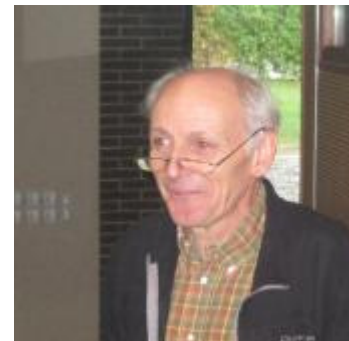




## **2012 :15th SESSION of ESMP**

**Lecture presented in Archamps (Salève Building) by :**

**Christian CACHARD (CREATIS Lyon)**



Erasmus MC  
Rotterdam  
The Netherlands



## Intravascular imaging

Nico de Jong

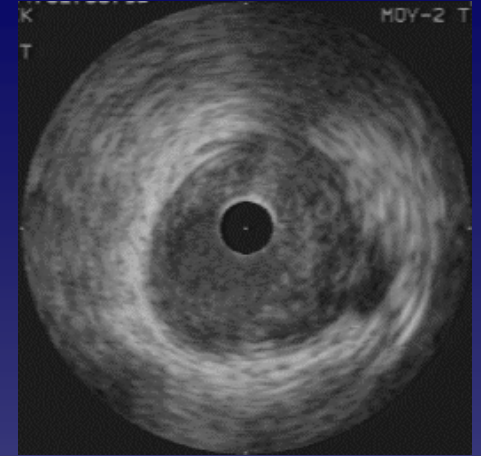
Presented (and adapted) by  
Christian Cachard



# Outline

- General presentation
  - principal features, contributions to diagnosis
- Image formation
  - Image formation
  - catheter technologies
  - Geometric artefacts
- IVUS in the clinic
- IVUS diagnostic modality under investigation

# General presentation



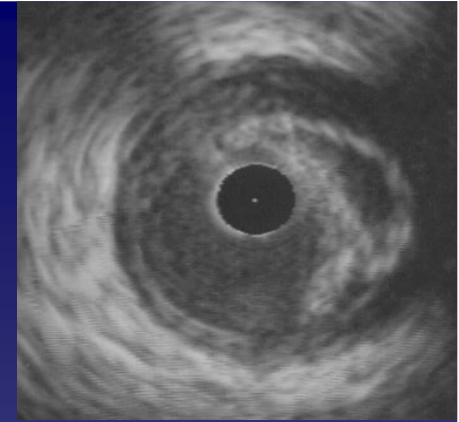
- Usefulness in cardiology
  - diagnosis of atherosclerotic coronary artery disease
  - guiding therapeutic procedures (balloon angioplasty, stenting)
- High resolution cross-sectional images of vessel walls in real time
- Frequency: 30-40 MHz, depth < 10 mm

# General Presentation

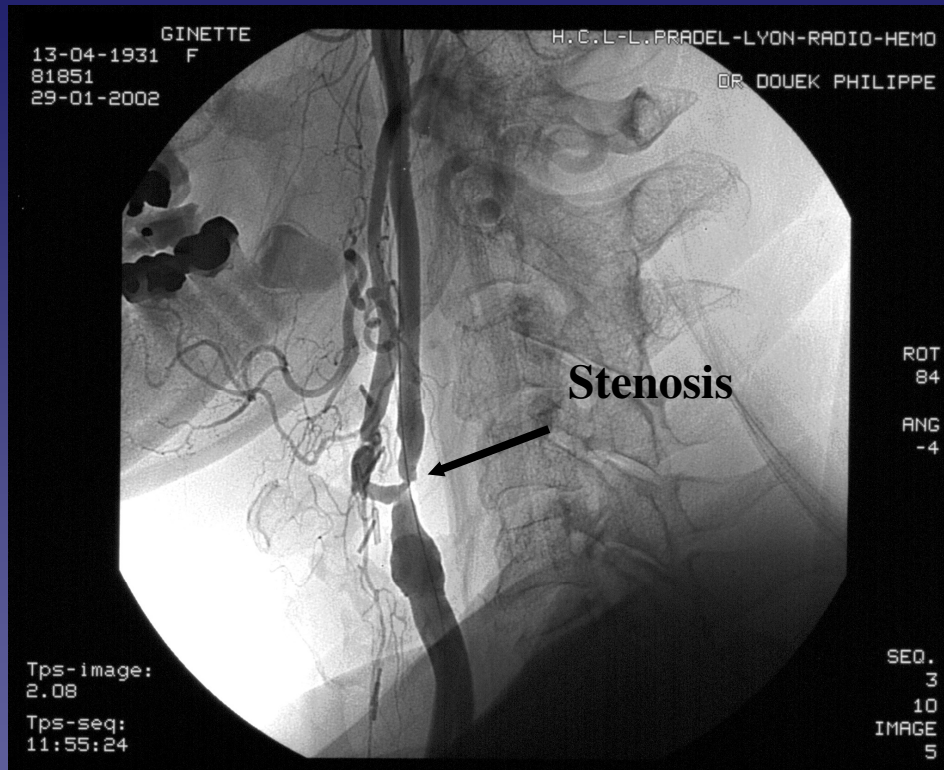
- Well spread in the middle of interventional cardiology
  - ex: in France, among 135 centres of angioplasty 30 have intravascular ultrasound imaging
- Time of examination : 5 to 10 mn
- Cost : 800 € (depends on the catheter used)
- Operating room

- Main advantages

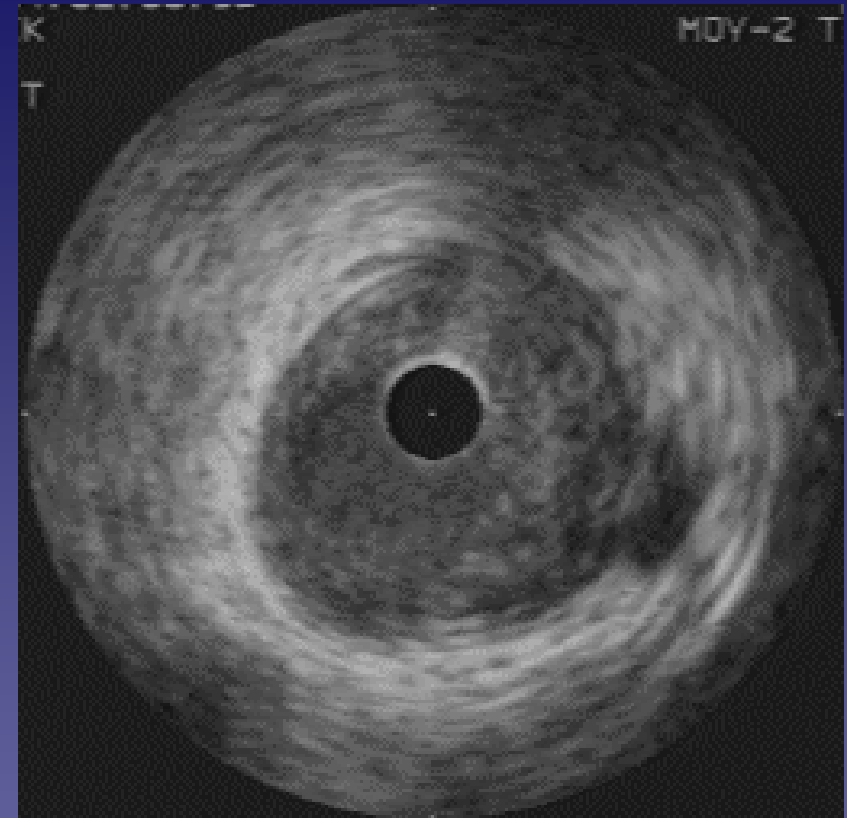
- qualitative analysis by characterising *roughly* plaque components, plaque rupture or acute thrombosis
- depicting atherosclerotic plaque morphology and remodeling
- 2D and 3D quantitative analyses by precise measurements
  - arterial dimensions (diameter and area)
  - % stenosis
  - plaque volume



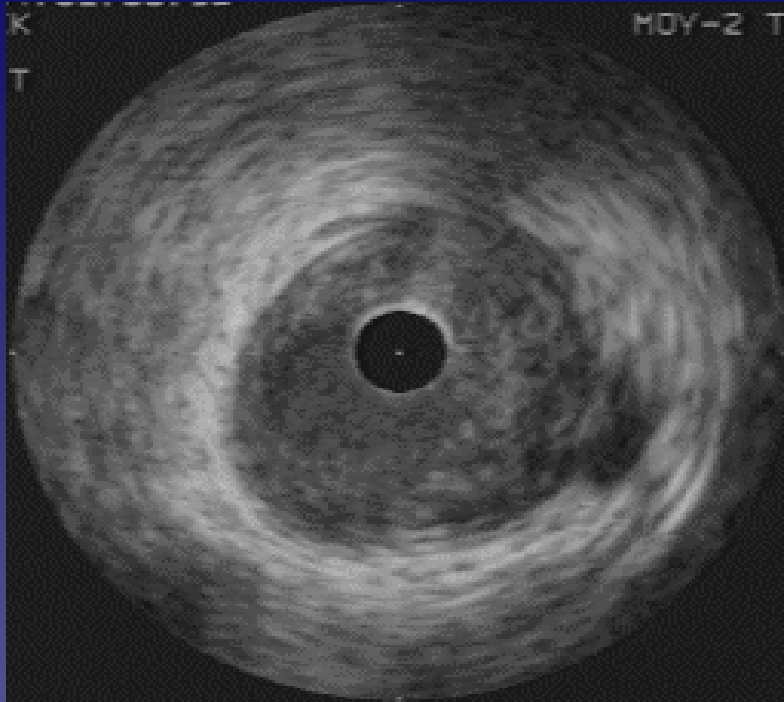
# Imaging of the vessels



X-ray angiography  
skeleton image of artery



Intravascular Ultrasound  
(IVUS)  
cross-sectional image of artery



## Intravascular Ultrasound (IVUS)

- IVUS provides **real time cross-sectional** images *in vivo* of vessels.

IVUS provides specific diagnostic information and guides interventional techniques for treatment of atherosclerotic luminal narrowing

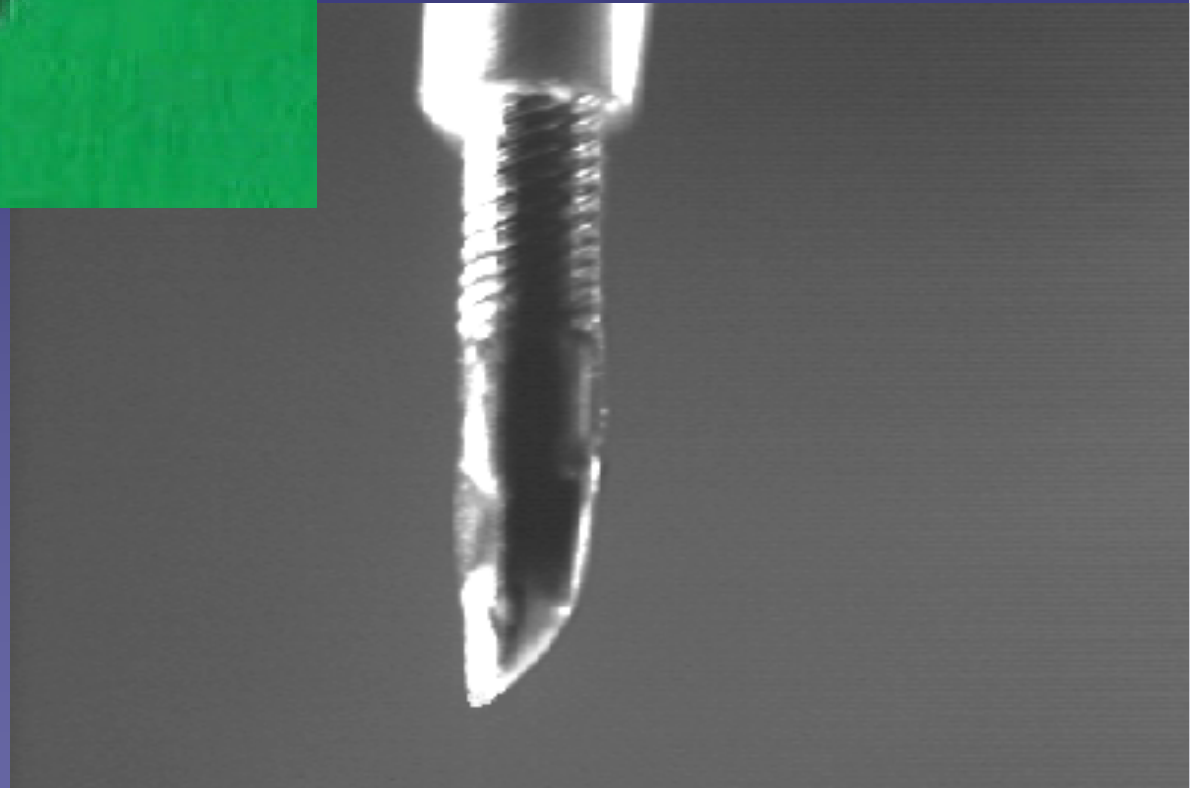
IVUS is used for studying the mechanisms for restenosis .



# Image formation

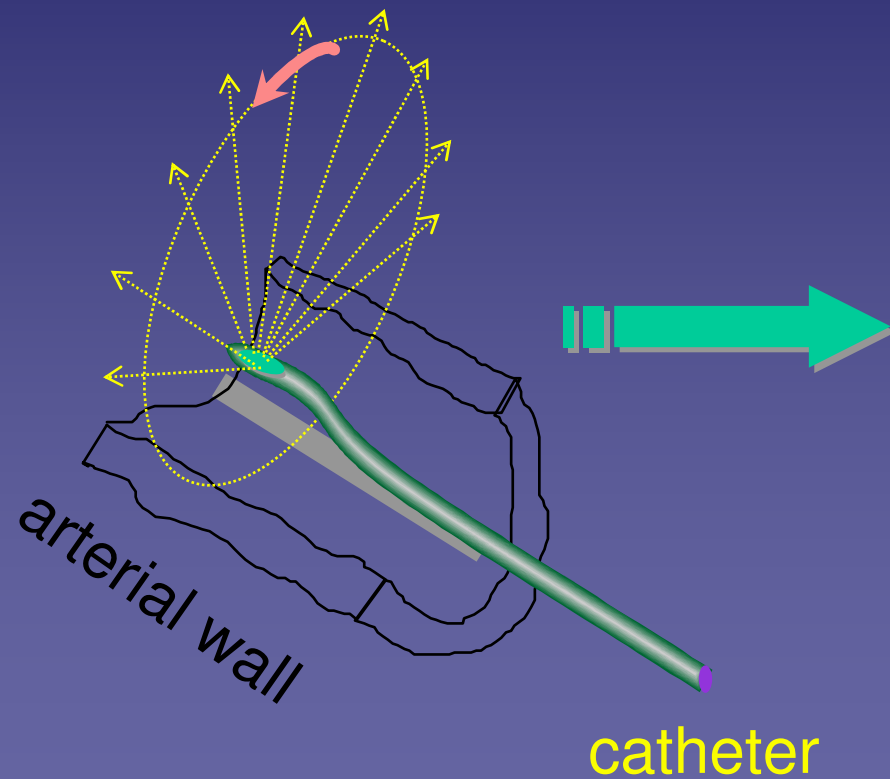
Catheter diameter  $\cong$  1mm

IVUS is an **invasive** imaging modality

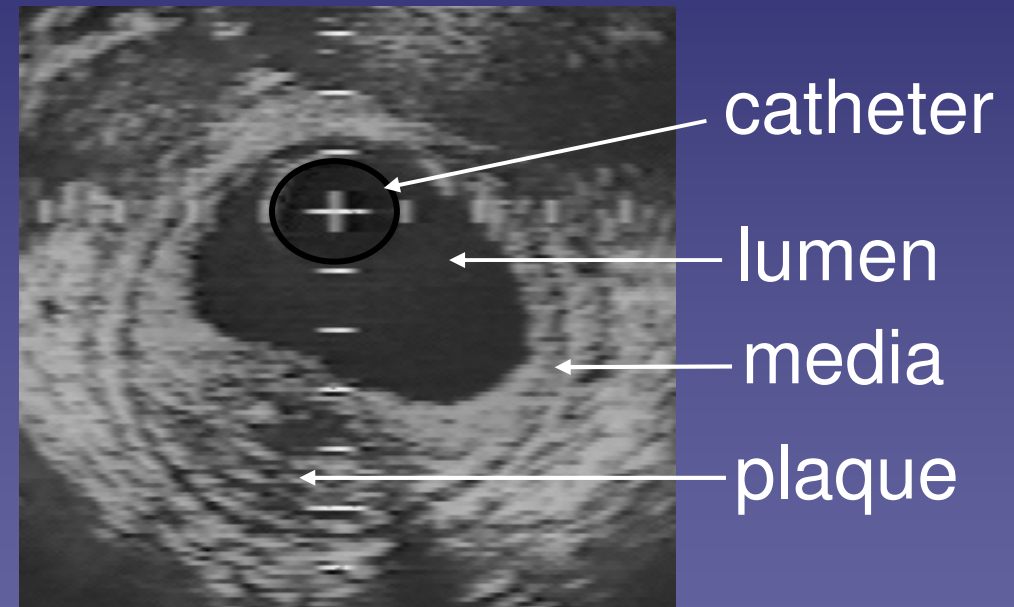


# Intravascular Ultrasound (IVUS) Imaging

ultrasound beam



IVUS image



# DISSECTION



# IVUS compare to classic probe

## Advantages of IVUS

↪ Frequency: **30 MHz**

↪ High frequency: **better resolution** and more attenuation

↪ Vessel size: some millimeters

↪ Wavelength:  $\lambda = c/f = 50 \mu\text{m}$

↪ Axial resolution :  $150 \mu\text{m}$  at 30 MHz

↪ Lateral resolution :  $250 \mu\text{m}$  at 30 MHz

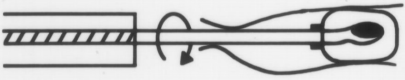

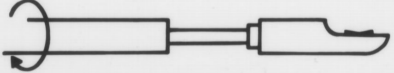



## Drawback

↪ **Invasive technique** (operating room)

