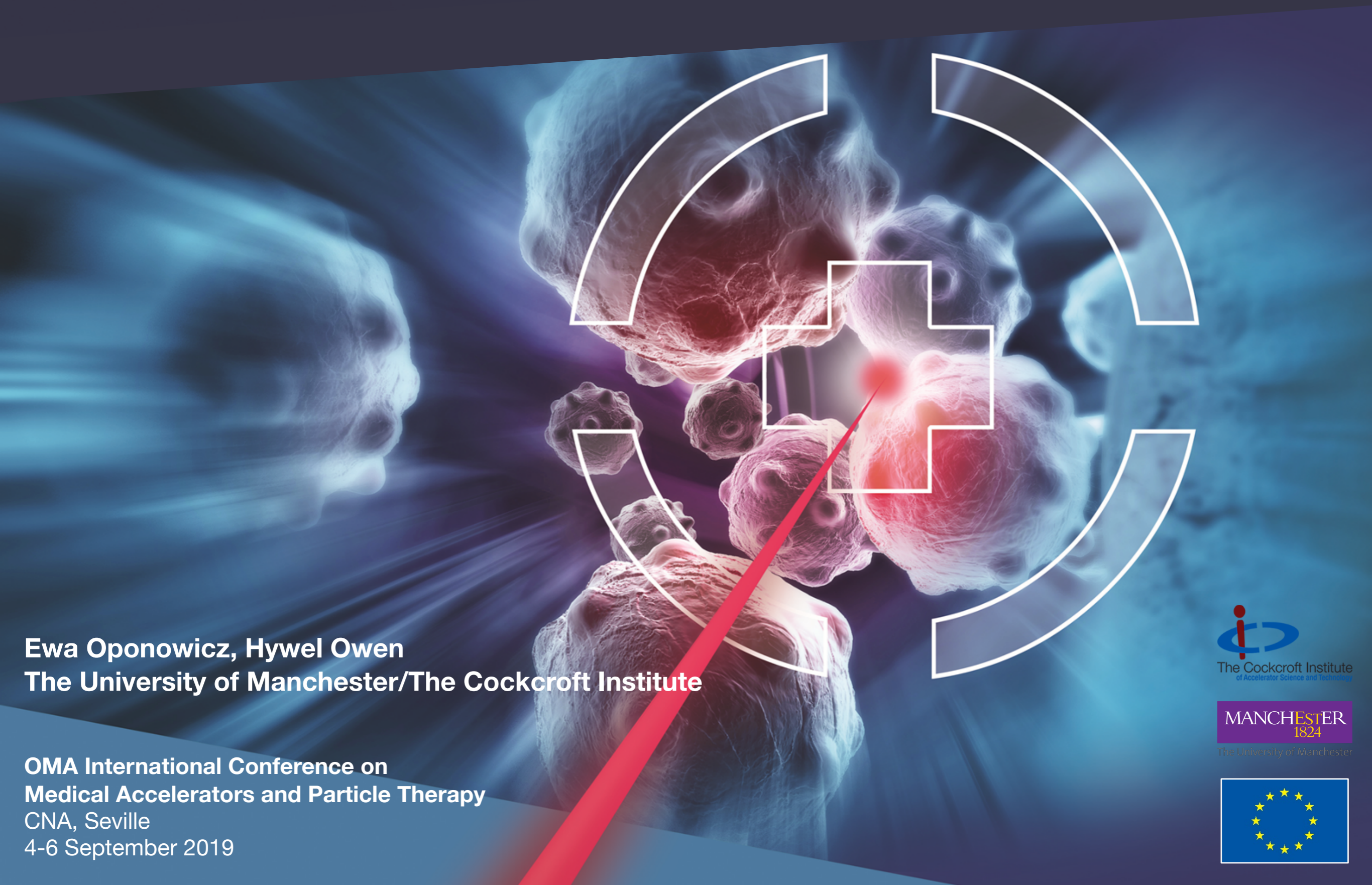




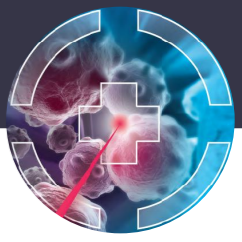
# Superconducting gantry for proton therapy and imaging



**Ewa Oponowicz, Hywel Owen**  
**The University of Manchester/The Cockcroft Institute**

**OMA International Conference on  
Medical Accelerators and Particle Therapy**  
CNA, Seville  
4-6 September 2019





## Main components:

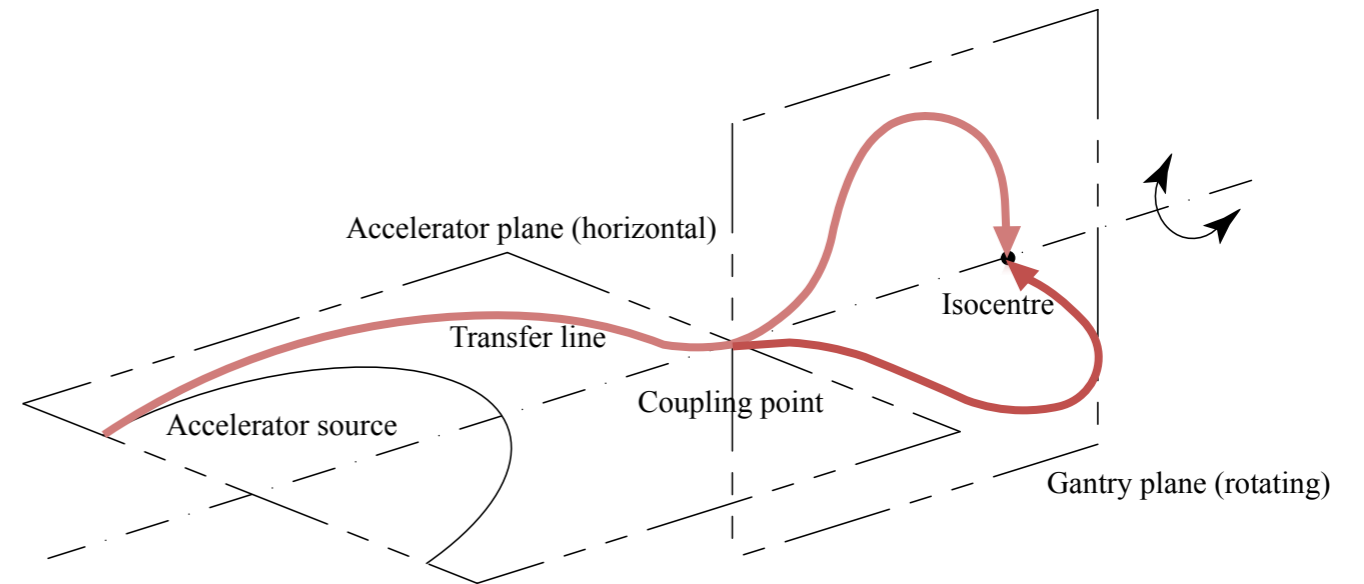
- Magnets (bending/focusing)
- Beam scanning system (downstream/upstream/combined)
- Beam instrumentation devices
- Vacuum and cooling systems
- Mechanical support system
- Drive mechanism

## Typical proton gantry:

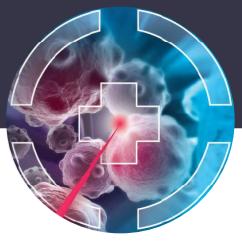
- Max. 250 MeV kinetic energy
- Isocentric (centre of min. sphere crossed by beam axis)
- Delivering beam to a supine patient on a rotating table
- 180/360 deg rotation capability
- Normal-conducting
- Occupies volume of 8m x 8m x 8m

## Imaging prior to the treatment:

- MRI
- X-ray CT



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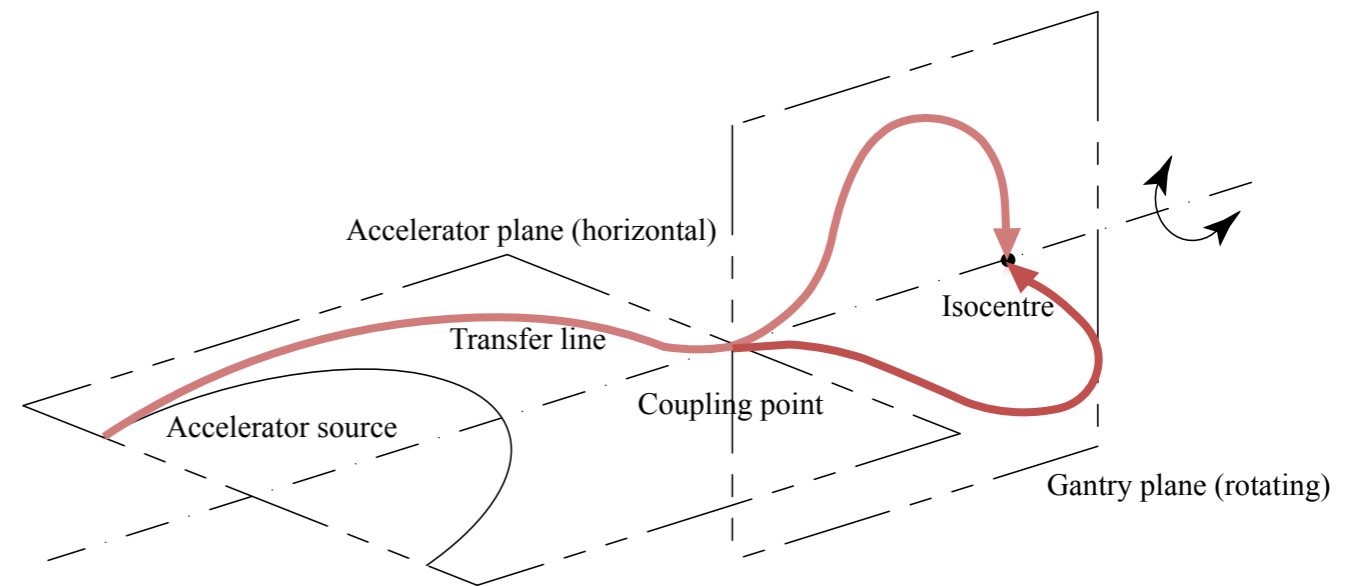
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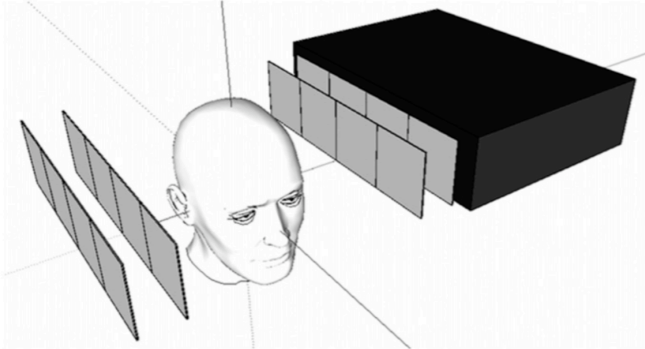
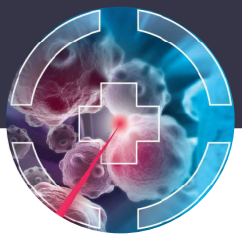
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➔ Conversion from HU to effective electron density: proton range uncertainty of up to 3.5%



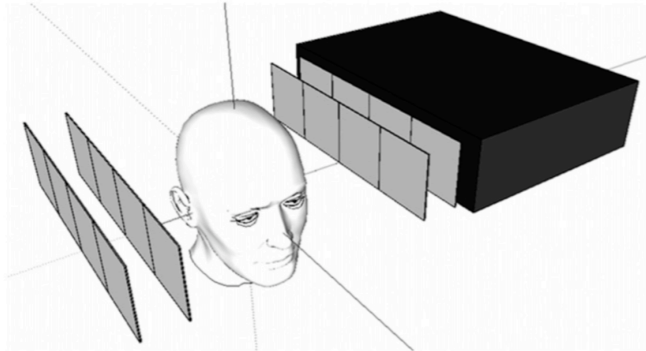
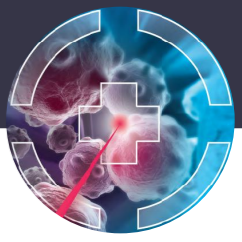
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## Proton CT:

- Proposed in 1963, not available in clinics yet
- Proton-tracking (detecting energy deposition and trajectories of individual particles)
- Proton-integrating (measuring integrated energy deposition)

## Proton CT scan of head:

- $10^8$  protons ( $\sim 0.2$  pA) compared to  $10^{11}$  protons for a single treatment fraction
- 1.4 mGy radiological dose compared to 50 mGy for an X-ray CT



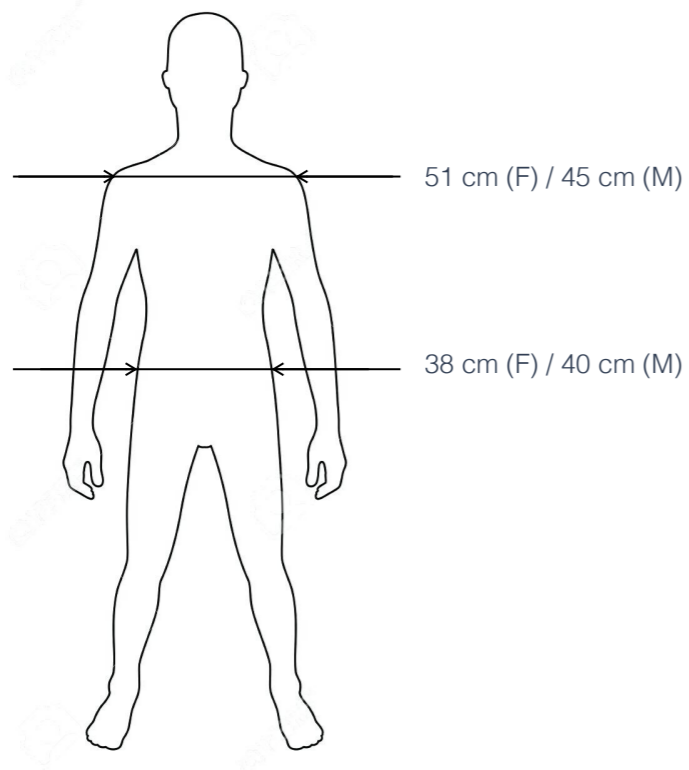
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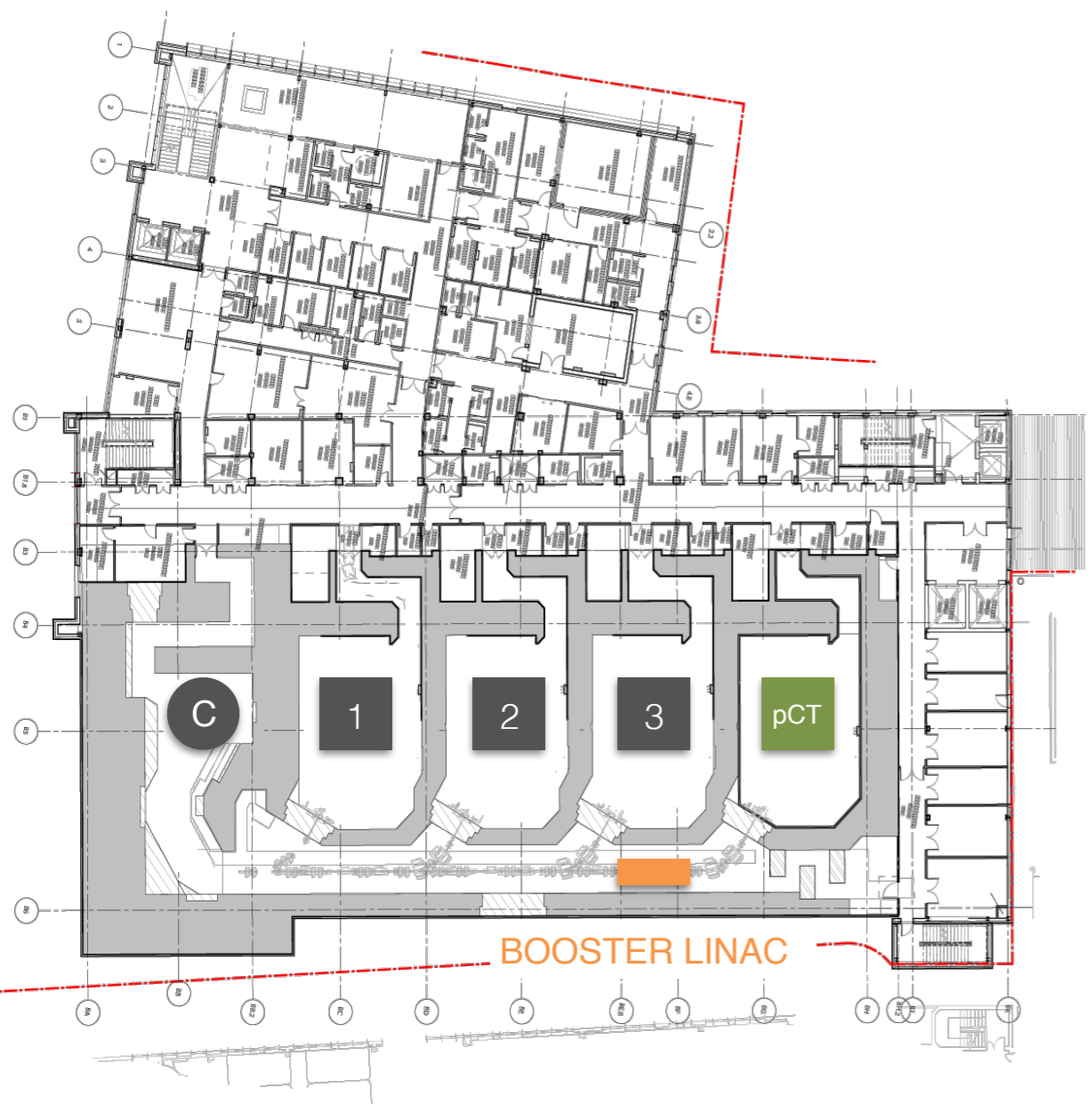
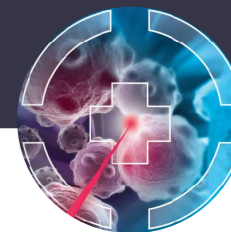
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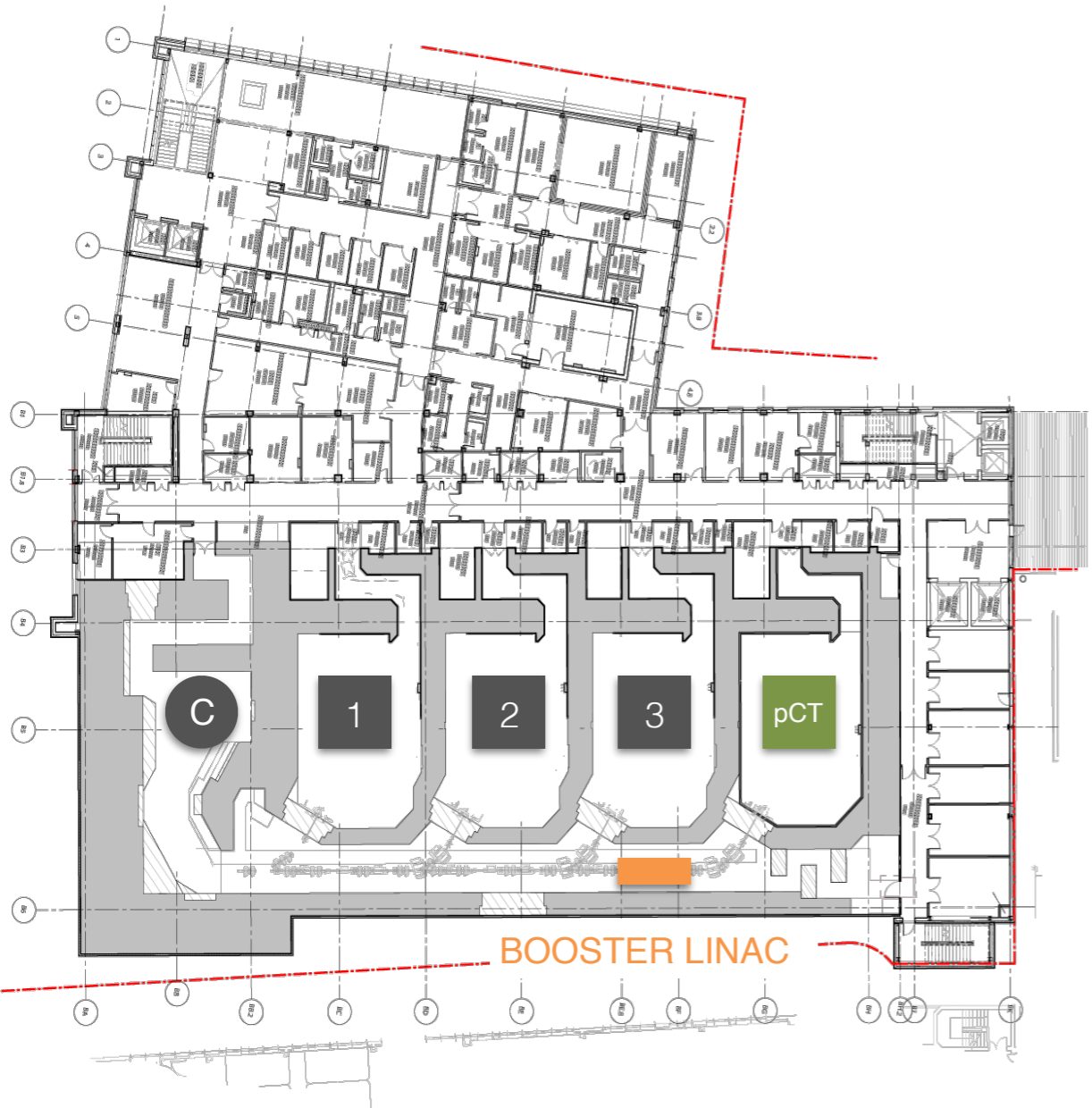
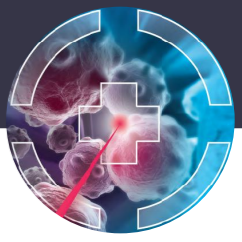
## Protons ranges in A-150 tissue equivalent plastic:

- 250 MeV:  $\sim 33.5$  cm
- 330 MeV:  $\sim 53.1$  cm



## Proton Therapy Centre at the Christie Hospital in Manchester:

- Opened in 2018
- 80 patients treated
- 3 treatment rooms, 1 research room
- 254 MeV SC Varian cyclotron

