



RI beam projects in NIRS

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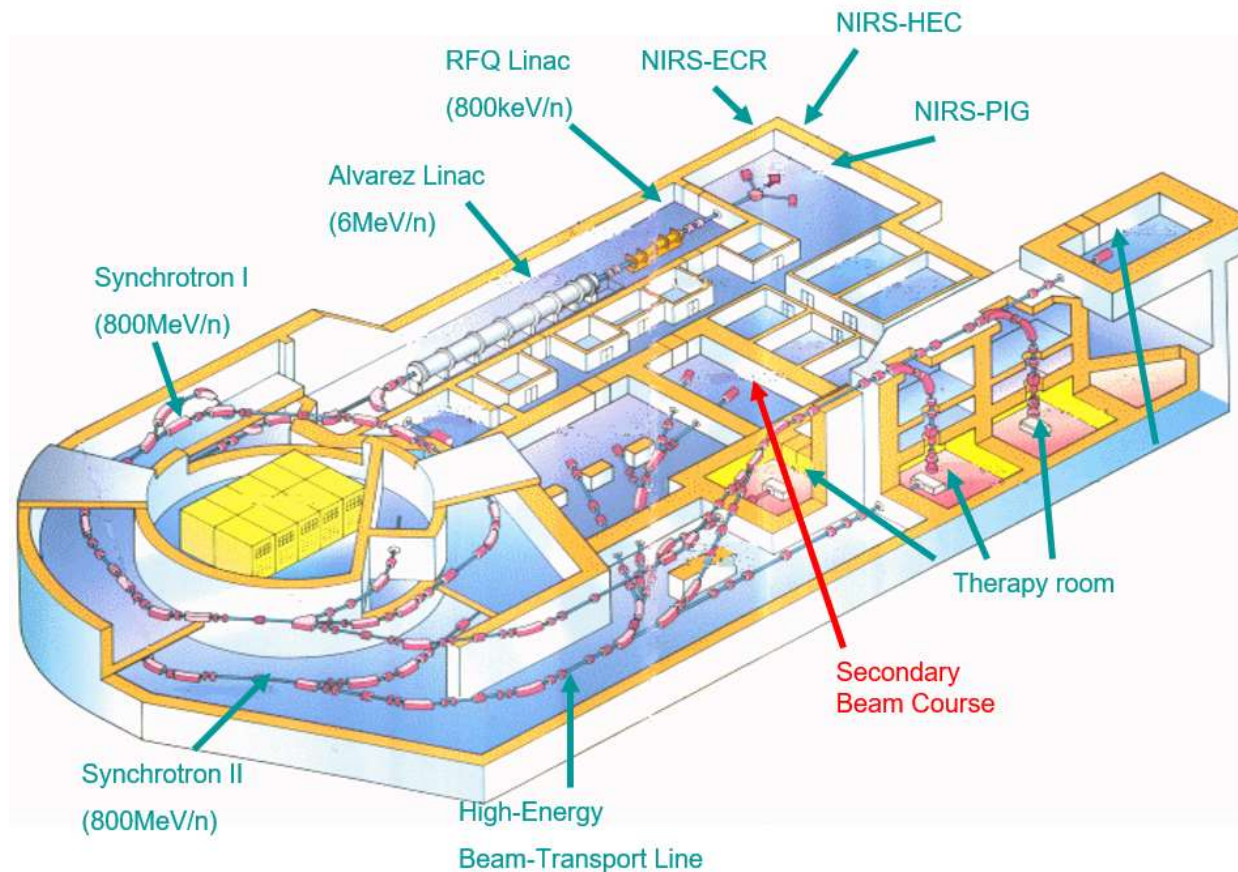
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- Secondary beam project
 - Projectile fragmentation
 - Spot scanning irradiation
 - Positron camera for range verification

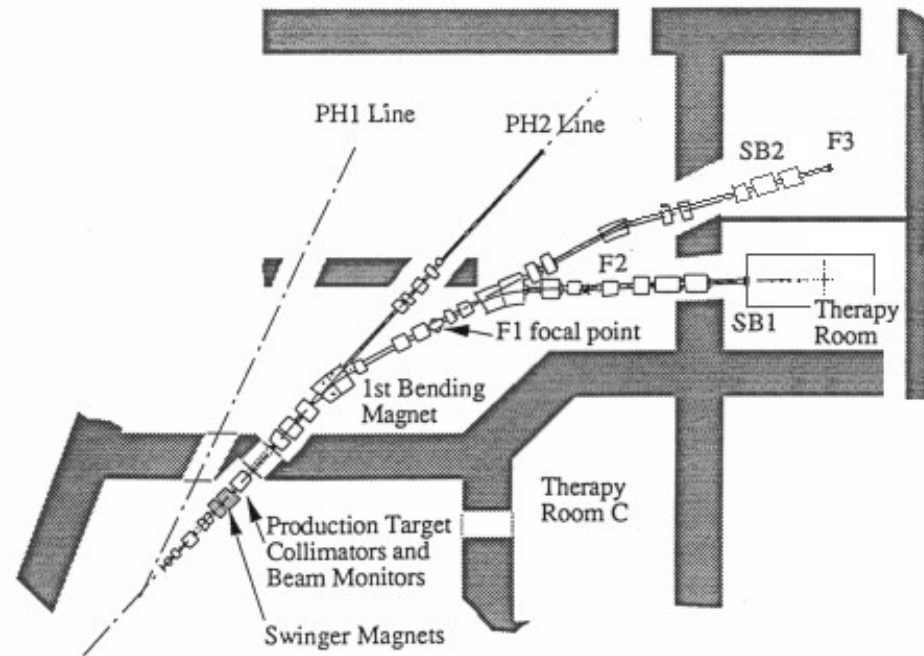
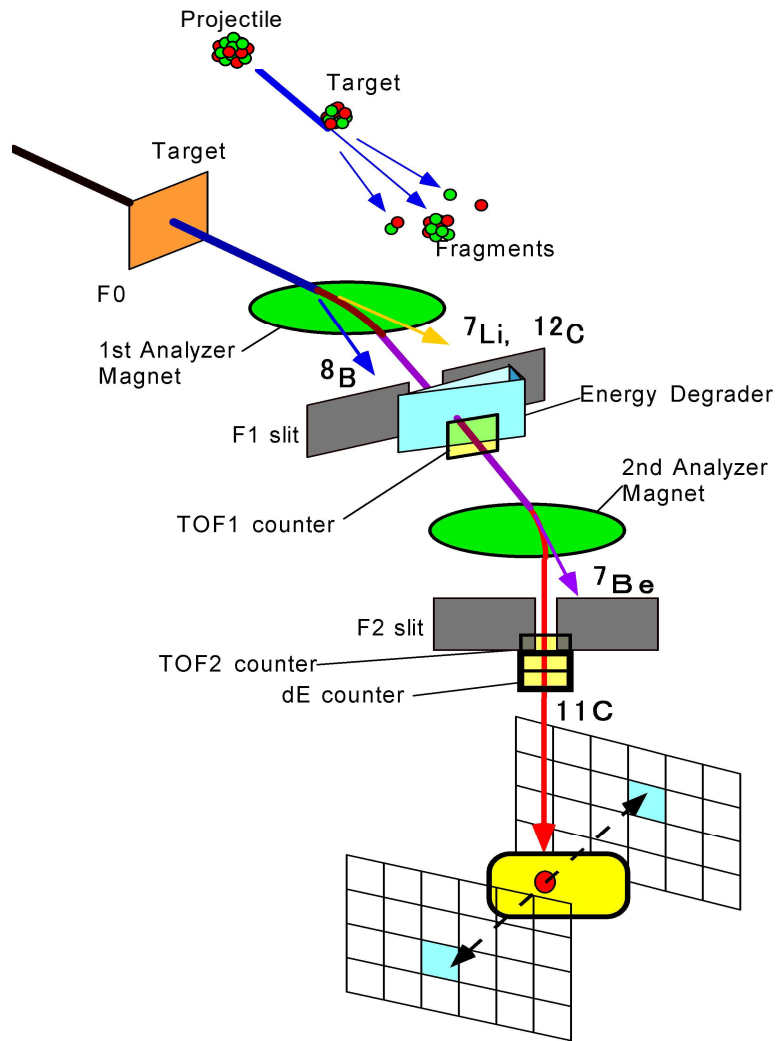
- ISOL research
 - RI generation
 - RI beam acceleration

- Detector development
 - Open PET

- 1995 ~ 1997 Secondary beam line construction
- 1998 ~ 1999 Irradiation room preparation
- 2000 ~ 2002 Beam test using positron camera
- 2002 ~ 2003 Washout measurements of RI in the rabbit



- Radioactive nuclear beam (RNB) course
 - Projectile fragmentation of relativistic high energy beam is used to produce various radioactive nuclei.
 - Secondary beam is directly used for the irradiation of cancer treatment.
- Beam irradiation system
 - In order to obtain a desired 3D shape, the spot scanning method is utilized.
- Detectors for the measurement of radioactive nuclei
 - Commercial PET system is available for the ^{11}C beam.
 - Positron camera is developed in order to obtain the 1D range information.



