



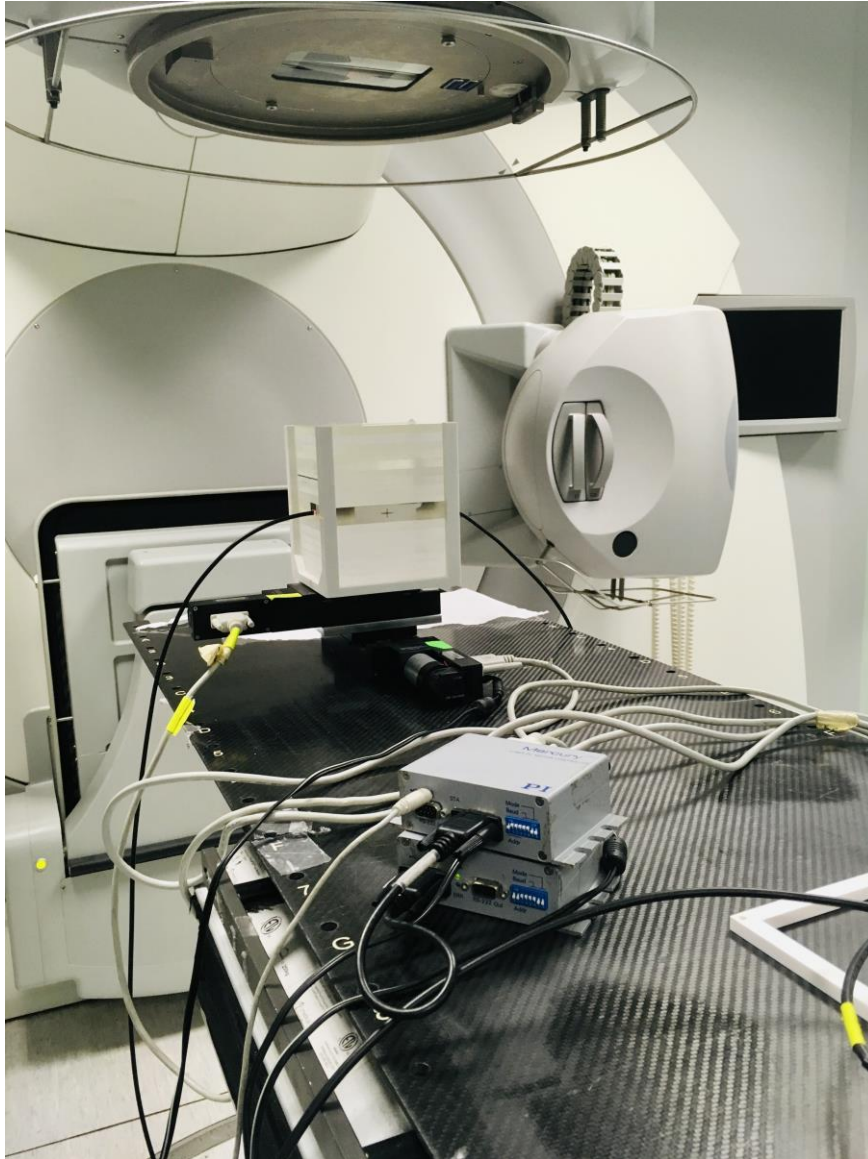
22nd International Workshop on Radiation Imaging Detectors



Istituto Nazionale di Fisica Nucleare

Intercalibration and comparative tests of 3D diamond and diamond on iridium detectors for medical dosimetry

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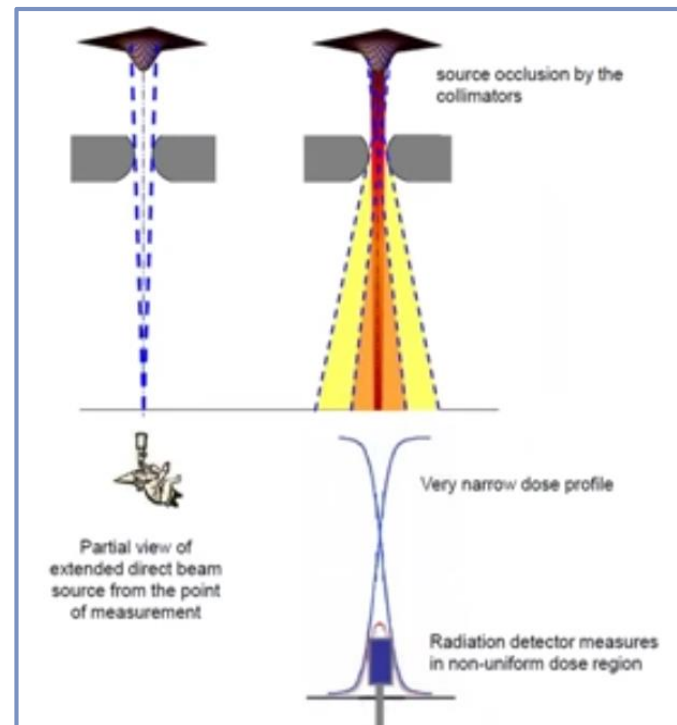
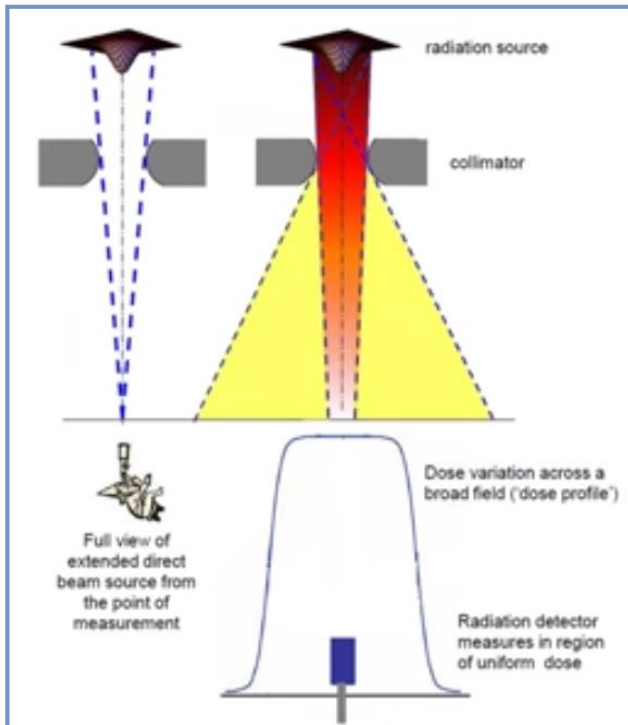
Collaborations:

University of Manchester

University of Wollongong

“The Christie” Hospital Manchester,
Santa Maria della Misericordia Perugia,
Careggi Firenze,
Santa Maria Terni,
Città di Castello.

- ✓ Small field dosimetry issues
- ✓ 3D diamond detectors
- ✓ Characterization of two 3D detectors made off different substrates (polycrystalline diamond and diamond on iridium) using an x-ray tube
- ✓ 3D polycrystalline diamond detector dosimetric measurements with a medical linear accelerator
- ✓ Conclusions



- Partial occlusion of the primary source + lack of electronic balance
- Strong dose reduction on the central axis of the beam



