

European Commission

juas  
Joint Universities Accelerator School

**LOW-ENERGY ELECTRON ACCELERATORS**

**Applications in medicine and industry**

**Wim Mondelaers**

Unit Standards for Nuclear Safety, Security and Safeguards  
Directorate Nuclear Safety and Security

**Joint Research Centre**  
the European Commission's in-house science service

ec.europa.eu/jrc

Joint Research Centre

<u>APPLICATION</u>		
<b>Accelerators in the world *</b>  <b>year 2007</b>  <b>(approximate numbers)</b>	High-energy physics research	120
	Synchrotron radiation sources	50
	Ion beam analysis	200
	<b>Photon or electron therapy</b>	<b>9100</b>
	Hadron therapy	30
	Radioisotope production	550
	Ion implantation	9500
	Neutrons for industry or security	1000
	<b>Radiation processing</b>	<b>2000</b>
	<b>Electron cutting and welding</b>	<b>4500</b>
	<b>Non-destructive testing</b>	<b>650</b>
		<b>TOTAL</b>

\* R. Hamm  
at 9th ICFA Seminar  
October 30, 2008

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**~ 60% low-energy electron accelerators**

### Low-energy electron machines

X-rays

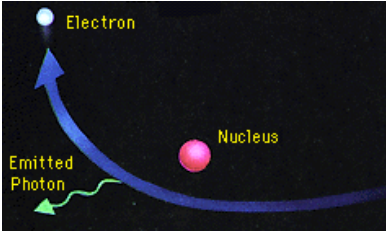
electrons

1. Basic principles of X-ray production
  - *bremsstrahlung*
  - *synchrotron radiation*
2. Physical, chemical and biological aspects of the application of electrons and bremsstrahlung photons
3. Electron accelerators in medicine
4. Electron accelerators in industry
5. Electron storage rings for medicine and industry

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### Radiation of electrons in a transverse field

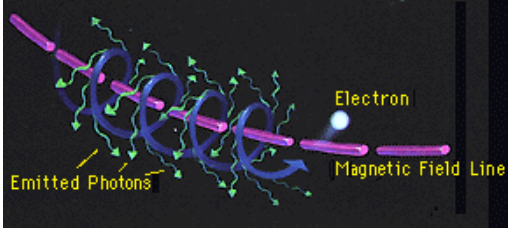
Coulomb field of atomic nuclei



**BREMSSTRAHLUNG**

*braking radiation*

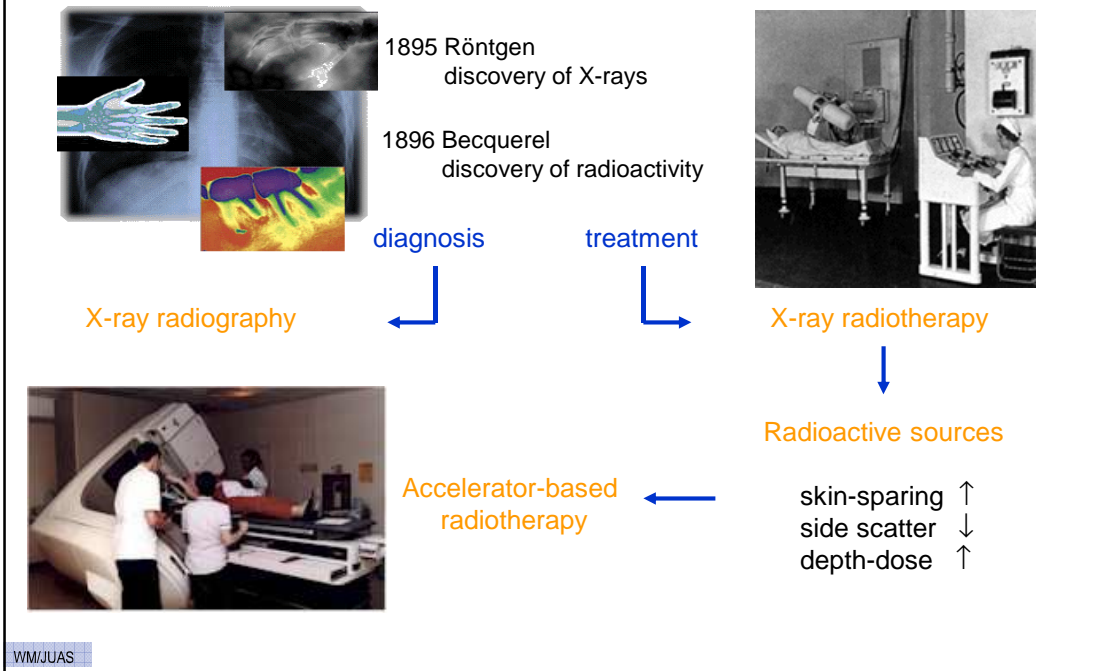
Magnetic field



**SYNCHROTRON RADIATION**

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### Low-energy electron accelerators in medicine



### Accelerator-based radiotherapy

- 1937 first hospital-based VAN DE GRAAFF
- 1946 first hospital-based BETATRON + WILSON:  
use of protons and ions
- 1952 first hospital-based RF LINAC
- 1990 first hospital-based PROTON SYNCHROTRON

Now electrons and photons: routine therapy  
 ↓  
 conformal therapy  
 protons and ions: unconventional

## Low-energy electron accelerators in industry



- 1905 APPLEBY and MILLER, patent:  
*'use of X-rays to bring about an improvement in the conditions of foodstuffs'*
- 1956 JOHNSON and JOHNSON  
*sterilisation of medical devices*

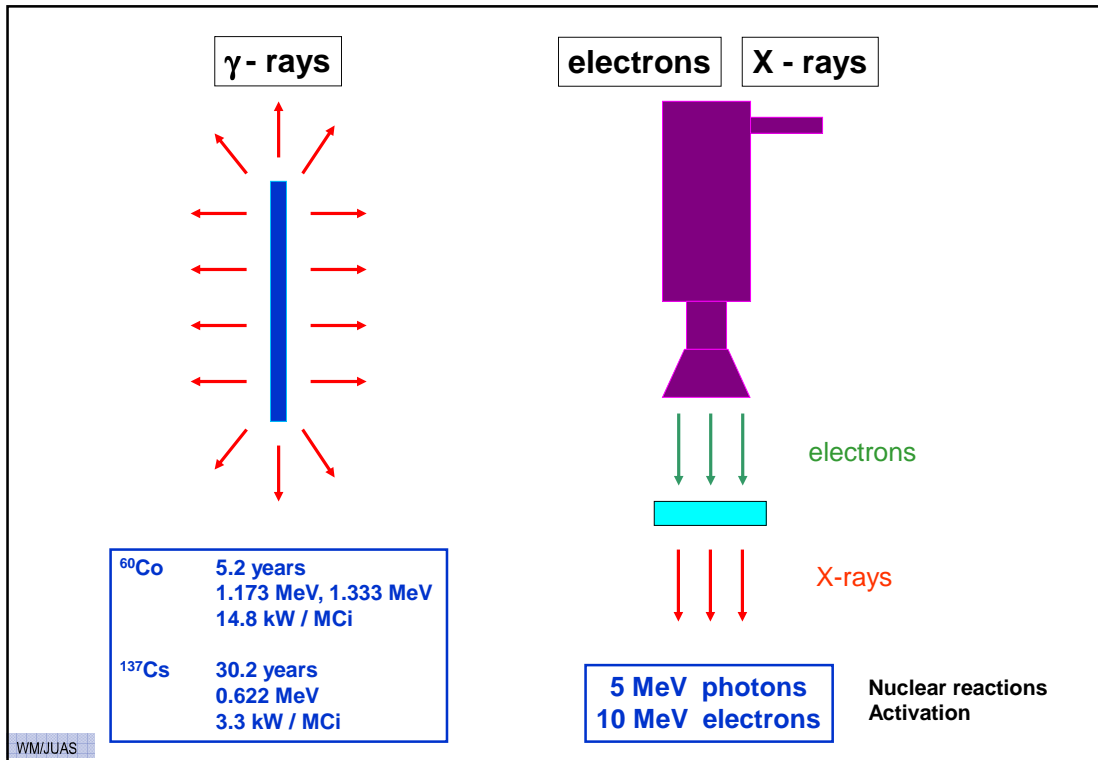
### INDUSTRY

in a car:  
in an airplane:  
at the doctor:  
in the supermarket:  
in the clothing shop:  
at home:  
in the human body:

### radiation processing

dashboard, tyres, cables, painting ...  
constructional components ...  
syringes, pharmaceuticals, sterile dressings ....  
strawberries, red meat, shrink packaging materials ...  
permanently-creased trousers or T-shirts, raincoats ...  
electrical cables, parquet ....  
prostheses, catheters, advanced drug-delivery systems ...

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### Bremsstrahlung production

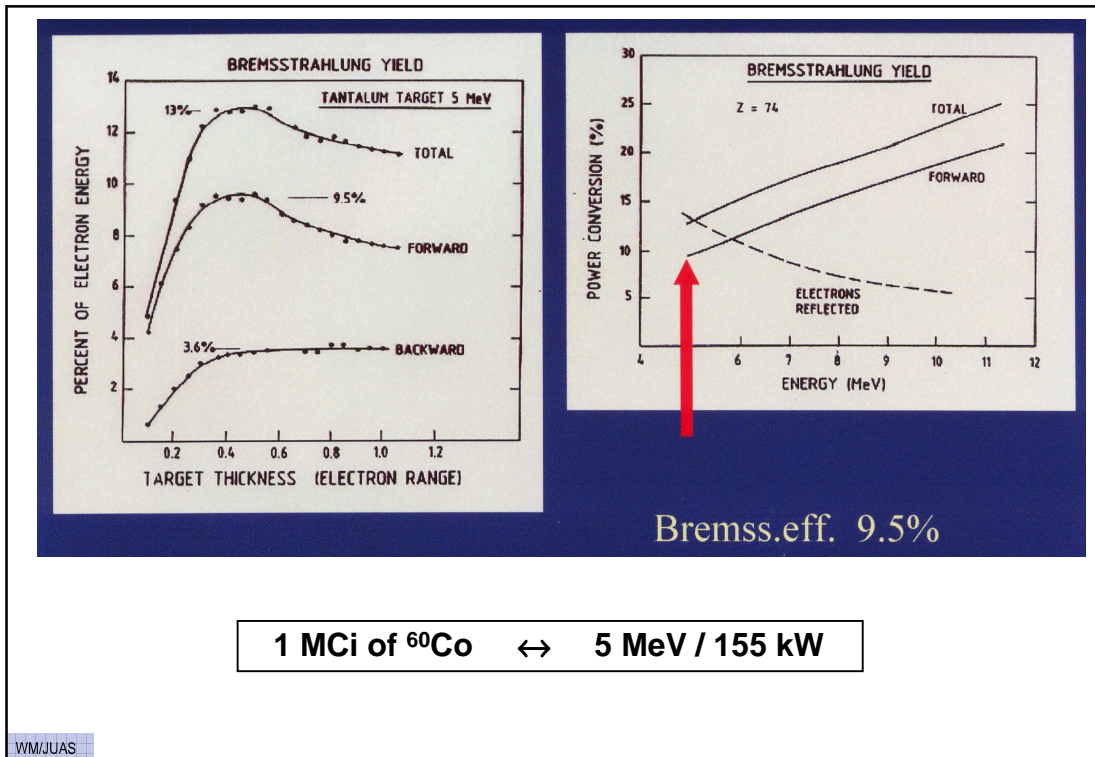
COLLISION STOPPING POWER → HEAT !!!

