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of Glasgow



Hybrid Pixel Detectors

Trends for novel imaging techniques



Overview

Where we've come from

Diagnostic CT

Medipix

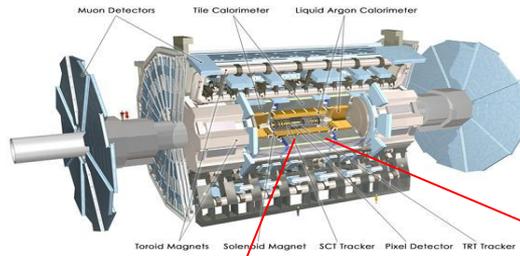
New Tricks

Where they're going (medicine)

Where we're going (technology)

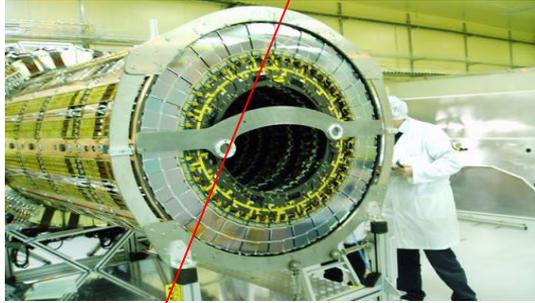


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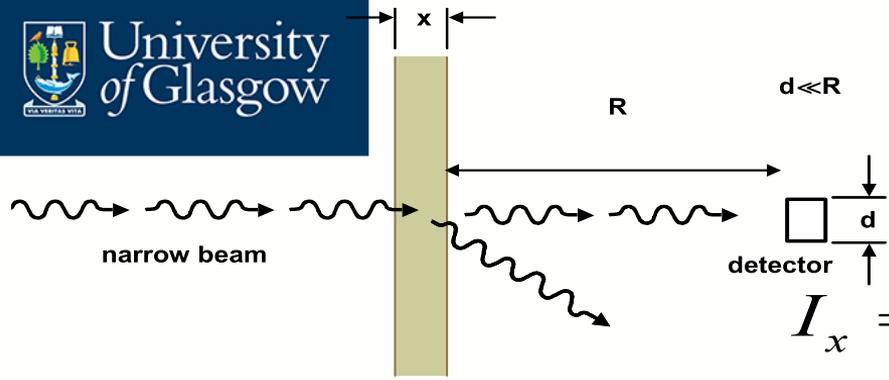


ATLAS SCT

(61m² of silicon sensors)

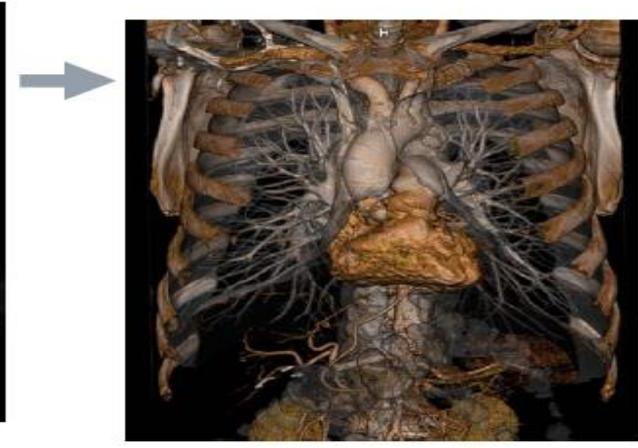
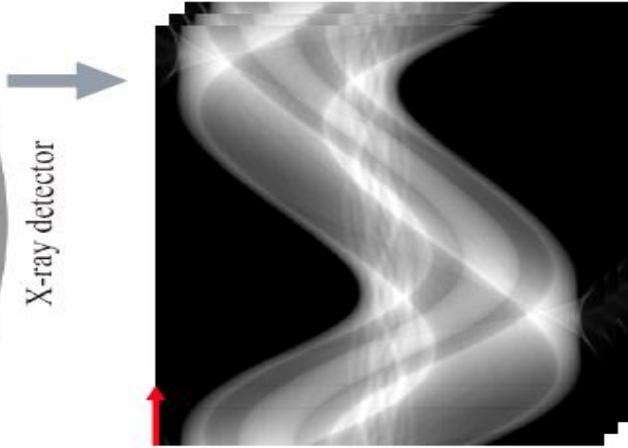
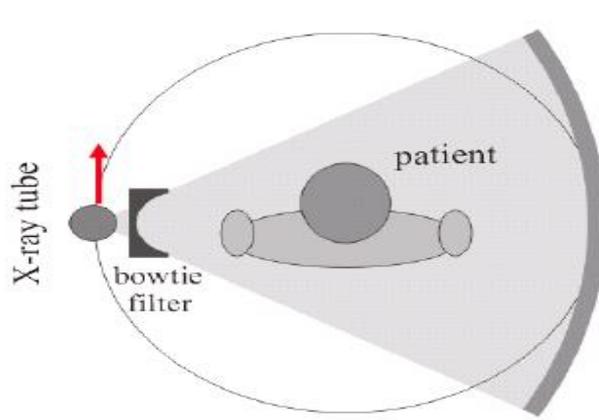
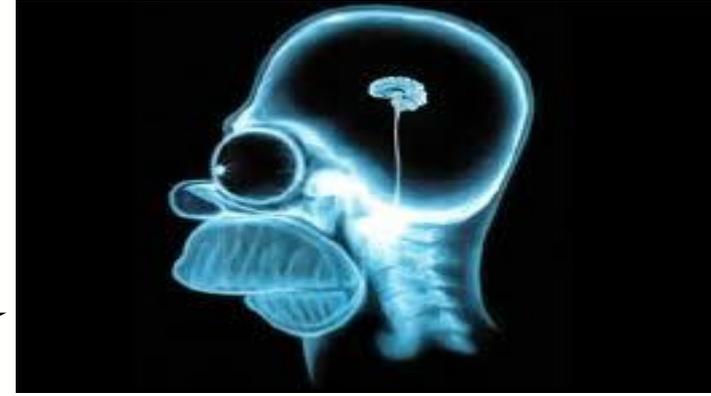


Diagnostic CT



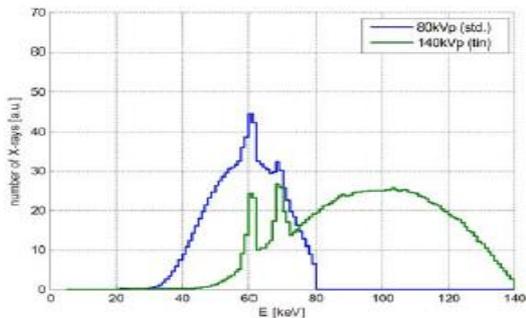
$$I_x = I_0 e^{-mx}$$

$$m = t + s + k$$





Dual-Source

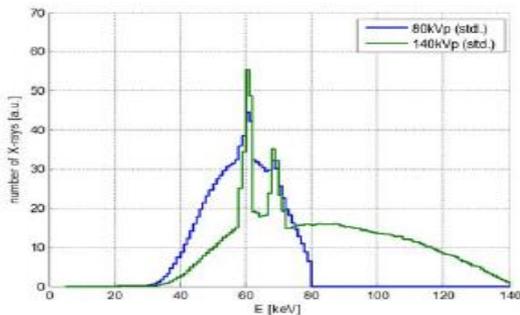


Well separated spectra due to filtration

Careful dose regulation needed

Geometrical registration is an issue

Fast kV-switching

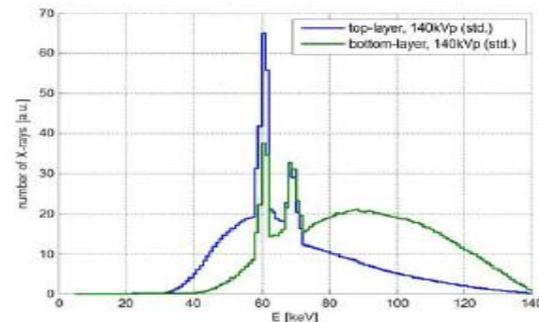


Single source device

Dose regulation is an issue

No filtration - spectral overlap
Sampling gaps

Dual-Layer



Single source device

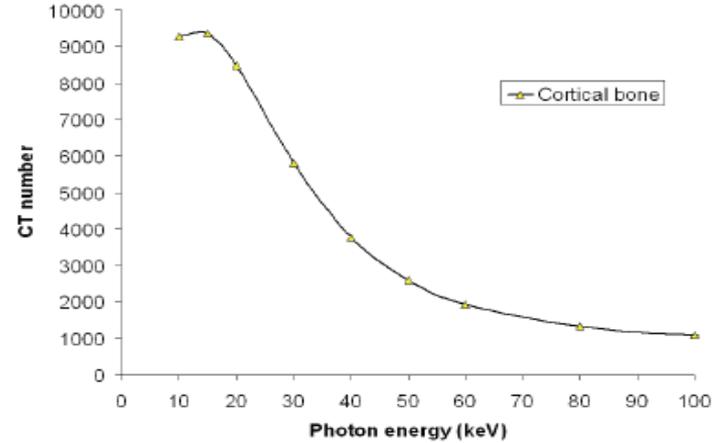
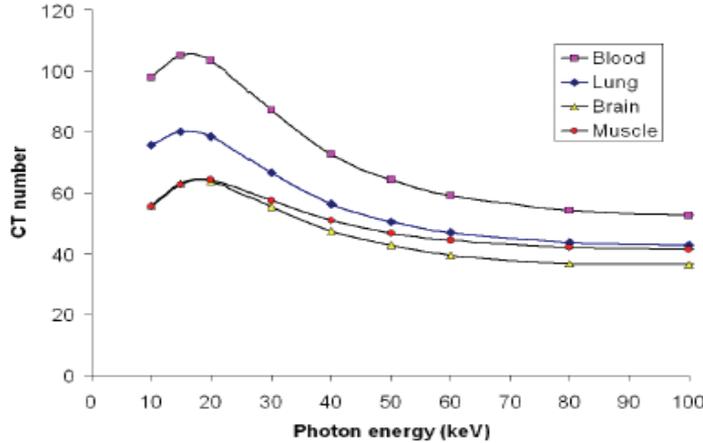
Data sets perfectly matched