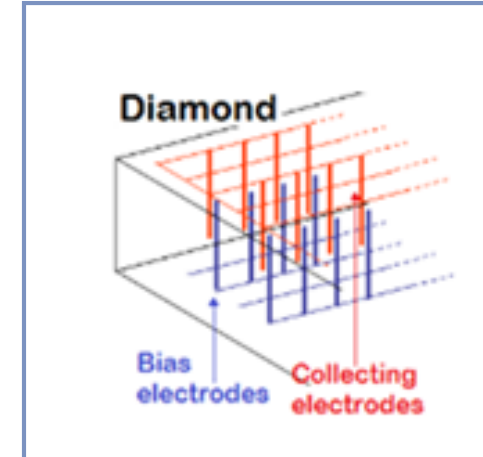
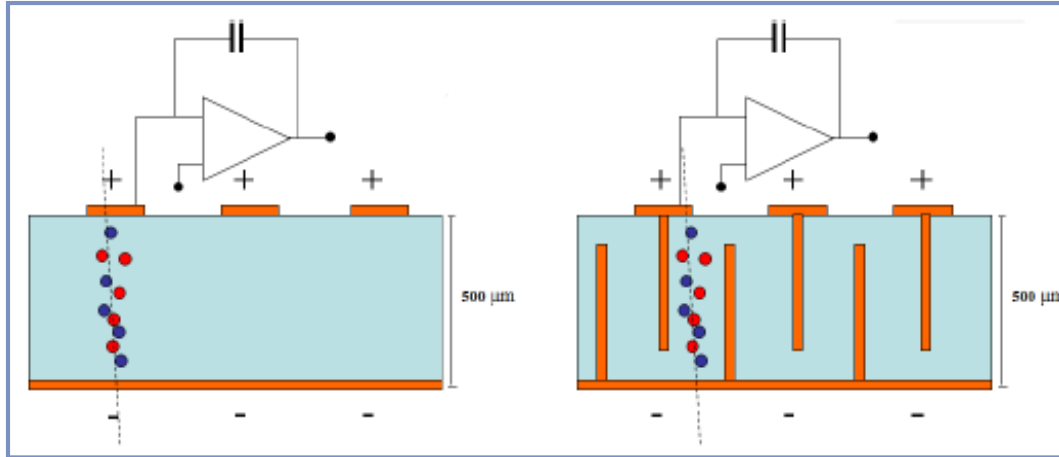
- Errors due to incorrect use of the detectors in the dosimetry of small fields

The presence of the dosimeter introduces a perturbation of the fluency of the charged particles because it is different in density and composition from the human body.

The effect depends on:

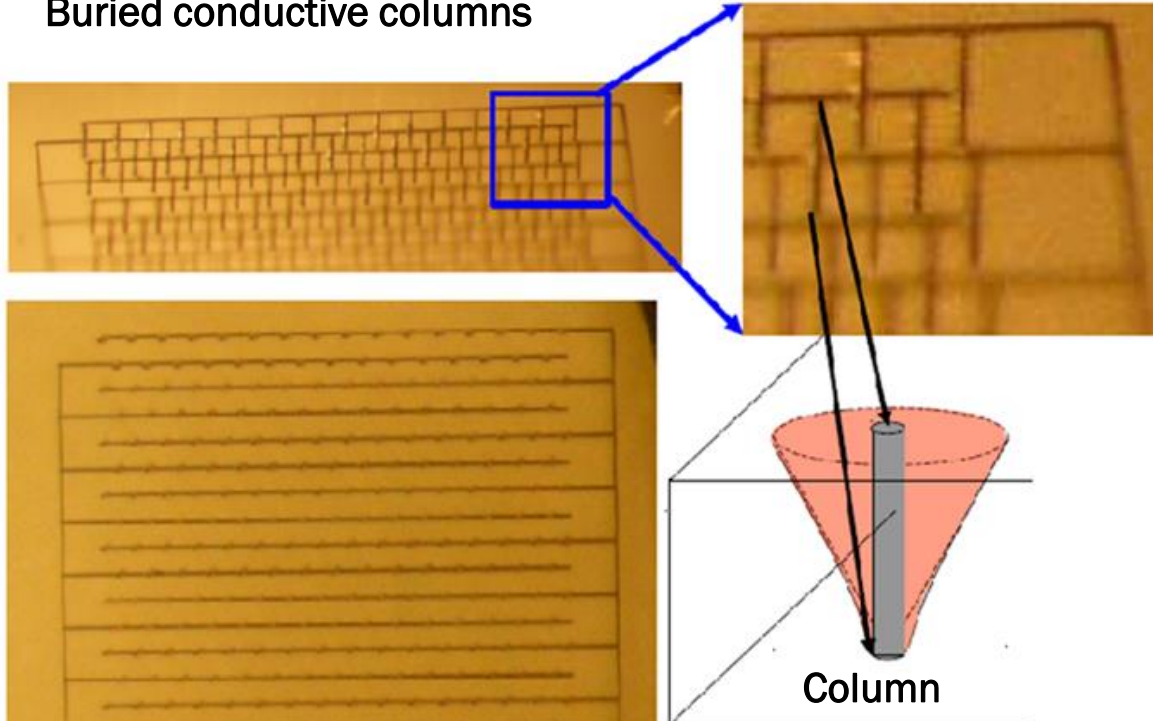
- the geometry and physical properties of the detector
- the medium in which the measurement is made
- the energy of the beam, the size of the field

| Properties | Diamond | Silicon | |
|---|---------|---------|--------------------|
| Gap [eV] | 5.5 | 1.12 | Low dark current |
| Hole Mobility [cm^2/Vs] | 1200 | 450 | |
| Electron Mobility [cm^2/Vs] | 1800 | 1450 | Fast Response Time |
| Effective atomic number Z_{eff} | 6 | 14 | Tissue Equivalence |
| Wigner Energy [eV] | 43 | 13-20 | Radiation Hardness |

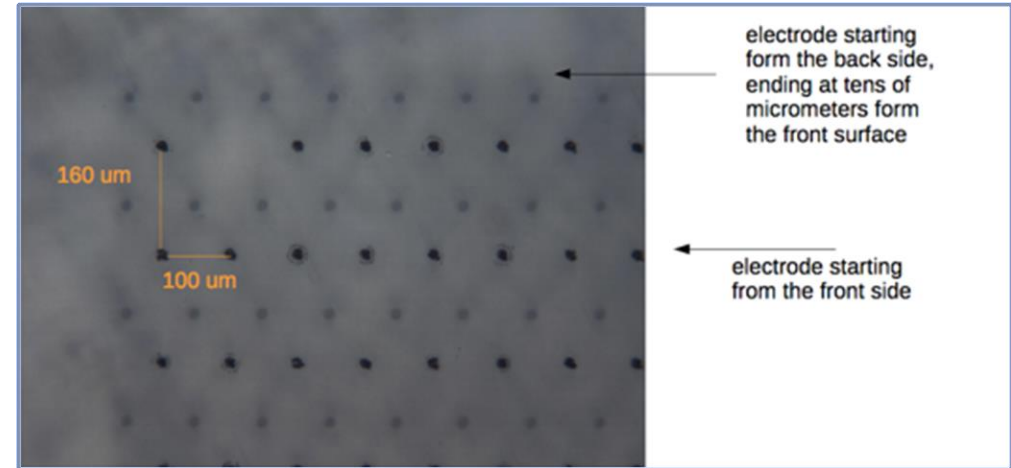


- Low bias voltage (few V) with high active volume;
- Reproducibility of the elementary 3D cell
- An 'all-carbon' detector exposed to the beam (tissue equivalence)
- High spatial segmentation, even $0.1 \times 0.1 \text{ mm}^2$
- High resistance to radiation damage

Buried conductive columns



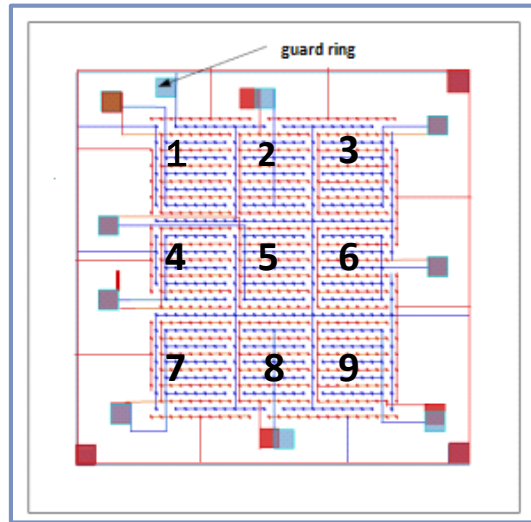
Polycrystalline diamond with 3D structures produced by laser pulses



Graphitic conductive path resistivity:

$$\rho \cong 60 \pm 20 \text{ m}\Omega\text{cm} \quad @\text{ns}$$

$$\rho \cong 900 \pm 300 \text{ m}\Omega\text{cm} \quad @\text{fs}$$



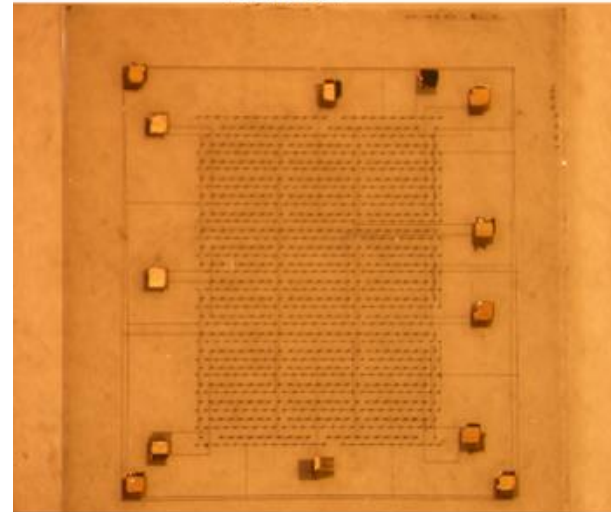
Schematic view of two 3D detectors with the same geometry & different substrates:



