

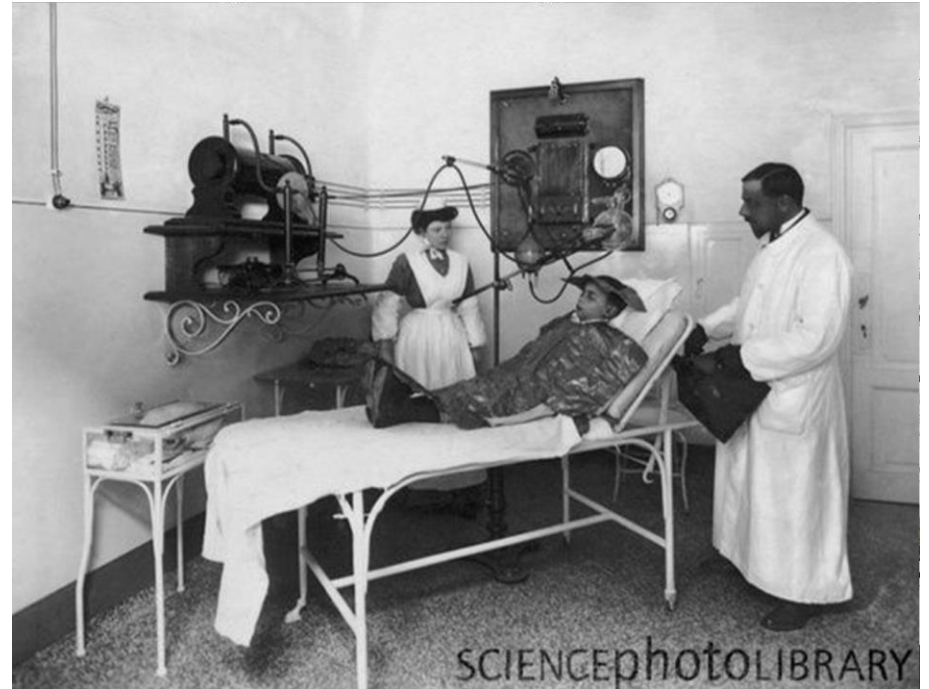
Generation of clinical proton minibeam using magnetic focussing

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Clinical proton minibeams
are used for
proton minibeam radiation therapy.

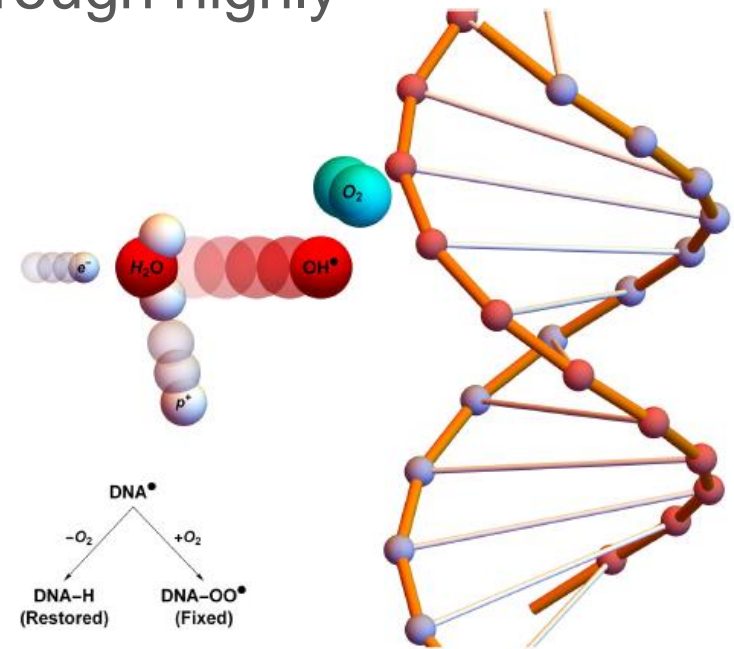
- radiation therapy: eliminate cancer using ionising radiation
- most treatments using x-rays
- x-rays discovered
Nov 1895 (Röntgen)
- first treatment with x-rays
Jan 1896 (Grubbé)
- proton therapy suggested
1946 (Wilson)
- first treatment with protons 1954



Source: Giap and Giap, *Historical perspective and evolution of charged particle beam therapy*, *Transl Cancer Res* 2012;1(3):127-136

Basic principle

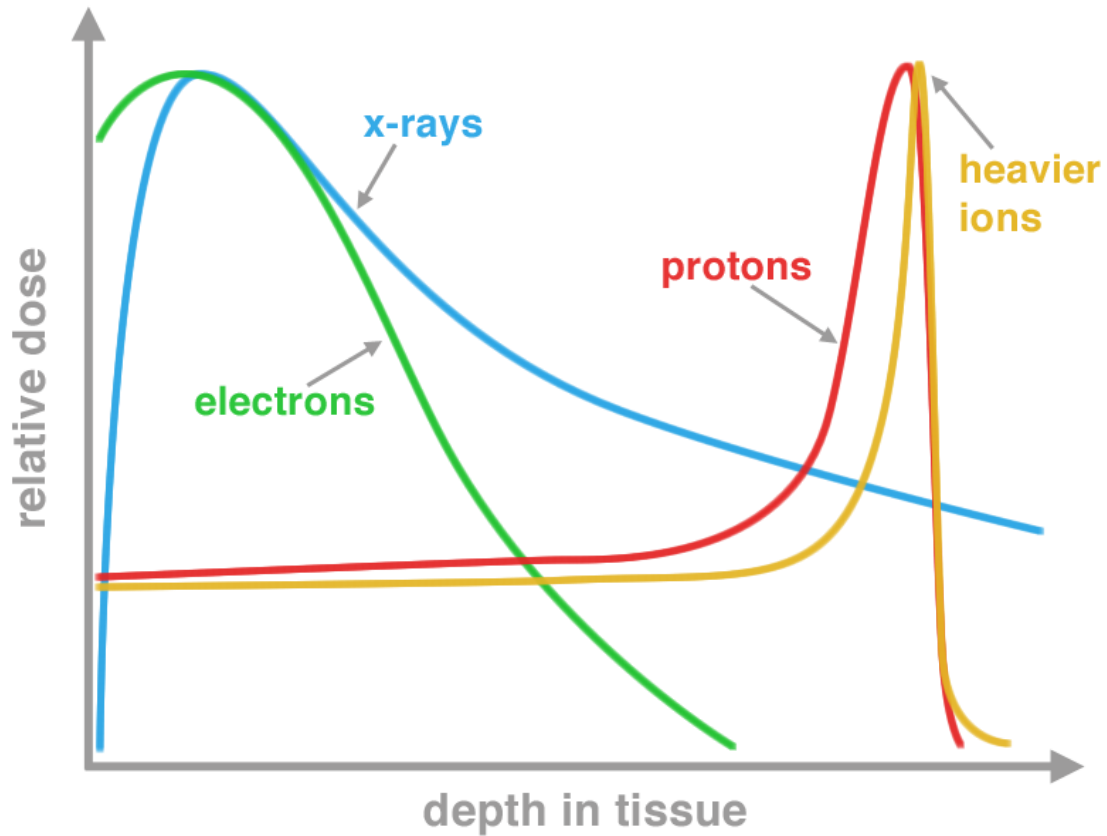
- 1) radiation ionises molecules throughout the cell
- 2) direct DNA damage or indirect through highly reactive (free) radicals
- 3) DNA damage accumulates (SSB, DSB, base damage...)
- 4) cell death