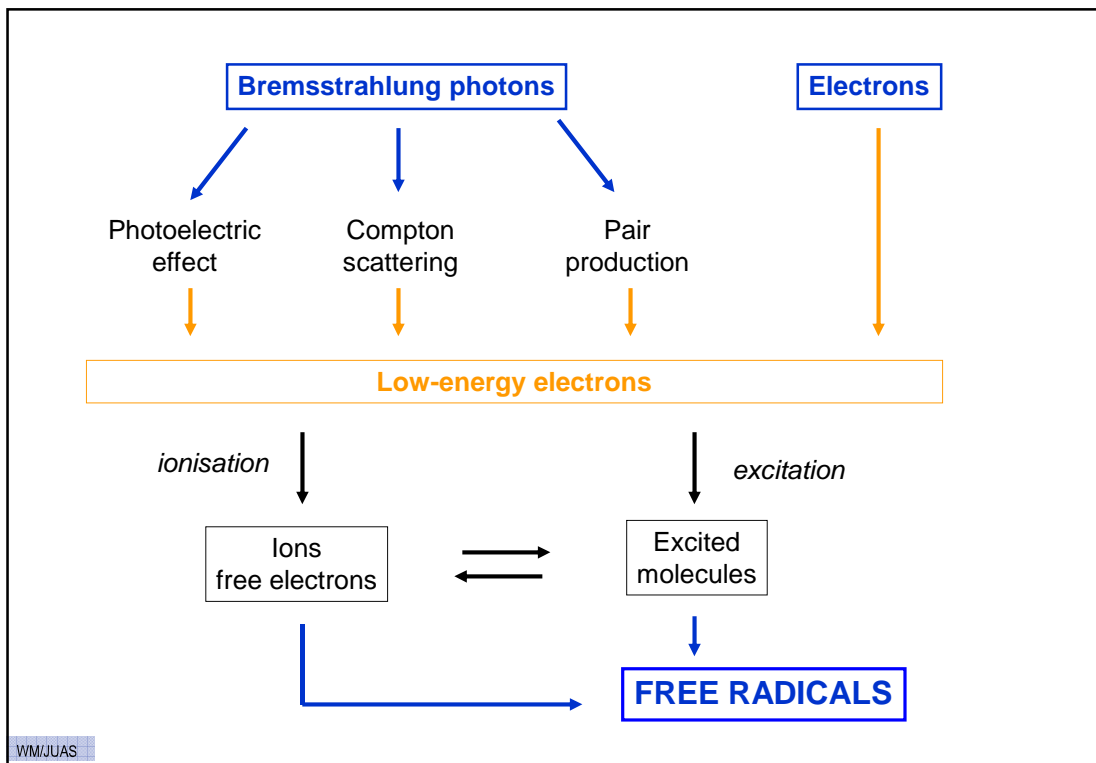
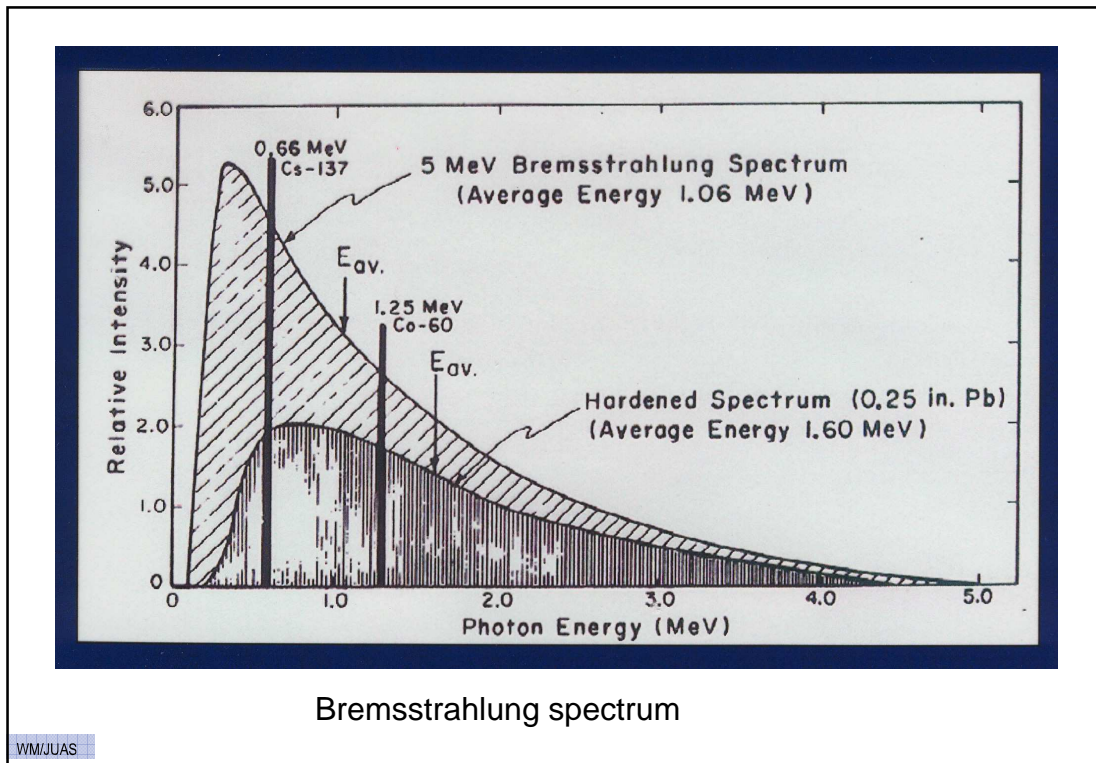
$$-\left(\frac{dT}{dx}\right)_c = 2\pi \frac{e^4 N Z}{m_e \beta^2 c^2} \left[ \ln \frac{m_e \beta^2 c^2 T}{2I^2 (1-\beta^2)} + (1-\beta^2) - \ln 2(2\sqrt{1-\beta^2} - 1 + \beta^2) + \frac{[1-\sqrt{1-\beta^2}]}{8} \right]$$

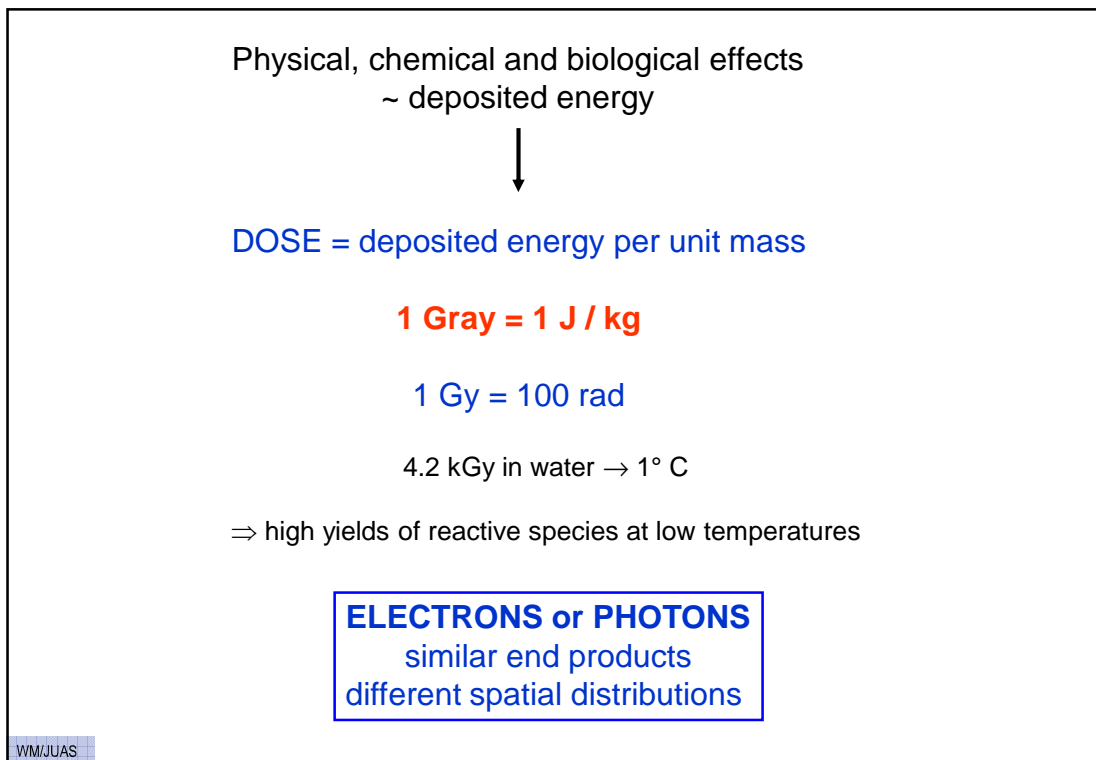
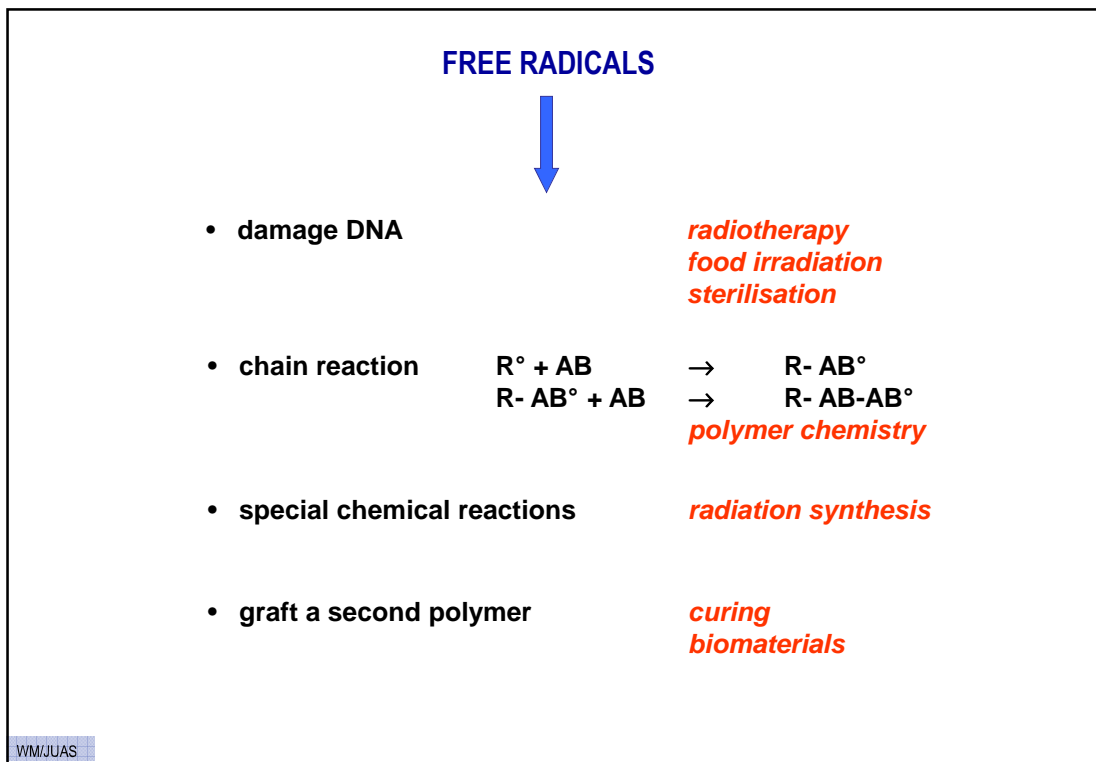
BREMSSTRAHLUNG STOPPING POWER

