

September 2019

---

## Advancements in Particle Therapy Systems - Acceleration and Delivery

Assoc. Prof. Jonathan Farr

---



*The following presentation of the AVO's LIGHT® Proton Therapy Solution is part of our Development roadmap and is subject to conformity assessment(s) by AVO's Notified Body as well as 510(k) clearance by the USA-FDA*

COI disclosure: Jonathan Farr is a shareholder of AVO and holds a senior leadership position in the company



# Proton Therapy System New Developments

## New horizons in particle therapy systems

Jonathan B. Farr<sup>a)</sup>

*Department of Medical Physics, Applications of Detectors and Accelerators to Medicine SA, 1217 Geneva, Switzerland*

Jacob B. Flanz

*Department of Radiation Oncology, Massachusetts General Hospital and Harvard Medical School, Boston, MA, USA*

Alexander Gerbershagen

*Department of Engineering, European Organization for Nuclear Research (CERN), 1211 Geneva 23, Switzerland*

Michael F. Moyers

*Department of Medical Physics, Shanghai Proton and Heavy Ion Center, Shanghai 201315, China*

e967 Farr *et al.*: Advanced particle therapy systems

e967

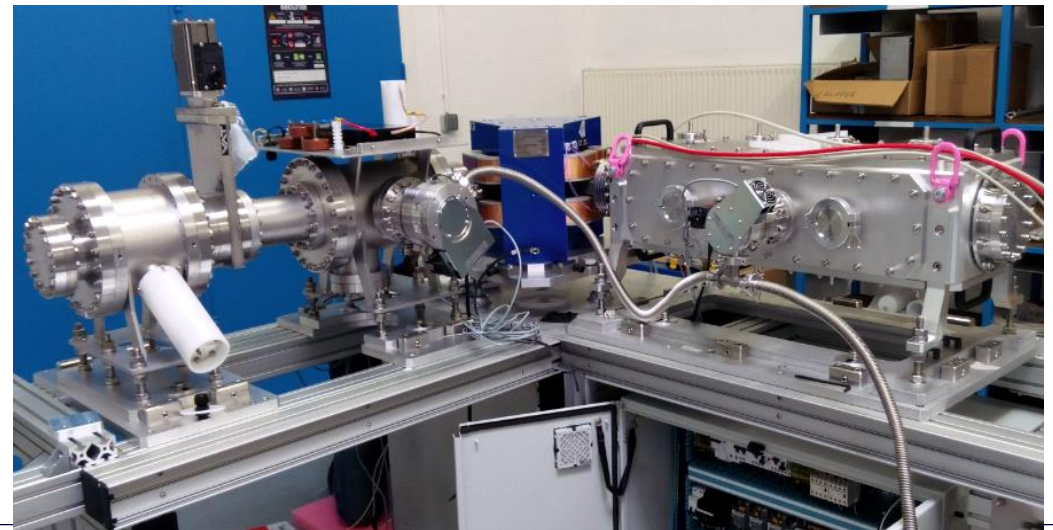
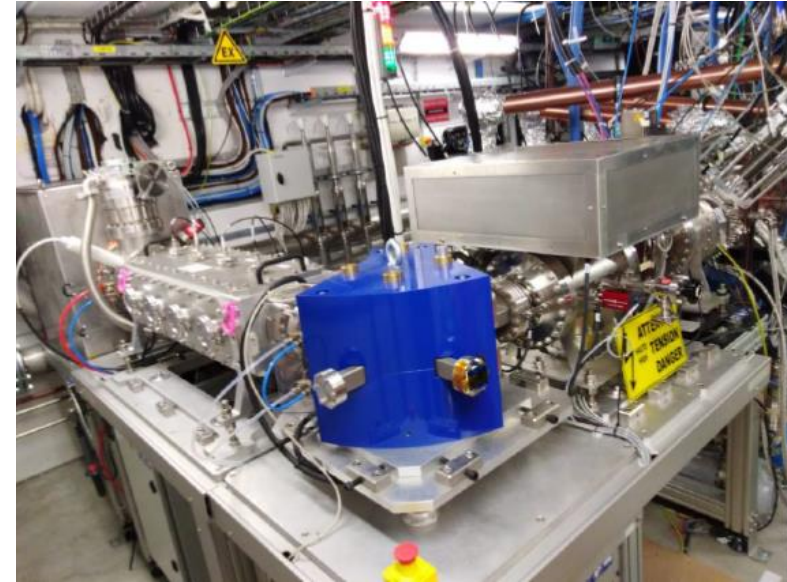
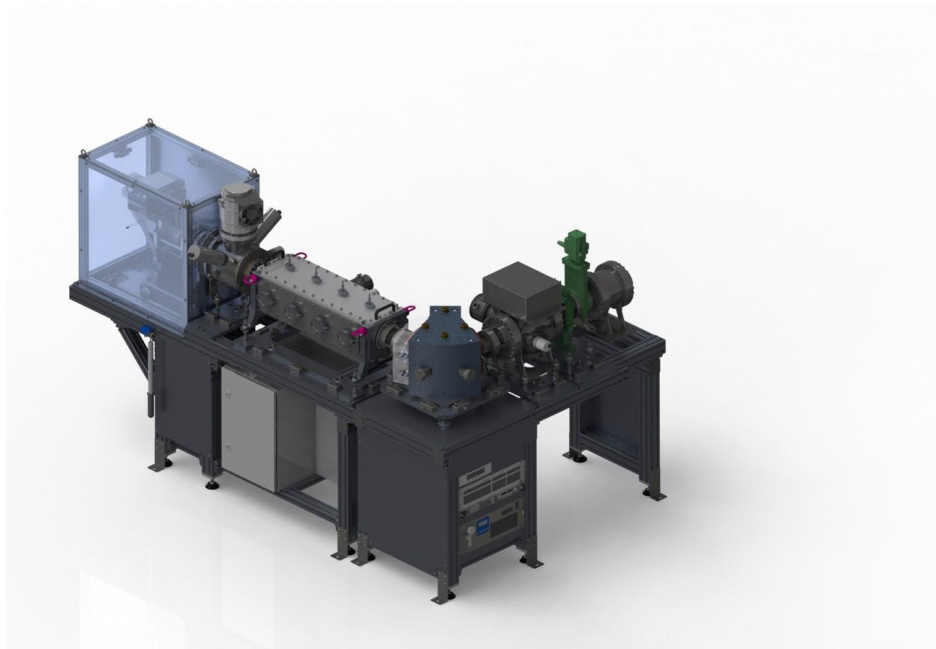
TABLE III. Desirable characteristics of new ion therapy systems compared to current systems.

#	Characteristic	Advantages
1	Reduced maintenance	Lower service contract costs, greater availability and higher utilization
2	Cheaper	Lower facility investment costs
3	Lighter	Lower capital and installation costs
4	Smaller	Lower building construction costs
5	Reduced shielding	Lower facility investment costs
6	Reduced activation	Lower decommissioning cost, faster maintenance access time

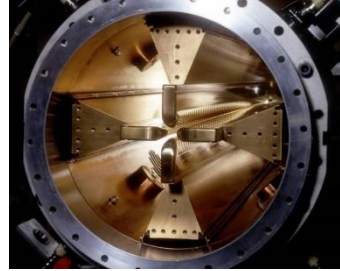
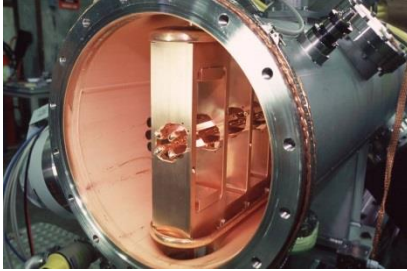
The Emergence of the proton therapy LINAC

# LIGHT Components

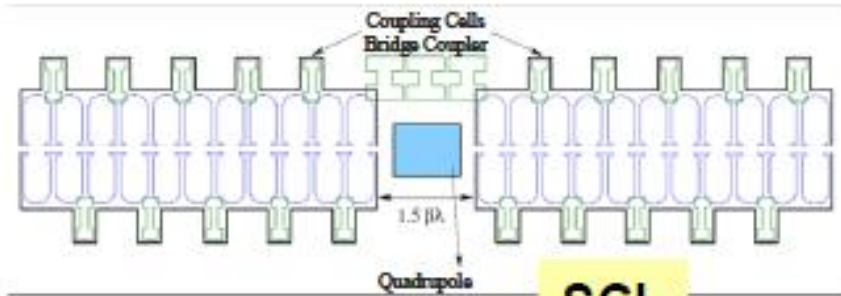
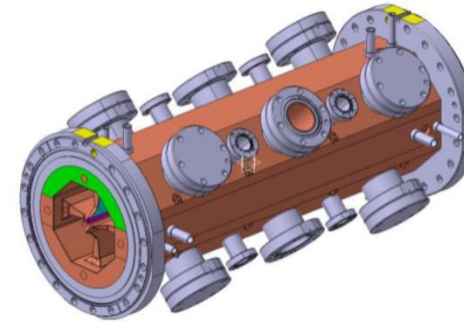
- **Proton source:**
  - MONO 1000 ECRIS
  - RF frequency 2.45 GHz
  - chopped at 200 Hz
  - 300 -1  $\mu$ A



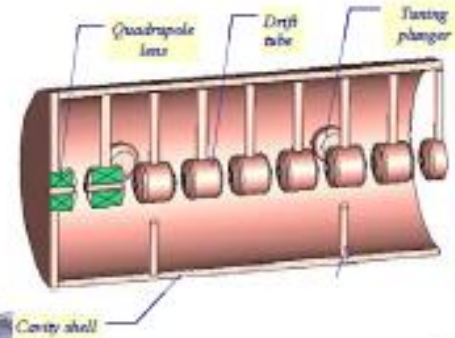
# Standing wave normal conducting structures



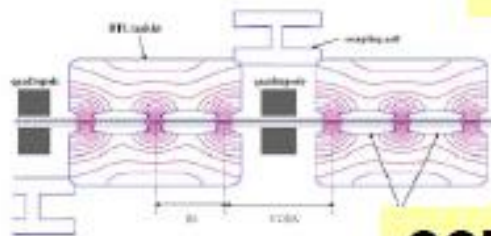
RFQ



SCL



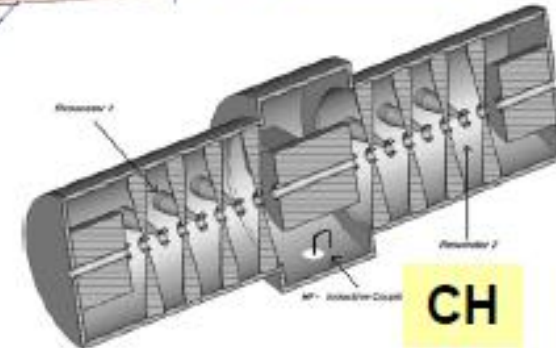
DTL



CCDTL



PIMS



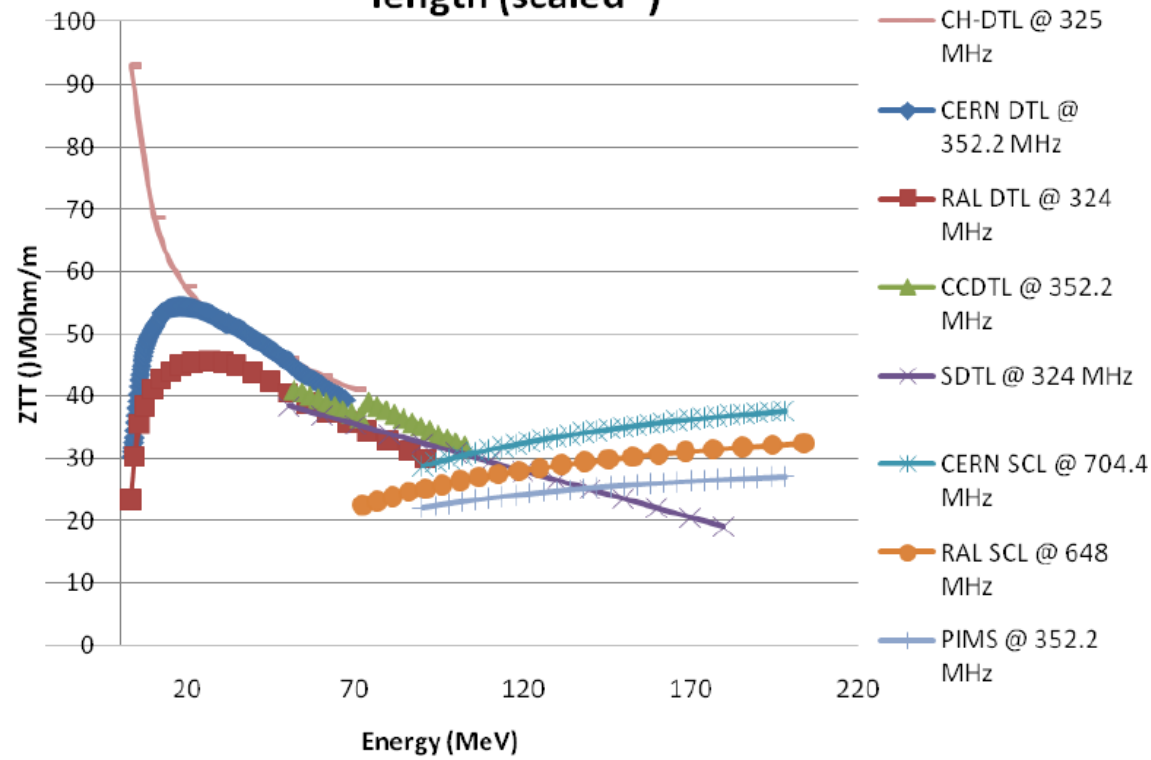
CH

M. Vretenar (CERN), CAS2013

# LIGHT Structures Sequence

The accelerating efficiency is strongly dependent on the type of structure used and on the beam energy