Source: <http://www.ox.ac.uk/news/science-blog/breath-fresh-air---shedding-light-oxygen-radiation-and-cancer-treatment>, 03.05.19

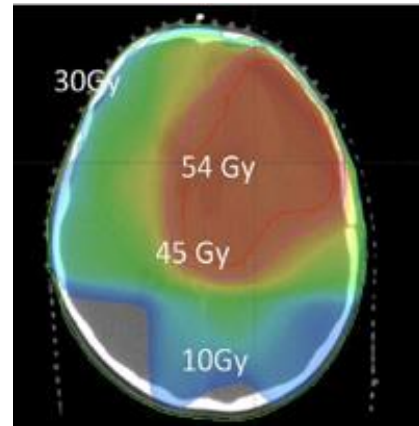
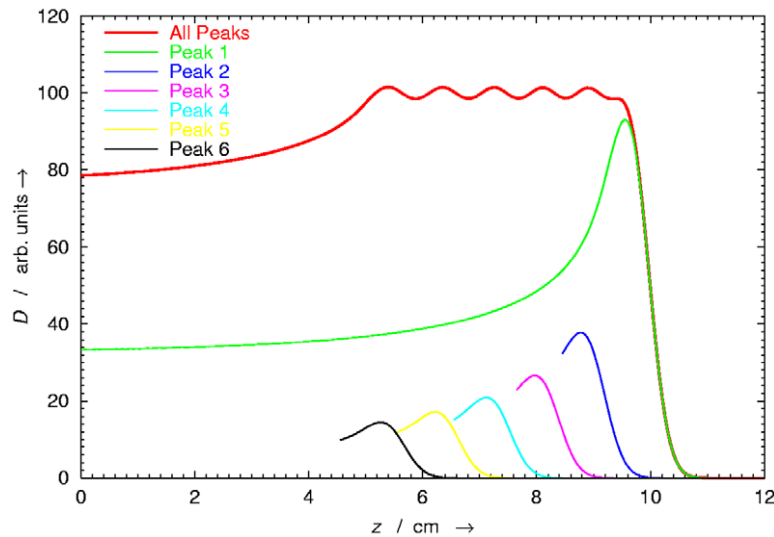
Clinical proton minibeam
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Particles used for RT

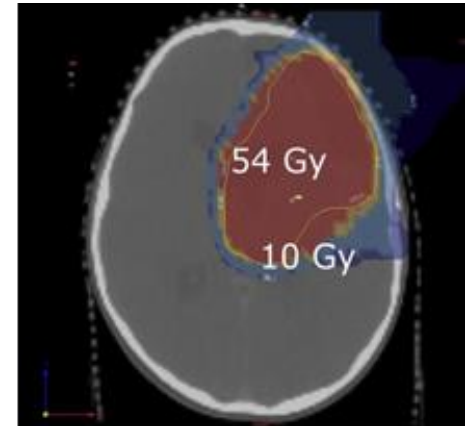


protons/ions
exhibit *Bragg peak*

- more targeted dose distribution (Bragg peak)
- combine multiple pristine Bragg peaks to form a spread-out Bragg peak



irradiating a brain tumor with X-rays



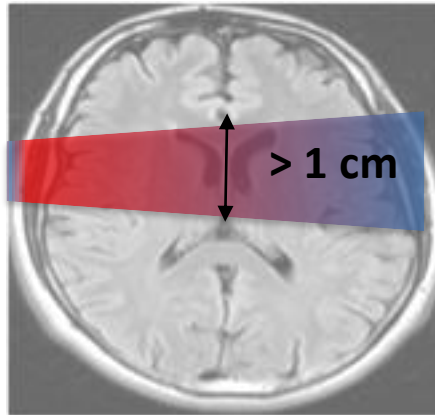
irradiating a brain tumor with protons

Source: Newhauser and Zhang, *The physics of proton therapy*, Phys Med Biol 2015

Clinical proton minibeams
are used for
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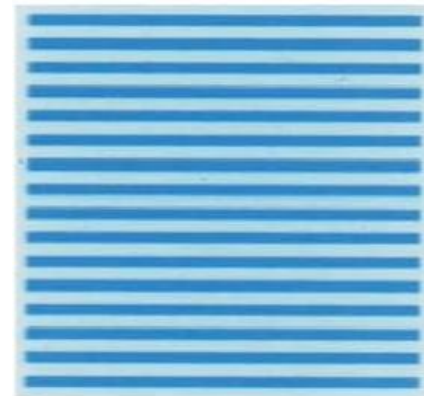
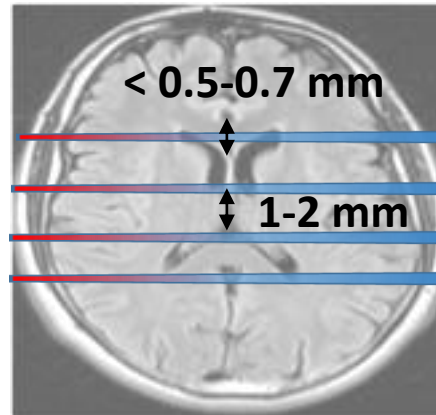
Standard RT