Complex detector design

Poor spectral separation



Variation with Energy



$$CT_{number} = \frac{\mu_{material} - \mu_{water}}{\mu_{water}} \times 1000$$

$$I_x = I_0 e^{-m(E)x}$$

$$m_{photo} \gg \frac{Z^{4-5}}{E^3}$$

Ideally, when comparing the ratio density of tumour tissue, bone density for implants etc., an accuracy of better than ± 0.5 HU is desirable.



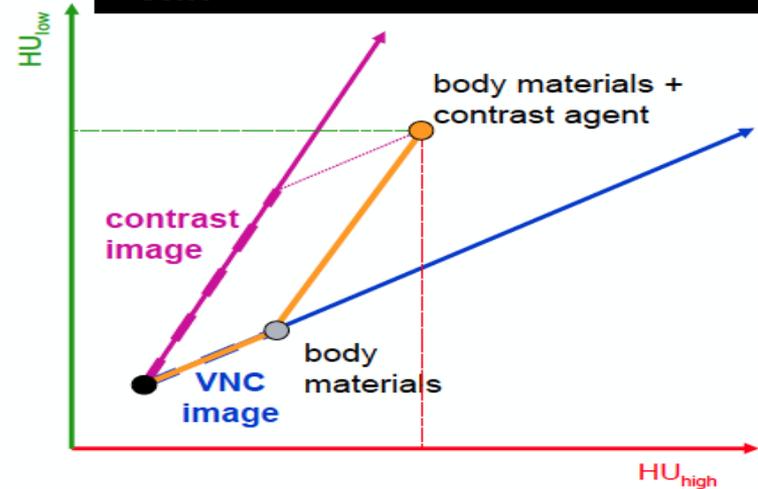
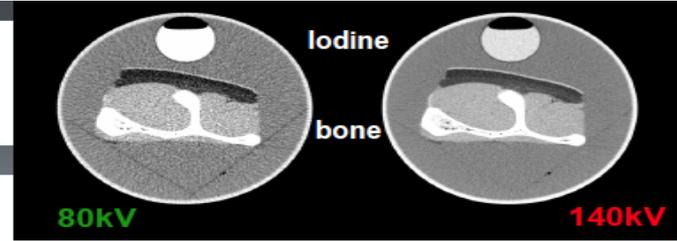
Dual-Energy

Dual-Energy Principle

- 2 scans with 2 different spectra
→ 2-dimensional HU space:
 HU_{low} vs. HU_{high} - -
- Coordinate transformations allow to change bases:
 Photoelectric vs. Compton
 Iodine vs. bone
 Contrast vs. VNC - -
- External constraints needed for higher order material classification

Clinical Applications

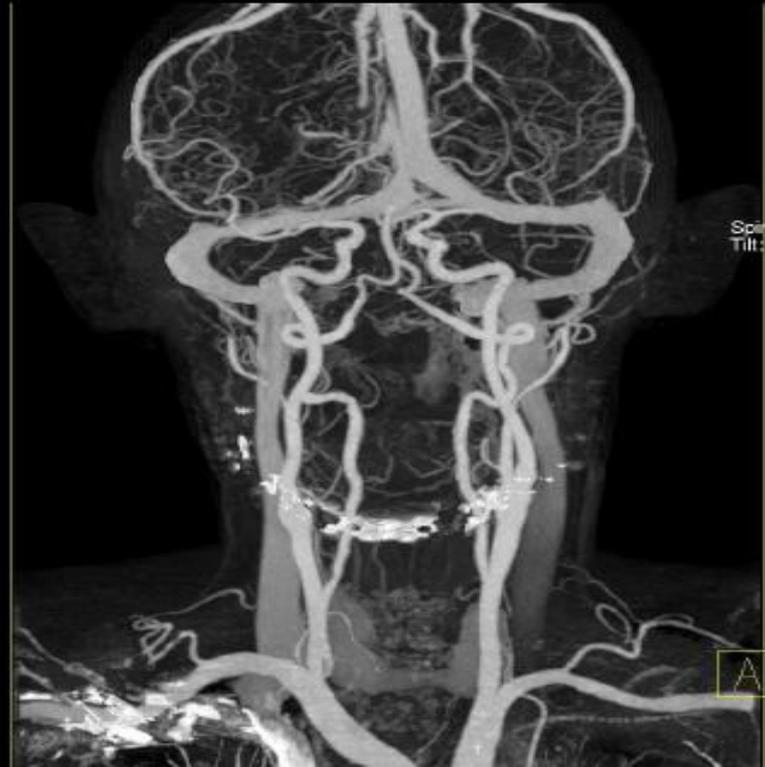
Bone removal, Iodine quantification, virtual non-contrast image (VNC), kidney-stone and gout characterization, pseudo-monoenergetic images, ...





Why Dual Energy??

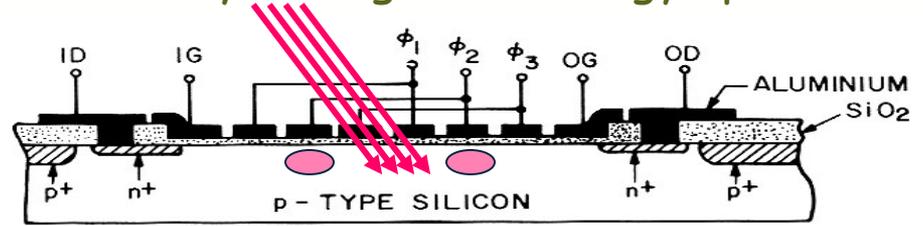
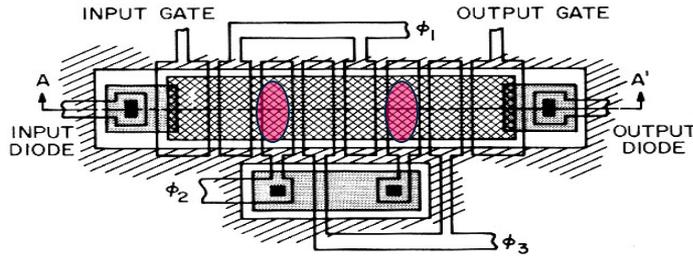
Bone Iodine separation - 'Bone removal'



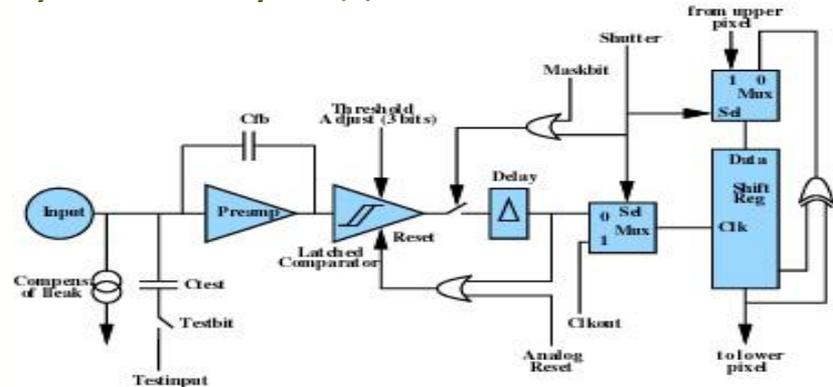
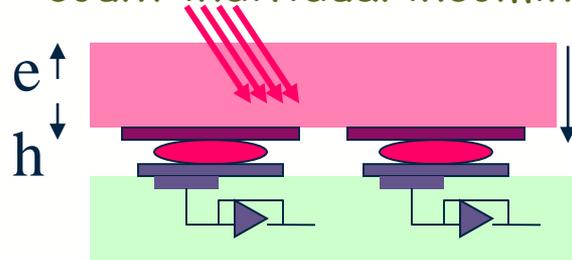