All Structures: Effective Shunt Impedance per unit length (scaled\*)



For proton linac, several structures are used in sequence to adapt to the increasing particle velocity  $\beta$

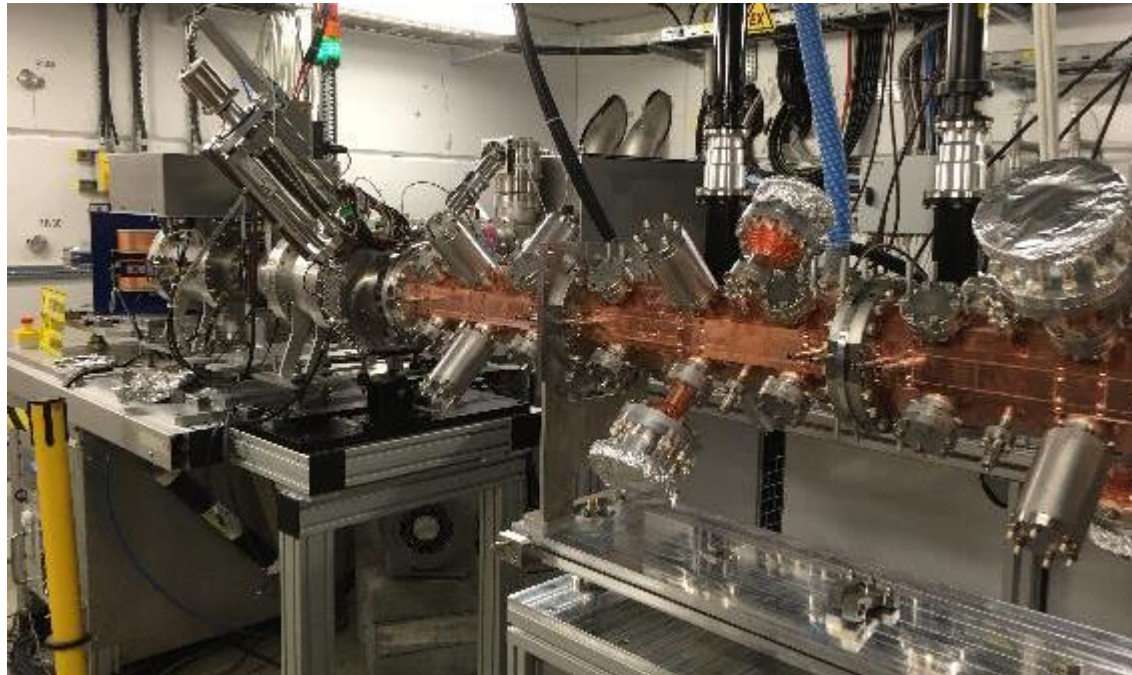
In order of increasing  $\beta$  typical structures are:

1. RFQ
2. DTL or SCDTL
3. CCL

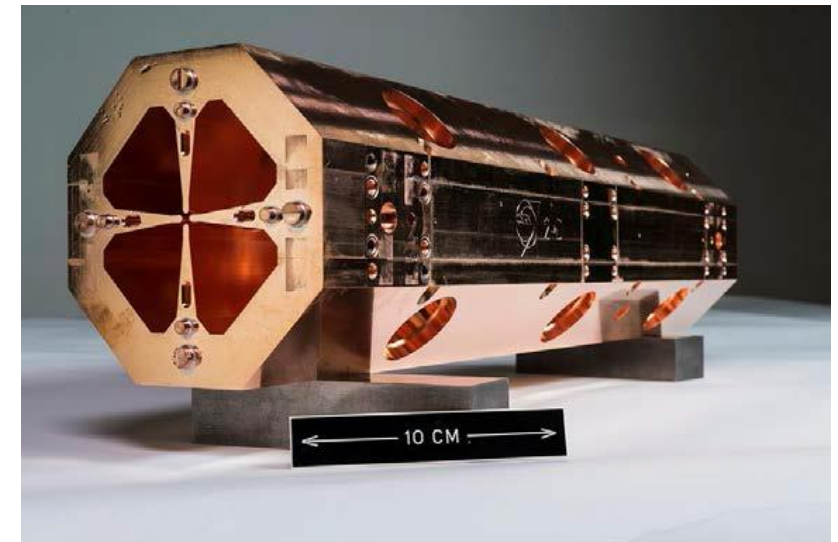
CARE-Report-2008-071-HIPPI (2008)

# LIGHT Components

- **High frequency RFQ designed by CERN**
  - 4 vanes type
  - 750 MHz (highest known)
  - 4 modules - 2 m
  - 5 MeV energy gain



Section	RFQ
RF frequency [GHz]	0.749
Energy [MeV]	0.04-5
Length [m]	2

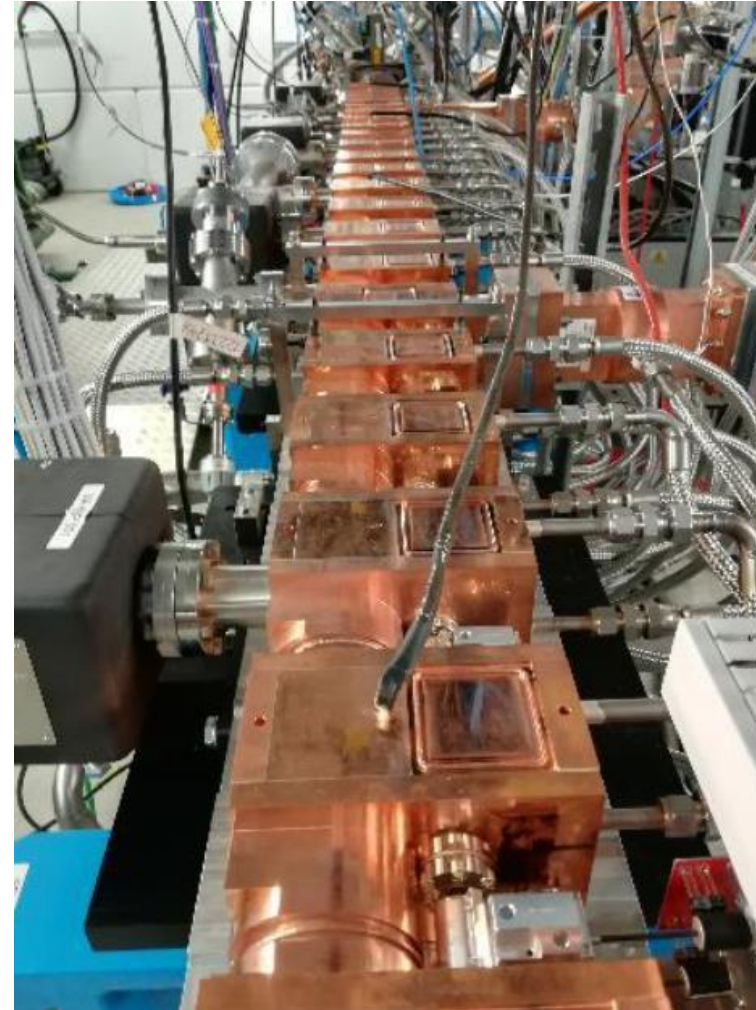


# LIGHT Components

## Side Coupled Drift Tube Linac

- **Designed by ENEA (Frascati, I)**
- **Manufactured at TSC/VDL**
  - SCDTL3 (TSC)
  - SCDTL1, SCDTL2, SCDTL4 (VDL)

Section	SCDTL
RF frequency [GHz]	2.998
Energy [MeV]	5-37.5
Length [m]	6.2

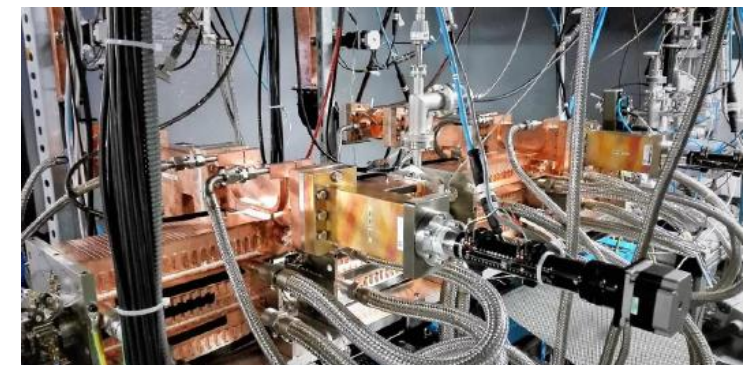
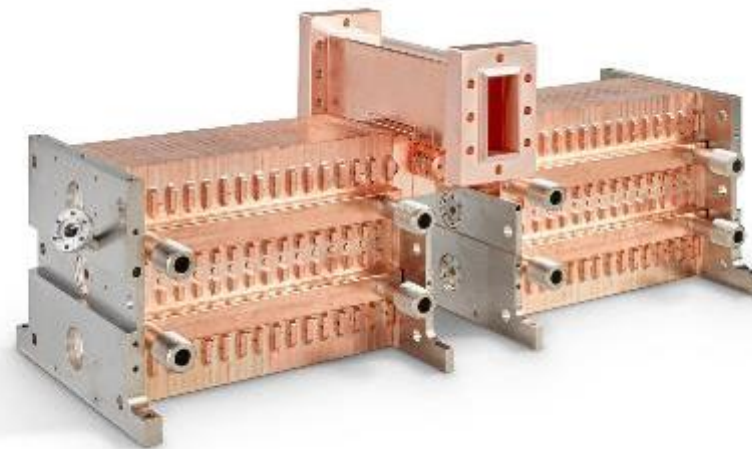
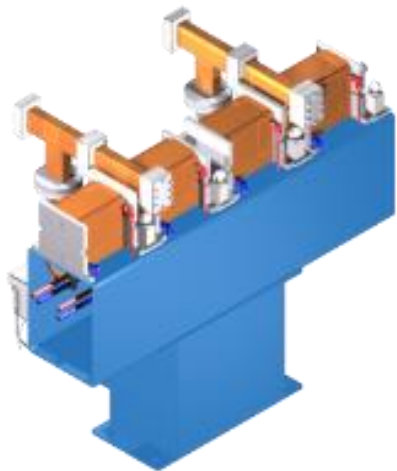


# LIGHT Components

## Coupled Cavity Linac

- Designed by ADAM
- Manufactured by VDL
- 4 modules already in the bunker (conditioned)
- CCL1 CCL2 operating
- All remaining modules in production

