



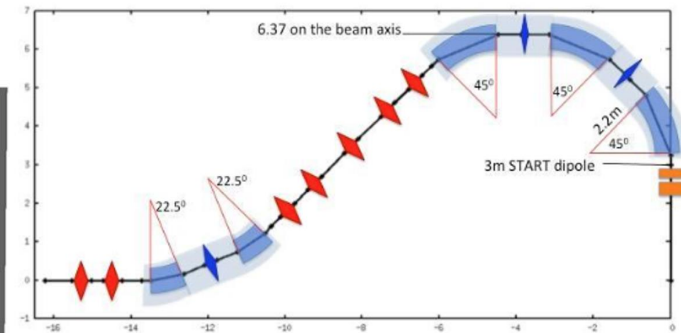
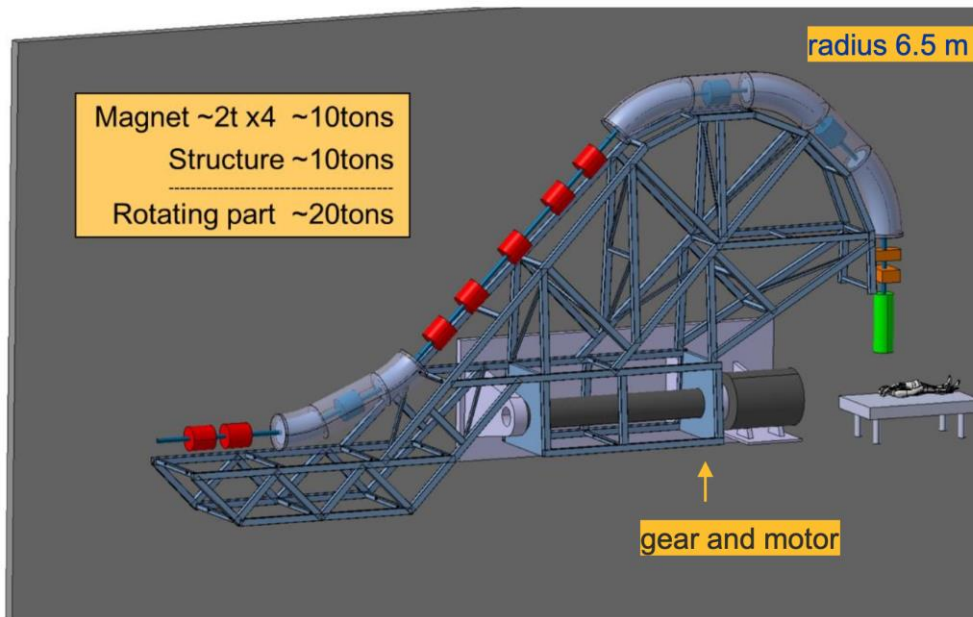
Gantry Design for the Heavy-Ion Therapy Medical Application

Andris Ratkus, Toms Torims, Jānis Vilcāns,
Luca Piacentini

30.06.2021

Gantry Mechanical Design

- **Gantry** – Rotating beam line sending the beam to precise positions to the patient



CNAO
Centro Nazionale di Adroterapia Oncologica

CNAO: Marco Pullia



CERN team: Mechanical & Materials
Engineering (MME) **Diego Perini, Luca Dassa**

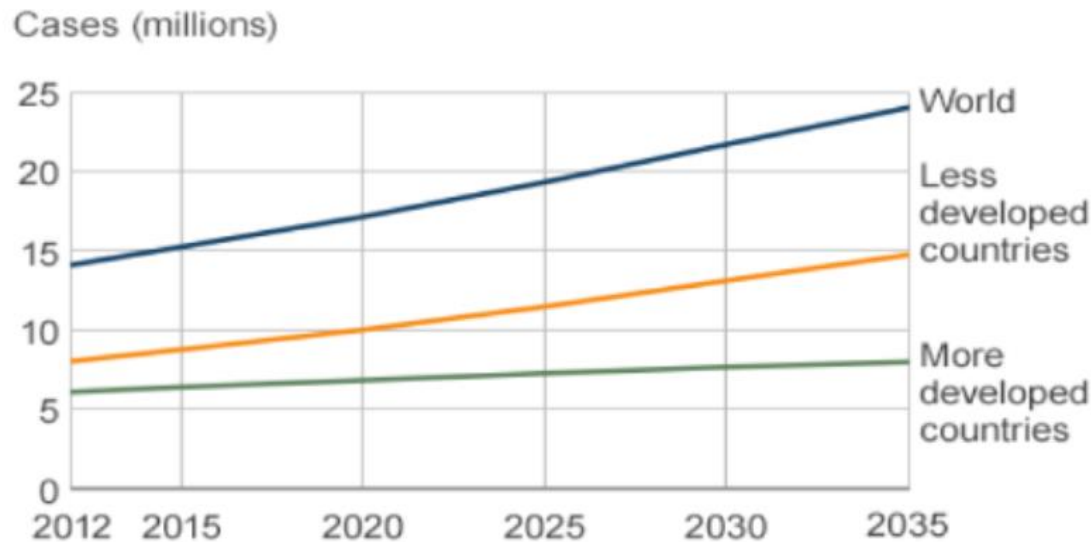
RTU Team: **Andris Ratkus,**
Toms Torims, Jānis Vilcāns, Luca Piacentini