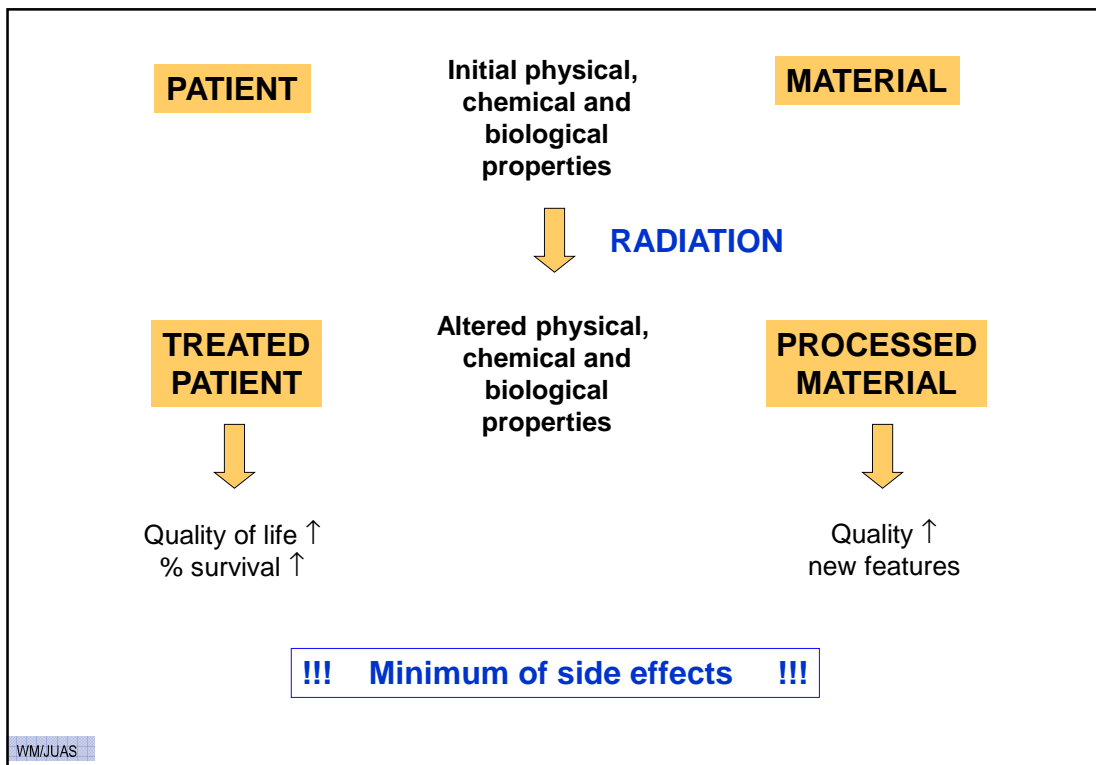
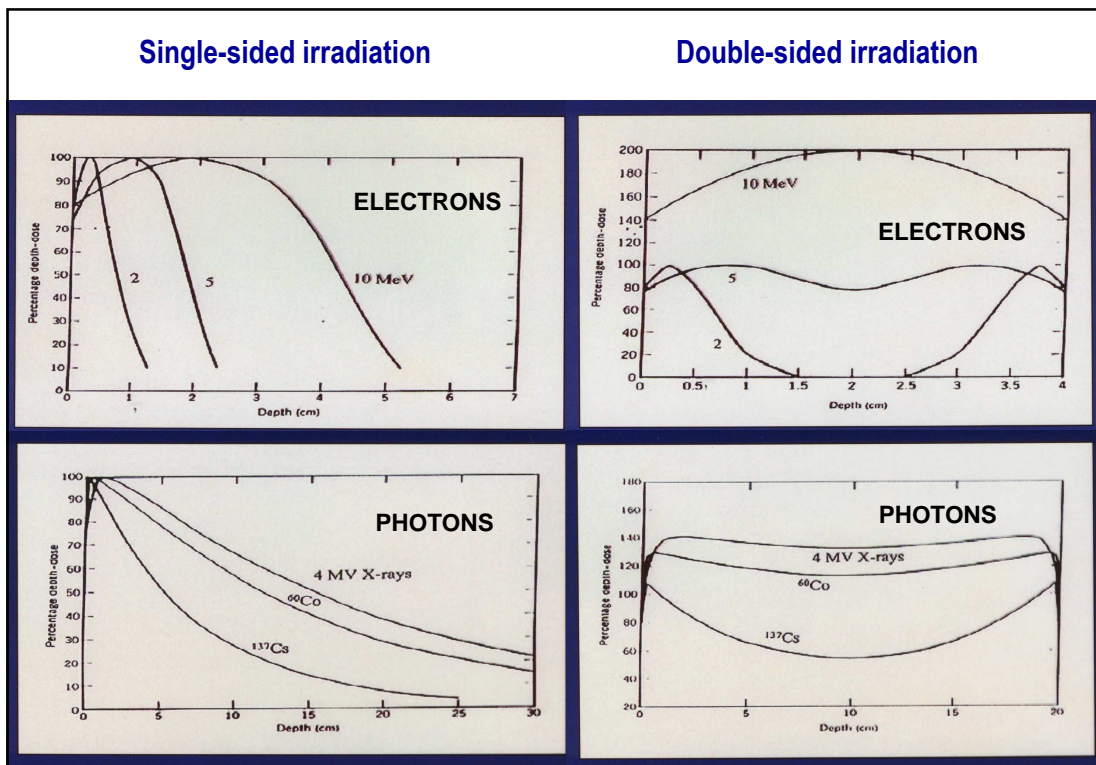
$$-\left(\frac{dT}{dx}\right)_r = \frac{NTZ(Z+1)e^4}{137m_e^2 c^4} \left[ 4 \ln \left( \frac{2T}{m_e c^2} \right) - \frac{4}{3} \right]$$

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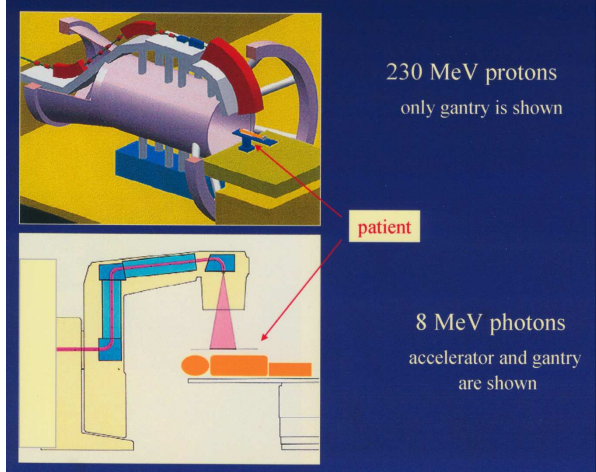
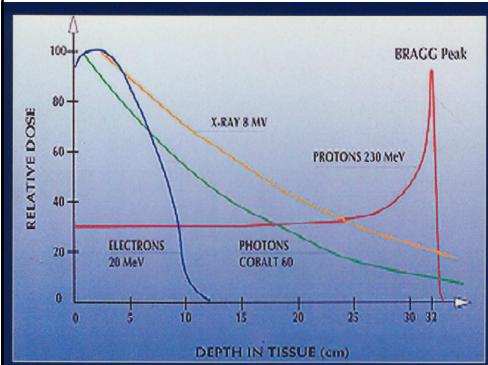






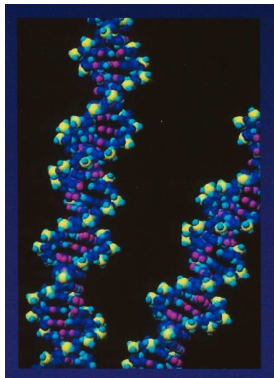


### Low-energy electron accelerators in medicine



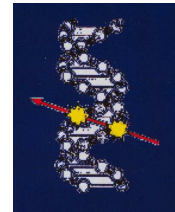
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### Photons and electrons in radiotherapy



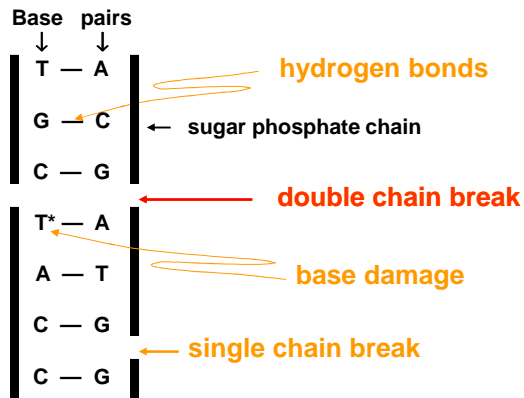
#### Radiation damage to DNA:

- direct
- indirect by free radicals and reactive species



#### Repair mechanisms

60 Gy survival probability  
 $10^{-9}$



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### Dose fractionation

- dose-dependent survival fraction
- oxygenation
- radiosensitivity during cell cycle

X-Rays  
Aerated Cells  
15% Hypoxic Cells  
Immediately After Irradiation  
Mostly Hypoxic Cells  
Reoxygenation

$\ln S/S_0$   
1  
 $10^{-5}$   
DOSE FRACTIONS  
FAST REPAIR  
SLOW REPAIR  
NO FRACTIONATION

Cell cycle  
SURVIVING FRACTION  
0.1  
0.05  
0.02  
0.005  
0.001  
0 3 6 9 12 15 18 21 24 25  
TIME (hrs)

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### Radiotherapy

30 fractions of 2 Gy

4 Gy / min

40 x 40 cm<sup>2</sup>

↓

Accuracy of dose delivery  
± 3.5 %

**Treatment dose  
PLANNING  
DELIVERY**

100%  
0%  
Dose to tumour  
probability to kill tumour  
probability to kill healthy cells  
survival probability

Collimator motion  
Table translation  
Source trajectory relative to patient

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### Conformal therapy: IMRT

The diagram illustrates conformal therapy using IMRT. On the left, a patient is shown with two different beam paths. The top path shows a beam passing through a target (A) and an organ at risk (OAR). The bottom path shows a beam passing through a target (B) and the same OAR. To the right, two cross-sectional diagrams compare the resulting intensity profiles. The first diagram shows a target (A) and OAR (B) where the target is larger than the OAR, resulting in a higher dose to the OAR, labeled  $D(B) > D(A)$ . The second diagram shows a target (A) and OAR (B) where the target is the same size as the OAR, resulting in equal doses, labeled  $D(B) = D(A)$ . Intensity profiles are shown as yellow curves with a dashed line for the target and a solid line for the OAR.