Section	CCL
RF frequency [GHz]	2.998
Energy [MeV]	37.5-230
Length [m]	15.5

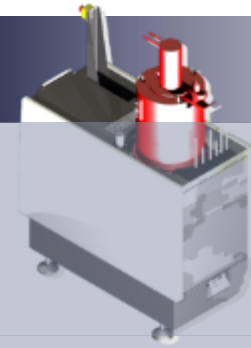




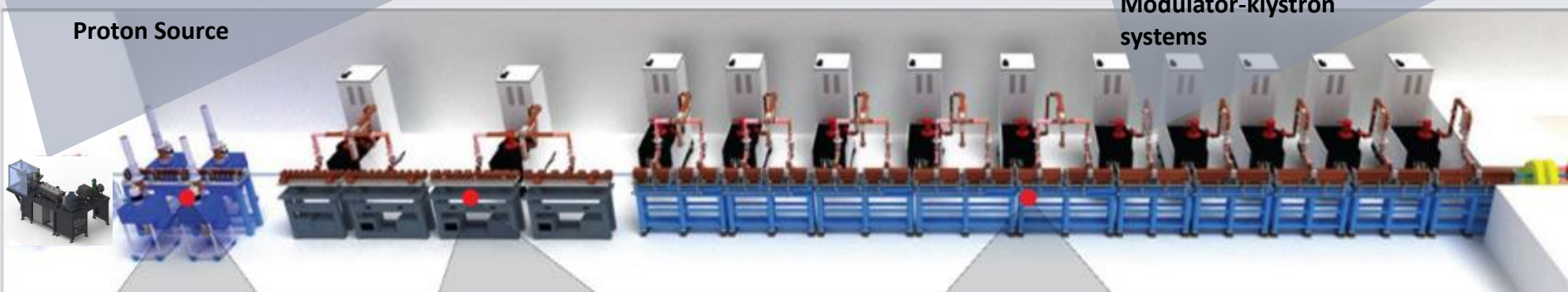
# LIGHT Beam Production System



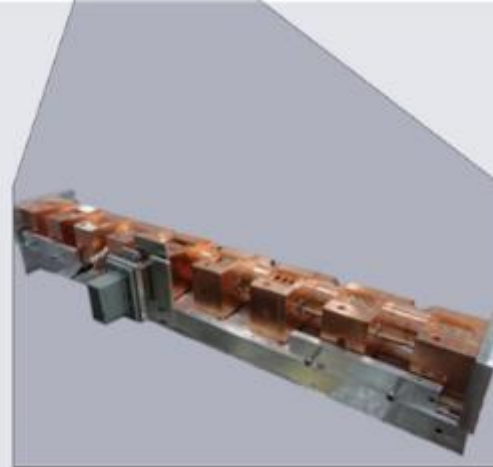
Proton Source



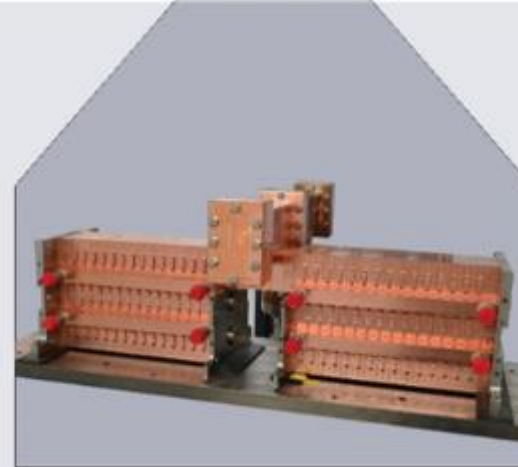
Modulator-klystron systems



Radio Frequency Quadrupole (RFQ)



Side Coupled Drift Tube Linac (SCDTL)



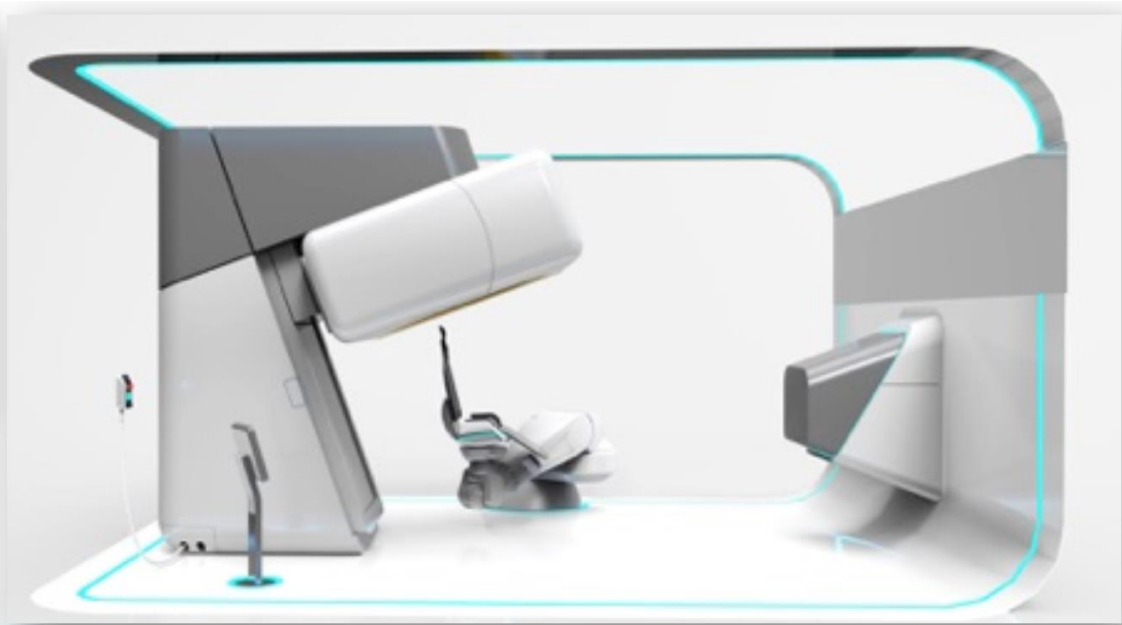
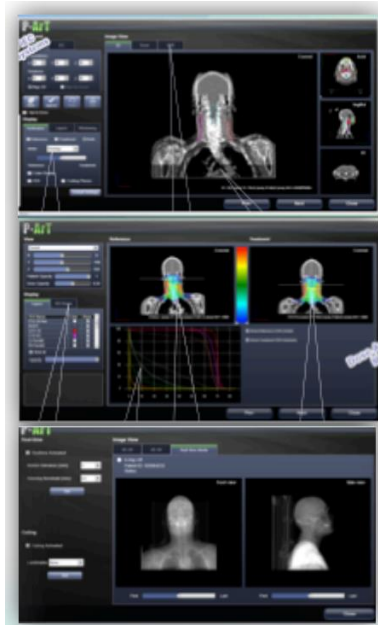
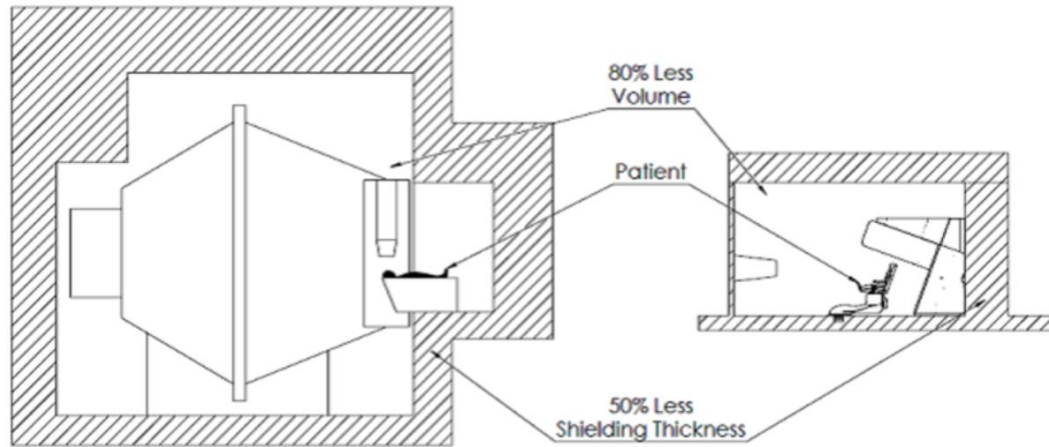
Coupled Cavity Linac (CCL)

# LIGHT features for proton therapy

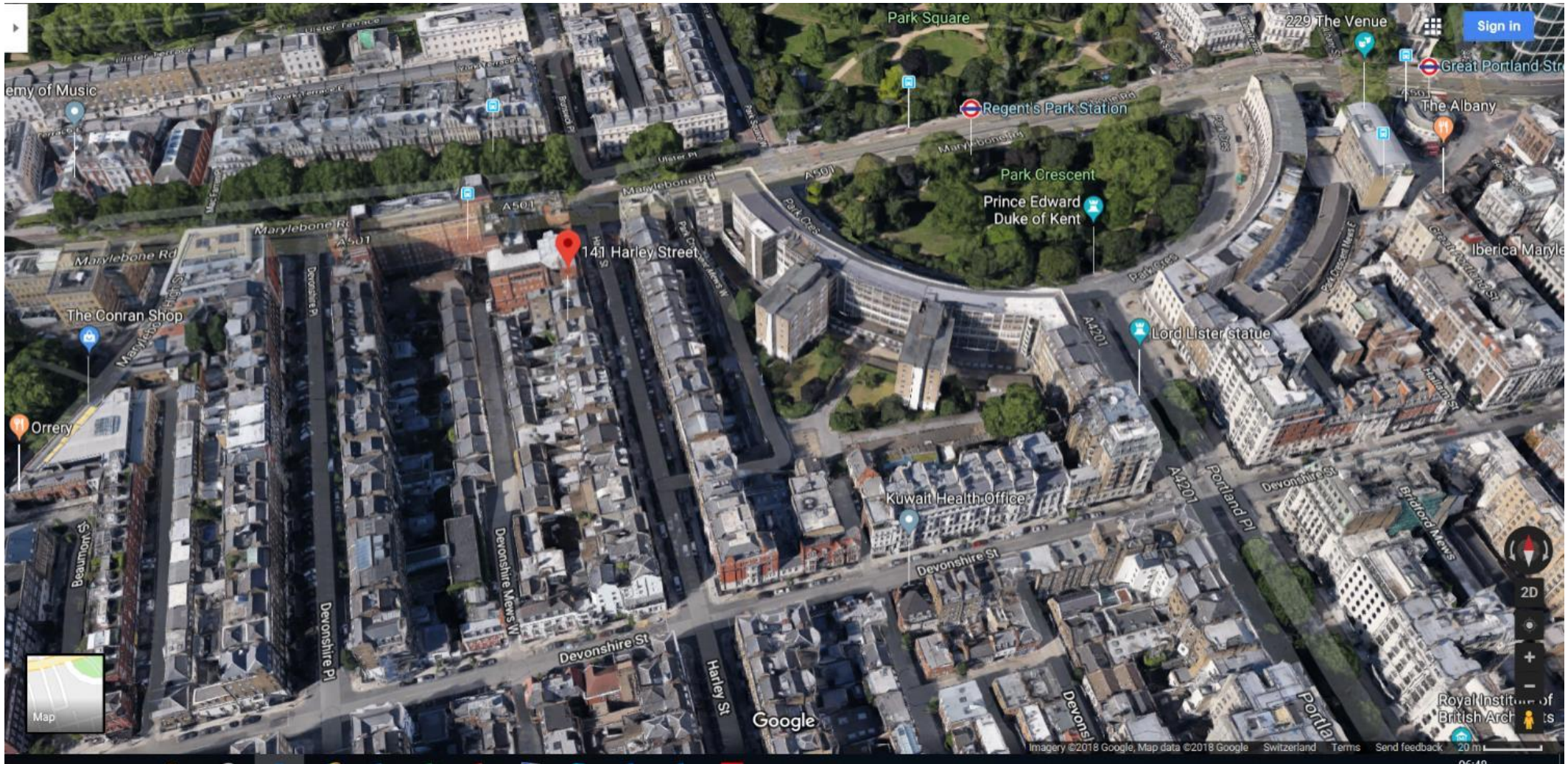
Our intention is to deliver:

- **Active energy modulation** → no absorber and degrader
- **Pulsed beam at 200 Hz** → intensity and energy modulation in 5 ms
- **Small beam emittance** → small magnets aperture
- **Almost no losses!** → reduced shielding

# LIGHT Treatment Room



# Harley Street Project - London



# Harley Street Project - London

*Harley Street, London, the First Site Housing LIGHT*



141/143 Harley Street  
Grade 2 listed buildings

**Challenge:**  
Install and Operate  
a high energy  
Proton Therapy  
Center here



**AVO revolutionises Proton Therapy – Size, cost, patient access**

# Proton therapy goes slimline

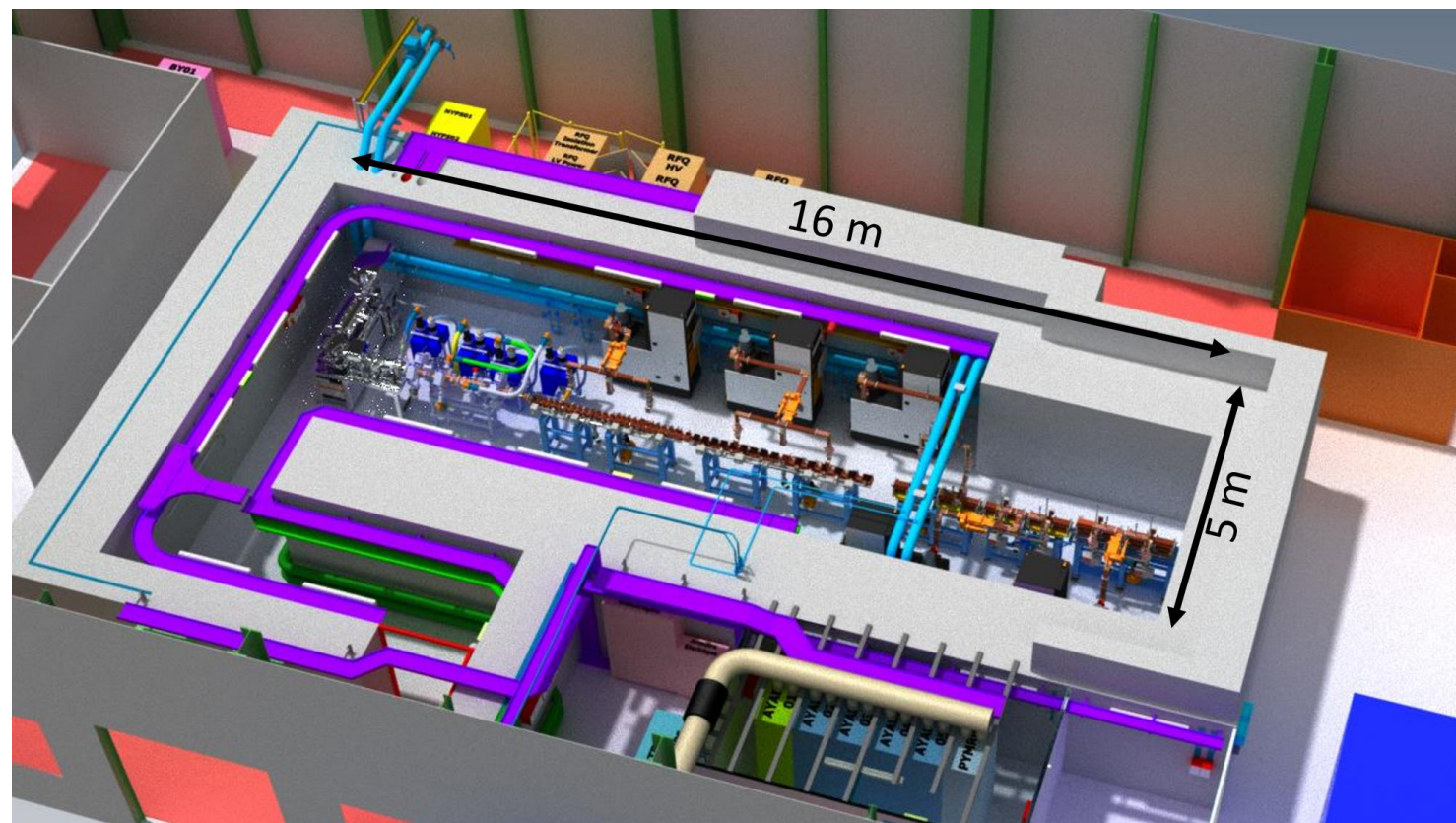
August 2018



Harley Street, London, the First Site Housing LIGHT

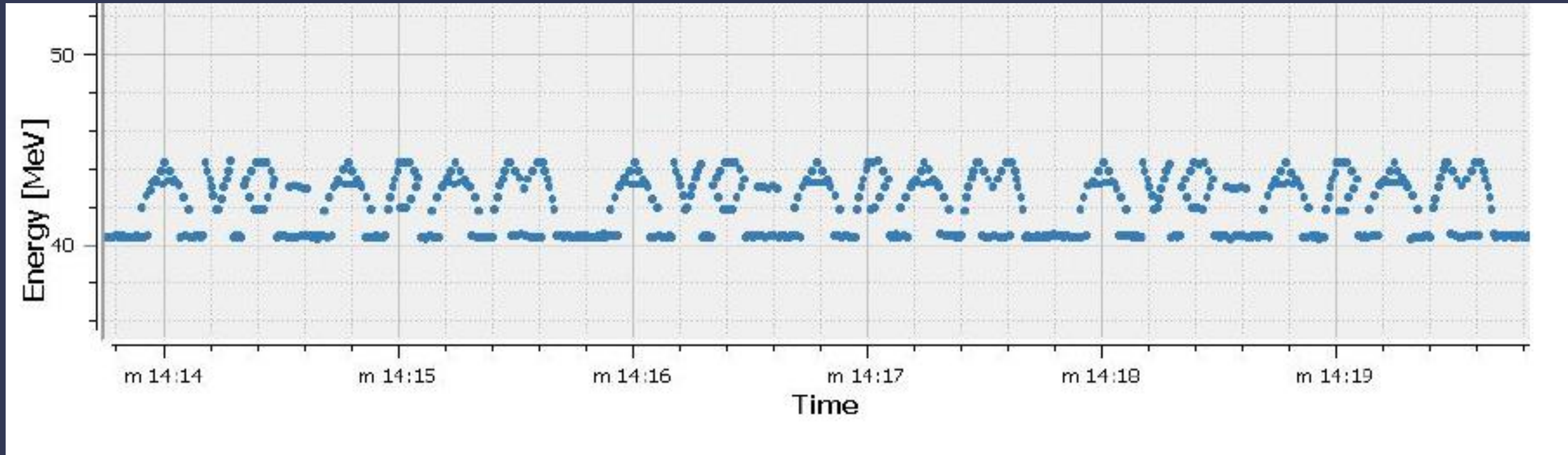
Video

# LIGHT Prototype Testing



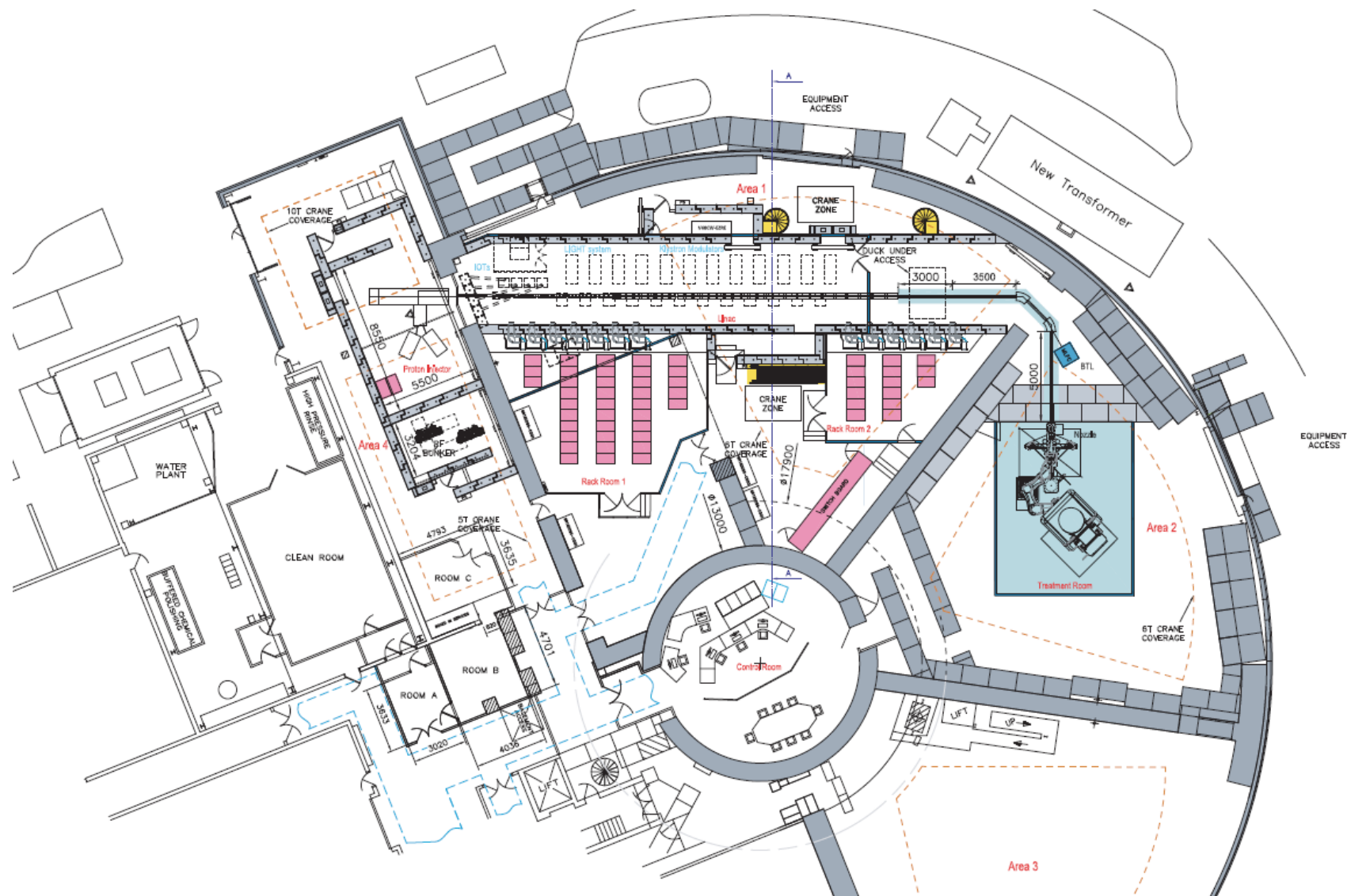


# LIGHT Prototype Testing



# COMMISSIONING OF LIGHT @ STFC, UK

- UK Science & Technology Facilities Council Partnership
- Daresbury laboratory is the AVO extended testing and assembly site
- Accelerator Science and Technology Centre
- CERN partner
- Cockcroft Institute
- R&D testing, including beam tests, will also continue in Geneva