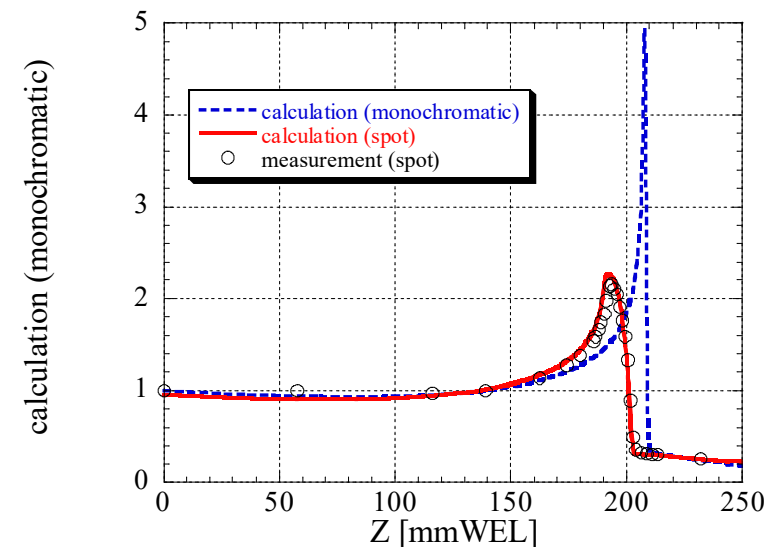
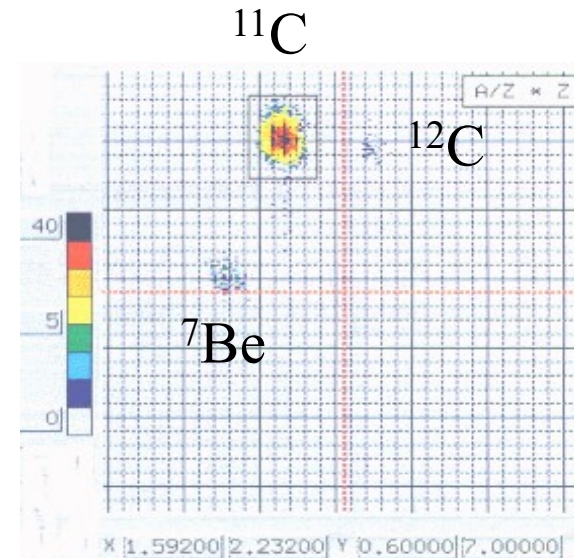
- Maximum magnetic rigidity 8.13Tm
- Radius of bending magnet 5m
- Maximum beam energy (for ^{20}Ne) 600MeV/n
- Momentum acceptance 5%(FW)
- Angular acceptance (h, v) 26mrad(FW)
- Momentum dispersion at F1 2.0m

Typical parameters

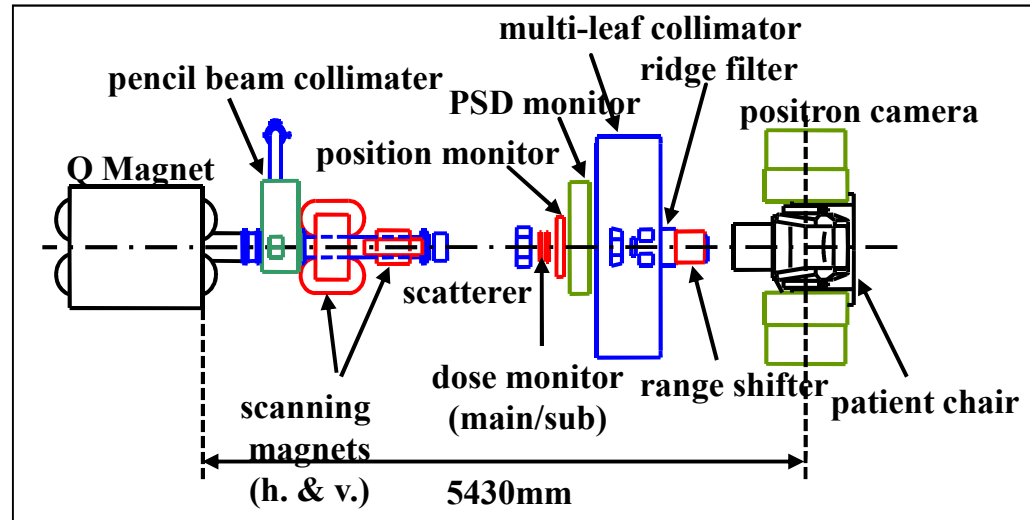
Energy of primary ^{12}C	430MeV/n
Thickness of Be target	51mm
Thickness of Al degrader	none
Rigidity window	2.0% (FW)
Angular window H.&V.	26mrad (FW)

Results

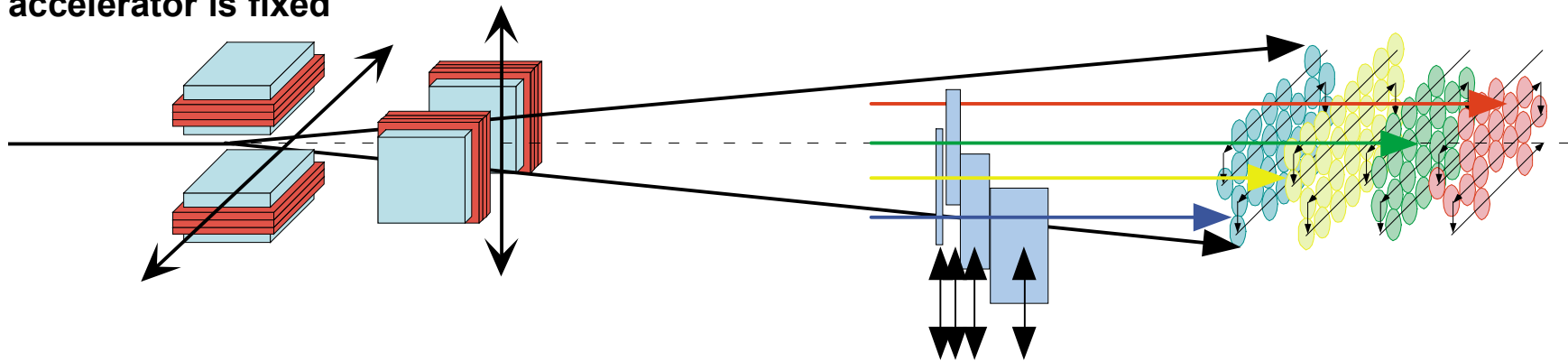
Energy of secondary ^{11}C	355MeV/n
Range in water	21cm
Production rate	0.4%
Purity	93%
Momentum spread	3.5% (FWHM)
Beam size at F2	4mm (FWHM)
Beam size at patient	9mm (FWHM)



