



New e- linac therapies and accelerator designs





OUTLINE



The Challenges of Radiotherapy
 New RT approaches

> VHEE therapy
 > State of the art
 > Milestones
 > New delivery doses modalities
 > Grid mini-beams
 > FLASH

Accelerators for VHEEE: linacs
 Low-energy e High-energy e-

> Summary and Future perspectives

CHALLENGES IN RADIOTHERAPY New RT approaches



- RT treatment of some radio resistant tumours, paediatric cancers and tumours close to a delicate structure (i.e. spinal cord) is currently limited
- One of the main challenges is to find approaches to increase the normal tissue resistance
- Standard RT is restricted to the few temporal and spatial schemes, dose rates, broad field sizes: mainly photons, 2 Gy/session, 1 session/day, 5 days/week, dose rates ~ 2 Gy/min, field sizes > cm², homogeneous dose distributions

Possible strategies to spare normal tissue

- > Different particle types: Very High Energy Electrons (VHEE)
- Different dose delivery methods: Grid Mini-beam or FLASH RT









State of the Art

- With recent High-Gradient linac technology developments, Very High Energy Electrons (VHEE) in the range 100–250 MeV offer the promise to be a cost-effective option in anticancer RT and open up innovative treatment modalities (Grid mini-beam, FLASH,..)
- Their ballistic and dosimetric properties can surpass those of photons, which are currently the most commonly used in RT
- Their position compared to protons need to be evaluated, but they can be produced at a reduced cost



State of the Art

> Pros

>> Cons

- > + Conformity ?
- > + Decrease of the integral dose rate
- > + High-dose rate
- > + Scanned beams
- > + Compact,Cheap
- > + Focused



- ➤ Bone dose ?
- > Penumbra?
- > Effect of inhomogeneities?
- > Neutrons ?

> -....







Milestones: Treatment Planning

Treatment plan comparison between VHEE, VMAT and PBS





Milestones: Beam dosimetry

- Beam Dosimetry studies with 50 70 MeV (NLCTA) and 160 MeV (SPARC) VHEE beams
- Beam dosimetry experiments with a 135 MeV laser-plasma wakefield accelerator (ALPHA-X)
- > Beam dosimetry in CLEAR with 200-250 MeV
 - Radiosensitive films for focusing
 - Ionisation chambers for charge
 - Alanine pellets for profile depth dose
 - Generate the total dose (~10 Gy) on
 biological dosimeters in a single pulse
 (<100 ms) for profile depth dose



- Dosimetry for ultra-high dose rate and development of dosimeters is mandatory for a clinical application (EURAMET - EMPIR 2018)
- No experiments to date with 200 250 MeV beams and focused electron beams on tissue like media – essential step before patient treatment planning



0.01

Quasi-homogeneous dose profile

erapy (MBRT)

0.01

Heterogeneous dose profile

S NEW DELIVERY DOSE MODALITIES What is FLASH RT?

New way of dose delivery consisting in ultra short irradiation time or "beam on time" (<500 ms) and very high-dose (60-200 Gy/s)</p>

Dose, dose-rate, beam-on time... what requisites for the "FLASH effect" ?

- No FLASH effect *in vitro* with clonogenic cell death as an endpoint (*Nias et al. Br J Radiol 42: 553, 1969*). The FLASH effect relates to normal, living tissue only.
- The beam-on time, not the dose-rate appears to be the major determinant of the FLASH effect
- Ultrahigh dose-rate pulses (e.g. 10¹³ Gy/s) will NOT provide a FLASH effect as long as the dose per pulse is low and the total length of radiation exposure exceeds 100-500 ms



FLASH THERAPY First Proof-of-Concept with low-energy e⁻



Radio-induced lung fibrosis in C57BL/6J mice 15 Gy in single dose (bilateral thorax irradiation)



FLASH THERAPY First Proof-of-Concept with low-energy e⁻



Sci Transl Med 6: 245ra93, 2014

- FLASH spared normal lung tissue at doses known to induce fibrosis in mice exposed to conventional dose-rate irradiation (CONV).
- FLASH spared smooth muscle cells in arterioles from radio-induced apoptosis.
- No difference between FLASH and CONV with regard to tumor growth inhibition.
- However, normal tissue sparing by FLASH allowed dose escalation without complications, resulting in complete tumor cure in some xenograft models.





