



Implementation of cylindrical PET scanners with block detector geometry in STIR

Parisa Khateri*

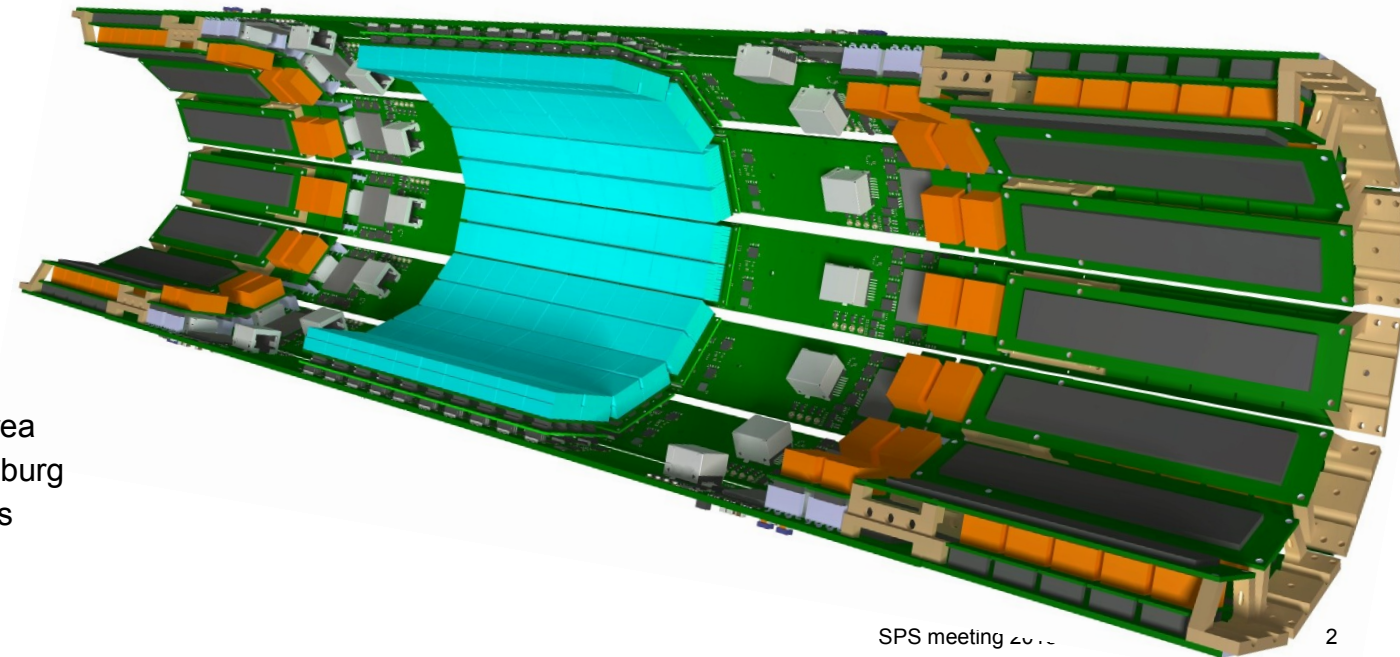
On behalf of the SAFIR collaboration

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SAFIR - Small Animal Fast Insert for MRI

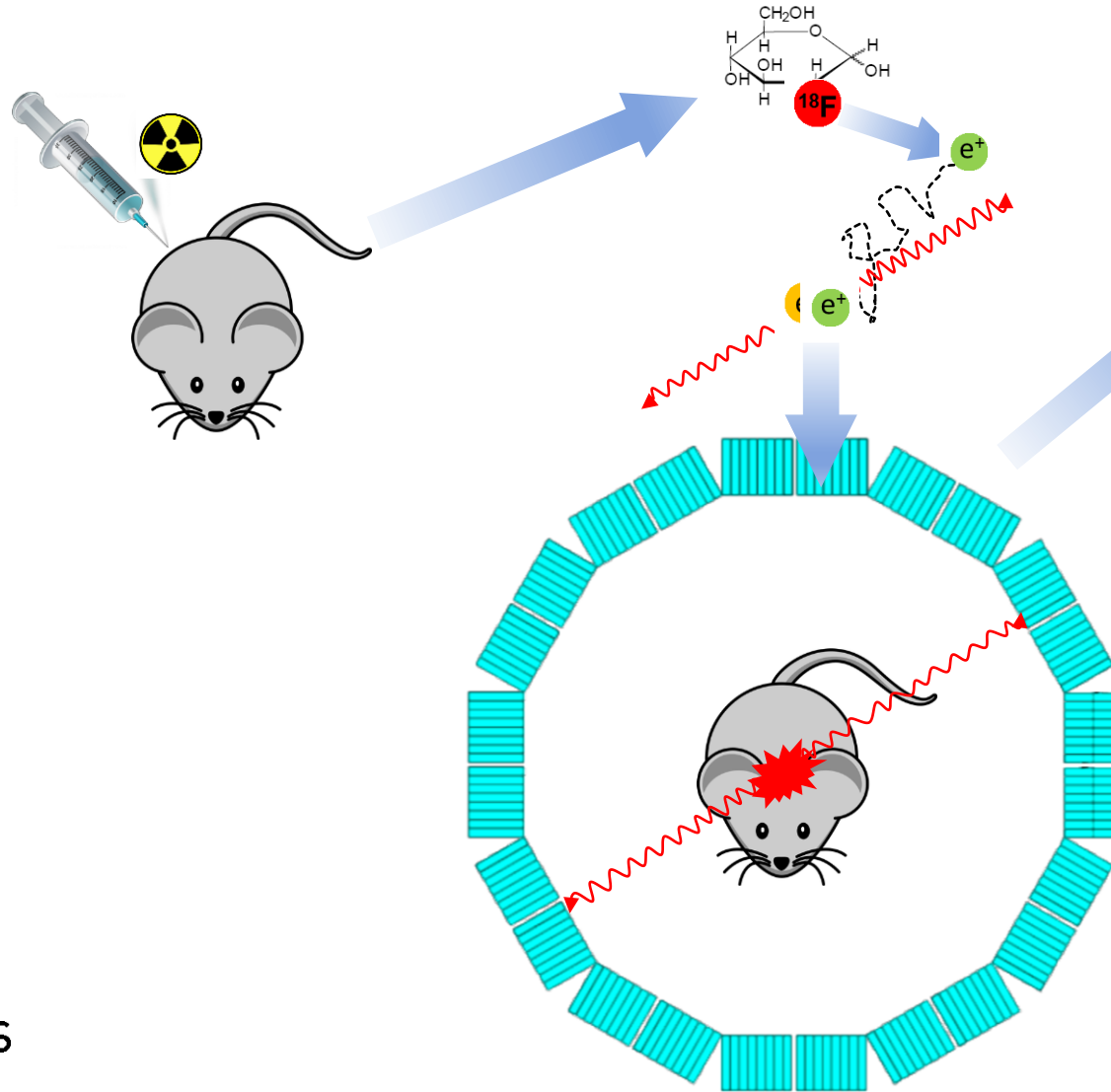


- Design, construction and characterization of a PET insert for a 7T Bruker BioSpec 70/30 pre-clinical MRI scanner
- Quantitative dynamic PET imaging simultaneous with MRI
- Data acquisition using short-lived isotopes such as ^{15}O
- An optimized reconstruction software