Maximum scanning volume
 10 x 10 x 18 cm (WE)
 Scanning speed (x, y)
 2 ms/cm

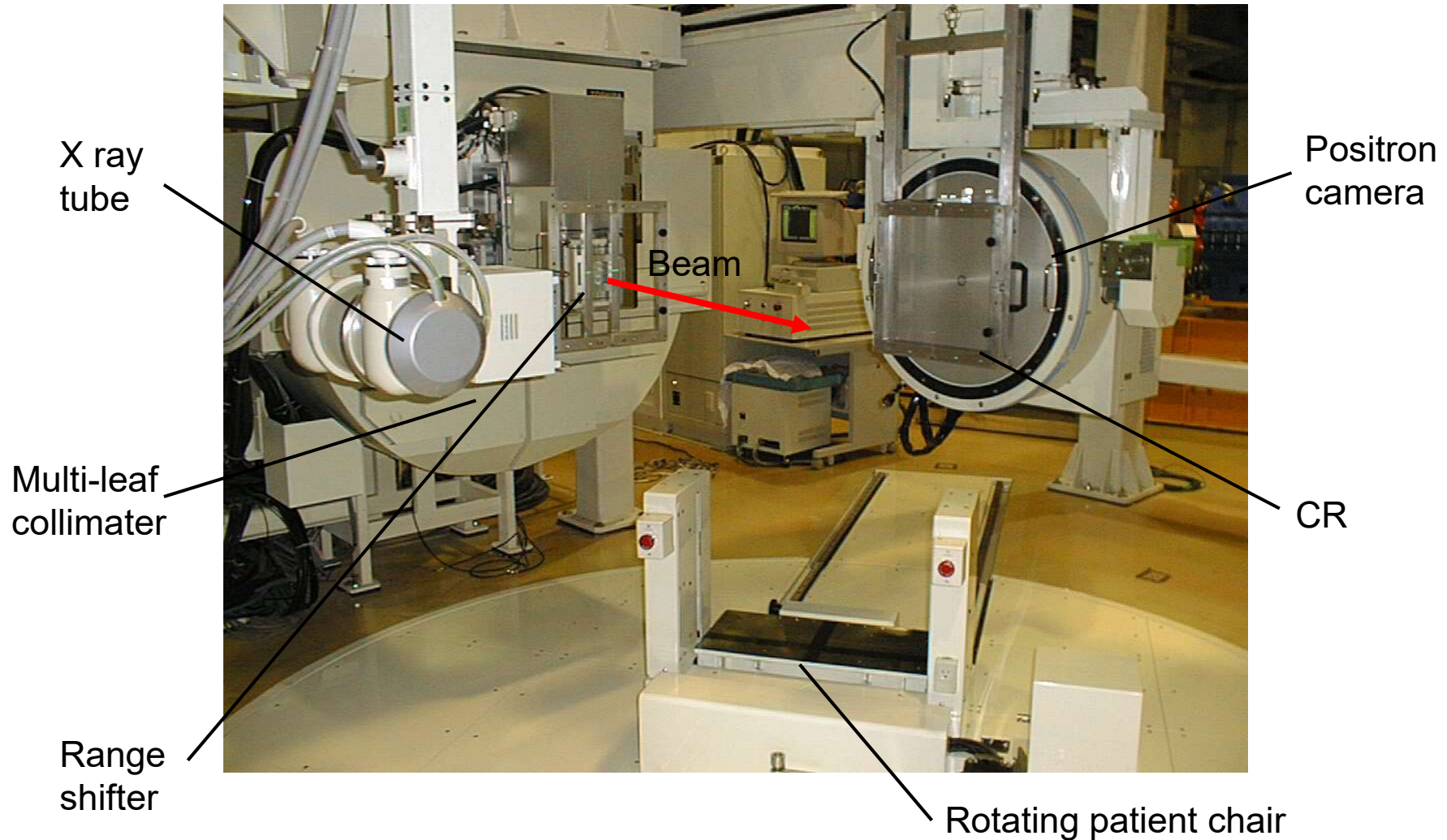


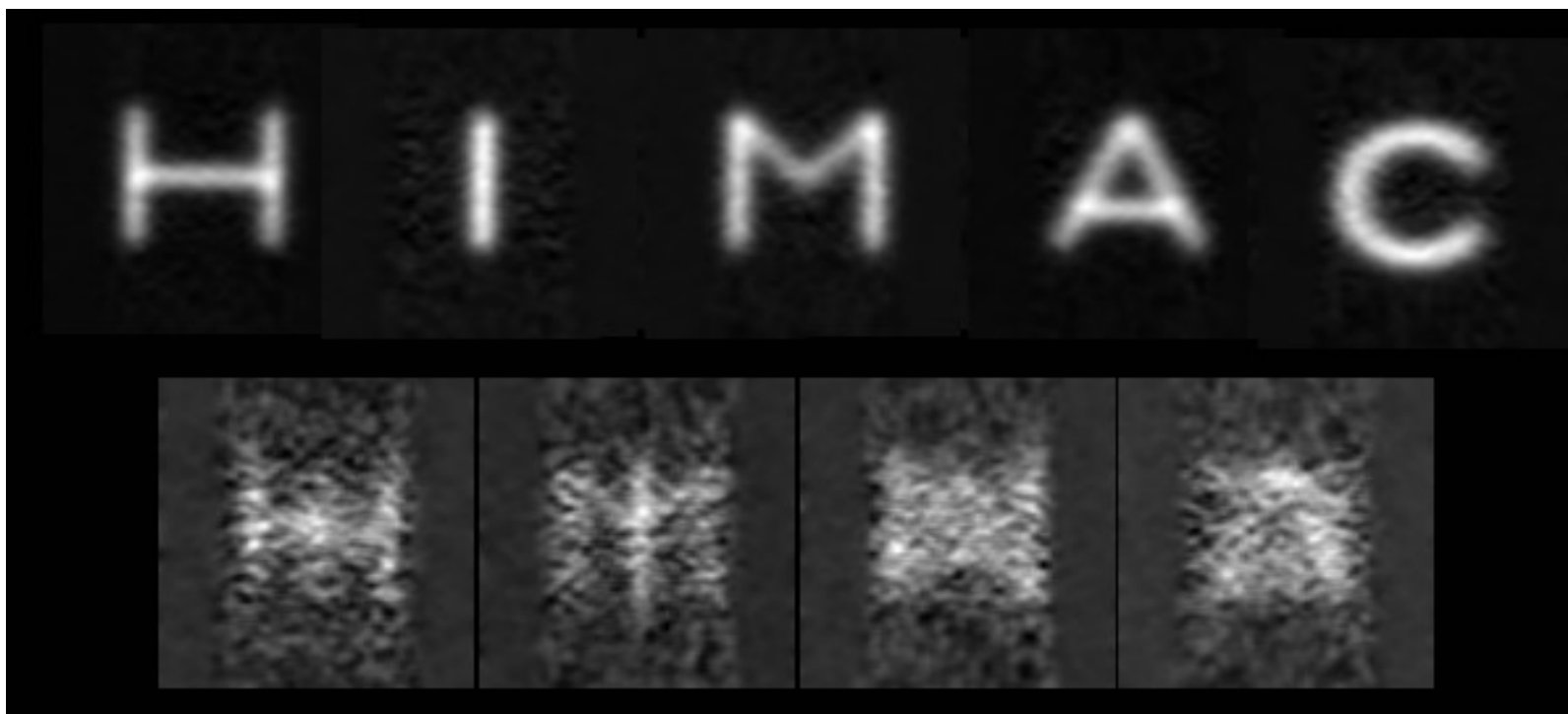
Beam energy from the accelerator is fixed