1st RAON workshop - A. Faus-Golfe



FLASH THERAPY What are the underlaying mechanisms in FLASH effect The role of the oxygen

HYP: FLASH-RT induces a transient radiation-induced hypoxia that protects only the normoxic tissues



FLASH THERAPY Towards a clinical practice





ACCELERATORS FOR VHEE Accelerators for FLASH-RT: low-energy e⁻



institut**Curie**

LINAC "Kinétron" (1987) 4.0-5.0 MeV electrons Triode electron gun

LET = 0.19 keV/µm RBE = 1.00 relative to ⁶⁰Co (Compton only)

Pulse width 0.05 - 2.2 µs Repeat frequency 0.1 - 200 Hz Peak current 0.01 - 220 mA Dose per pulse 0.001 - 50 Gy

Mean dose-rate 0.01 - 7000 Gy.s⁻¹ Maximum dose-rate during the pulse ≈ 2 10⁷ Gy.s⁻¹



FLASH in vivo





PRÁE









December 2017



ACCELERATORS FOR VHEE Accelerators for FLASH-RT: high-energy e⁻

> S-band: RF gun+ Linac (HG)

+ 1	-			111
		N		
-	36	11	-	

MIL	instrur
Lar	

research instruments	-

	·
Parameters	
Energy	70 – 140 [MeV]
Charge (variable)	0.00005 – 2 [nC]
Normalized emittance	3-10 [mm mrad]
RF frequency	3.0 [GHz]
Repetition rate	50 [Hz]
Bunch length, rms	< 10 [psec]
Energy spread, rms	< 0.2 %
Bunches per pulse	1

Platform for Research and Applications with Electrons







ACCELERATORS FOR VHEE Accelerators for FLASH-RT: high-energy e



Preliminary considerations









A. Grudiev



ACCELERATORS FOR VHEE Accelerators for FLASH-RT: high-energy e⁻



Preliminary considerations

Version 1: Dimensions







SUMMARY and FUTURE PERSPECTIVES

Challenge in RT is to find possible strategies to spare normal tissue

- Different particle types: Very High Energy Electrons (VHEE)
- Different dose delivery methods: Grid mini-beam or FLASH RT



3-5 April 2019

- Srid mini-beams consists of combination of VHEE (> 70 MeV) with spatial fractionation (400-700 μm, scanning, small divergence) with high-dose healthy tissue tolerance
- FLASH consists of ultra short irradiation time or "beam on time" (<500 ms) and very high-dose (60-200 Gy/s), that spare normal tissues from radiation-induced toxicities
 - Understanding the FLASH-RT limits (min/max dose/time)
 - > Minimum beam on-time: ms => μ m=> ns ? Bunching structure?
 - Maximun dose > 200 Gy/s ?
 - Understanding the FLASH-RT underlying mechanism:
 - > Biological studies
 - Chemical and kinetic: role of the oxygen
 - Extending to other species: p, ¹²C
- Dosimetry for ultra-high dose rate is a key stone, development of dosimeters is mandatory for a clinical application (EURAMET - EMPIR 2018)

> Which Accelerator is the most suitable to cope the necessary performances? ²³



APPLICATIONS OF PARTICLE ACCELERATORS IN EUROPE





THANKS:

- LAL: Y. Han, B. Bai, C. Vallerand, P. Duchesne, P. Lepercq
- CERN: M. Dosanjh, S. Stapnes, W.
 Wuensch, A. Grudiev, R. Corsini, A. Latina,
 W. Farbolini, A. Gerbershagen,
- Institut Curie: P. Poortmans, V. Favaudon,
 A. Patriarca, C. Fouillade, F. Pouzolet
- CHUV: M.C. Vozenin, P. Montay-Gruel, J. Bouris
- > IMNC: Y. Prezado, R. Delorme
- Quiron Madrid: A. Mazal



RADIOTHERAPY

What are the CHALLENGES ?

> Particle therapy

- Improved accelerator design (FFAG hybrid, linacs, dielectric wall or laser based acceleration)
- SC technology (4T)
- High-Intensity protons and ions
- Beam delivery and control (gantries)
- Combined imaging and treatment (including MRI)
- Other particles: VHEE, BNCT, He...
- Other beam delivery dose techniques: mini-beams, FLASH

> Political and Societal

- More Research/Industry collaboration
- Improved Computer Modelling, Control and Monitoring (Artificial Intelligence)











RADIOTHERAPY What are the needed R&D?

- Multidisciplinary approach, including biological info and immunological protocols -> personalised medicine
- Multi-particle facility design, SC technology (gantries), high-gradient ions accelerators
- Systematic RBE experiments, including in-vivo animal studies and clinical studies for new therapies
- Reduction of initial investment and functional costs
- Cooperation between academics, industry, research centres and hospitals













FLASH THERAP What are the underlaying mechanisms in FLASH effect? The role of the oxygen

Playing with the oxygen tension = modify ROS production

- 1 Make mice breathe 95% of oxygen (before and during IR)
- 2 Increase oxygen tension in the brain
- 3 Deliver FLASH or conventional dose-rate irradiation
- 4 Evaluate memory



Increase in O2 tension reverses the FLASH effect

Less ROS produced by FLASH-RT?