large beam sizes
($> 1 \text{ cm}^2$)
+
homogeneous
dose distributions



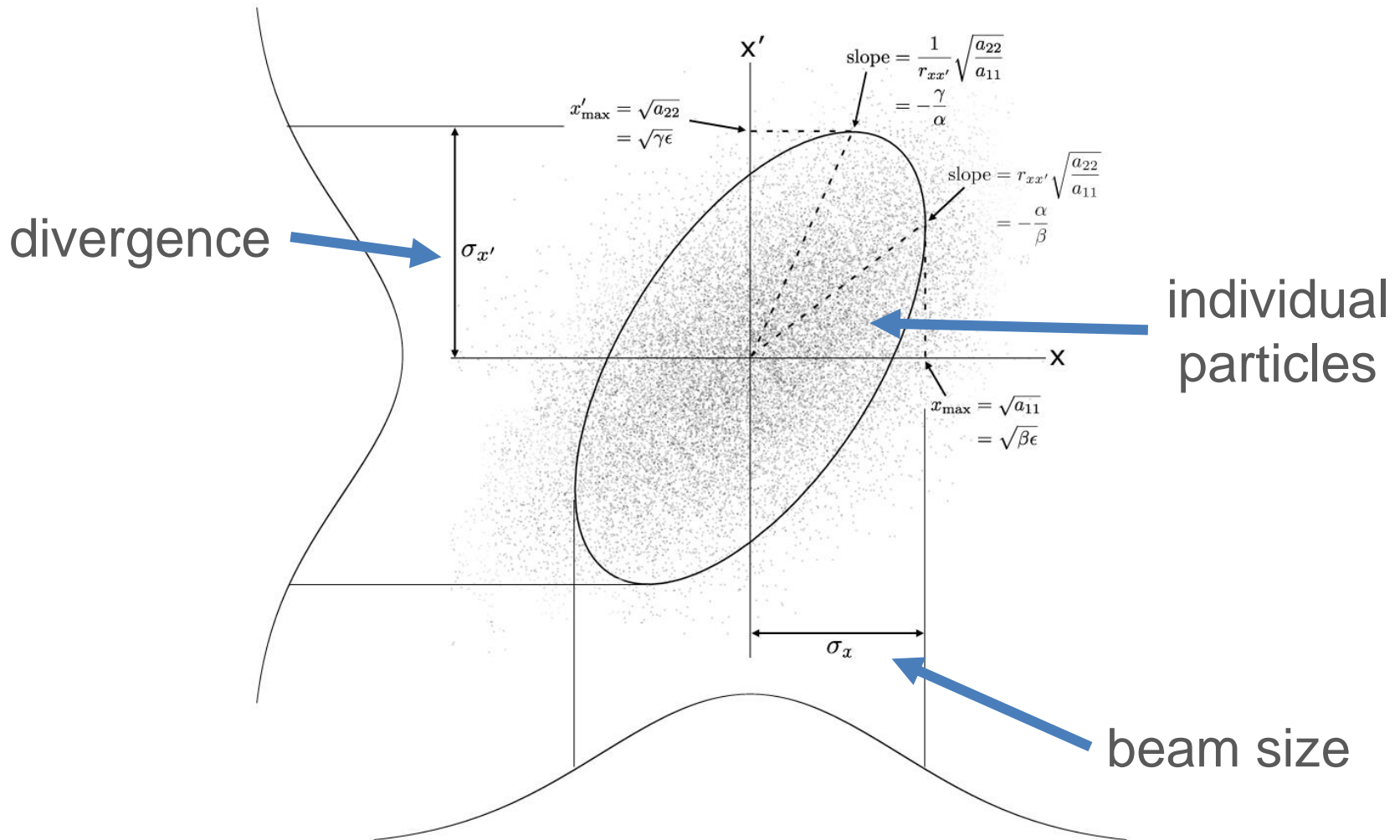
Spatially fractionated RT

**very narrow
beam sizes**
separated by
areas of low dose
+
heterogeneous
distributions



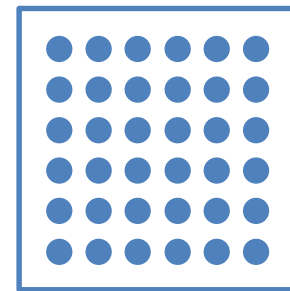
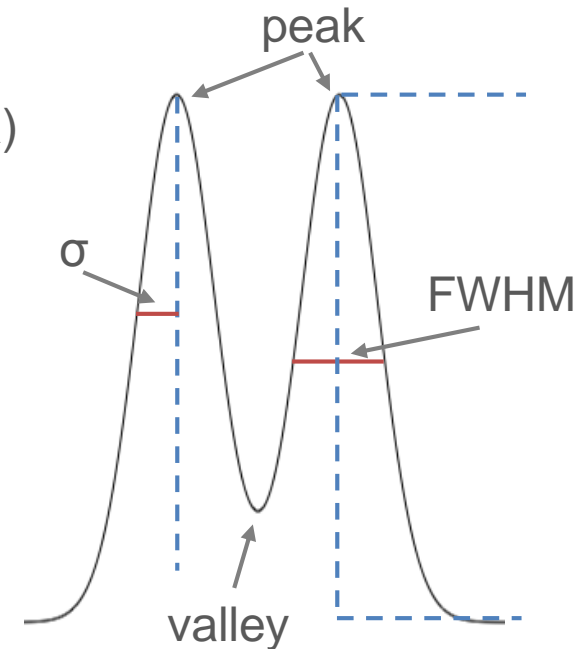
→ tolerance of
normal tissue
increases

Beam ellipse in phase space



Vocabulary for SFRT:

- peaks and valleys: peak-to-valley dose ratio (**PVDR**)
- beam width: σ , full width at half maximum (**FWHM**)
- GRID therapy
 - 2D “grid” of beams
- microbeam RT (MRT)
 - 1D “array” of beams
 - beam width 25 – 75 μm
- minibeam RT (MBRT)
 - 1D “array” of beams
 - beam width 300 μm – 1 mm



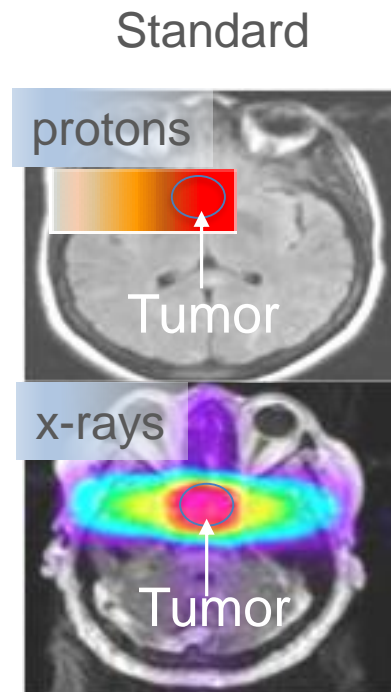
2D grid



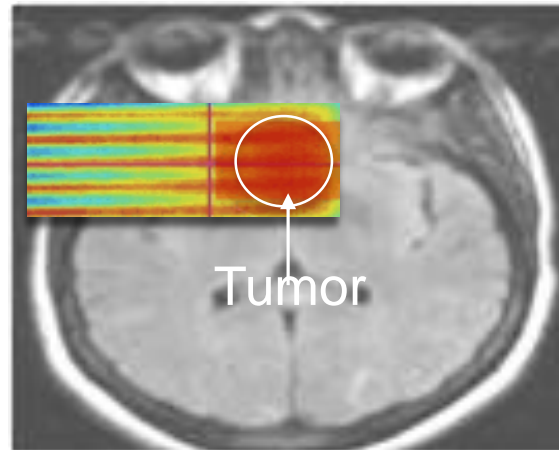
1D array

Our proposal: a novel approach in disruption with standard RT
(Prezado et al 2013)