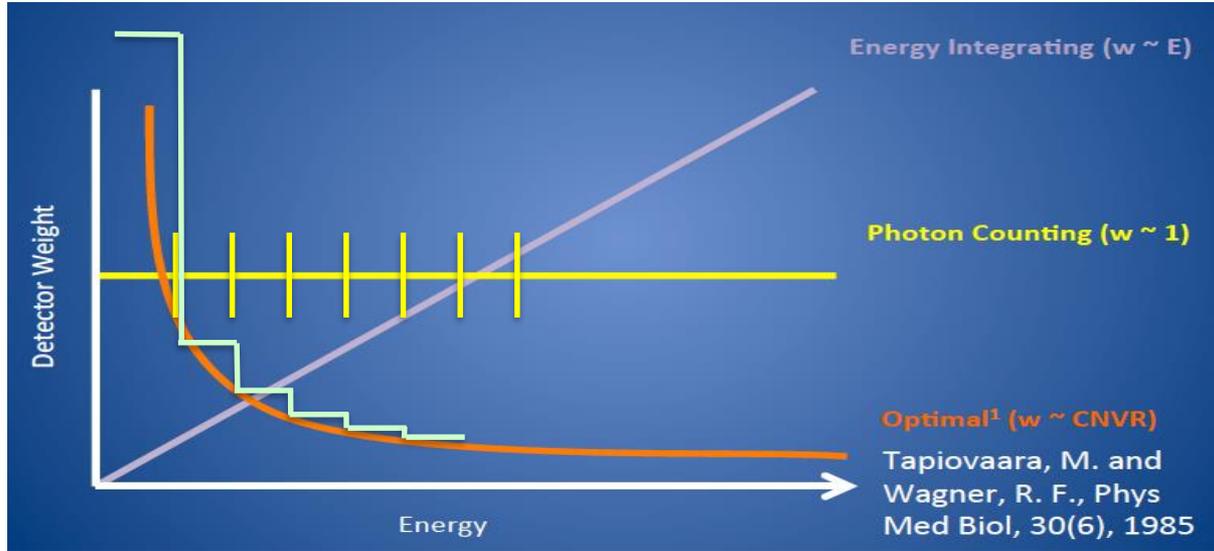
integration vs photon counting

CCD system: charge integration, affected by leakage and energy spread



count individual incoming photons, no leakage effects





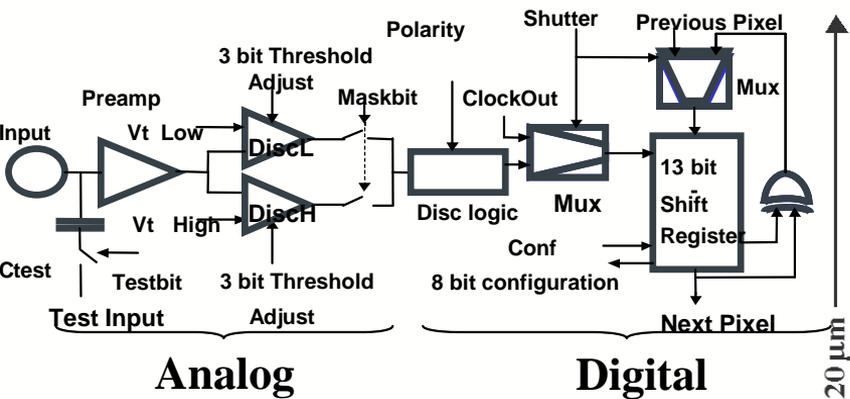
$$I_x = I_0 e^{-m(E)x}$$

$$m_{photo} \gg \frac{Z^{4-5}}{E^3}$$

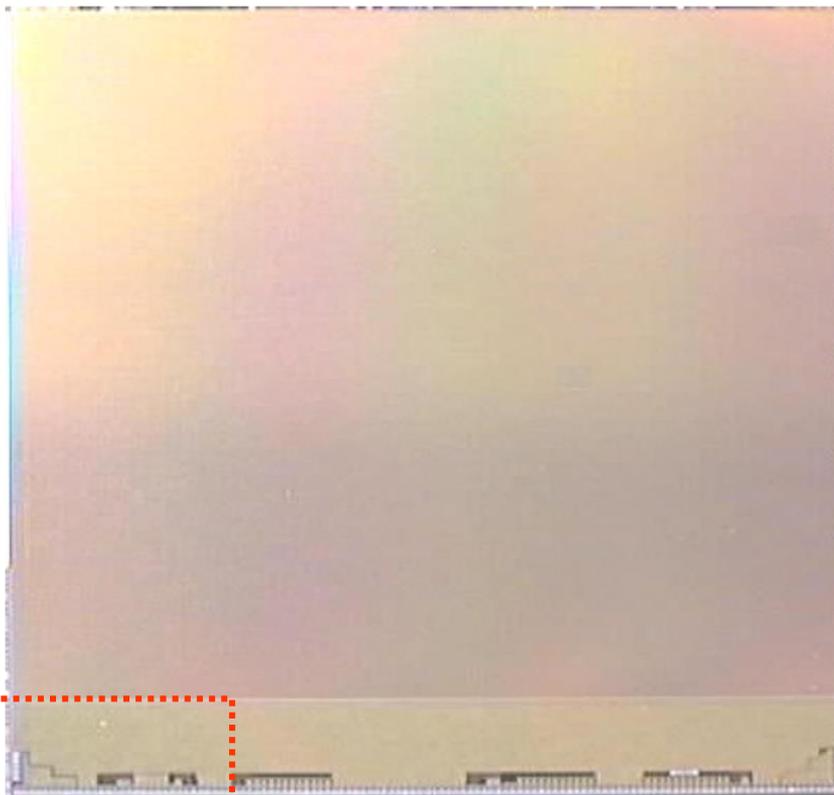
Simulations show that ~ 35% reduction in dose for equivalent image quality can be achieved