# Proton Therapy Clinical Challenges

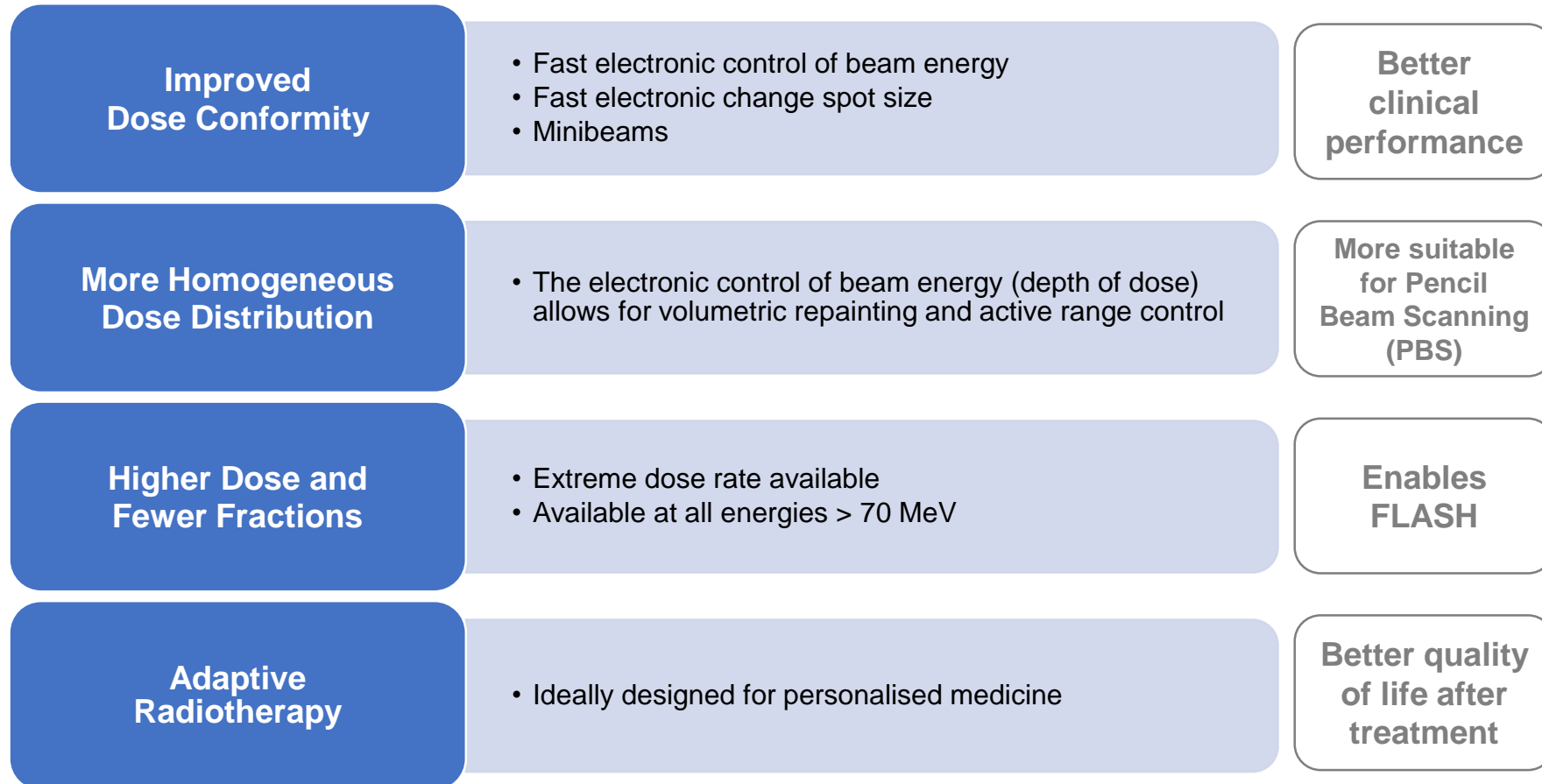
## New horizons in particle therapy systems

e967 Farr *et al.*: Advanced particle therapy systems

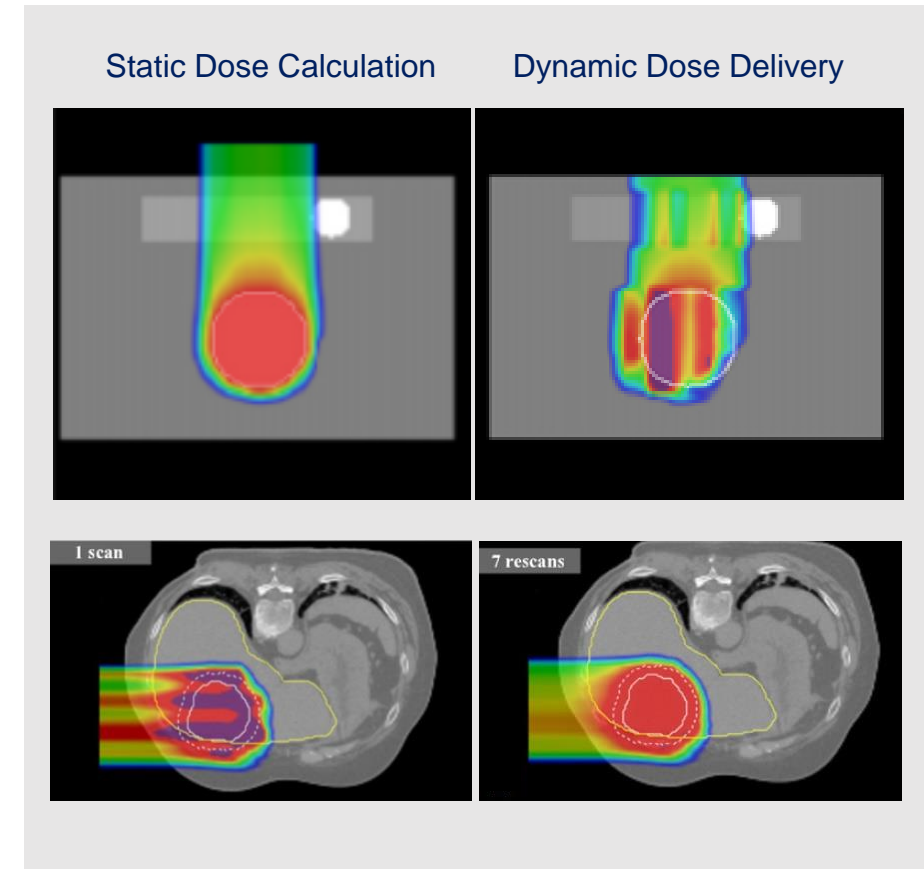
e967

8	Faster energy changes	Shorter treatment times, 3D rescanning
9	Faster, more sensitive instrumentation	In order to accommodate some of the desired parameters, one needs better instrumentation.
10	Higher flux	(assuming fast energy changes, scanning, and better instrumentation); shorter treatment times leading to less patient motion and more patients treated per day
11	Smaller spots or collimation	Better conformal avoidance, hypofractionation, SRS, and SBRT, although some may claim the current performance is at a physical limit
12	Variable spot size and shape, faster than currently available	Better conformal avoidance, faster delivery
13	Ions heavier than protons	Radiobiological effectiveness, geometric sparing, hypofractionation, SRS, and SBRT
14	Rapid gantry angle changes	Some claim this may lead to better conformality to targets, better conformal avoidance to organs-at-risk, others claim this is not necessary with optimized scanning techniques
15	Lower input power (green machine)	Lower operating costs

e953 Med. Phys. 45 (11), November 2018 0094-2405/2018/45(11)/e953/31 © 2018 American Association of Physicists in Medicine e953

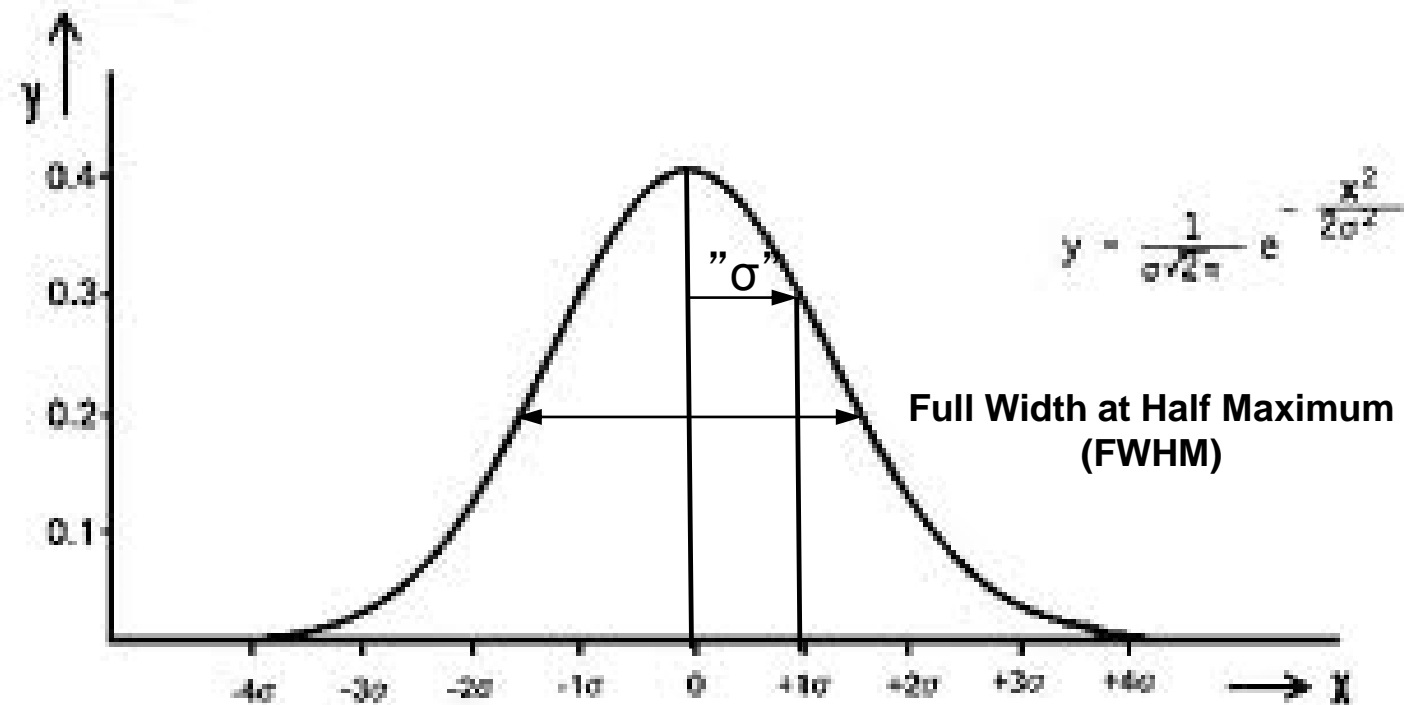


- Current proton systems change energy slowly, resulting in inhomogeneous dose to the tumour, potentially compromising care
- LIGHT® is expected to provide volumetric rescanning with fast 5 millisecond energy changes, maximizing the advantage of proton treatment
- LIGHT® is expected to improve the accuracy of treating moving targets such as lung and liver and the esophagus
- LIGHT® is expected to provide 3D dynamic beam patient target alignment using 5 millisecond active range control



Sources: "Adequate margin definition for scanned particle therapy in the incidence of intrafractional motion", Antje-Christin Knopf, et al, *Physics in Medicine and Biology*, Volume 58, Number 17 (2013); "Comparative study of layered and volumetric rescanning for different scanning speeds of proton beam in liver patients", K Bernatowicz, A J Lomax et al, *Physics in Medicine and Biology*, Volume 58, Number 22 (2013),