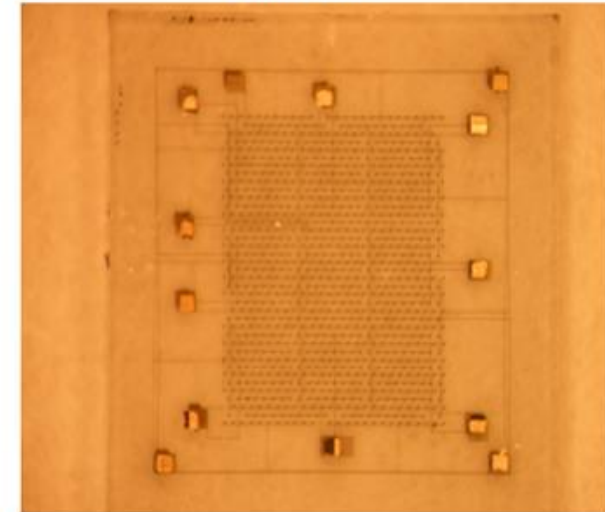
Diamond & Diamond on Iridium

3D DETECTORS

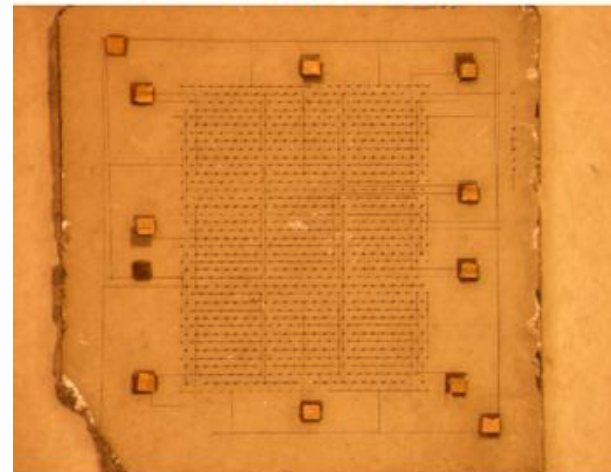
BACK DOI



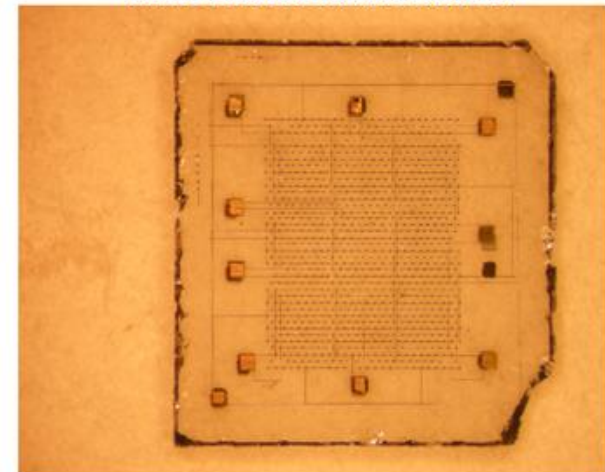
FRONT DOI



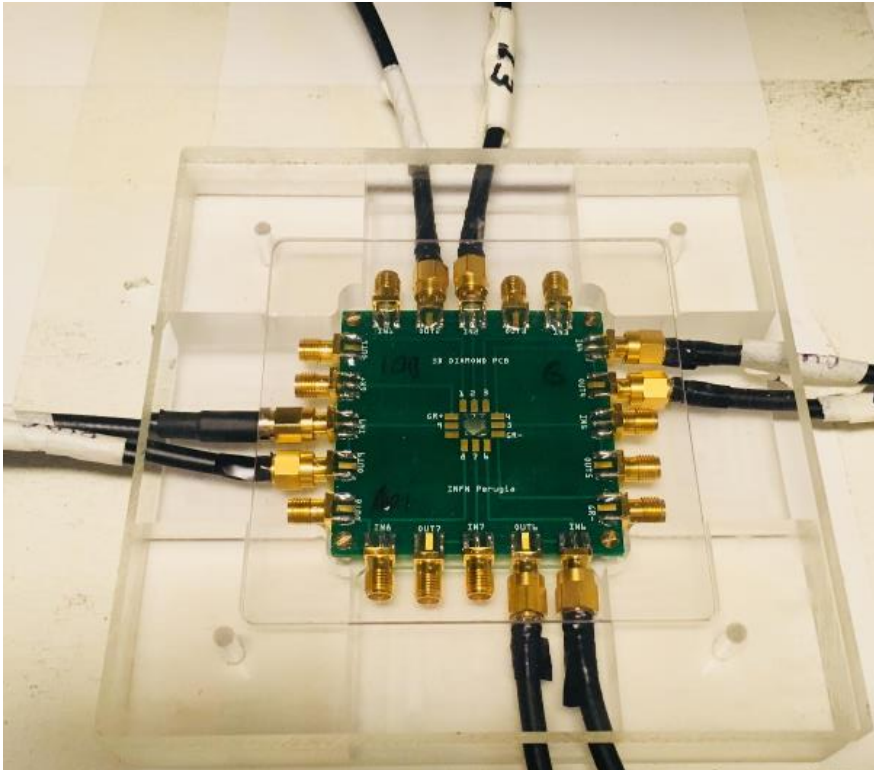
BACK POLYCRYSTALLINE DIAMOND



FRONT POLYCRYSTALLINE DIAMOND

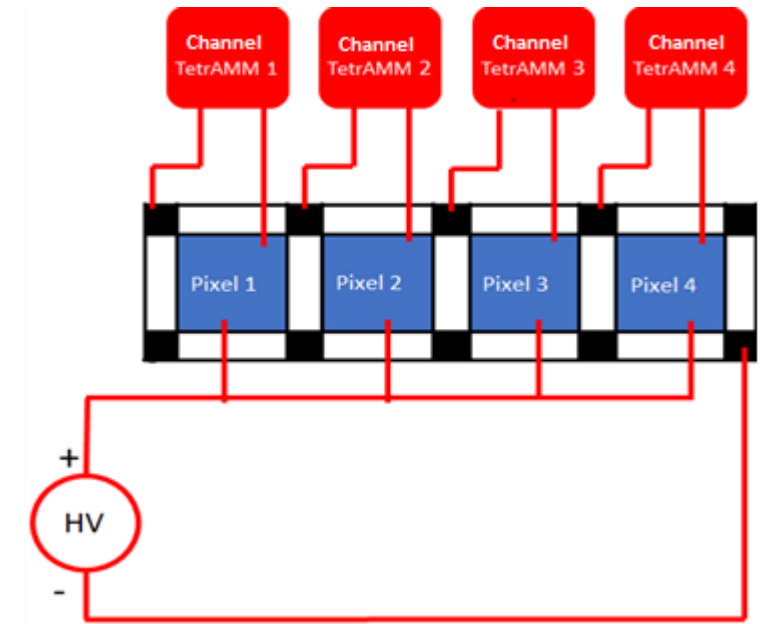


4/8 cells readout in parallel