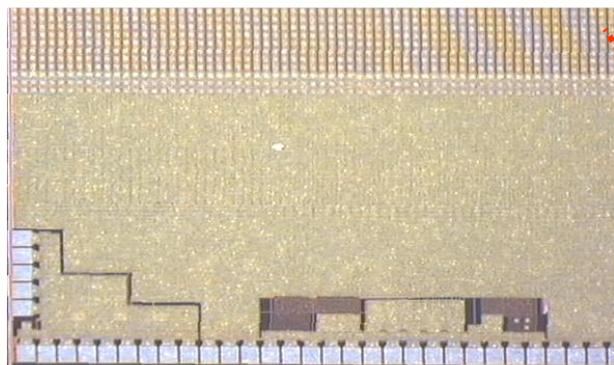
Medipix 2 ASIC



← 14111 μm → 256X55=14080

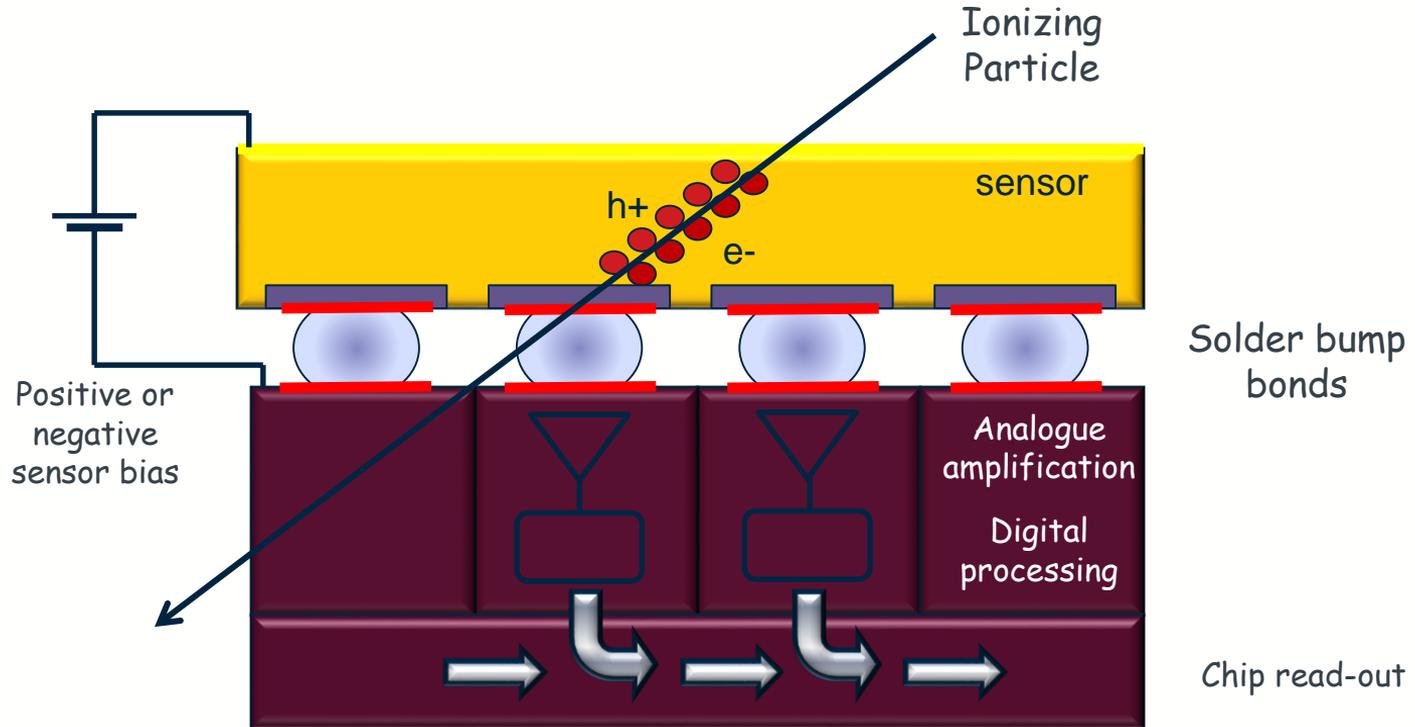


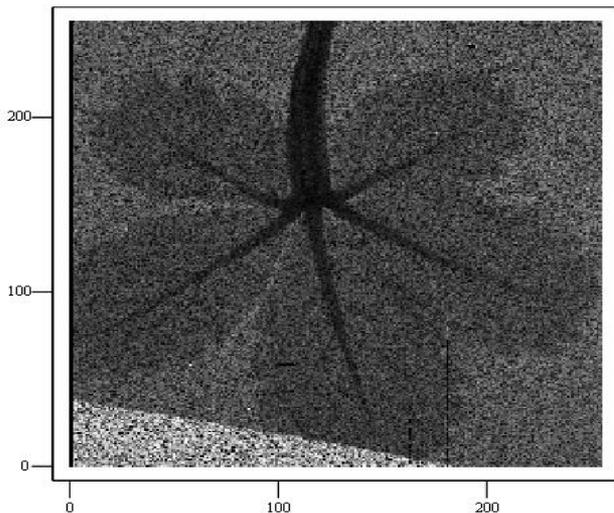
16120 μm



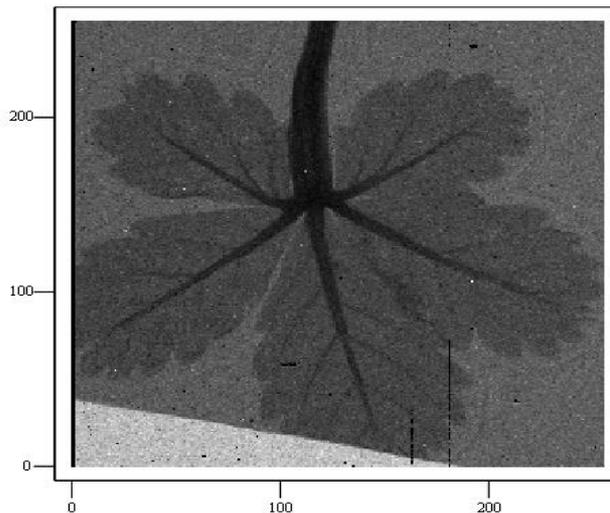


Bump Bonding

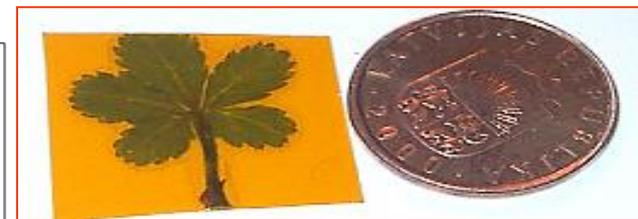




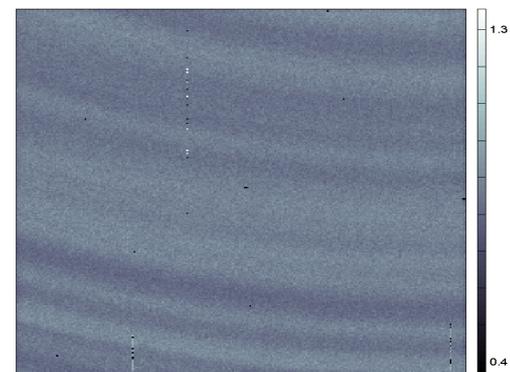
Uncorrected image



Corrected image



K8 S18



- Original image take during 10min with Fe^{55}
- 7 flood field images (2 hours each) were taken in order to find a flat field correction matrix



Timepix ASIC

Change discriminator to clock

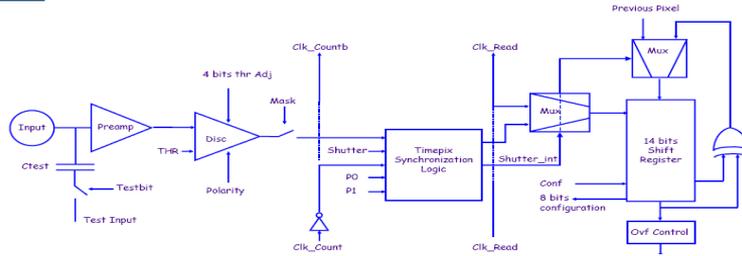
Use same config register

Can measure ToT

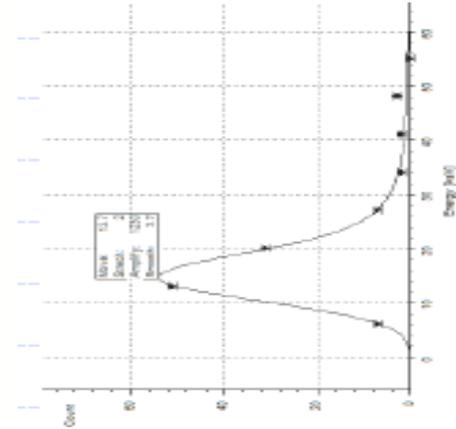
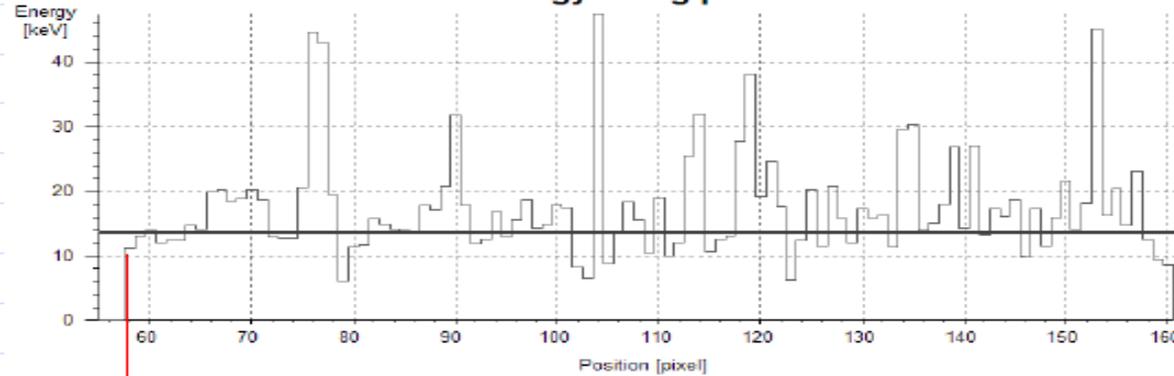
Can measure time to start/stop

Can photon count

Uses same ~ 500 transistors



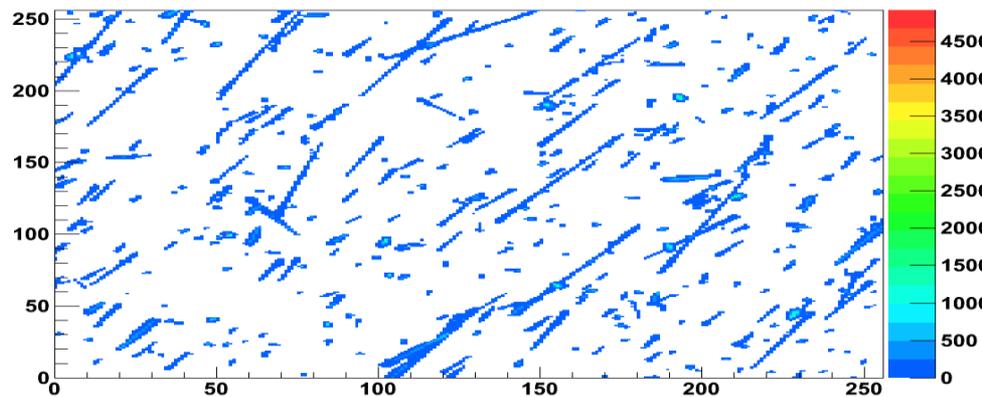
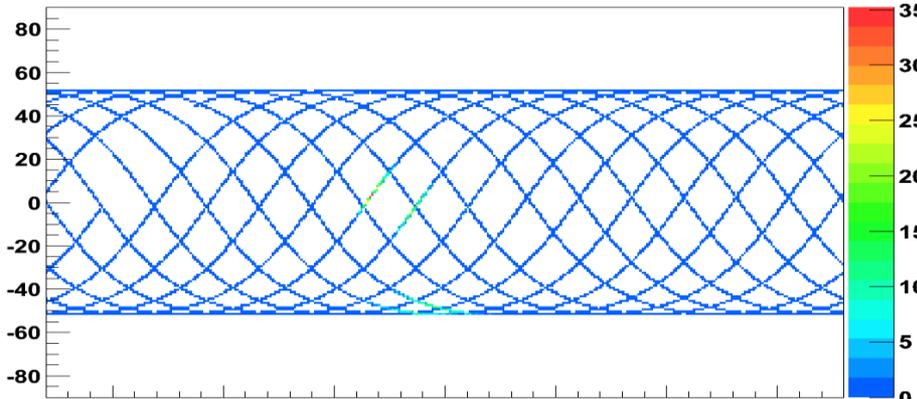
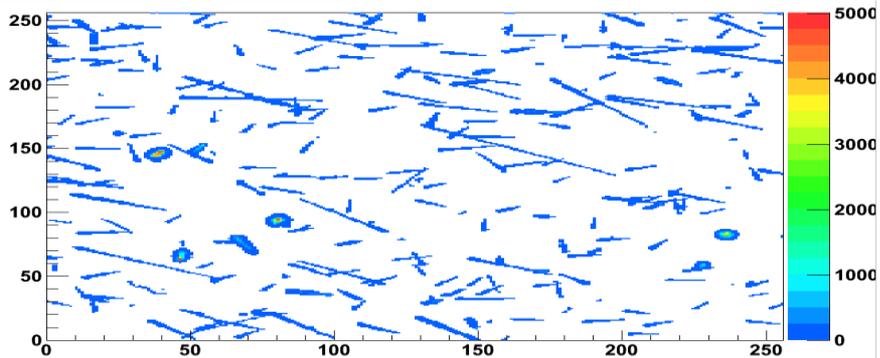
Energy along path