# Proton Spot Size

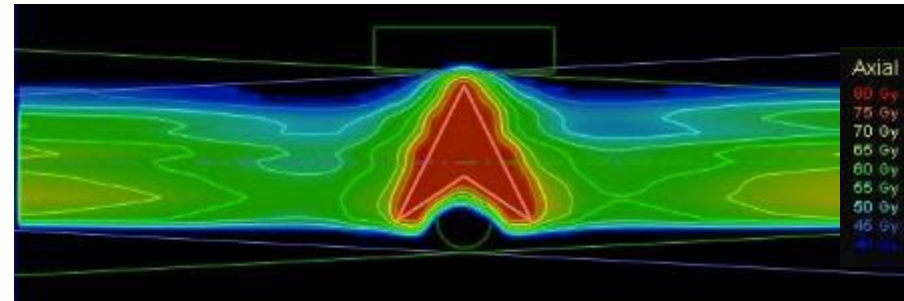


1 FWHM = 2.35 “ $\sigma$ ”

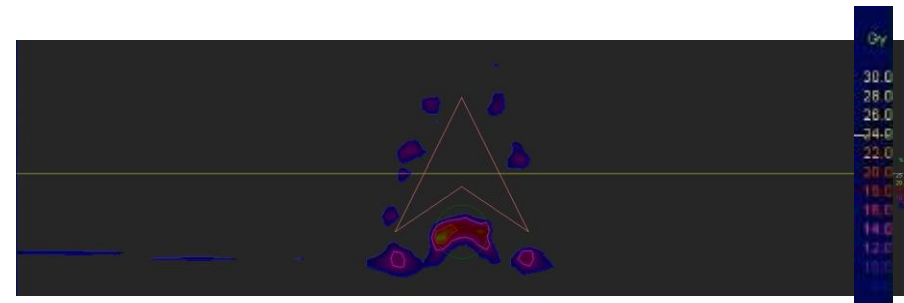
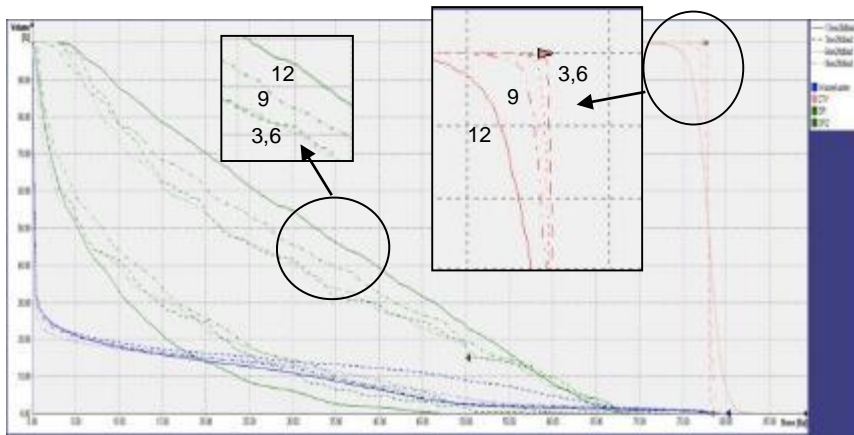
# Proton Spot Size

- The phantom QI's indicated a significant sensitivity to beam size.
- A reasonable QI was only achieved by the 3 and 6 mm  $\sigma$  beams.

	Conformity	OAR Hit	QI
<b>Prostate Phantom</b>			
3mm - 2 Field	1	1.0	1
6mm - 2 Field	2	1.1	2
9mm - 2 Field	5	1.1	5
12mm - 2 Field	17	1.2	14



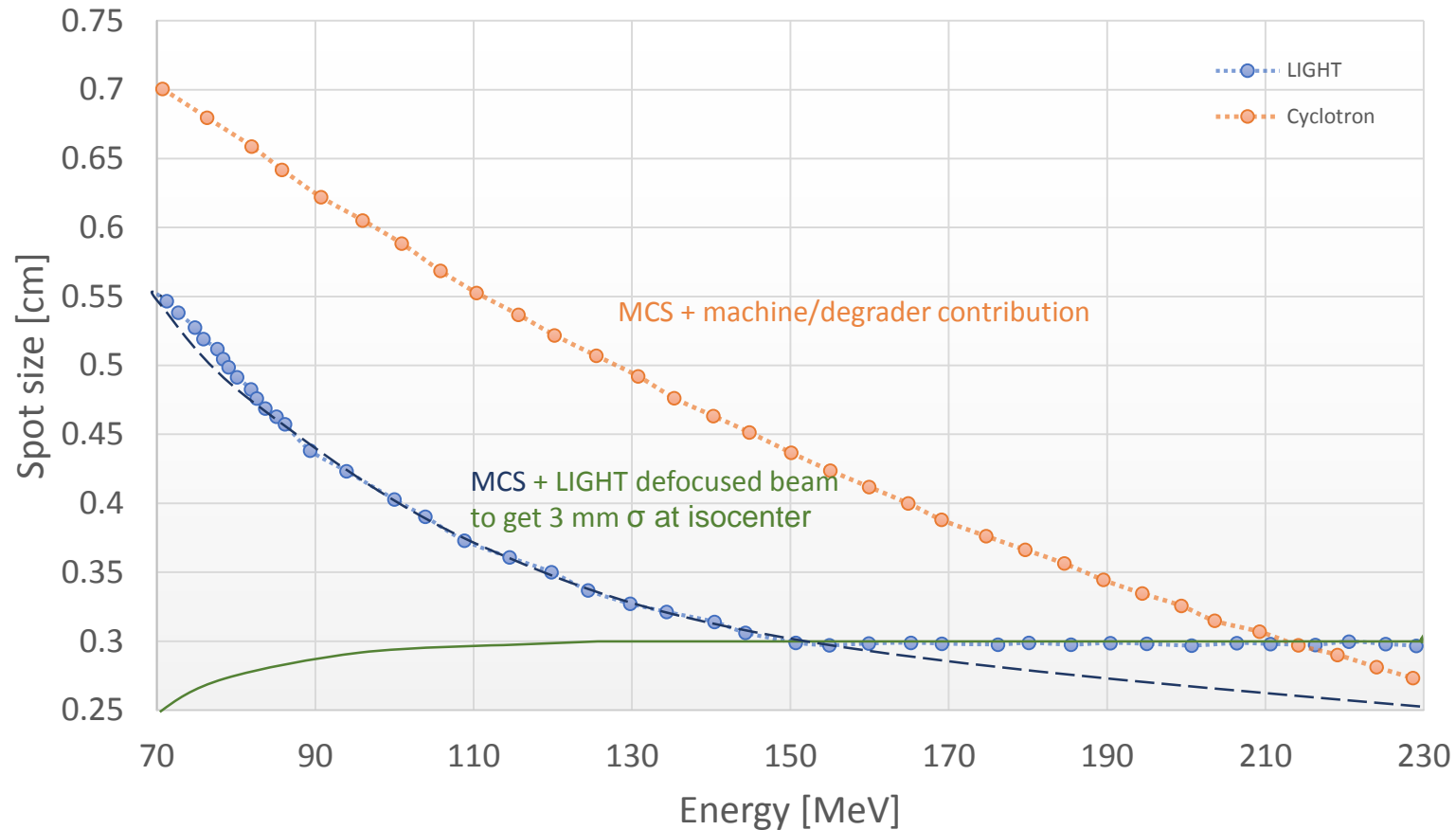
Highly conformal 3 mm  $\sigma$  plan result



% dose difference between 3 mm and 12 mm  $\sigma$  plans indicating excess dose to the simulated OAR

J. Farr, D. Geismar, A. Kaiser, M. Stuschke, Westdeutsches Protonentherapiezentrum and Universitätsklinikum Essen, "Investigation of the relative conformality and efficiency for a series of different spot sizes in intensity modulated proton therapy," Oral presentation, DEGRO, June 2009, Bremen, Germany.

## Spot Size LIGHT vs Cyclotron

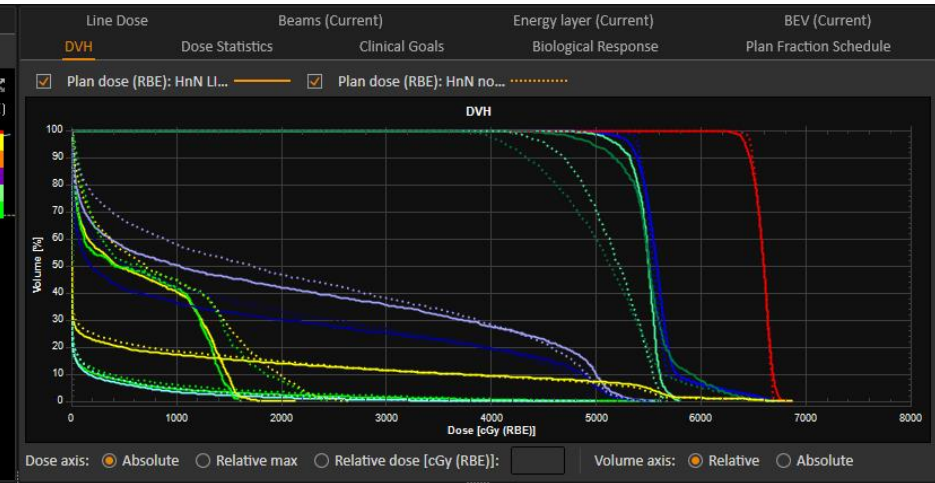
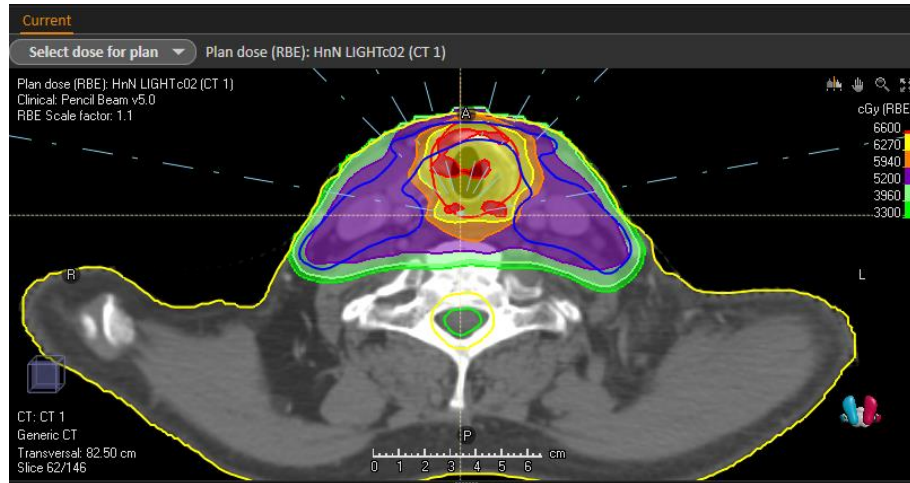


LIGHT can generate very small spot sizes. In order to match standard 3 mm  $\sigma$  at isocenter, the beam is defocused. In contrast, standard machine spot size is dictated by the beam deterioration after passing through the energy degrader.