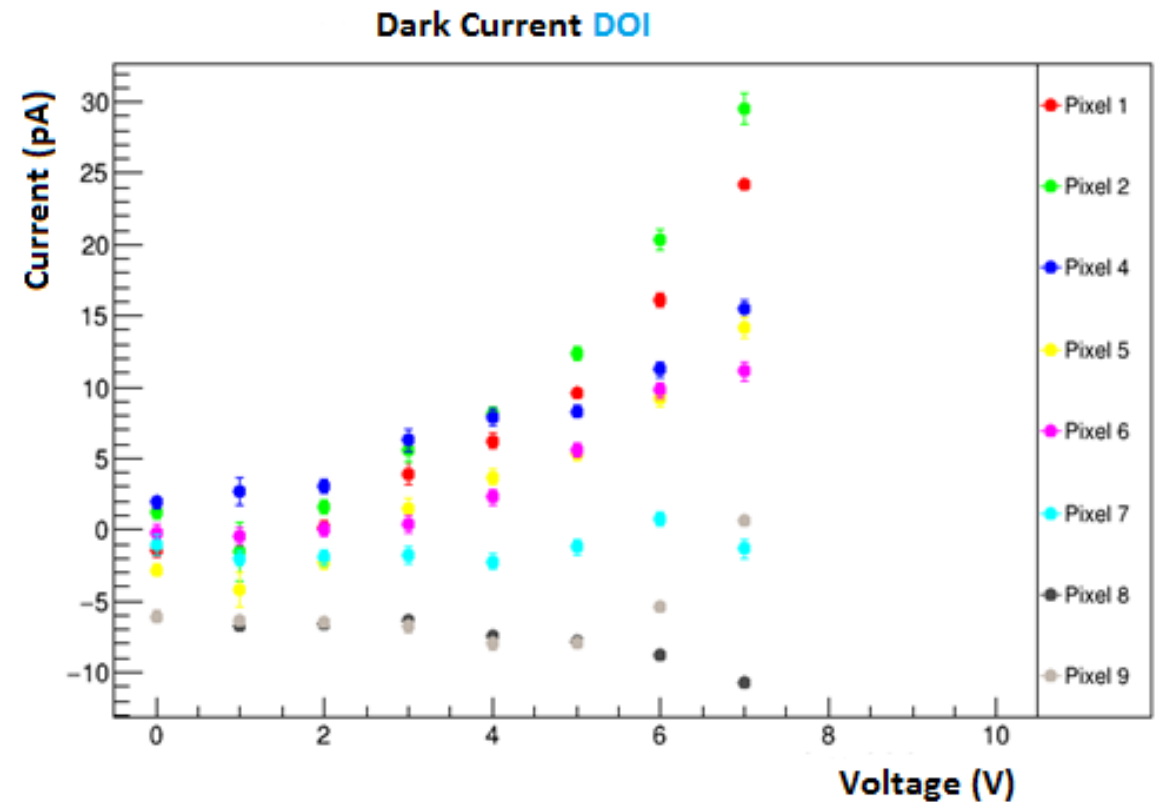
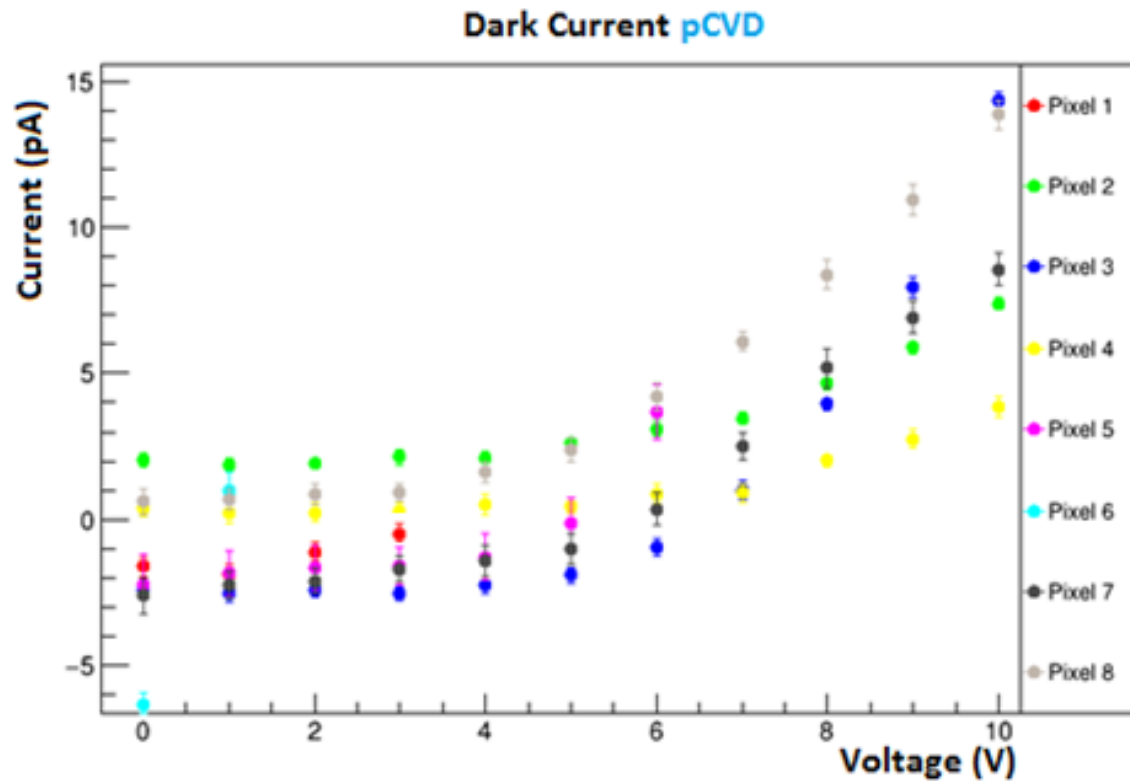


TETRAMM Picoamperometer :

4 readout channels + 1 integrated high voltage source



Before irradiating the detectors:



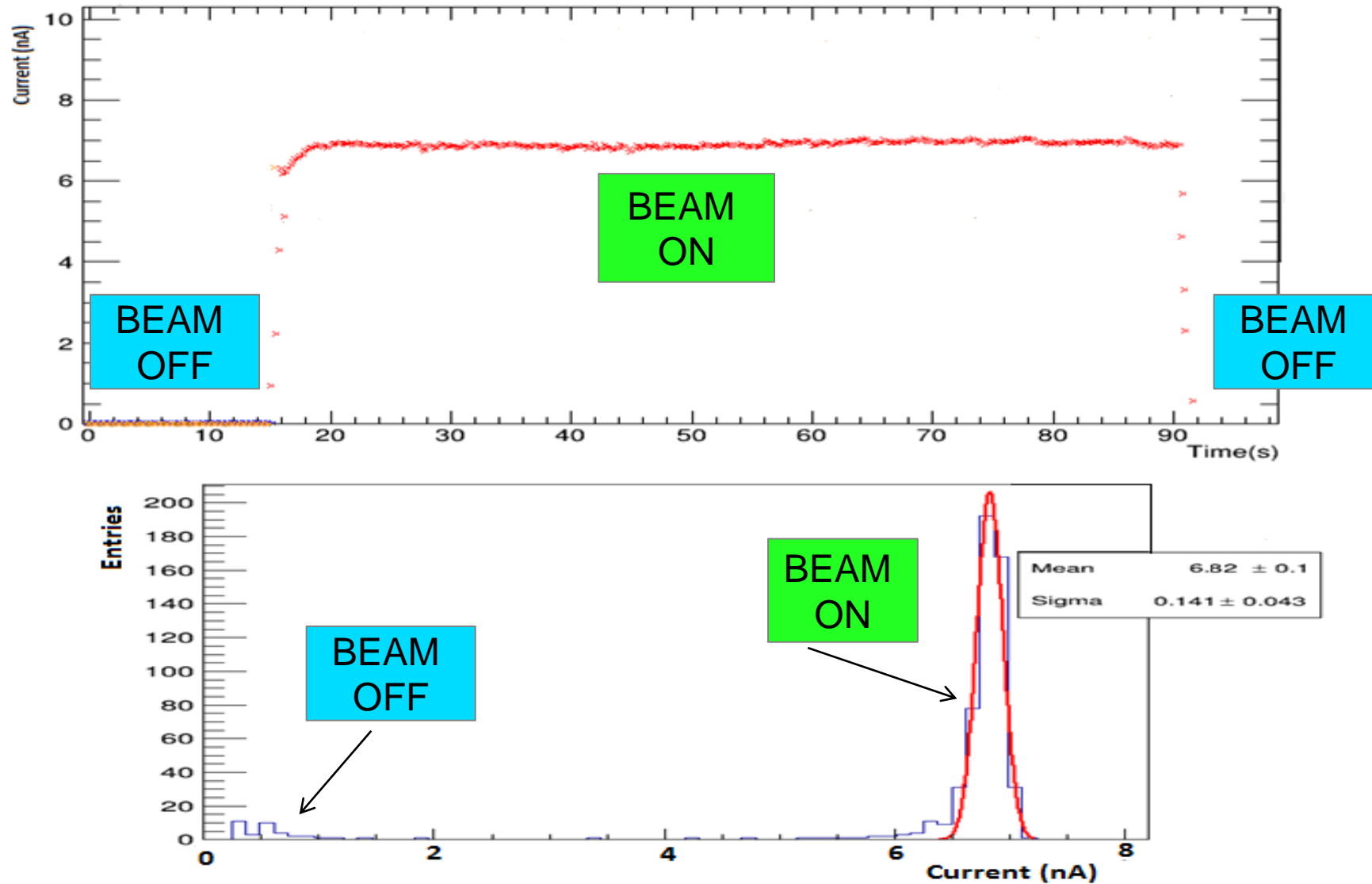
For the diamond on iridium substrate detector, it was not possible to apply voltages over 7V because the dark current became too high and the response unstable.