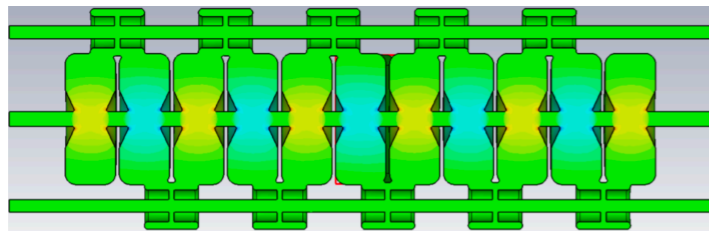


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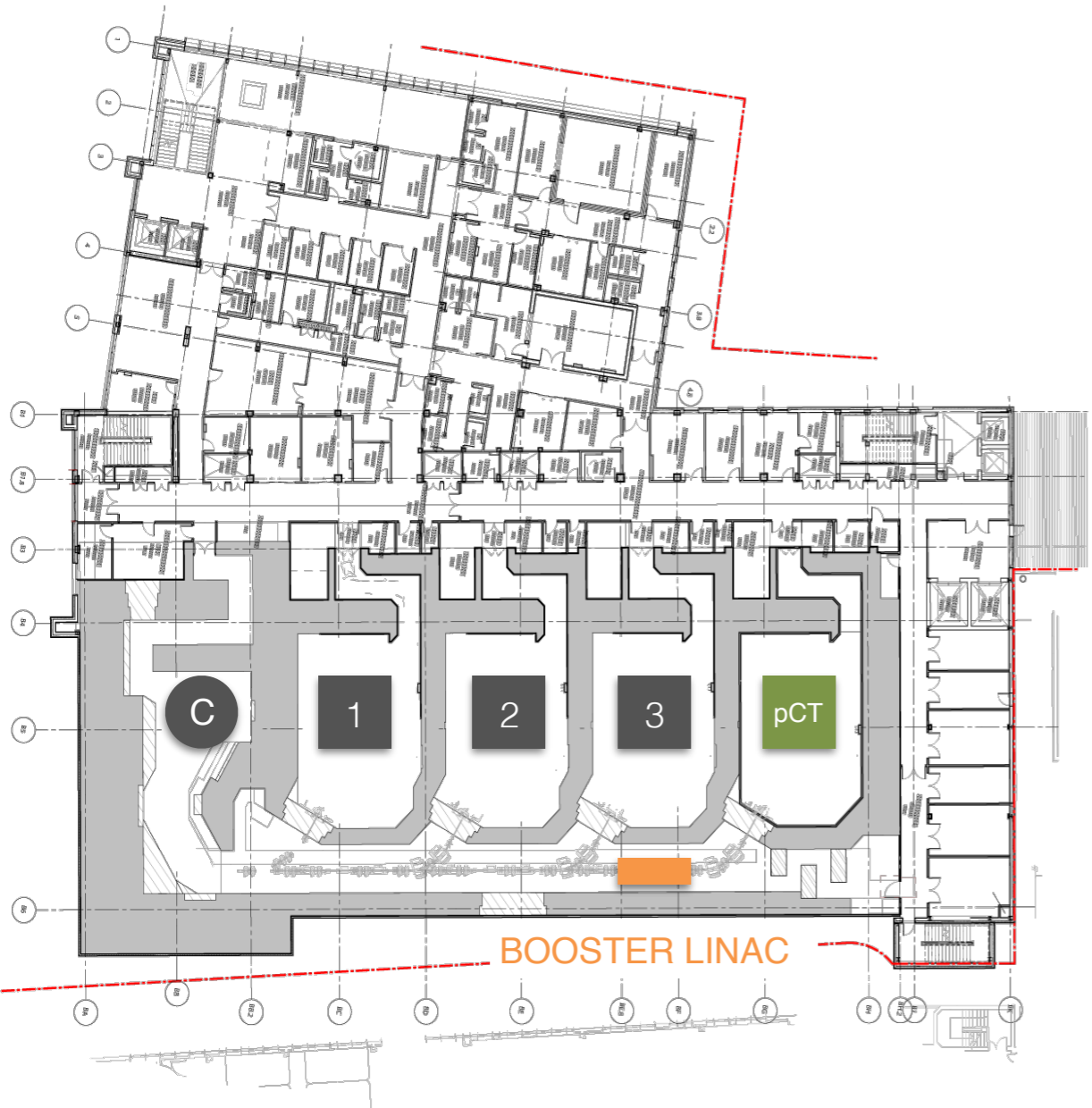
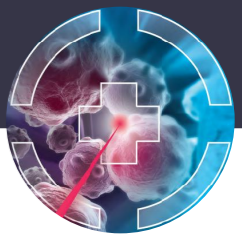
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## ProBE: Proton Boosting Extension for Imaging and Therapy:

- 250 MeV to 350 MeV
- Two 54 V/m S-band structures
- Less than 3 m long
- Before the research room
- Frequency mismatch between cyclotron/linac RF systems - large beam losses (more than 90%)
- Beam losses not problematic for pCT (low beam currents)



R Apsimon et al, Coupled longitudinal and transverse beam dynamics studies for hadron therapy linacs, 2017.

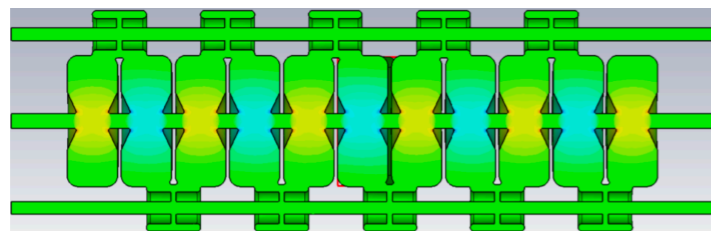


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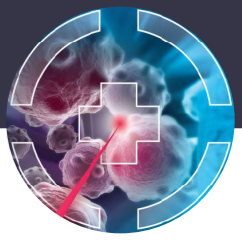


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## pCT gantry requirements:

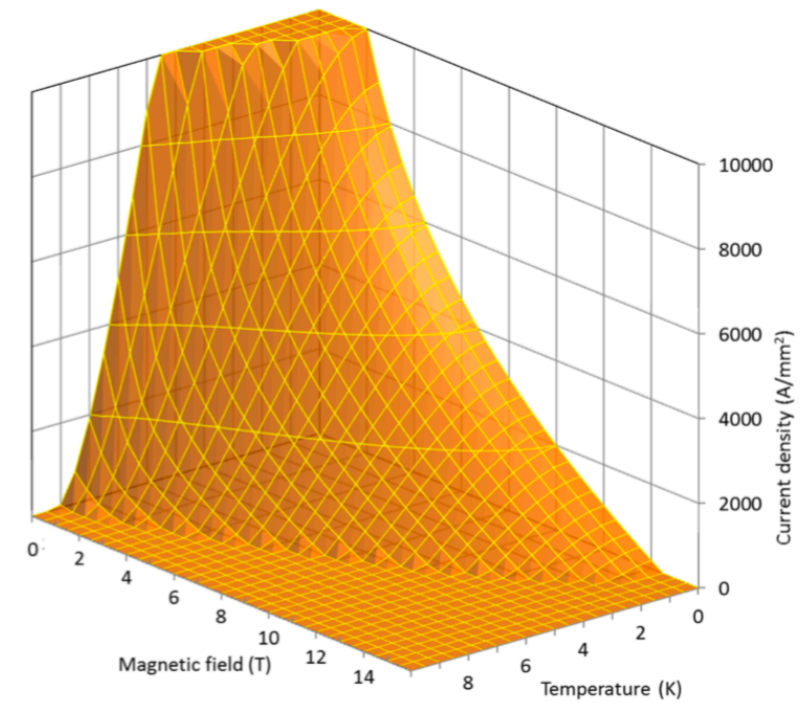
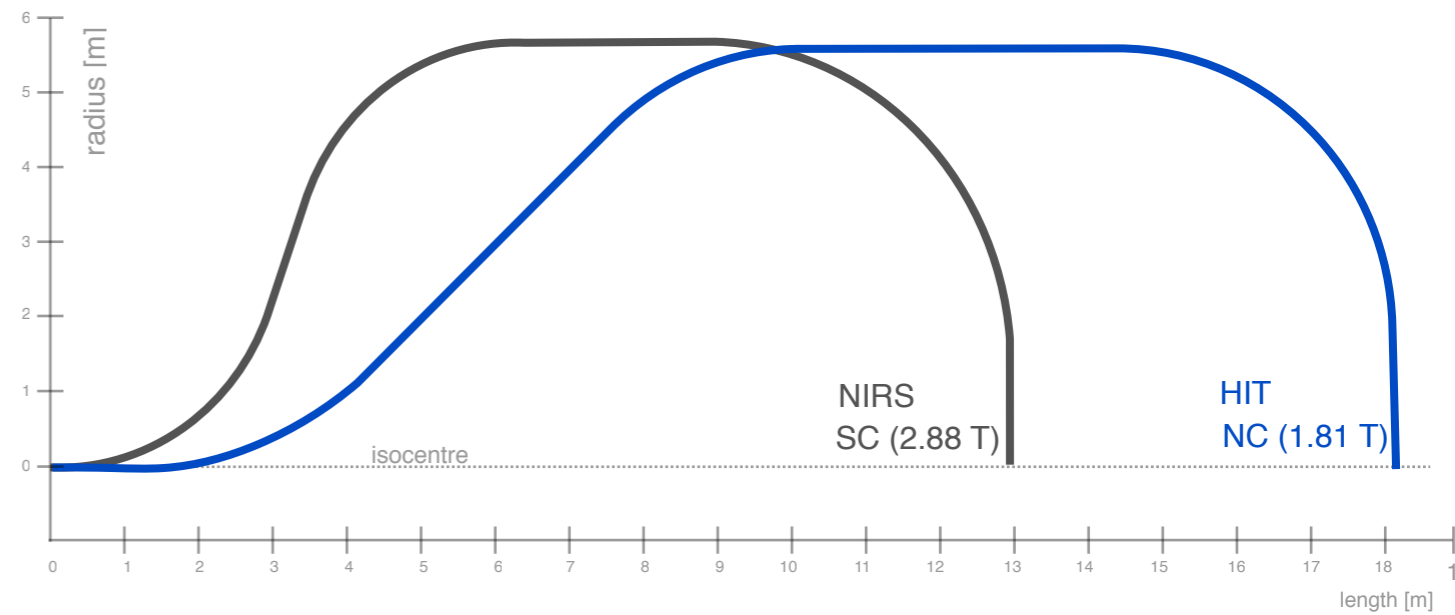
- 2.84 Tm beam rigidity for 330 MeV (2.43 Tm for 250 MeV)
- Source-to-axis distance: min. 2 m
- Downstream pencil beam scanning system
- Occupying the space of a conventional treatment gantry



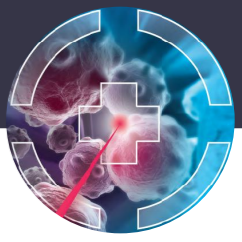


## Advantages:

- **Weight reduction** (300t at NIRS vs 600t at HIT for carbon ions, 25t ProNova vs 200t PSI Gantry 2)
- **Size reduction** for carbon ion therapy / pCT (for protons mostly dictated by beam optics and SAD)
- **Footprint and cost reduction**
- **Lower power consumption** (in SC dipoles comes mainly from AC losses, but refrigeration power needed)
- **Combined function magnets**

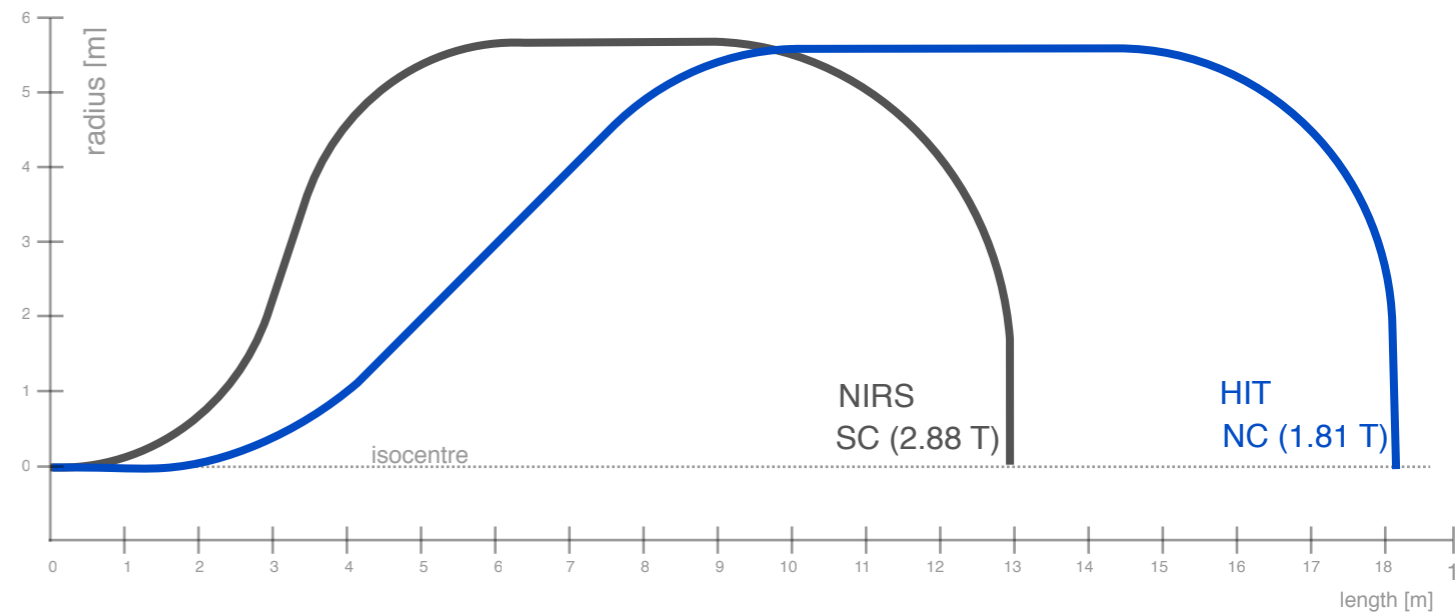


Critical surface of NbTi (P. Ferracin, JUAS 2017)  
L Bottura, A practical fit for the critical surface of NbTi, 1999.