Fighting against Cancer

- Cancer is the **second** leading cause of death globally
- Globally, nearly 1 in 6 deaths is due to cancer (WHO)

Predicted Global Cancer Cases



Source: WHO GloboCan

Timeline: 4 year,
started
1st of April 2021

HITRI
Heavy Ion Therapy Research Integration *plus*

Heavy Ion Therapy Research Integration *plus*

Why hadron therapy (proton or ions)

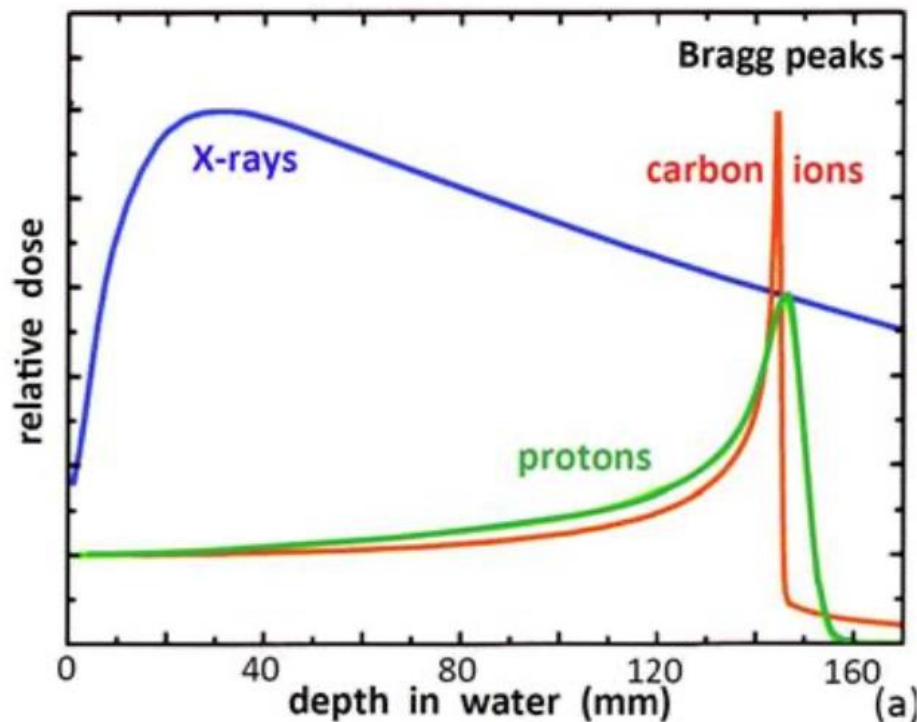
Different from X-rays or electrons, protons (and ions) deposit their energy at a given depth inside the tissues, **minimising dose to the organs close to the tumour**, sparing nearby organs.

Physical phenomena:

X-ray Radiation Therapy is improving as well

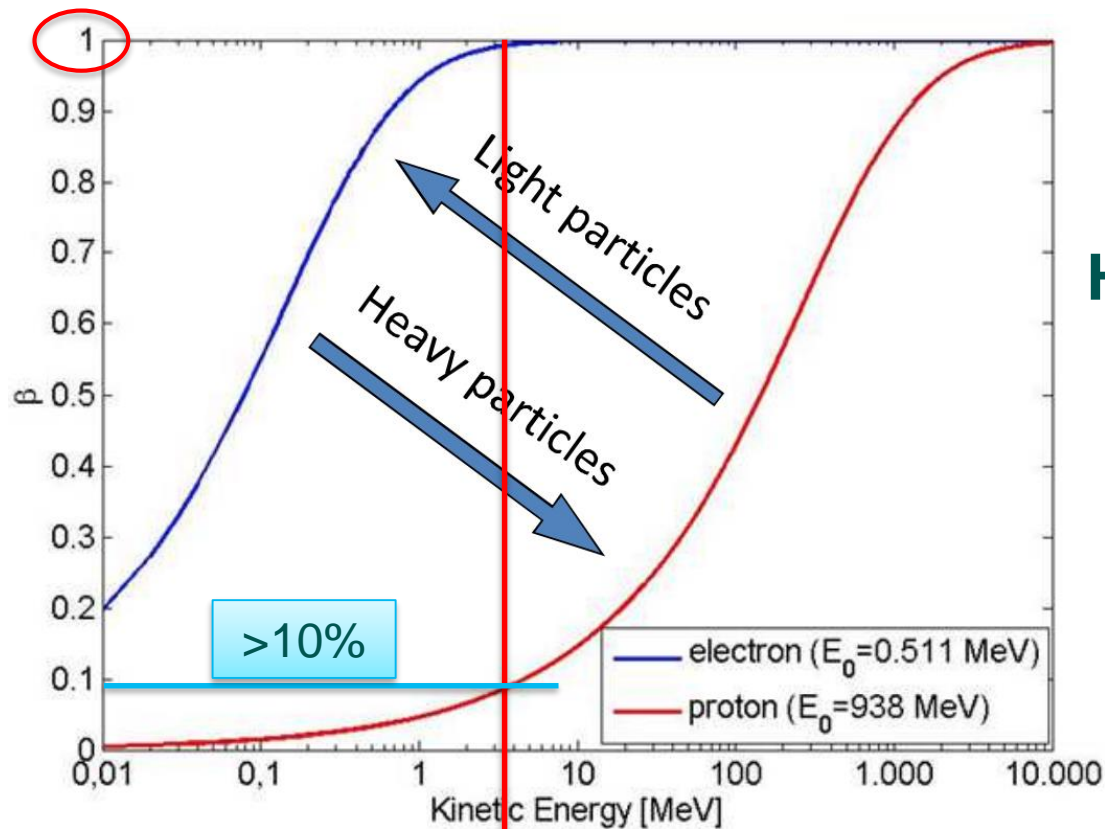
Proton therapy is mainly recommended for:

- Some specific tumours close to critical organs
- Niche therapy



Circumstances to be taken into account

- A proton is approx. **1800 times heavier** than an electron.
- Higher energy is needed to accelerate protons and ions

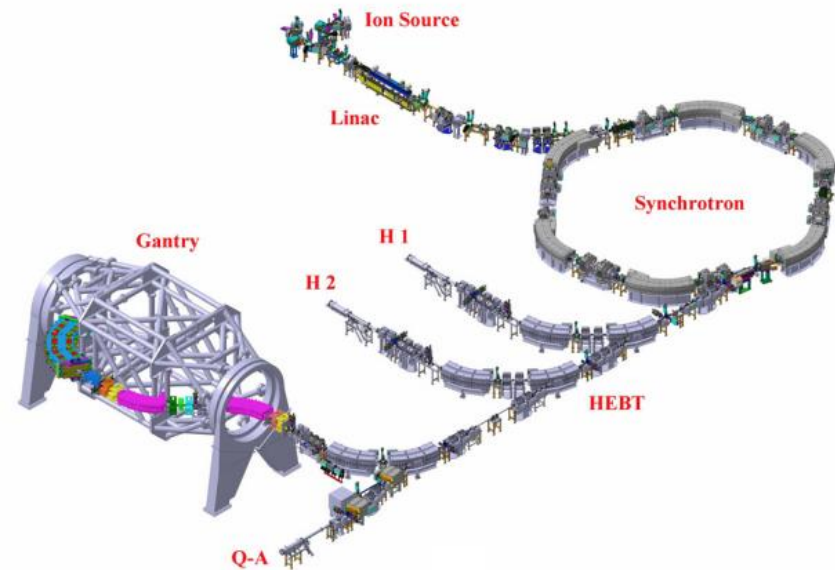


**Higher energy –
LARGER SIZE !!!**

~3 MeV

Existing facilities

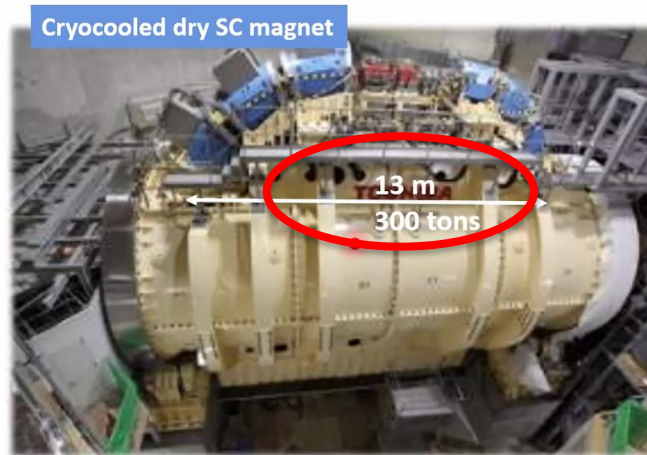
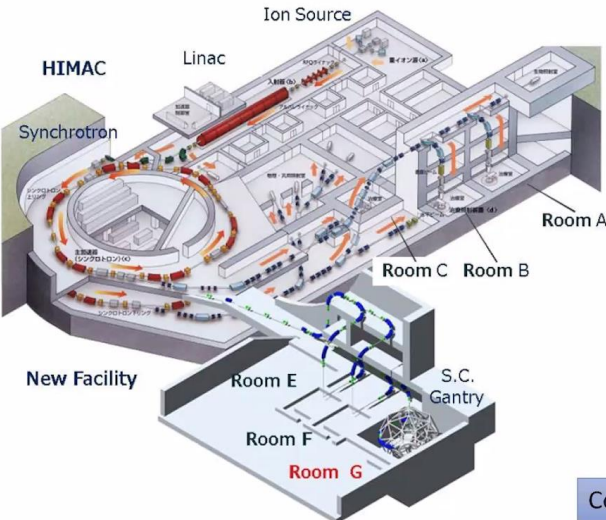
The Heidelberg Ion Therapy Facility gantry (RT magnets):
 $L=25\text{ m}$, $F = 13\text{ m}$, **600 tons**