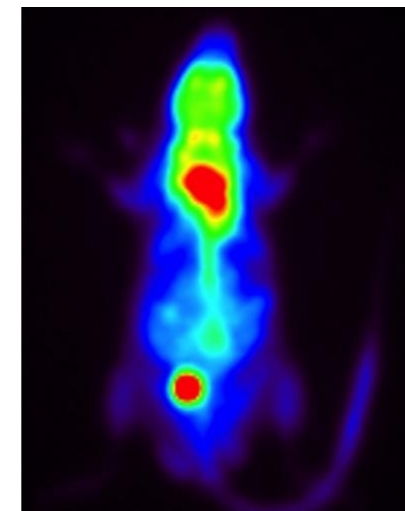
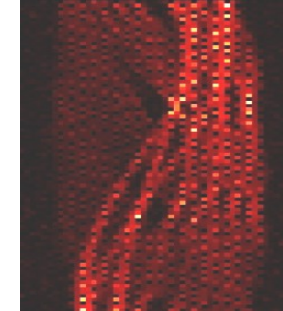
Institute for Particle Physics and Astrophysics - ETH Zurich
Institute for Pharmacology and Toxicology - University of Zurich
Institute for Biomedical Engineering - ETH Zurich
Clinic of Nuclear Medicine - University of Zürich
Instituto de Física Corpuscular - Universitat de València
Institute for Biomedical Engineering - ETH Zürich
Department of Nuclear and Quantum Engineering – KAIST - South Korea
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Institute of Cardiovascular and Metabolic Medicine - University of Leeds
Institute of Computer Engineering - University of Heidelberg

PET - Positron Emission Tomography

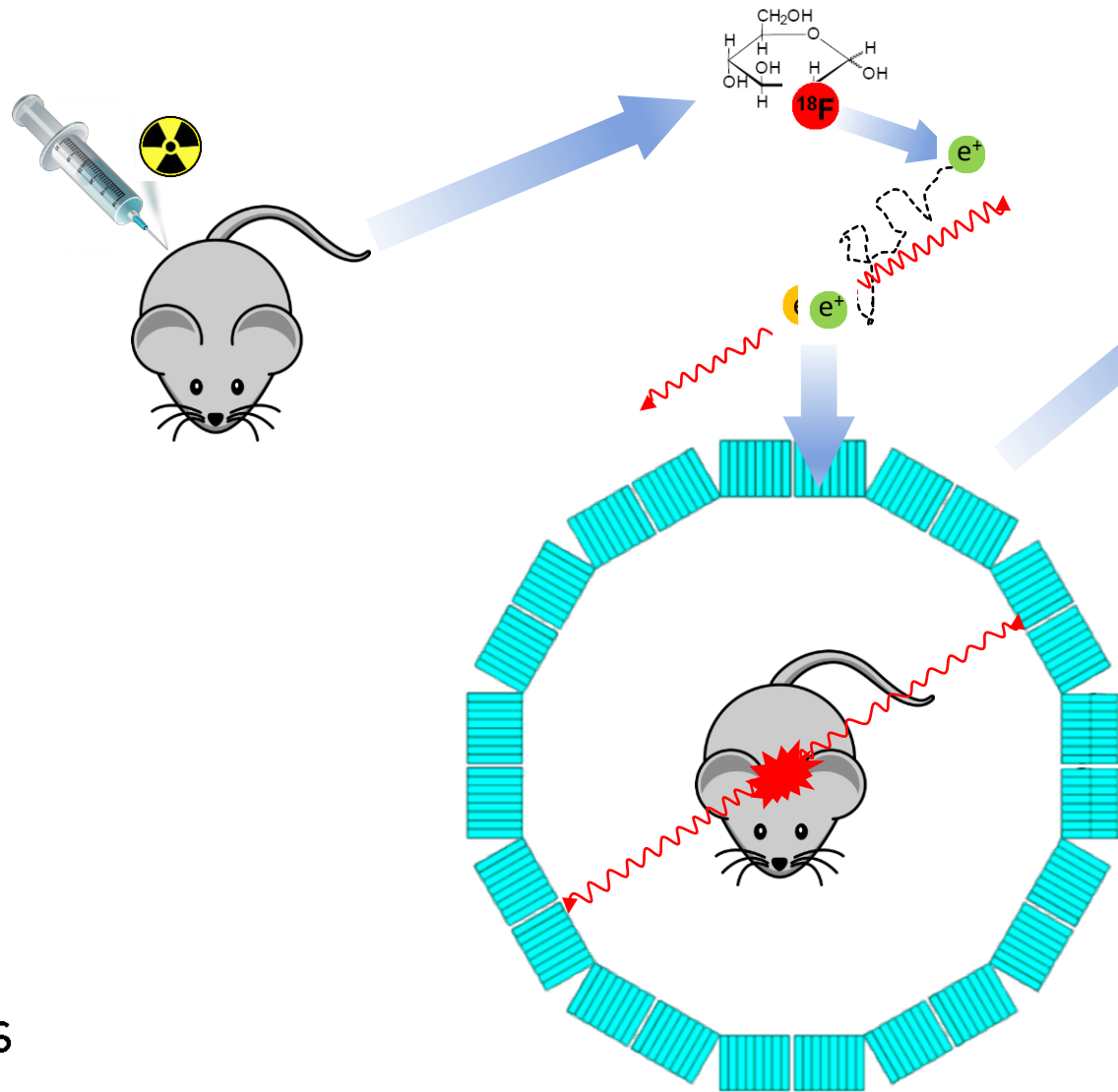


Coincidence events:

- Energy
- Time
- Detector pairs

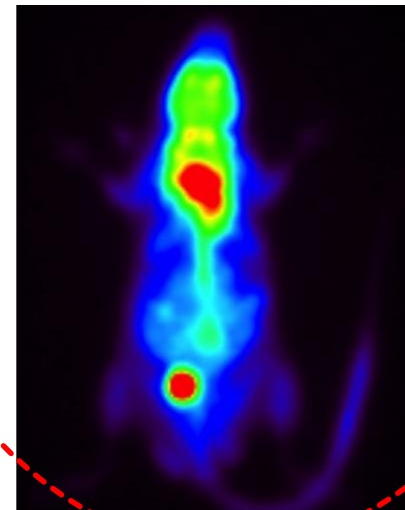
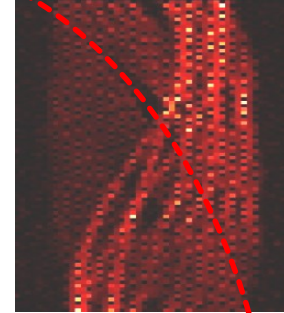


PET - Positron Emission Tomography



Coincidence events:

- Energy
- Time
- Detector pairs



Iterative Reconstruction

- Reconstruct images by MLEM or OSEM.

last update of voxel v

measured sinogram

$$f_v^{k+1} = \frac{f_v^k}{\sum_b a_{bv}} \sum_b a_{bv} \left(\frac{m_b}{\sum_v a_{bv} f_v^k + s_b + r_b} \right)$$

Next update of voxel v

Iterative Reconstruction

- Reconstruct images by MLEM or OSEM.

The diagram illustrates the iterative reconstruction formula for MLEM or OSEM. The formula is:
$$f_v^{k+1} = \frac{f_v^k}{\sum_b a_{bv}} \sum_b a_{bv} \left(\frac{m_b}{\sum_v a_{bv} f_v^k + s_b + r_b} \right)$$
 The terms are labeled as follows:

- f_v^{k+1} : Next update of voxel v
- f_v^k : last update of voxel v
- a_{bv} : System matrix
- m_b : measured sinogram
- s_b : scatter
- r_b : random

 A red arrow points from the a_{bv} term to the text "System matrix".