Position scanning in a slice
 by the scanning magnets

Range scanning
 by the range shifter

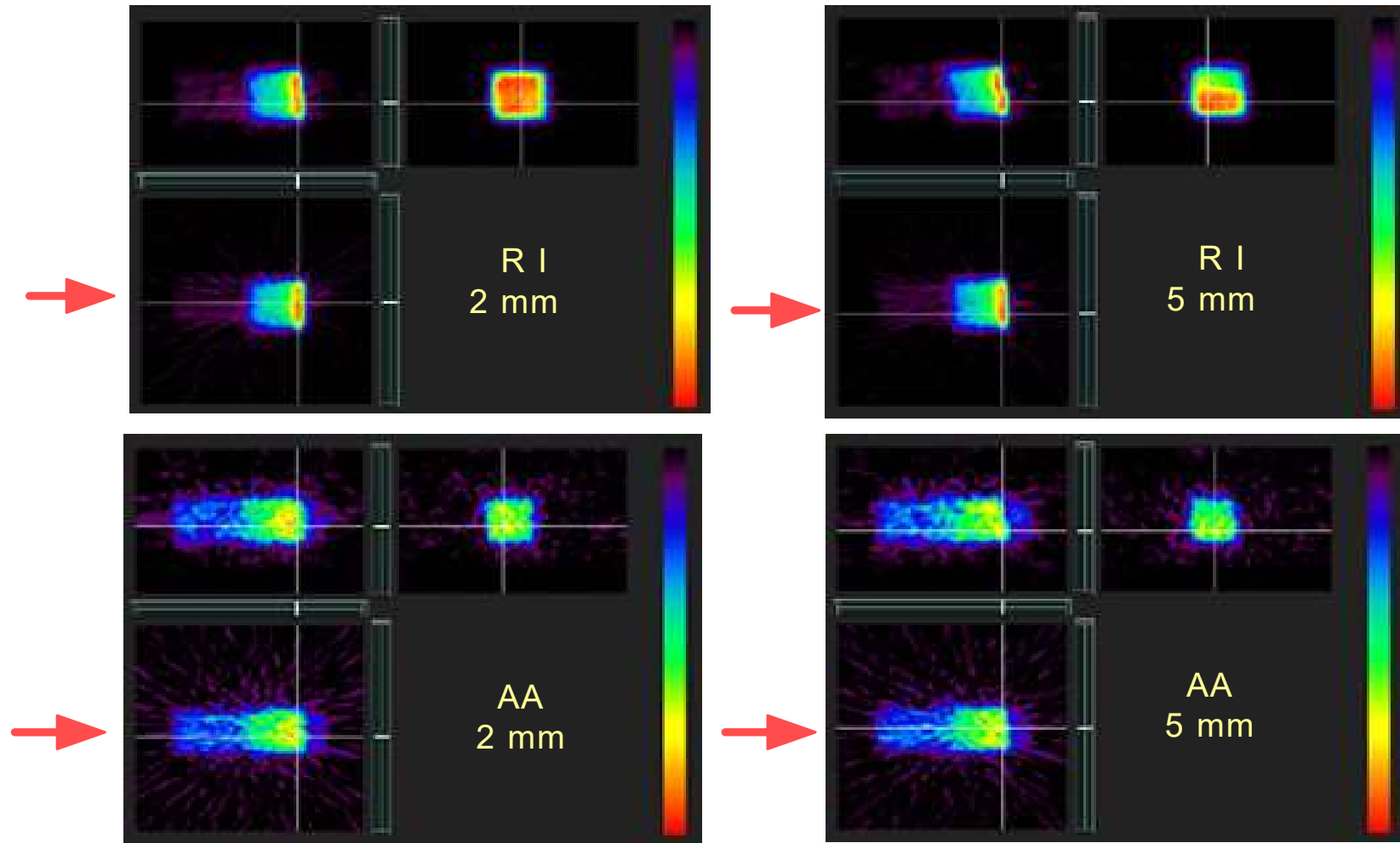




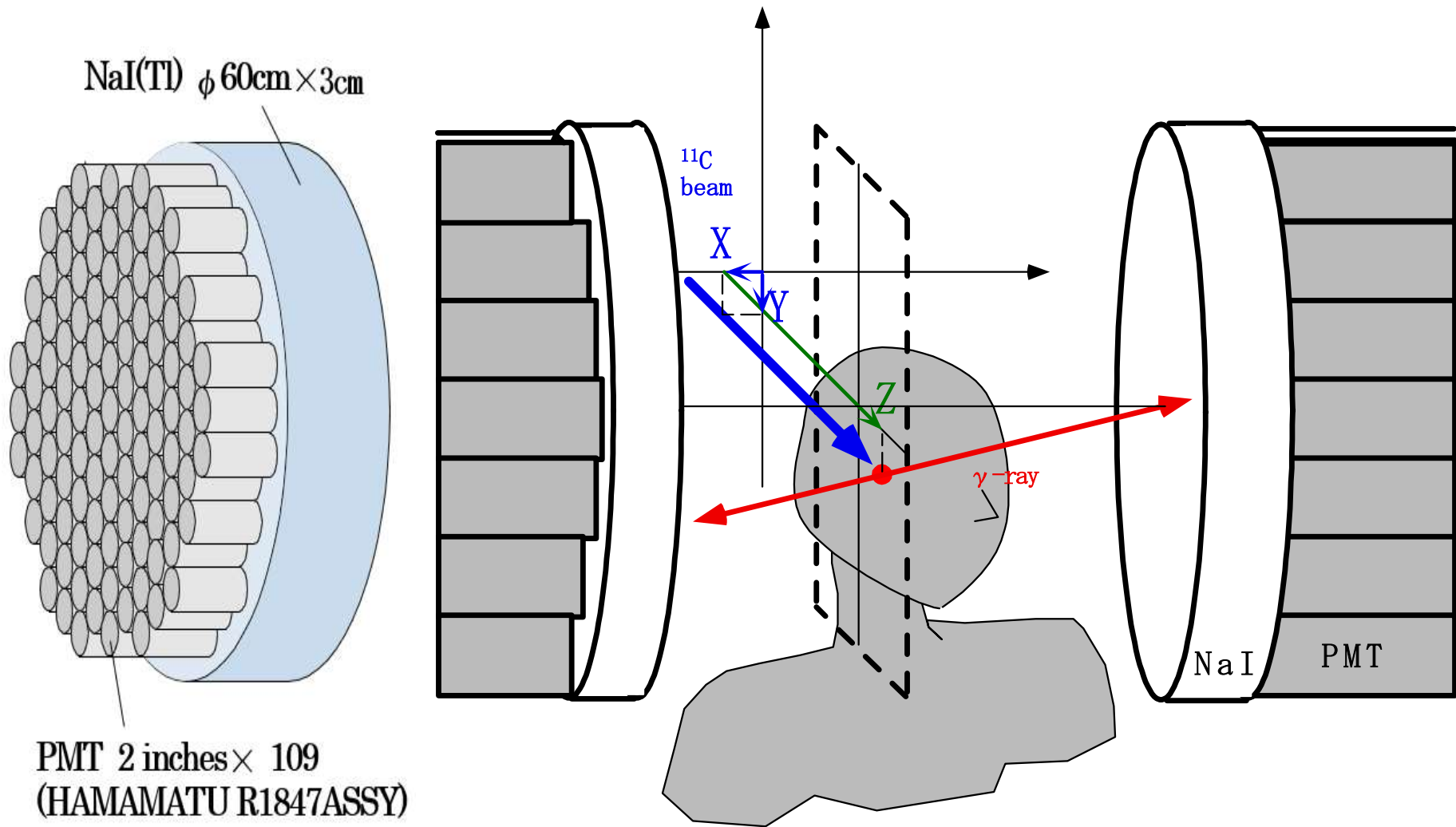
Pattern Test

63x63 mm, 20 mm apart,
3 mm step

- Positron Emission Tomography (PET)
 - For the check of the irradiation volume after the treatment, a 3D image can be observed by a commercial PET system.
 - ^{11}C beam is used for the treatment instead of ^{12}C beam.
- Positron Camera
 - In order to determine a precise beam range, a pilot pencil beam and positron camera are used.
 - A pilot pencil ^{11}C beam with a few dose is necessary.
 - By using more short-lived ^{10}C (half life is 19s) beam, the range can be measured on line without any biological effects.

Comparison of ^{11}C Beam (RI) and Autoactivation (AA)

Irradiation Dose: 1 Gy, Irradiation Field: 35x35x50 mm WE



C-11 beam irradiation (3,500k particles)

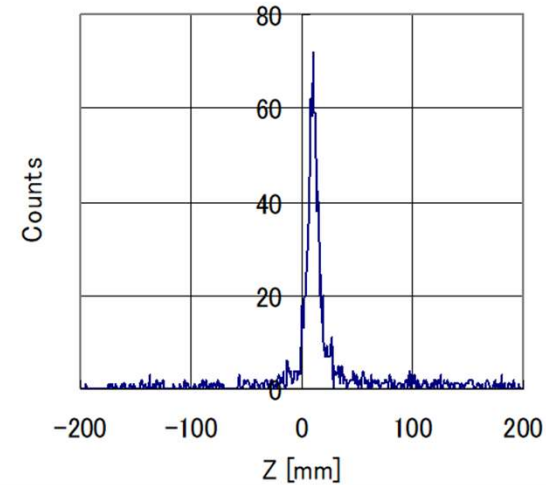


Measurement time 100s

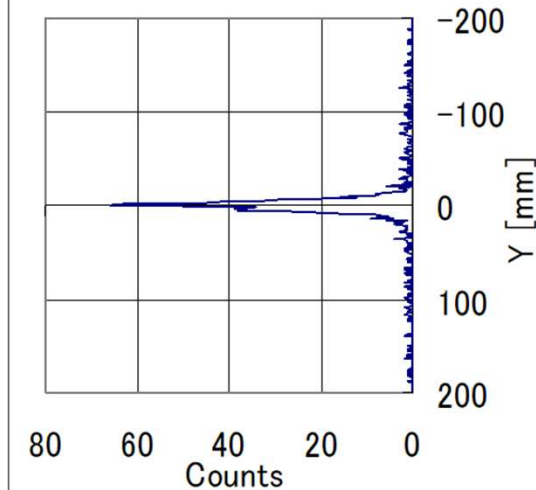


$\sigma_z \sim 5.7$ mm (gauss fitting)

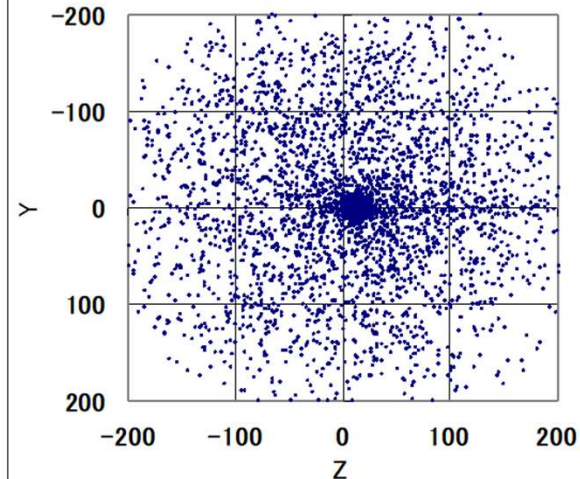
Activity distribution (beam axis)



Activity distribution (vertical axis)



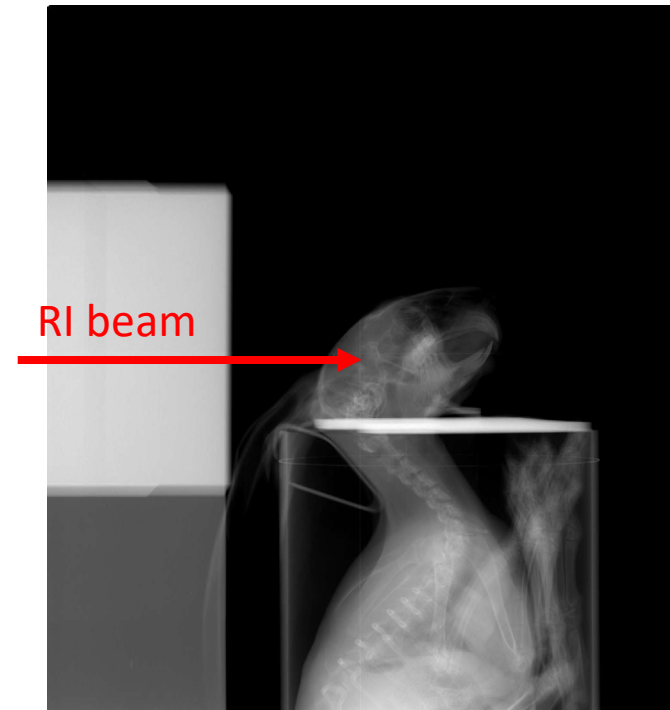
2D activity distribution



Beam

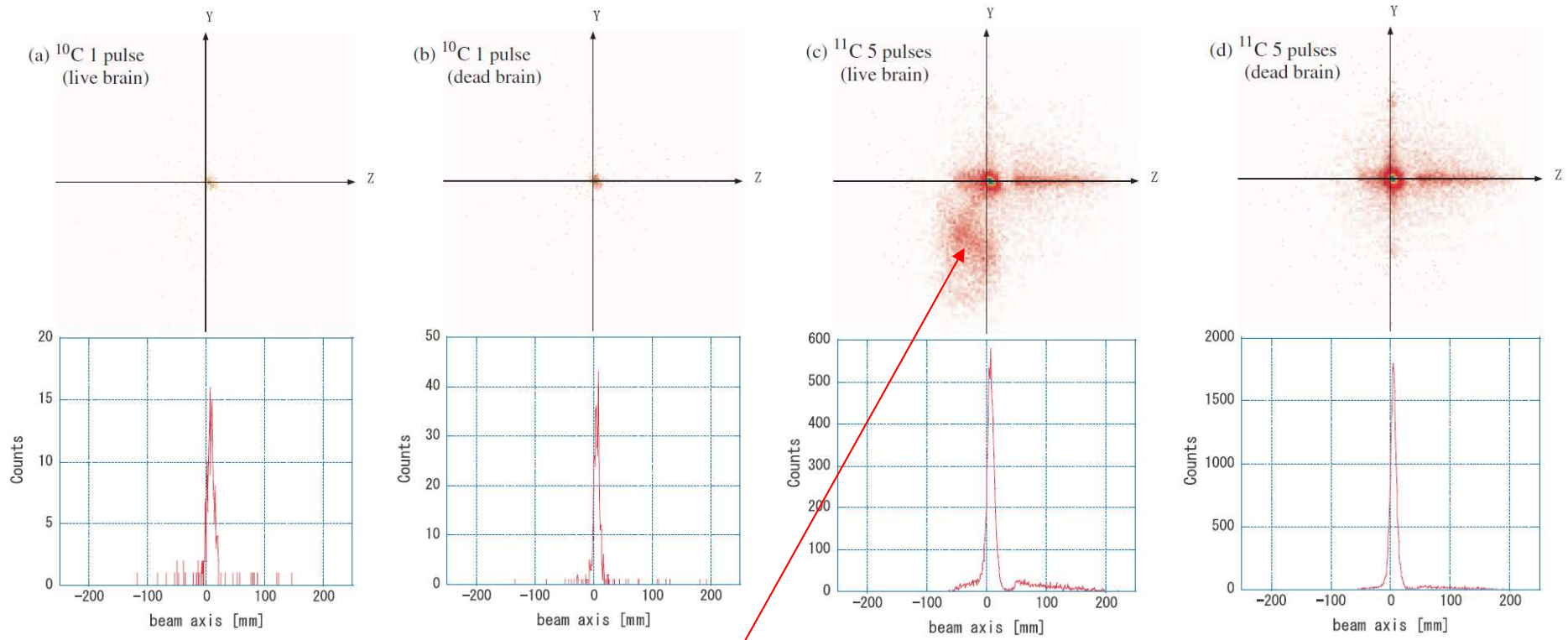


To study the washout effect, rabbit was irradiated by C-10 and C-11 beams.