MBRT + superior dose distribution of protons

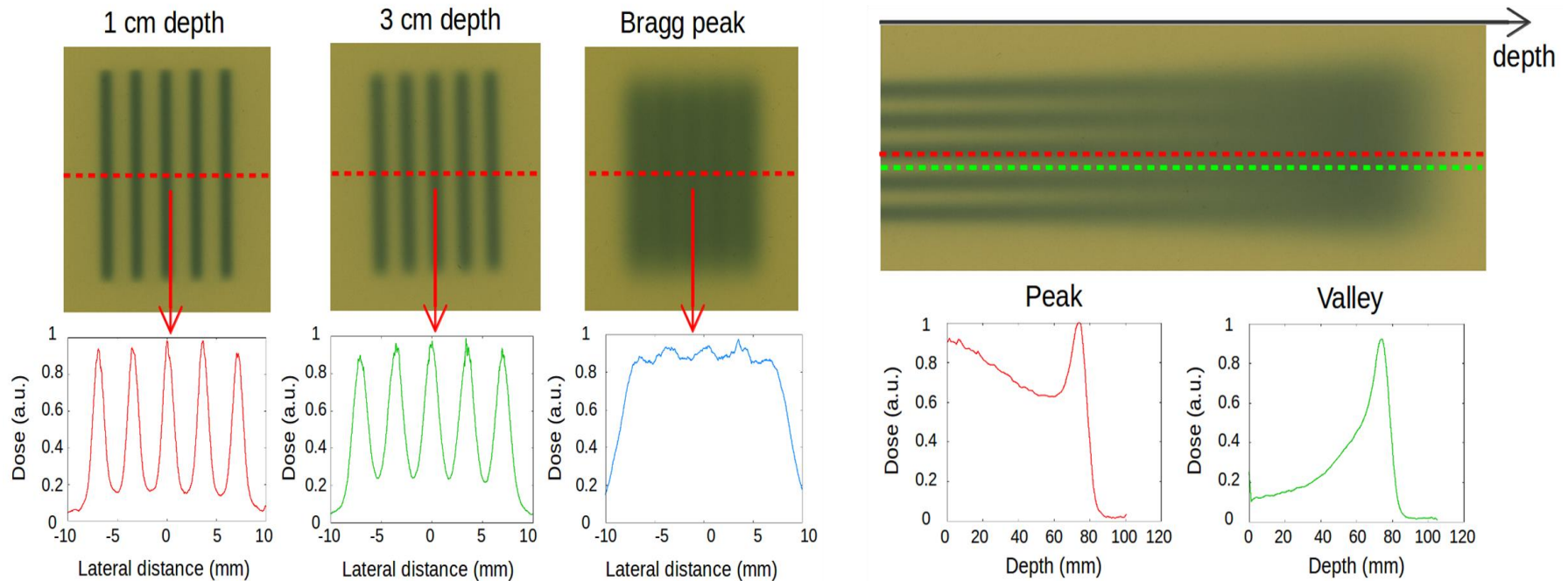
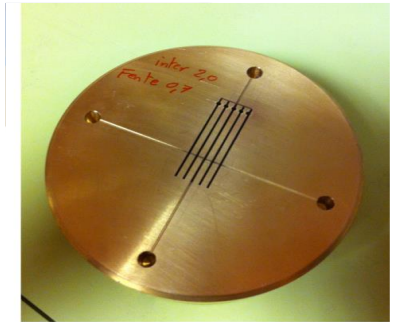


Proton minibeam radiation therapy (pMBRT)



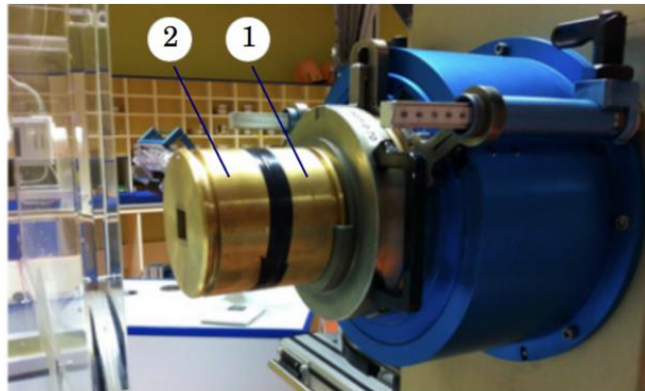
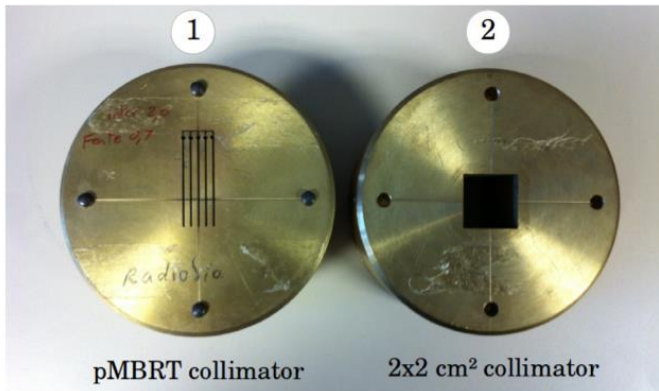
Homogeneous dose in the tumour
+
Spatial fractionation in normal tissue
+
Biological advantages of protons

- experimental proof of concept: dose distributions assessed with gafchromic films (Peucelle et al, Med. Phys. 2015)
- minibeam generation: a first prototype with mechanical collimation