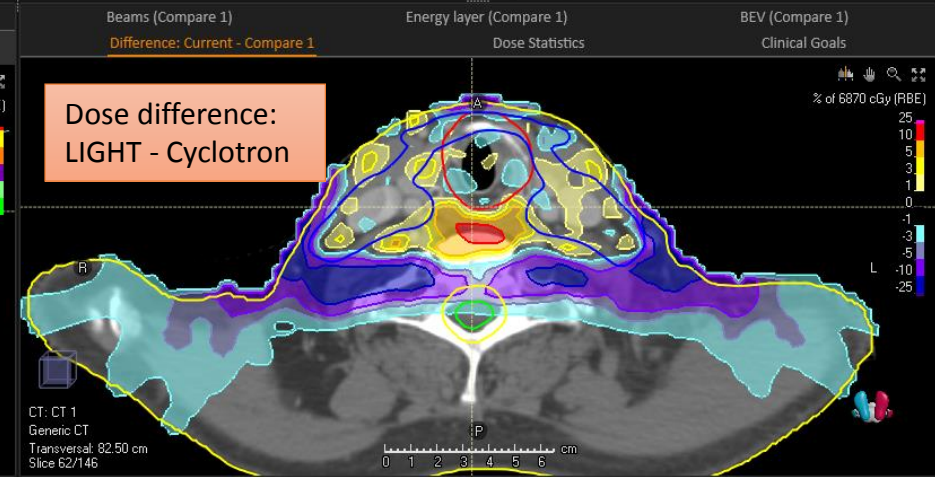


# LIGHT®: More Conformal Dose Distribution – Spot Quality

LIGHT

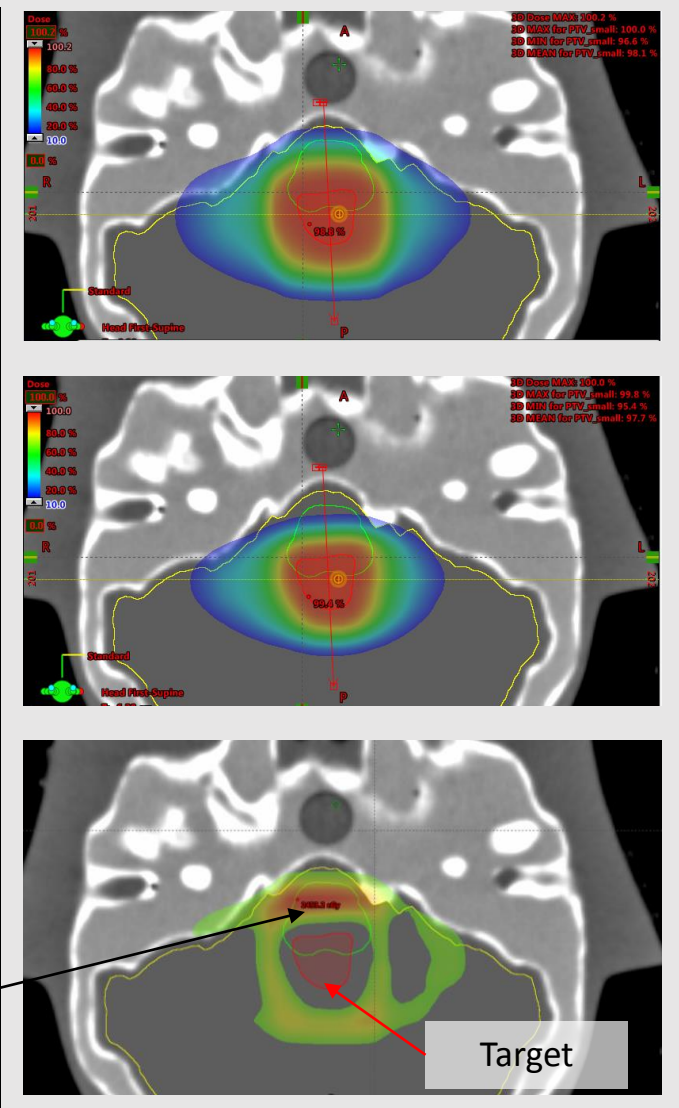
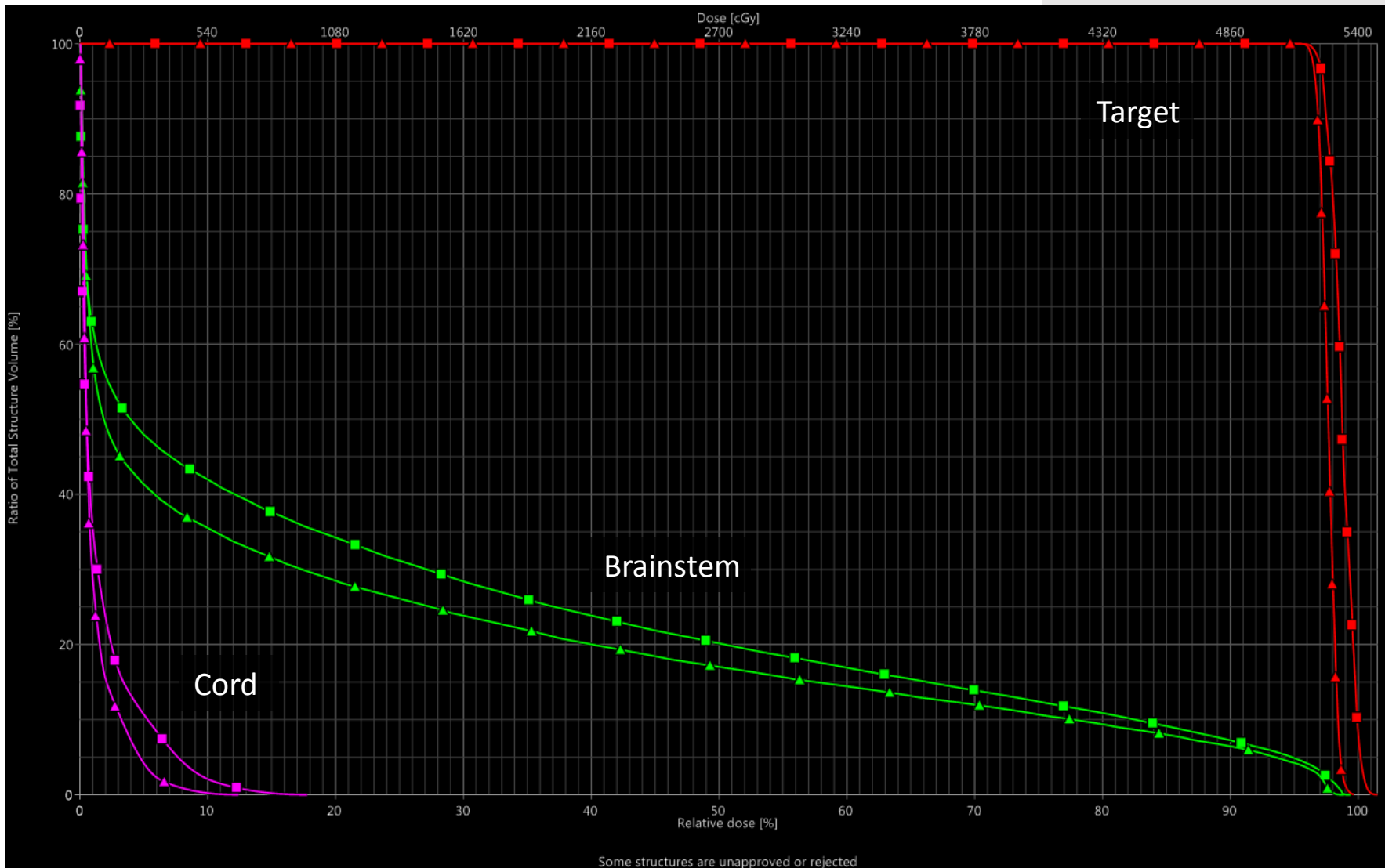


Cyclotron



1) In draft for ESTRO 2020

# LIGHT®: More Conformal Dose Distribution – Proton Minibeams

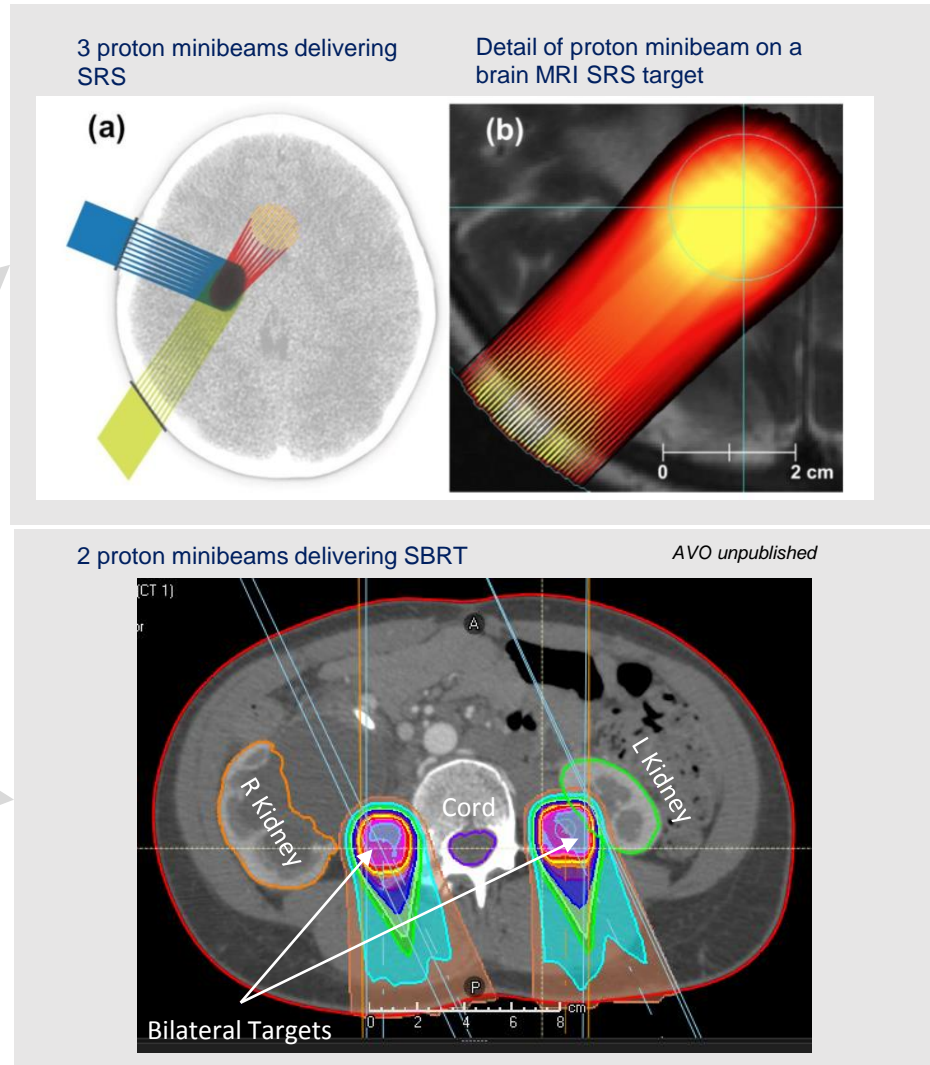


# LIGHT®: Higher Dose and Fewer Fractions



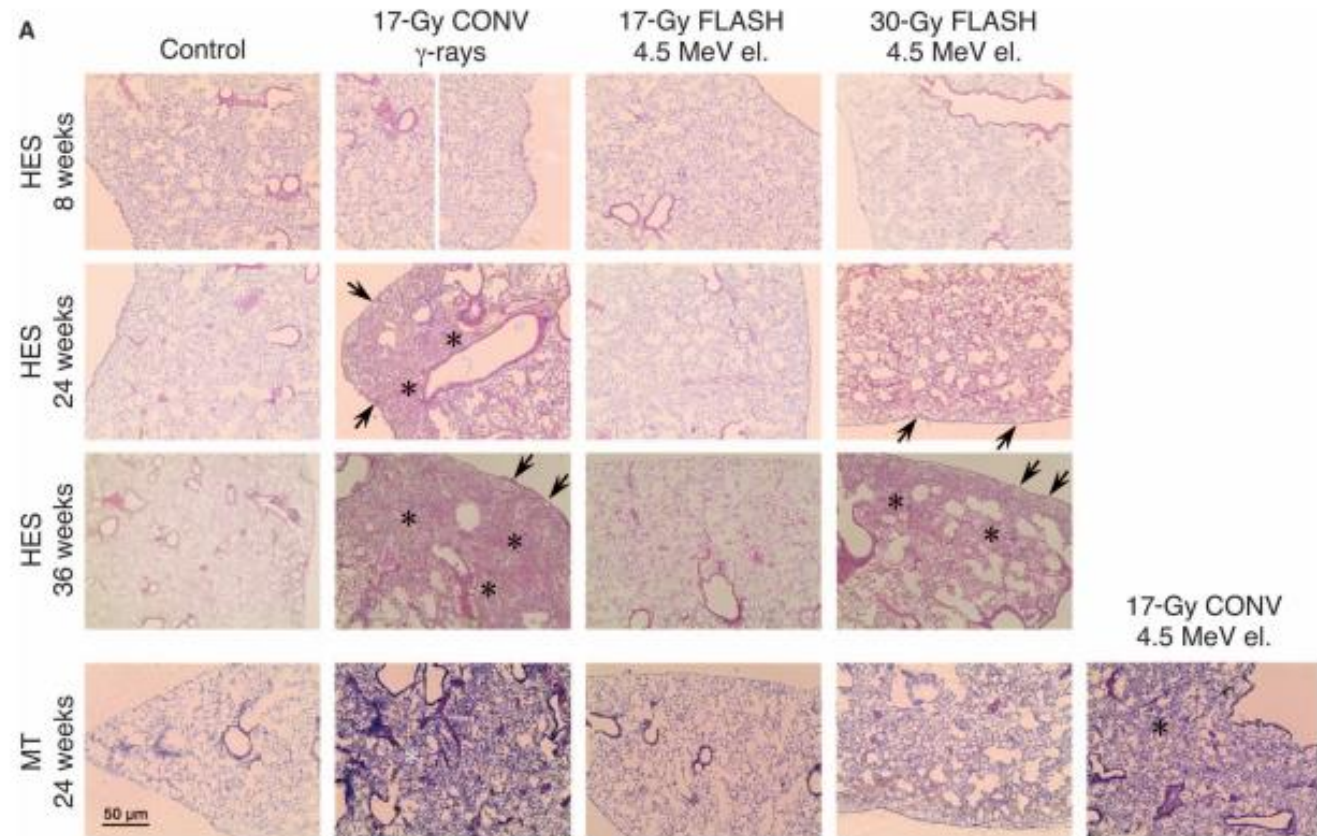
Source: Dilmanian, F. A., et al. (2015). "Minibeam therapy with protons and light ions: physical feasibility and potential to reduce radiation side effects and to facilitate hypofractionation." *Int J Radiat Oncol Biol Phys* 92(2): 469-474.