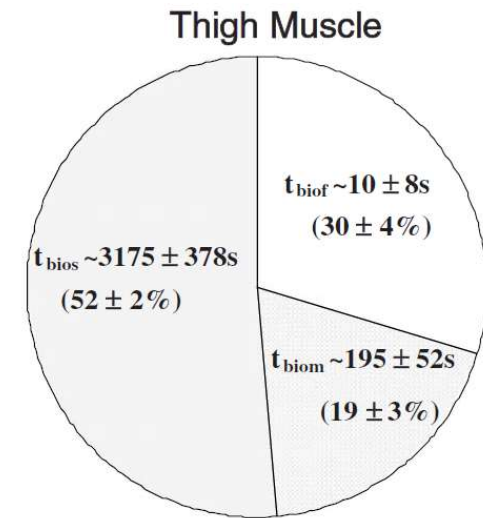
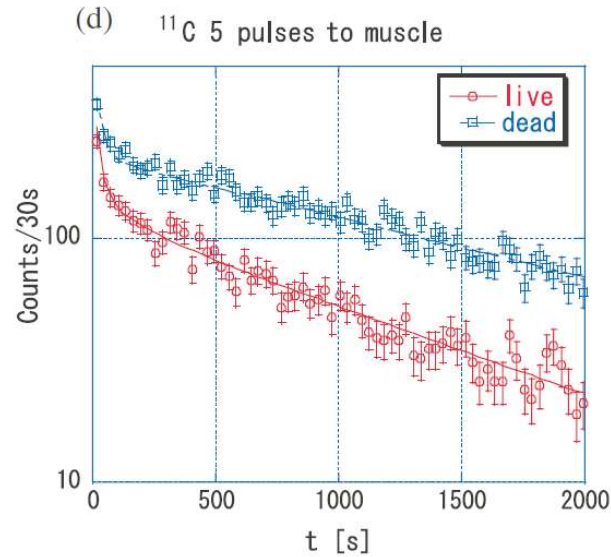
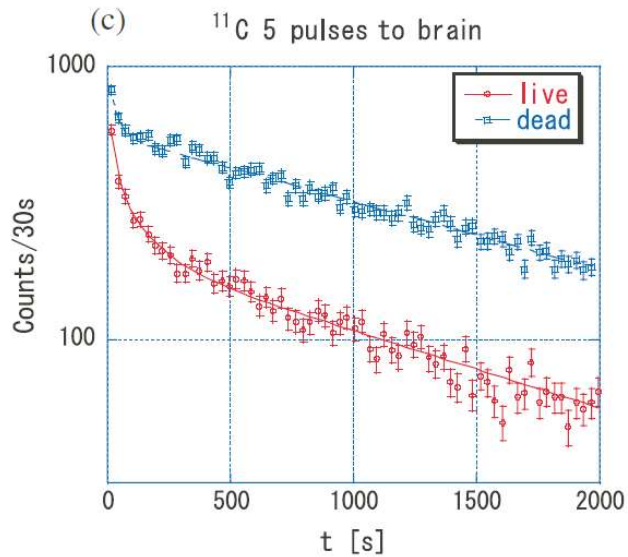
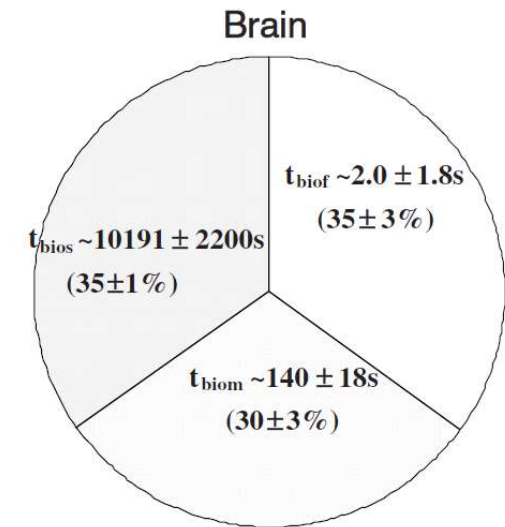
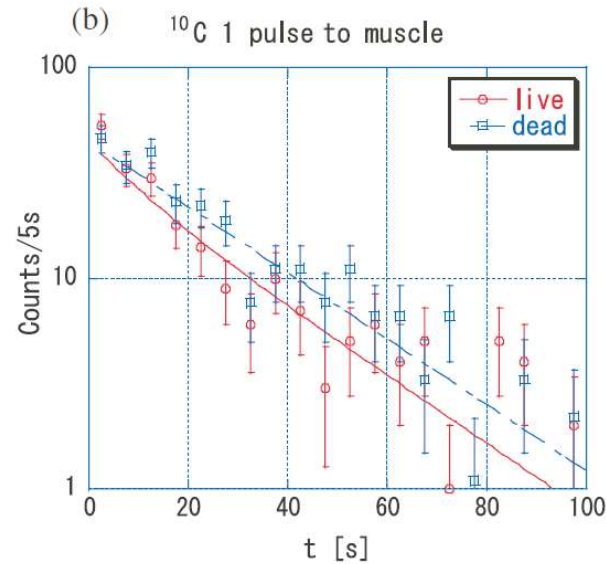
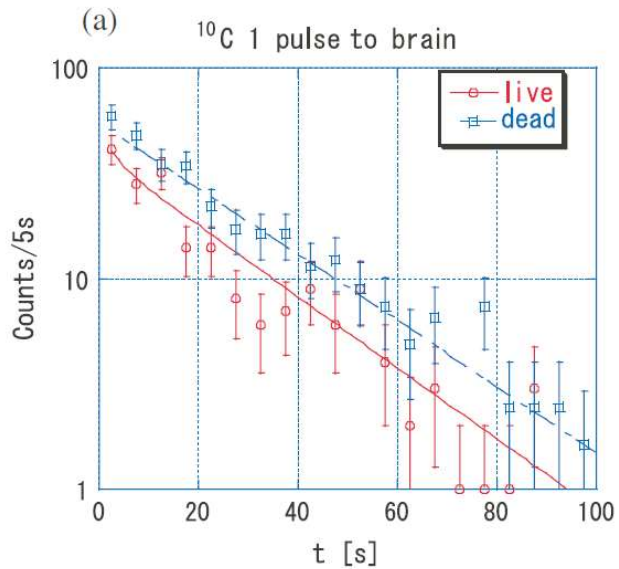


Brain and thigh muscle were selected as targets.

One- and Two-dimensional position distribution of brain irradiation.
(Beam comes from right side.)



Washout effect was clearly seen for C-11 irradiation to live brain.