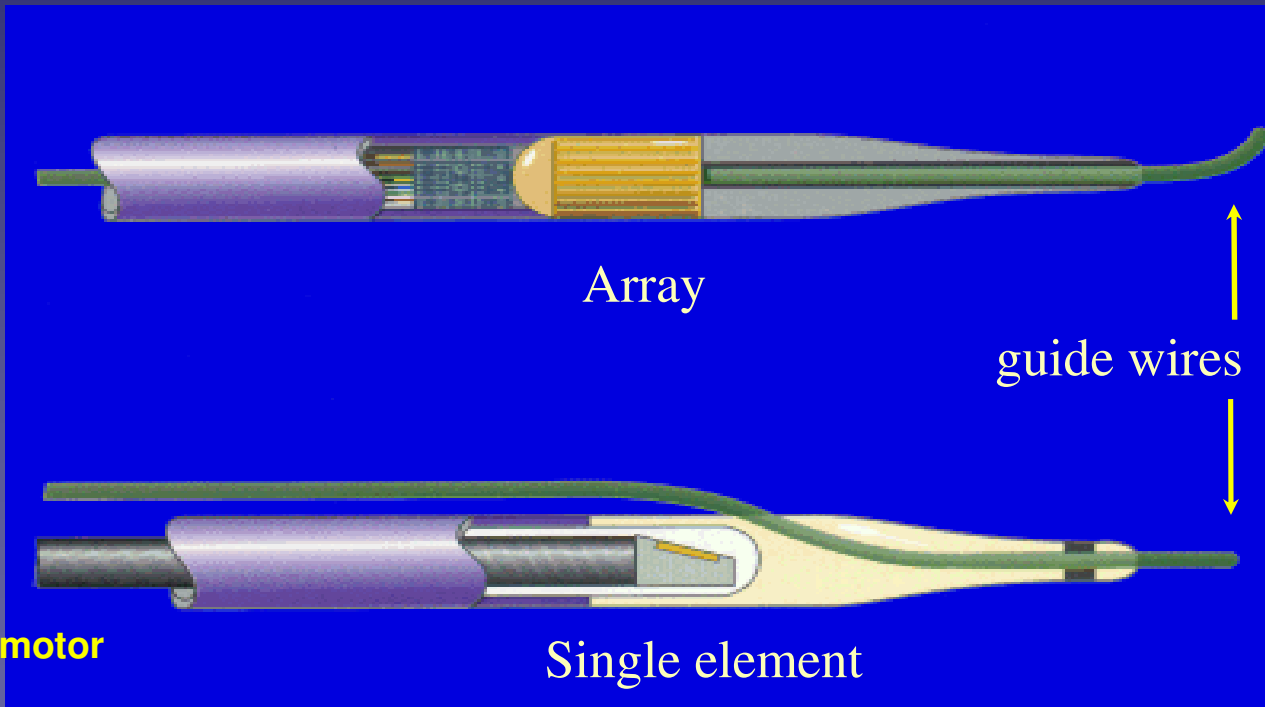
# Construction of an IVUS catheter

- Catheter based imaging technique

**INTRALUMINAL IMAGING**

Wild	1955	echo-endoscope		rectal tumour location
Omoto	1962	rotating probe C-scan		intracardiac tomography
Ebina	1964	transesophageal P.P.I. scanning		heart and vessels
Wells	1965	rotating mirror		intravenous
Eggleton .	1969	4-elements e.c.g. triggered		heart
Bom	1971	32-elements cylindrical phased array		intracardiac tomography

# Intravascular Ultrasound Catheters



rotating motor

Single element

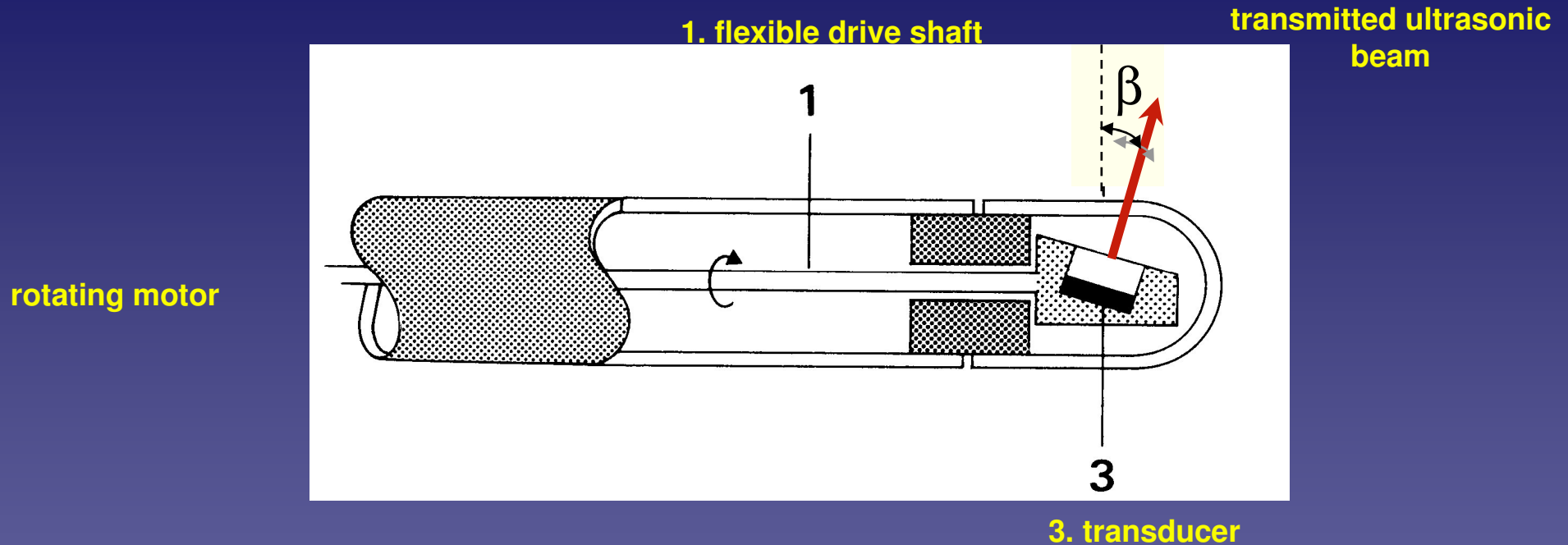
Electronic probe

guide wires

Mechanical probe



- Mechanical rotating single element catheter



↳ *Typical features*

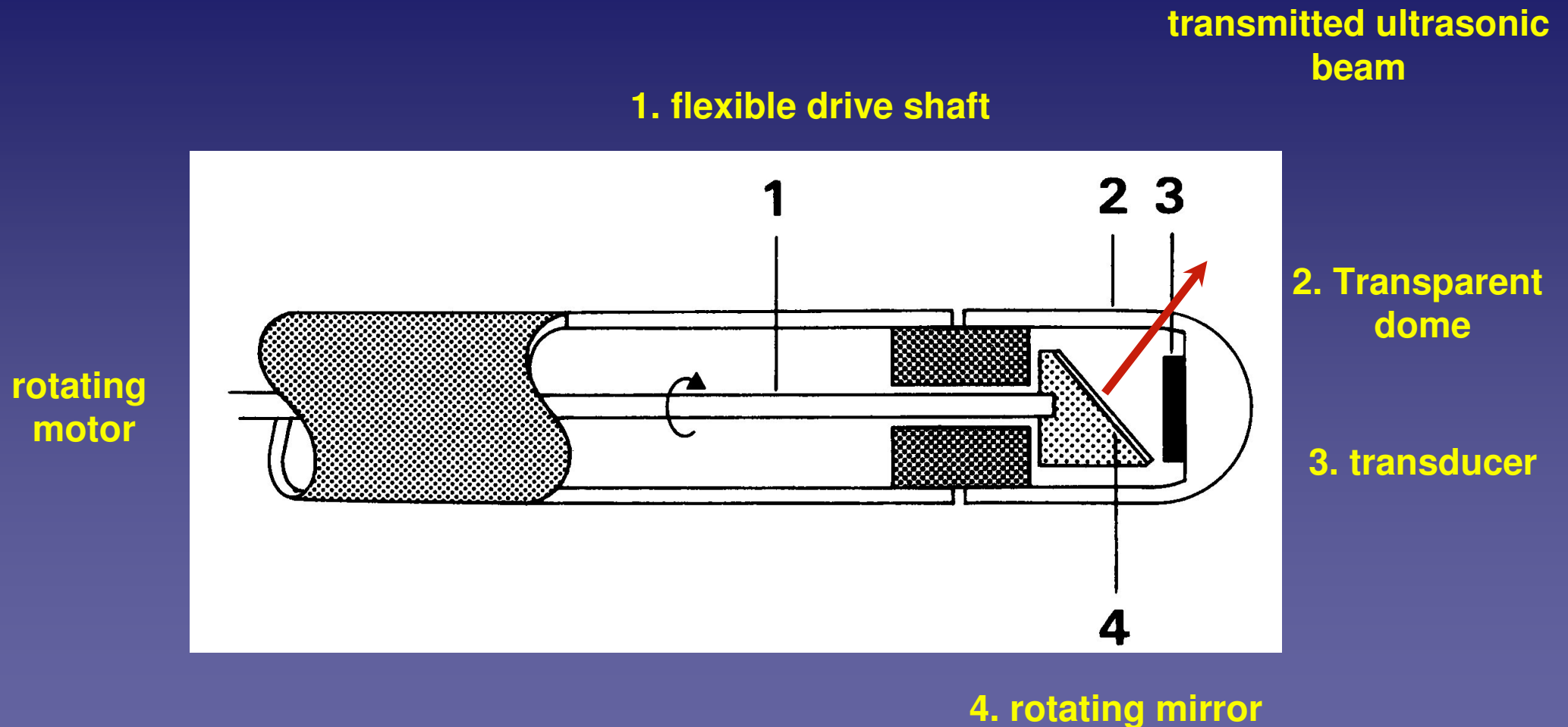
catheter diameter : 0.9 mm (~3 French)

aperture :  $14^\circ$

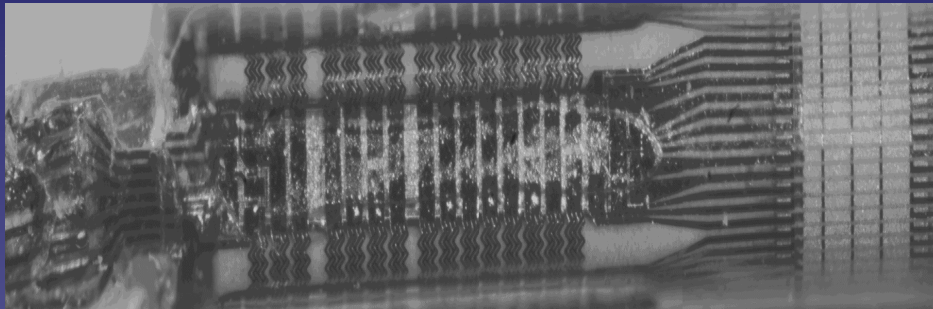
forward inclination angle :  $\beta = 10 - 15^\circ$

central frequency : 30 - 40 MHz

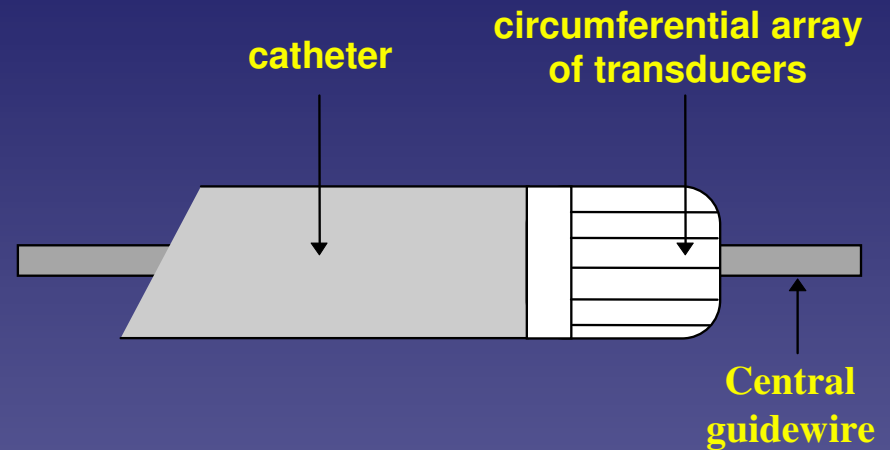
- Mechanical rotating mirror



- Electronically switched **phased circular array** catheter



*64-element probe, Endosonics*



↳ *Typical features*

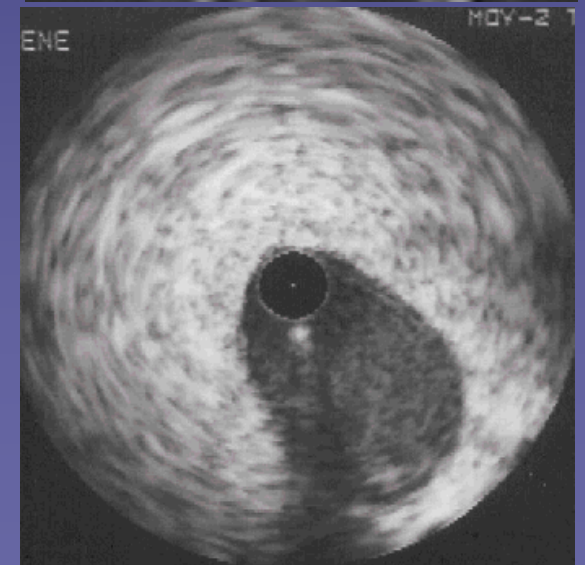
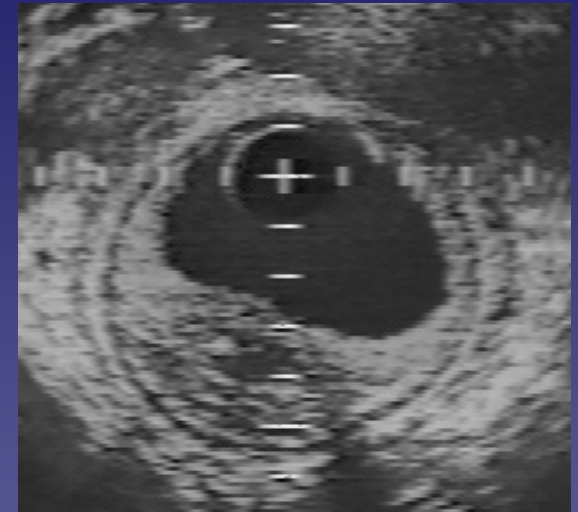
catheter diameter : 1.2 mm (~4F)

elements number : 16, 32, 64 or 128

Bom N, Lancée CT, Van Egmond FC (1972) An ultrasonic intracardiac scanner. Ultrasonics 10