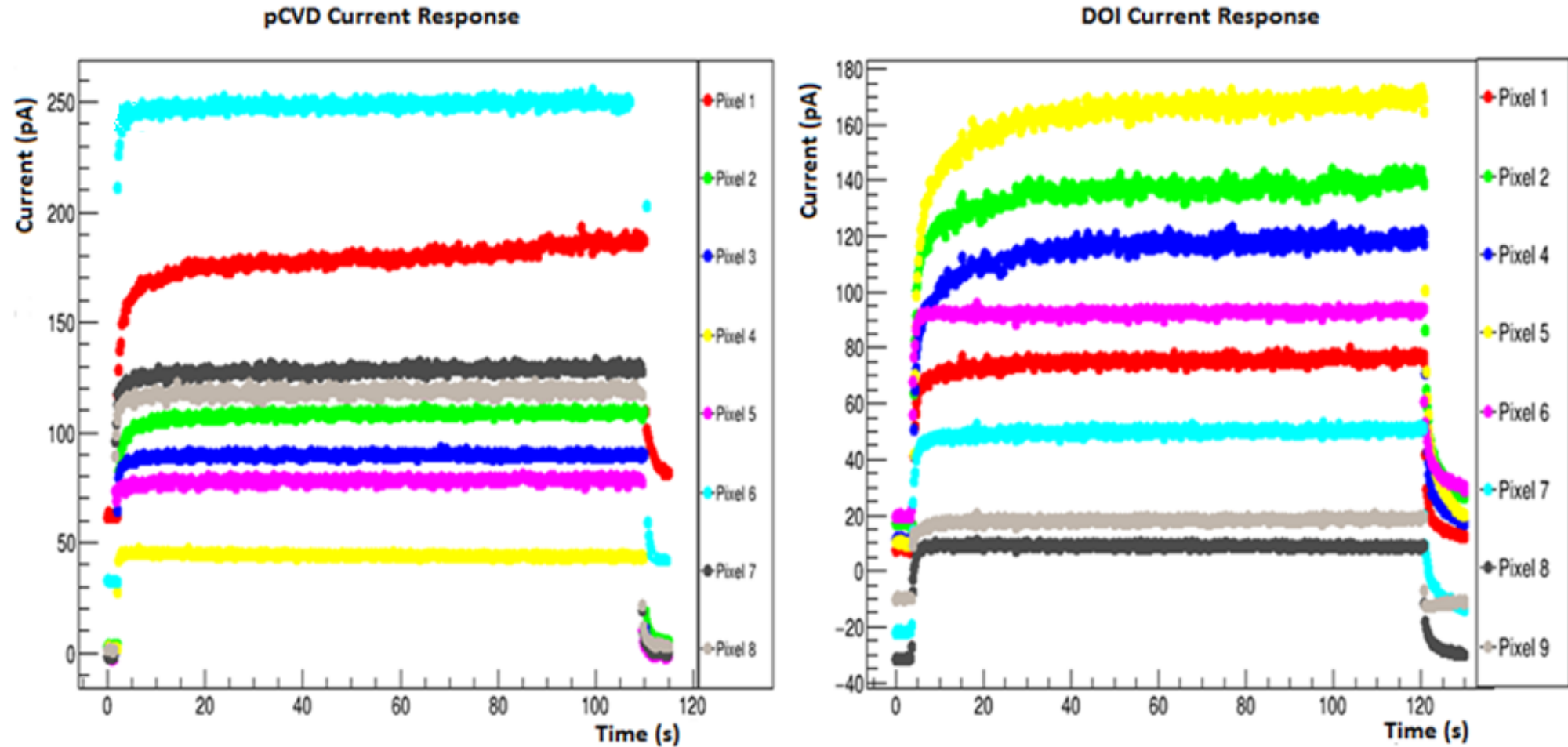
Newton scientific X-ray tube



- ✓ Max voltage 50 kV
- ✓ Max current 200 μ A
- ✓ Opening angle of the emitted cone 100°



XRay tube voltage 30 kV, current 140 μ A. Detector bias voltage 4V.



XRay tube voltage 30 kV, current 140 uA. Detector bias voltage 4V.

pCVD

| Pixel | Rise Time (s) | Fall Time (s) |
|-------|---------------|---------------|
| 1 | 2.50 | 5.00 |
| 2 | 0.30 | 0.60 |
| 3 | 0.50 | 0.20 |
| 4 | 0.30 | 0.30 |
| 5 | 0.10 | 0.30 |
| 6 | 0.60 | 0.40 |
| 7 | 0.60 | 0.20 |
| 8 | 0.50 | 0.40 |

Except pixel 1, rise and fall time of the pCVD pixels response are below 1s

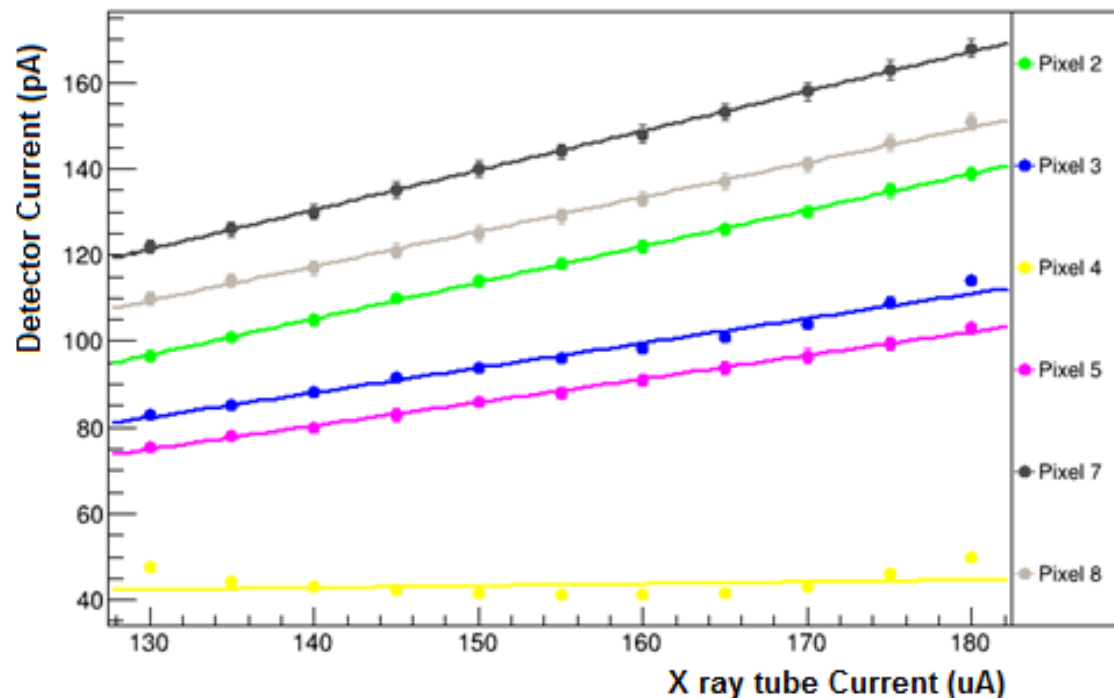
DOI

| Pixel | Rise Time (s) | Fall Time (s) |
|-------|---------------|---------------|
| 1 | 2.50 | 3.40 |
| 2 | 4.50 | 6.60 |
| 4 | 6.10 | 4.60 |
| 5 | 6.20 | 5.00 |
| 6 | 1.00 | 9.40 |
| 7 | 1.40 | 9.20 |
| 8 | 1.20 | 3.00 |
| 9 | 3.10 | 0.20 |