Iterative Reconstruction

- Reconstruct images by MLEM or OSEM.

$$f_v^{k+1} = \frac{f_v^k}{\sum_b a_{bv}} \sum_b a_{bv} \left(\frac{m_b}{\sum_v a_{bv} f_v^k + s_b + r_b} \right)$$

System matrix $\rightarrow \mathbf{A} = \mathbf{N} * \mathbf{L} * \mathbf{X}$

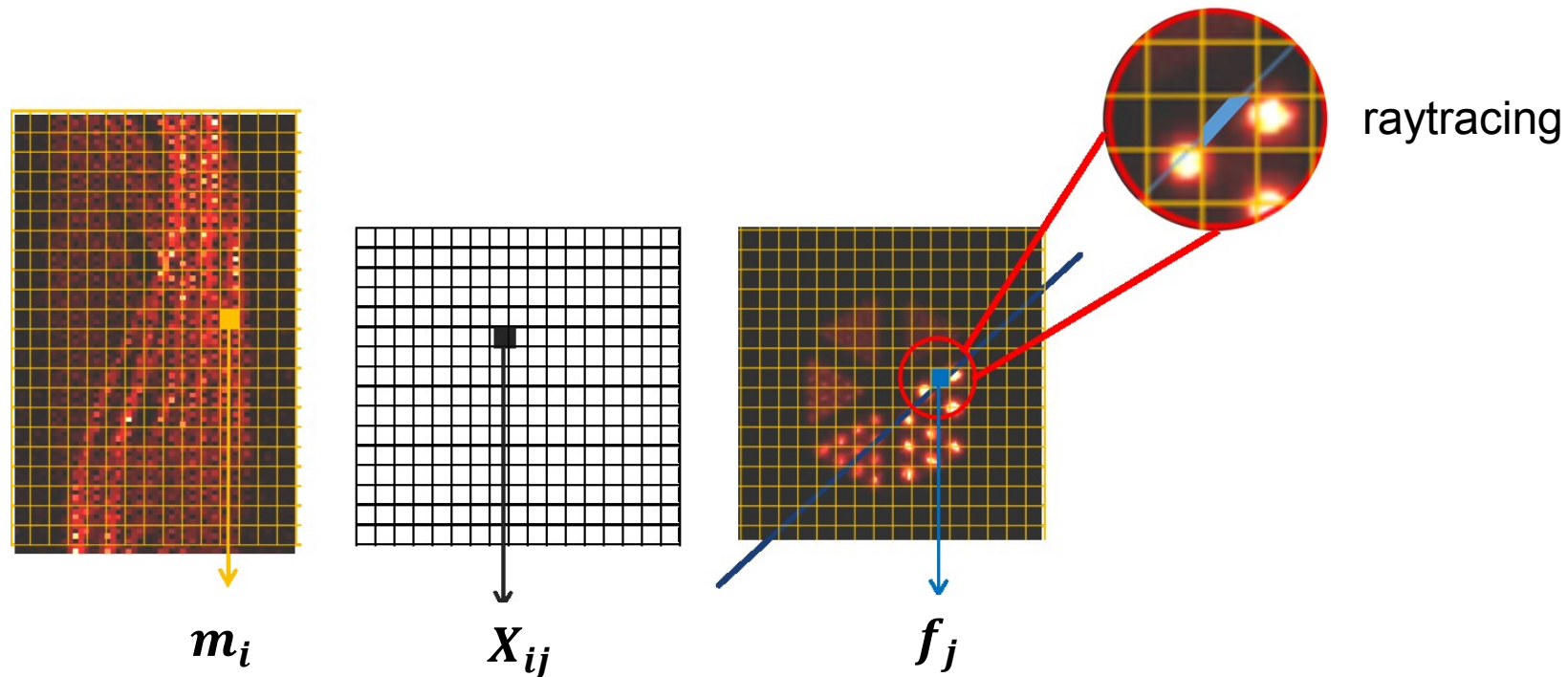
Attenuation

Normalization

Geometry

STIR – Software for Tomographic Image Reconstruction

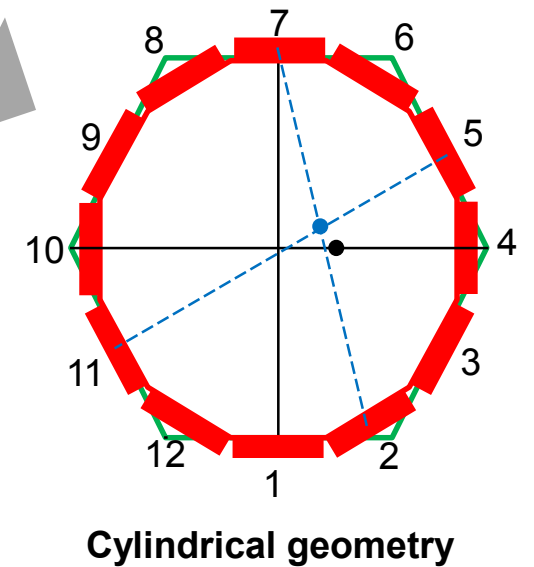
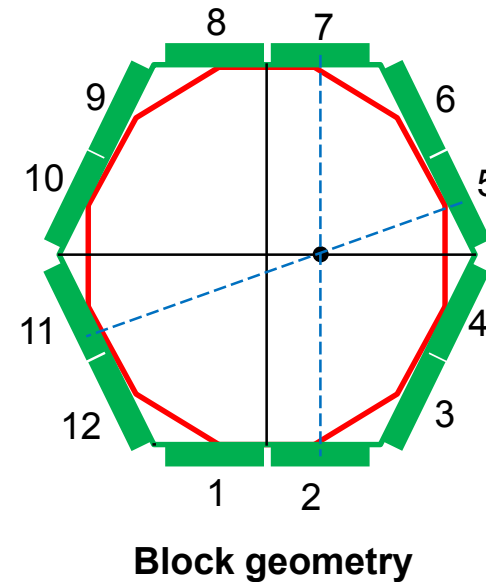
- MLEM: Maximum Likelihood Expectation Maximization
- OSEM: Ordered Subset Expectation maximization
- Siddon's algorithm



STIR – Software for Tomographic Image Reconstruction

■ Block vs. Cylindrical

- Scanner model
- Projection data bins $\left. \begin{array}{l} \theta \\ \phi \\ t \\ s \end{array} \right\}$
- System matrix
- Symmetries to speed up the calculation

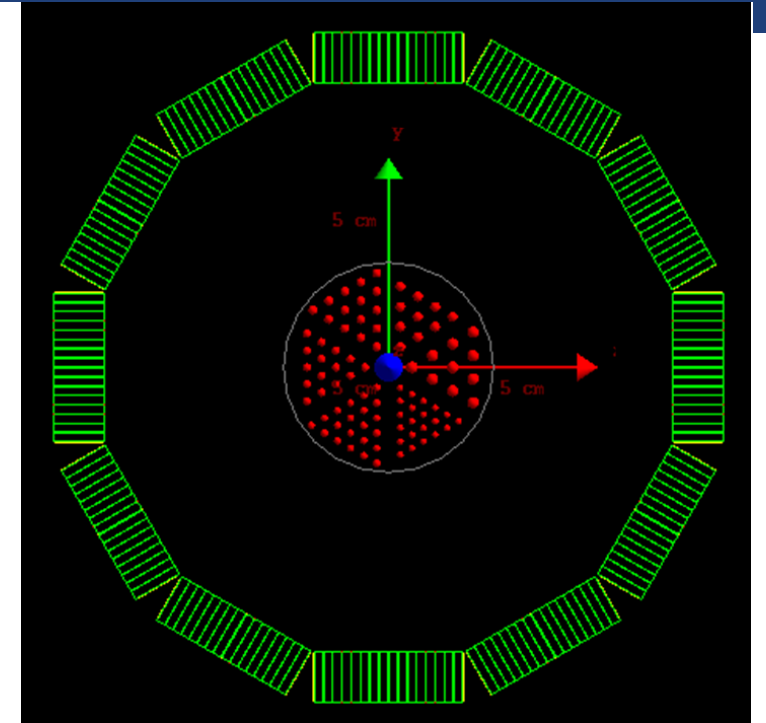


Simulation data

- Gate v7.2
- Scanner: SAFIR prototype
 - 2 blocks in axial direction
 - 24 blocks in trans-axial direction