Japan: **HIMAC** at QST-NIRS
First SC Gantry in operation 2018



Source: The Heidelberg Ion Therapy Facility (HIT)



Courtesy of T. Shirai, QST-NIRS

Rīgas Tehniskā universitāte

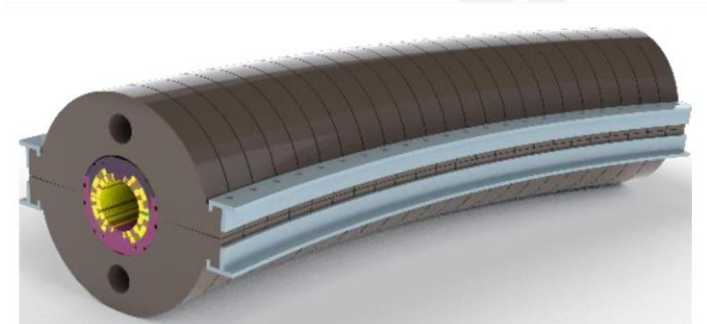
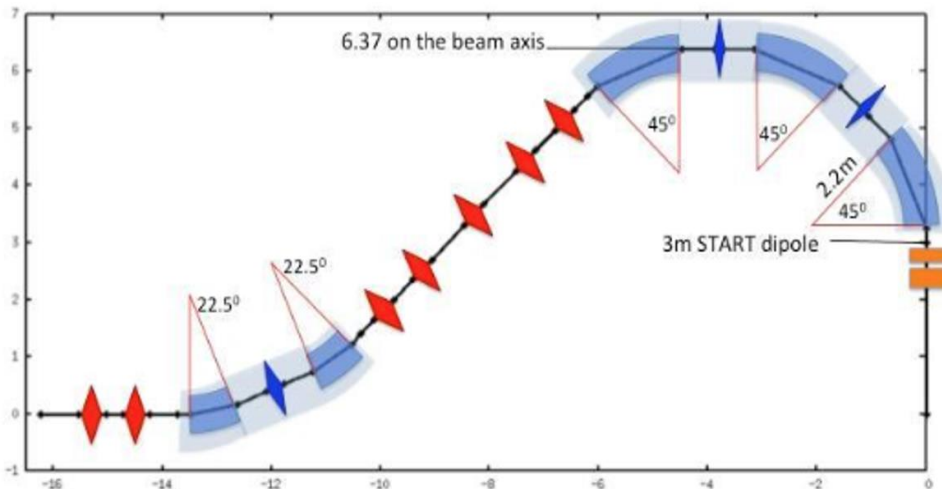
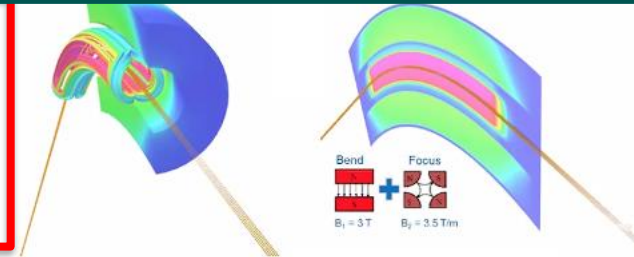