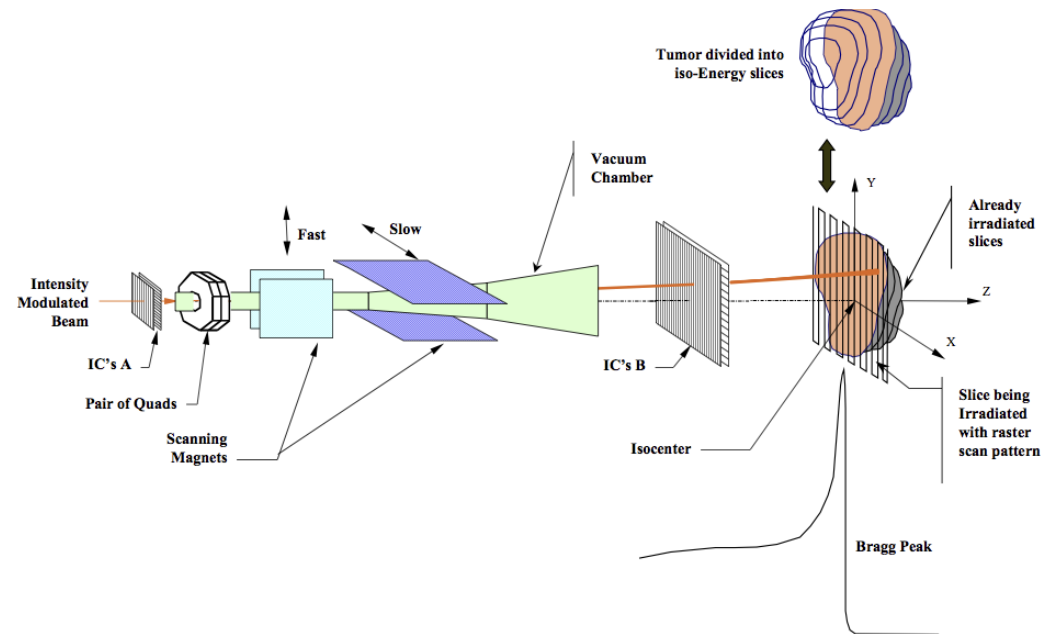


Source: Peucelle et al., Proton minibeam radiation therapy: Experimental dosimetry evaluation, Med Phys 2015

Mechanical collimation



Magnetic focussing



schematic of a PBS (pencil beam scanning) nozzle

Source: Peucelle, *Spatial fractionation of the dose in charged particle therapy*, PhD thesis; Marchand et al., *IBA proton pencil beam scanning: an innovative solution for cancer treatment*, Proceedings of EPAC, Vienna, 2000.

Mechanical collimation

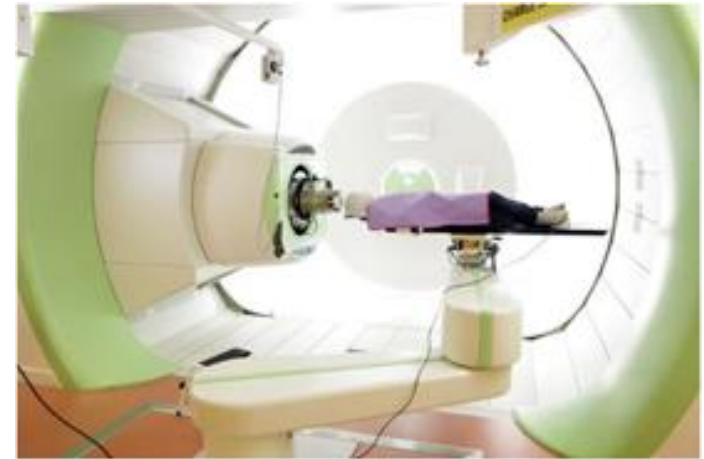
- inefficient
- inflexible (possibly new collimator for different tumors and different energies)
- production of harmful secondary particles (neutrons) close to patient

Magnetic focussing

- full beam used to irradiate tumor
 - higher dose rate
 - higher PVDR expected
 - basically like PBS
- BUT** beam much (>10x) smaller
- *main challenge:*
generate (sub-)millimetric beams at clinical energies/accelerators and beamlines (existing facilities are designed to deliver beam spots ≥ 1 cm FWHM)

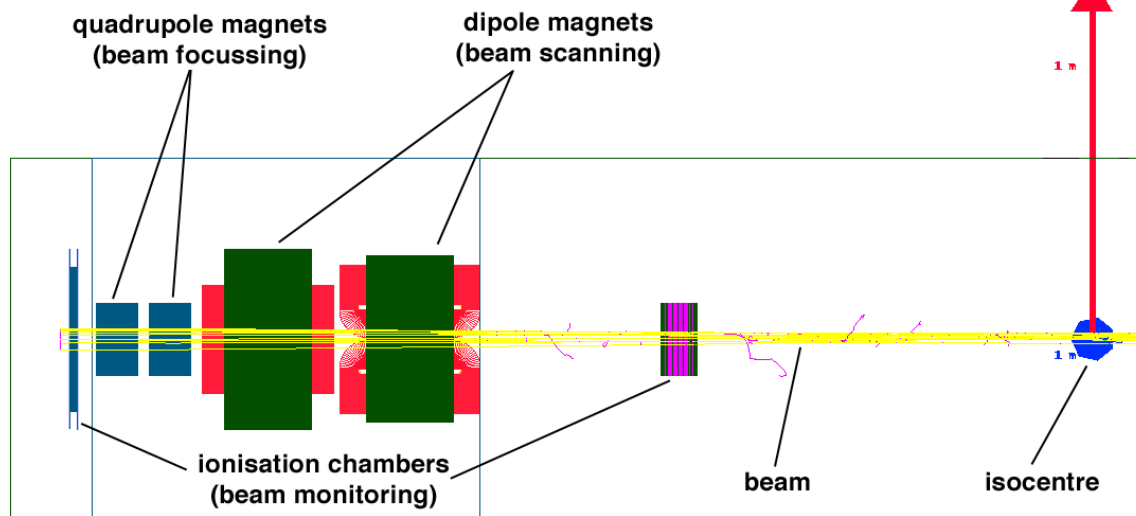
Centre de protonthérapie d'Orsay (CPO)

- more than 7700 patients treated since 1991
- IBA 230 MeV cyclotron
- treat with 70 to 230 MeV proton beams