- **Hypofractions (large dose fractions) offer advantages:**
  - Fewer total treatments are required
  - Greater patient convenience
  - More patients treated in the facility per year
  - Increased revenue
- **Expected LIGHT® Hypofractionation performance:**
  - Stereotactic Radiosurgery (SRS): Competing with GammaKnife treatments, the AVO partner is investigating SRS conformity with modelled LIGHT® minibeam.
  - Stereotactic Body Radiotherapy (SBRT): Using rapid 3D rescanning and Active Range Control, LIGHT® is designed expected to be a breakthrough proton SBRT platform.
- **In addition, LIGHT® is intended for FLASH treatment and may be uniquely suited to the most effective application of FLASH**

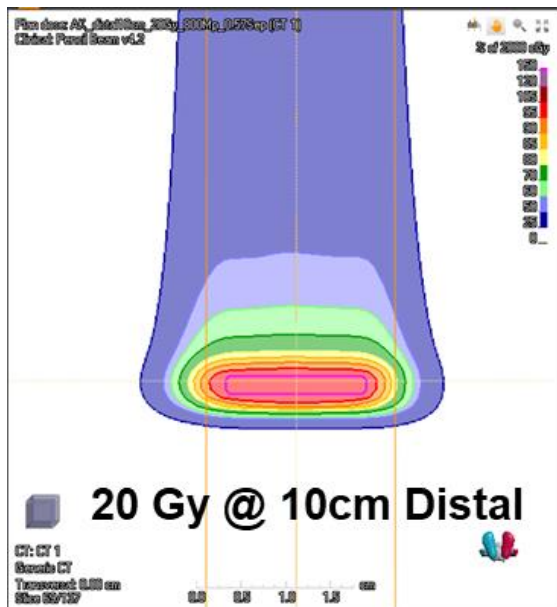


# FLASH

- FLASH involves high dose rates.
- Researchers are finding that tumours respond the same to FLASH treatments as they do with regular treatments, but that normal tissues have almost no response to FLASH
- Additional protection to normal tissue is provided
- Potential major impact on curing more cancer with less toxicity to the patient



# Proton FLASH



FLASHLIGHT planned irradiation to a 2 cm target cross-section at 10 cm depth in water.

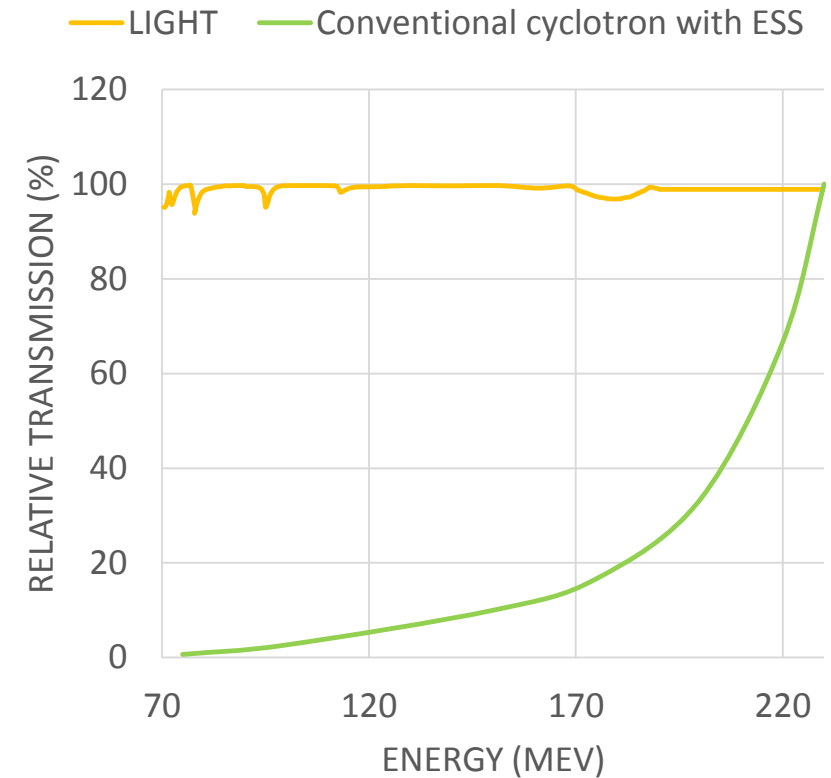
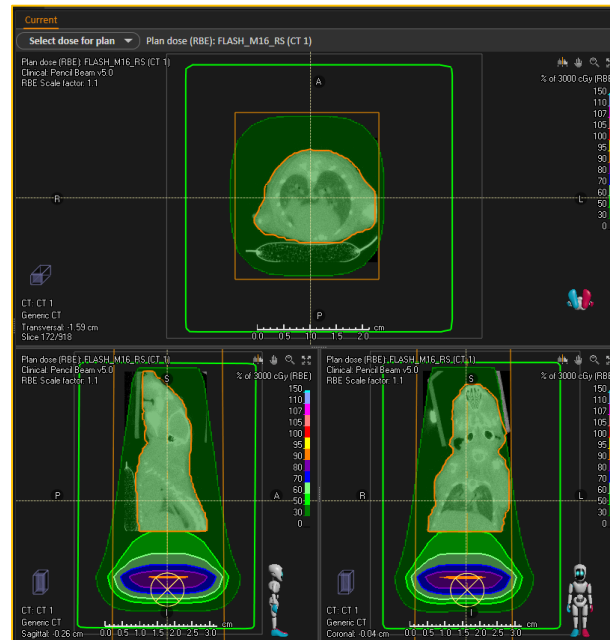
*LIGHT intends to provide FLASH treatments and may be uniquely suited to the most effective application of FLASH.*

		Dose [Gy]	Machine Max NP per pulse [Mp]	Min spot weight [10 <sup>6</sup> NP]	Max spot weight [10 <sup>6</sup> NP]	No of layers	Spot spacing [cm]	Snout position [cm]	No of repaintings	Time to deliver [s]	Mean Dose rate [Gy/s]
2 cm <sup>2</sup> x 0.2 cm	0.2 cm Depth	10	200	1.05	190.00	4	0.6	0.2	1	0.49	20.4
		20	500	17.21	474.98		0.62			0.49	41.3
		30	800	1.06	759.99		0.59			0.53	57.3
		40	800	1.56	760.00		0.59			0.50	80.2
	10 cm Depth	10	200	4.80	190.00	4	0.5	0.2	1	0.50	20.2
		20	500	8.62	474.95		0.5			0.47	43.0
		30	800	2.27	760.00		0.57			0.42	72.3
		40	800	81.69	760.00		0.57			0.43	93.1

# Proton FLASH

- Cyclotron
- Synchrocyclotron
- Synchrotron?
- Linac
- Scattering?
- Scanning?
- Target size?
- Target depth?

10 Gy FLASH dose  
distribution of a mouse  
planned using beam plateau.



A.M. Kolano, A. Degiovanni, **J. B. Farr**, Applications of Detectors and Accelerators to Medicine (ADAM) SA, Geneva, Switzerland, "Investigation on FLASH therapy using a high frequency linac for protons," ePoster, PTCOG, June, 2019, Manchester, England.

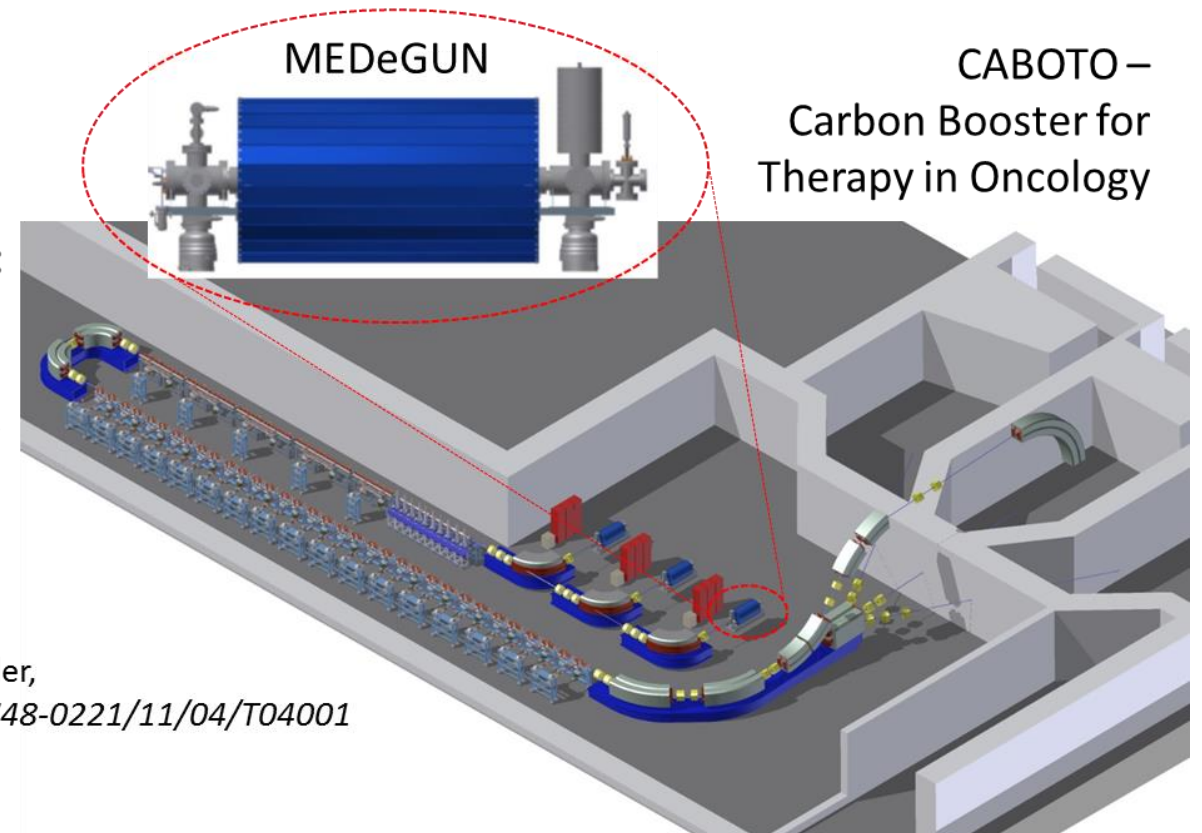
## CERN PIMMS2 Development

- Multiple ion sources
- 750 MHz RFQ
- High gradient LINAC cavities
- High gradient means high RF power: needs efficient low-cost RF power sources.
- The linac offers the advantage of pulse-to-pulse energy modulation at high repetition frequency.

HF-linac requirements:

- 300 – 400 Hz
- < 5  $\mu$ s pulses
- $10^8$  C<sup>6+</sup> ions per pulse

\* A. Shornikov and F. Wenander,  
<http://dx.doi.org/10.1088/1748-0221/11/04/T04001>



# Acknowledgements

Prof. Steve Myers  
Dr. Alberto DeGiovanni  
Dr. Anna-Maria Kolano  
Mr. Ondrej Sevela  
Dr. Sandra Aumon  
Dr. Manuel Gallas  
The Access Point 2 “Bunker Team”

Prof. Ugo Amaldi  
Dr. Mike Sinclair  
Mr. Nicolas Serandour  
The TERRA Fondation  
CERN  
UK Science & Technology Facilities Council  
AVO Investors  
RaySearch Labs AB