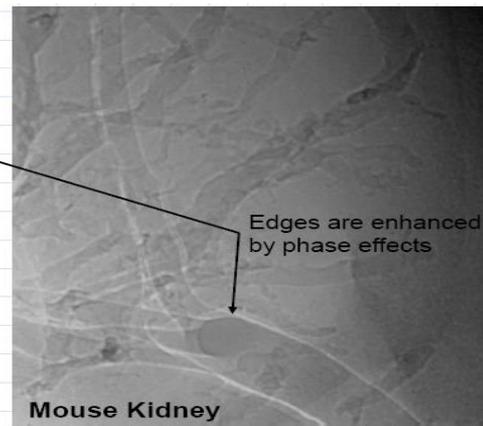
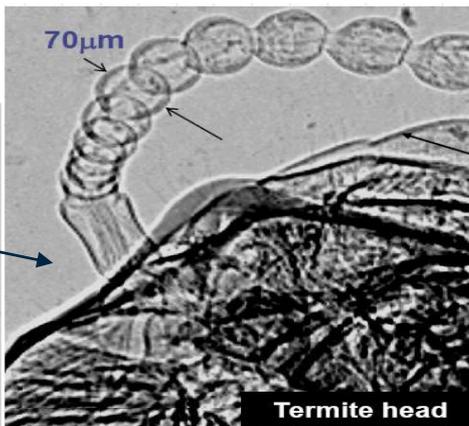
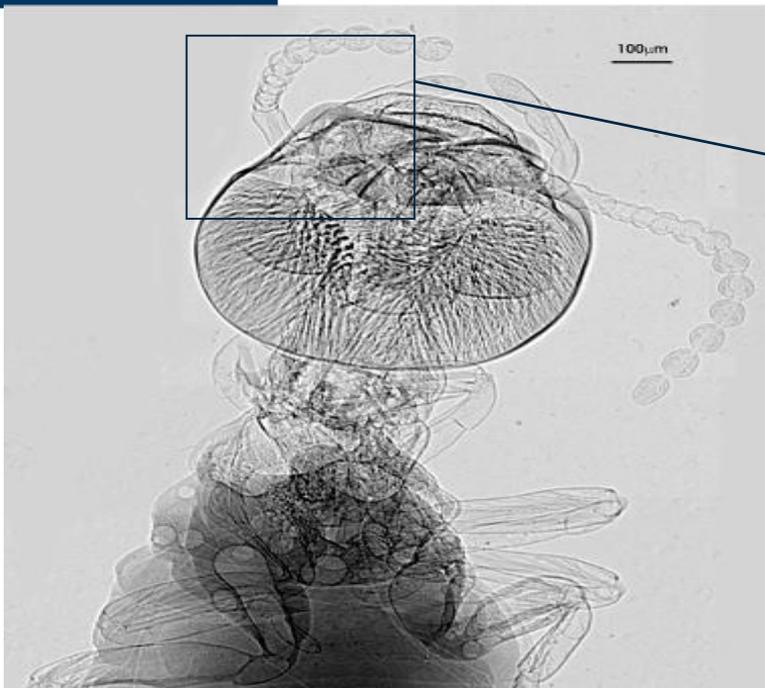


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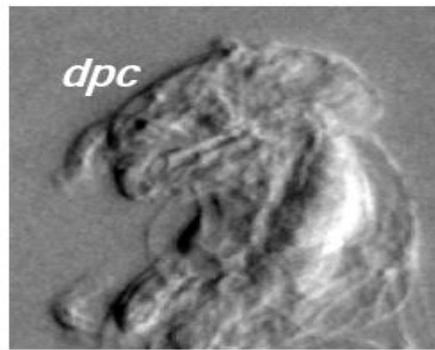
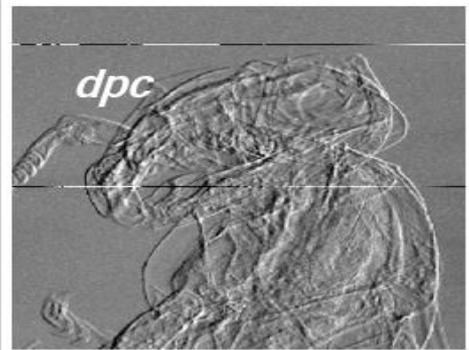
Dosimetry on ISS



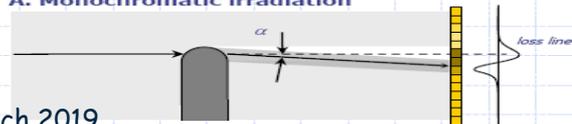
Val O'Shea CERN/Renault March 2019



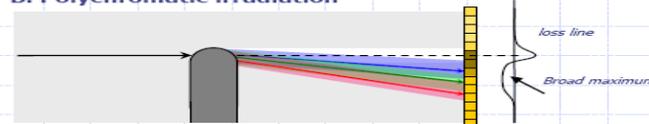
Edges are enhanced by phase effects



A. Monochromatic irradiation

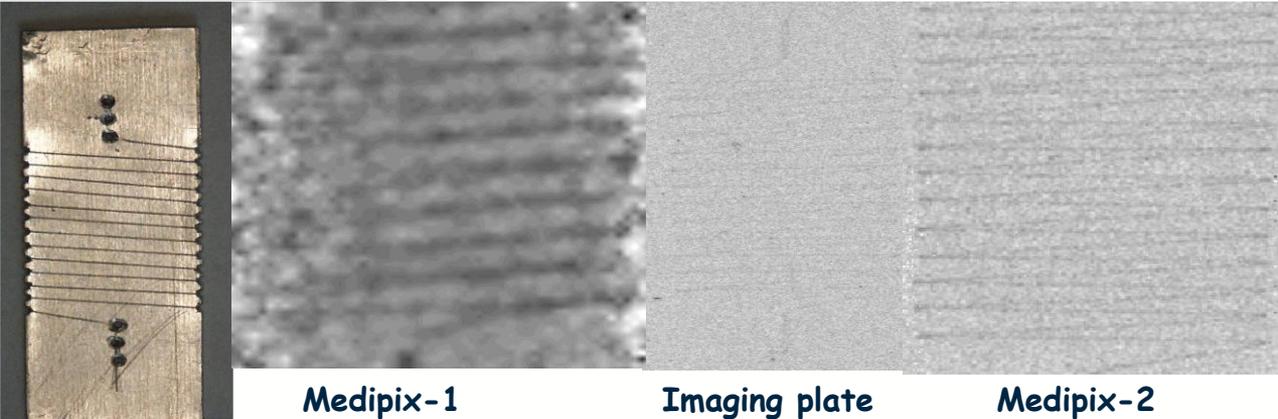


B. Polychromatic irradiation





Nylon Fishing line (0.1 mm)