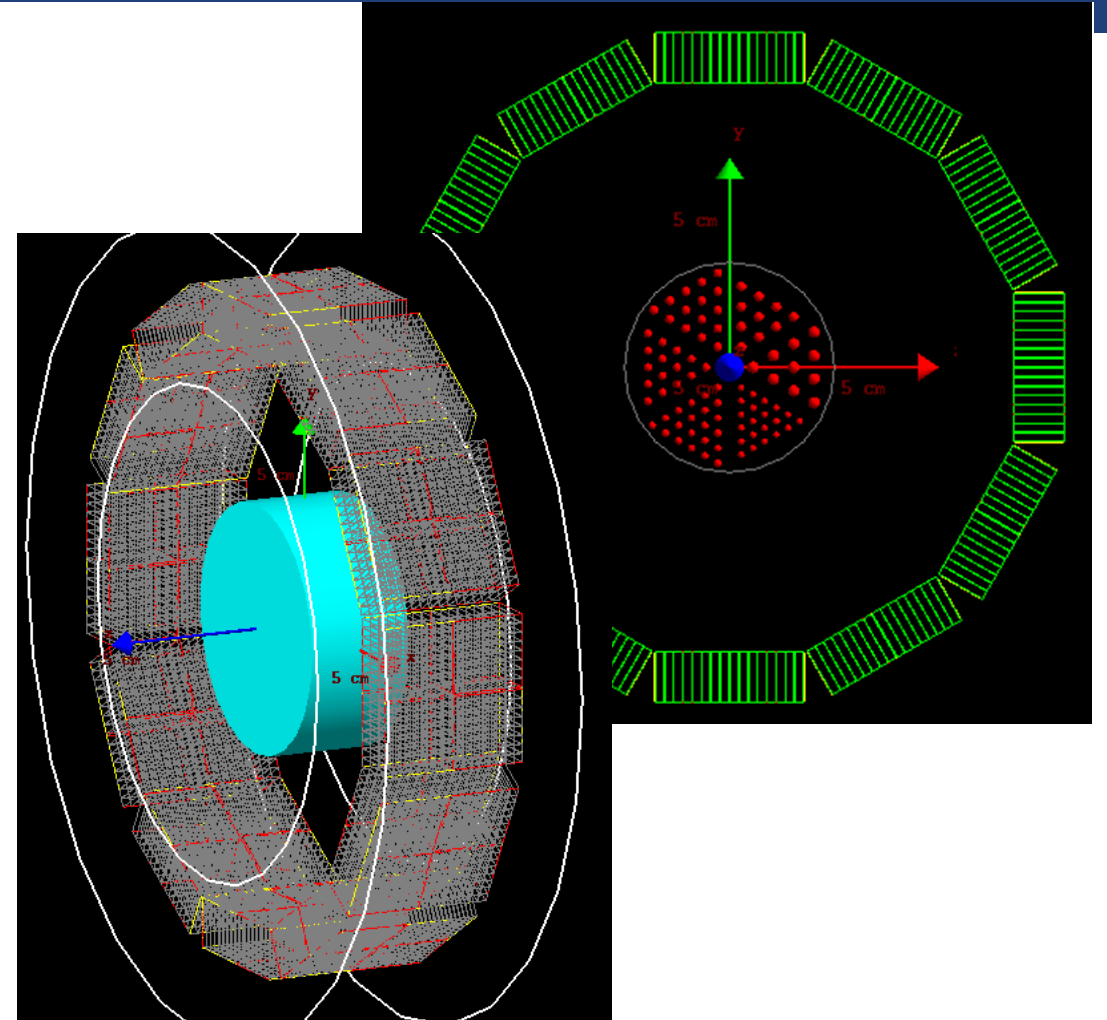
Simulation data

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 - 2 blocks in axial direction
 - 24 blocks in trans-axial direction
- Phantoms:
 1. Derenzo phantom



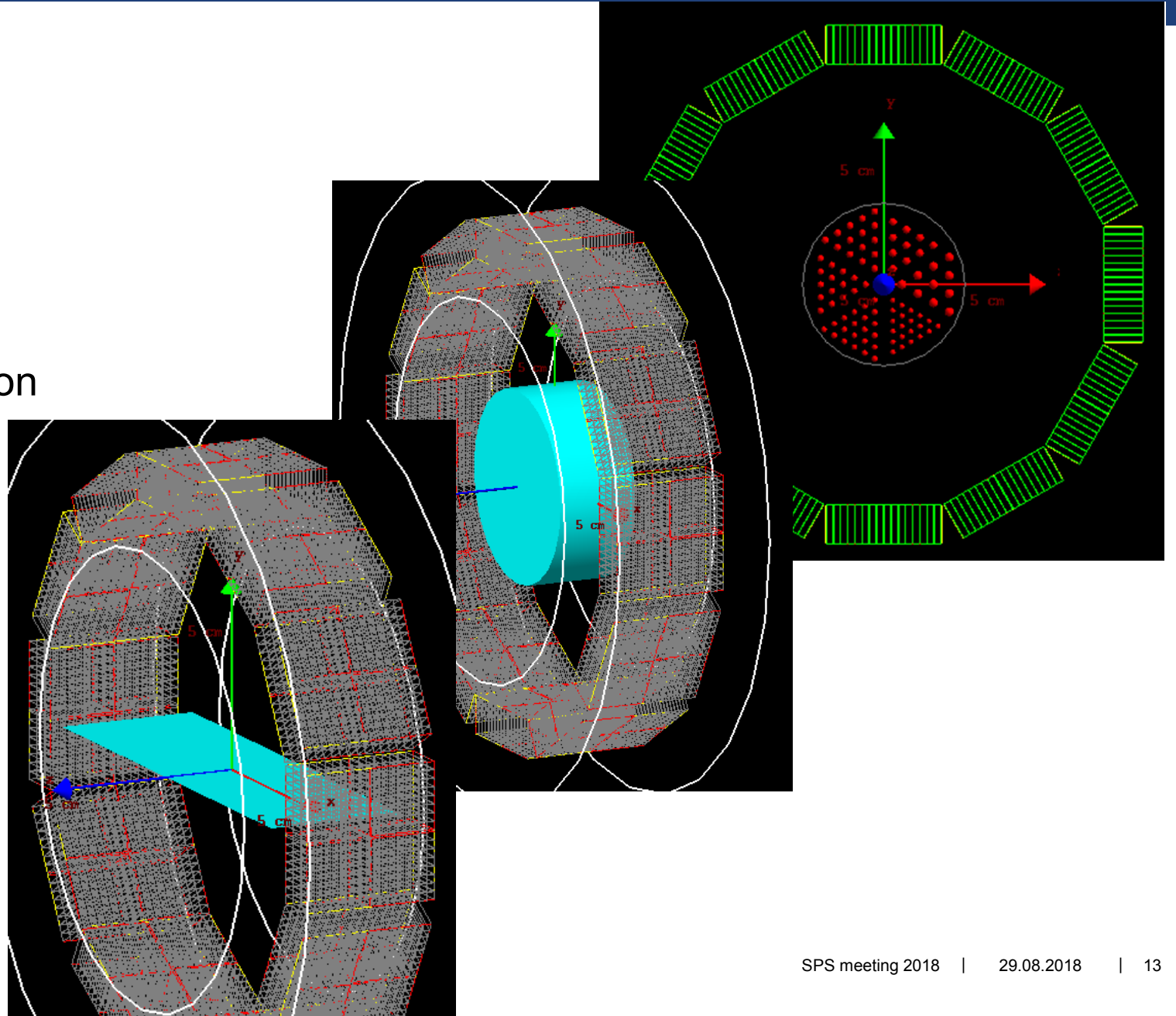
Simulation data

- Gate v7.2
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 - 24 blocks in trans-axial direction
- Phantoms:
 1. Derenzo phantom
 2. Uniform cylinder