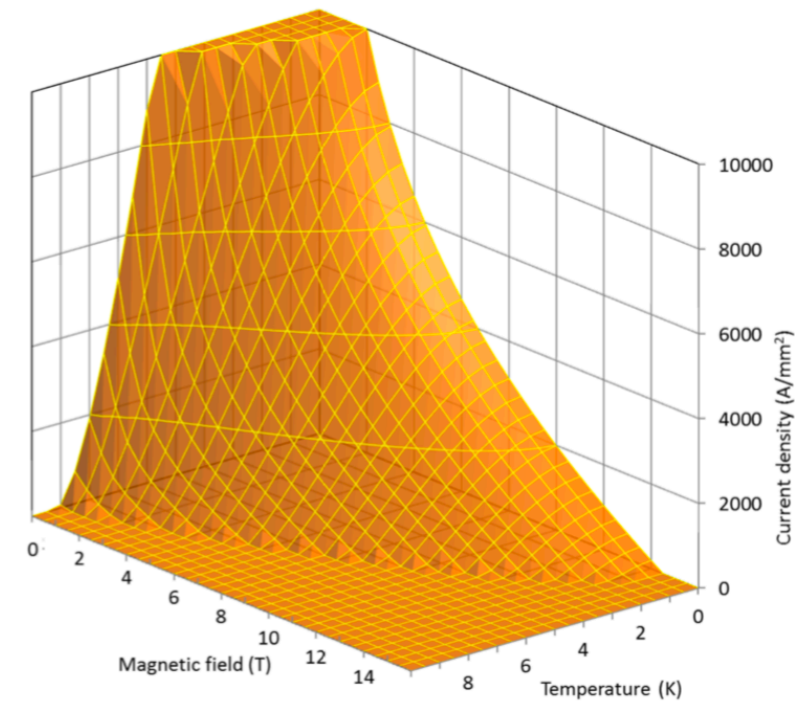
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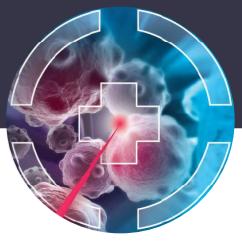


## Challenges:

- **Strong magnetic fields** (stray fields, max. 0.5 mT at isocentre)
- **Slower ramping** (high energy acceptance gantries such - fixed field during treatment/imaging)
- **Cryogenics in a rotating system** (cryogen-free cryocoolers)
- **Quenches** (proton therapy facilities require high machine availability, typically more than 95%)

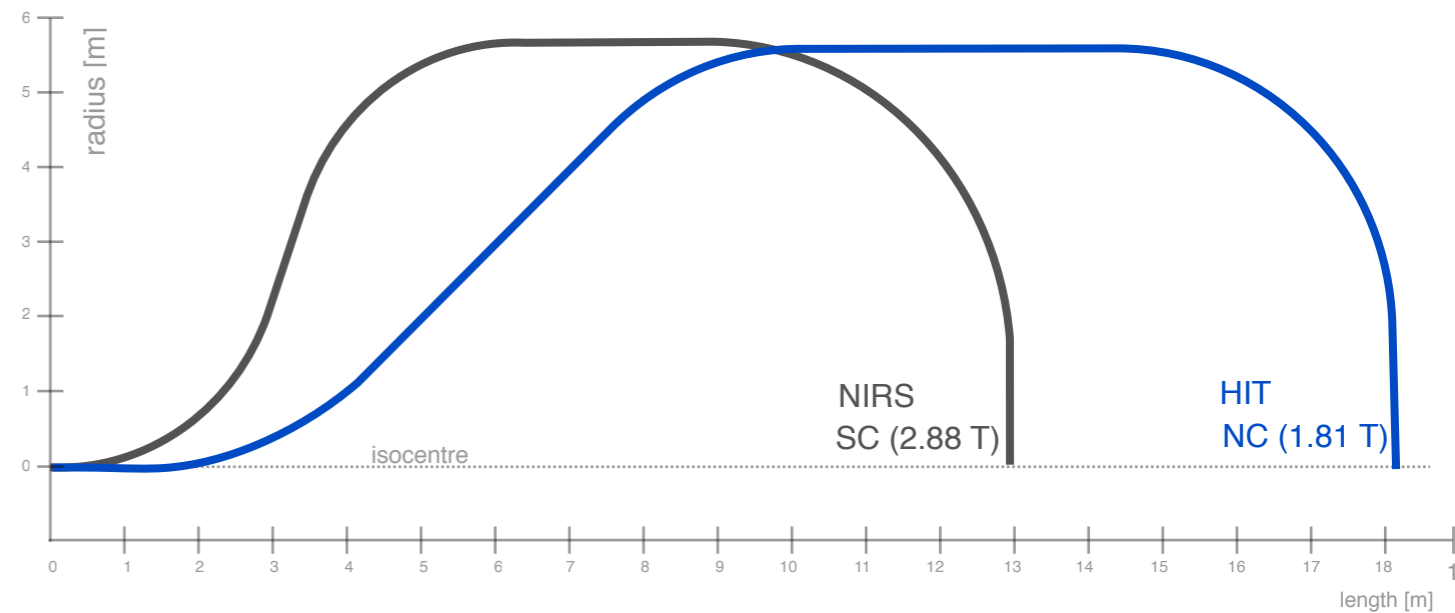


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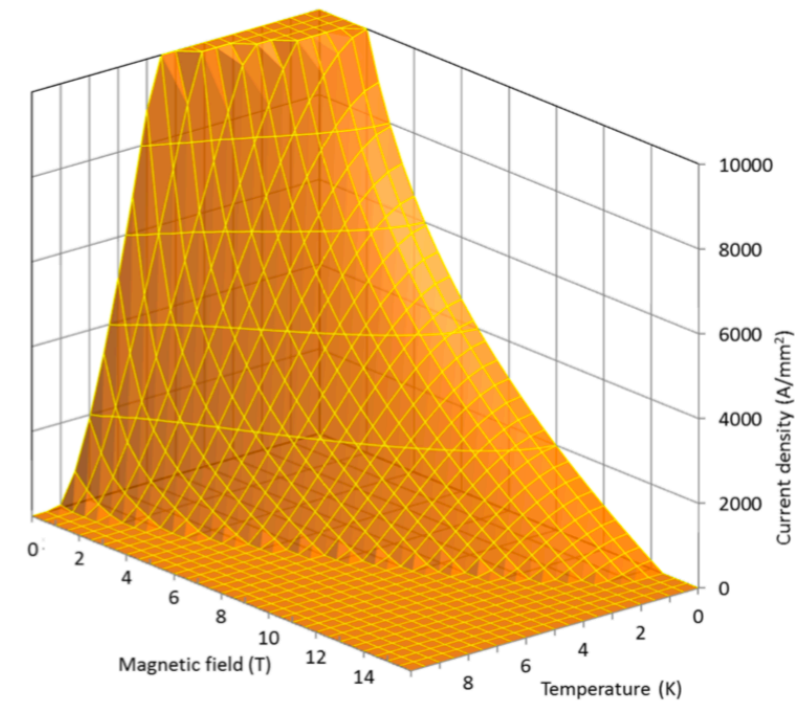


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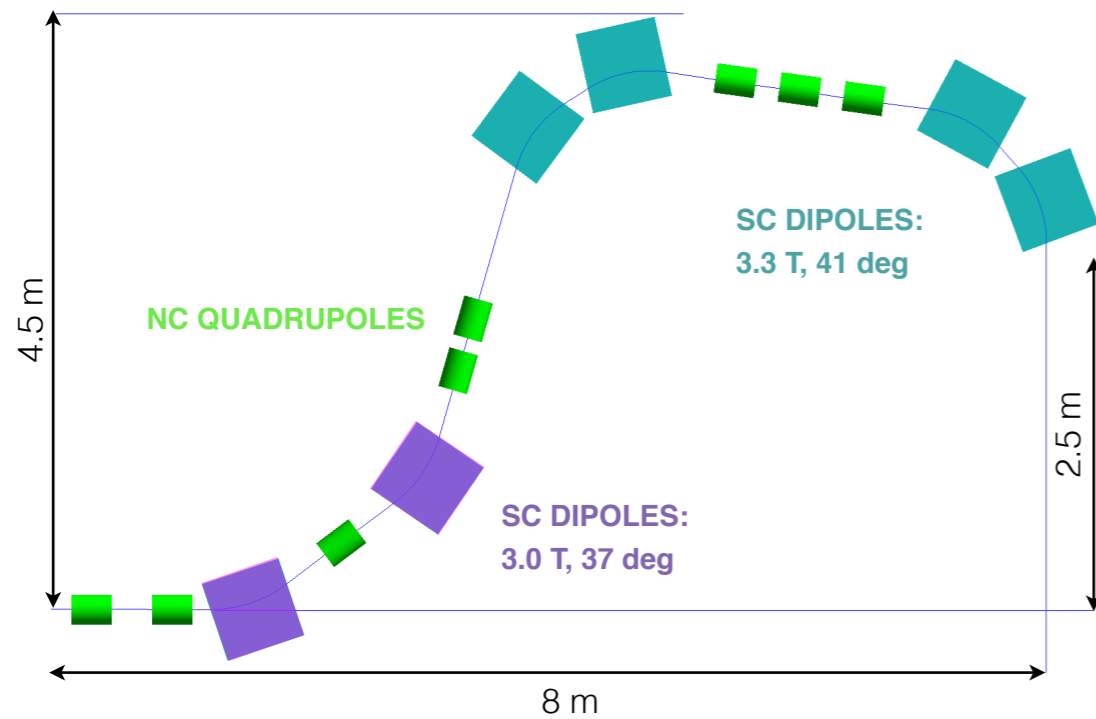
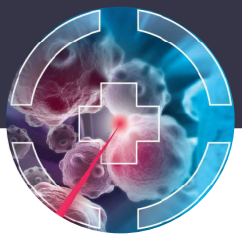
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## Example in proton therapy: ProNova Solutions SC360

- 250 MeV protons
- Radius: more than 4 m, length: less than 5 m
- No considerable size reduction (235 m<sup>3</sup> compared to 250 m<sup>3</sup> Gantry 2 at PSI)
- Max. magnetic field 4 T in superconducting dipoles