# Geometric artefacts

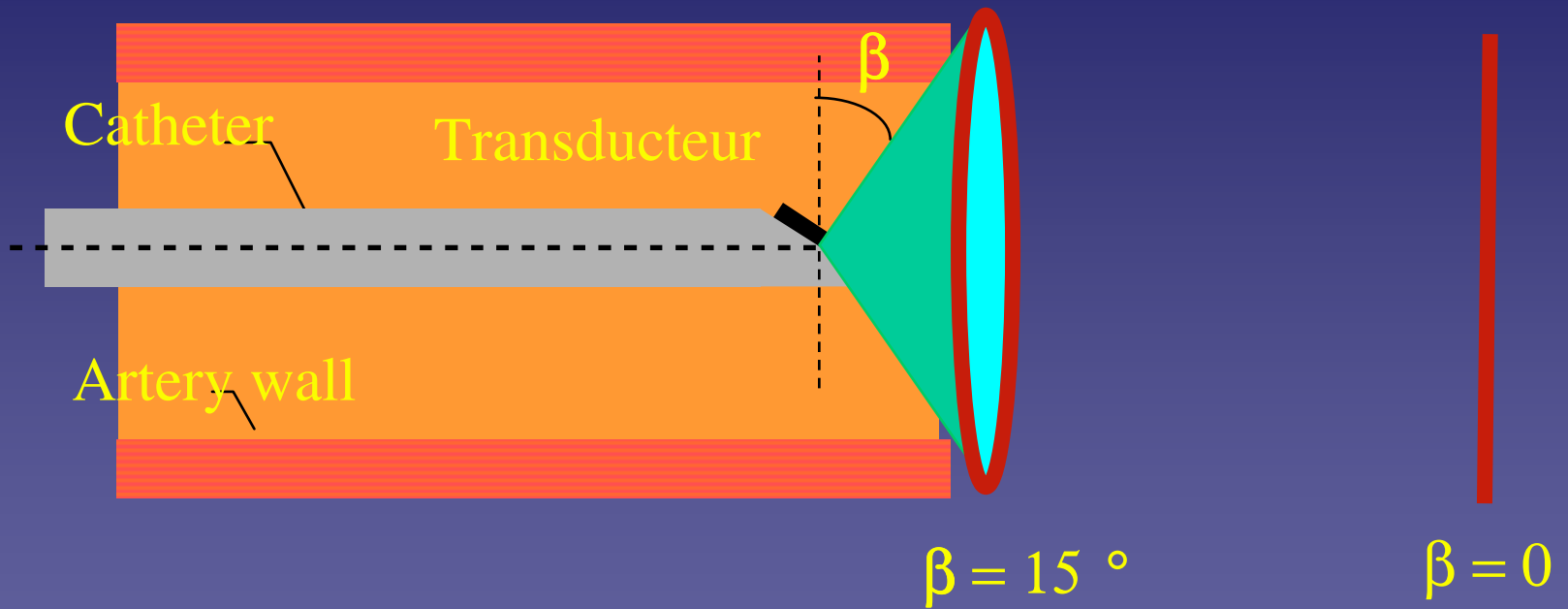
- Geometric distortion are caused by the position of the ultrasound catheter within the artery
- A circular artery is seen on IVUS images as a noncircular vessel represented by more or less complex shapes



- The main distortions are due:
  - to the inclination of the catheter (its long axis is not coaxial the vessel axis), angle  $\alpha$
  - to the off centered position of the catheter (the axis catheter is not located on the axis of the vessel),  $\delta x$  and  $\delta y$
- These artefacts are amplified by the geometry of the probe
  - the origin of the ultrasound beam is not the center of the catheter:  $\rho$
  - the ultrasound beam looks forward (not perpendicular to the long axis of the catheter), angle  $\beta$

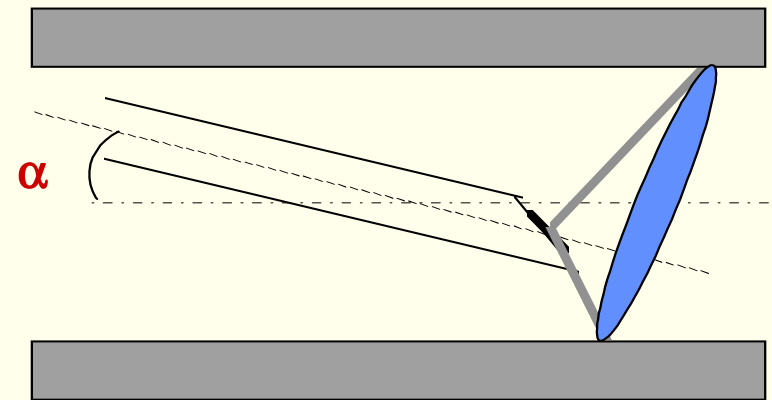
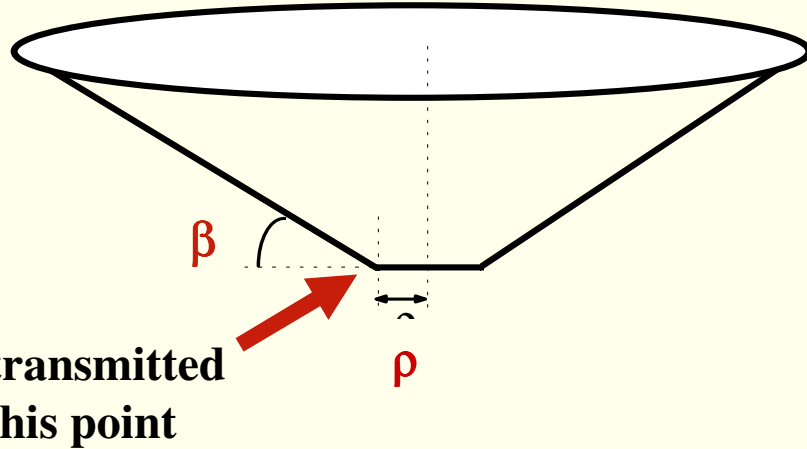
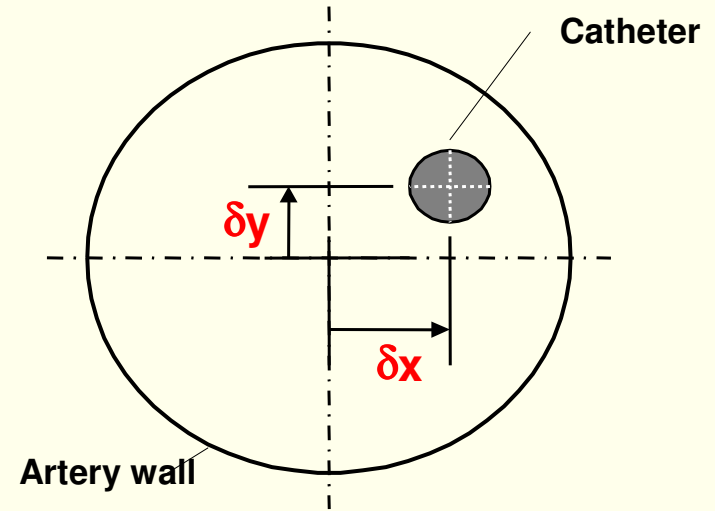
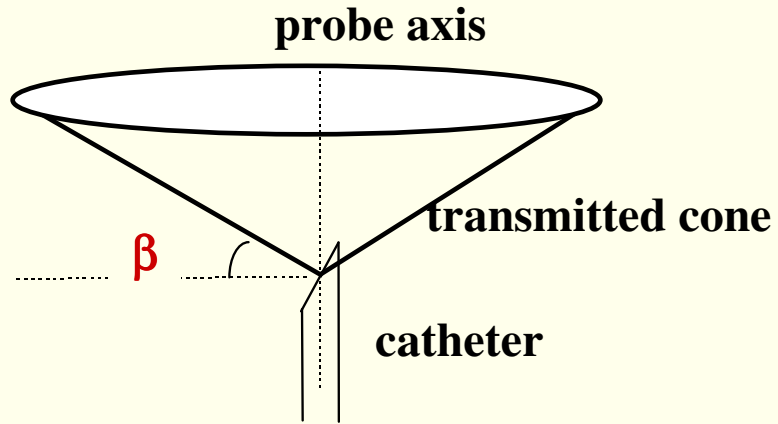
# Forward inclination angle $\beta$

Transmitting cone swept by the ultrasound beam

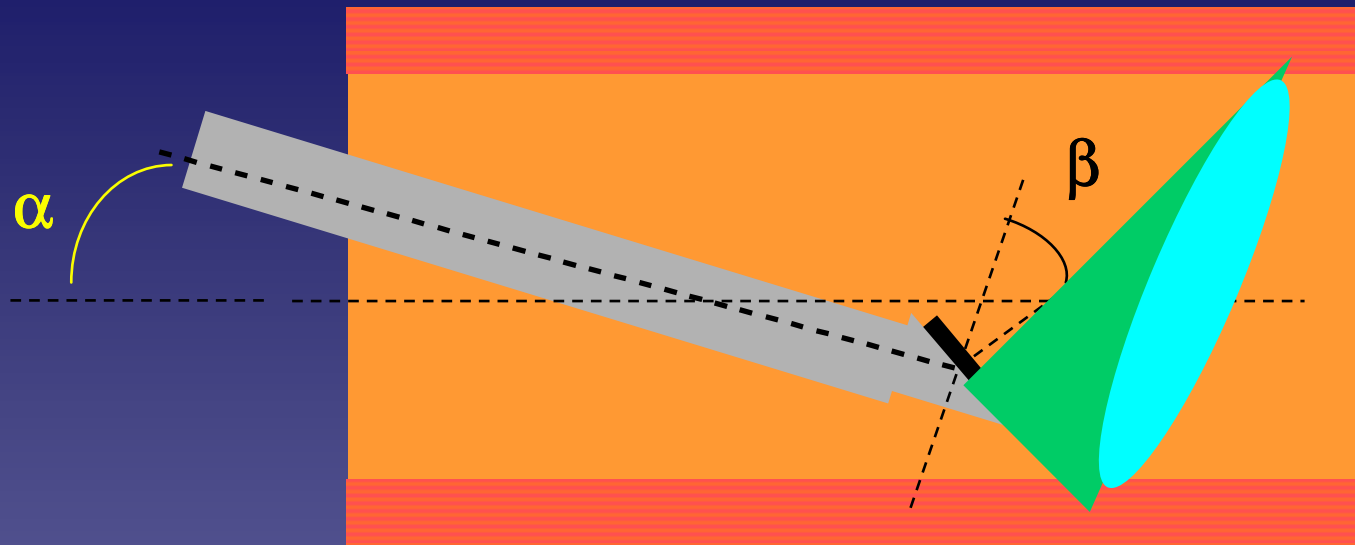


- The forward inclination of the piezoelectric element avoids direct reflection on the vessel wall and the multiple reflection. The scattering is reinforced

### Four origins for geometric artefacts







combination:

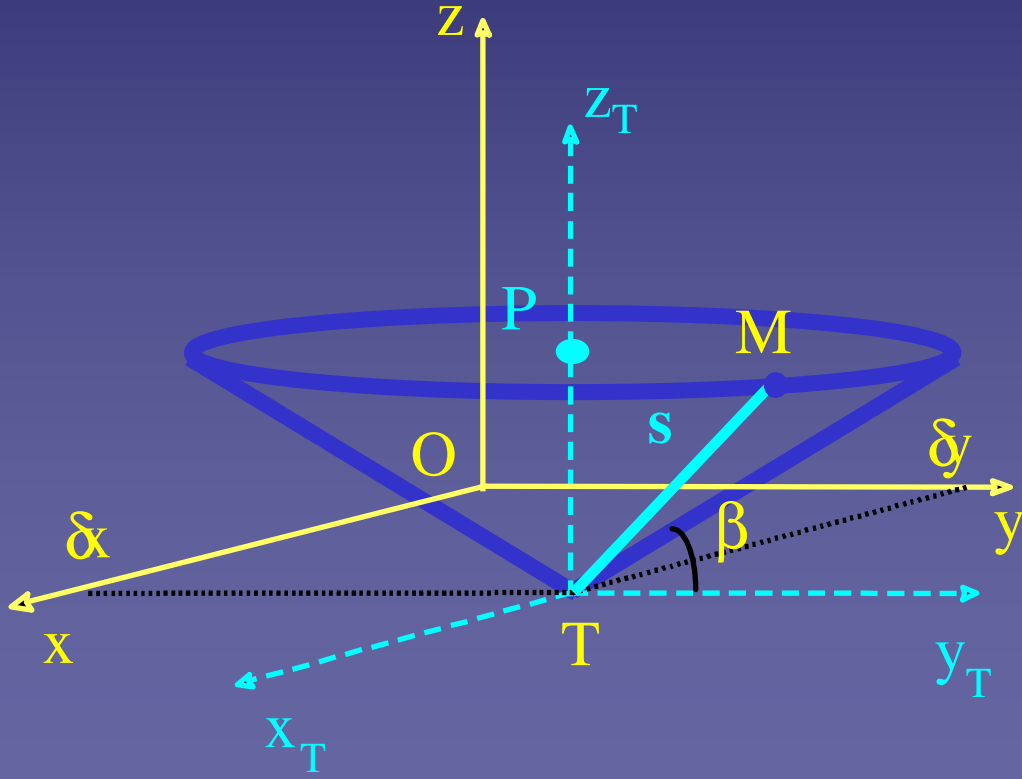
forward inclination angle  $\beta$   
inclination of the probe axis  $\alpha$ ,  
off centered position  $\delta x$  et  $\delta y$

# Modelisation of the geometry

Reference coordinate system:  $R ( O, x, y, z )$

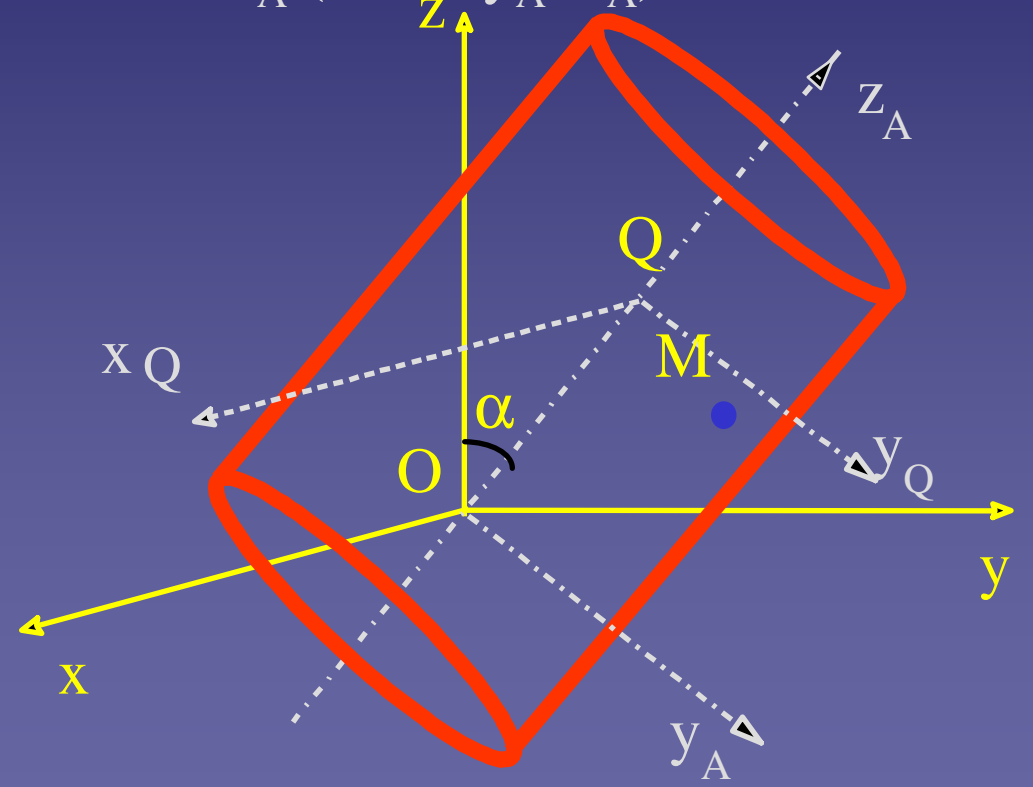
Probe coordinate système:

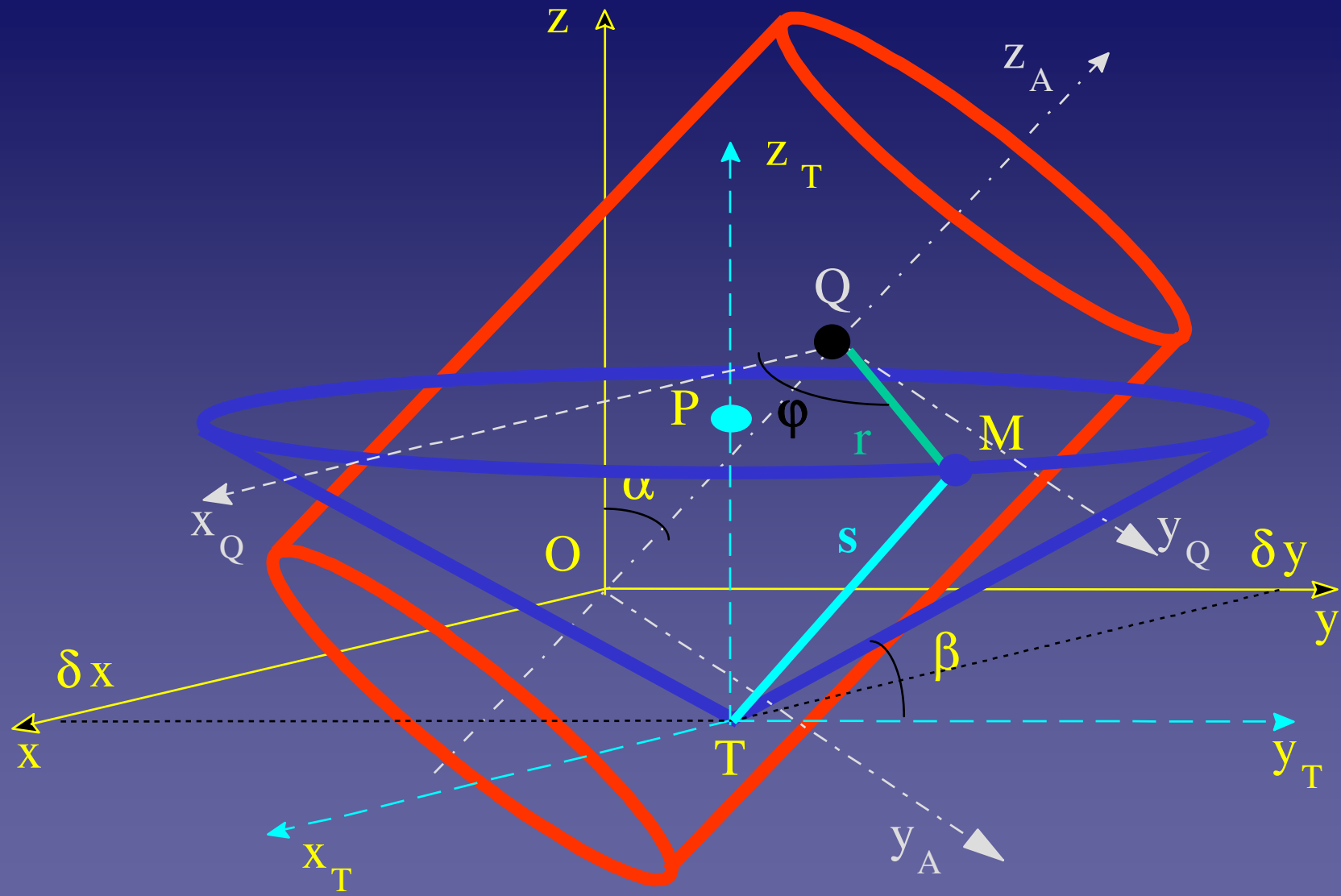
$$R_T ( T, x_T, y_T, z_T )$$



Artery coordinate systeme:

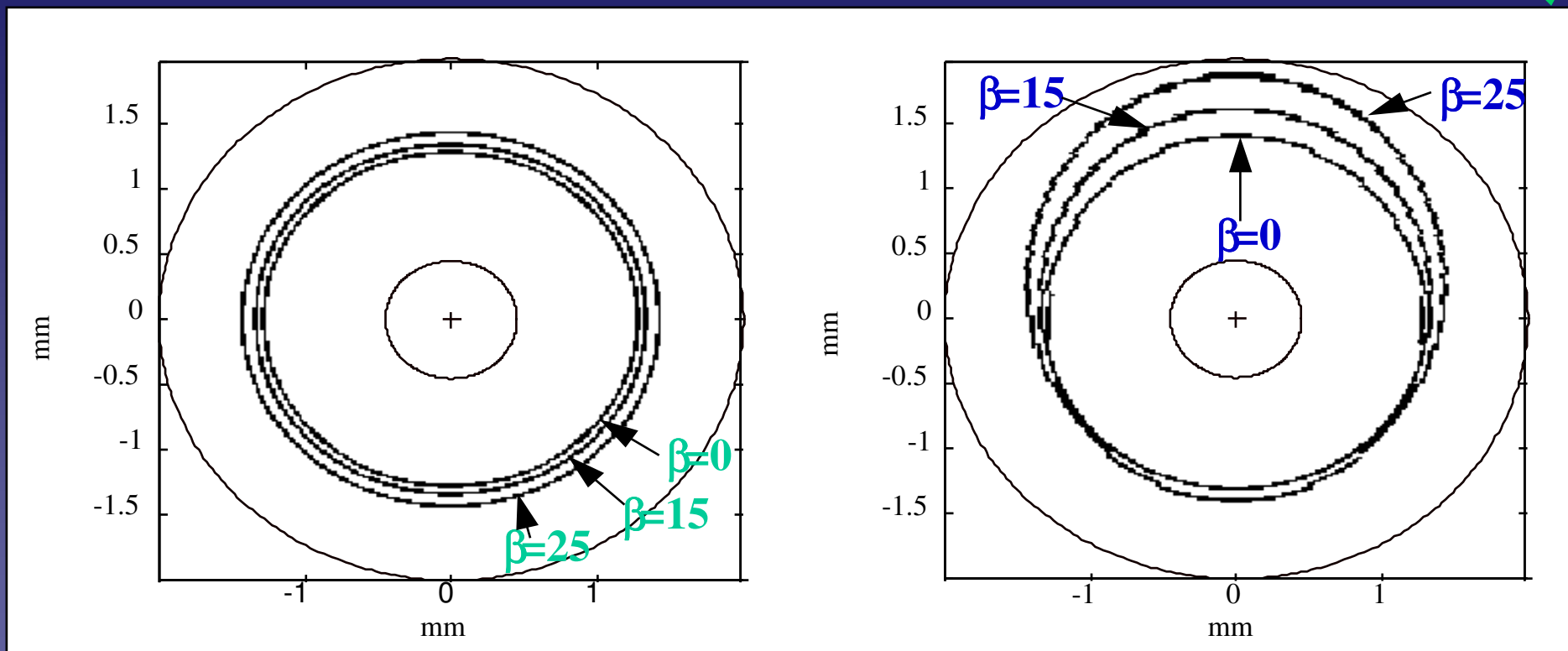
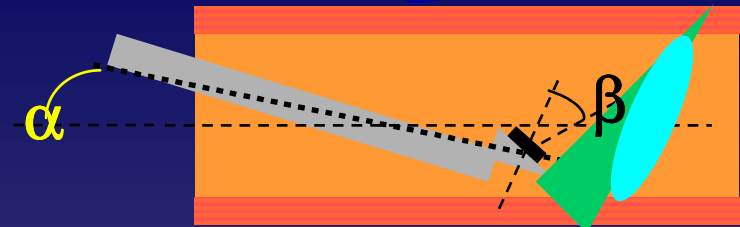
$$R_A ( O, x, y, z )$$





Delachartre P., Cachard C. and al., *Ultrasound in Medicine and Biology*, 1999, vol. 25

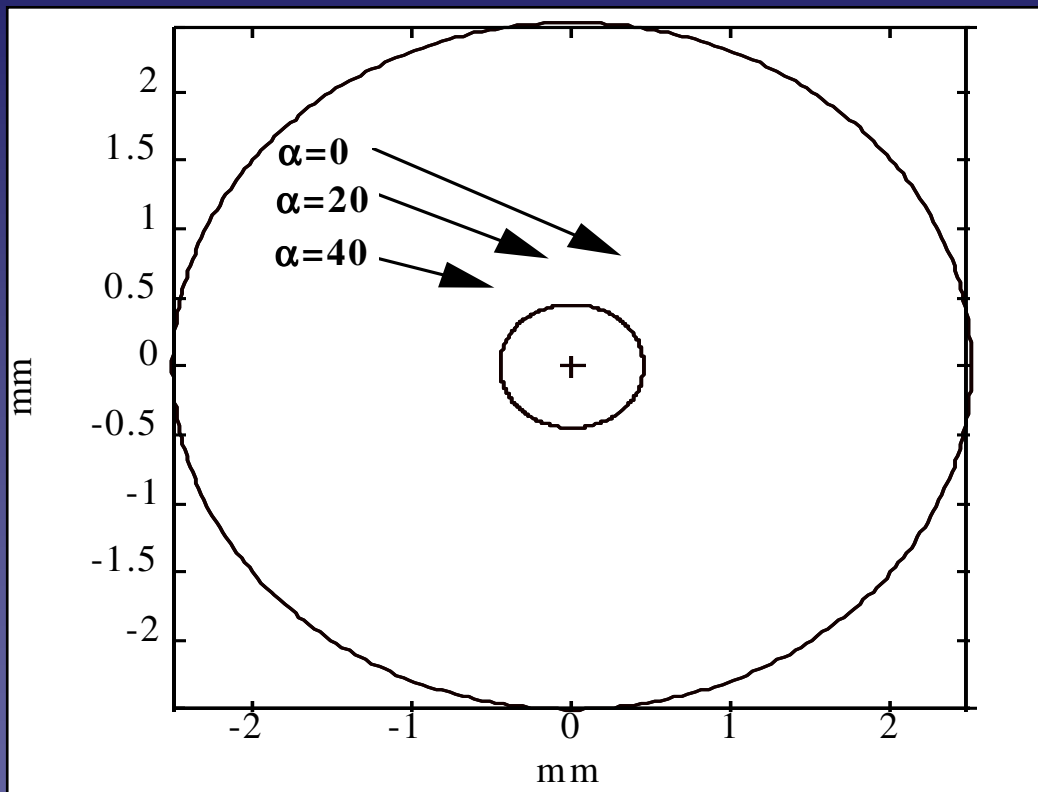
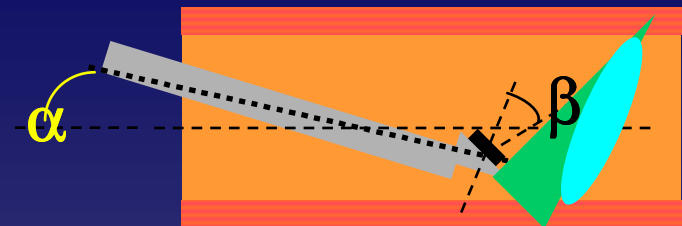
# ■ forward inclination angle $\beta$



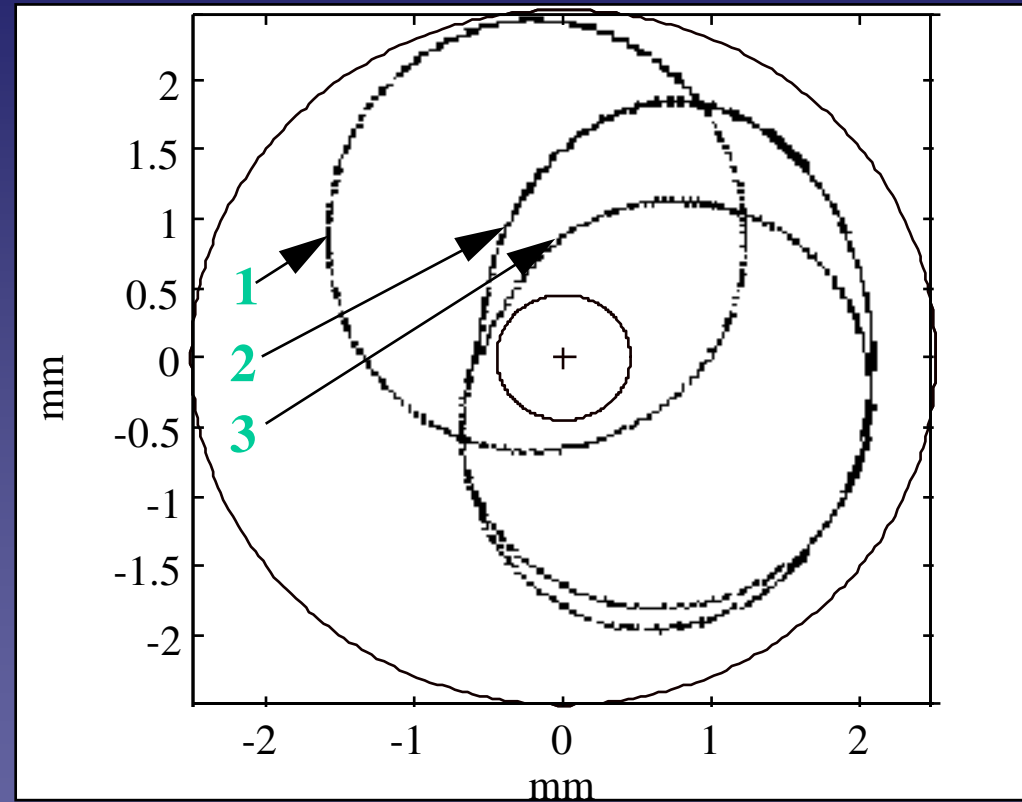
inclination  $\alpha = 0$   
off centered position  $\delta x = 0$  mm,  $\delta y = 0$  mm  
off axis of transmission point  $\rho = 0.4$  mm

inclination  $\alpha = 20^\circ$

■ Inclination of the catheter axis:  $\alpha$



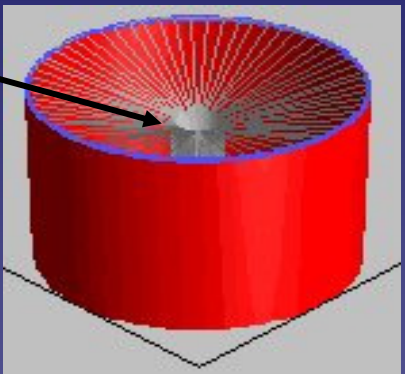
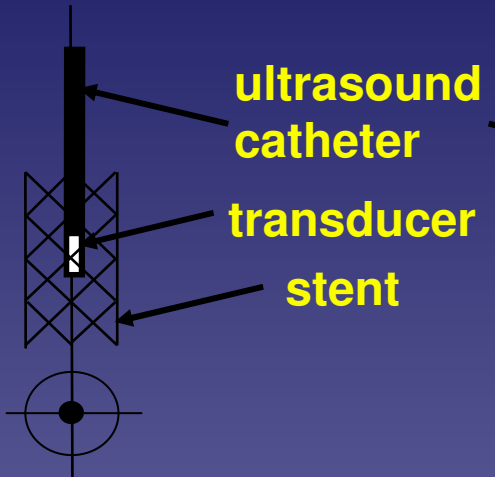
$\delta x = -0.7 \text{ mm}$ ,  $\delta y = 0.5 \text{ mm}$   
 $\beta = 15^\circ$   
 $\rho = 0.4 \text{ mm}$



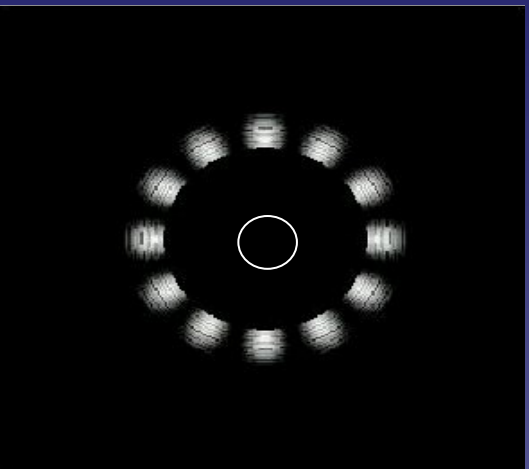
1 :  $\alpha = 20^\circ$ ,  $\delta x = 0.2$  et  $\delta y = -0.7$ ;  
 2 :  $\alpha = 40^\circ$ ,  $\delta x = -0.7$  et  $\delta y = 0.5$ ;  
 3 :  $\alpha = 20^\circ$ ,  $\delta x = -0.7$  et  $\delta y = 0.5$   
 ( $\beta = 15^\circ$  et  $\rho = 0.4 \text{ mm}$ ).