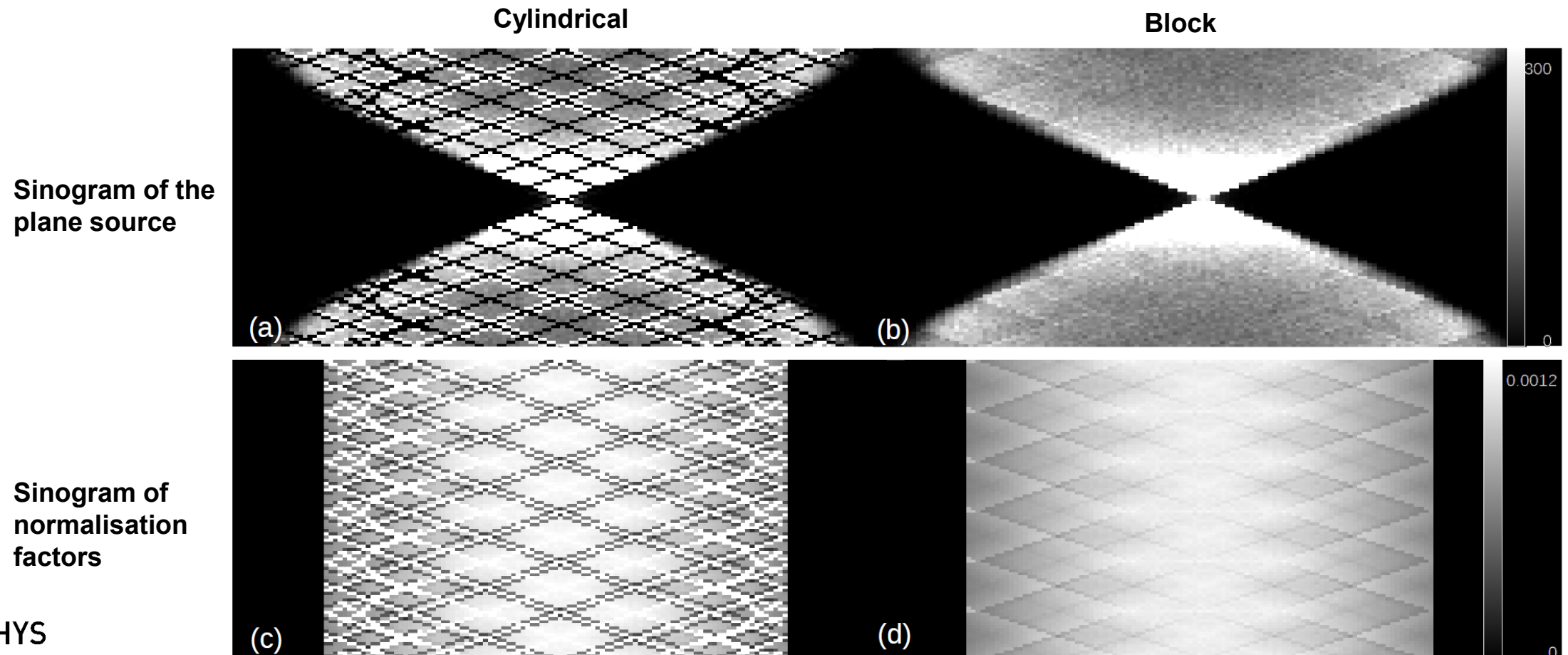
Simulation data

- Gate v7.2
- Scanner: SAFIR prototype
 - 2 blocks in axial direction
 - 24 blocks in trans-axial direction
- Phantoms:
 1. Derenzo phantom
 2. Uniform cylinder
 3. Rotating plane



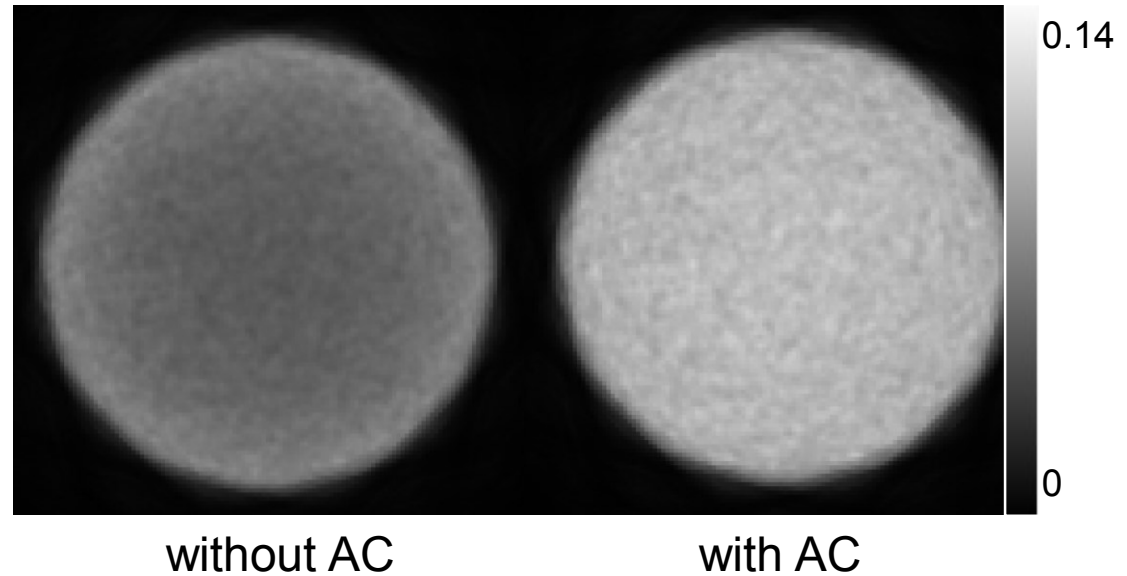
Reconstruction

- Projection bins: of about $\sim 4M$
- Normalization Correction (NC)