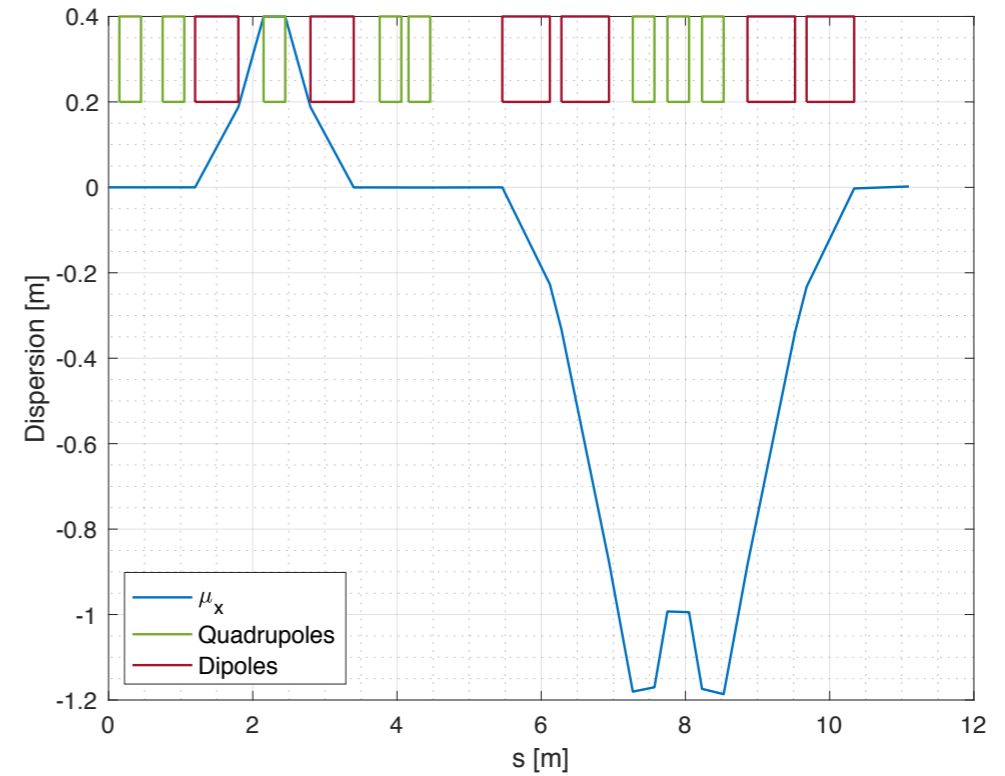
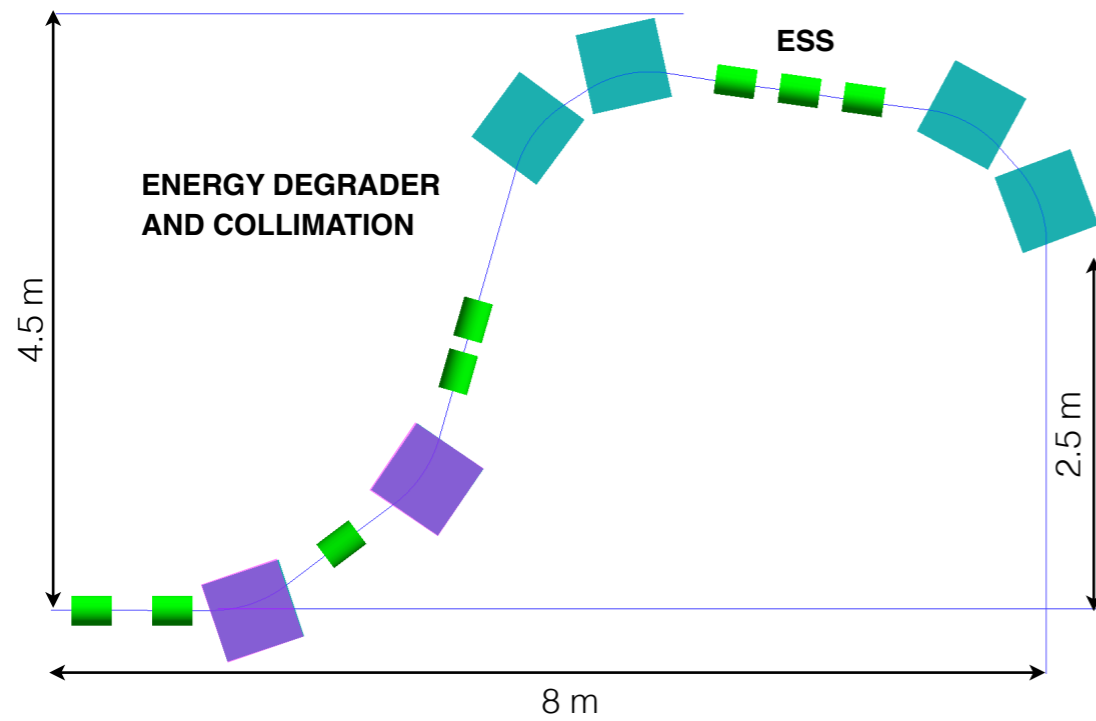
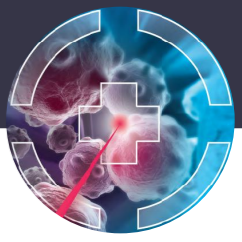


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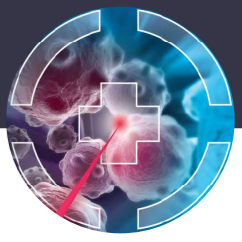
## Basic gantry parameters

Length of dipole Type A	0.6 m
Integrated field over physical length (A)	3.0 T
Length of dipole Type B	0.66 m
Integrated field over physical length (B)	3.3 T
Maximum quadrupole coefficient	27 T/m
Gantry length	8 m
Gantry radius	4.5 m
Source-to-axis distance	> 2 m



## pCT gantry:

- Double achromat design
- Local and global achromaticity
- Beam degrader and collimation system integration



CYCLOTRON EXIT 



MMAP1X/2Y 

QMA1 

QMA2 

QMA3 

MMAP5X/6Y 

DEGRADER 

KMA3 

KMA4 

MMAP9X/10Y 

KMA5 

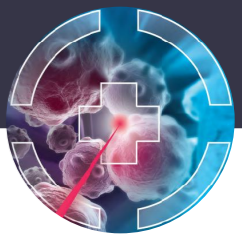
QMA4 

QMA5 

MMAP11X/12Y 

# Energy degrader

PAUL SCHERRER INSTITUT



CYCLOTRON EXIT

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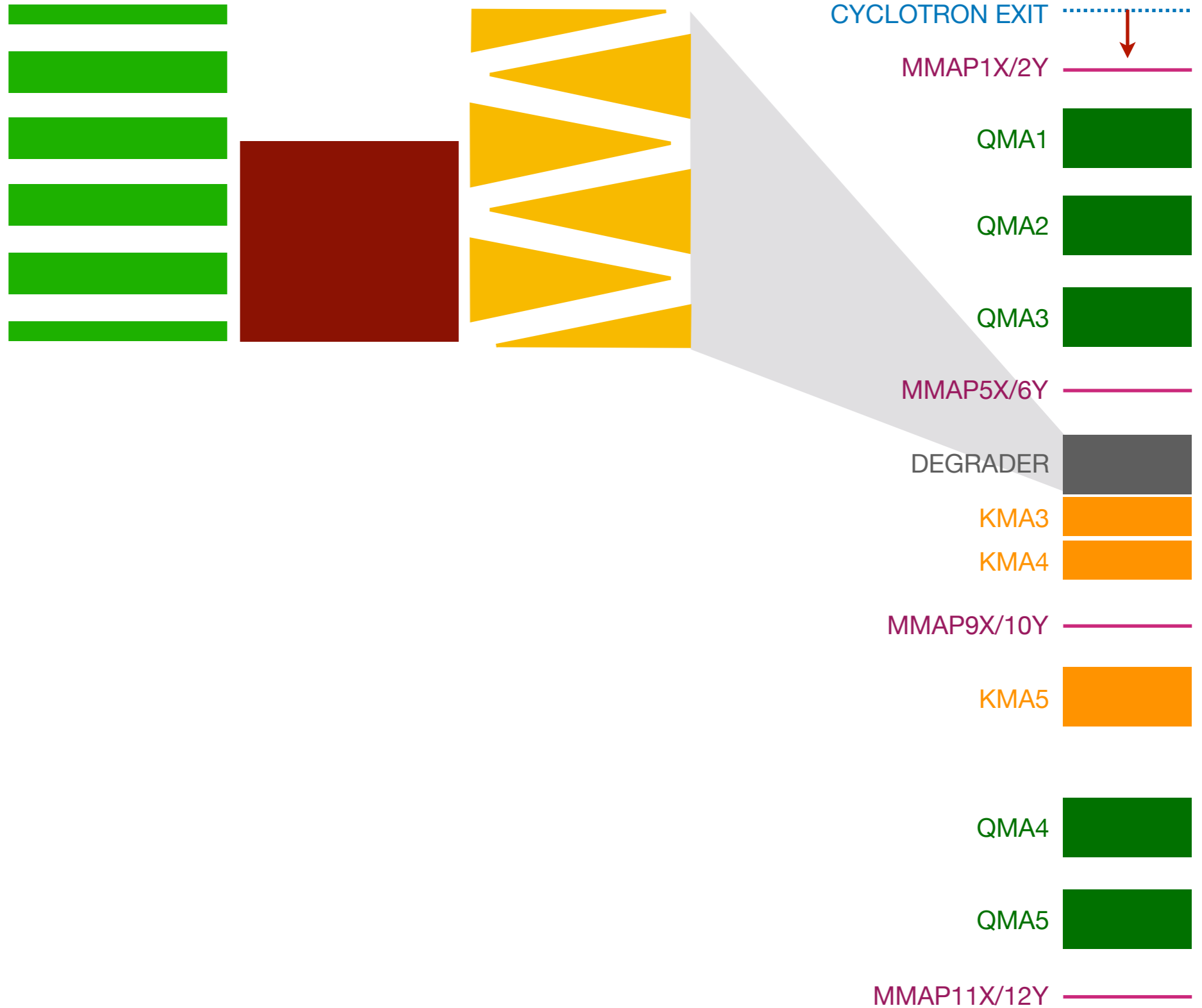
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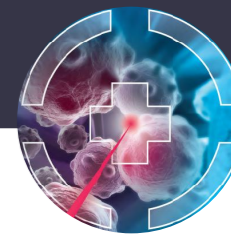
## Degrader properties

Material	Graphite
Density	1.87 g/cm <sup>3</sup>
Ionisation potential	81 eV
A	12.02
Z	6
Full wedge angle	23 deg