None of the DOI pixels has both rise and fall time below 1s

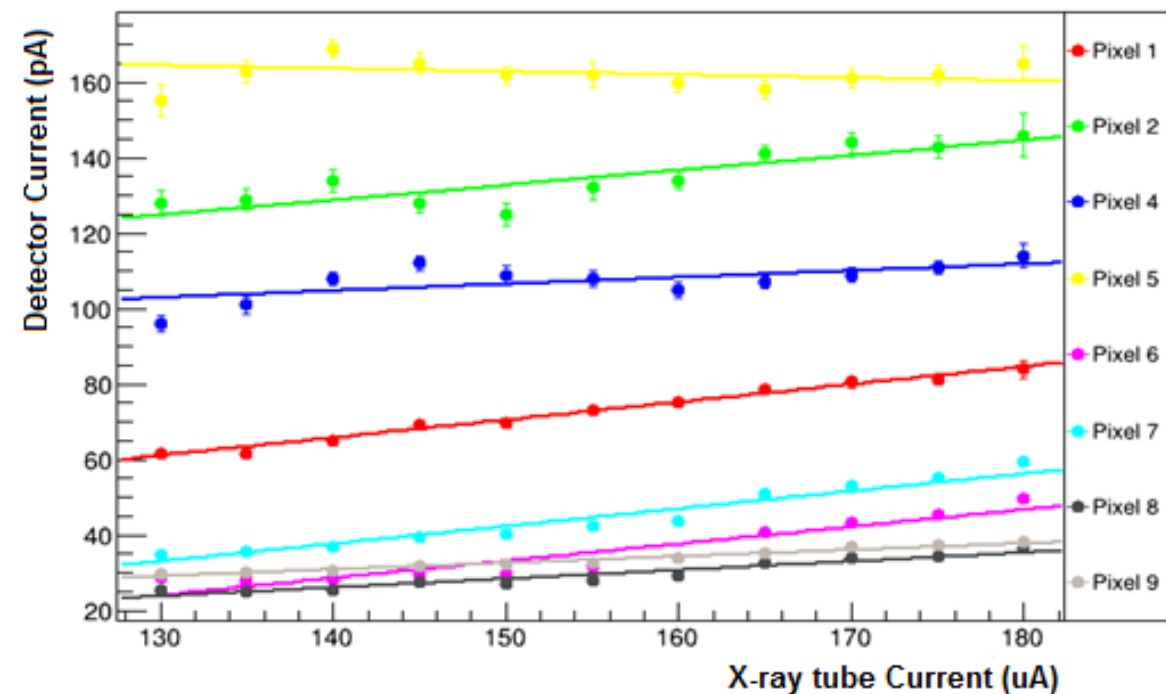
XRay tube voltage 30 kV, current 140 uA. Detector bias voltage 4V.

pCVD



Max deviation from linearity: <3%
 pixel 4: bad pixel

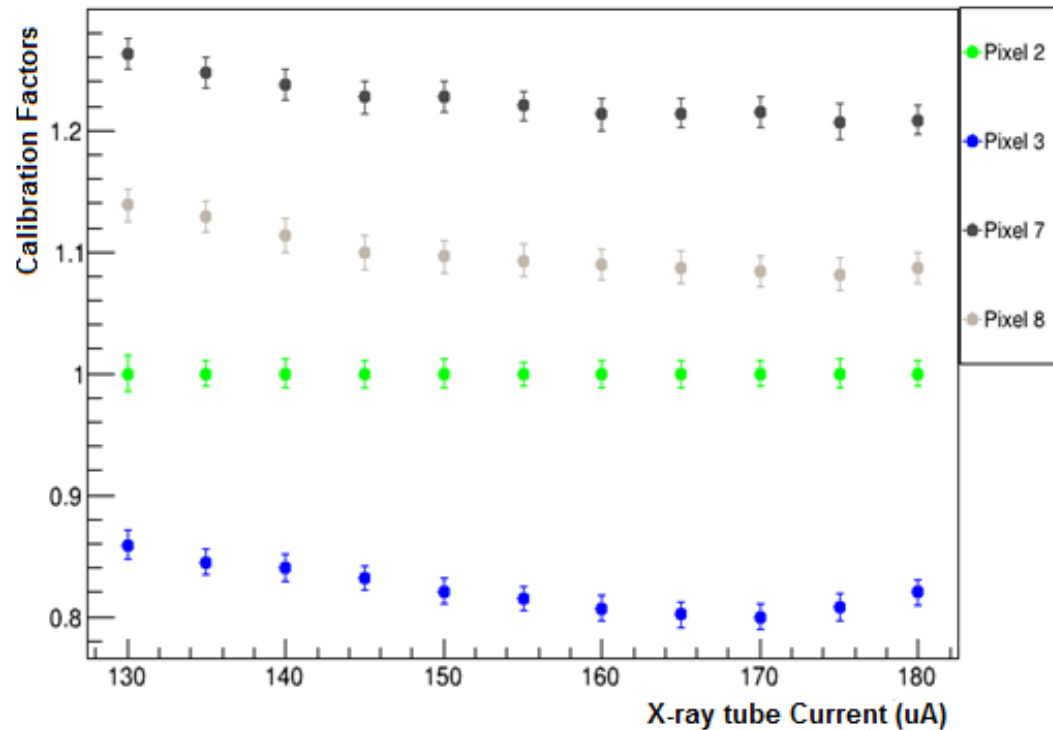
DOI



Max deviation from linearity: >3%
 Pixel 4,5: bad pixels

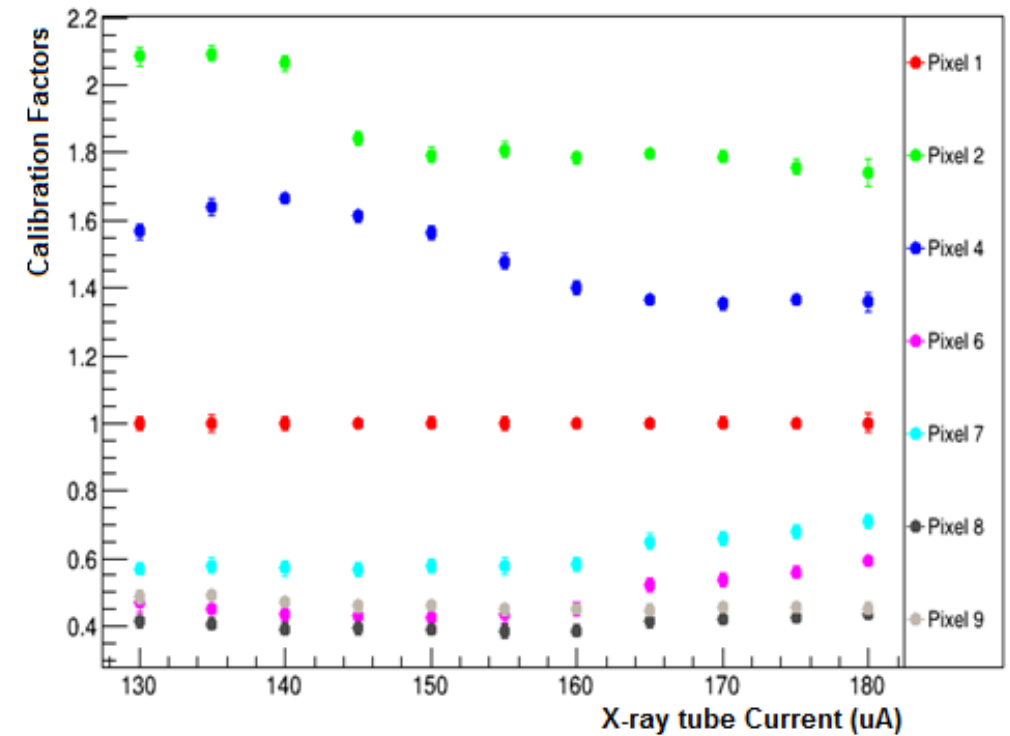
XRay tube voltage 30 kV, current 140 uA. Detector bias voltage 4V.