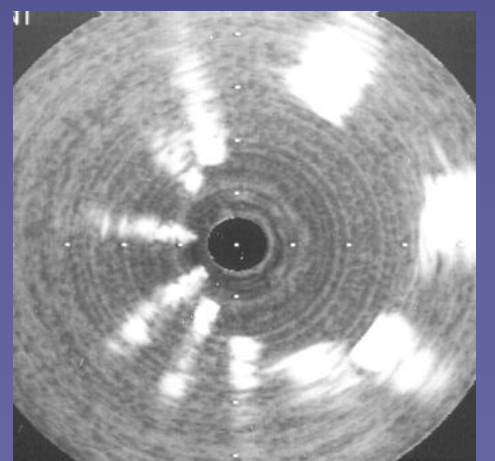
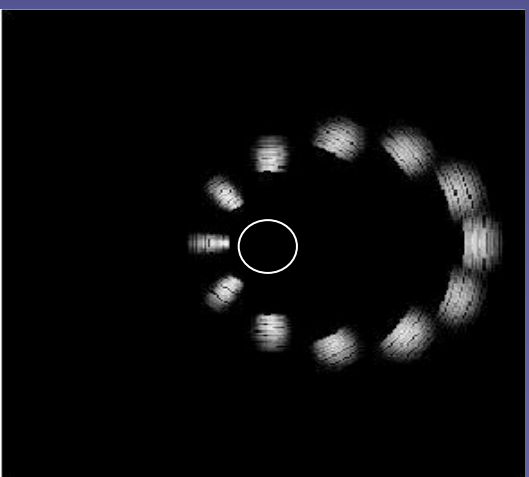
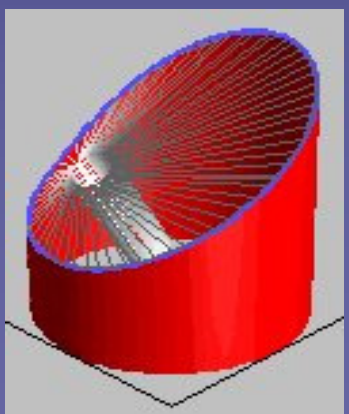
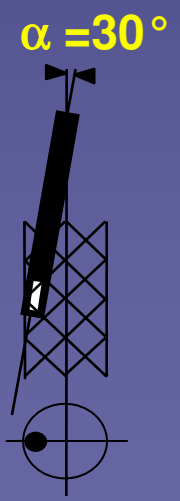
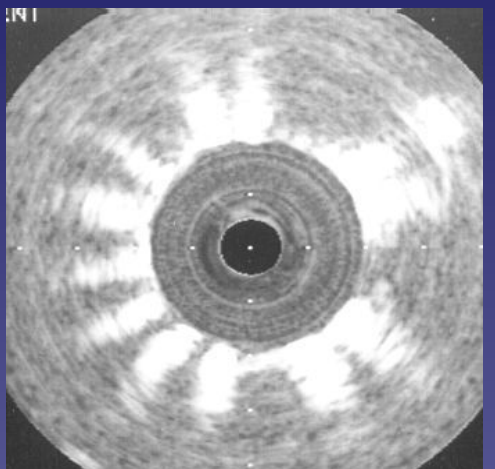
# Geometric artifacts



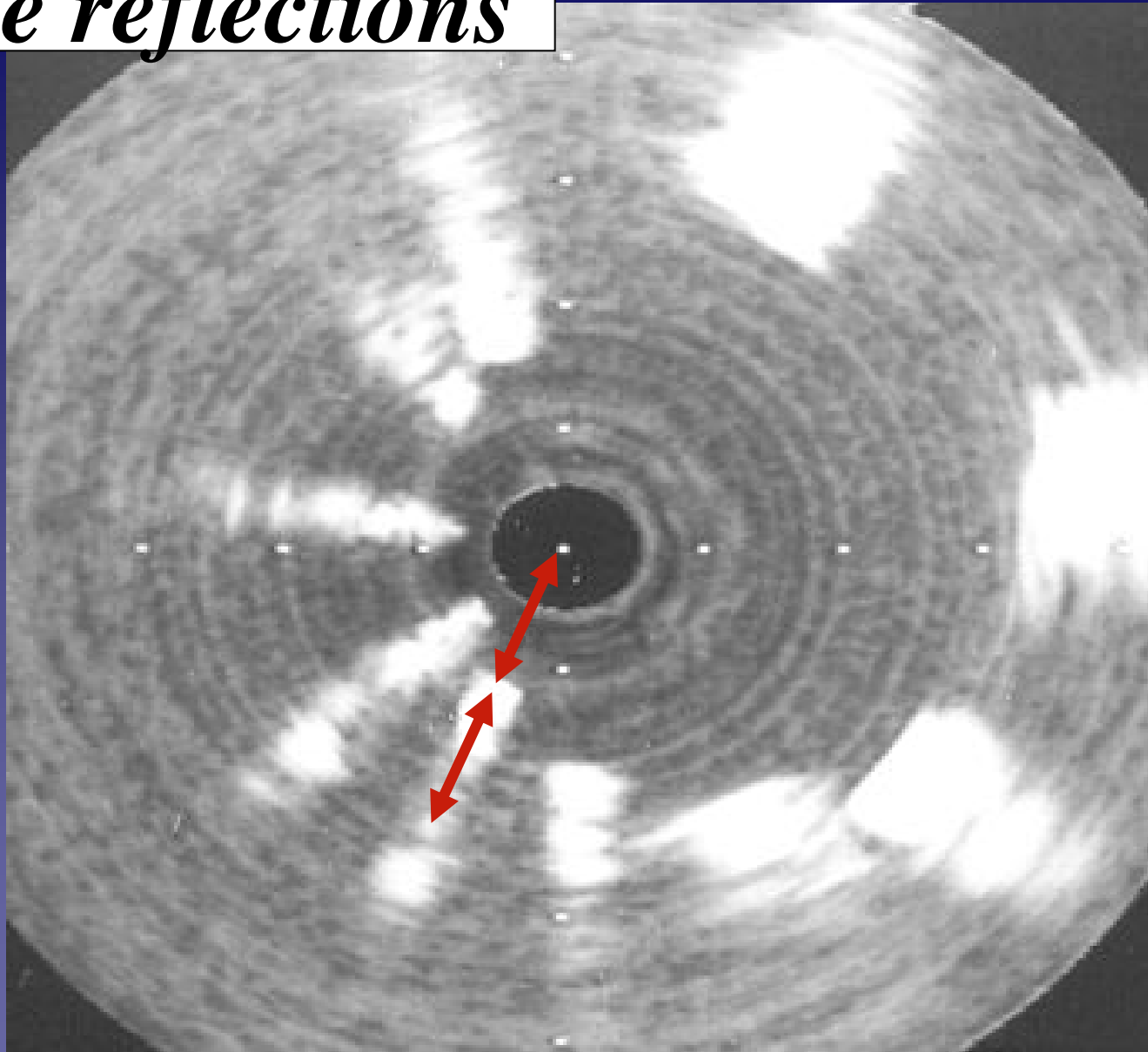
*simulation*



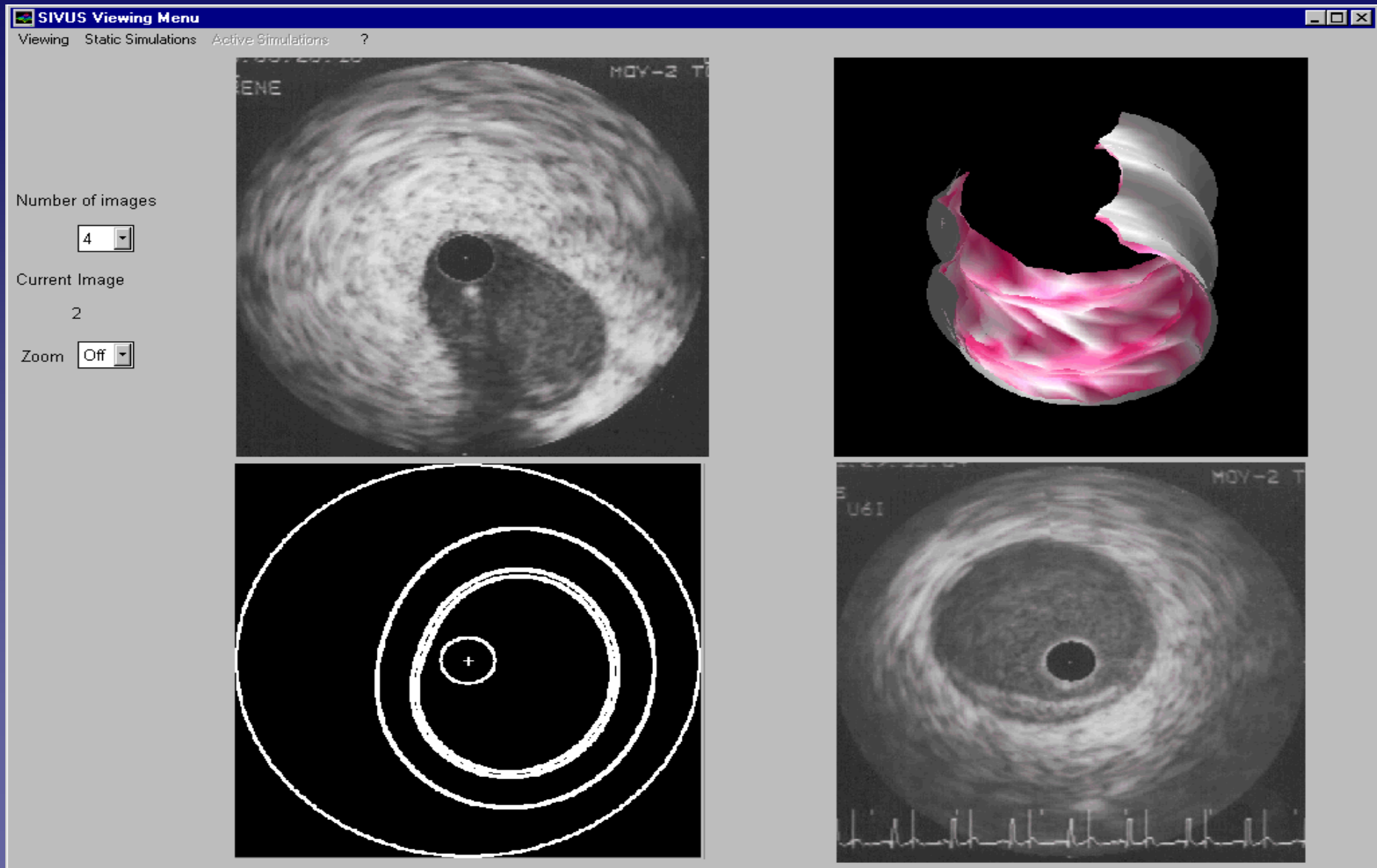
*experiment*



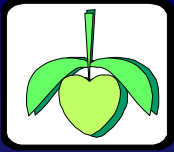
# *Multiple reflections*





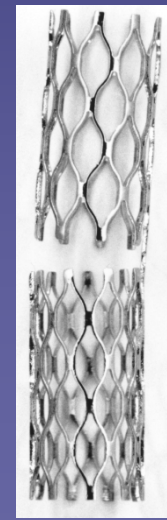
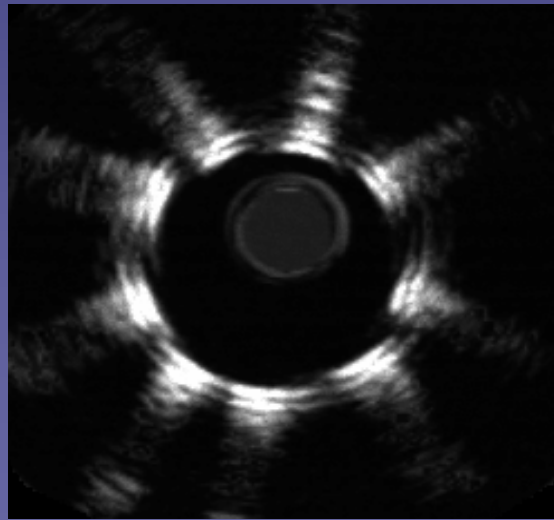
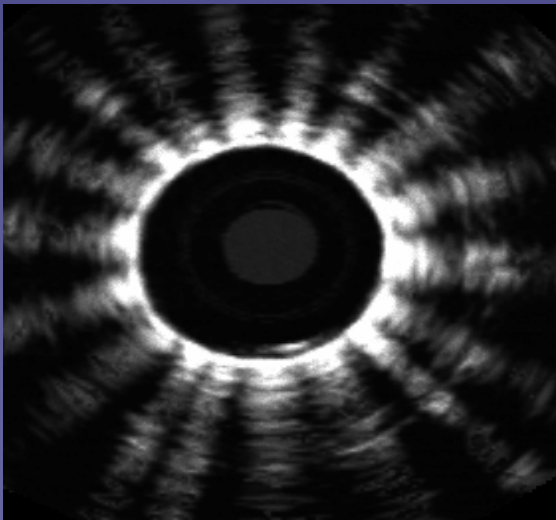
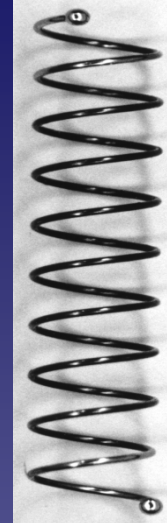
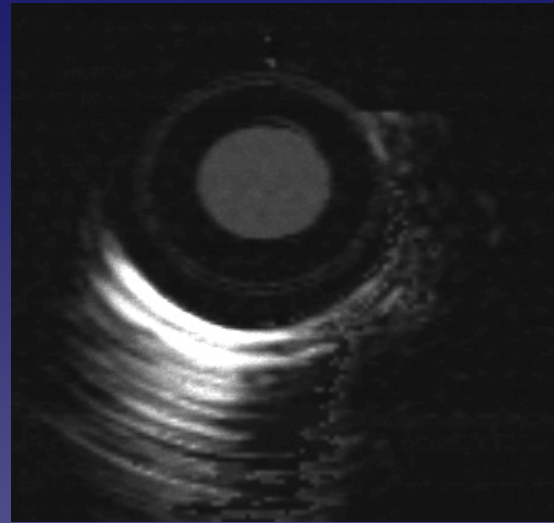
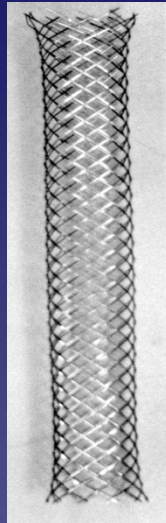
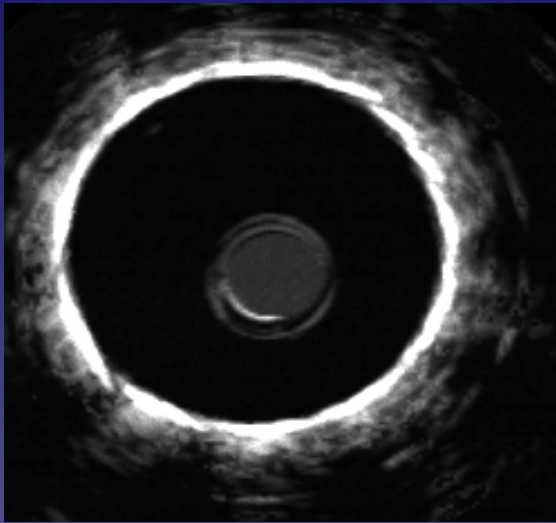