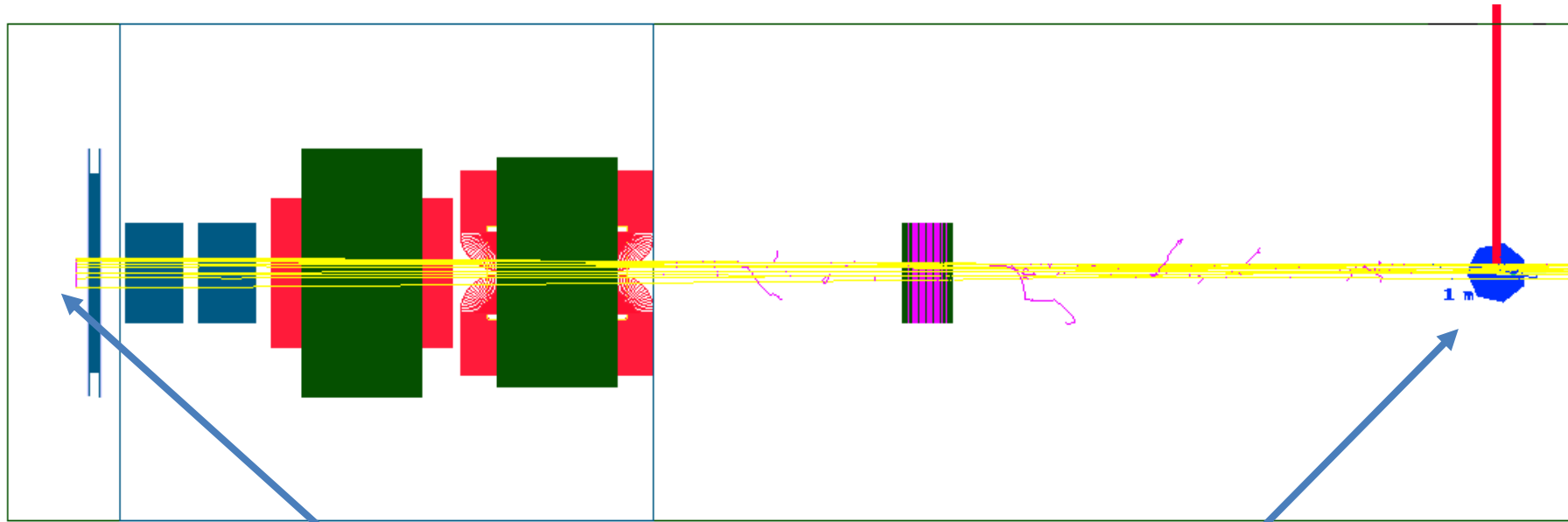


Source: Centre de protonthérapie d'Orsay

Schematic of pencil beam scanning (PBS) nozzle



Current beam sizes at CPO



Beam FWHM at nozzle entrance

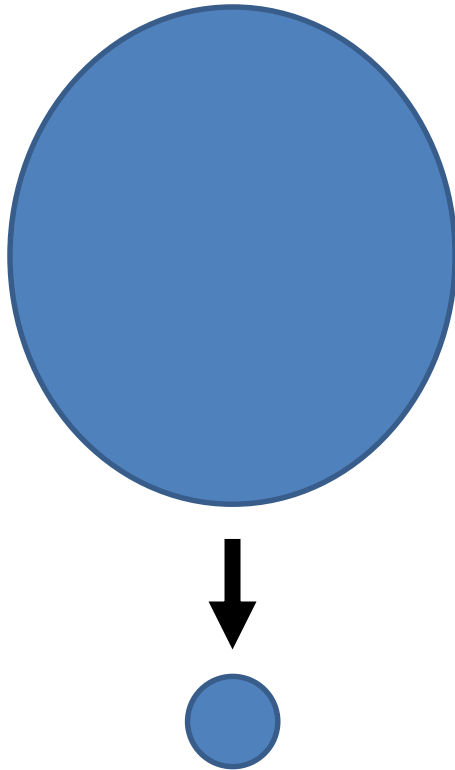
100 MeV: 20.9 / 30.6 mm
200 MeV: 9.3 / 13.3 mm

Beam FWHM at isocentre

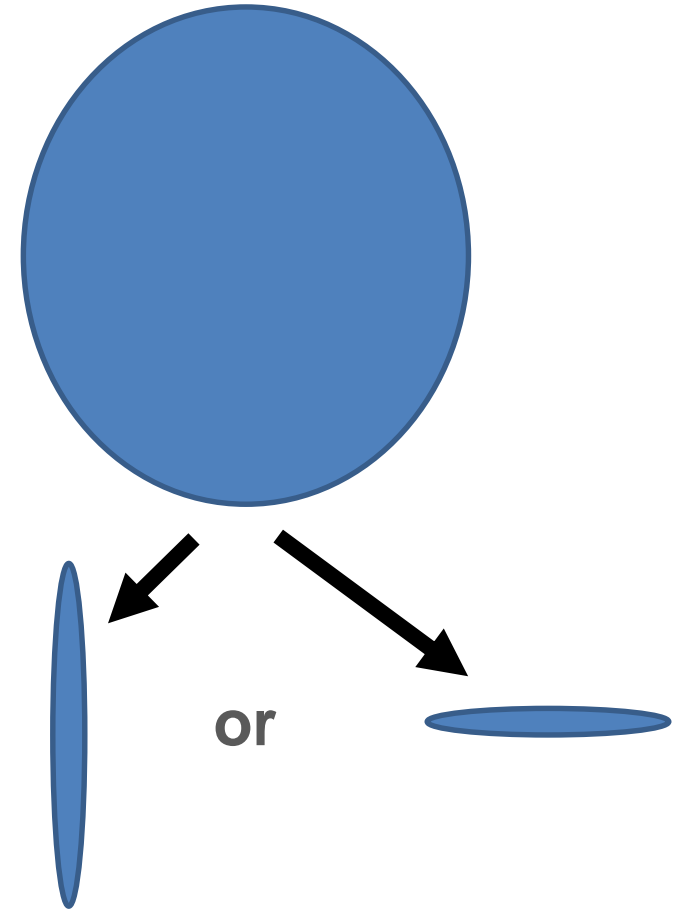
100 MeV: 18.2 / 17.6 mm
200 MeV: 10.5 / 9.9 mm

Reduction by a factor 10-20 required!

symmetrically small

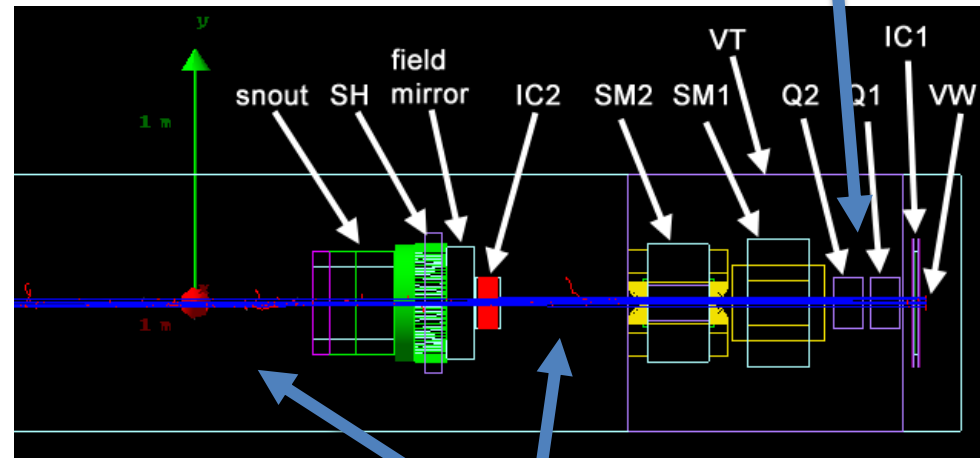
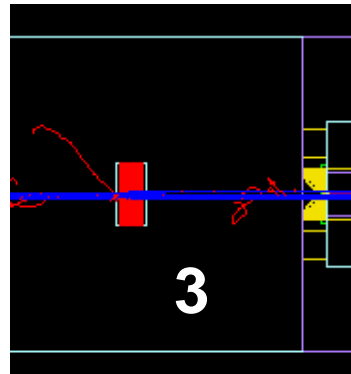
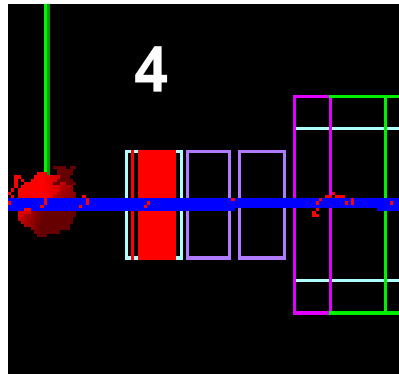


unidirectionally small



starting from PBS nozzle at CPO:

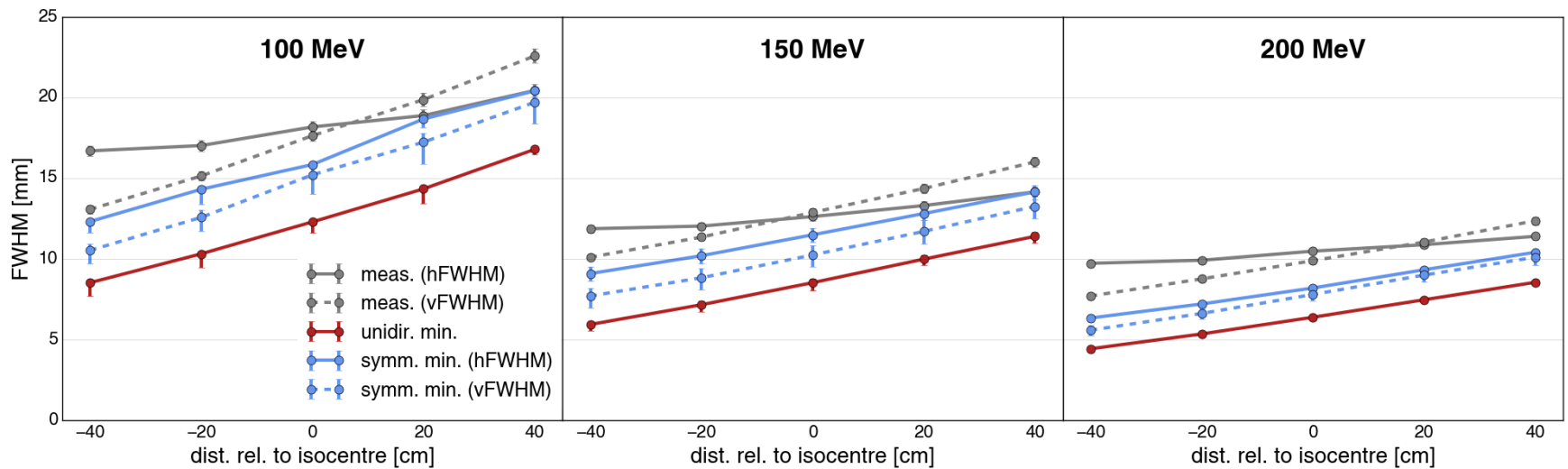
- 1) change magnetic fields (quadrupoles)
- 2) remove air from beam path (not practically feasible)
- 3) reduce distance to target
- 4) introduce additional focussing magnets

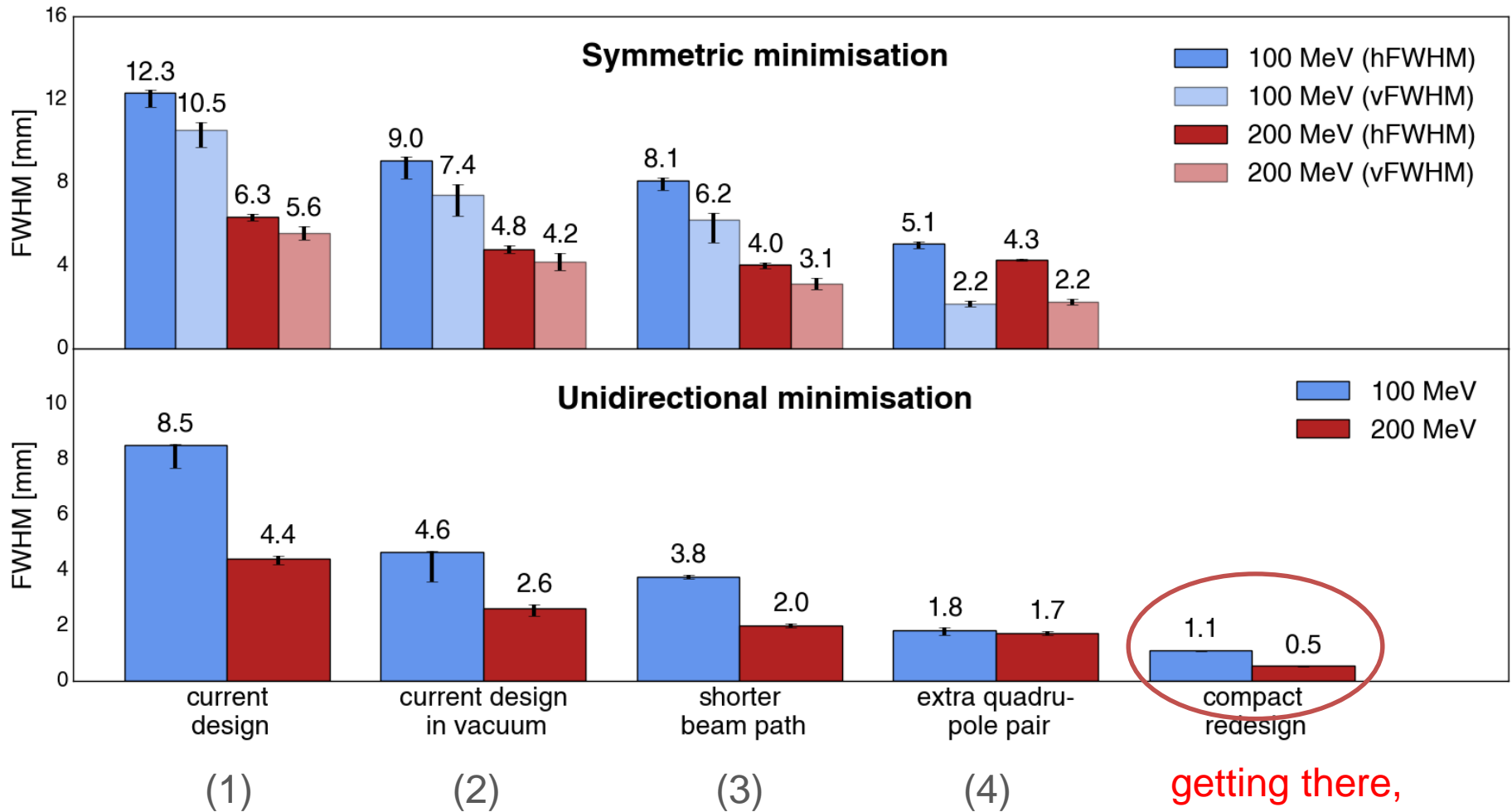


1

2

same nozzle, changing only quadrupole fields (1)