pCVD



Max deviation <4%

DOI



Max deviation >8%

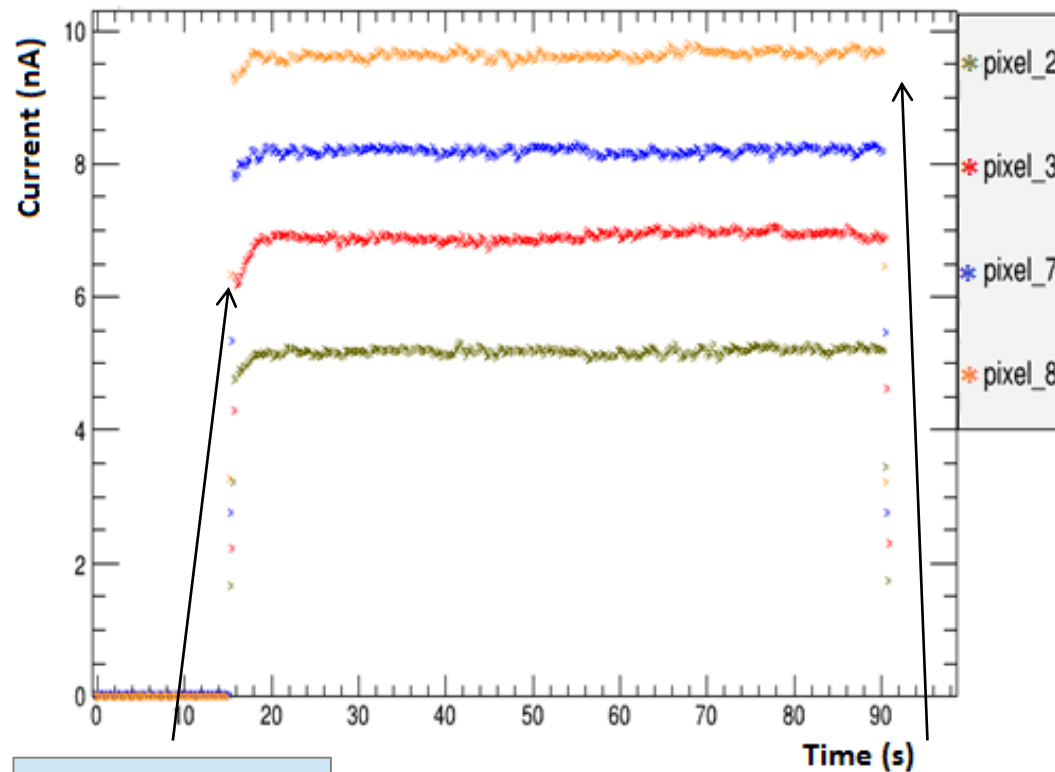
Pixel 2,4 bad pixels

| | pCVD | DOI |
|----------------------------------|---------------------------------------|---------------------------------------|
| Dark Current | < 15 pA | < 30 pA |
| Operating Voltage | ≥ 4 V | 4 V |
| Repeatability | < 3 % | < 3 % |
| Stability | < 3 % | < 5 % |
| Linearity | < 2.7 % | > 3 % |
| Max signal to noise ratio | 1845 | 412 |
| Intercalibration factors | < 4 % | > 8 % |
| Mean rise time | (0.73 ± 0.39) s | (3.25 ± 2.13) s |
| Mean fall time | (0.35 ± 0.19) s | (5.18 ± 3.14) s |



- ✓ Medical linear accelerator (Elekta Synergy Sband)
 - ✓ 6 MV photons
 - ✓ $10 \times 10 \text{ cm}^2$ field
 - ✓ $1.6 \times 1.6 \text{ cm}^2$
 - ✓ $0.8 \times 0.8 \text{ cm}^2$
- ✓ The detector encapsulated inside a $14 \times 14 \times 14 \text{ cm}^3$ PMMA block at 10 cm depth
- ✓ placed at 100 cm from the beam source.