# IVUS in the clinic



Thoraxcentre  
Rotterdam

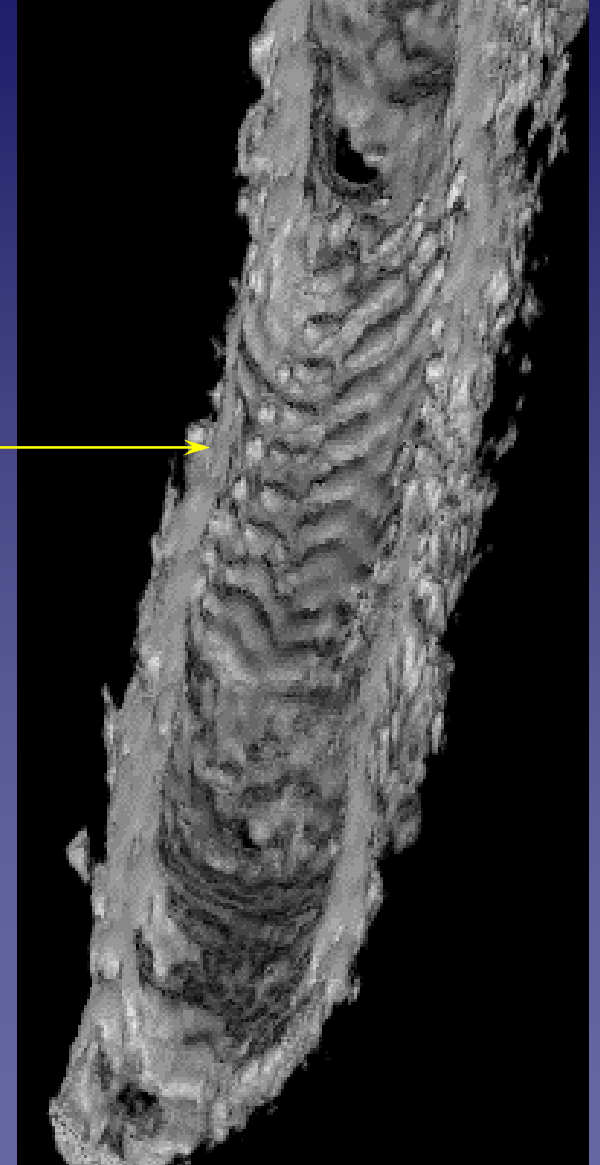
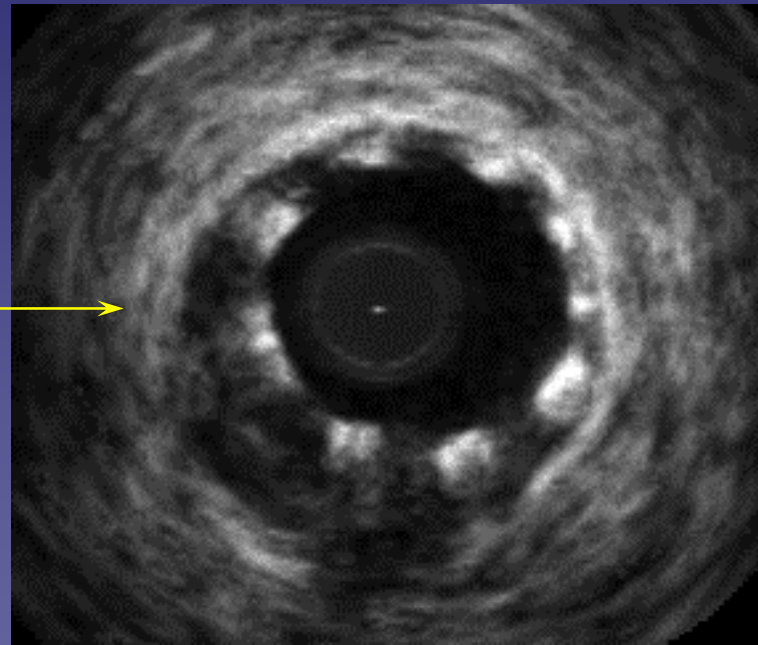
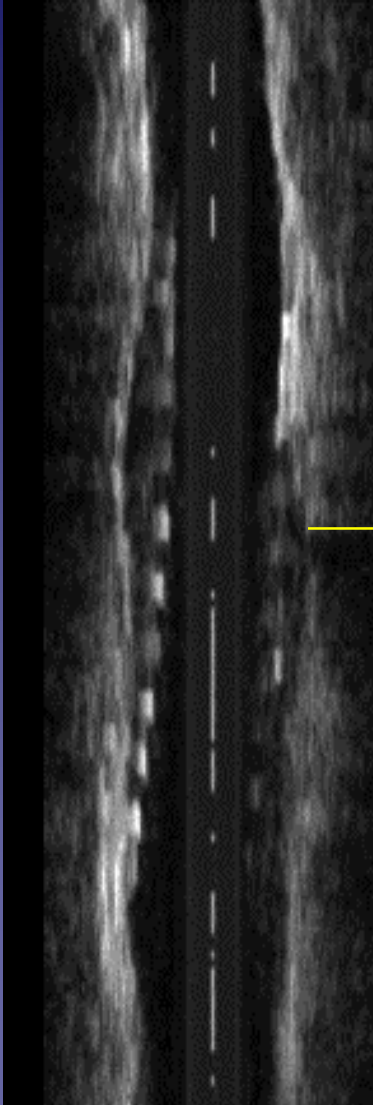
# ICUS appearances of Coronary Stents





Thoraxcentre  
Rotterdam

# Wallstent / Acute result II

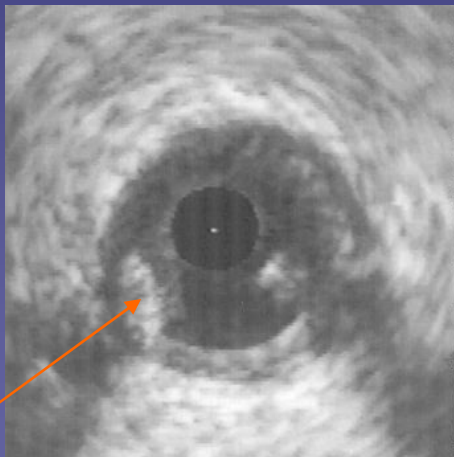


N. Bruining  
Wallstent/acute II

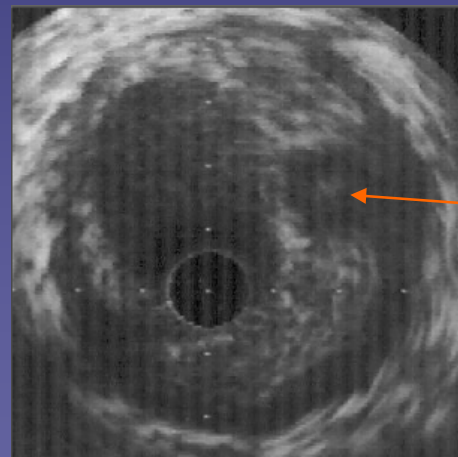
European School of Medical Physics - Archamps

# Plaque

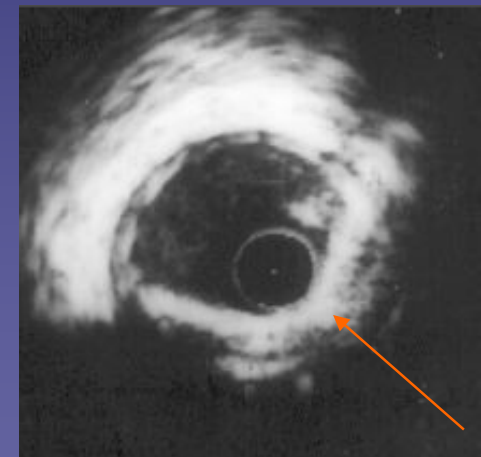
**Calcified component**  
*Hyper-reflectivity*  
*following by shadowing*