Amorphous ^{10}B , naturally occurring 80%

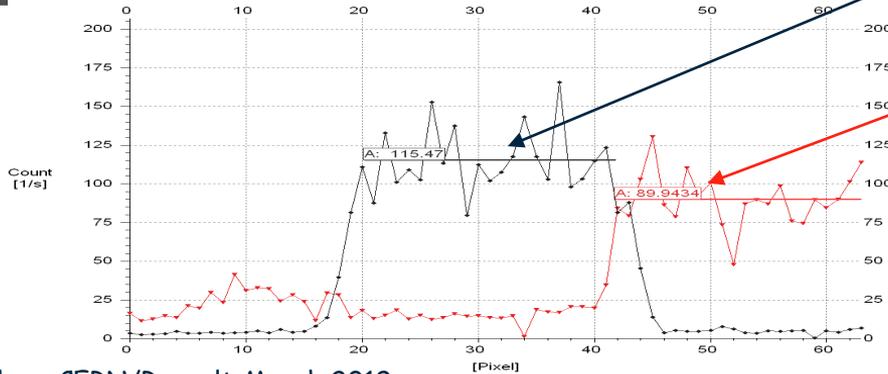
Medipix-1

Imaging plate

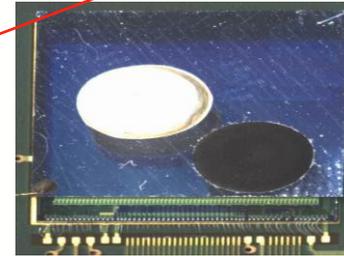
Medipix-2

Converter efficiency comparison

^6LiF , enrichment 90%



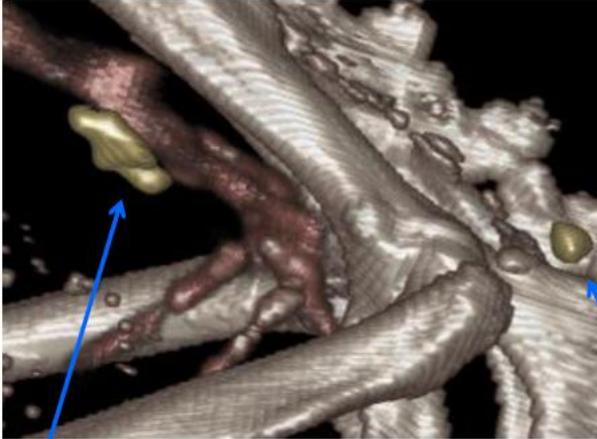
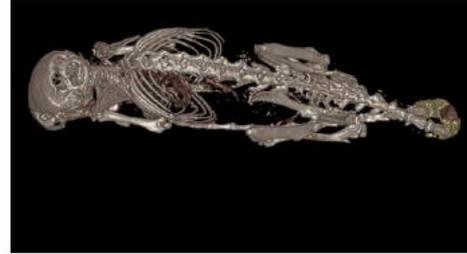
-0. ^{10}B
+1. ^6LiF



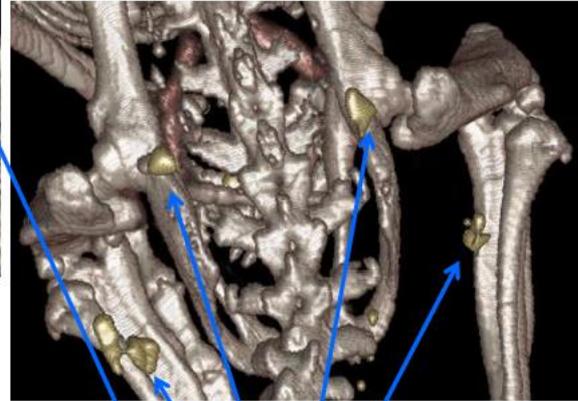
Ratio between ^6LiF efficiency and ^{10}B is 1.28



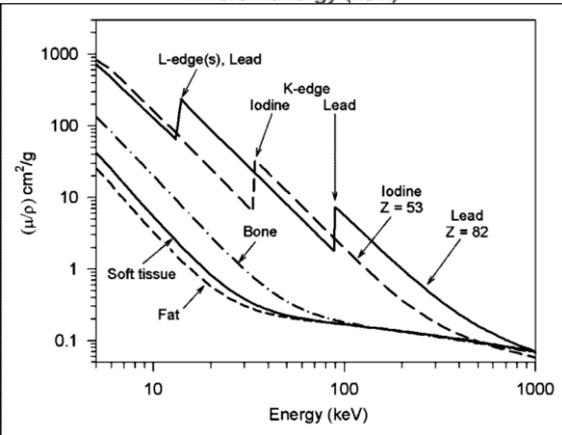
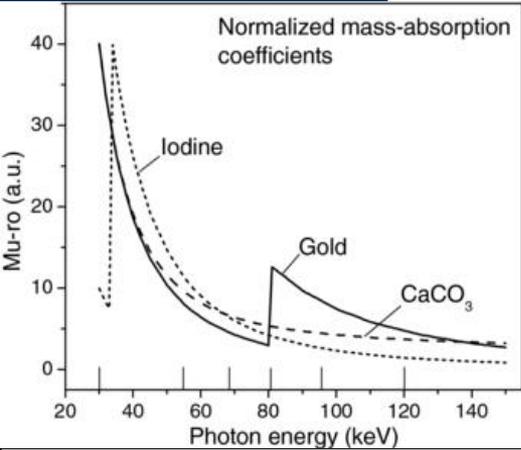
AU-HDL Macrophage-Imaging Spectral CT results



Aortic Bifurcation
“Vulnerable Plaque” detection
by Au-NP uptake of macrophages



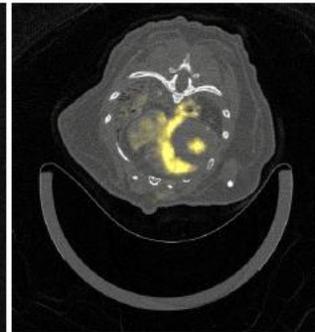
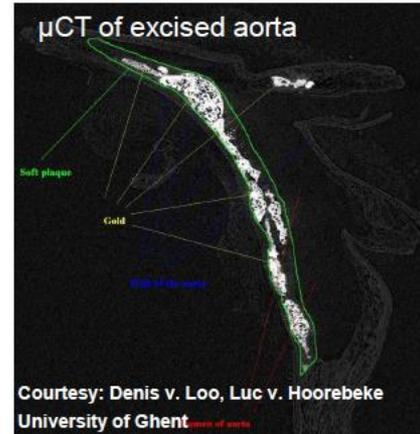
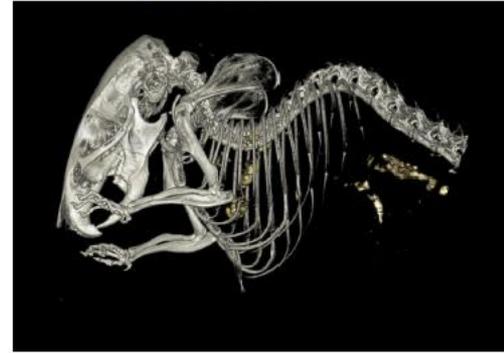
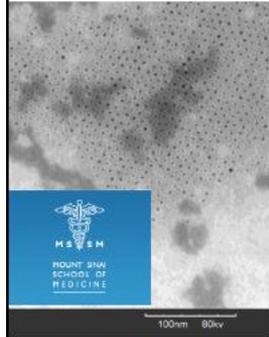
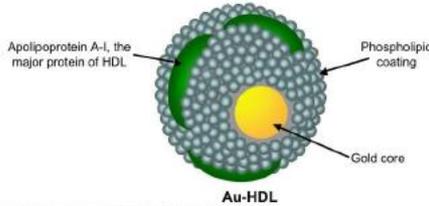
Uptake in 4 lymphnodes



K-edge imaging of gold

High-density lipoprotein (HDL)-coated gold nano-particles: Au-HDL

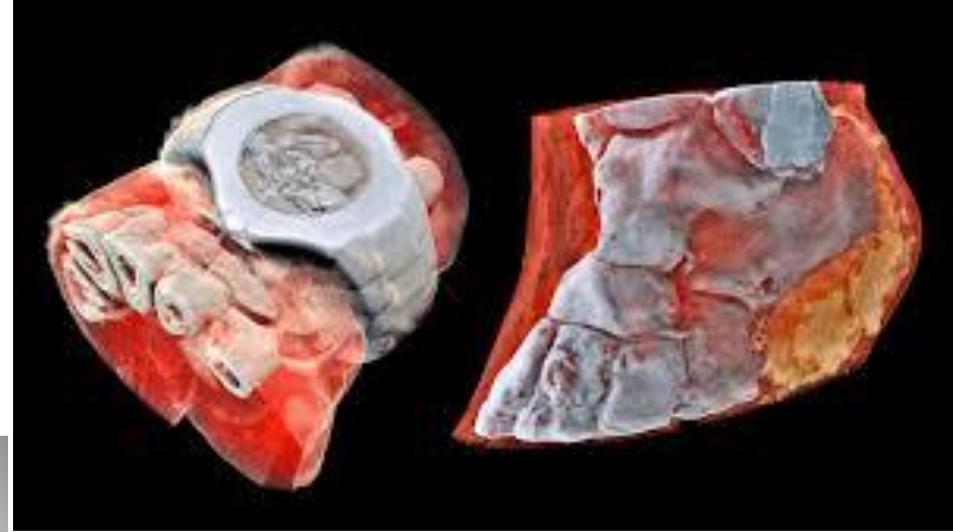
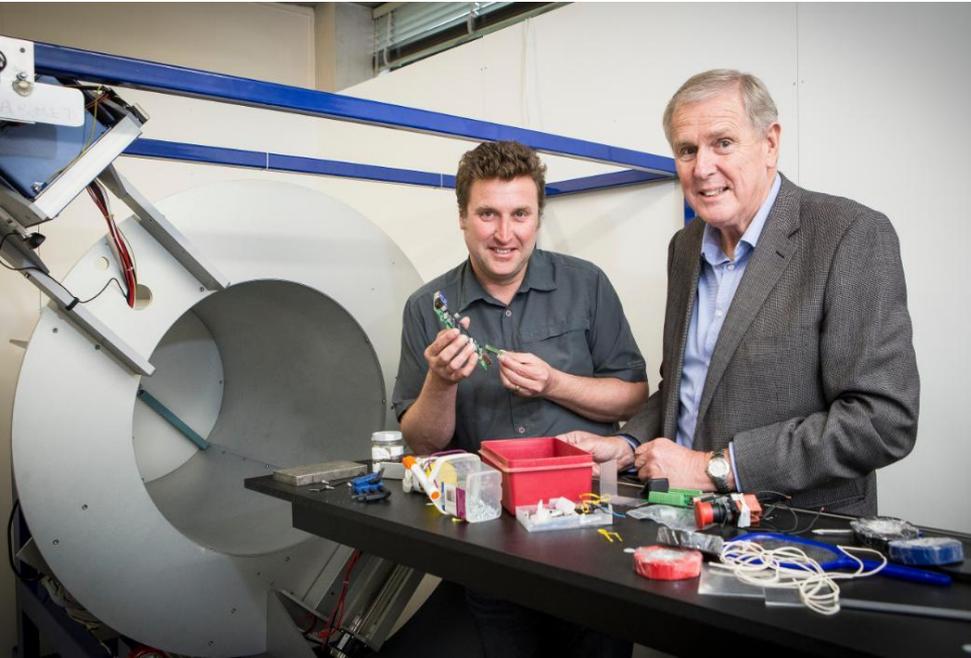
- Nano-particle being taken up by macrophages
- High risk atherosclerotic plaque has increased macrophage density
- Au-HDL is ~10 nm in diameter