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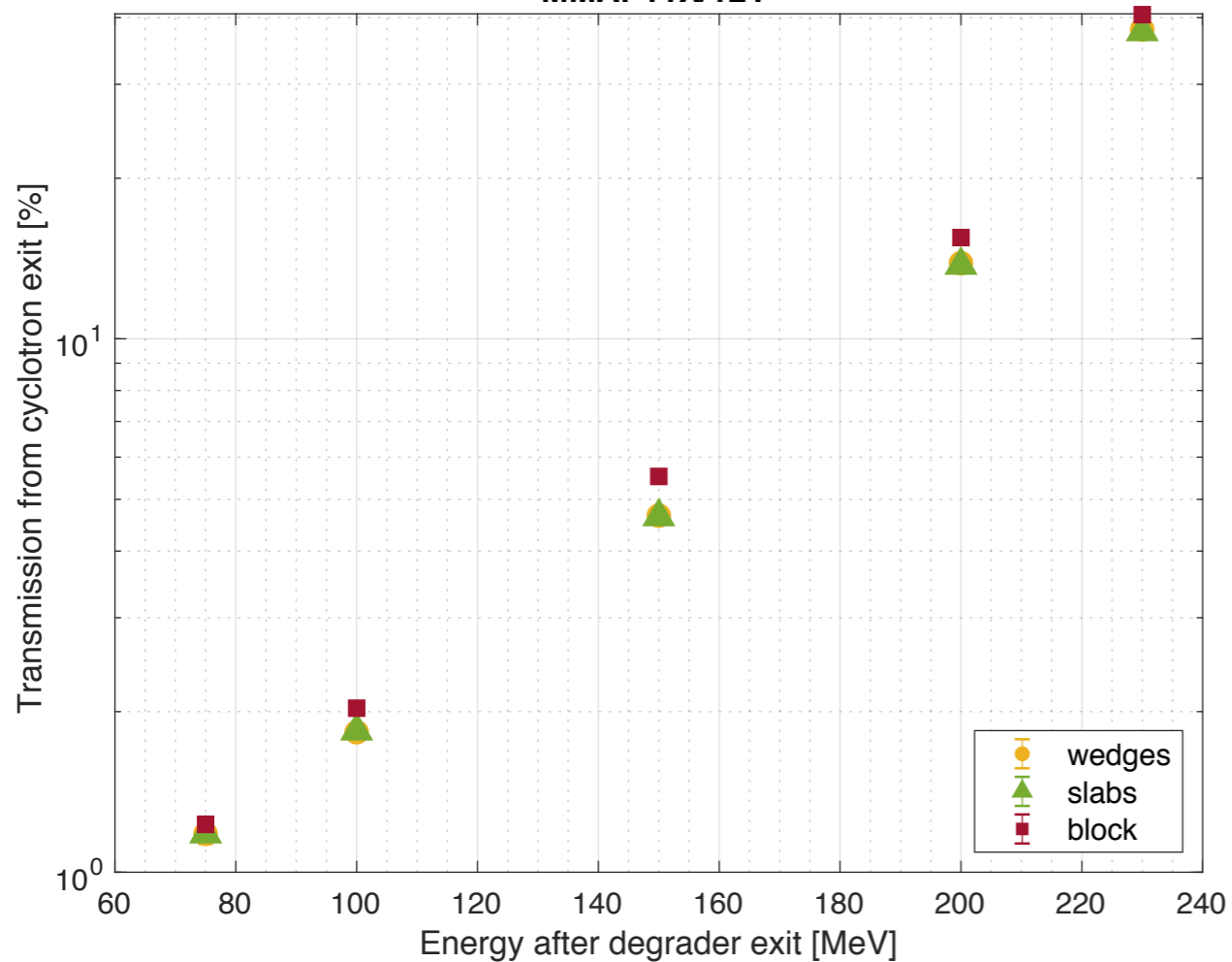
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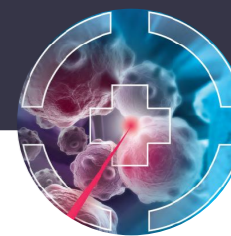
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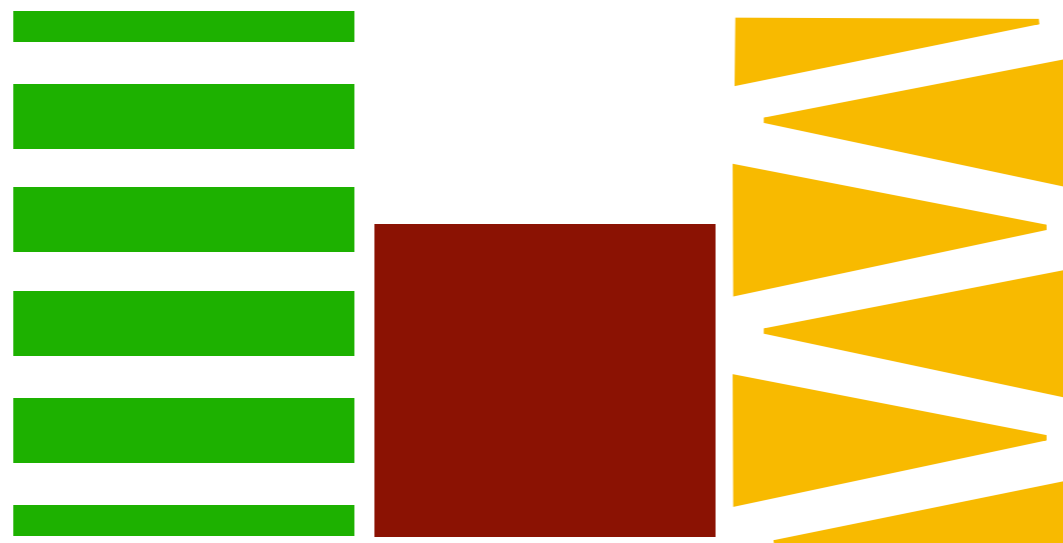
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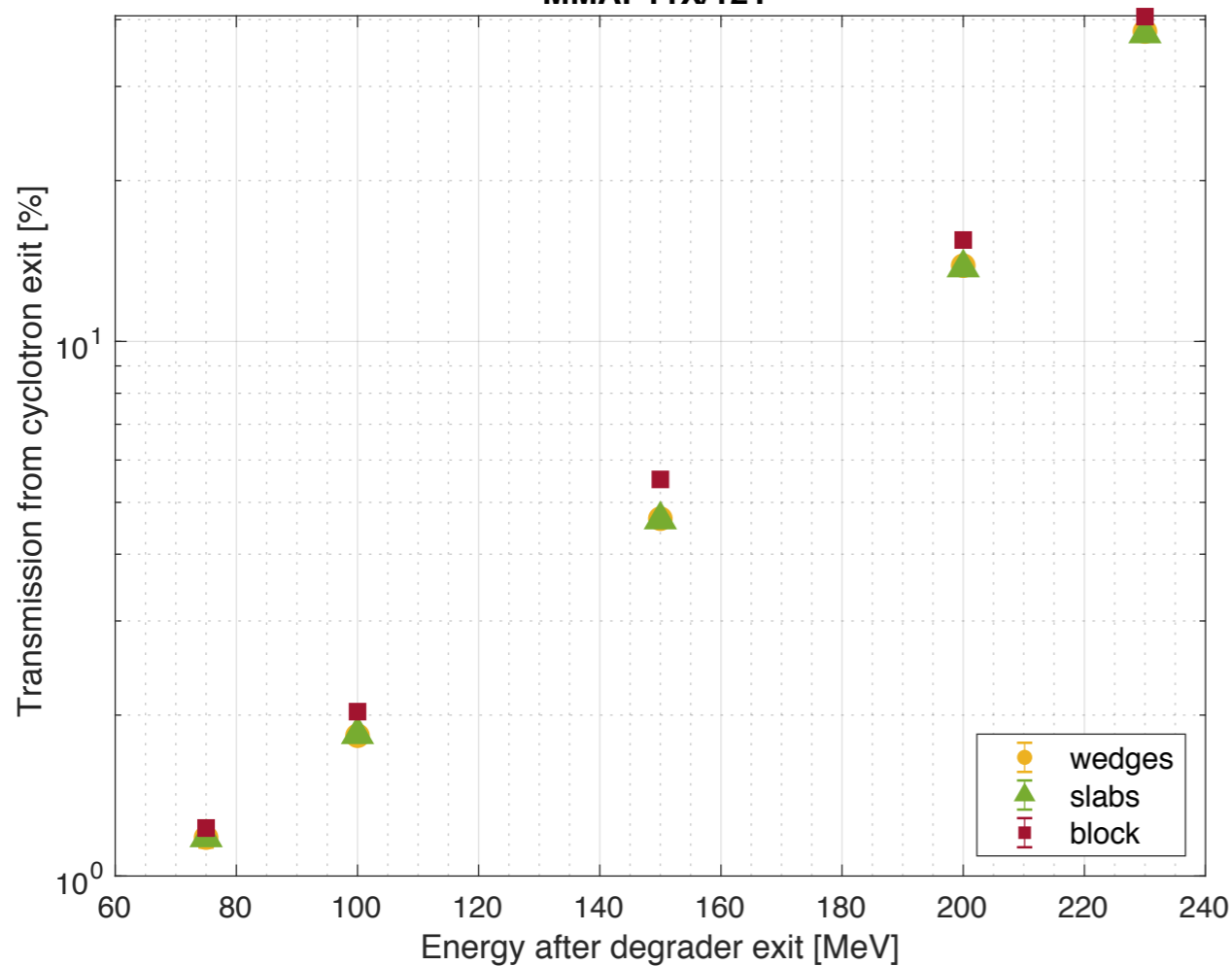
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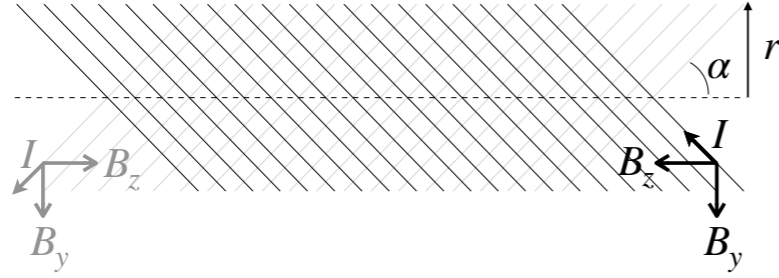
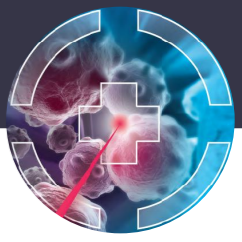


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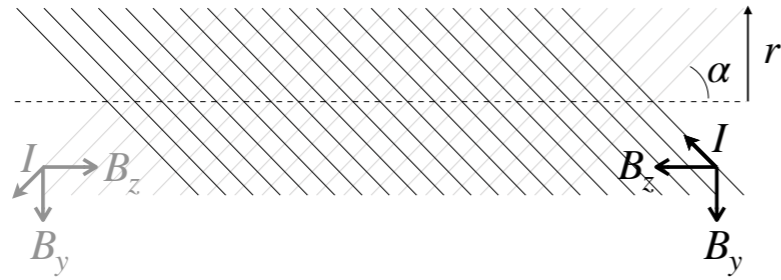
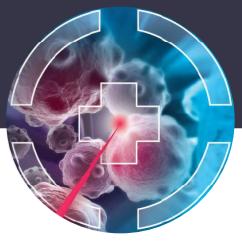


ALTERNATIVE MATERIAL:  
BORON CARBIDE B4C

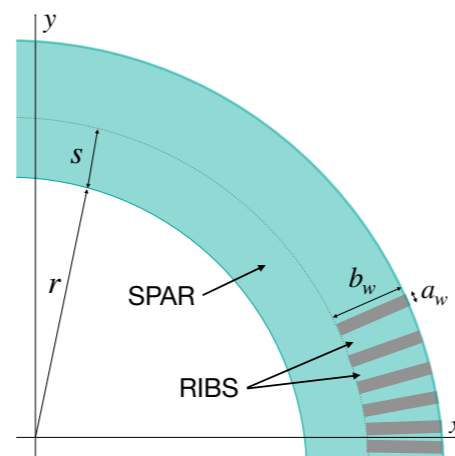
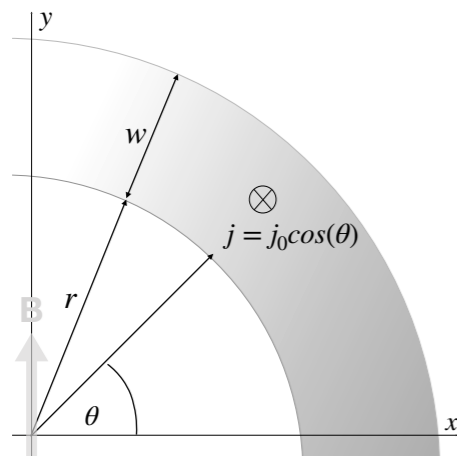
# Canted cosine theta magnet



- Conductor layers are wound such that:
- Transverse field components sum
  - Solenoidal field components cancel

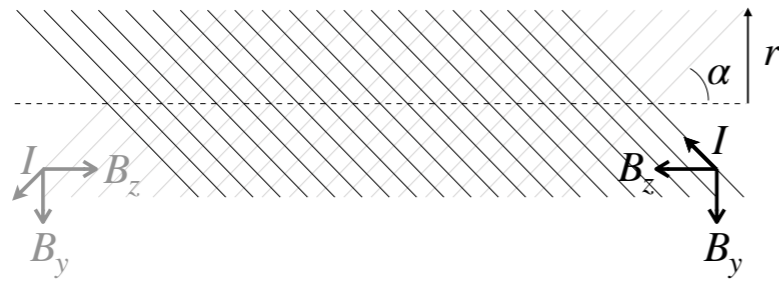
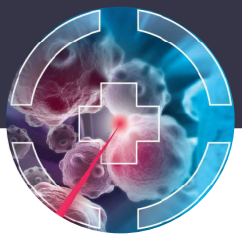


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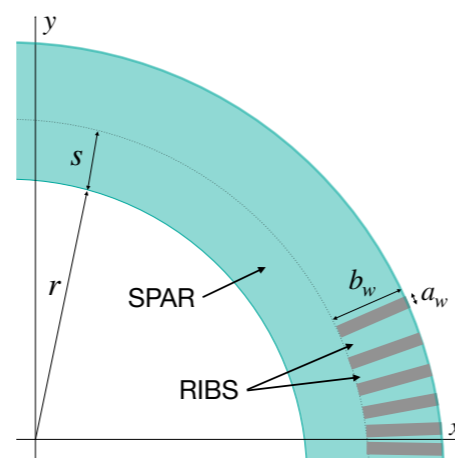
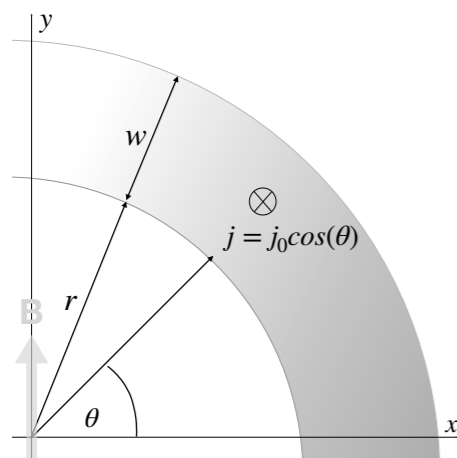