Comparison of conventional and intensity-modulated radiotherapy. The left diagram shows conventional radiotherapy with a uniform beam passing through a tumor (GTV) and an organ at risk. The right diagram shows intensity-modulated radiotherapy where the beam intensity is modulated to conform to the shape of the tumor, sparing the organ at risk.

Comparison of conventional and intensity-modulated radiotherapy.

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### IMRT

Multileaf collimation

Scanned elementary beams

(a) Static technique: A-Leaves + B-Leaves = Target

(b) Dynamic technique:  $v(t) \rightarrow v(t) \rightarrow \dots \rightarrow v(t) = \text{Target}$

Intensity modulation with a multi-leaf collimator using the static technique (a) and the dynamic technique (b).

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### Radiation field requirements

#### BEAM

- well defined
- variable in size
- moveable in three dimensions
- variable energy
- variable intensity
- X-ray  $\leftrightarrow$  electron mode
- pure and well-confined

#### TREATMENT UNIT

- reliable and reproducible
- easy maneuverable
- simple and fail-safe
- very compact

#### DOSE RATE

- high
- irradiation time  $\sim$  1/2 minute
- accurately monitored
- fail-safe feedback to accelerator

#### DOSE DISTRIBUTION

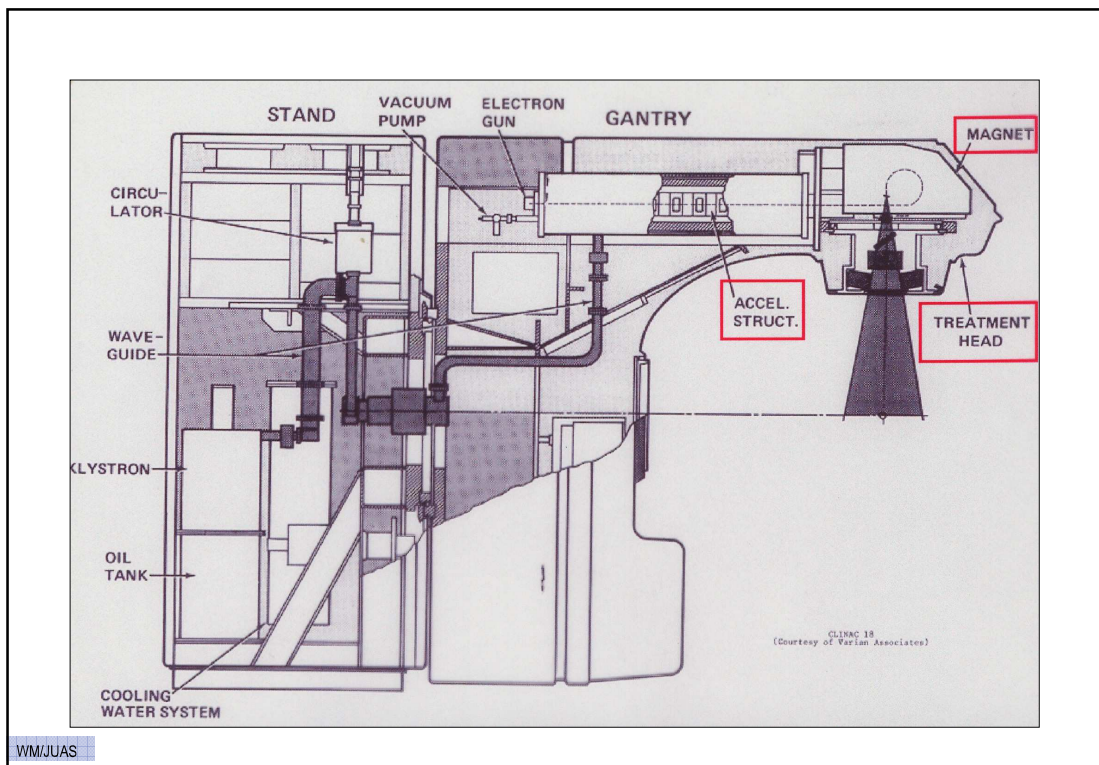
- uniform or
- non-uniform in predefined way
- controllable
- reproducible
- stable

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### Machine requirements

- |                                  |                                  |
|----------------------------------|----------------------------------|
| • energy range                   | 4 - 25 MeV                       |
| • intensity range                | 0.5 - 50 $\mu$ A                 |
| • dose rates                     | 1 - 4 Gy / min                   |
| • number of electron energies    | 5                                |
| • number of X-ray energies       | 2                                |
| • homogeneity of X-ray fields    | 5 % over 40 x 40 cm <sup>2</sup> |
| • homogeneity of electron fields | 5 % over 25 x 25 cm <sup>2</sup> |
| • leakage doses                  | below 10 <sup>-3</sup> at 1 m    |
| • gantry rotation                | 360°                             |
| • isocentre definition           | 1 mm                             |
| • degrees of freedom             | 15 (rotation and translation)    |
| • good definition at target      | energy, position, direction      |
| • volume                         | 5 x 3 x 3 m <sup>3</sup>         |

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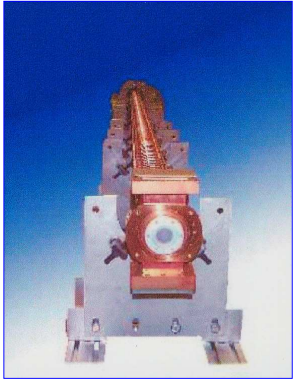


### Energy of the electron accelerator

$$V = \sqrt{(1 - e^{-2\tau})P_0 R_0 L} - \frac{R_0 L I}{2} \left[ 1 - 2\tau \frac{e^{-2\tau}}{1 - e^{-2\tau}} \right]$$

- V = energy of accelerator section in MeV
- L = length accelerator structure in meters
- $P_0$  = high-frequency peak power in MW
- $R_0$  = shunt impedance in  $M\Omega/m$
- $\tau$  = attenuation constant
- I = accelerated peak current in Amperes

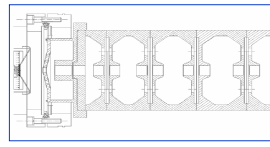
### Accelerating structures



Energy: 4 - 25 MeV

Length: ~ 1 m

HF power: 2 - 5 MW<sub>p</sub>    magnetron  
5 - 10 MW<sub>p</sub>    klystron



↓

### Disc-loaded waveguides

Shunt impedance ↑↑

$$R_0 = -\frac{E_0^2}{\frac{dP}{dz}}$$

→

- travelling wave structure
- standing wave structure

- biperiodic structure
- side-coupled structure

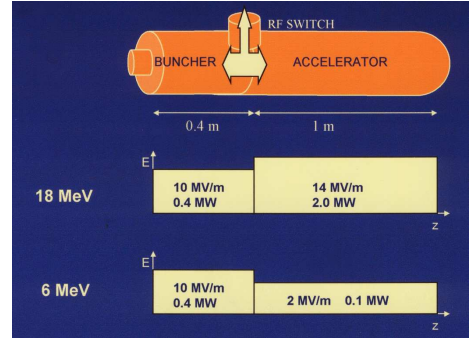
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### Energy variation

1. Variation of input power P<sub>0</sub> or accelerated current I

$$V = \sqrt{(1 - e^{-2\tau})P_0 R_0 L} - \frac{R_0 LI}{2} \left[ 1 - 2\tau \frac{e^{-2\tau}}{1 - e^{-2\tau}} \right] \quad \text{BEAM LOADING}$$

2. Variation of RF frequency
3. Buncher + accelerator section



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### Electrons in bending magnet systems

$$\text{Magnetic rigidity} \quad \chi_b = B\rho = \frac{1}{299.79} \sqrt{V(V+1.022)}$$

- V = energy of electrons in MeV
- B = magnetic field induction in Tesla
- $\rho$  = bending radius in meters

$$\text{Excitation of room-temperature magnet} \quad NI \approx \frac{B}{\mu_0} g$$

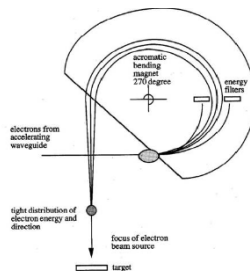
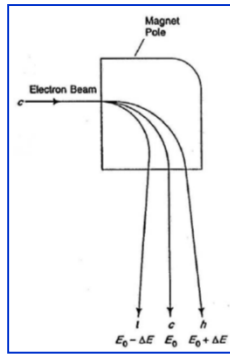
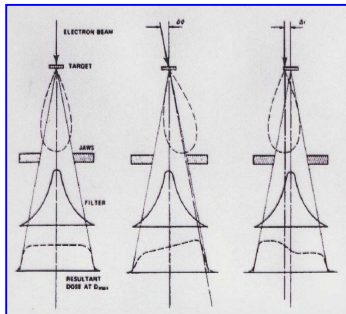
- NI = number of Ampere-turns
- B = magnetic field induction in Tesla
- g = gap between magnet poles in meters
- $\mu_0 = 4\pi \cdot 10^{-7} \text{ Tm/A}$

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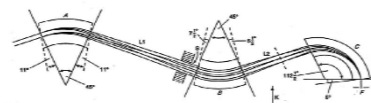
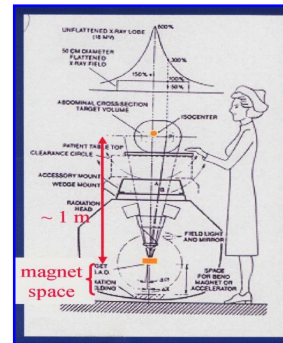
### Bending magnet systems

$$x_1 = m_{11}x_0 + m_{12}x'_0 + m_{13} \frac{\Delta p}{p}$$

$$x'_1 = m_{21}x_0 + m_{22}x'_0 + m_{23} \frac{\Delta p}{p}$$



Energy spread  
 medical ~ 10 %  
 research < 1 %



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**Bending magnet systems****TRANSPORT calculations****DRIFT PIECE**Length  $L$ 

$$M_H = \begin{pmatrix} 1 & L & 0 \\ 0 & 1 & 0 \\ 0 & 0 & 1 \end{pmatrix}$$

$$M_V = \begin{pmatrix} 1 & L \\ 0 & 1 \end{pmatrix}$$

**HOMOGENEOUS BENDING MAGNET**Length  $L$ Bending angle  $\alpha$ Bending radius  $\rho$ 

$$M_H = \begin{pmatrix} \cos\alpha & \rho\sin\alpha & \rho(1-\cos\alpha) \\ -\frac{\sin\alpha}{\rho} & \cos\alpha & \sin\alpha \\ 0 & 0 & 1 \end{pmatrix}$$

$$M_V = \begin{pmatrix} 1 & \rho L \\ 0 & 1 \end{pmatrix}$$

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**WEAK FOCUSING BENDING MAGNET**Field index  $0 < n < 1$ Length  $L$ Bending angle  $\alpha$ Bending radius  $\rho$ 

$$M_H = \begin{pmatrix} \cos\sqrt{1-n}\alpha & \frac{\rho\sin\sqrt{1-n}\alpha}{\sqrt{1-n}} & \frac{\rho(1-\cos\sqrt{1-n}\alpha)}{1-n} \\ -\frac{\sqrt{1-n}\sin\sqrt{1-n}\alpha}{\rho} & \cos\sqrt{1-n}\alpha & \frac{\sin\sqrt{1-n}\alpha}{\sqrt{1-n}} \\ 0 & 0 & 1 \end{pmatrix}$$

$$M_V = \begin{pmatrix} \cos\sqrt{n}\alpha & \frac{\rho\sin\sqrt{n}\alpha}{\sqrt{n}} \\ -\frac{\sqrt{n}\sin\sqrt{n}\alpha}{\rho} & \cos\sqrt{n}\alpha \end{pmatrix}$$