New generation of compact ion therapy accelerators

NIMMS— Next Ion Medical Machine Study by Elena Benedetto

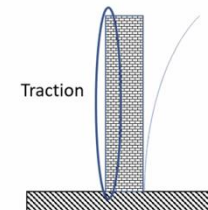
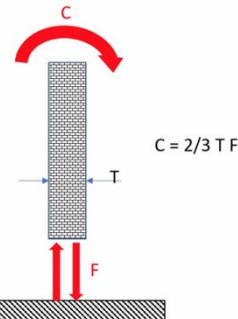
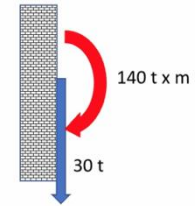
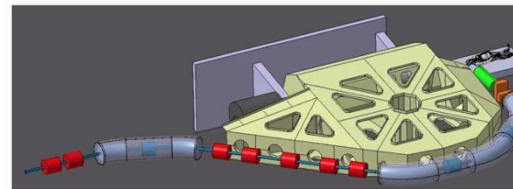
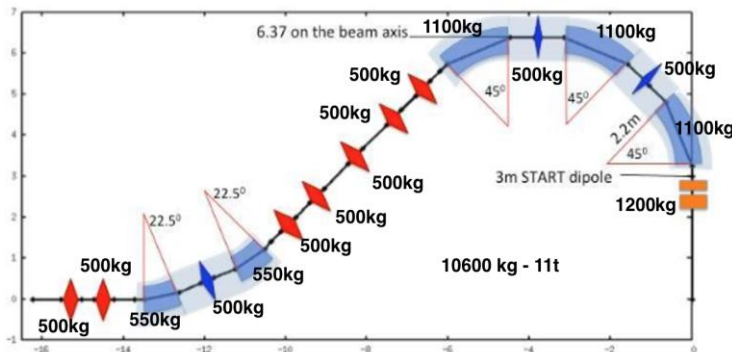
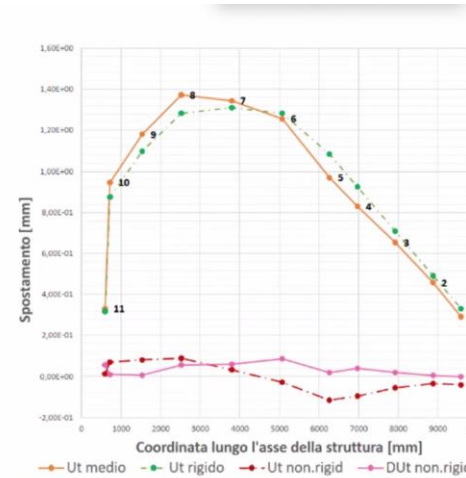
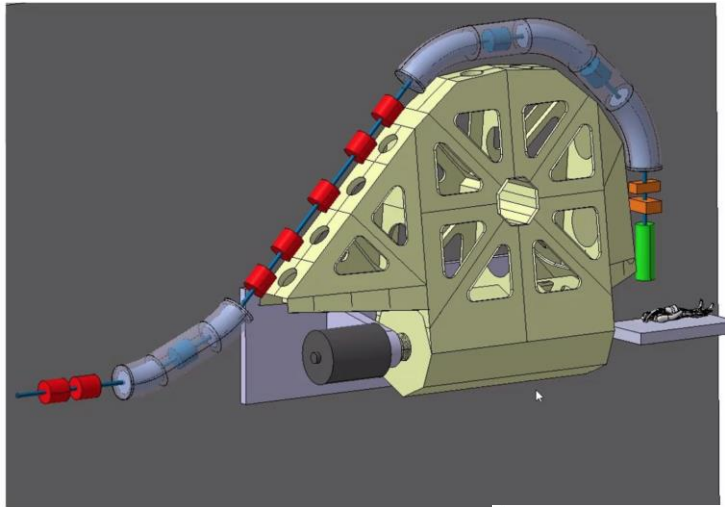
WP 7 (One WP of 14 WP) Challenges

- New superconducting magnets
- Optimised beam transport and instrumentation
- Higher accelerating gradient
- **Lower costs**
- **Weight lower than 100 tons and length below 16 metres**



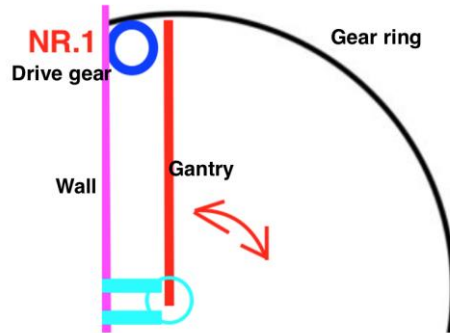
Assumptions/ calculation I

- $360^\circ \rightarrow 220^\circ$ to reduce dimensions
- Remove drive from axis

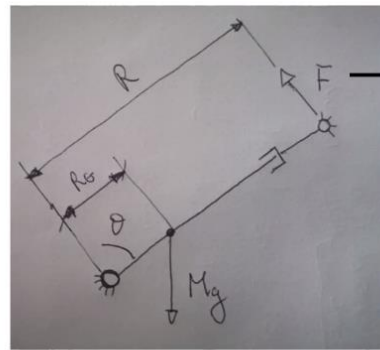
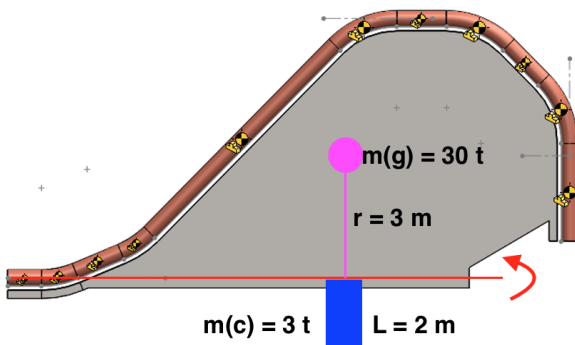


Assumptions/ calculation II

- Gears
- Inertia
- Torques etc.