**Cell component**  
(blood, lipidic, inflammatory cells)  
*~ no reflectivity*



**Fibrous component**  
*hypo or hyper reflectivity* (collagen density)

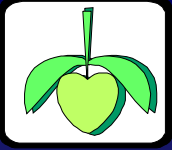


**Hyaline fibrosis**



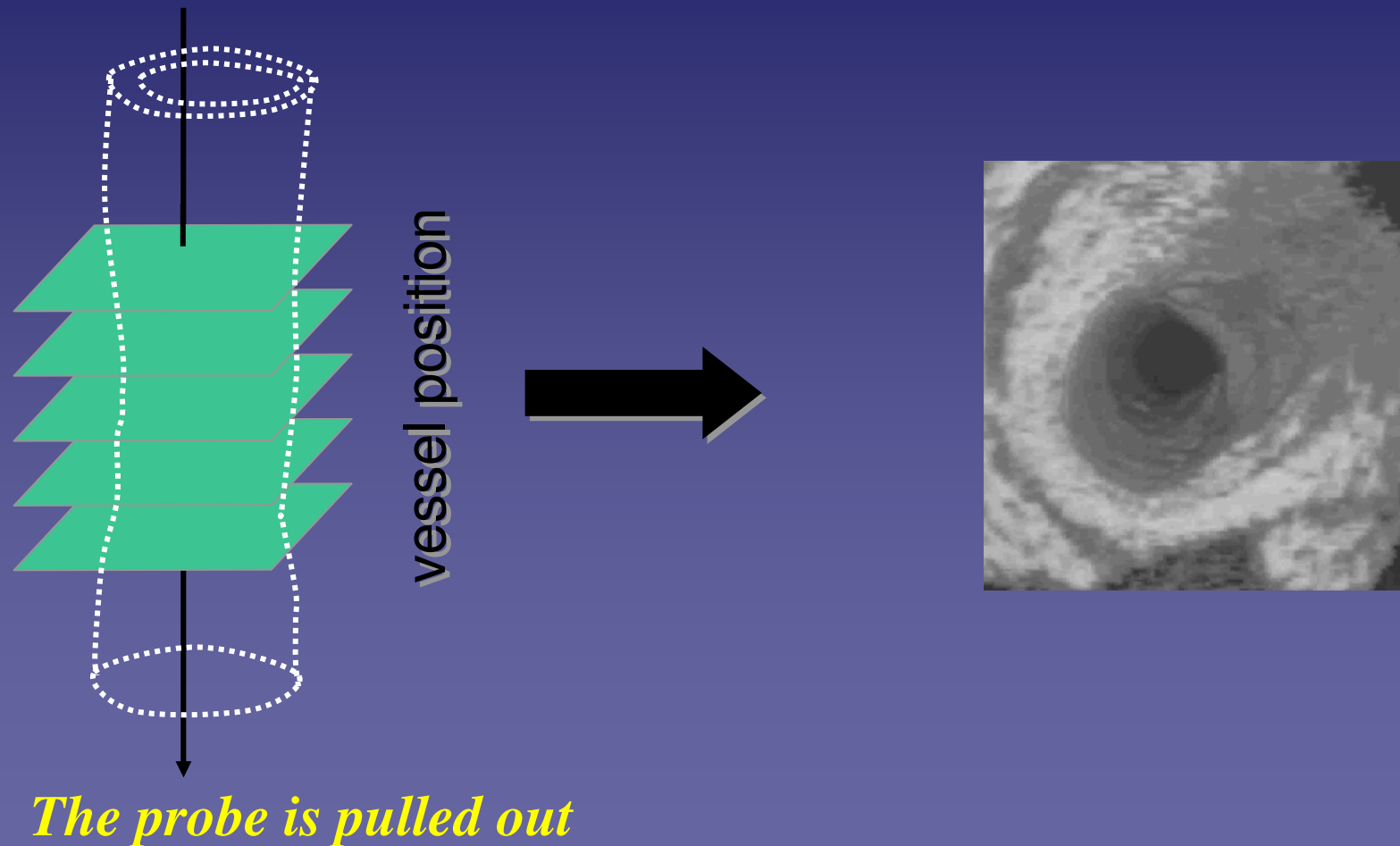
*Possible misinterpretations*

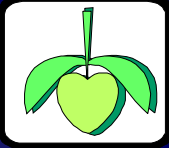
# Quantifying plaque volume



Thoraxcentre  
Rotterdam

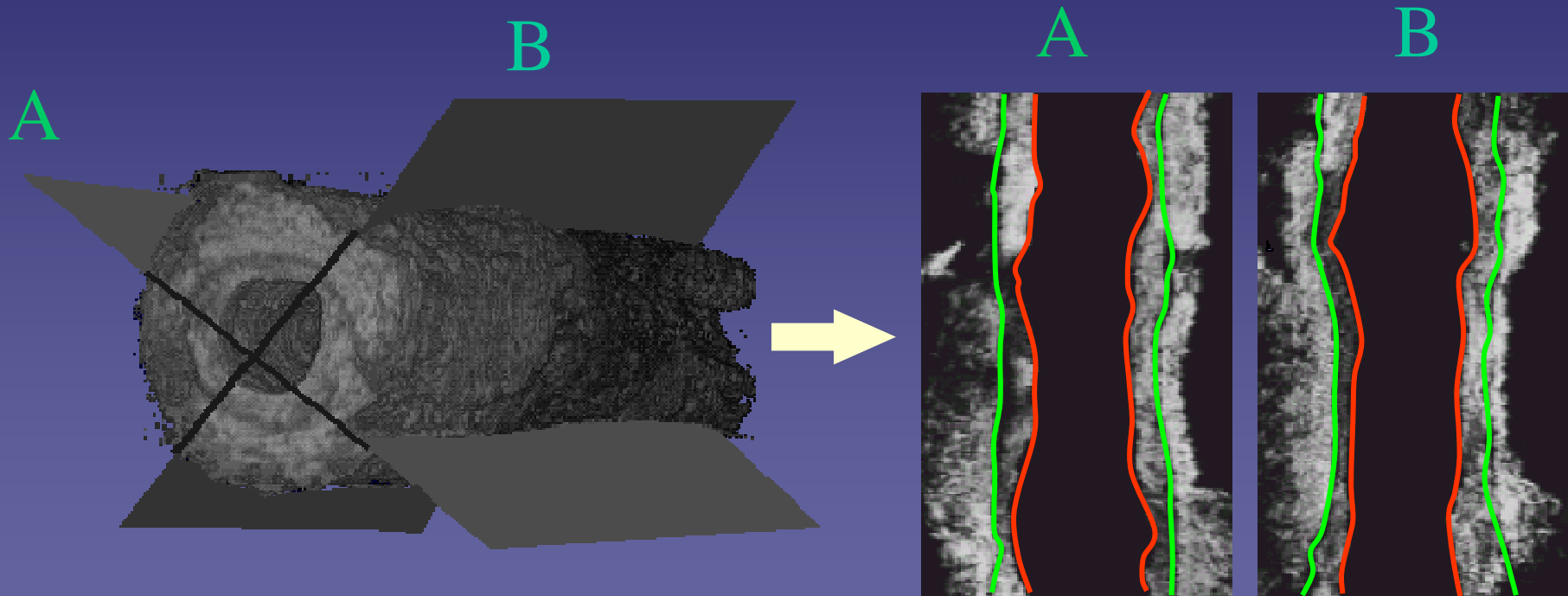
# Three-Dimensional Data Acquisition



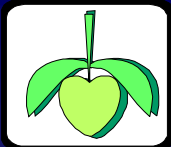


Thoraxcentre  
Rotterdam

# Longitudinal Contour Detection

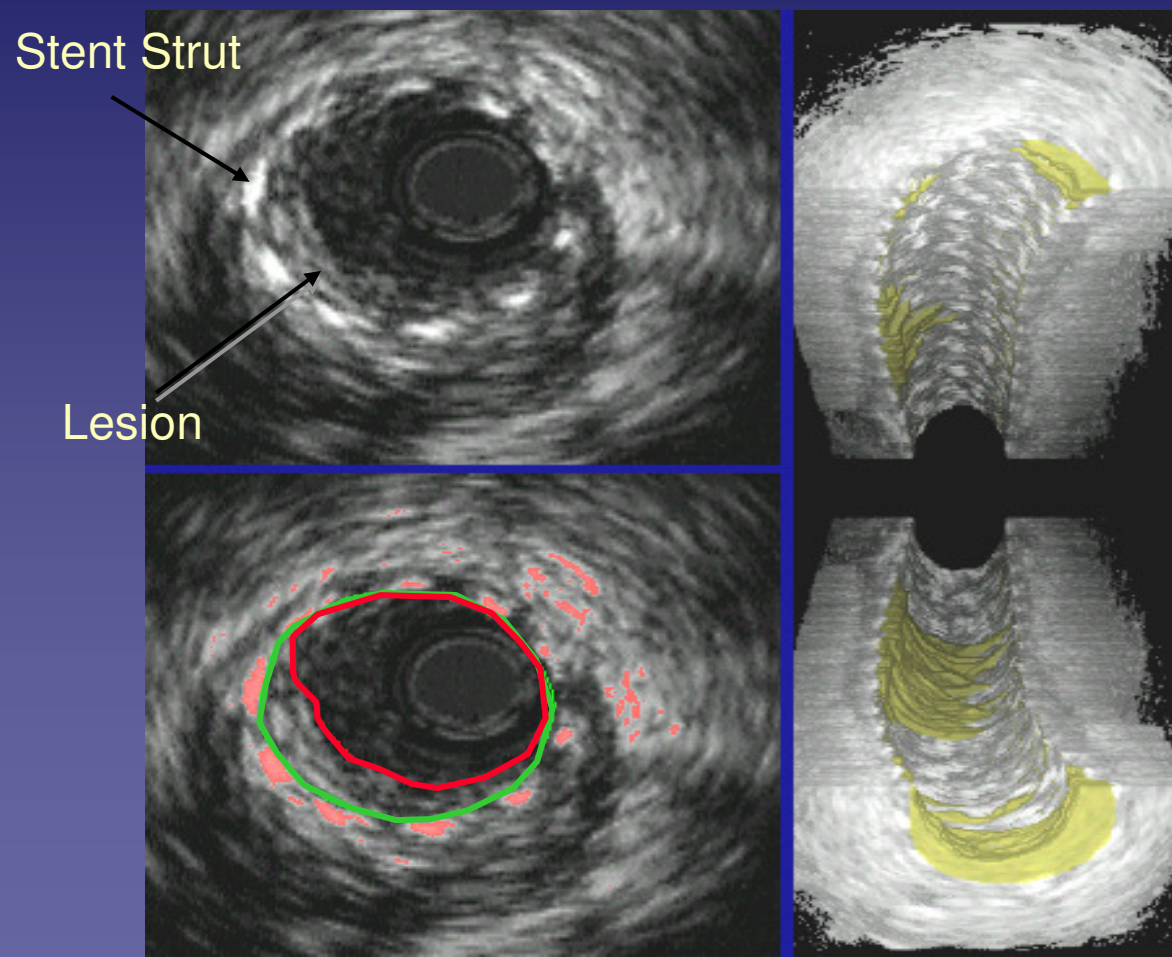




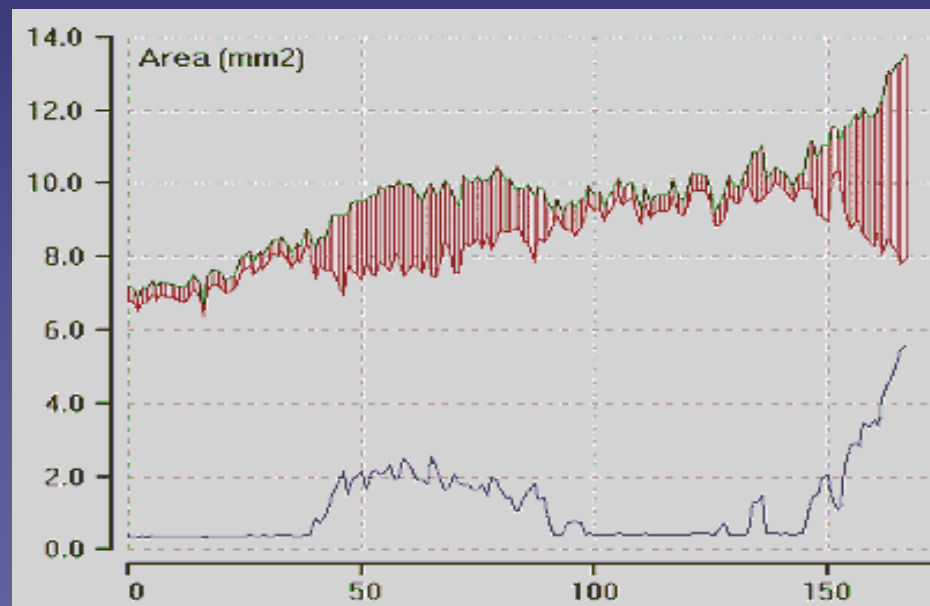


Thoraxcentre  
Rotterdam

# In-stent Restenosis Assessed with 3D IVUS



Lumen, Stent and Lesion Areas



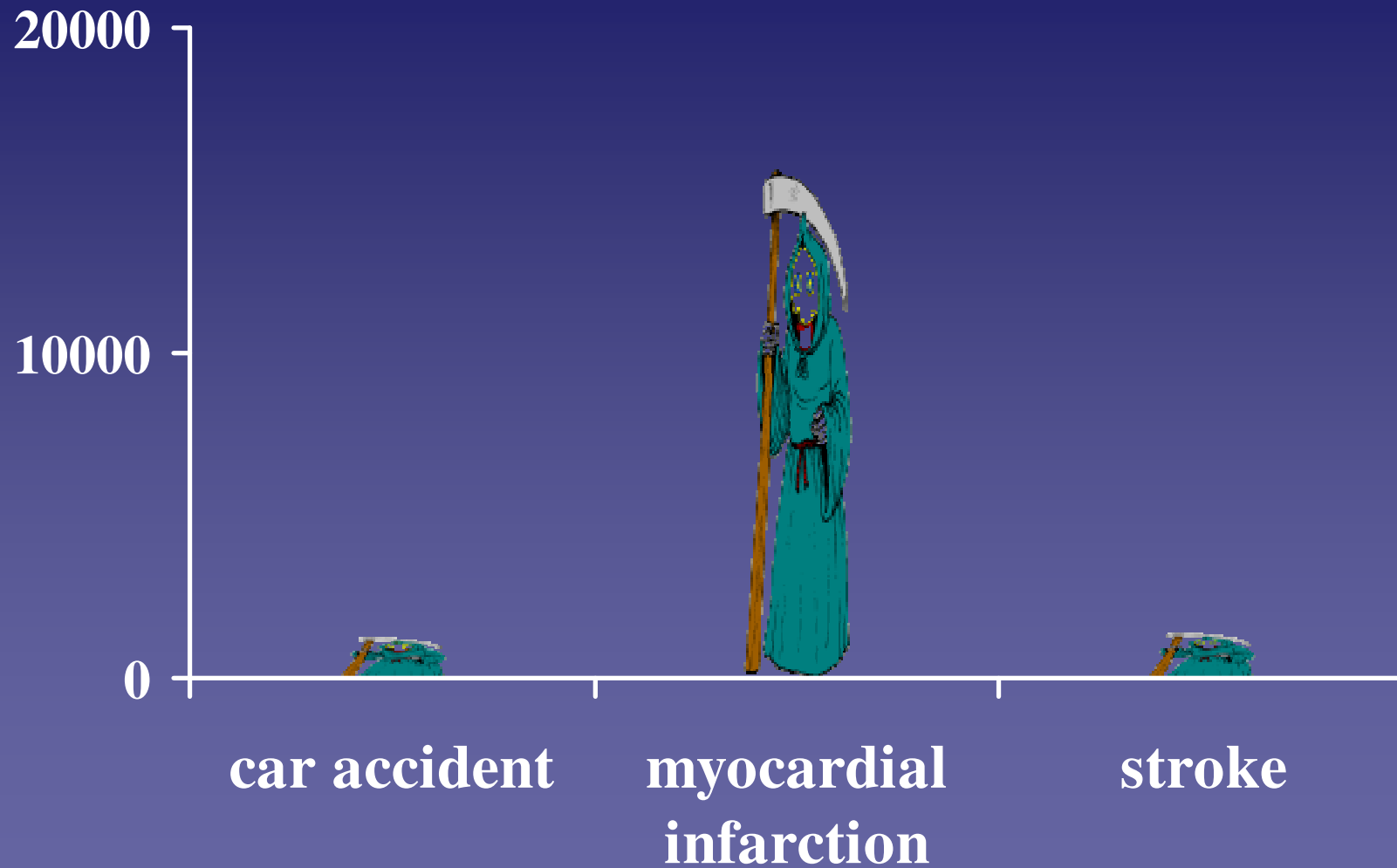
*Lesion Volume: 24.85 mm<sup>3</sup>*

Li et al. 1994-1997

DuMed

# Vulnerabele Plaque Characterization

# Mortality per annum The Netherlands

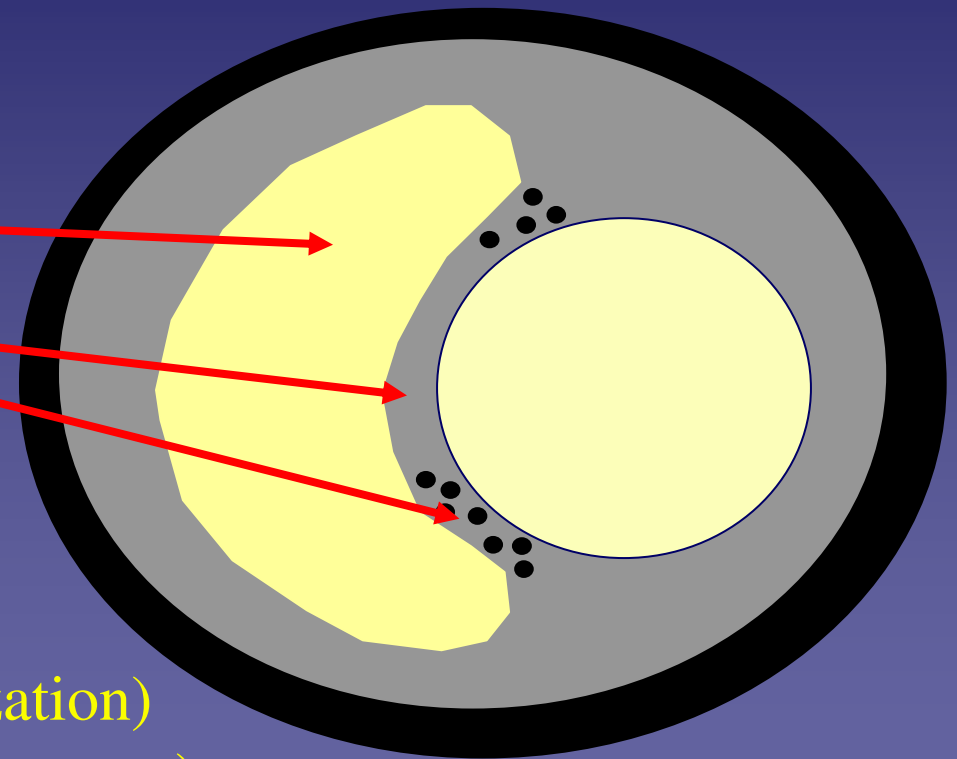


<http://cvdinfobase.ic.gc.ca/gcvi/default.htm>  
[www.cbs.nl](http://www.cbs.nl)

# Vulnerable Plaque

## Plaque composition

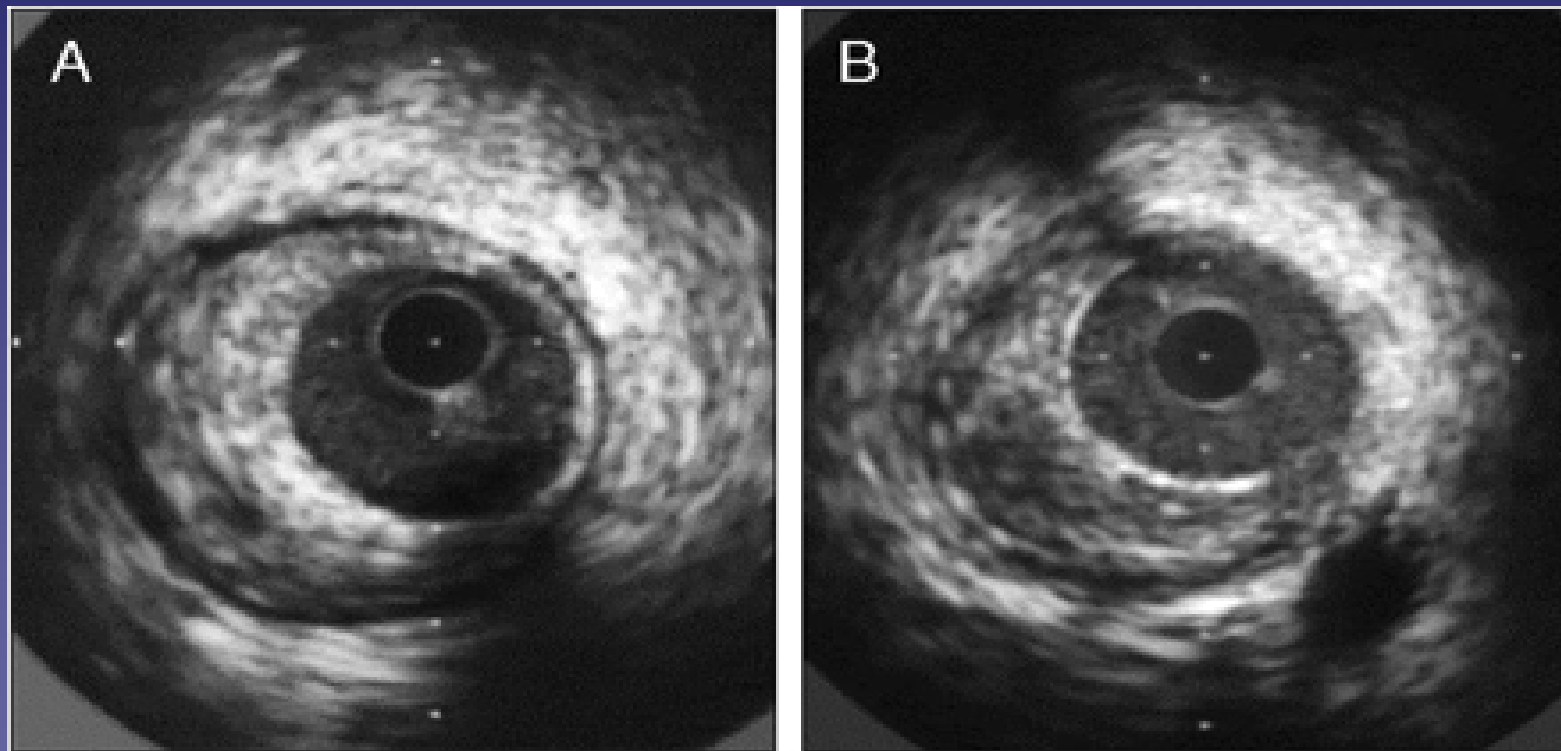
- Large lipid pool
- Thin fibrous cap
- presence of Macrophages



## The challenge:

- % of the lipid core (tissue characterization)
- metabolism, inflammation (pH, temperature)
- thickness of the cap (range = 0 – 200  $\mu\text{m}$ )
- stability of the cap (strain)

# Vulnerable plaque with IVUS



Boston  
Scientific

Nissen & Yock Circ 2001;103:604-616

# IVUS diagnostic modality under investigation

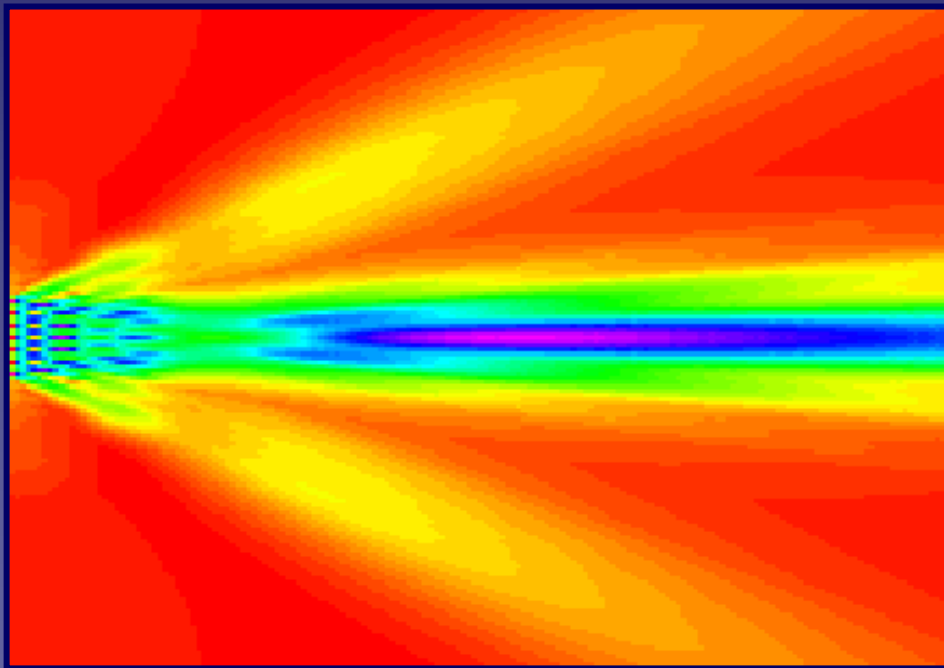
- Elastography and Palpography
- Harmonics
- Thermography
- Modulography
- Contrast agents