Montay-Gruel et al (in revision)

FLASH THERAPY What are the underlaying mechanisms in FLASH effect? The role of the oxygen

ROS Scavenging RT of fish eggs → Development assessment 1700 1600 Fish length (pixels) 1500 1400 1300 1200 *** 1100 1000 *** 900 1 CONV 800 100 NN Control 8 Gy CONV 8 Gy FLASH (n=18) (n=18) (n=19) FLASH → Antioxydant partially reverses the CONV effect → No effect of antioxydant on the FLASH-RT (still less armful)

Toxicity is not mediated by ROS production with FLASH-RT



Montay-Gruel et al (in revision)

FLASH THERAPY

What are the underlaying mechanisms in FLASH effect?



>> The efficiency of the chain is maximal at low dose-rate and decreases in inverse ratio to the square root of the dose-rate.

The RF gun "revisited"



Operation frequency	2998,55 MHz (30°C, in vacuum)
Charge	1 nC
Laser wavelength, pulse energy	266 nm, 100 μJ
RF Gun Q and Rs	14400, 49 MΩ/m
RF Gun accelerating gradient	80 MV/m @ 5 MW
Normalized emittance (rms)	4.4 π mm mrad
Energy spread	0.4 %
Bunch length (rms)	5 ps

new coil configurations focusing coil bucking coil

2.5 cells RF gun designed and produced at LAL for ThomX



CST-Particle in cells, simulation results





The High-Gradient linac

Parameter	Value
Length	3.5m
Number of Couplers + Cells	1+96+1
Туре	Constant gradient
Phase Advance	2π/3
Frequency	2998.55 @ 30°C
Pulse Width	Зµs
Repetition Rate	50Hz
Max. input Power	40 MW
Max. average power	5 kW
Guaranteed unloaded energy gain	>65MeV

TW S-Band structures from RI



- The Structures are SLAC-type structures
- Constant gradient
- Race track coupler for quadrupole compensation
- BIG Splitter for dipole compensation
- 2 RF loads









FUTURES PERSPECTIVES
Extending FLASH RT to others species: p, 12C, ...
The dose rate D is defined as:

$$D = \frac{N}{dS} \frac{(dE/dx)}{\rho}$$
To deposit 1 Gy, the fluency:

$$D = \frac{N}{dS} \frac{(dE/dx)}{\rho}$$
For electrons, with LET 0.2 MeV/mm :

$$1Gy = \frac{N}{dS} \frac{0.2 \, 10^6 \times 1.6 \, 10^{-19}}{10^{-6}} \Rightarrow \frac{N}{dS} \approx 3.1 \, 10^7 \, e^-/mm^2 = 5 \, 10^{-3} \, nC/mm^2$$
For protons, with LET 3 MeV/mm at the Bragg peak:

$$1Gy = \frac{N}{dS} \frac{3 \, 10^6 \times 1.6 \, 10^{-19}}{10^{-6}} \Rightarrow \frac{N}{dS} \approx 2 \, 10^6 \, p/mm^2 = 3.2 \, 10^{-4} \, nC/mm^2$$
For 1²C ions, with LET 80 MeV/mm at the Bragg peak:

$$1Gy = \frac{N}{dS} \frac{80 \, 10^6 \times 1.6 \, 10^{-19}}{10^{-6}} \Rightarrow \frac{N}{dS} \approx 8 \, 10^{4-12}C/mm^2 = 1.3 \, 10^{-5} \, nC/mm^2$$

FUTURE PERSPECTIVES Accelerators for FLASH-RT



FLASH	Dose rate	Volume	Use
FLASH e-			
Kinetron Curie 4.4 MeV	0.1-300 Gy/s	10x10 cm ²	Preclinical studies Clinical studies for superficial tumours
Oriatron CHUV 5.5 MeV	0.1-1000 Gy/s	10x10 cm ²	Preclinical studies Clinical studies for superficial tumours
Modified linac Stanford 20 MeV	0.1-250 Gy/s	10x10 cm ²	Preclinical studies
Modified linac Lund 20 MeV	0.1-250 Gy/s	10x10 cm ²	Preclinical studies
FLASH p			
RARAF 4,5 MeV	0.05-1000 Gy/s	Round 11 mm	Biological studies
CPO-Orsay 130-198 MeV	40 Gy/s	12x12 mm²	Preclinical studies
FLASH ¹² C ????			
RAON 310 MeV/u	0.03-33.3 Gy/s	20x20 cm ²	Under study