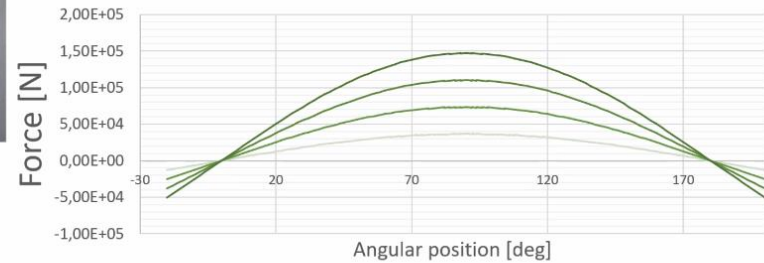


Wt (kN)	S45C tensile str. 628/3 (N/mm ²)	Module (mm)	Dp 1/mod (mm ⁻¹)	F Face width of gear (mm)	with TWO drive gears Face width of gear/ 2 (mm)	Y Lewis Factor	Number of tooth	Small gear contacting pitch circle diameter (mm)
450	209	16	0,0625	340	170	0,396	40	640
450	209	16	0,0625	350	175	0,384	38	608
450	209	16	0,0625	360	180	0,374	34	544
450	209	16	0,0625	370	185	0,364	30	480
450	209	20	0,05	290	145	0,371	34	680
450	209	20	0,05	300	150	0,359	30	600
450	209	20	0,05	310	155	0,347	26	520
450	209	20	0,05	320	160	0,336	22	440