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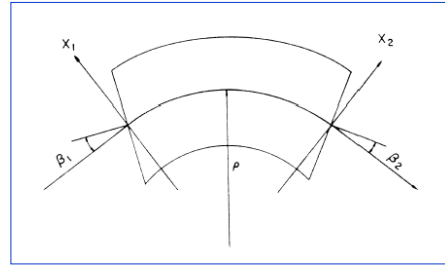


**HOMOGENEOUS BENDING MAGNET with ROTATED POLE SHOE EDGES**

Length L Bending angle  $\alpha$  Bending radius  $\rho$

$\beta_1$  angle of pole edge rotation at entrance

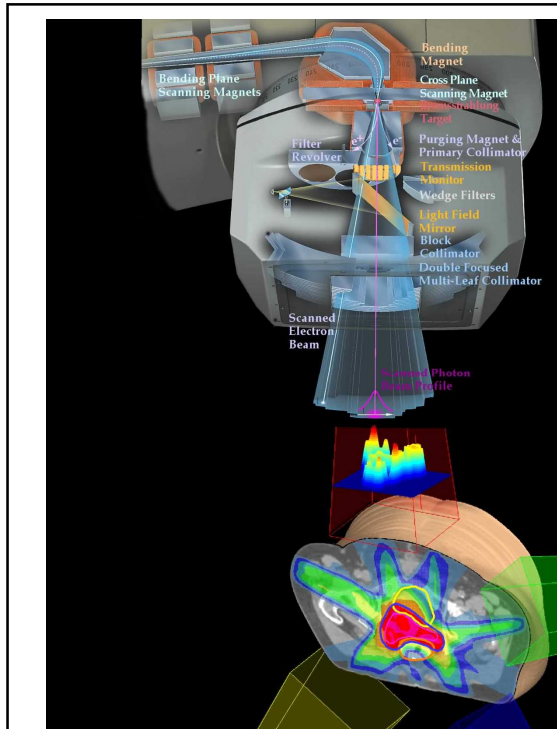
$\beta_2$  angle of pole edge rotation at exit



$$M_H = \begin{pmatrix} 1 & 0 & 0 \\ \frac{\tan\beta_2}{\rho} & 1 & 0 \\ 0 & 0 & 1 \end{pmatrix} \begin{pmatrix} \cos\alpha & \rho\sin\alpha & \rho(1-\cos\alpha) \\ -\frac{\sin\alpha}{\rho} & \cos\alpha & \sin\alpha \\ 0 & 0 & 1 \end{pmatrix} \begin{pmatrix} 1 & 0 & 0 \\ \frac{\tan\beta_1}{\rho} & 1 & 0 \\ 0 & 0 & 1 \end{pmatrix}$$

$$M_V = \begin{pmatrix} 1 & 0 \\ -\frac{\tan\beta_2}{\rho} & 1 \end{pmatrix} \begin{pmatrix} 1 & \rho\alpha \\ 0 & 1 \end{pmatrix} \begin{pmatrix} 1 & 0 \\ -\frac{\tan\beta_1}{\rho} & 1 \end{pmatrix}$$

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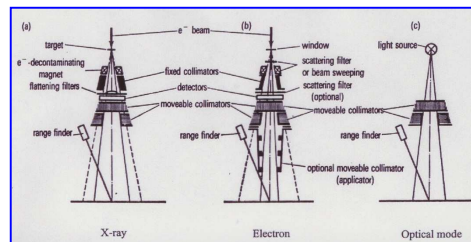


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**Treatment head**



Multileaf collimator



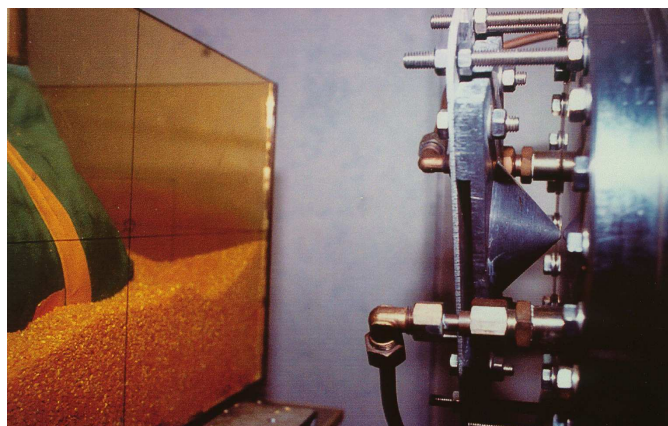
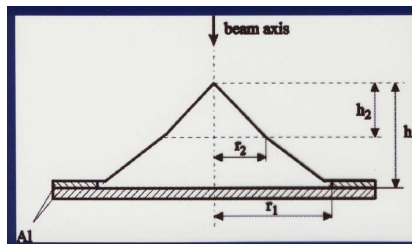
### New trends

- intensity-modulated radiotherapy
- thomotherapy
- image-guided radiotherapy
- stereotactic radiosurgery
- intra-operative radiotherapy

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### Extracorporeal bone tumours irradiation

Homogeneity  
< 2 %



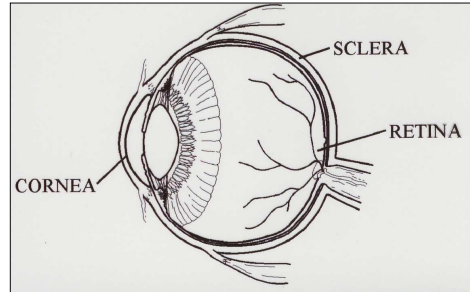
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### Radiation treatment of human grafts and artificial implants

• **sclerae of the human eye**

prosthesis → inflammation  
rejection

⇒ 'packed' in human sclerae  
- less reactions  
- synchronous movement



lyophilisation → sterilisation 25 kGy → tissue bank

- **bone fragments:** maxillo-facial reconstruction
- **human implants:** cardiological stents, polymeric implants, hydrogels
- **blood products:** lymphocytes 40 Gy (graft-versus-host disease)

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### Low-energy electron accelerators in industry

$$\text{BEAM POWER} = \text{ENERGY} \times \text{INTENSITY}$$

DOSE RATE  
↓  
INTENSITY

Energy

< 10 MeV electrons  
< 5 MeV photons

~ penetration depth

150 KW

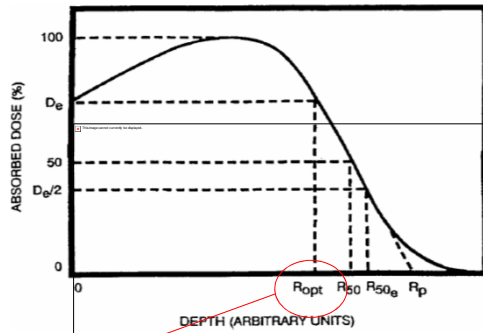
5 MeV / 30 mA  
0.5 MeV / 300 mA

ACCELERATORS

3 energy ranges      0.1 – 0.5 MeV  
                                 0.5 – 5 MeV  
                                 5 – 10 MeV

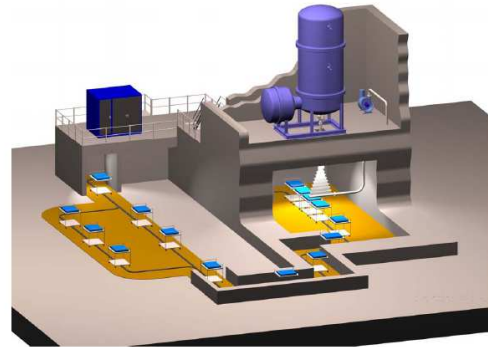
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### Electron range in radiation processing



$R_{opt}$  : exit dose equals entrance dose

$R_{opt}$  = optimal range in  $g/cm^2$   
 $V$  = energy of electrons in MeV



$$R_{opt} = 0,404V - 0,161$$

$$R_{opt} (cm) = R_{opt} (g/cm^2) / \rho (g/cm^3)$$

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### Throughput in radiation processing (electron and X-ray mode)

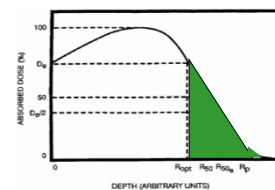
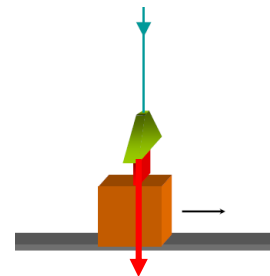
Mass throughput

$$\frac{M}{T} = F(e)F(i) \frac{P}{D(ave)}$$

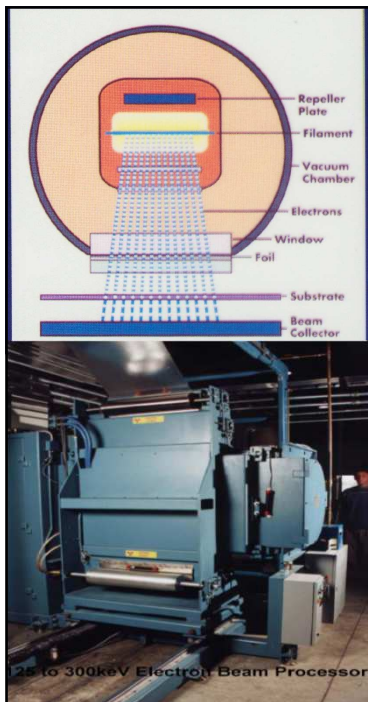
$M$  = mass in kg  
 $T$  = time in seconds  
 $P$  = emitted radiation power in kW  
 $D(ave)$  = average absorbed dose on kGy

$F(i)$  = fraction of emitted beam current intercepted by material

$F(e)$  = fraction of incident electron energy absorbed by material



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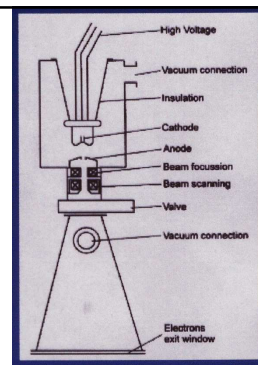
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**BROAD BEAM**

**Energy range 0.1 - 0.5 MeV**

**Single-stage machines**

- self-shielding
- low penetration capability
- integrated in production line
- beam widths ~ 2.5 m



**SCANNING TYPE**

**APPLICATIONS:**

- surface treatment
- irradiation of coatings, adhesives, inks
- e.g. thin film packaging
- printing industry