# IVUS diagnostic modality under investigation

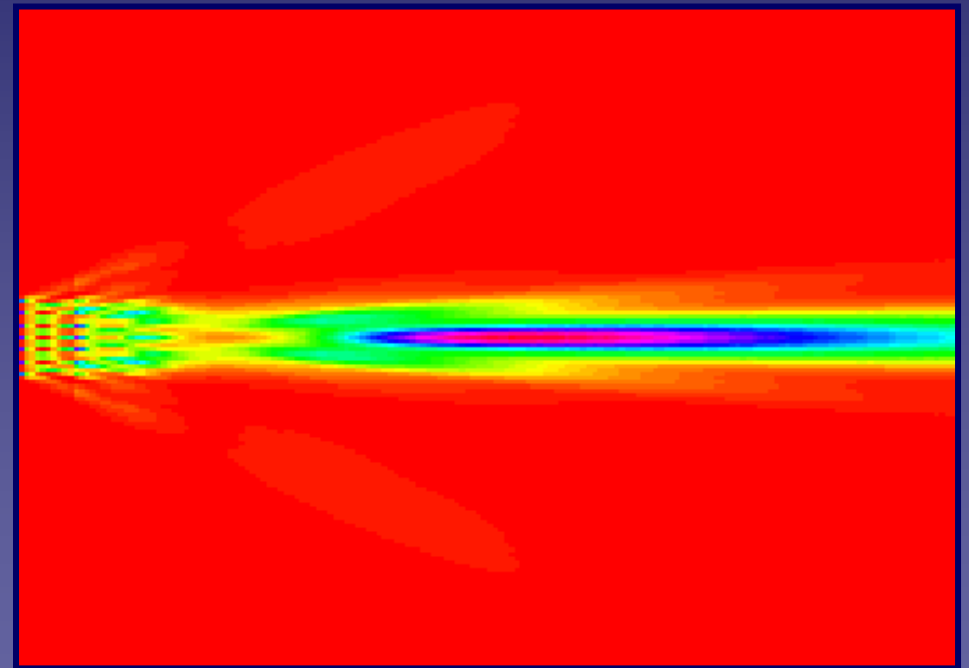
- Elastography and Palpography
- **Harmonics**
- Contrast agents
- Thermography
- Modulography

# Harmonic Imaging

Fundamental



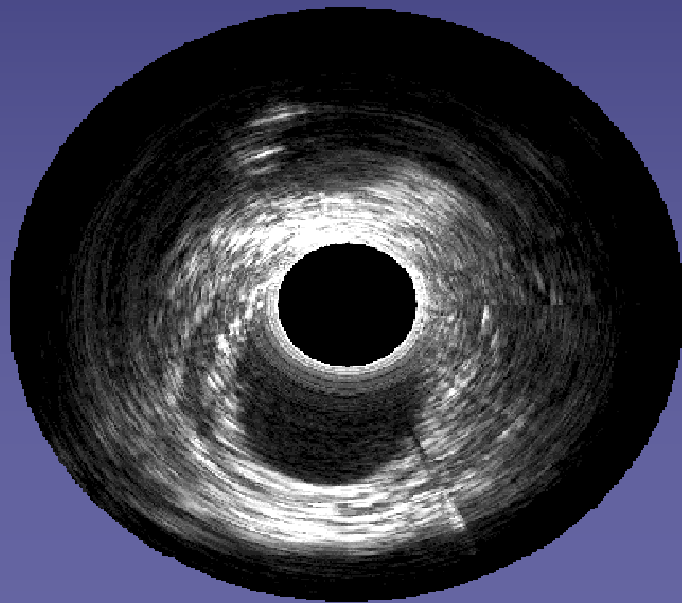
Second harmonic



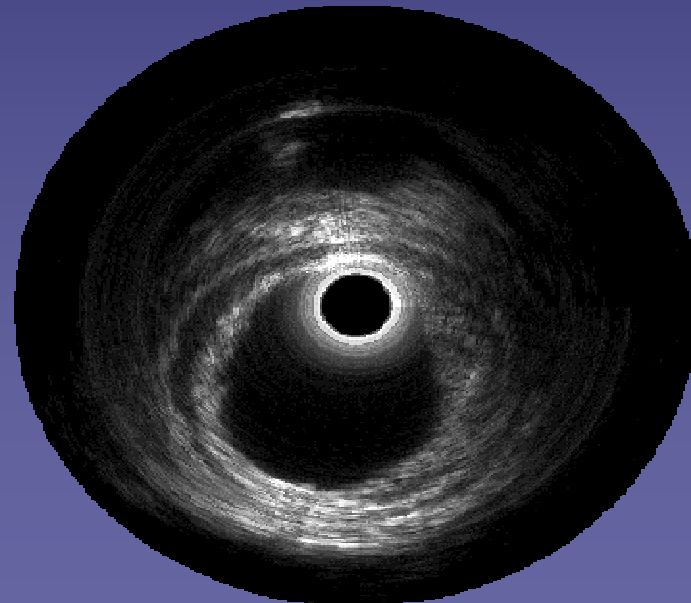


- A pilot study in Toronto (A.F.W. van der Steen et al., 1999) showed already the feasibility of Harmonic Imaging at higher frequencies.

Fundamental 20 MHz



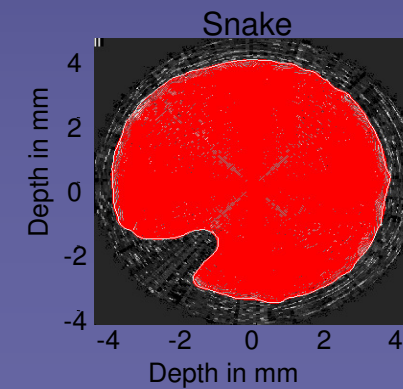
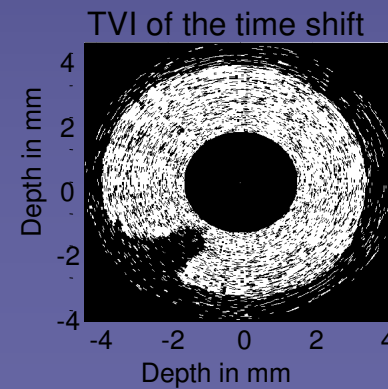
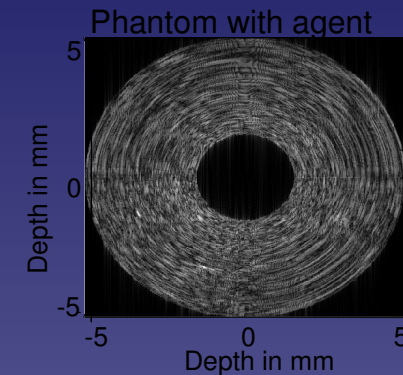
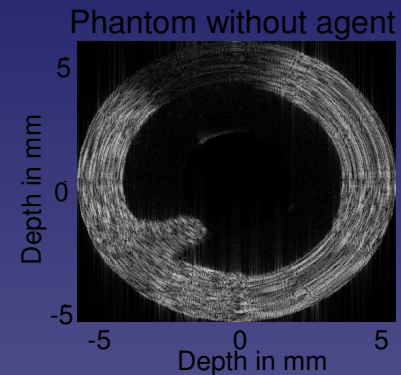
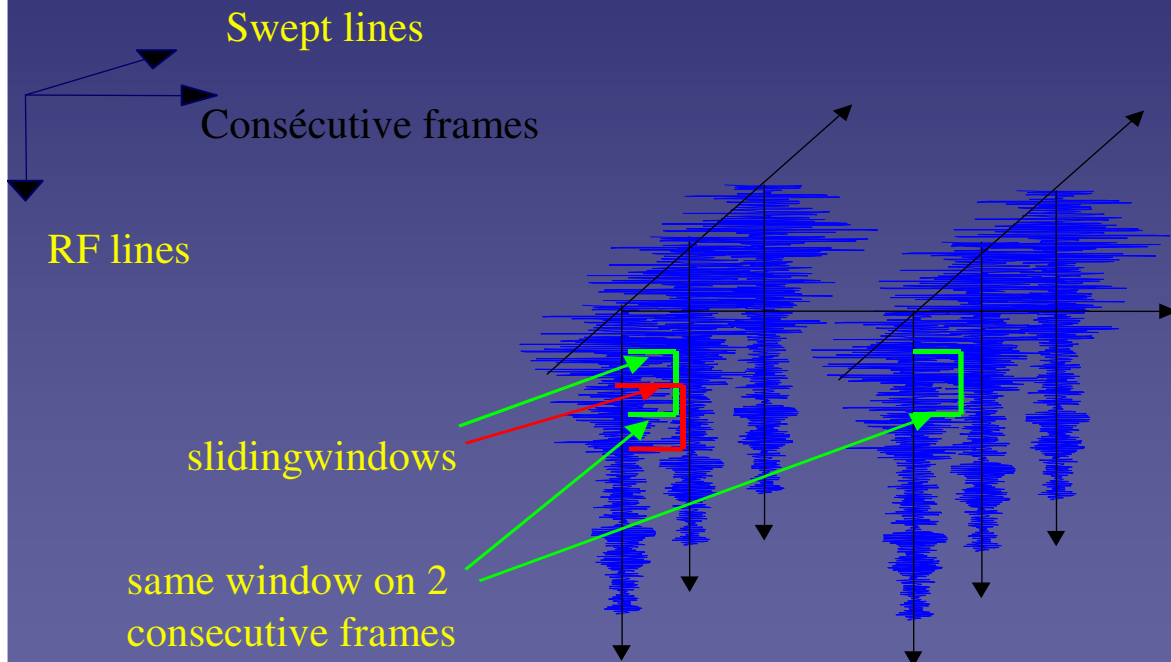
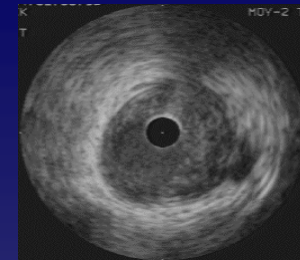
Harmonic 40 MHz



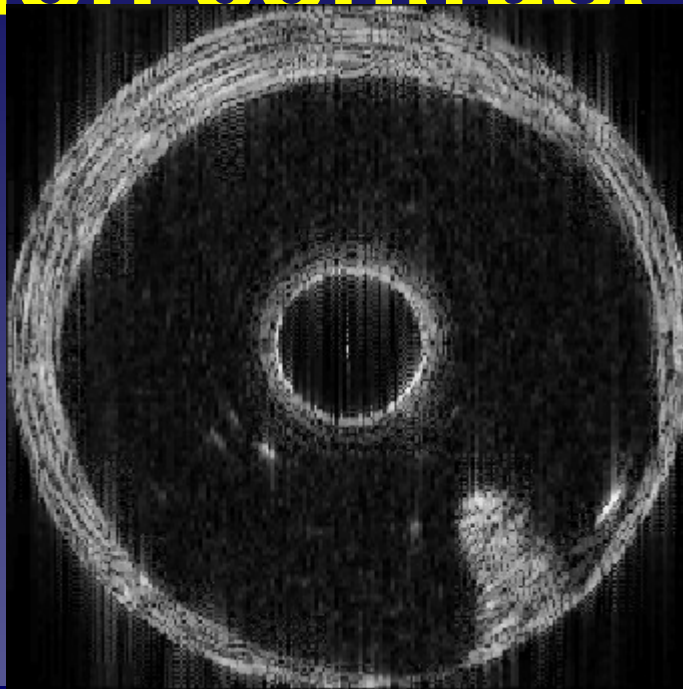
# IVUS diagnostic modality under investigation

- Elastography and Palpography
- Harmonics
- Contrast agents
- Thermography
- Modulography

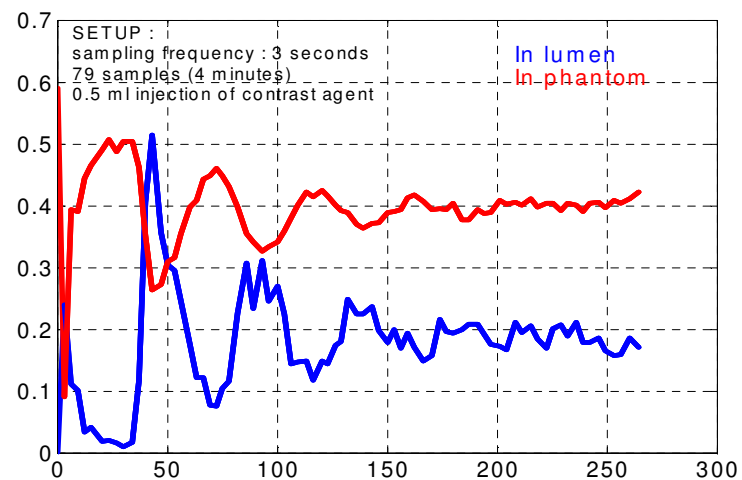
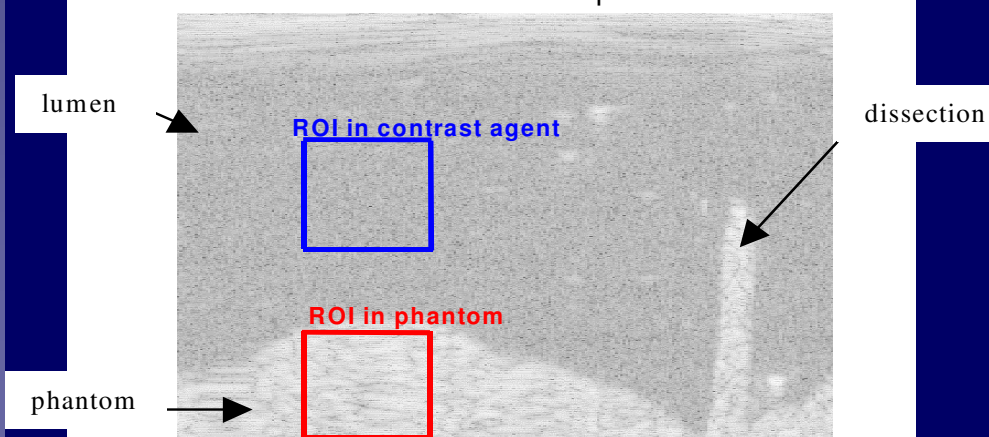
# ULTRASOUND CONTRAST AGENT IN INTRAVASCULAR ECHOGRAPHY: Parametric mapping based on RF output



# Injection contrast agent



ROIs in lumen and in phantom



# Conclusions

IVUS can provide the answer to all relevant diagnostic problems and therapy guidance related to atherosclerosis and restenosis

# IVUS

## What it is good at

- Tomographic imaging
- Free lumen assessment
- Plaque burden assessment
- Qualitative flow imaging
- Therapy guidance:
  - PTCA
  - Stent
  - Brachytherapy

## What it is not yet good at

- Plaque characterization
- Vulnerable plaque detection
- For moderate stenosis: “Should I treat it or not?”
- Quantitative flow measurement
- Shear stress measurement

# Future of intravascular

- Obtain more parameters

*wall characteristics*

*perfusion data*

- Combine with therapy and other modalities
- Make it less expensive

# Aknowledgement/coworkers

## Erasmus MC, Rotterdam

- Ton van der Steen
- Charles Lancee
- Nico de Jong
- Jolanda Wenzel
- Dave Goertz
- Martijn frijlink
- Antoinette ten Have
- Frits Mastik
- Chris de Korte
- Peter Burns
- Peter Frinking
- Jos Roelandt
- Folkert ten Cate
- Rob Krams
- Patrick Serruys

## CREATIS, Lyon

- Gerard Finet
- Elisabeth Brusseau
- Philippe Delacharte



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