### CCT cross section:

- Each conductor sits in its own channel;
- Channels separated by the ribs (transferring Lorentz forces to the spar)



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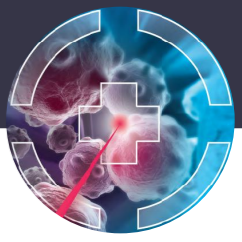


### Advantages of a CCT magnet:

- No or little pre-stress required (no coil movement)
- Any harmonics or superposition of harmonics (combined-function)
- Lower number of components compared to i.e. sector magnet
- Lower cost

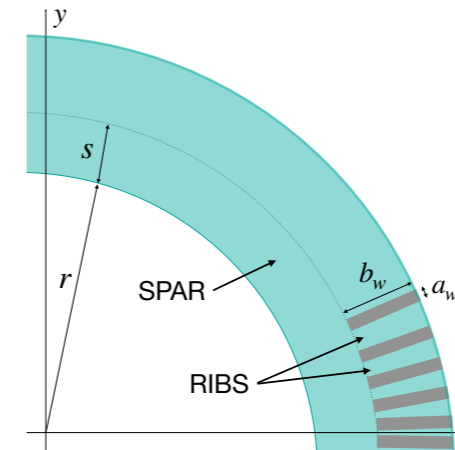
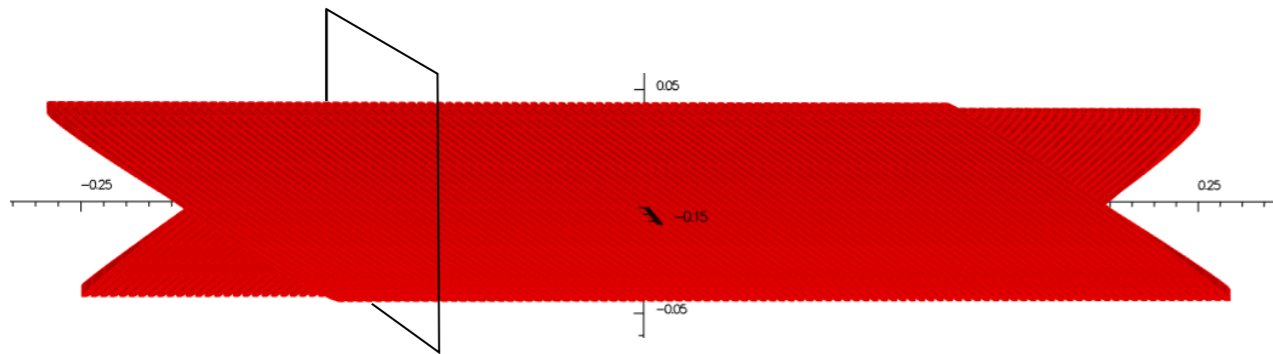
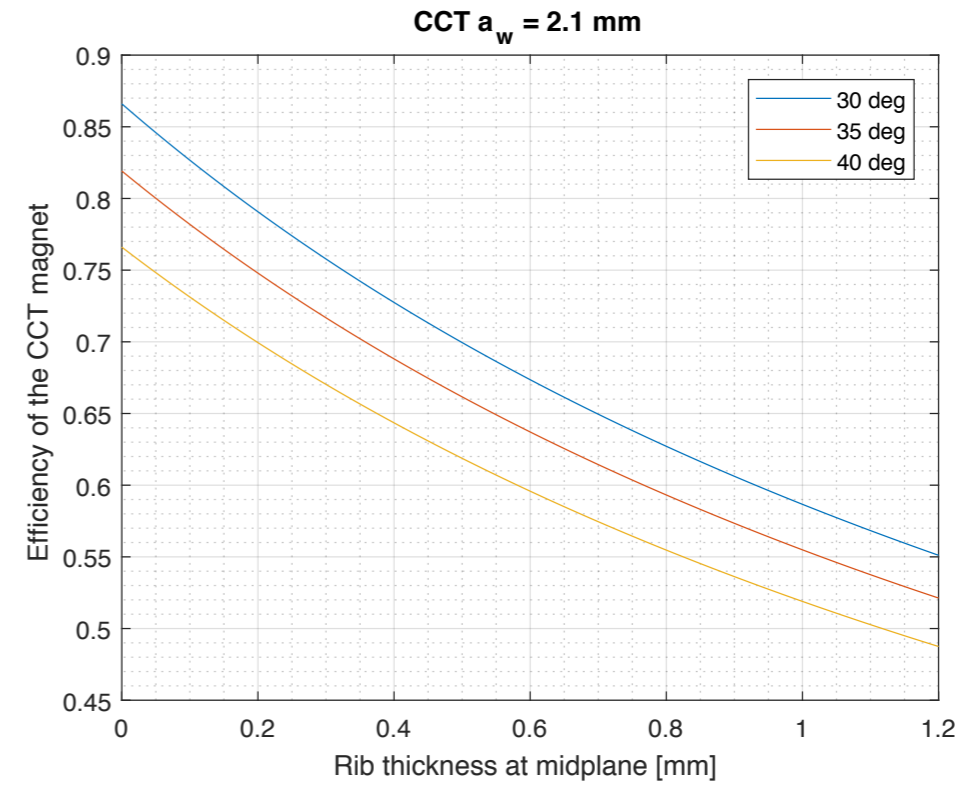
S. Caspi, A 16T Canted-Cosine-Theta (CCT) An option for the FCC, 2015

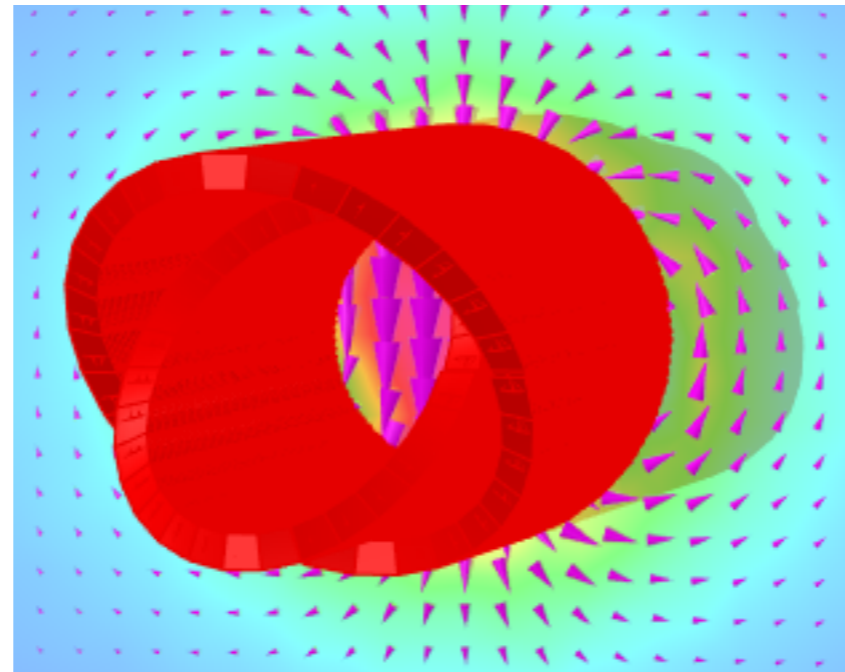
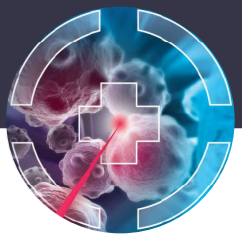
# Canted cosine theta magnet



## Design parameters:

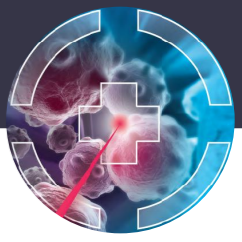
- Bore radius
- Physical length
- Magnetic field
- Rib thickness in the midplane
- Wire: material, dimensions, number of wires in the channel
- Number of layers
- Current density
- Skew angle



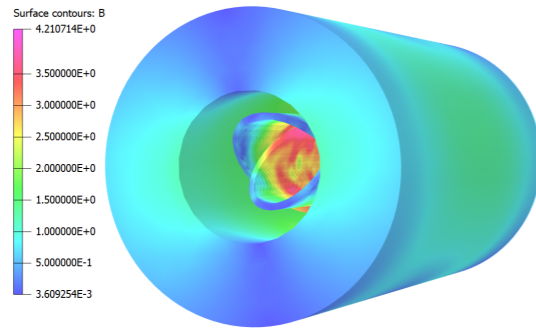


## Dipole parameters

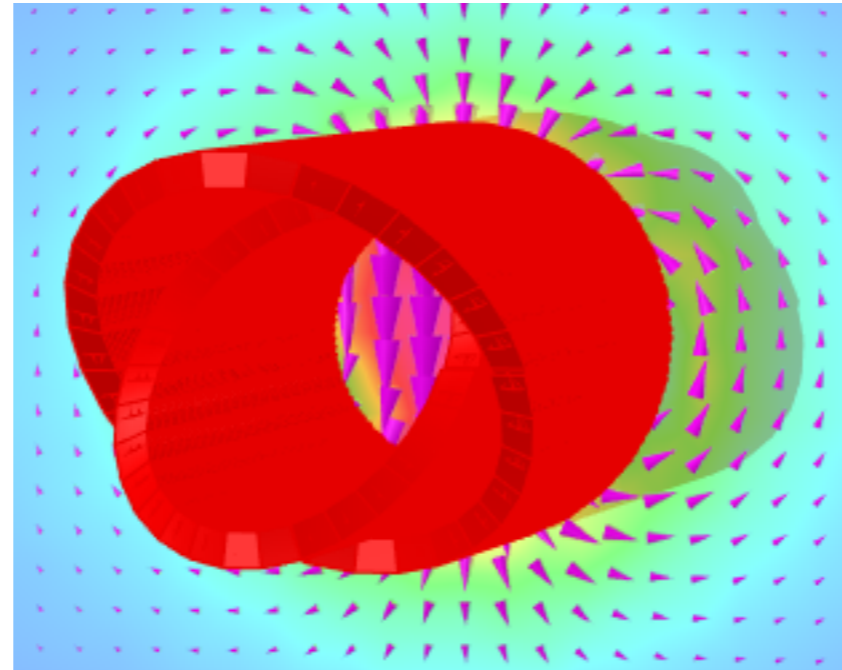
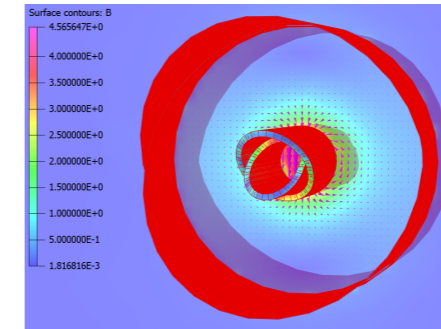
Tilt angle of the coil	31.8 deg
Length of the magnet	0.52 m
Midplane rib thickness	0.3 mm
Wire material	NbTi
Wire non-Cu/Cu ratio	0.51
Wire diameter	0.825 mm