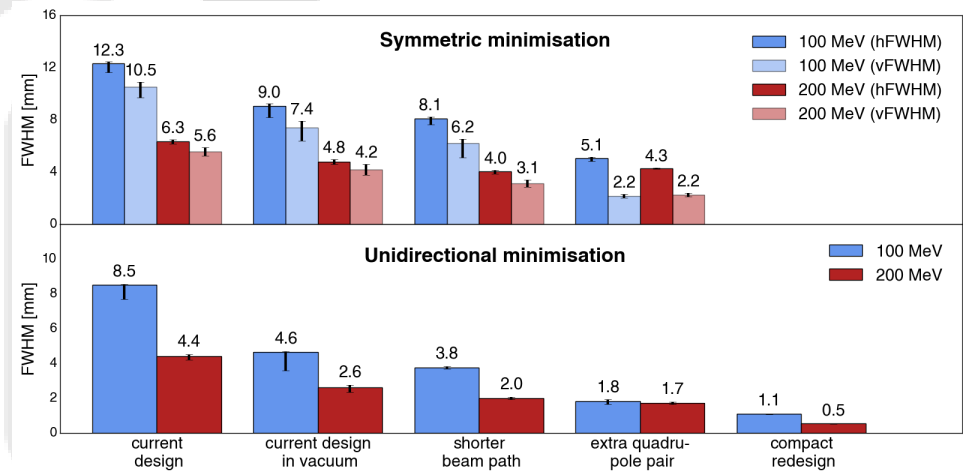
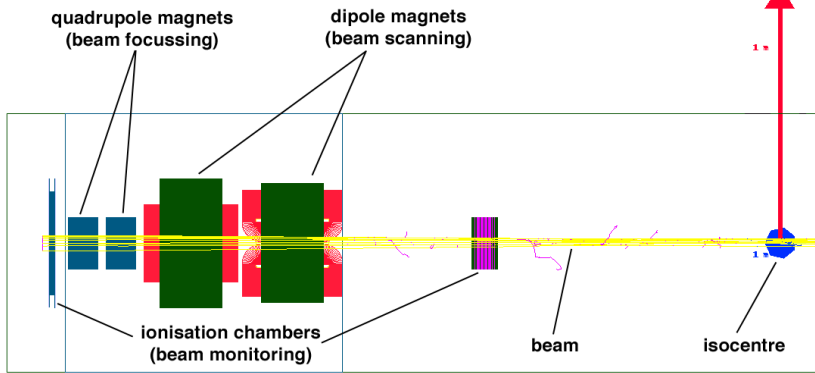




getting there,
but not really satisfactory

- design a new nozzle (more compact, shorter distance to patient)
- define requirements for beam entering nozzle
- check compatibility with existing accelerators/beamlines
- build prototype?

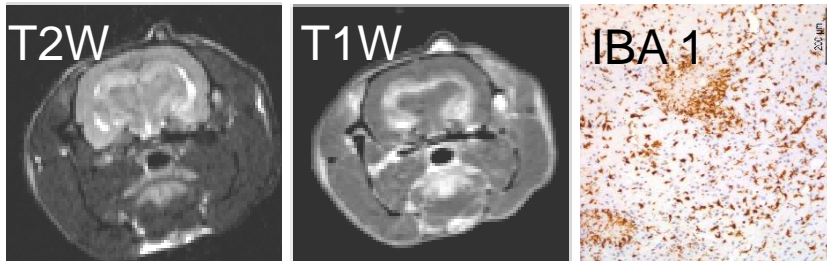
Thank you for your attention!



Whole normal rat brain irradiations (6 months follow up) with 100 MeV proton minibeam

Standard proton therapy (25 Gy/one fraction, n=8)

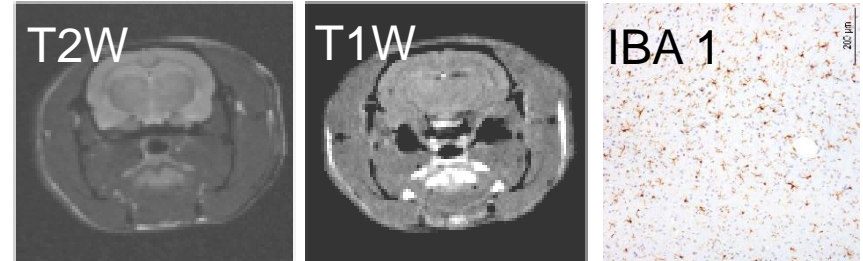
- skin: moist desquamation
- permanent epilation
- important brain damage



pMBRT

(58 Gy peak dose/one fraction, n=8)

- no skin damage
- reversible epilation
- no brain damage observed



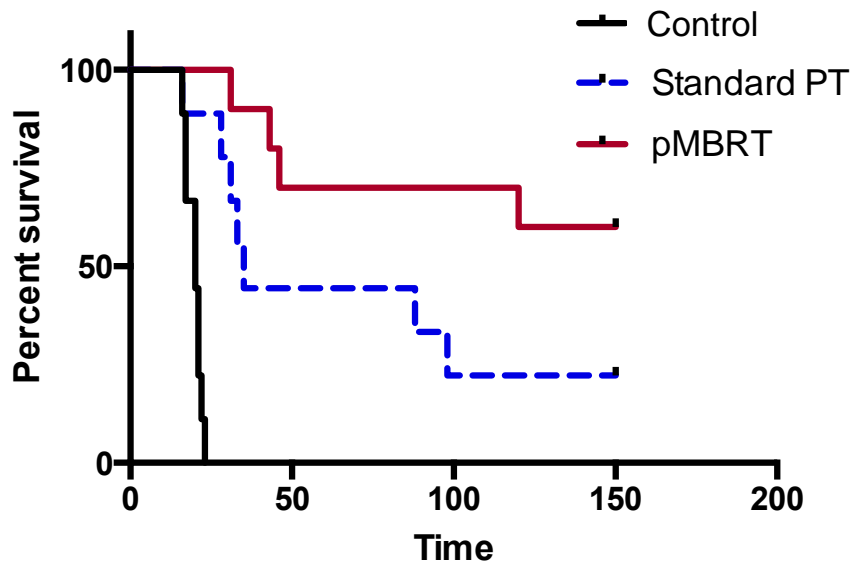
pMBRT offers a net gain in normal tissue resistance

Prezado et al. Scie. Reports 2017

Three groups

- Control (n=9)
- Standard PT (n=9) 25 Gy
- pMBRT (n=9) 25 Gy

IR 4 days after implantation
5000 cells RG2



Median survival

Controls 20 days

Standard 35 days 20 % of long-term survivals (> 6 months)

pMBRT >150 days 60 % of long-term survivals (> 6 months)