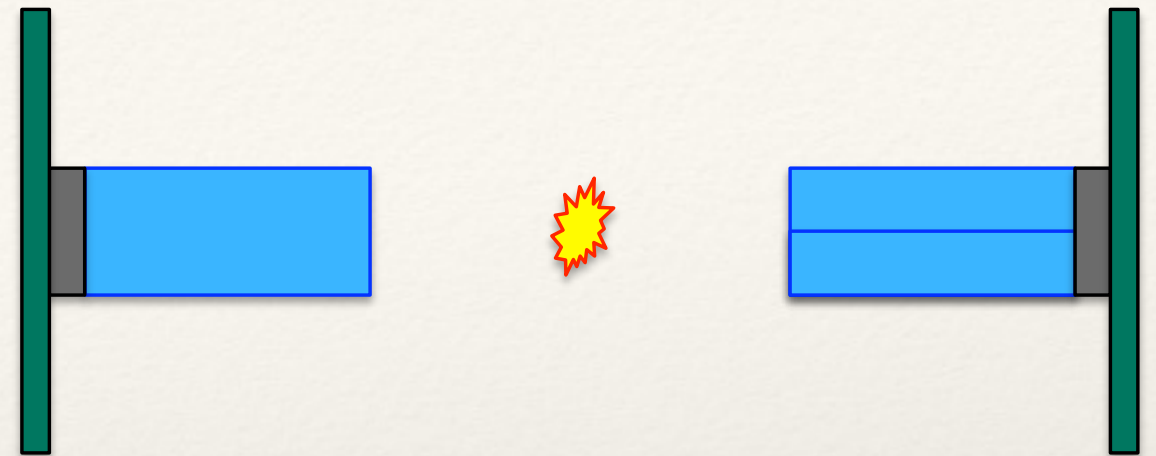
Development of a practical DOI calibration method without using an external tagging crystal.



# Coincidence Time Resolution

The CTR is a fundamental parameter to reduce the signal to noise ratio. Using the NINO chip (a low power front-end amplifier and discriminator) we measured the timing performances of the module.

First measurement: CTR  $\sim$  300 ps FWHM

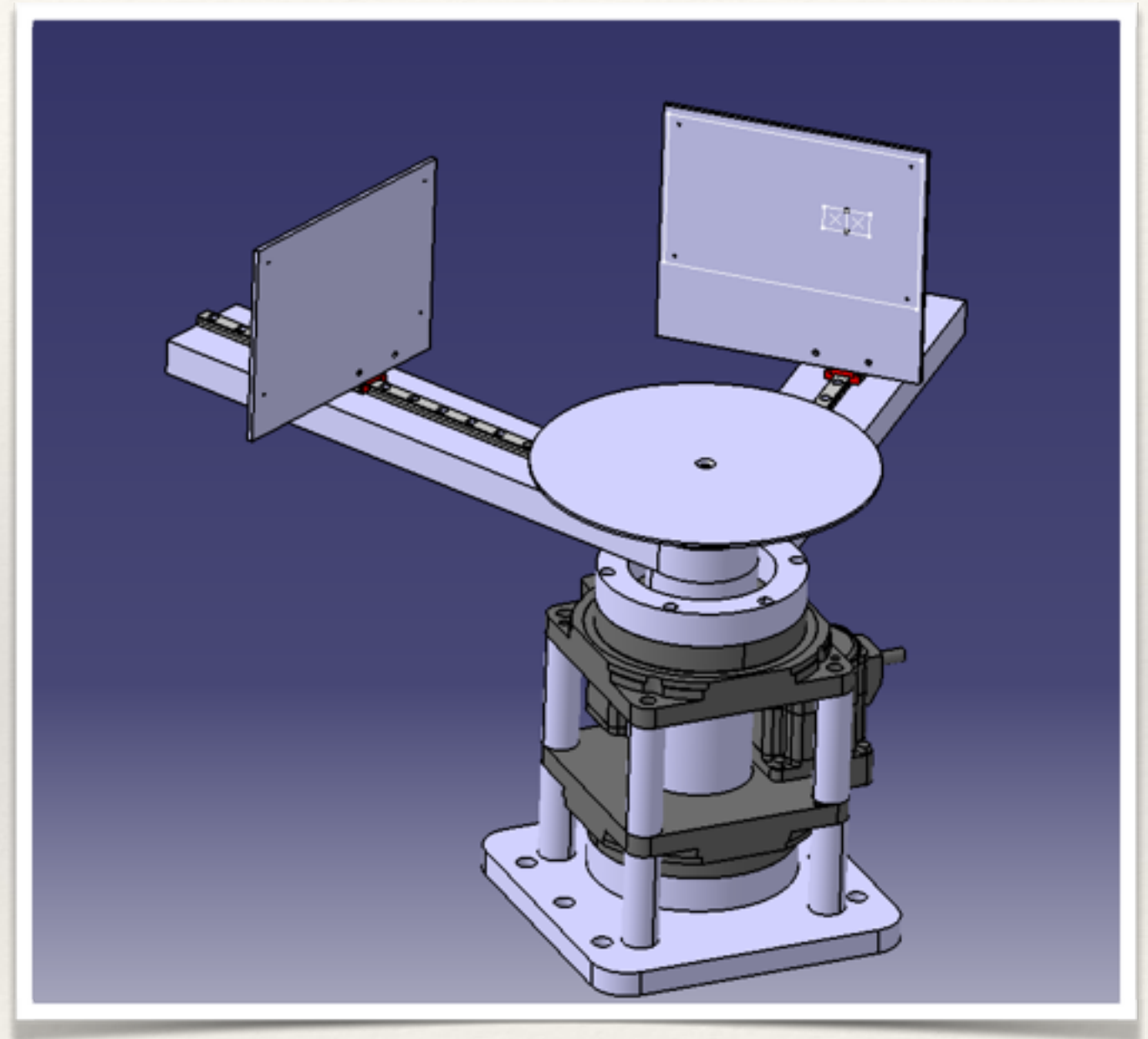




# Ongoing...

Small PET demonstrator:

- ❖ Two rotating arms
- ❖ Integration of the charge
- ❖ Time information
- ❖ Reconstruction algorithm (STIR)



Credit: Oscar Sacristan De Frutos