$$F = Mg \frac{R_G}{R} \sin \theta$$

Comparison between forces with the COG at different radial distances



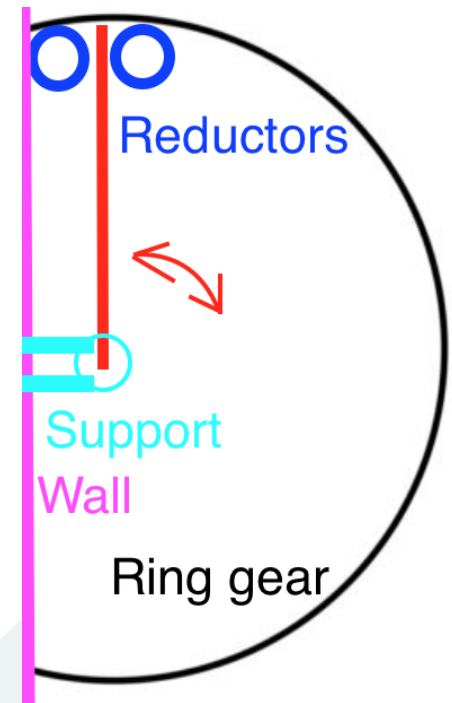
↑ 10% **Weight**

↑ 1.5% **Inertia**

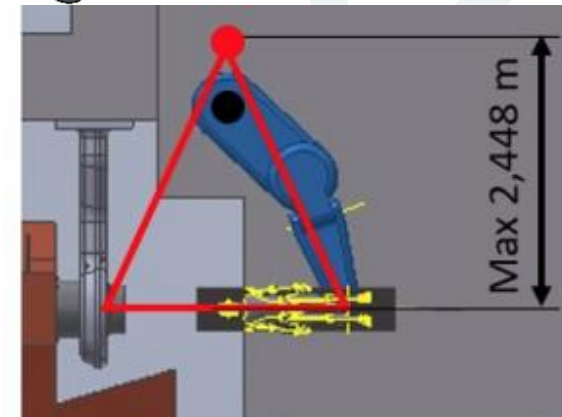
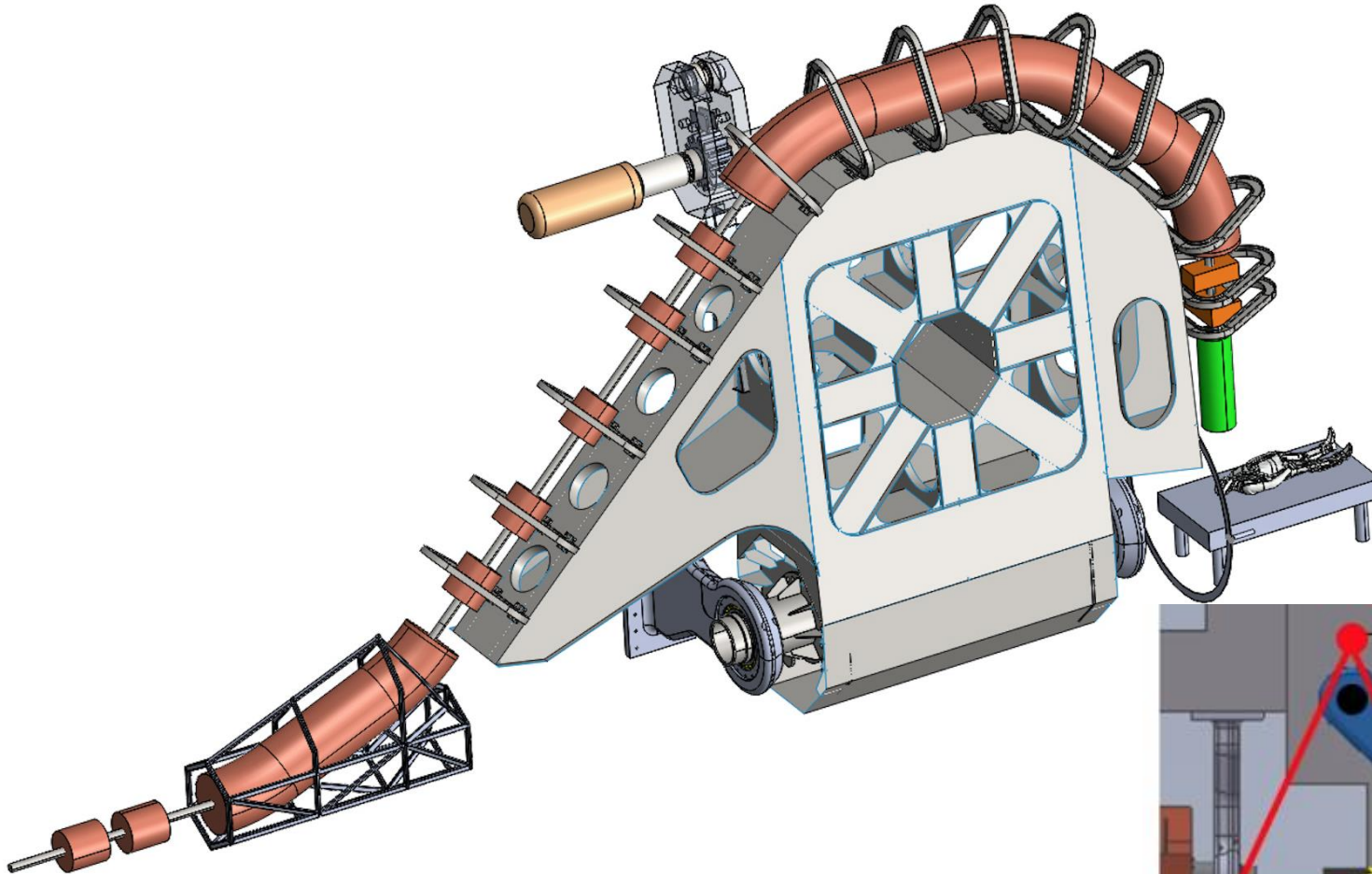
Assumptions/ calculation III

Gantry speeds:

- Target speed – 1 rpm \gg 30 sec.
- 1 rpm – average speed value with steps:
 - “Soft start”
 - “Accelerating stage”
 - **“MAX speed”**
 - “Deaccelerating stage”
 - “Positioning stage”
- “MAX speed” $>$ 1rpm



Iteration process



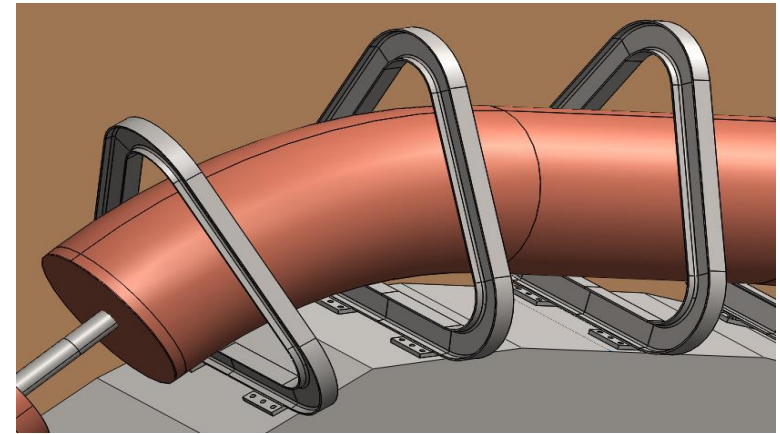
Evaluation of solutions

Config	Pros	Cons	wearables	Safety	Deformation Performances	Moving Mass	Inertia	Loads on wall	Brakes position	green
Large gear	<ol style="list-style-type: none"> 1. Brakes on the outside 2. Driven from outside 3. Available components on the market 4. Reduction 5. Multiple braking system points 	<ol style="list-style-type: none"> 1. High load on teeth 2. Difficult to manufacture or expensive 3. Constrain complexity 4. Reduction 5. (Accuracy of the large gear) 	<ol style="list-style-type: none"> 1. Gears 2. Motor 3. Bearings 4. Brakes 				N/A			
Double piston	<ol style="list-style-type: none"> 1. Accumulator possibility 2. Available components on the market 	<ol style="list-style-type: none"> 1. Space 2. Size of the pistons (length) 3. Brakes still on the axis 4. Accuracy 5. ... 	<ol style="list-style-type: none"> 1. Sealings 2. Bearings 							
			<ol style="list-style-type: none"> 5. Motor 6. Pulleys, rollers 7. Ropes 8. Brakes 9. Fluid 				N/A			
Motor-reduction	<ol style="list-style-type: none"> 1. Compact solution 2. (compensation of rigid rotation) 	<ol style="list-style-type: none"> 1. Reversibility due to reduction 2. Accuracy from reductor play deformations 3. ... 	<ol style="list-style-type: none"> 1. Gears 2. Motor 3. Bearings 4. Brakes 				N/A			