**Energy range 0.5 - 5 MeV**

**Multi-stage machines**

- high penetration capability
- up to 300 kW
- beam widths ~ 2 m

**COCKROFT-WALTON**

**INSULATED-CORE TRANSFORMER**

**DYNAMITRON**

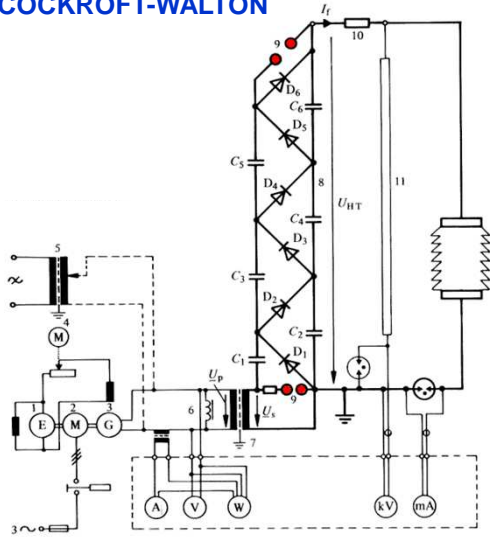
**APPLICATIONS:**

- processing of thick sheets
- wires and cables
- tubes and pipes
- fiber composites
- tire components
- heat-shrinkable products
- foamed polyethylene

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Energy range 0.5 - 5 MeV

**COCKROFT-WALTON**

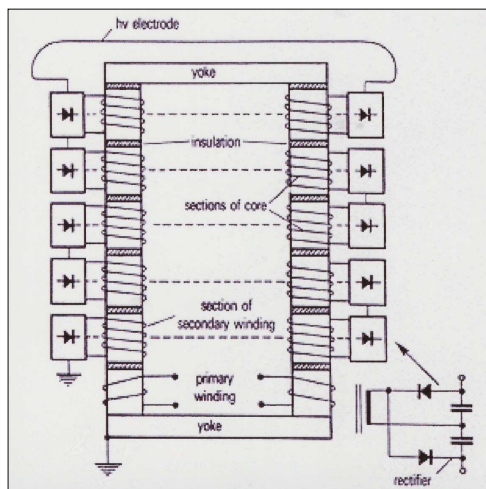


**Greinacher cascade generator**

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Energy range 0.5 - 5 MeV

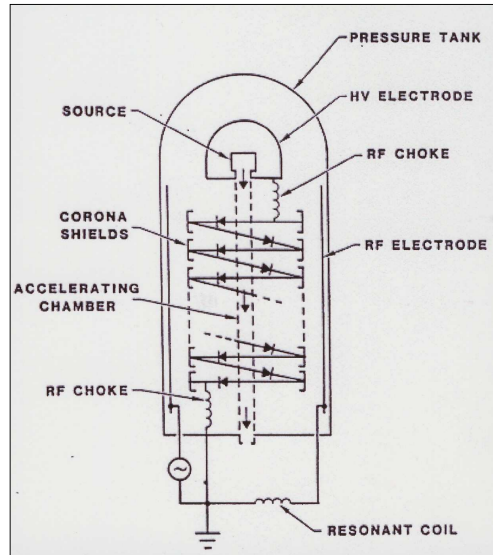
**INSULATED-CORE TRANSFORMER**



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Energy range 0.5 - 5 MeV

**DYNAMITRON**



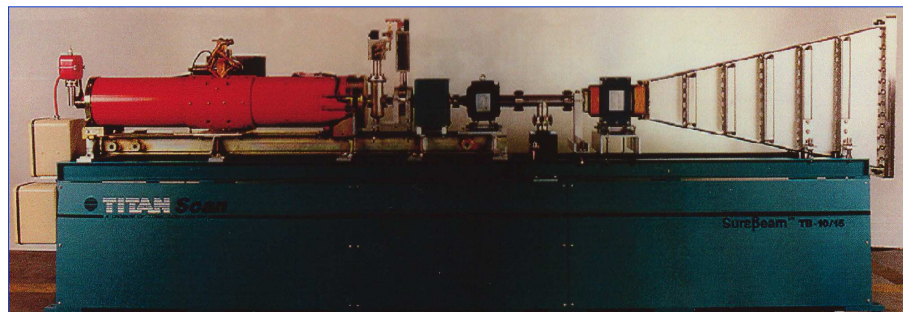
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Energy range 5 - 10 MeV

- RF linear accelerator → 50 kW
- RHODOTRON → 200 kW up to 1 MW

**APPLICATIONS:** < 5 MeV applications  
 medical sterilisation  
 food processing  
 polymer crosslinking, grafting, degradation

**LINAC**



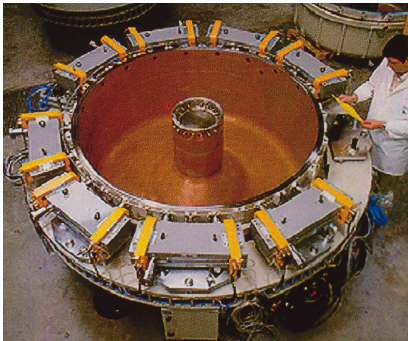
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Energy range 5 - 10 MeV

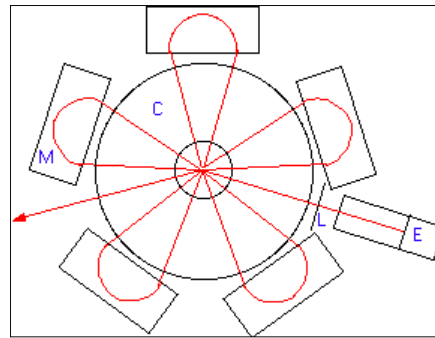
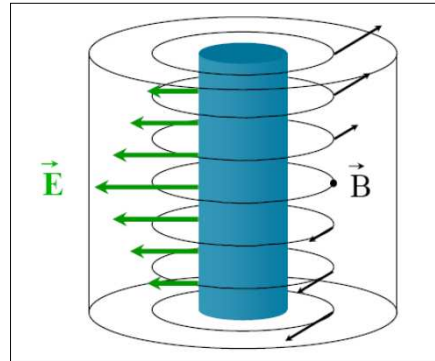
### RHODOTRON

$$E = \frac{E_0}{r} \cos 2\pi \frac{z}{\lambda} \sin(\omega t + \varphi)$$

$$B = \frac{B_0}{r} \sin 2\pi \frac{z}{\lambda} \cos(\omega t + \varphi)$$



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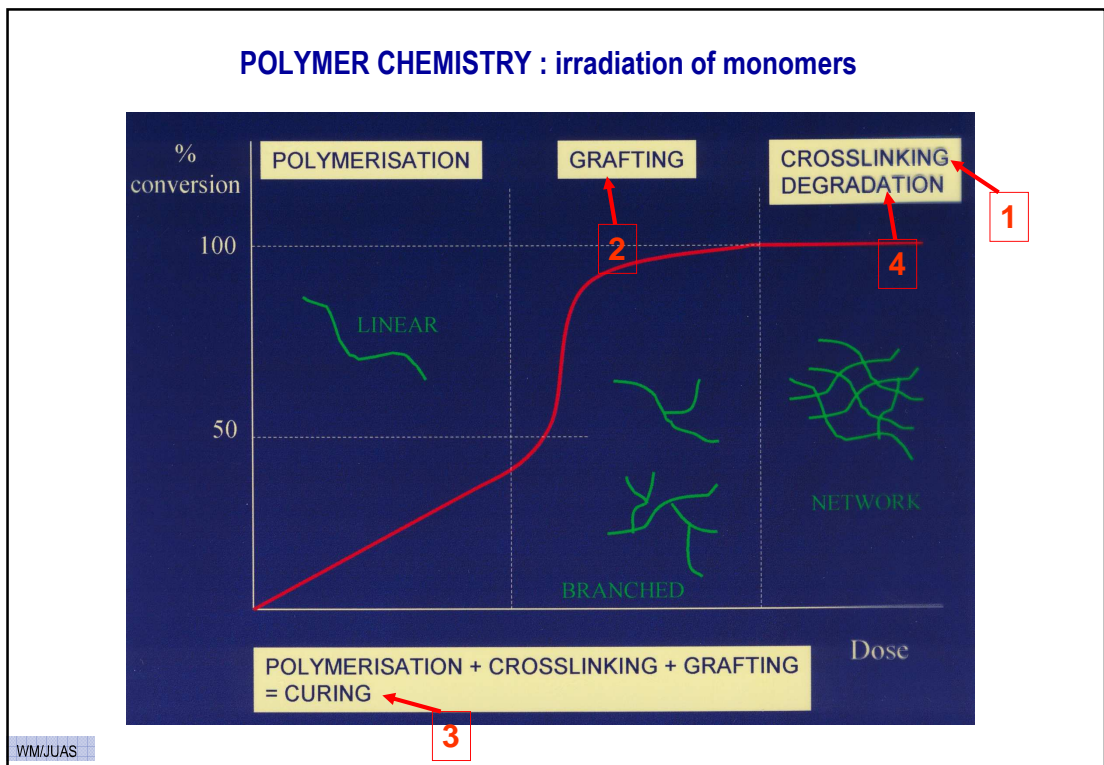


### INDUSTRIAL APPLICATIONS of ELECTRONS and BREMSSTRAHLUNG

1. POLYMER CHEMISTRY
  - crosslinking
  - grafting
  - curing
  - degradation
2. STERILISATION
3. FOOD TREATMENT
4. RADIOGRAPHY
5. WELDING AND CUTTING

WM/JUAS





### CROSSLINKING

Linear molecule → 3D structure  
e.g. polyethylene

↓

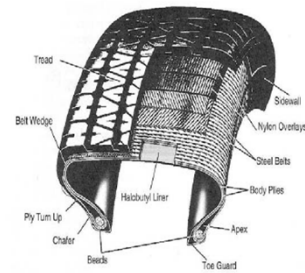
≠ physical properties

- heat resistance ↑↑
- insulation properties ↑
- mechanical strength ↑
- breakdown voltage ↑
- chemical resistance ↑
- creep ↑
- 'memory effect'

- cable insulation
- tubes, pipes and mouldings
- heat-shrinkable films
- vulcanisation of rubber and tires
- synthesis of biomaterials

### EXAMPLE : Pre-vulcanisation of tires

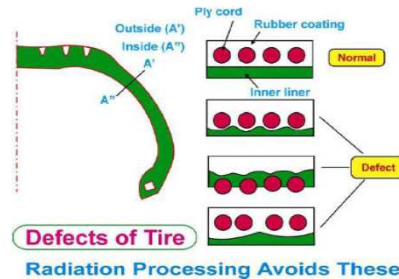
partial crosslinking before the tire is assembled:



- stabilizes thickness of sections during final thermal curing process
- prevents steel belt from migrating through its supporting rubber layer



- improves manufacturability
- better dimensional stability
- higher quality tire
- more uniform thickness
- better balance
- thinner thus generating less frictional