Lowest bin (25-34 keV) with Au-overlay



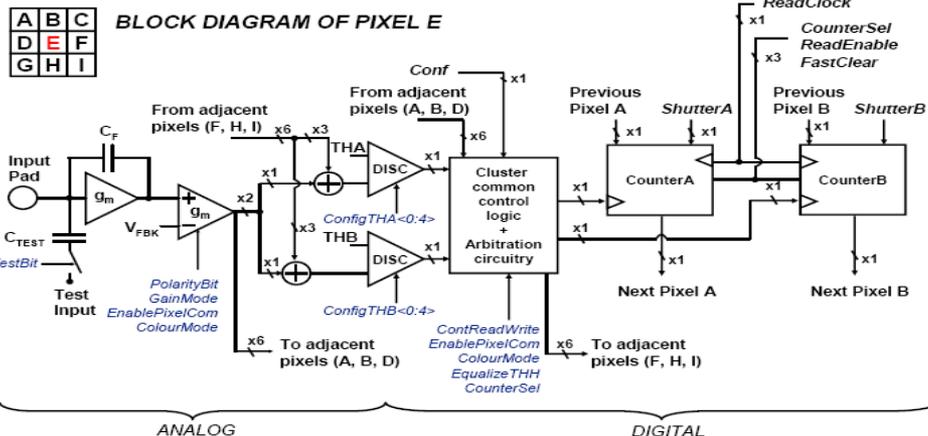
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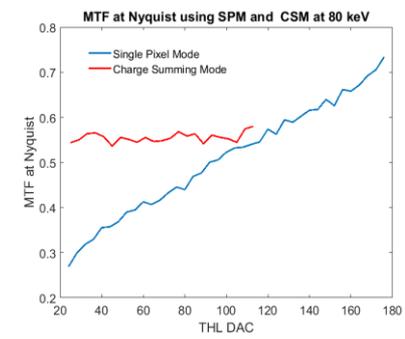
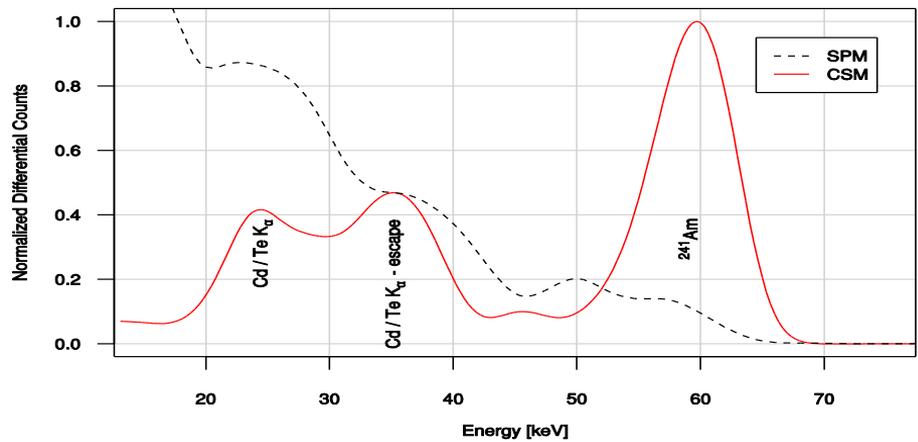
Mars Bioimaging small animal spectral CT scanner used to image live human tissue in trial - 2018. Scanner uses Medipix technology.



- o ~1400 transistors per pixel
- o Simultaneous read/write
- o Charge summing mode
- o Colour mode



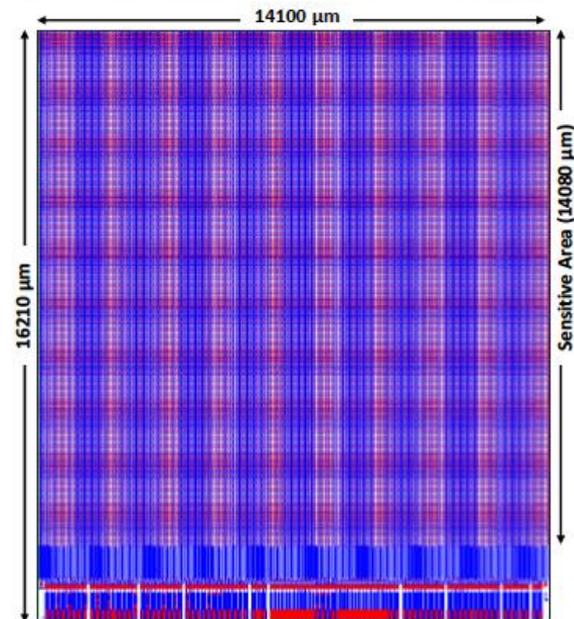
Charge sharing eliminated for 55 um pixels
 TSVs for seamless tiling of large surfaces
 Integration into small animal CT scanners





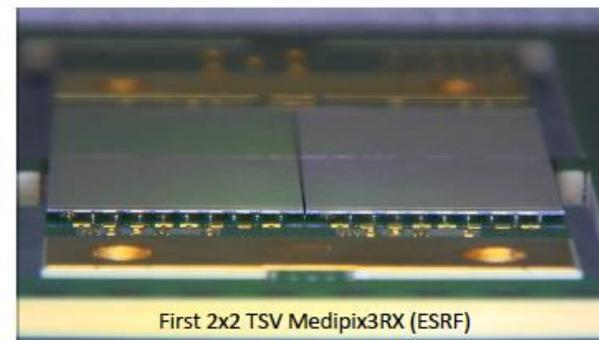
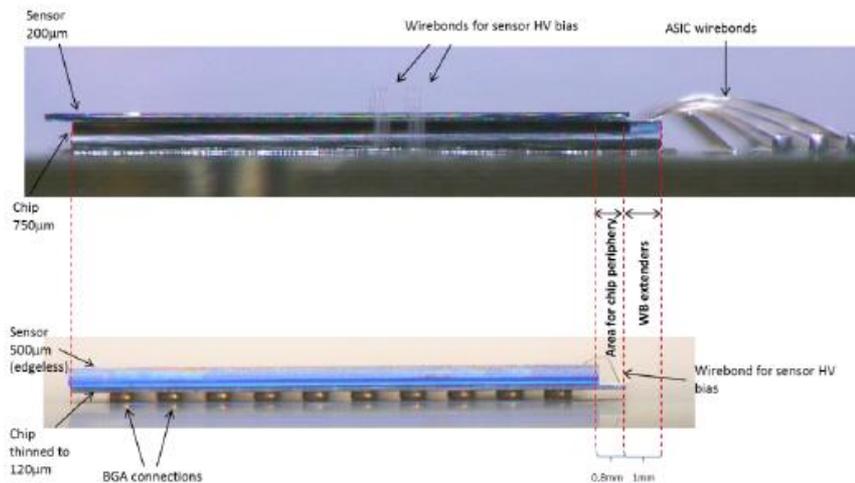
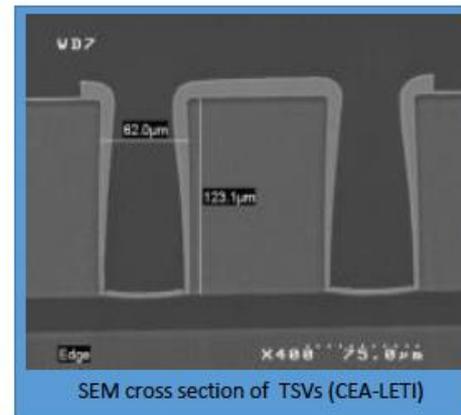
Timepix3 (2013)