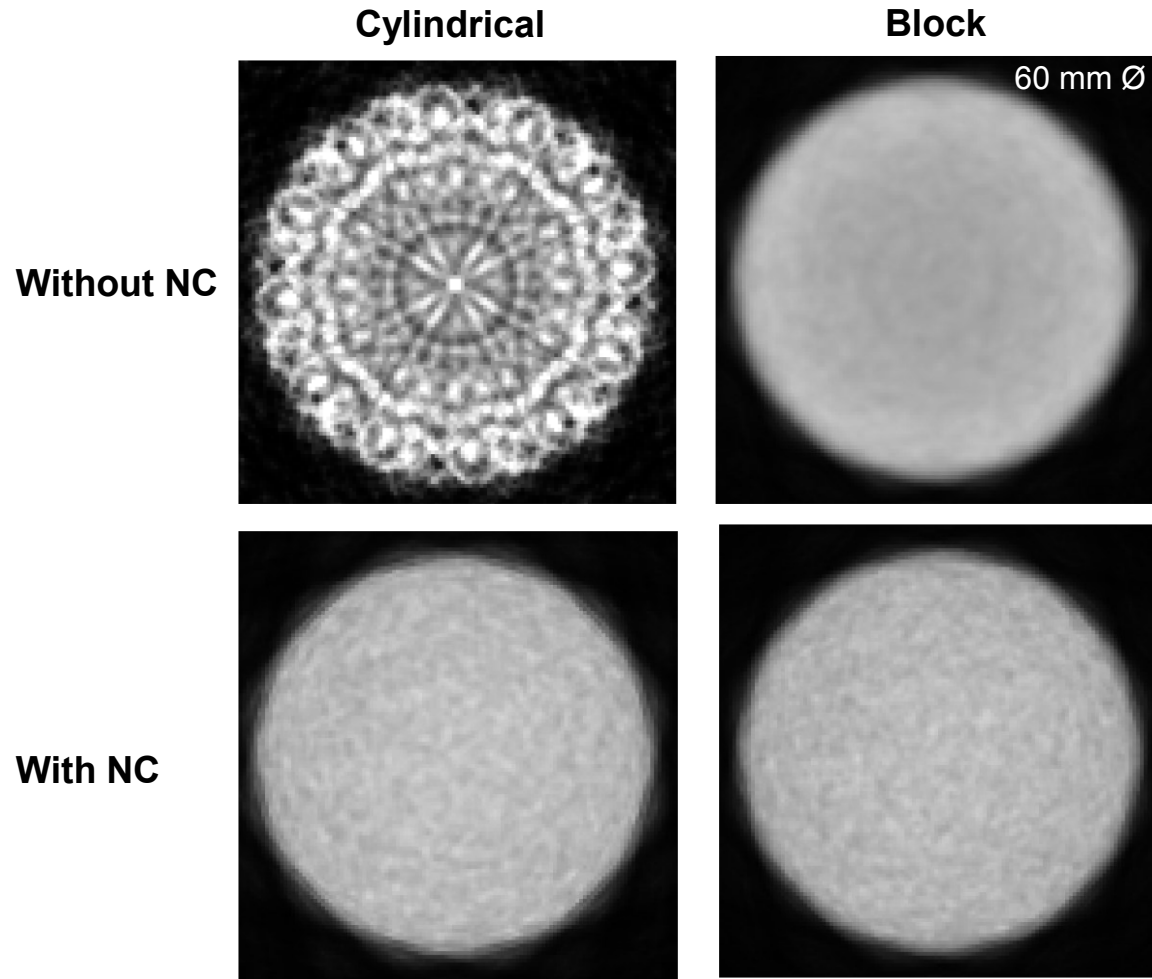
Reconstruction

- Projection bins: of about ~ 4 M LORs
- Normalization Correction (NC)
- Attenuation Correction (AC)
- OSEM: Ordered Subset Expectation maximization
 - 6 subsets, 24 iterations



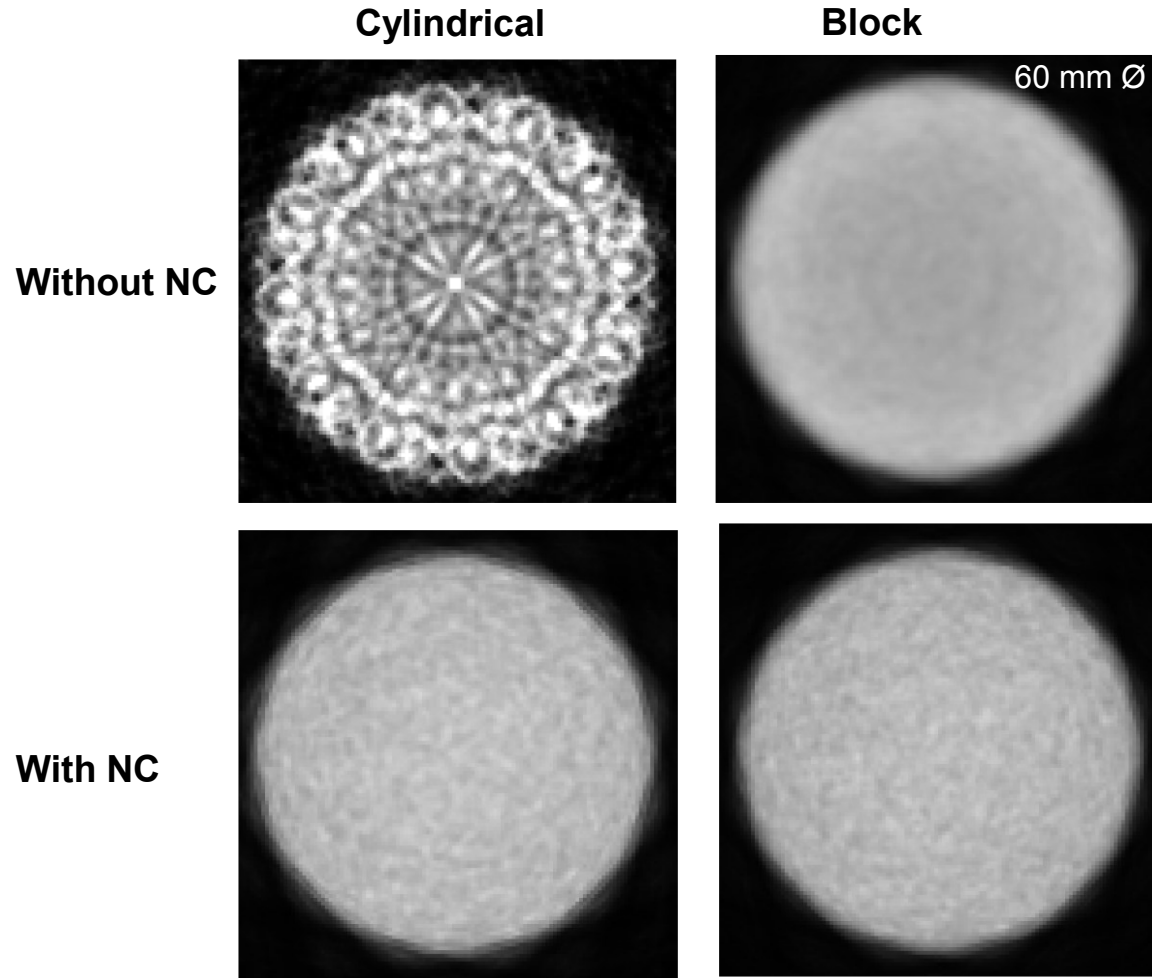
Results

Uniform cylinder phantom



Results

Uniform cylinder phantom

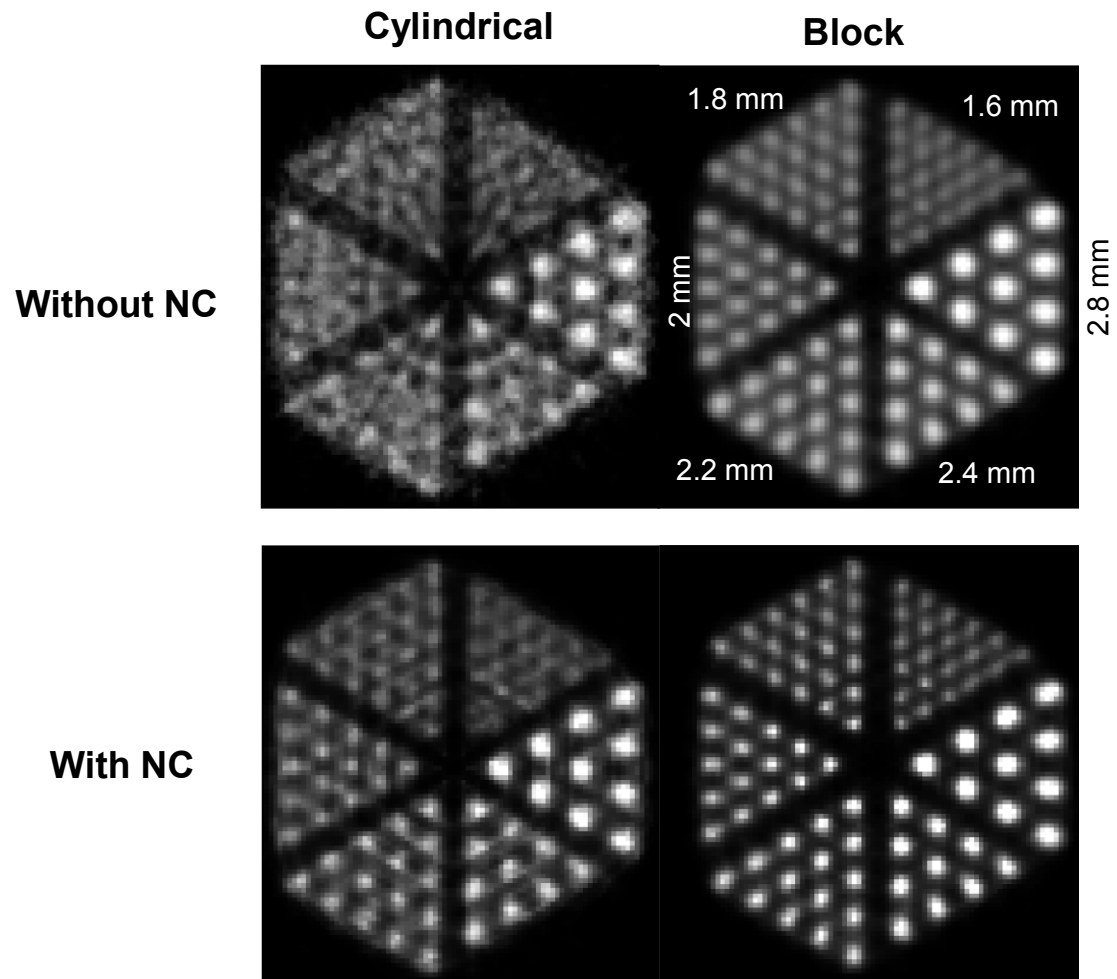


coefficient of variation (CoV): $\frac{\text{standard deviation}_{ROI}}{\text{mean}_{ROI}}$