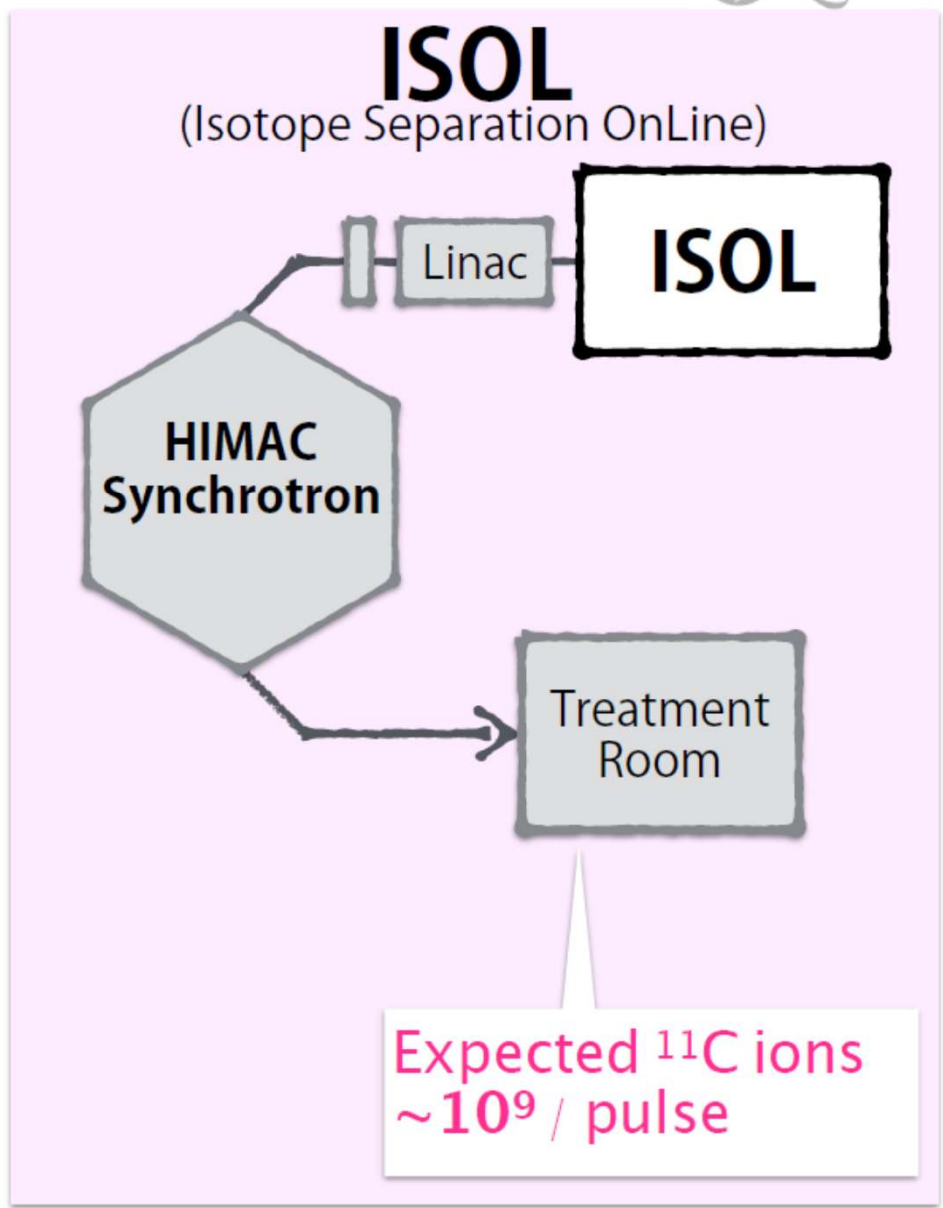
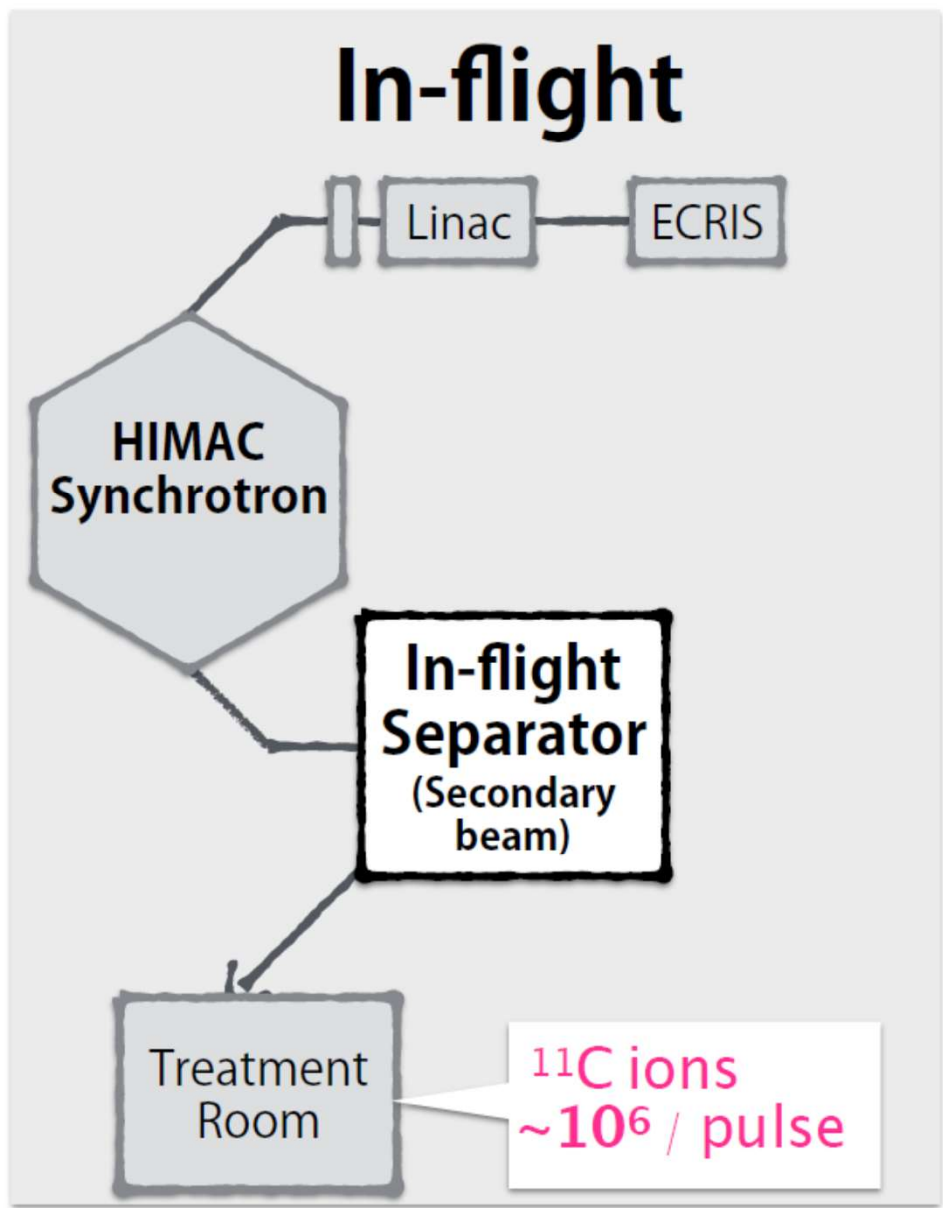


3 components were exist for the wash out effect.

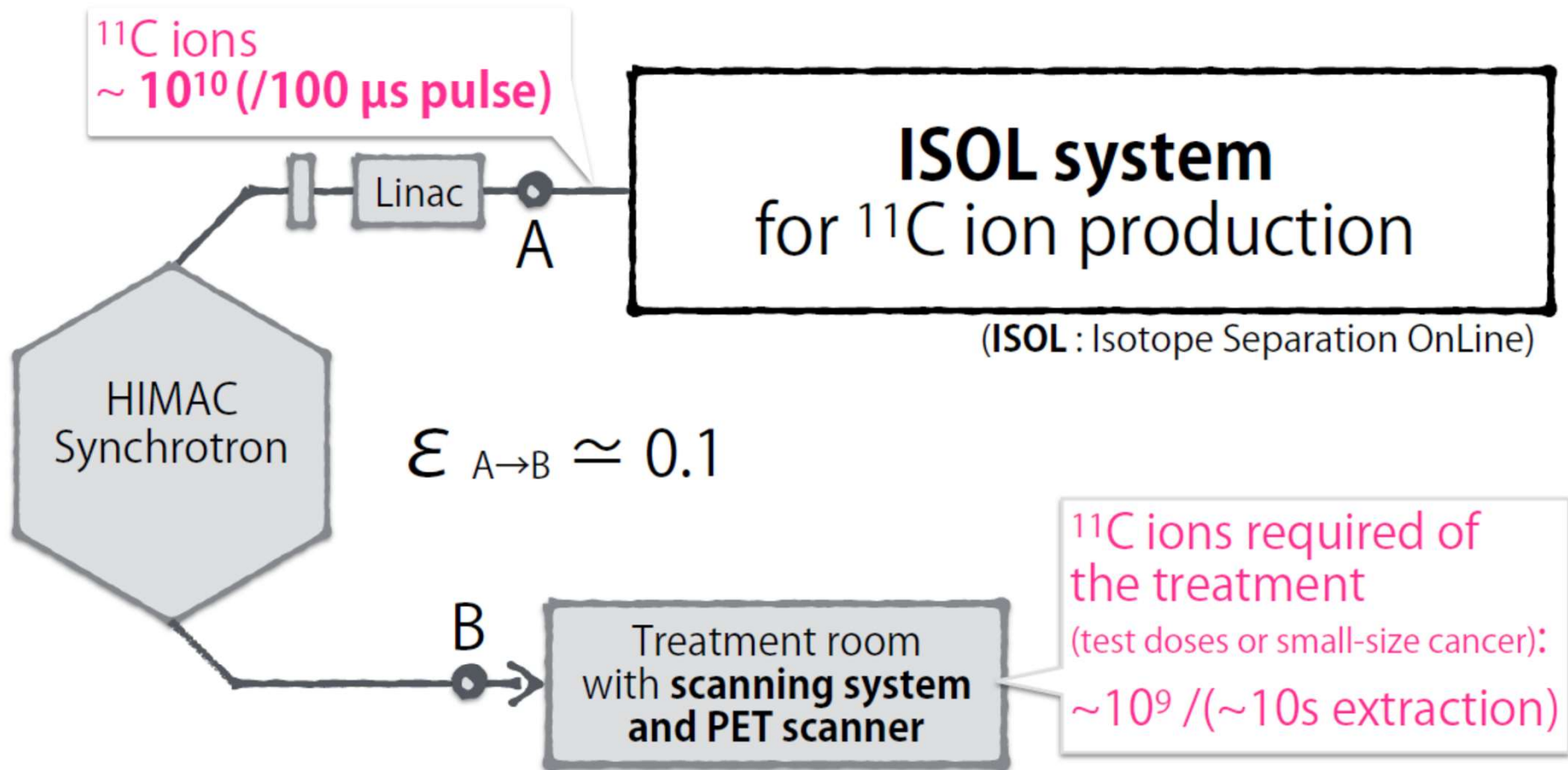
To apply these techniques to real clinical situation,

- washout effect should be studied more in detail.
- the intensity of RI beam (^{10}C and ^{11}C) should be increased.