Application	General Purpose particle tracking
Technology	IBM 130nm DM 4-1
Pixel size	55 x 55 μm^2
Pixel arrangement	256 x 256 (2x4 superpixels)
Acquisition modes	<ol style="list-style-type: none"> 1) Time (TOA) AND Charge (TOT) 2) Time (TOA) 3) PC & integral charge (iTOT)
Readout Type	<ol style="list-style-type: none"> 1) Data driven (Shutter-less) 2) Frame-based (Shutter)
Thresholds	1
Minimum threshold	> 500 e-
Time resolution (TOA)	1.562 ns
Energy Resolution (TOT)	$\sim 2 \text{ keV}_{\text{FWHM}}$
Power consumption	<1.5W @1.5 V
Floorplan	3 sides buttable and minimum periphery
TSVs possibility	YES. With 1.2mm periphery
Count Rate	Data-Driven: $\sim 0.43 \times 10^6 \text{ hits/mm}^2/\text{s}$ Frame-based: $826 \times 10^6 \text{ hits/mm}^2/\text{s}$
Output bandwidth	1 to 8 SLVS DDR @640Mbps each



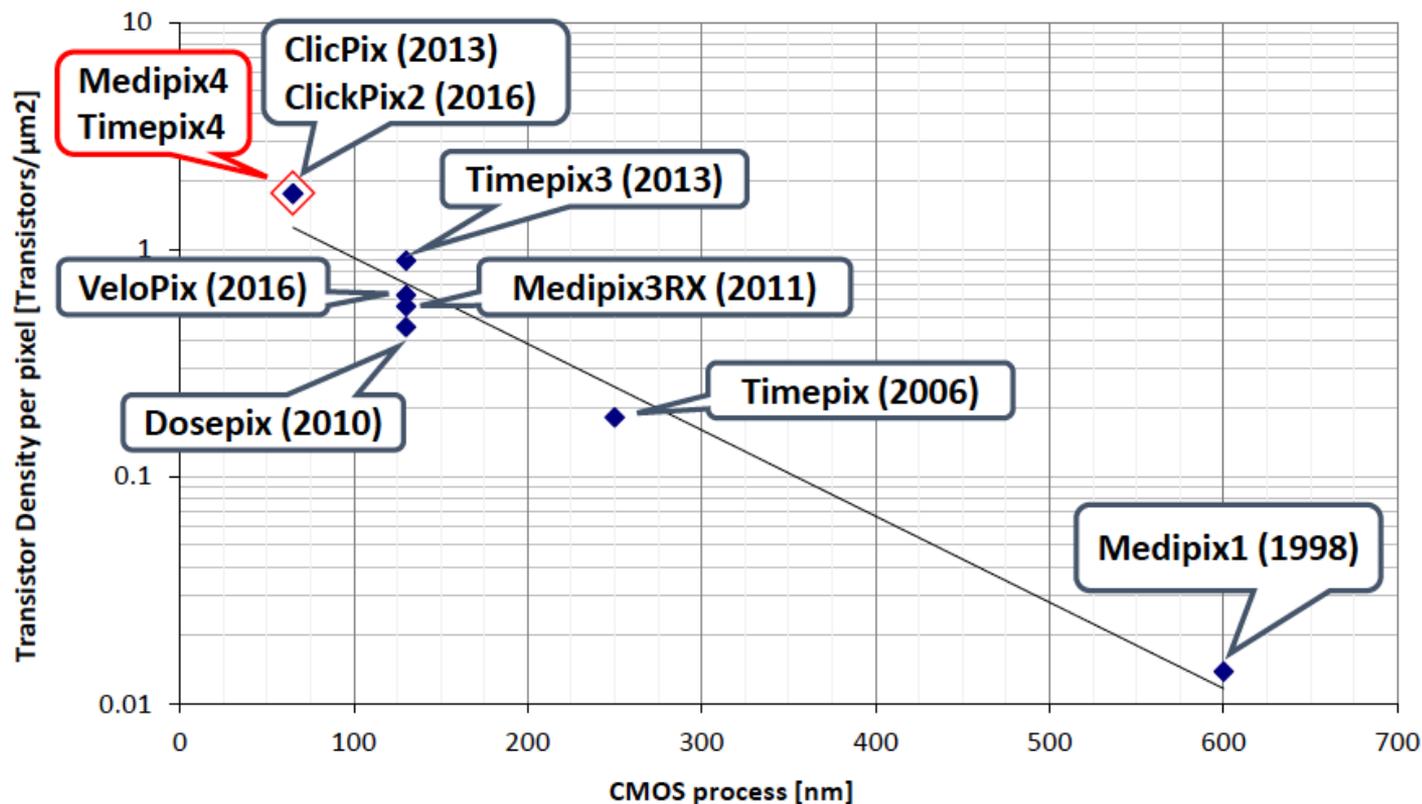


TSV Process





Pixel detectors ASICs developed @CERN





Timepix3 → Timepix4

Timepix4: A 4-side tillable large single threshold particle detector chip with improved energy and time resolution and with high-rate imaging capabilities

			Timepix3 (2013)	Timepix4 (2018/19)	
Technology			CMOS 130nm – 8 metal	CMOS 65nm – 10 metal	
Pixel Size			55 x 55 μm	55 x 55 μm	
Pixel arrangement			3-side buttable 256 x 256	4-side buttable 512 x 448 3.5x	
Sensitive area			1.98 cm^2	6.94 cm^2	
Readout Modes	Data driven (Tracking)	Mode	TOT and TOA		
		Event Packet	48-bit	64-bit 33%	
		Max rate	< 43 Mhits/ cm^2/s	178.8 Mhits/ cm^2/s 4x	
	Frame based (Imaging)	Mode	PC (10-bit) and iTOT (14-bit)	CRW: PC (8 or 16-bit)	
		Frame	Zero-suppressed (with pixel addr)	Full Frame (without pixel addr) CRW (8-bit / 16-bit) Up to 44 KHz frame @8b	
		Max count rate	82 Ghits/ cm^2/s	~800 Ghits/ cm^2/s 10x	
TOT energy resolution			< 2KeV	< 1KeV 2x	
Time resolution			1.56ns	~200ps 8x	
Readout bandwidth			≤5.12Gb (8x SLVS@640 Mbps)	≤81.92 Gbps (16x @5.12 Gbps)	
Target global minimum threshold			<500 e^-	<500 e^-	



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Swiss technology comparison



Timepix (2006)



Timepix3 (2013)



Serenity

• Generic development card

- Different FPGAs – KU115, KU15P, VU9P
- Multiple SerDes routing topologies

• Samtec Interposer Connector Array

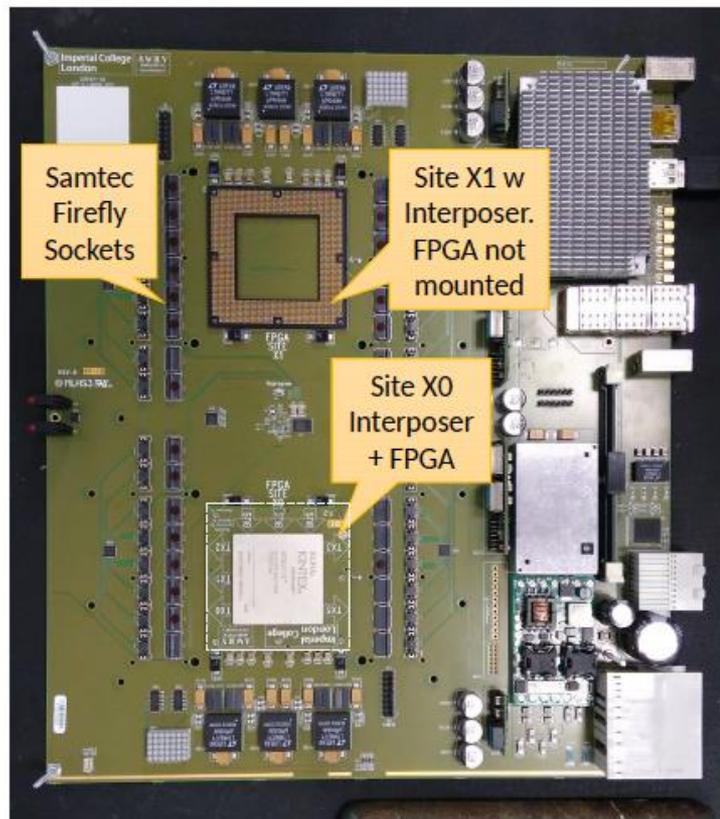
- Dual 72 Rx/Tx Chan Optical Site
 - Plus 64 inter-interposer pairs
- Dual 96 Rx/Tx Chan Optical Site
 - Plus 16 inter-interposer pairs
- QSFP for DAQ

• Slow Control / SOC

- COM-Express Type 10
 - Quad-core Atom, up to 2.2 GHz, 8 GB RAM
- IPBus over PCIe/AXI

Bristol University, Imperial College, Ioannina, INFN, KIT, RAL, SACLAY, TIFR

So much data - we need one of these...





University
of Glasgow

Thank You..... Questions?

val.o'shea@glasgow.ac.uk

#UofGWorldChangers



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