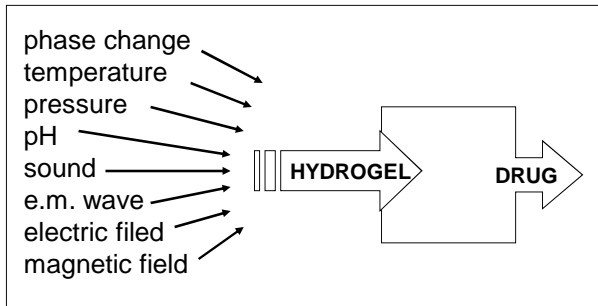


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### EXAMPLE : Synthesis of biomaterials

HYDROGELS = crosslinked macromolecular networks swollen in water

- rubbery structure
- substantial water content
- ~ soft living tissue → **BIOCOMPATIBLE**
- porous network → **BIOFUNCTIONAL**



- biodegradable polymers
- hydrogels for burn wounds
- porous polymeric hydrogels for advanced drug delivery systems

constant release  
signal responsive

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### GRAFTING

Polymer backbone + monomer

≠ surface properties

- biocompatibility
- adhesion
- permeability
- wettability
- chemical resistance
- chemical compatibility
- printability
- hydrophilic / phobic quantities
- functionalisation
- mechanical properties

- finishing of textiles
- adhesion of polyethylene on aluminium
- weak hydrogels on polymeric support
- biofunctional groups on inactive supports

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### EXAMPLE : Immobilisation of bioactive agents

Grafting of biofunctional groups on polymer supports

#### • HEPARINE FILTER

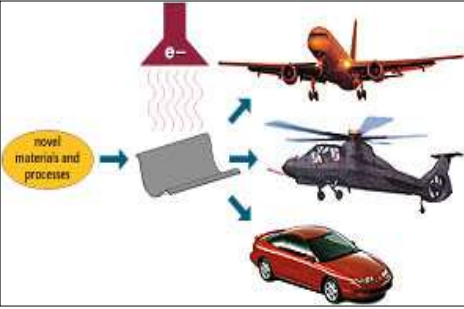
= heparine adsorber

Hemodialysis of uremic patients  
blood + artificial surfaces → coagulation

#### heparine adsorbing filters

- FIXATION of HD CELL CULTURES
- natural skin
- pancreas cells

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e.g. carbon fiber reinforced epoxies

- automobiles
- aircraft
- ships
- space vehicles
- building materials
- sporting goods
- printed circuit boards

### CURING


Polymerisation + crosslinking + grafting

on SURFACES (mainly with electrons)

- antistatic films
- laminates (credits cards, telephone cards)
- offset printing
- door finishing
- parquet coating
- protective films....

in BULK MATERIAL (mainly bremsstrahlung)

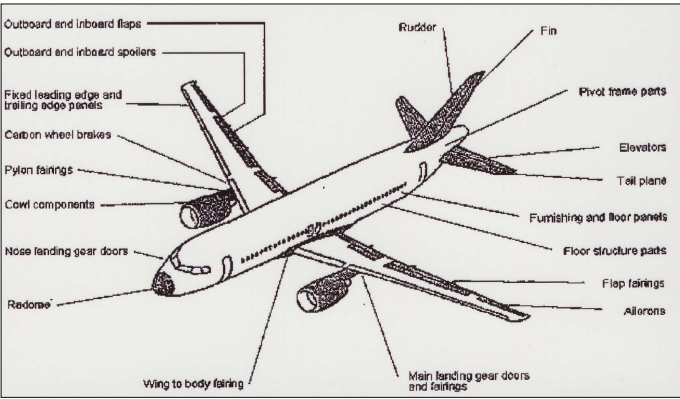
- wood-polymer composites
- concrete-polymer composites
- advanced composites



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### EXAMPLE : On-aircraft repair

Composite materials (carbon-reinforced epoxies):




strength-to-weight ratio ↑  
 stiffness-to-weight ratio ↑  
 corrosion resistance  
 impact damage tolerance  
 wear properties

↓

20 - 25 % of aircraft structural weight


**AIR CANADA**    Airbus A320  
 on aircraft repair with mobile accelerator

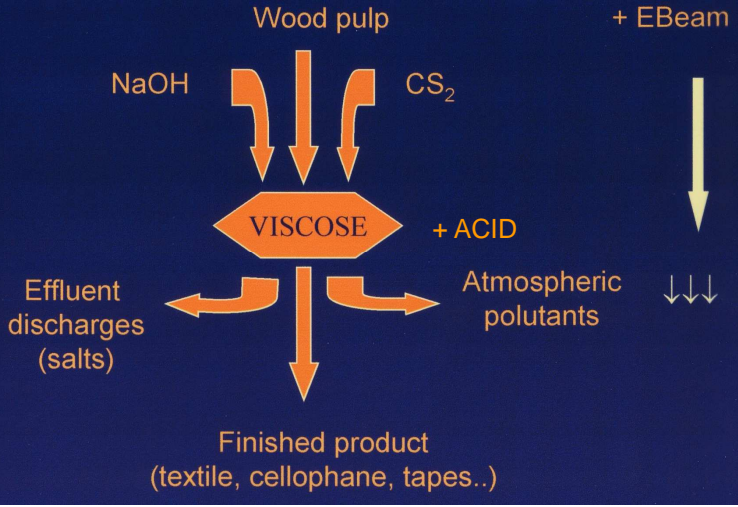


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### DEGRADATION

- cellulose in viscose industry

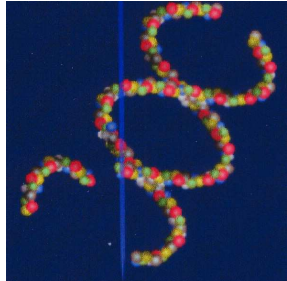




- powdered Teflon molecular weight ↓  
lubricants, high quality inks
- degradation of pollutants  
water, industrial or hospital waste  
sewage sludge, flue gases


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### STERILISATION




#### Radiation killing of pathogenic microorganisms

- energy-efficient (↔ heat)
- low temperature (↔ heat)
- no toxic residues (↔ EtO)
- total sterilisation (↔ EtO)
- no ozone depletion (↔ Met.B.)




- medical disposables

*syringes, needles, surgical sutures  
wound and burn dressings  
gloves, masks, gowns  
Petri dishes and pipettes*



- medical implants

*artificial organs  
bone grafts  
human eyeballs*



- pharmaceuticals  
- cosmetics

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## FOOD TREATMENT

### Low Dose Applications (< 1 kGy)

- **Phytosanitary** Insect disinfection (grains, papayas, mangoes, avocados...)
- **Sprouting Inhibition** (potatoes, onions, garlic...)
- **Delaying of maturation, parasite disinfection**

### Medium Dose Applications (1 to 10 kGy)

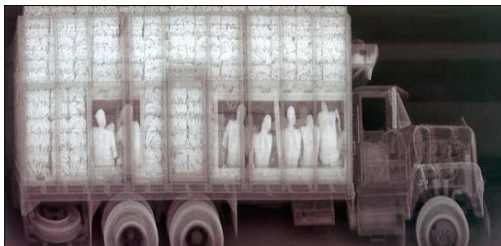
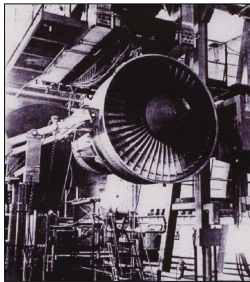
- **Control of foodborne pathogens** (beef, eggs, crab meat, oysters...)
- **Shelf-life extension** (chicken, pork, low fat fish, strawberries, mushrooms...)
- **Spice irradiation**

### High Dose Applications (> 10 kGy)

- **Food sterilisation** (meat, poultry, seafood...)

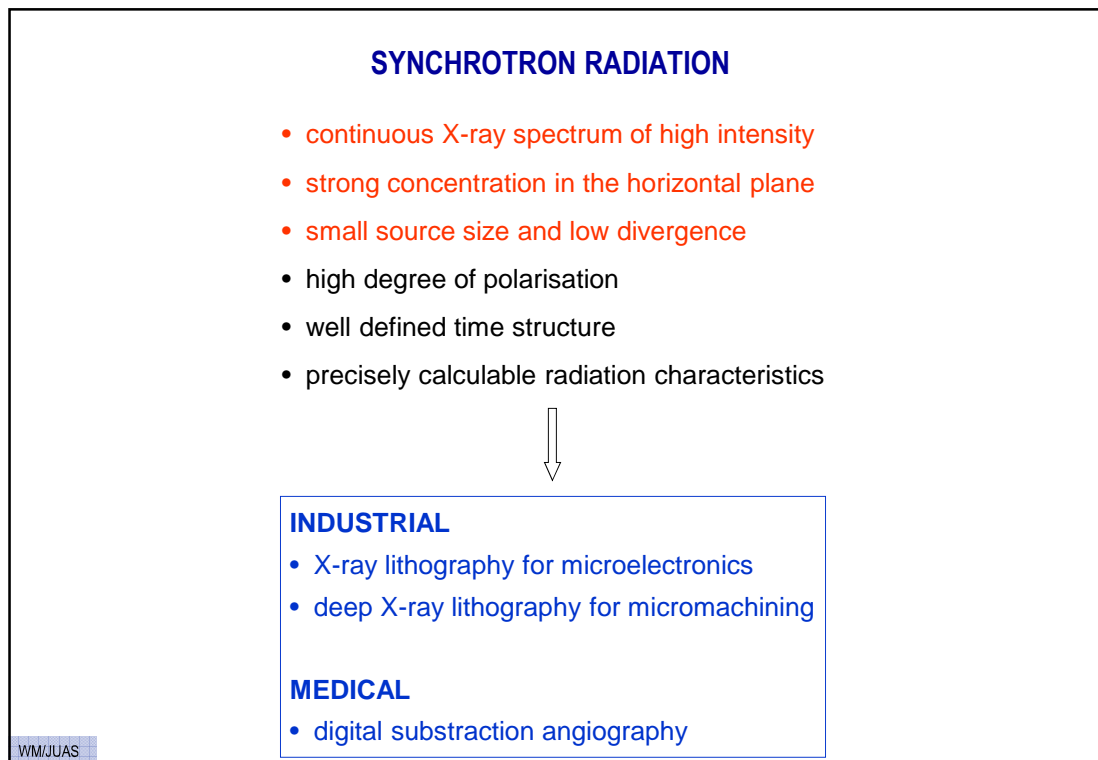
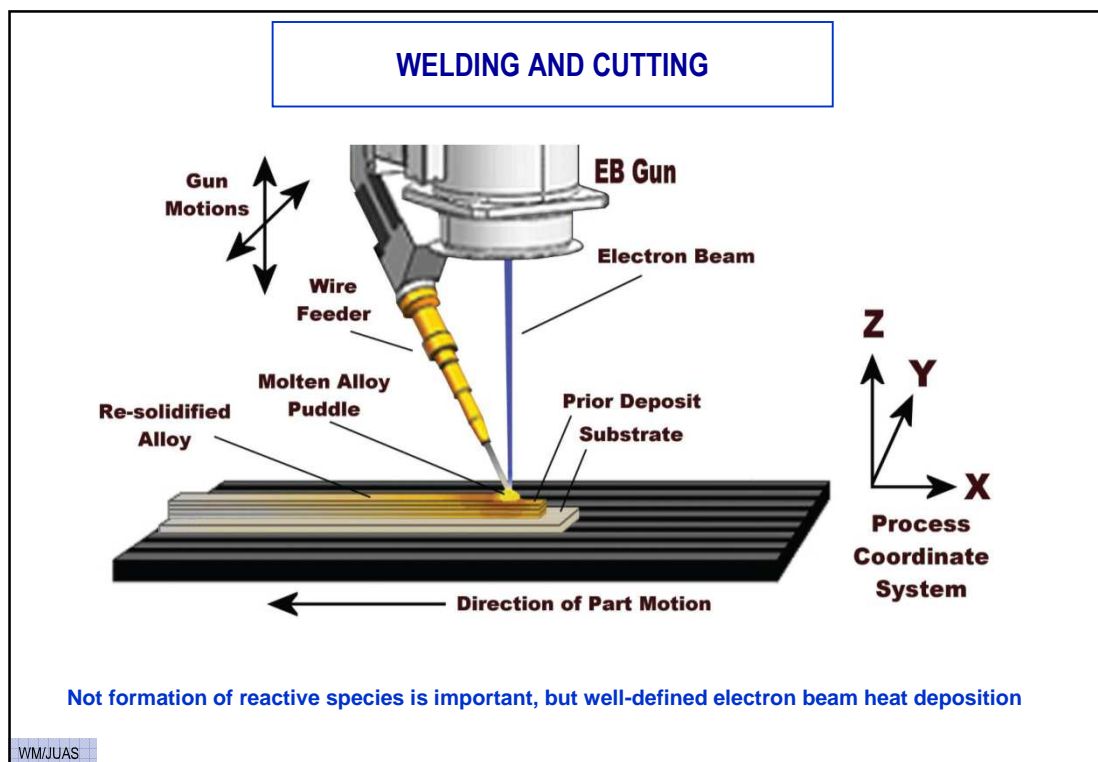
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## RADIOGRAPHY