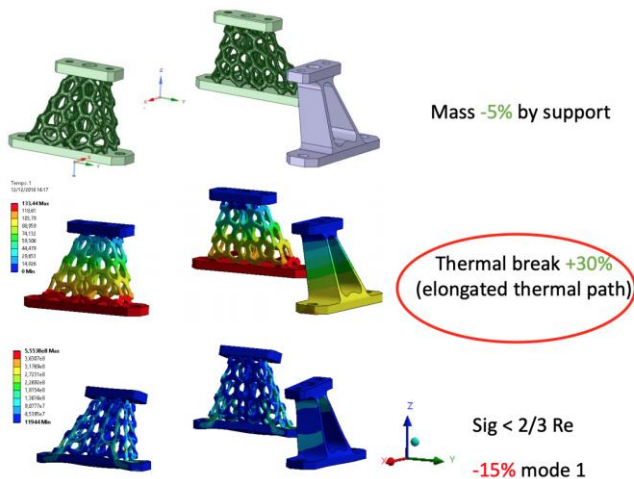
Solutions evaluation and Feasibility check should be continued

Future steps

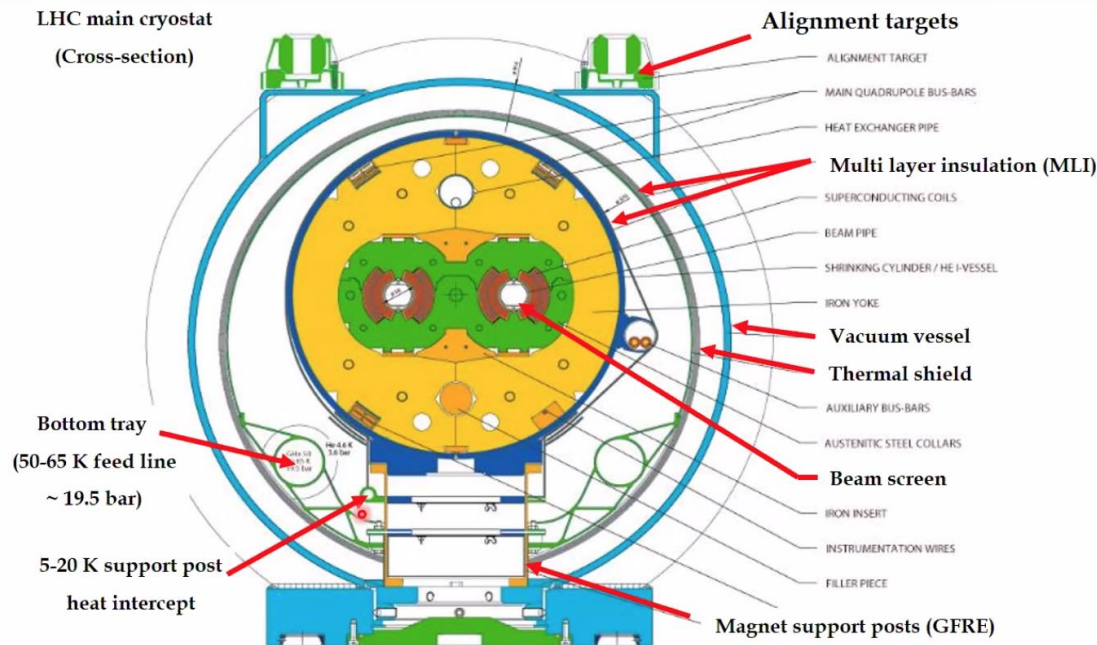
- The gantry design
- Cryogenic – vacuum “tube” fix to to the gantry
- Magnet fix in cryogenic “tube”



Cryogenic application: Dipole magnets of the LHC



Source: Y. Jan (CERN)



Source: T. Koettig CERN TE/CRG

Team and PhD thesis

CERN: Mechanical & Materials Engineering (MME) **Diego Perini,**
Luca Dassa

RTU: **Toms Torims, Andris Ratkus** and two PhD students **Jānis Vilcāns, Luca Piacentini**

- **Jānis Vilcāns**

Development of the rotational (mobile) cryostat system for the superconducting magnets in the hadron therapy installations.

- **Luca Piacentini**

Gantry design integration and development

Thanks