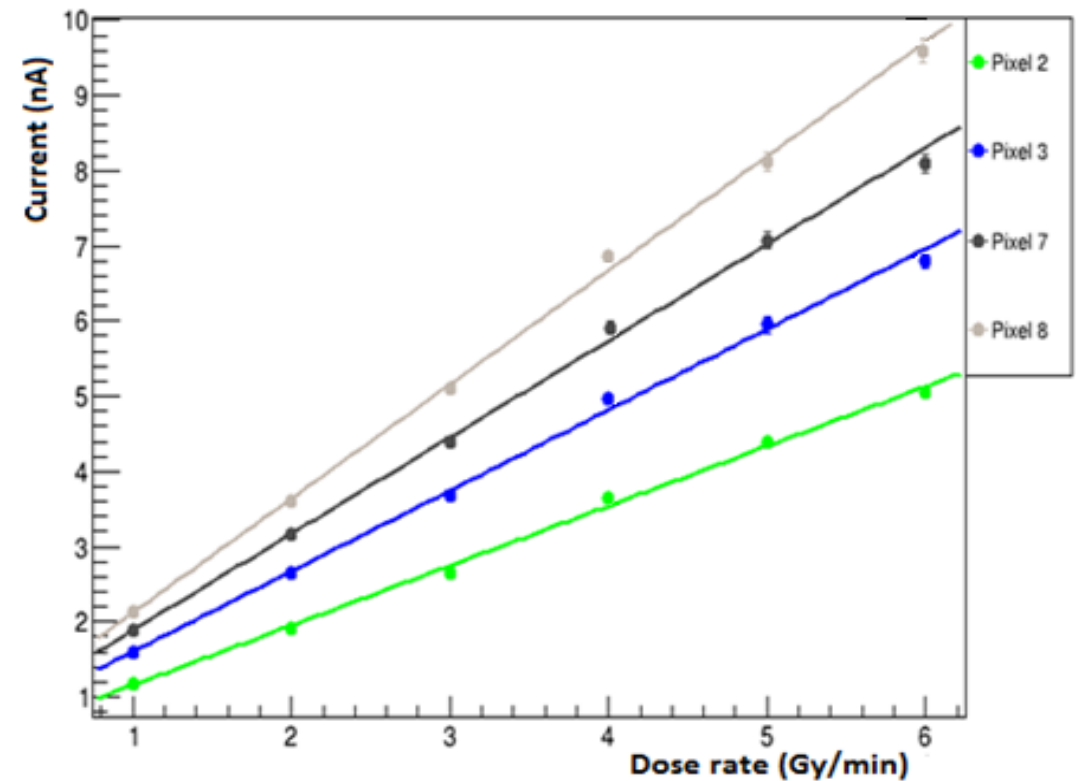
Detector response at 6 Gy/min



Rise time <0.5 s
at 6Gy/min

Fall time <0.3 s
at 6Gy/min

Dose rate linearity



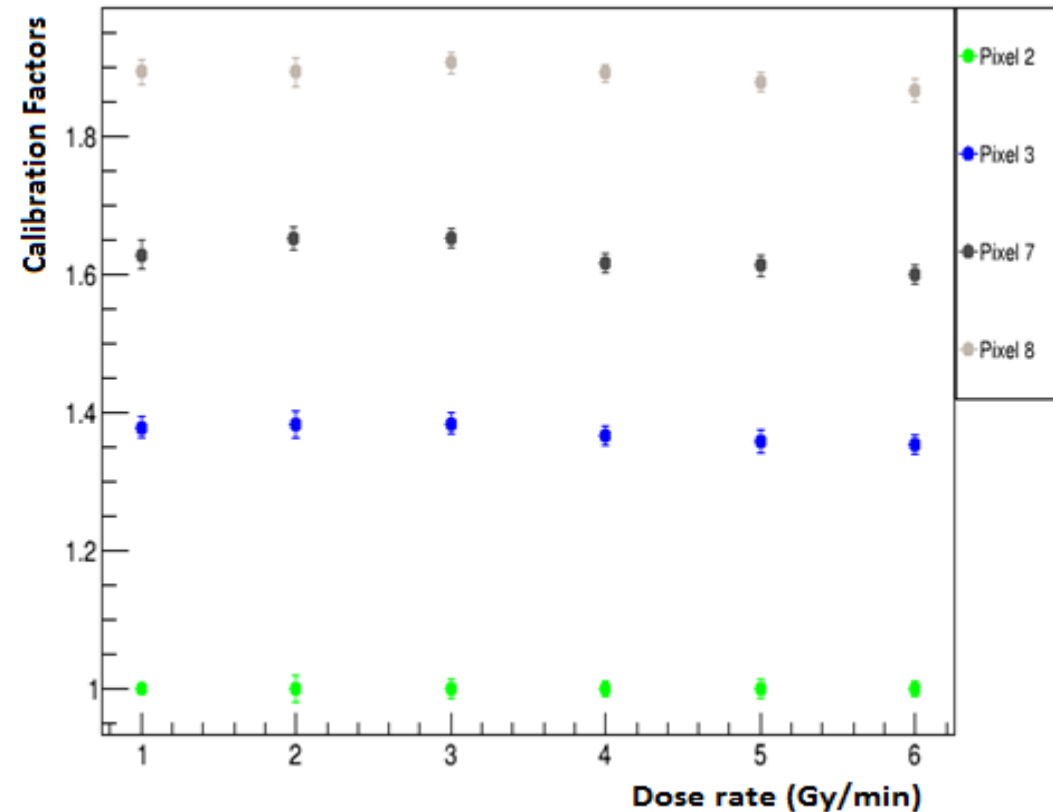
Max deviation from linearity 2%

Repeatability

| Pixel | Dose-rate | |
|-------|-----------|----------|
| | 2 Gy/min | 6 Gy/min |
| 2 | 0.87% | 0.72% |
| 3 | 0.10% | 0.91% |
| 7 | 0.18% | 0.47% |
| 8 | 0.26% | 0.41% |

Max deviation < 1%

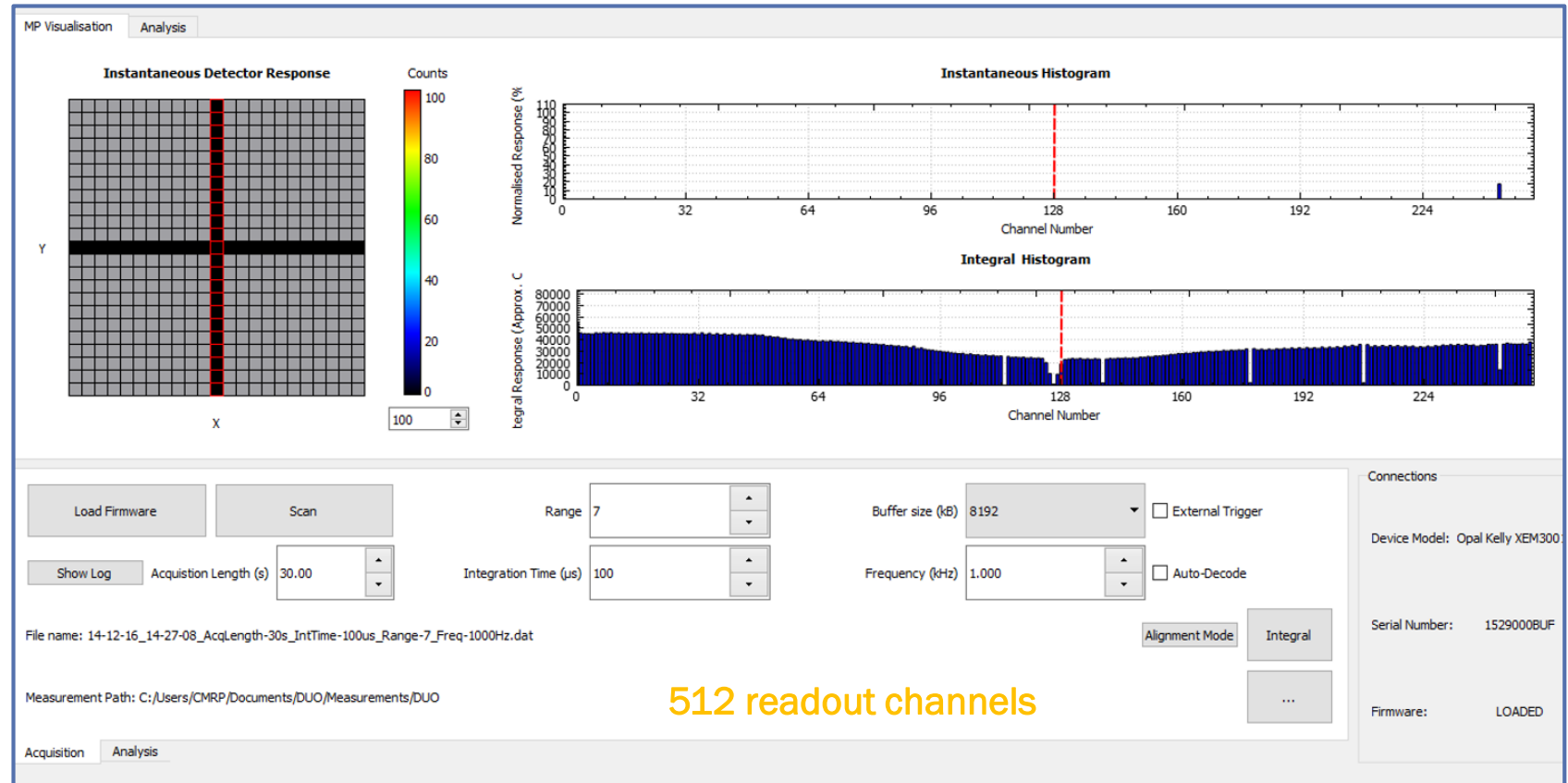
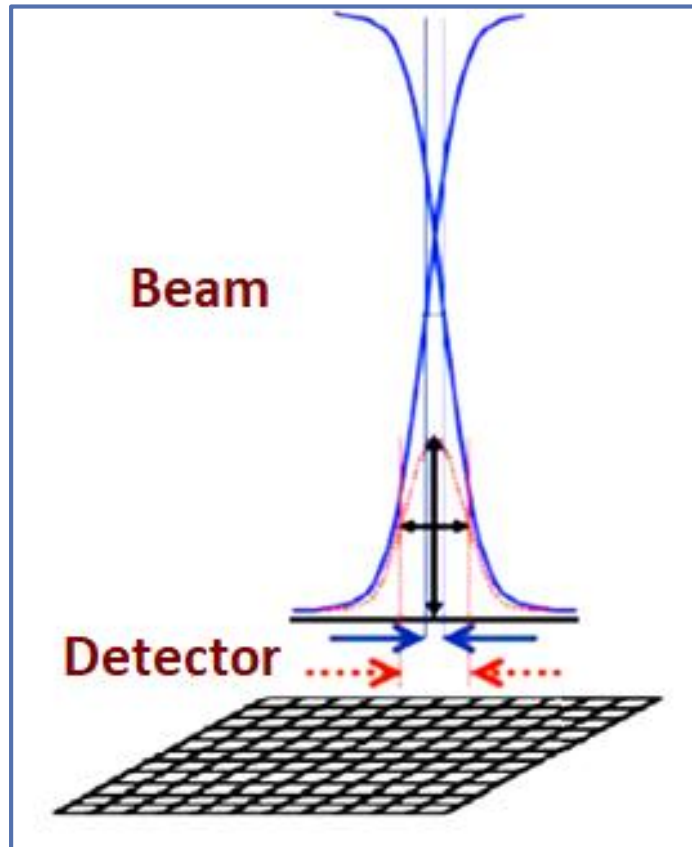
Calibration factors normalized to pixel 2



Max deviation of calibration factors 2%

Multi-channel read-out system

Wollongong University



- ✓ Results demonstrate that the polycrystalline diamond substrate compared to the diamond on iridium is more suitable for dosimetric applications since it shows better linearity, repeatability and time stability and has a faster response to the photon beam.
- ✓ Each single pixel of the detector has a different sensitivity to the radiation beam and is partially influenced by the experimental environment, but the response is linear and stable hence different calibration factors can be applied to obtain an overall detector response and reduce the uncertainty of the delivered dose.
- ✓ A new highly segmented polycrystalline diamond dosimeter will be produced. Due to the simultaneous measurement of many points, a higher accuracy in measurements of very small size field profiles would be possible and the need of using many not standard correction factors will be greatly reduced.

Thank You For Your Attention

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