Reconstruction Method	Correction	CoV
Cylindrical	Without NC	33.2%
Block	Without NC	18.4%
Cylindrical	With NC	25.8%
Block	With NC	20.9%

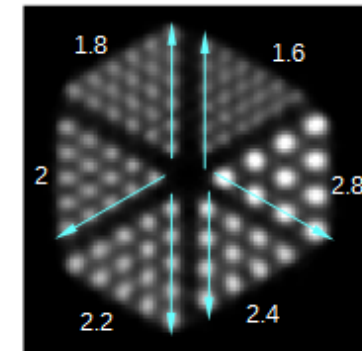
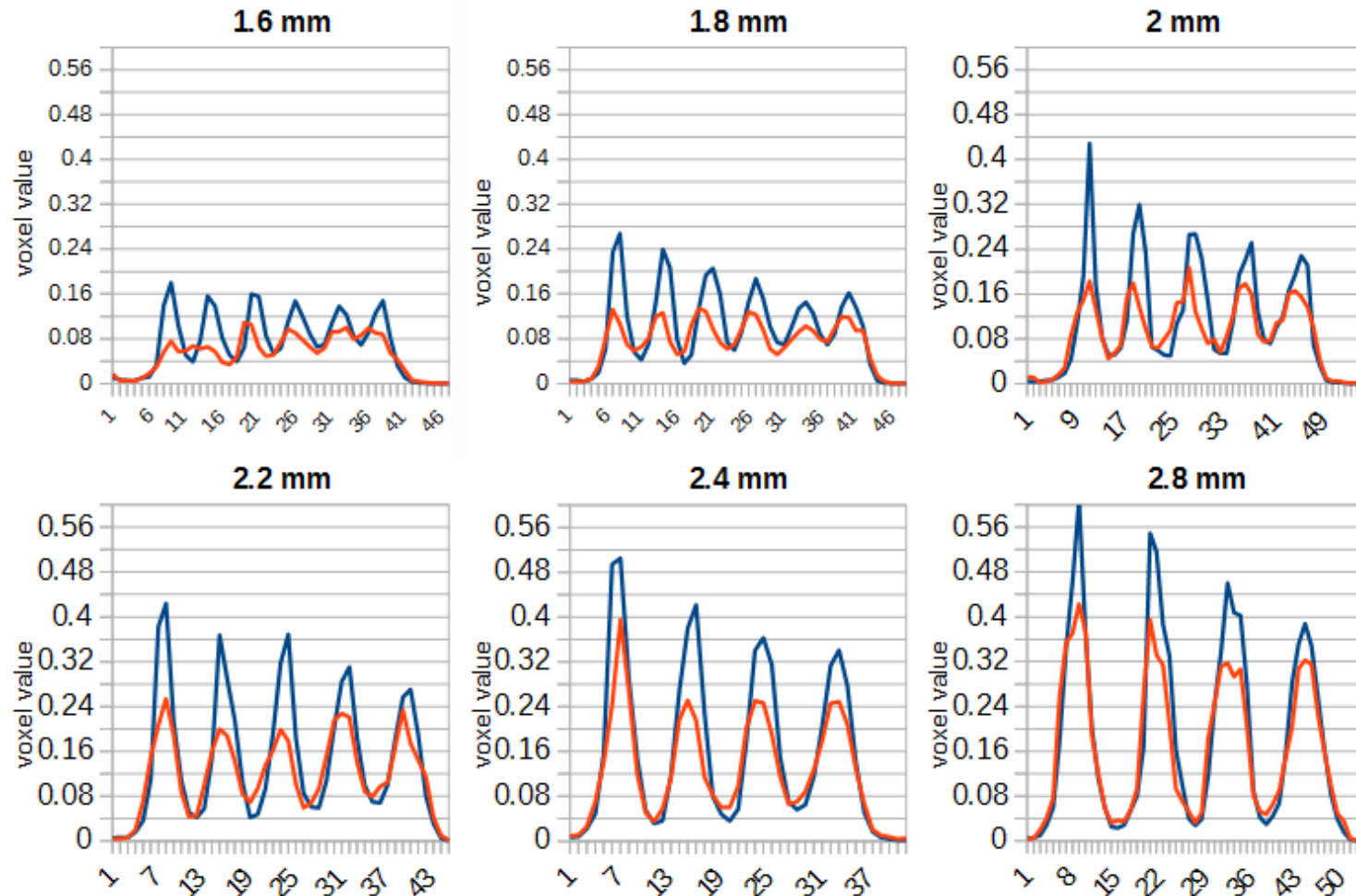
Results