- dynamically inspecting jet engines
- X-ray screening of cargo containers
- inspecting concrete structure integrity
- inspecting castings
- reverse engineering CT studies
- nuclear waste inspection
- border control

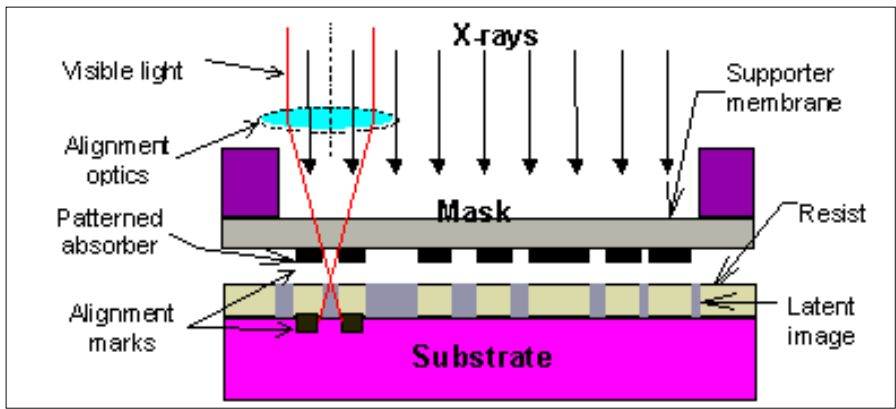
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### X-ray lithography for microelectronics

the **SMALLER** the wavelength the better the resolution

X-ray lithography  
(resolution better than 100 nm)

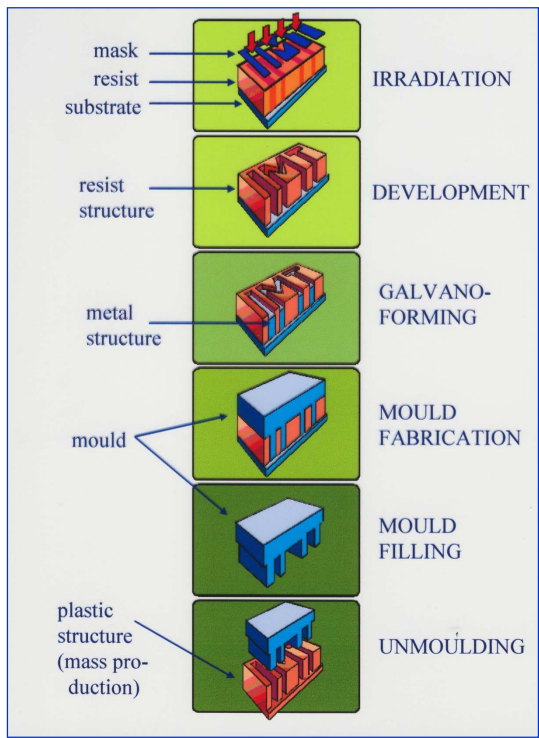


X-ray energy : 1 keV

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### Deep X-ray lithography for micromachining

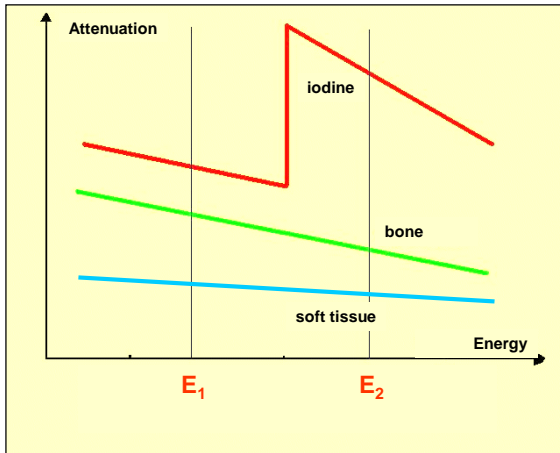
#### LIGA process



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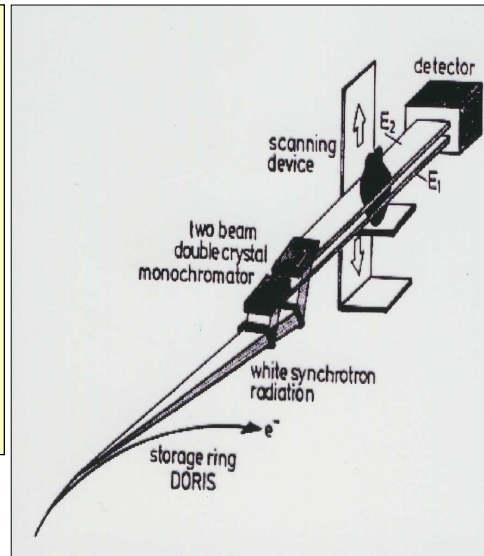


### Digital subtraction angiography



Monochromatic X-rays

X-ray energy : 33 keV



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### Basic design considerations

<u>Critical wavelength:</u>	1 nm	X-ray lithography
	0,2 nm	deep X-ray lithography
	0,0037 nm	digital subtraction angiography

Photon flux: 2.10<sup>11</sup> - 2.10<sup>12</sup> ph/sec-mm<sup>2</sup>

Required radiation at the lowest price



**COMPACT SR FACILITIES**



Research SR facilities

**2<sup>nd</sup> generation**



DESIGN CRITERIA

- 0.7 – 3 GeV range
- high photon flux
- small size
- low investment and operating cost
- not too complex
- easy to operate
- applications define ring parameters

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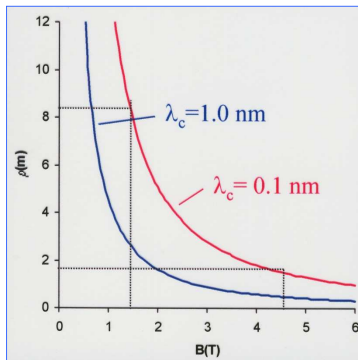
## 1. MAGNETS

### COMPACTNESS

#### Normal-conducting



- simplify existing storage ring design
- remove some quadrupoles
- dimensions ↓



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#### superconducting magnets ?



- unusual storage ring design
- new optical schemes
- dimensions ↓↓

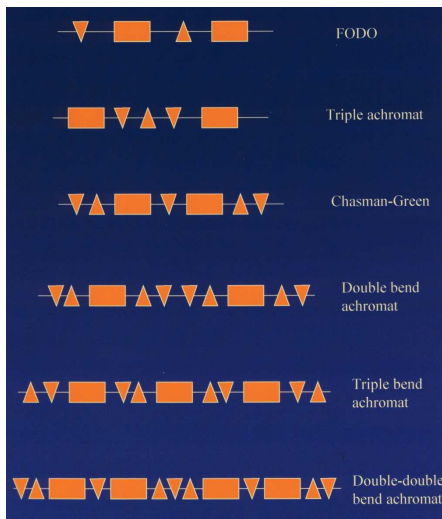
$$\lambda_c = \frac{20.7}{\rho^2(\text{m})B^3(\text{T})}$$

Normal conducting      1,5 T

Superconducting      4,5 T     $\rho/5$

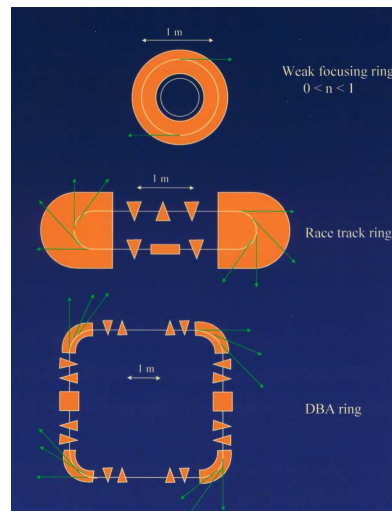
## 2. LATTICES

### IRON MAGNET LATTICES



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### SUPERCONDUCTING LATTICES



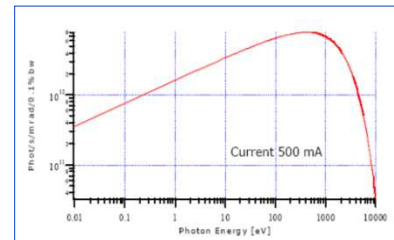


## HELIOS

HELIOS 1 IBM East Fishkill  
 HELIOS 2 Singapore

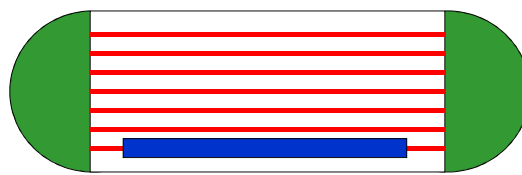


- Energy 700 MeV
- Stored current 620 mA
- Magnets 2 superconducting 180°
- Critical wavelength 0.84 m
- Nb of beamports 20
- Dimensions 6 m x 2m
- Injector 200 MeV linac (HELIOS 1)  
100 MeV microtron (HELIOS 2)



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### Stable motion in HELIOS ring



Stability condition in periodic rings:

$$-1 \leq \frac{1}{2} \text{trace}M \leq 1$$

period

$$M = \begin{pmatrix} m_{11} & m_{12} \\ m_{21} & m_{22} \end{pmatrix}$$

traceM = trace of matrix M, it is equal to the sum of the diagonal elements of matrix M

M is transfer matrix of one period in ring

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