ISOL technique for further amount of ^{11}C



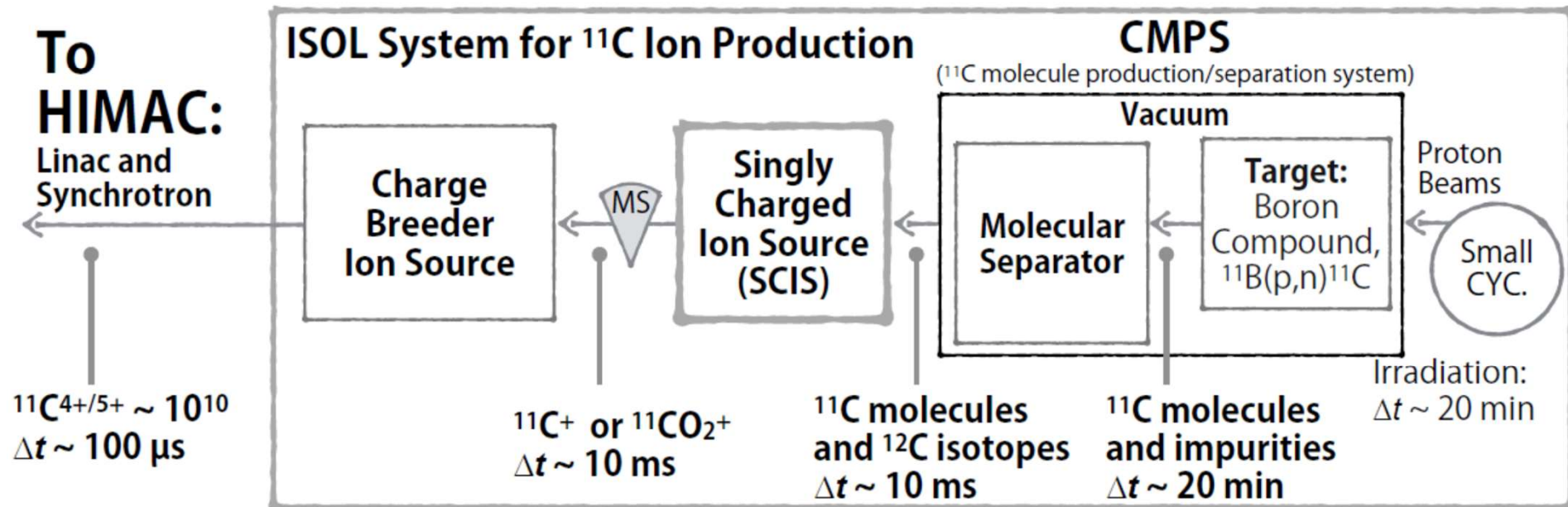
Purpose: development of an ISOL system for ^{11}C ion acceleration



Conditions required of the ISOL system:

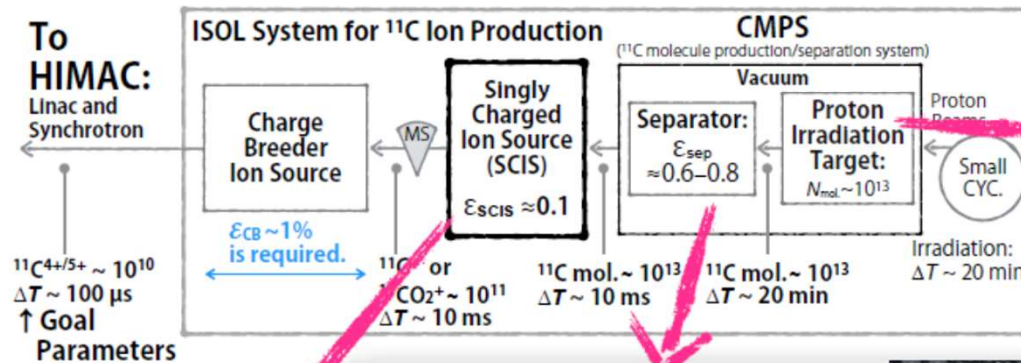
^{11}C ions $\sim 10^{10}$, $\Delta T \sim 100 \mu\text{s}$

ISOL system for ^{11}C ion production



- providing **one pulse every 20 min**; production and accumulation of ^{11}C molecules with a commercially available cyclotron ($\sim 20 \mu\text{A}$).
- pulse compression required of the injection into synchrotron;
20 min \rightarrow 100 μs
- **EBIS** (Electron-Beam Ion Source)-charge breeder enables **highly efficient use of ^{11}C** by trapping ions. *cf.* cw-ECRIS

Each module that has been developed so far has good performances: **target, separator and SCIS**



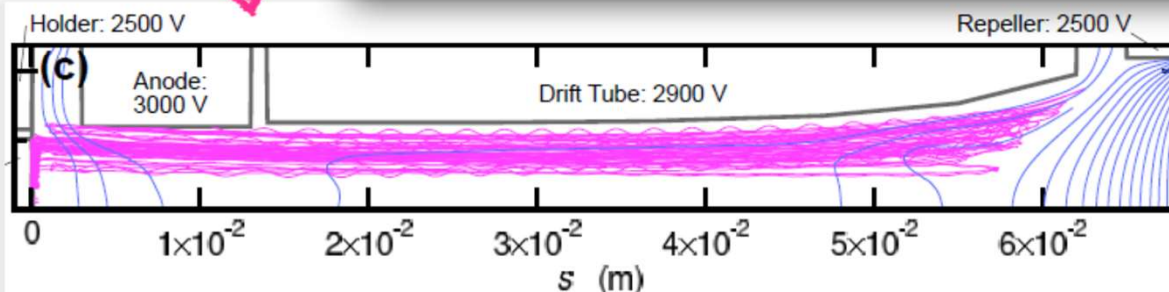
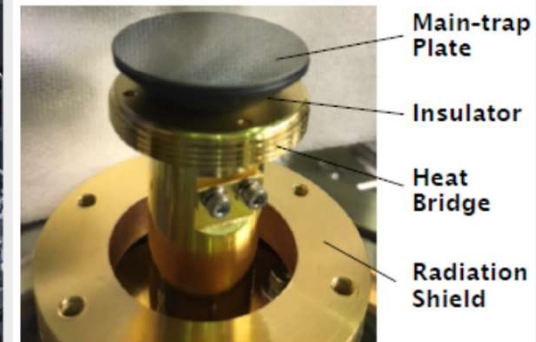
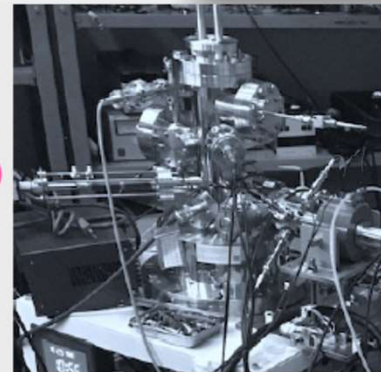
Target	Beam current \times Irradiation time (μC)	Produced ^{11}C mol.	Residual in target (%)	Corrected ^{11}C mol. (%)	No. of corrected ^{11}C mol.
$\text{NaBH}_4^{[3]}$	1.94×10^4 (18 μA , 18 min)	$^{11}\text{CH}_4$	70.4%	29.3%	5.0×10^{12}
B_2O_3	1.92×10^4 (16 μA , 20 min)	$^{11}\text{CO}_2$	21.2%	76.4%	1.4×10^{13}

Target: $N \sim 10^{13}$

K. Katagiri et al., Rev. Sci. Instrum. 85, 02C305 (2014).

Separator:
 $\epsilon \approx 60-80\%$

K. Katagiri et al., Rev. Sci. Instrum. 86, 123303 (2015).



SCIS: $\epsilon \approx 10\%$

K. Katagiri et al., Rev. Sci. Instrum. 89, 113302 (2018).

K. Katagiri et al., Rev. Sci. Instrum. "Ion-production efficiency of a singly charged ion source using low energy electron beam", to be submitted.



OpenPET : PET-guided particle therapy

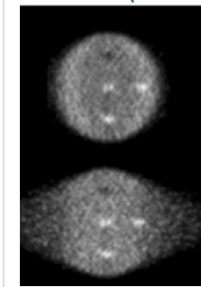
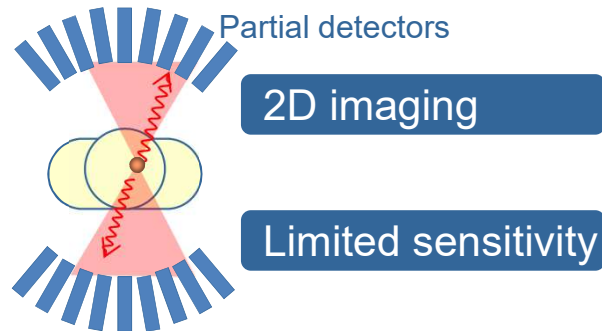
“OpenPET”