Derenzo phantom



Results

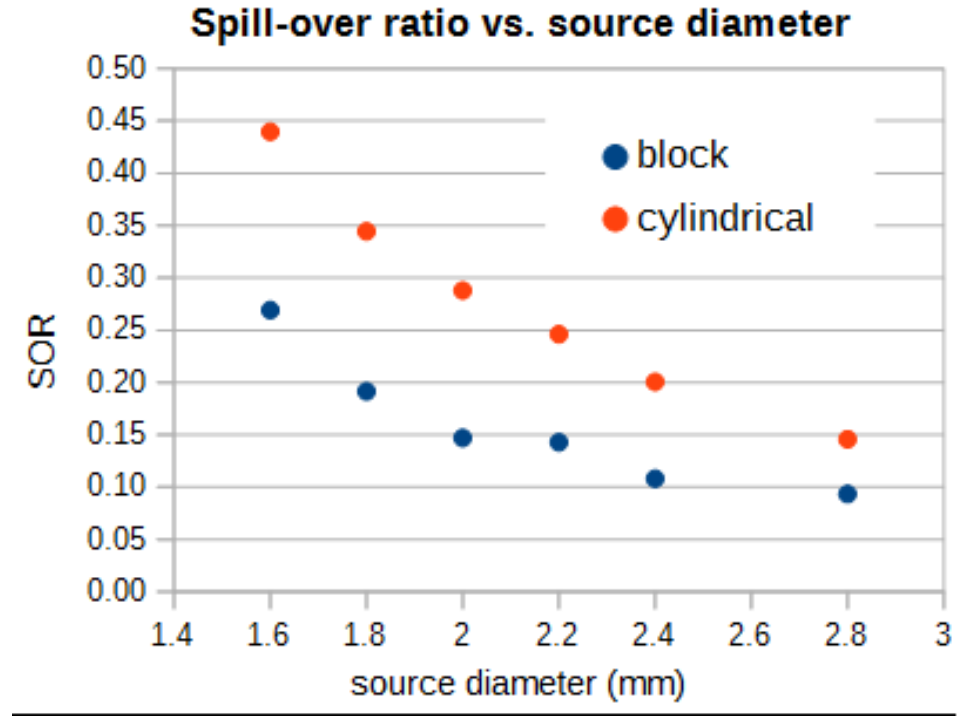
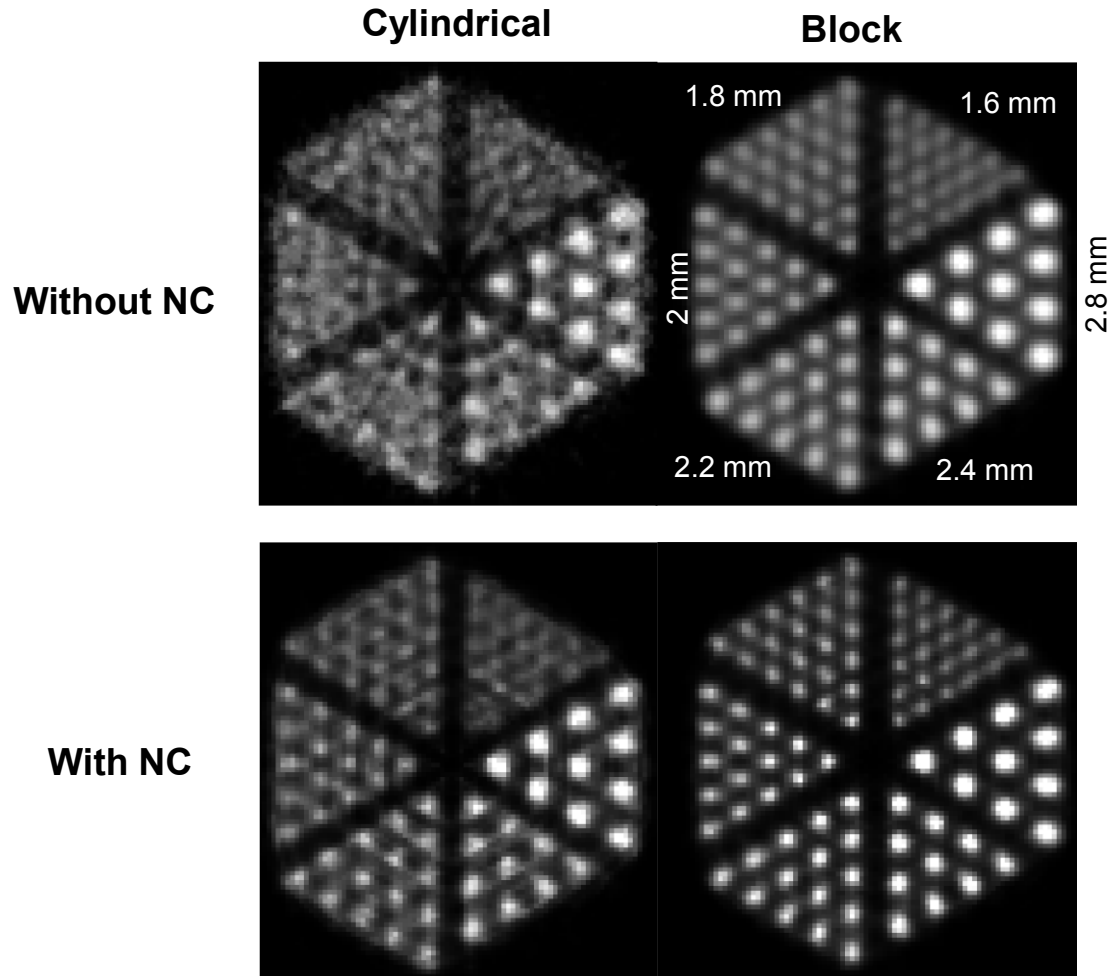
Line profiles through Derenzo phantom



— block
— cylindrical

Results

Derenzo phantom



Summary

- Image reconstruction for the SAFIR PET scanner is implemented using STIR.
- An accurate system matrix is necessary for quantitative PET image reconstruction.
- The scanner model - as a key component to the system matrix – is simplified in STIR.
- A realistic scanner model has been implemented in STIR.
- The new model enhanced the image quality in terms of Resolution and Uniformity.
 - decrease the partial volume effect and enhance the contrast

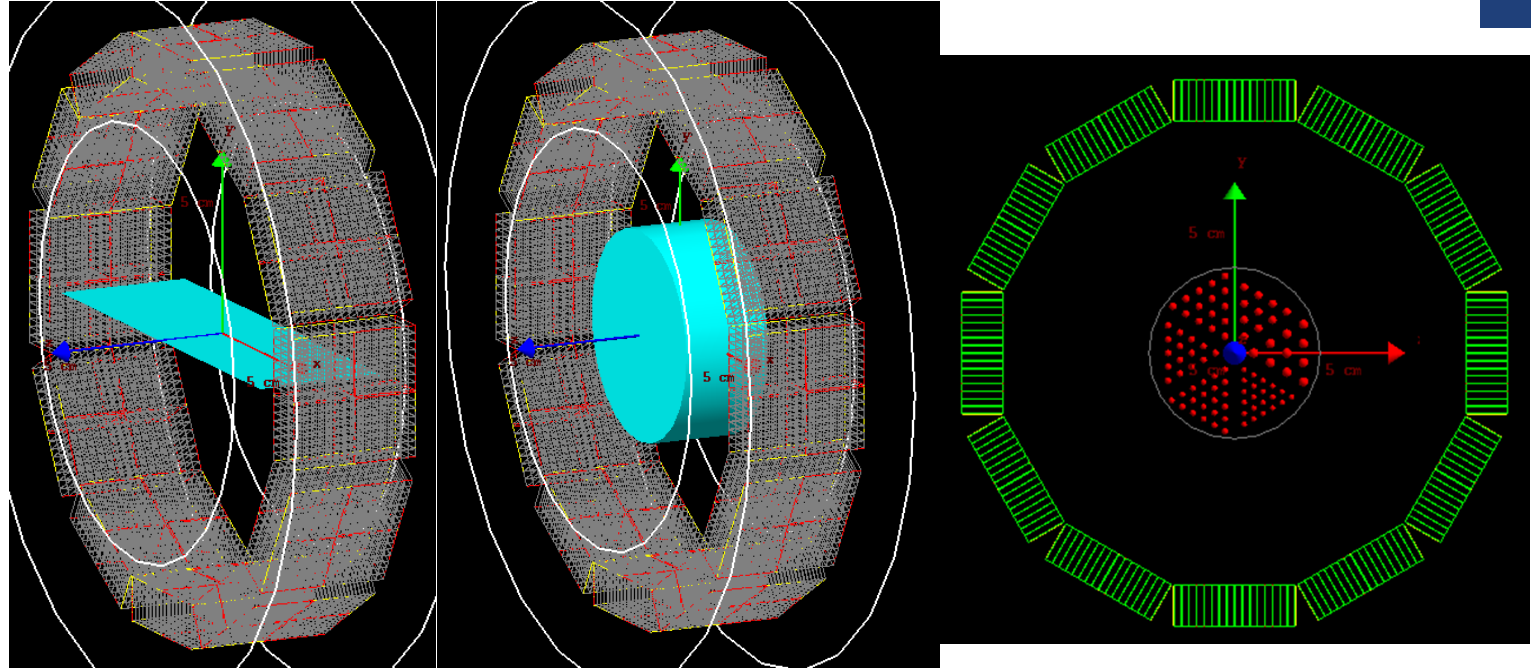
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Thank you!

Simulation data

- Gate v7.2
 - Scanner: SAFIR prototype
 - 2 blocks in axial direction
 - 24 blocks in trans-axial direction
 - 8×8 detector blocks
 - dodecagon prism
 - Length: 32.20 mm
 - Inner radius: 67.75 mm
 - Phantoms:
 1. Derenzo phantom:
 - 100 MBq of ^{18}F
 - acquisition time: 5 s
- Energy window: [350, 650] keV
 ■ Coincidence time window: 1 ns



2. Uniform cylinder:

- water-filled cylinder (25 mm × 60 mm Ø)
- 100 MBq of ^{18}F
- acquisition time: 2.5 min

3. Rotating plane:

- plane (32 mm × 120 mm)
- 6 equally spaced angles
- acquisition time: 80 min per position
- back-to-back 511 keV gammas

Results

Derenzo phantom