## PASSIVE SHIELDING

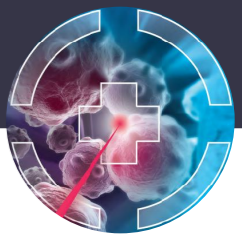


## ACTIVE SHIELDING

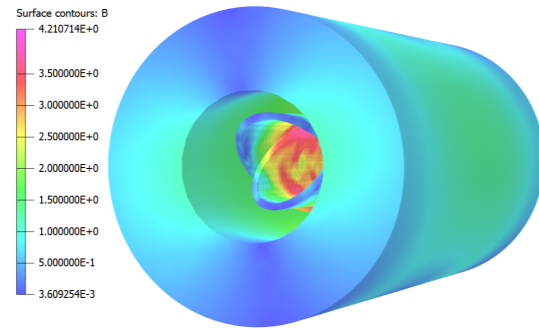


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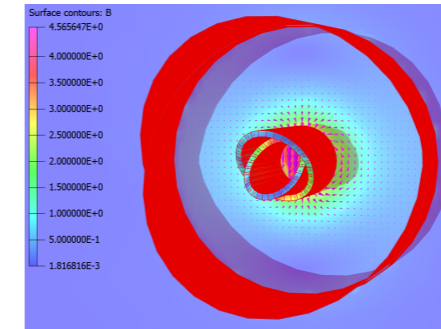
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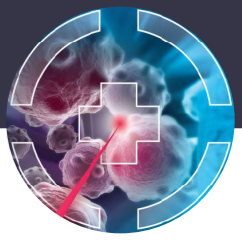
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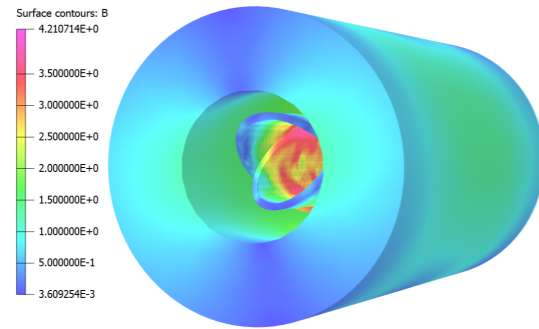
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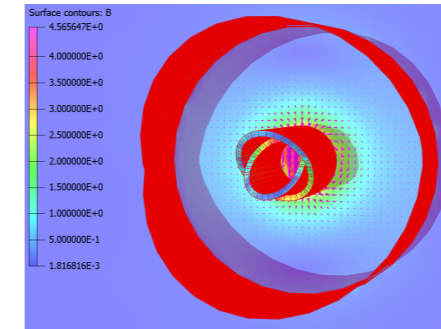
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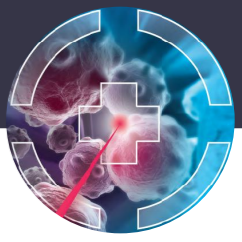


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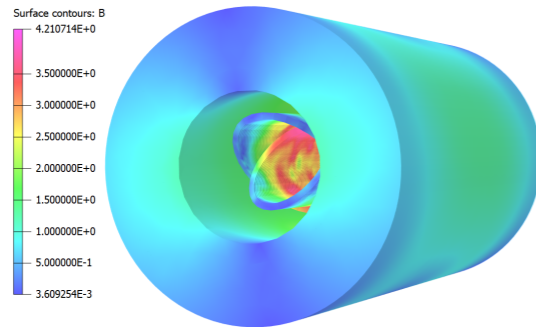
Eng. current [A]	268 A
Peak field in the conductor	4.2 T
Number of wires	8x2
Yoke inner radius	74 mm
Yoke weight	270 kg
Total length of SC strand	1.14 km

## ACTIVE SHIELDING





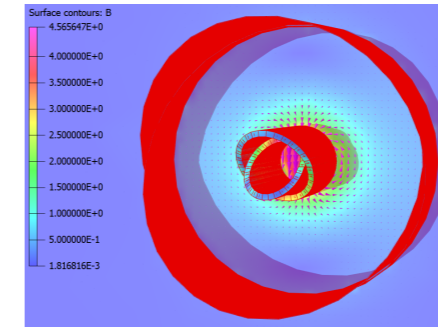
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### Passive shielding dipole parameters

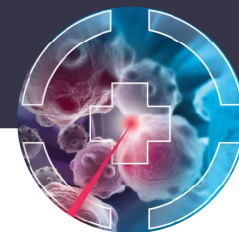
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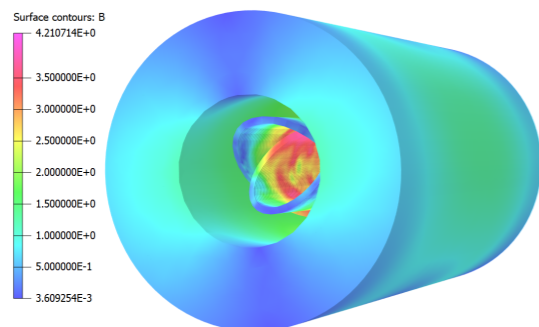


### Active shielding dipole parameters

Eng. current [A]	283 A
Peak field in the conductor	5.0 T
Number of wires	11x2
Inner radius of the sh. coil	220 mm
Tilt angle of sh. coil	62.2 deg
Total length of SC strand	2.74 km



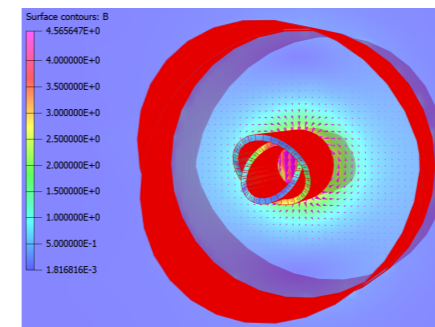
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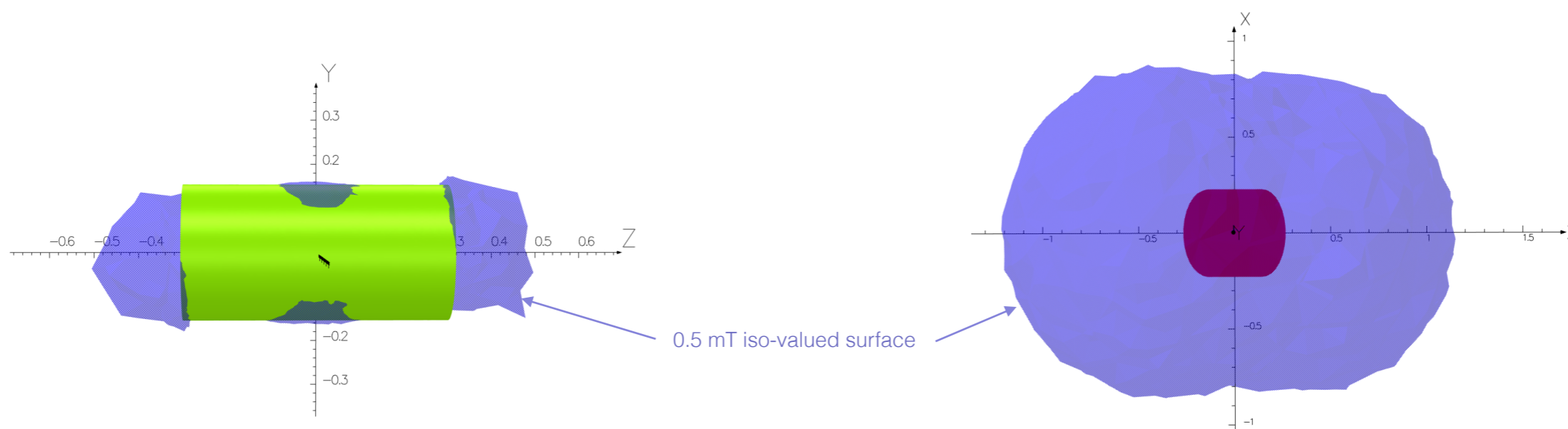
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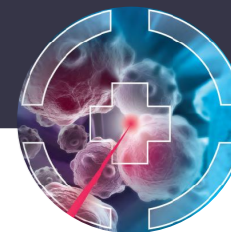


### Active shielding dipole parameters

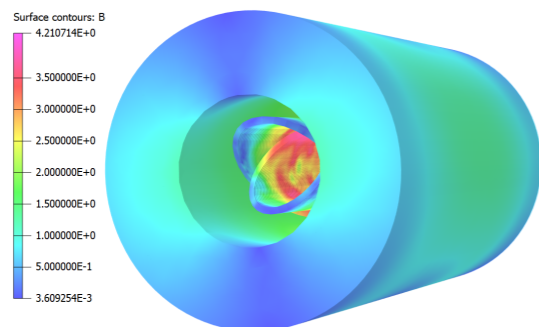
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0.5 mT iso-valued surface

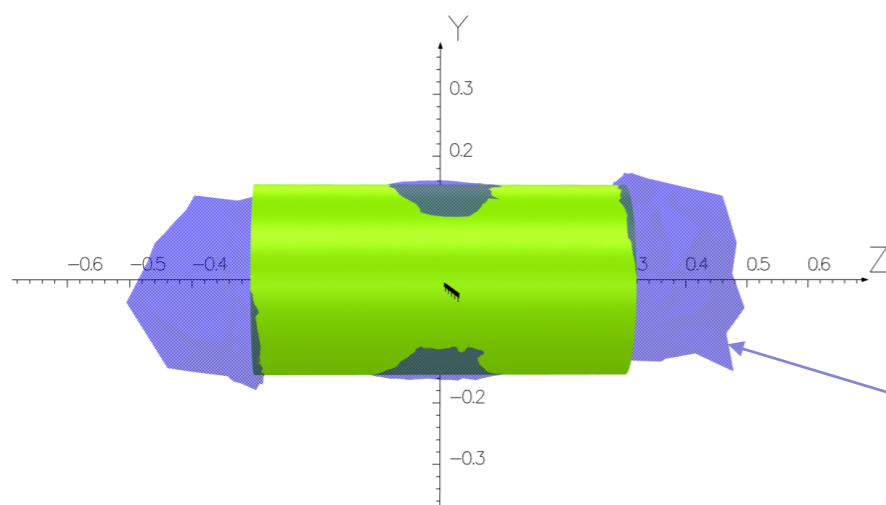


## PASSIVE SHIELDING



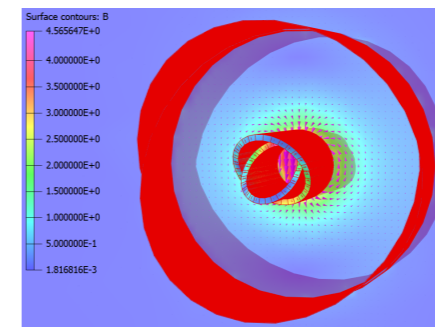
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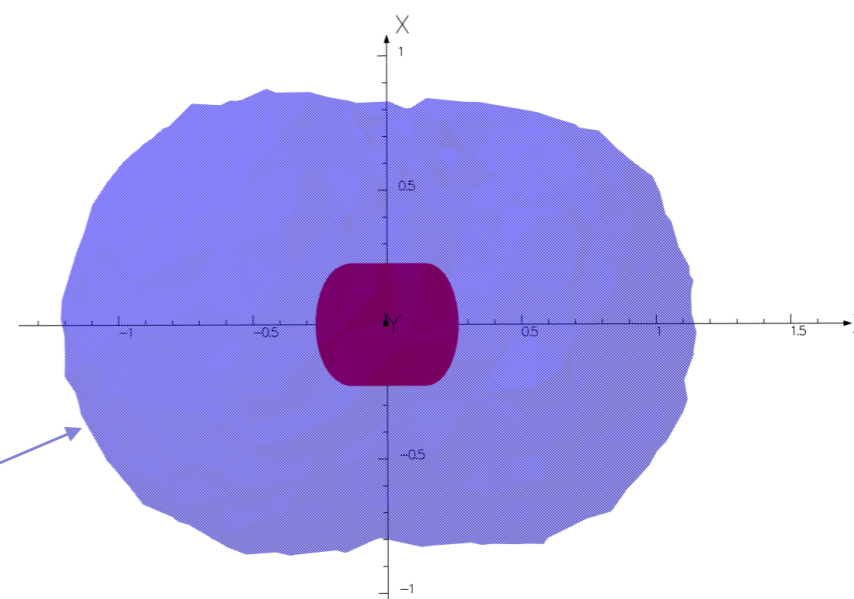
- Heavier
- More efficient stray fields shielding

## ACTIVE SHIELDING



### Active shielding dipole parameters

Eng. current [A]	283 A
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- Larger cryostat, larger cold mass
- More conductor
- Worse stray fields cancellation

# Summary

## Conclusions:

- Compact gantry capable of transporting protons for therapy and imaging
- Superconducting NbTi CCT dipoles with passive shielding (iron yoke)
- Single block boron carbide energy degrader for higher particle transmission

## Next steps:

- Energy degrader integration into the gantry
- Collimation system
- Lower dispersion - larger energy acceptance of the system
- Quadrupole gradient incorporation to the final bending section dipoles

# Summary

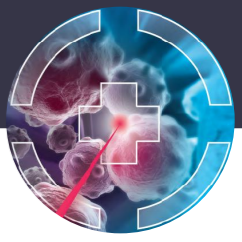
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Thank you!



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