our idea for 3D in-beam PET

Conventional in-beam PET



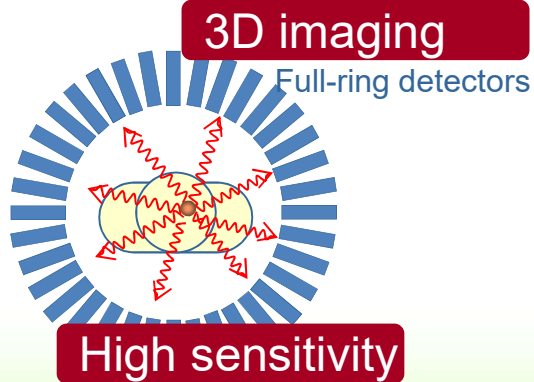
GSI
Pawelke et al, 1996



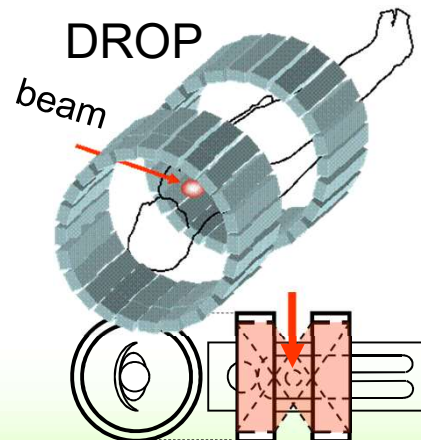
TOF
200ps

Non-TOF

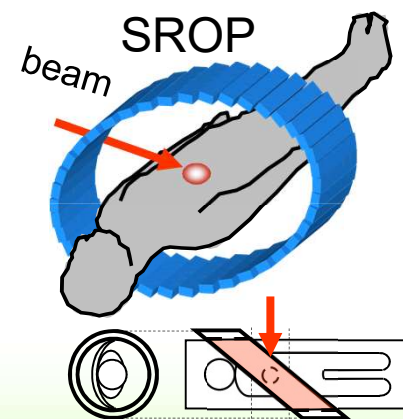
OpenPET

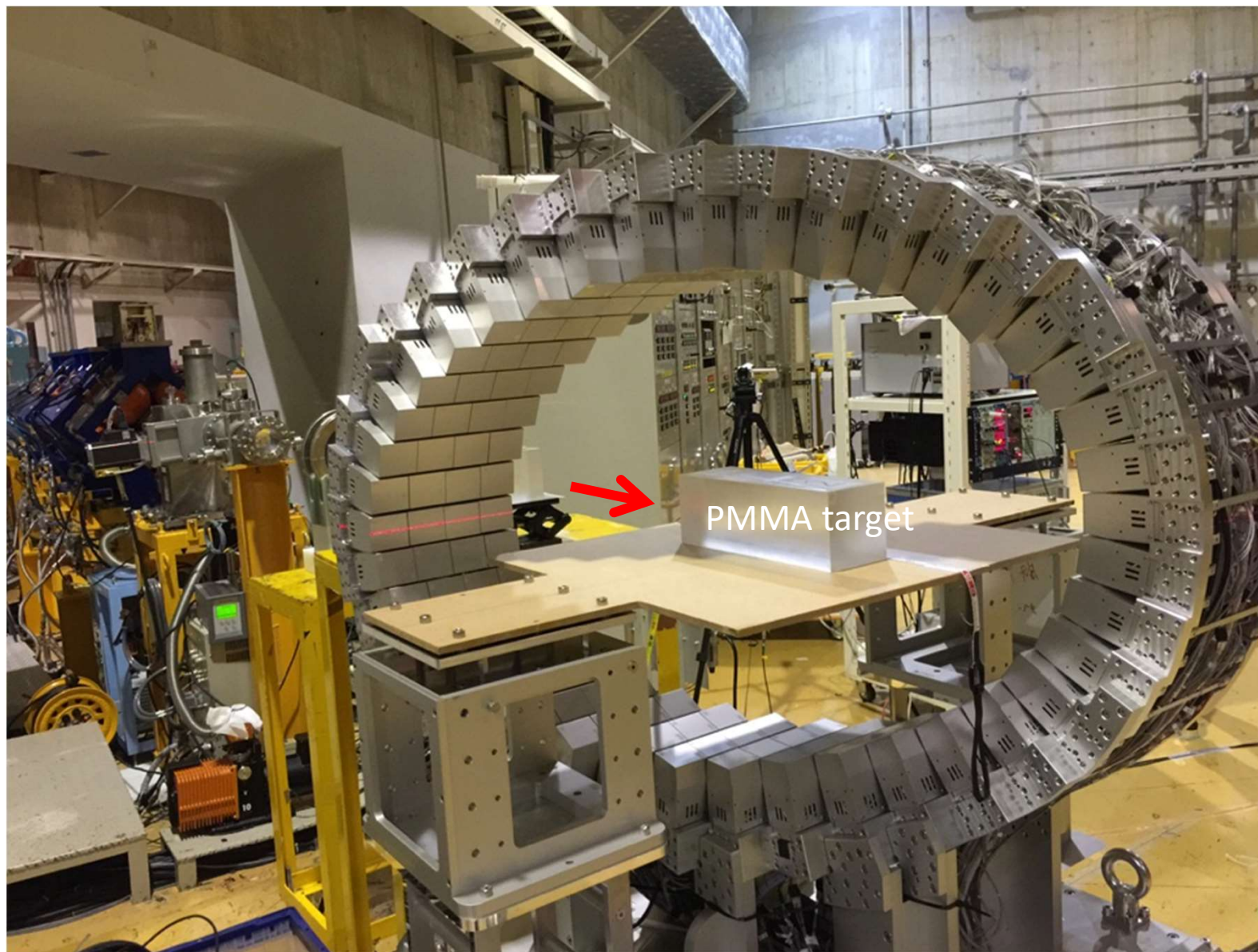


Yamaya PMB 2008



Tashima PMB 2012



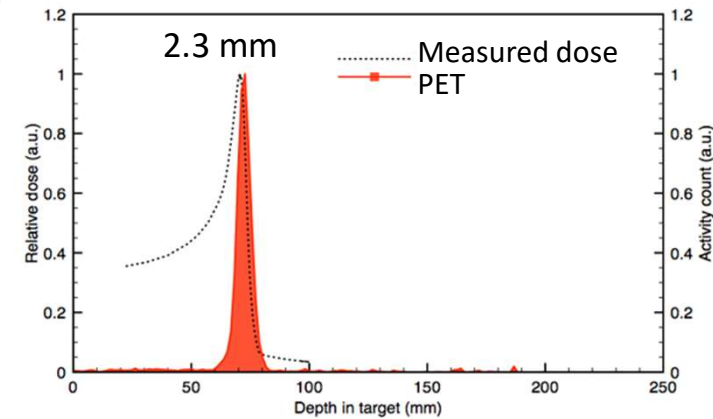
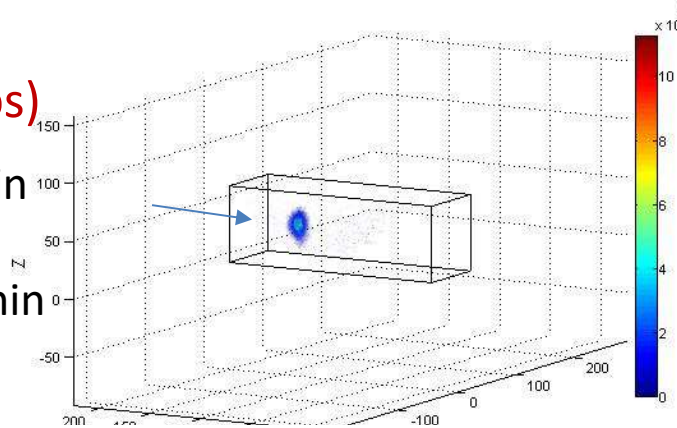


Spill off + beam off
 OSEM
 1.5 mm³ voxel

Akram Mohammadi, et al., NIMA 2017 p76

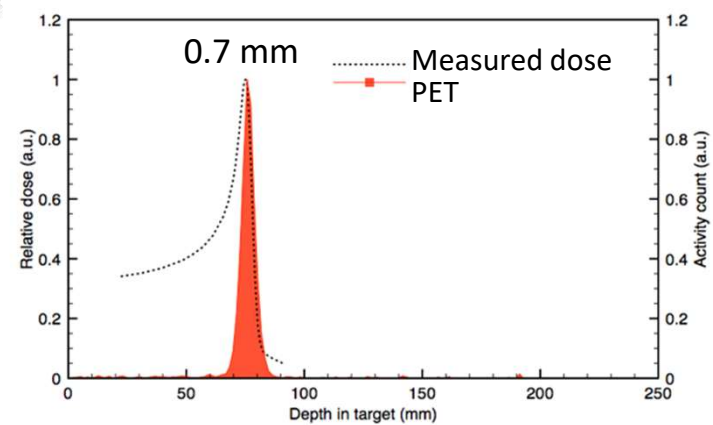
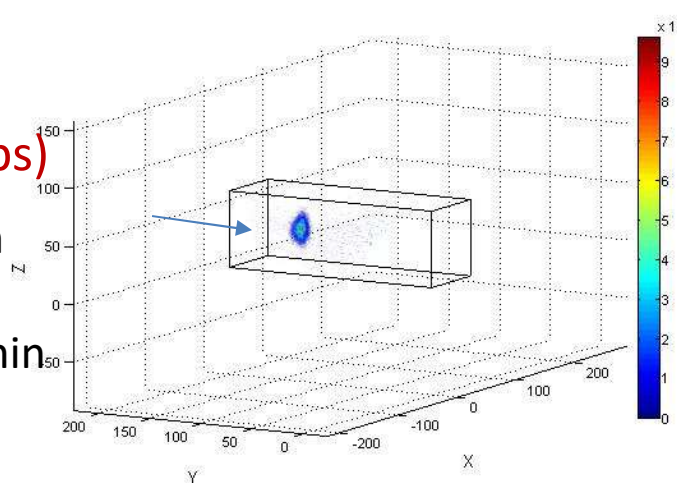
¹¹C (6x10⁶ pps)

- Half life: ~20 min
- 3 spills
- Scan time: 23 min



¹⁵O (7x10⁶ pps)

- Half life: ~2 min
- 2 spills
- Scan time: 13 min



- By secondary beam project, the beam course was developed and studies on biological washout effects were performed.
- To overcome the low intensity RI beam, ISOL research is ongoing.
- OpenPET was developed for efficient use of the limited signal from RI.

Thank you for your attention

